

1 **Title: - Development of an imaging toolbox to assess the therapeutic potential and biodistribution of**
2 **macrophages in a mouse model of multiple organ dysfunction**

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10 **Abstract**

11 Cell-based regenerative medicine therapies require robust preclinical safety, efficacy, biodistribution
12 and engraftment data prior to clinical testing. To address these challenges, we have developed an
13 imaging toolbox comprising multi-spectral optoacoustic tomography and ultrasonography, which
14 allows the degree of kidney, liver and cardiac injury and the extent of functional recovery to be
15 assessed non-invasively in a mouse model of multi-organ dysfunction. This toolbox allowed us to
16 determine the therapeutic effects of adoptively transferred M2 macrophages. Using bioluminescence
17 imaging, we could then investigate the association between amelioration and biodistribution.
18 Macrophage therapy improved kidney and liver function to a limited extent, but did not ameliorate
19 histological damage. No improvement in cardiac function was observed. Biodistribution analysis
20 showed that macrophages homed and persisted in the injured kidneys and liver, but did not populate
21 the heart. Our data suggest that the limited improvement observed in kidney and liver function could
22 be mediated by M2 macrophages.

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30 **Introduction**

31 Cell-based regenerative medicine therapies (RMTs), which include pluripotent stem cells,
32 mesenchymal stromal cells and macrophages, have the potential to treat a variety of human diseases.
33 However, before these therapies can be routinely used in the clinic, accurate information regarding
34 their safety and efficacy should be obtained from appropriate preclinical models. It is also important
35 to gain an understanding of the therapeutic mechanisms of the RMTs, such as whether their ability to
36 ameliorate injury is dependent on their engraftment in the damaged tissues. Issues which currently
37 prevent the generation of such data include (i) the limitations associated with commonly used blood
38 biomarkers of organ injury, such as serum creatinine (SCr) for renal function (Molitoris et al., 2007,
39 Kellum et al., 2002, Ferguson et al., 2008, Chertow et al., 2005, Bonventre et al., 2010), and alanine
40 aminotransferase for liver function (Vanderlinde, 1986, Ozer et al., 2010, Marrer and Dieterle, 2010);
41 (ii) the technical limitations in repeated blood and urine sampling in small rodents; and (iii) the
42 difficulties associated with monitoring organ function in small animal species longitudinally. The
43 assessment of organ injury in small rodents classically involves measurements of serum or urine
44 biomarkers, or histopathological analysis. Since the latter is usually only undertaken at post-mortem,
45 it fails to allow the progression of injury to be monitored in the same animals longitudinally, requiring
46 animals to be culled at multiple time points, which is not in keeping with NC3Rs' principles and also
47 reduces the power of the statistical tests. Furthermore, current methods make it difficult to assess the
48 safety, efficacy and therapeutic mechanisms of cell-based RMTs in comorbid conditions where more
49 than one organ is affected, such as in the cardiorenal and hepatorenal syndromes (Mayfield et al.,
50 2016, Gonzalez-Calero et al., 2014, Erly et al., 2015).

51 In this current study we set out to develop a multimodal imaging strategy to monitor the function of
52 the liver, kidney and heart longitudinally in BALB/c mice in a single imaging session. We utilised
53 multispectral optoacoustic tomography (MSOT) to assess kidney and liver function, and traditional
54 ultrasound (US) measurements to assess cardiac function. MSOT is a technique which uses multiple
55 excitation wavelengths to resolve specific sources of absorption, whether they are endogenous or
56 exogenous (Taruttis et al., 2012). It relies on thermoelastic expansion which occurs when energy from
57 a laser capable of emitting light at a range of wavelengths is absorbed by molecules within the tissues.
58 This causes electrons to move to an excited state, generating heat and a resultant pressure wave
59 which is detected by an ultrasound detector. The specific absorption profile of endogenous or
60 exogenous molecules allows their identification within living animals in a minimally invasive manner
61 (Comenge et al., 2018). We have previously described methods of monitoring kidney or liver function

62 using MSOT in models of chronic kidney injury and acute liver injury (Brillant et al., 2017, Scarfe et al.,
63 2015).

64 Here, we utilised an acute model of adriamycin (ADR) - (doxorubicin-) induced multi-organ injury and
65 assessed organ function on days one and four post drug administration in order to determine the
66 extent of disease progression. ADR is an anthracycline antibiotic which is clinically administered as a
67 chemotherapeutic agent; however, its use is limited predominantly due to cardiotoxicity mediated
68 through a number of mechanisms. In rodents it can induce both chronic and acute kidney injury, as
69 well as cardiac and hepatic dysfunction (Roomi et al., 2014, Saad et al., 2001, Scarfe et al., 2015).

70 To test the effectiveness of this MSOT-US bi-modal imaging strategy for monitoring the ameliorative
71 potential of cell-based RMTs, after recording the extent of kidney, liver and cardiac dysfunction on
72 day one, mouse bone marrow-derived alternatively activated (M2) macrophages (BMDMs) were
73 administered intravenously into BALB/c mice and their ability to improve the function of the
74 aforementioned organs was monitored on day four and compared with a saline placebo. M2 BMDMs
75 were used in this study because previous reports have already demonstrated that they can ameliorate
76 kidney injury, liver injury and cardiac injury (Wang et al., 2008, Bai et al., 2017, Shiraishi et al., 2016).
77 However, as far as we are aware, M2 BMDMs have not previously been assessed for their ability to
78 ameliorate the injury of multiple organs simultaneously. We then set out to assess the relationship
79 between the biodistribution of the M2 BMDMs and their ability to ameliorate injury in each of the
80 three organs by utilising bioluminescent imaging of M2 BMDMs expressing luciferase.

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91 **Results**

92 Use of high frequency ultrasonography to investigate the effect of BMDMs on cardiac function in ADR-
93 dosed mice

94 High frequency ultrasonography was used to determine whether cardiac function was affected in
95 treated (ADR+BMDM), injured (ADR) and control mice (Fig 1) by measuring the following functional
96 parameters: fractional shortening (FS), ejection fraction (EF), stroke volume (SV) and cardiac output
97 (CO). The mean Δ FS (Fig 2A) and Δ EF (Fig 4B) was decreased in the ADR and ADR+BMDM groups when
98 compared to uninjured controls, but not significantly so. However, there were significant changes in
99 Δ CO (Fig 2C) and Δ SV (Fig 2D), with both parameters being significantly reduced in the ADR and
100 ADR+BMDM groups compared to healthy controls.

101 Use of MSOT to investigate the effect of BMDMs on renal function in ADR-dosed mice

102 MSOT was used to assess renal function in healthy mice, those which received ADR and those which
103 received ADR+BMDMs, on days 1 and 4 following ADR administration (Fig 1). Uninjured control mice
104 lost approximately 2.5% of their bodyweight over the 4 day time-course of the experiment whereas
105 animals that received ADR lost approximately 18% of their bodyweight, irrespective of whether they
106 were administered macrophages (Sup Fig 2, Table 1). Kidney function was assessed using MSOT, as
107 previously described (Scarfe et al, 2015), to measure the renal clearance of the near infrared dye,
108 IRDye 800 carboxylate (IRDye) which is exclusively filtered by the kidney (Sup Fig 1). Regions of interest
109 were drawn around the cortico-medullary region and the renal pelvis to generate intensity data for
110 quantitative measurements (Fig 3A). We observed that the typical clearance curves of IRDye on day 4
111 in both cortex and pelvis were changed in animals with ADR-induced kidney injury when compared to
112 those of healthy control mice (Fig. 3B, C). Specifically, instead of a single peak and subsequent decay
113 in the cortex, the curve peaked, dropped but then rose again and slowly decreased over time. In the
114 pelvis, a peak was observed at the same time point as in the cortex, followed by a second peak and
115 subsequent rise in the signal intensity. The clearance kinetics of IRDye in mice after ADR injury and
116 BMDM administration were also altered compared to the healthy controls (Fig 3D). To assess renal
117 function we utilised the ratio of the AUC for the cortex and pelvis (AUC C:P) rather than the Tmax
118 delay (difference in time at which signal was at maximum between cortex and pelvis) or cortex
119 exponential decay time used previously (Scarfe et al, 2015). For quantitative analysis of the changes
120 observed in each individual animal, IRDye clearance data were expressed as the difference in the AUC
121 Cortex: Pelvis between the measurements taken on days 1 and 4 (Δ AUC C:P). There was a significant
122 increase in the Δ AUC C:P between healthy and the ADR group, but not between healthy and the

123 ADR+BMDM group (Fig 3E). In addition, we assessed renal function using classical markers of blood
124 urea nitrogen (BUN) and serum creatinine (SCr) on day 4 (Fig 3F, G respectively). BUN was significantly
125 elevated in the ADR and ADR+BMDM groups compared to healthy controls, whereas there were no
126 significant changes in SCr between all three treatment groups. Furthermore, there was a significant
127 correlation between the AUC C:P and day 4 BUN measurements (Fig 3H, $P=0.013$, $R^2=0.39$).

128 Use of MSOT to investigate the effect of BMDMs on hepatic function in ADR-dosed mice

129 We assessed liver function by measuring the clearance of indocyanine green (ICG) which is exclusively
130 eliminated from blood by the liver using MSOT, as previously described (Brillant et al., 2017).
131 Representative MSOT snap shot images illustrate the change in ICG signal in the ischiatic vessel (Fig
132 4A). Plotting of the signal intensities over time showed that ICG clearance was delayed both in the
133 ADR+BMDM and the ADR groups compared to the saline group (Fig 4 B-D). To investigate the
134 ameliorative potential of BMDMs on liver function, we determined the change in AUC for ICG between
135 days 1 and 4 in each individual mouse (Δ ICG AUC) (Fig. 4E). There was a significant elevation in Δ ICG
136 AUC in the ADR group compared to healthy controls, but not between controls and ADR+BMDM
137 groups, nor between the ADR and ADR+BMDM groups (Fig. 4E). Alanine aminotransferase (ALT) was
138 significantly elevated in the sera of the ADR and ADR+BMDM groups compared to the controls on day
139 4 (Fig. 4F), and correlated significantly with ICG AUC ($P=0.0009$, $R^2=0.59$) (Fig. 4G). To investigate the
140 relationship between cardiac, kidney and liver injury, we plotted cardiac output together with the
141 MSOT data for kidney and liver function on a 3-D graph. This shows the relationship between CO,
142 kidney and liver function for each animal (Sup Fig 3).

143 BMDMs failed to ameliorate ADR-induced histological damage in the kidney and liver

144 The functional data from the MSOT analyses suggested that BMDMs had a tendency to improve renal
145 and hepatic function in ADR-dosed mice, but did not improve cardiac function. To investigate whether
146 the apparent improvement in renal and hepatic function was associated with an amelioration of tissue
147 damage, histological analysis of the liver and kidneys of mice was carried out at the study endpoint.
148 Kidney sections were assessed for the presence of intratubular protein casts and flattened tubular
149 epithelium, and liver sections for hepatocellular degeneration and necrosis. There was a significant
150 difference between healthy and ADR injured animals, but in contrast to the functional data,
151 administration of BMDMs failed to improve the extent of histological damage in the kidney or liver.
152 Histologically, the kidneys of control mice showed no evidence of injury (Fig 5A) whereas kidneys of
153 ADR mice had intratubular protein casts and flattening of tubular epithelial cells (Fig 5B, arrow)
154 regardless of BMDM administration. Likewise, the livers of control mice showed no signs of injury (Fig

155 5C) whereas ADR and ADR+BMDM mice showed evidence of hepatocellular degeneration (Fig 5(1))
156 and necrosis (Fig 5D(2)). Histological scoring in both the kidney and liver showed that control mice had
157 no evidence of histological damage whereas both the ADR and ADR+BMDM groups showed varying
158 degrees of injury (Fig 5E, F respectively).

159 Bioluminescence imaging shows that BMDMs accumulated in the kidneys and liver following ADR-
160 induced injury, but not in the heart

161 In order to investigate the effect of organ injury on BMDM distribution, mice were imaged on the
162 same day, or 3 days after administration of luciferase+ BMDMs, which corresponded to the 1st and 4th
163 day following saline or ADR administration. Bioluminescence imaging showed that on day 1, cells were
164 mostly in the lungs of both control and ADR animals. By day 4, BMDMs were no longer detectable in
165 the controls, but had a widespread distribution in the ADR group (Fig 6A, B). Given the poor spatial
166 resolution of bioluminescence imaging, it was not possible to determine which organs the BMDMs
167 had populated in the ADR group at day 4. Therefore, immediately after in vivo imaging on day 1, three
168 animals were immediately sacrificed to quantify the biodistribution of BMDMs in the major organs ex
169 vivo, with the remaining three mice being sacrificed on day 4. Similarly to the in vivo data, ex vivo
170 analysis of organs on day 1 showed no obvious difference between control and ADR mice, with most
171 BMDMs being in the lungs, and some detected in the spleen (Fig. 6C, D). By day 4, BMDMs could only
172 be detected in the lungs of control animals, but were present in the lungs, spleen, kidneys and liver of
173 ADR animals. BMDMs were not detected in the hearts of control or ADR animals (Fig. 6E, F).

174 We measured the total flux from the individual organs ex vivo to quantify the differences in organ
175 biodistribution between the treatment groups and time points (Fig. 7). The total flux from the heart,
176 lungs and spleen decreased between days 1 and 4 in both the control and ADR mice (Fig 7A, B, C). The
177 same trend was observed for the liver and kidney in the controls, with total flux decreasing between
178 days 1 and 4. On the other hand, in the ADR mice, total flux increased significantly in the liver and
179 kidneys between days 1 and 4 (Fig 7D, E).

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185 **Discussion**

186 In the current investigation, cardiac function was measured by ultrasonography alongside hepatic and
187 renal function by MSOT under the same anaesthesia session. This allowed us to determine the
188 functions of 3 separate organs utilising a multimodal imaging approach. The cardiac measurements
189 taken easily and quickly with the ultrasound software revealed that there were no significant changes
190 in fractional shortening or ejection fraction between days 1 and 4 in the ADR and ADR+BMDM groups
191 when compared to the healthy mice. However, significant decreases in cardiac output and stroke
192 volume between days 1 and 4 were detected when comparing the saline treated mice to those which
193 received adriamycin, regardless of the addition of the RMT. This suggests that a single dose of
194 adriamycin significantly reduces cardiac function between days 1 and 4 of this study; however, the
195 addition of BMDMs as a RMT show no beneficial effect on cardiac function.

196 We have previously used MSOT to monitor renal function in a mouse model of adriamycin-induced
197 chronic kidney disease by measuring the clearance kinetics of IRDye (Scarfe et al., 2015). The two
198 parameters used in this earlier study, which focussed on the chronic stage of renal injury, were the
199 T_{max} delay, and the exponential decay time of the IRDye in the renal cortex, which were measured at
200 week 5 following ADR dosing, when the nadir of acute renal injury had passed. However, in the current
201 study, which focussed on the acute phase of adriamycin-induced injury, these parameters were not
202 appropriate because many animals did not display an IRDye 'peak' in the pelvis, nor an exponential
203 decay in the renal cortex. Therefore, we considered that the most appropriate parameter in this case
204 would be the ratio of the area under the curve (AUC) of the cortex and pelvis kinetic curves (AUC C:P),
205 as this measurement reflects both impaired clearance through the cortex and delayed accumulation
206 in the pelvis, and could be measured in all animals. A single dose of adriamycin caused a significant
207 reduction in kidney function when compared to healthy mice over a 4 day period. Administration of
208 M2 BMDMs 1 day after adriamycin administration resulted in a non-significant reduction in kidney
209 function when compared to control mice. The AUC C:P showed a strong positive correlation with a
210 more traditional biomarker of kidney injury, BUN, which reinforces the utility of AUC C:P as a measure
211 of kidney function. There were, however, no differences between the mean BUN measurements in
212 mice which received adriamycin alone and those which received adriamycin and M2 BMDMs. SCr was
213 not significantly different between any of the groups, which highlights the lack of sensitivity of this
214 biomarker for indicating renal function in rodents. Histological analyses of the kidneys showed
215 evidence of intratubular protein casts and flattening of tubular epithelium in mice which received
216 adriamycin, irrespective of whether they were administered BMDMs or not. Therefore, although
217 MSOT showed that the M2 BMDMs appeared to cause a subtle improvement in renal function, there

218 was no corresponding improvement in histological damage or BUN levels. A study by Lu and colleagues
219 had previously demonstrated that M2 macrophages reduce inflammatory infiltrates in adriamycin-
220 induced nephropathy; however, macrophages were not administered until 5 days after adriamycin
221 administration and biomarker analyses not carried out until day 28 (Lu et al., 2013). It is possible in
222 this current study that analysis of kidney function at later time points than day 4 may have yielded
223 more significant improvements in function. Wang and colleagues studied the effect of M0, M1 and
224 M2 activated macrophages in a mouse model of chronic adriamycin nephropathy (Wang et al., 2007).
225 These authors had found that by 4 weeks, M0 macrophages had no effect on renal injury, while M1
226 macrophages promoted histological damage, and M2 macrophages significantly ameliorated tubular
227 and glomerular injury (Wang et al., 2007). By contrast, we failed to observe any ameliorative effects
228 of the M2 macrophages on tissue damage, but this may have been because our analysis was
229 performed at 4 days, rather than at 4 weeks. Consistent with our current study, Wang and colleagues
230 showed that M2 macrophages trafficked to inflamed kidneys. In addition, they provided evidence that
231 the exogenous M2 macrophages ameliorate injury by reducing the infiltration of resident
232 macrophages, thereby reducing inflammation.

233 In the current study the clearance of ICG from the blood of mice was used as a measure of liver
234 function. ICG is a fluorescent cyanine dye which is used clinically in a number of diagnostic procedures
235 including measurement of cardiac output, liver blood flow, ophthalmic angiography and hepatic
236 function (Caesar et al., 1961, Okochi et al., 2002, Iijima et al., 1997). It absorbs in the near infrared
237 region which makes it an ideal optoacoustic contrast agent. This, combined with the fact that ICG is
238 microsomal metabolised in the liver and cleared through the hepatobiliary route make it an ideal
239 agent for determination of liver function with MSOT. Using the ICG AUC we show here that there was
240 no change in liver function in healthy mice between days 1 and 4 whereas mice which received
241 adriamycin had a significantly decreased liver function in the same time window. Liver function was
242 also decreased between days 1 and 4 in mice which received adriamycin and M2 BMDMs but not
243 significantly so when compared to healthy mice. This suggests that a single high dose of adriamycin
244 reduces liver function while the addition of M2 BMDMs has a beneficial effect on the function of the
245 liver. The ICG AUC on day 4 of the study correlates strongly and significantly with serum ALT levels,
246 reinforcing the utility of ICG AUC as a functional liver parameter. Histological analyses showed no
247 evidence of liver injury in healthy mice while hepatocellular degeneration and necrosis was observed
248 in all mice which received adriamycin. Again, much like the kidney histopathology and biomarker
249 analysis, there were no differences in ALT or liver histology between mice which received adriamycin
250 alone and those which received adriamycin and the M2 BMDMs. Previous work by Thomas and
251 colleagues found that exogenous unpolarised BMDMs had a beneficial effect on mice with carbon

252 tetrachloride induced liver injury through the recruitment of MMP (matrix metalloproteinase)-
253 producing host cells into the liver (Thomas et al., 2011). This in turn increased host macrophage
254 recruitment and elevated IL-10 and MMP levels. The study also showed modest but significant
255 increases in serum albumin, suggesting liver regeneration (Thomas et al., 2011). The results we
256 present here also suggest a modest improvement in liver function as measured by MSOT, albeit
257 insignificantly. It should be noted that the effect of M2 BMDMs on adriamycin-induced liver injury has
258 not been previously investigated.

259 The aforementioned multimodal imaging strategy can monitor changes in the functions of the liver,
260 kidney and heart, and identify potential efficacy of M2 BMDMs as a RMT. To investigate the
261 relationship between biodistribution of the M2 BMDMs and any therapeutic effect, we administered
262 M2 BMDMs expressing firefly luciferase which allowed the luminescent imaging and quantification of
263 cells in the mice and organs (three on day 1 and three on day 4). At day 1, we observed no difference
264 in luminescence distribution between both groups of mice, with signals only present in the lungs and
265 spleen after IV cell administration. This pattern of biodistribution has been reported widely after IV
266 administration of cells (Sharkey et al., 2016). However, on day 4 of the study the biodistribution of the
267 cells in saline or adriamycin-dosed mice had changed dramatically. In the saline treated mice there
268 remained only a weak luminescent signal in the lungs of the mice, indicating the cells rapidly die after
269 IV administration. However, in mice which received adriamycin this was not the case; luminescence
270 was detected over the whole body of the mouse when imaged *in vivo*, and in the liver, kidneys, lungs
271 and spleen, but not the heart, when imaged *ex vivo*. While the luminescent signal intensity decreased
272 from day 1 to 4 in the lungs and spleen, it was still observable. On the other hand, the signal intensity
273 in the liver and kidneys was significantly elevated between days 1 and 4. Of note, the total flux in the
274 whole body images on day 4 in ADR treated mice appeared greater than on day 1; however M2
275 BMDMs do not have a great proliferative capacity so this was likely a result of the weight loss in the
276 ADR treated mice causing less attenuation of light.

277 Summary

278 This investigation demonstrates that changes in the function of the liver, kidney and heart can be
279 tracked over time in individual healthy animals and those that have received a single high dose of
280 adriamycin. We show that these changes in liver and kidney function correlate well with traditional
281 serum biomarkers of injury and show histological evidence of injury. We also show that the addition
282 of M2 BMDMs improves kidney and liver function over the study as measured by MSOT. However
283 neither biomarker nor histological analyses showed a reduction in the severity of injury. This may
284 suggest that subtle changes in organ function can be detected using MSOT imaging prior to changes

285 in organ histopathology and accumulation of serum biomarkers. Therefore, MSOT allows the
286 assessment of the efficacy of a potential RMT in mice without the need for repeated blood or urine
287 sampling. Secondly this study demonstrates an imaging technique to monitor the biodistribution of
288 M2 BMDMs in healthy animals and those with organ dysfunction. Unfortunately, to accurately assess
289 the intra-organ biodistribution of M2 BMDMs, it is required that animals are sacrificed prior to
290 imaging. We show that adriamycin affected the biodistribution of M2 BMDMs since mice with kidney
291 and liver dysfunction demonstrated an increase in longevity and migration of the therapeutic cells to
292 both organs, which incidentally also appeared to provided signs of efficacy in the functional study. No
293 signs of efficacy were observed in the heart, which showed no evidence that BMDMs migrated
294 towards it.

295 This current study describes and demonstrates an “imaging toolbox” to assess murine renal, hepatic
296 and cardiac function in a minimally invasive manner using both MSOT and ultrasound in a single
297 anaesthesia session. Comorbidities are common clinically so the ability to utilise an imaging toolbox
298 to investigate the potential of regenerative therapies in preclinical species is crucial. This toolbox
299 allows more accurate assessment of the efficacy of potential regenerative therapies than current
300 histological and biomarker analyses as it allows the extent of the recovery to be measured in individual
301 animals over time. Many regenerative therapies which show efficacy in preclinical species are not
302 effective clinically which may be a result of improper methods to assess their efficacy in individual
303 animals preclinically. This toolbox may allow more accurate assessment of efficacy and enable a more
304 robust determination of the risk: benefit ratio of a potential regenerative therapy prior to clinical
305 translation and therefore reduce the number of therapies that don’t show true efficacy that are tested
306 in human patients. This toolbox also improves understanding of the mechanism in which cell therapies
307 elicit efficacy through the study of their biodistribution. We can determine whether cells must reach
308 the target organ and engraft to show efficacy, which is important for determining the optimal
309 administration route.

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316 **Materials and Methods**

317 Animals

318 Mice were purchased from Charles River, UK, and were housed with *ad libitum* access to food and
319 water. All animal experiments were performed under a license granted under the Animals (Scientific
320 Procedures) Act 1986 and were approved by the University of Liverpool ethics committee.
321 Experiments are reported in line with the ARRIVE guidelines.

322 Primary macrophage isolation

323 Primary bone marrow derived macrophages (BMDMs) were prepared as previously described
324 (Sharkey et al., 2017). Male BALB/c mice were used to isolate BMDMs for the efficacy study whereas
325 for the biodistribution study, mice with a mixed background (L2G85 mice bred to wild type FVB mice)
326 expressing the CAG-luc-eGFP L2G85 transgene were used (FVB-Tg(CAG-luc,-GFP)L2G85Chco/J).
327 Briefly, femurs and tibias of mice (8-10 weeks) were harvested and muscle tissue removed from the
328 bones in a sterile fume hood. Bone marrow was flushed from the bones using a sterile syringe with
329 Dulbecco's Modified Eagle's Medium (DMEM): F12 cell culture medium (Gibco) supplemented with
330 10 % foetal bovine serum 2mM glutamine and 1 x penicillin/streptomycin (Invitrogen). The bone
331 marrow was suspended in the medium before being passed through a cell strainer (40 µm) and then
332 cultured in DMEM: F12 media containing 20 ng/ml murine recombinant macrophage colony
333 stimulating factor (MCSF-1). Bone marrow suspensions were cultured at 37 °C, 5 % CO₂ and medium
334 was replaced every other day. On day 7, macrophages were considered fully differentiated as
335 determined by the expression of both CD11b and F4/80 (Biolegend) by flow cytometry. Mature
336 BMDMs were then polarised towards an M2-like phenotype by the overnight addition of recombinant
337 murine interleukin (IL)-4 (20 ng/ml).

338 Induction of organ dysfunction

339 Male BALB/c mice (8 – 10 weeks) received either adriamycin (20 mg/kg, n=11) or saline (0.9 %, n=4)
340 intra-peritoneally (IP) on day 0. Adriamycin (doxorubicin hydrochloride, Tocris Bioscience) was
341 dissolved in warm saline (0.9 %) to make a stock solution (10 mg/ml) before administration. Mice were
342 weighed on a daily basis to monitor their wellbeing and mice which received adriamycin were provided
343 with a wet food diet.

344 Imaging protocol

345 Imaging was carried out on day 1 and 4 under the same imaging session and using the following
346 protocol: Mice were anaesthetised and fur was removed from the torso by shaving and epilating. Mice

347 were then imaged by ultrasound to generate functional cardiac parameters. The tail veins of mice
348 were then cannulated and mice moved to the MSOT system and received ICG (Carl Roth, Germany)
349 for liver functional measurements. The catheter was flushed with saline before administration of
350 IRDye800 carboxylate (LI-COR) for functional liver measurements. Mice were then allowed to recover
351 in a heat box before being returned to their home cage. A schematic showing how the study was
352 carried out can be found in Fig. 1. Results for MSOT and ultrasound analyses are expressed as the
353 change in each parameter between days 1 and 4 in the study. Detailed descriptions of each imaging
354 protocol are provided below.

355 Assessment of cardiac function

356 Cardiac function was assessed using the Prospect 2.0 ultrasound system (S-Sharp, Taiwan). Mice were
357 anaesthetised using isoflurane and oxygen and the mice were placed dorsally on a heated platform.
358 Mice were fixed in place during imaging using surgical tape. Ultrasound gel was applied to the chest
359 area of the mice and the ultrasound transducer positioned above the chest area. The following
360 parameters were measured: epicardial area and endocardial area in the long axis view, left ventricle
361 length, epicardial areas in the short axis view, M-mode images of both the long and short axis views
362 in order to measure heart rate, left ventricular interior diameter and wall thickness in both diastole
363 and systole. These parameters were used to calculate fractional shortening (FS), ejection fraction (EF),
364 stroke volume (SV) and cardiac output (CO).

365 Assessment of liver function

366 Liver function was assessed using the inVision 256-TF MSOT imaging system (iThera Medical, Munich).
367 Immediately after assessment of cardiac function the mice were moved to the MSOT imaging system.
368 Prior to being placed into the system the tail vein of the mice was cannulated to allow injection of the
369 optical imaging contrast agents during photoacoustic imaging. Mice were placed in the system and
370 allowed to acclimatise for 15 minutes prior to recording data. Imaging focussed on the ischiatic vessels
371 close to the hips of the mice for detection of indocyanine green (ICG) and its subsequent clearance.
372 The following parameters were used: an acquisition rate of 10 frames per second (consecutive frames
373 averaged to minimise effects of respiration movement), with wavelengths of 700, 730, 760, 800, 850
374 and 900 nm being recorded. Data were recorded for 3 minutes prior to intravenous (IV) injection of
375 ICG (40 nmol, 100 μ l) over a 10 s period. Data were reconstructed using a model linear algorithm (View
376 MSOT software) and multispectral processing using linear regression for ICG, deoxy- and oxy-
377 haemoglobin spectra to resolve the signal for the ICG dye. Regions of interest drawn around the
378 ischiatic vessels of each mouse were used to quantify the ICG dye signal (as mean pixel intensity) in

379 the vessels of the mice. These data were used to calculate the area under the clearance curve (AUC).
380 Data expressed as the change in ICG AUC in each individual mouse between days 1 and 4 (Δ ICG AUC).

381 Assessment of kidney function

382 Kidney function was assessed utilising a similar method as the assessment of liver function. After liver
383 function assessment, the catheter was flushed with a small amount of saline. Data were recorded
384 using the following parameters: wavelengths of 775 and 850 nm and an acquisition rate of 10 frames
385 per second (consecutive frames averaged). Imaging focussed on the centre of the right kidney of the
386 mouse where the renal pelvis was visible. Data was recorded for 3 minutes prior to the injection
387 through the tail vein catheter of IRDye 800 carboxylate (20 nmol, 100 μ l) over a period of 10 s. Data
388 was reconstructed using a model linear algorithm and a difference protocol (775 nm – 850 nm) to
389 resolve the signal for the IRDye 800 carboxylate. Regions of interest were drawn around the renal
390 cortex and the renal papilla/pelvis region of the right kidney in each mouse to quantify the IRDye signal
391 in the kidney. The mean pixel intensity data were used to calculate the AUC of both the renal cortex
392 and papilla/pelvis. Data were expressed as the change in the ratio between the AUC of the cortex and
393 the AUC of the pelvis regions between days 1 and 4 (Δ AUC C:P).

394 Therapeutic cell administration

395 M2-like primary BMDMs were administered to mice which received adriamycin (n=6) on day 1
396 immediately after cardiac, hepatic and renal imaging. BMDMs were harvested from low adherence
397 flasks (Corning) after maturation and polarisation by gentle agitation and scraping. Cells were then
398 counted and suspended to a concentration of 10^7 cells/100 μ l saline. After mice were removed from
399 the MSOT imaging system, 100 μ l of the cell suspension was administered via the tail vein cannula and
400 mice were allowed to recover in a heat box before being returned to their home cage. Mice which did
401 not receive BMDMs received 100 μ l saline via the tail vein catheter.

402 Quantification of serum biomarkers

403 On day 4 mice were culled using an increasing concentration of CO₂ and exsanguinated by cardiac
404 puncture. Blood was allowed to clot at room temperature before centrifugation to isolate the serum.

405 Blood urea nitrogen (BUN, QuantiChrom Urea Assay Kit, BioAssay Systems), serum creatinine (SCr,
406 Serum Creatinine detection kit, ARBOR ASSAYS) and alanine aminotransferase activity (ALT, Thermo
407 Fisher) were quantified according to manufacturer's instructions in a 96 well plate and were read using
408 a FLUOstar Omega microplate reader (BMG LABTECH).

409

410 Histopathological analysis

411 Kidney and liver tissues were fixed in 4 % paraformaldehyde (4 °C) for 24 hours before being washed
412 in PBS, dehydrated with increasing concentrations of ethanol and subsequently embedded in paraffin.
413 The kidneys were sectioned in order to obtain two symmetrical halves, to include the cortex, and
414 medulla extending to the renal pelvis. For the liver, the large lobe was collected for analysis. Tissue
415 sections were cut (5 µm) and were stained with haematoxylin and eosin (HE) and Periodic Acid Schiff
416 (PAS) by standard methods. Kidney injury was scored 0-5 on 10 consecutive 200x microscopic fields in
417 the outer stripe of the outer medulla and cortex on PAS stained slides adapting the method described
418 from Wang and colleagues (Wang et al., 2005) . For liver, histological sections were assessed semi
419 quantitatively for degeneration and necrosis following a semi quantitative scale representative for the
420 section area involved (0=0%; 1=1-25%; 2=26-50%; 3=51-75%; 4=76-100%). Veterinary pathologist (LR) was
421 blinded in regard to the experimental groups.

422 Determining cellular biodistribution

423 To determine cellular biodistribution by bioluminescence imaging, male BALB/c mice (8 – 10 weeks)
424 were used. The same adriamycin and macrophage dosing schedule was used as in the previous study:
425 Mice received either 20 mg/kg adriamycin IP (n=6) or saline IP (n=6). 24 hours later all mice received
426 IV injections of 10⁷ PMDMs isolated from mice expressing the CAG-luc-eGFP L2G85 transgene. All mice
427 received luciferin (1.5 mg/kg, IP) before being imaged using an IVIS Spectrum *in Vivo* Imaging System
428 (Perkin Elmer). Mice were imaged in both dorsal and ventral positions using an automatic exposure
429 time before being sacrificed. Organs were then dissected and imaged using the same protocol. The
430 remaining mice were returned to their home cages until day 4 post adriamycin administration (the
431 study end point) when they were imaged as previously described.

432 Statistical analysis

433 Statistical analyses were carried out using Origin software. One-way ANOVA analysis was used for
434 comparison of two groups and one-way ANOVA followed by Tukey analysis was used to compare
435 multiple groups. Results were determined to be significant when $P < 0.05$. To assess whether
436 correlations between results were significant Pearson's correlation coefficient was calculated.

437

438 **Acknowledgements**

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538 **Figures**

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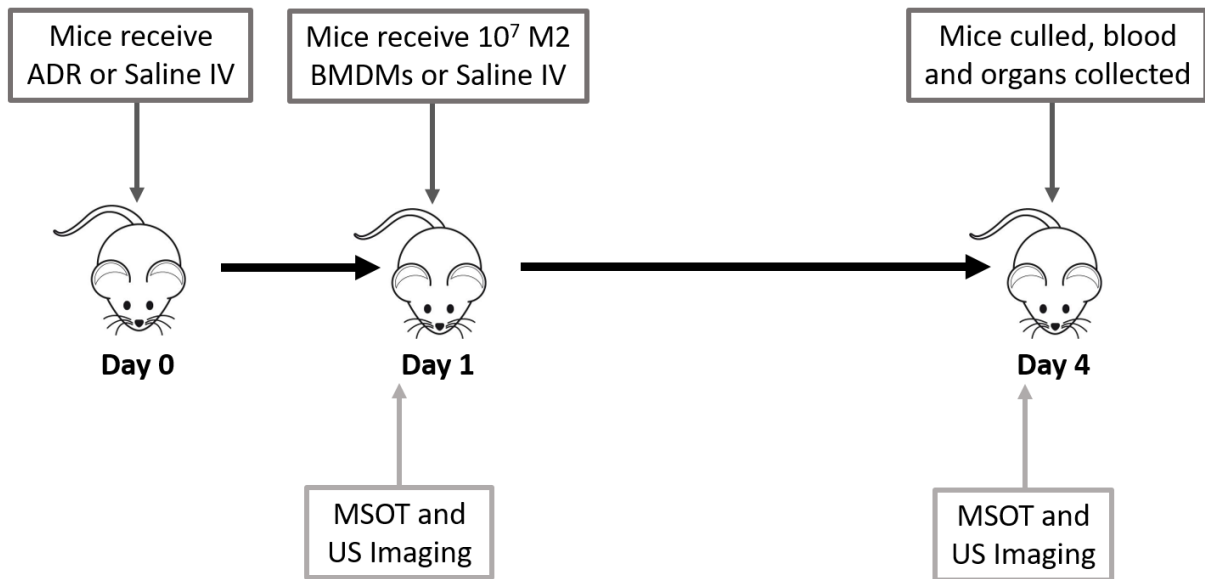
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546 **Figure 1:-** Schematic showing the experimental protocol.

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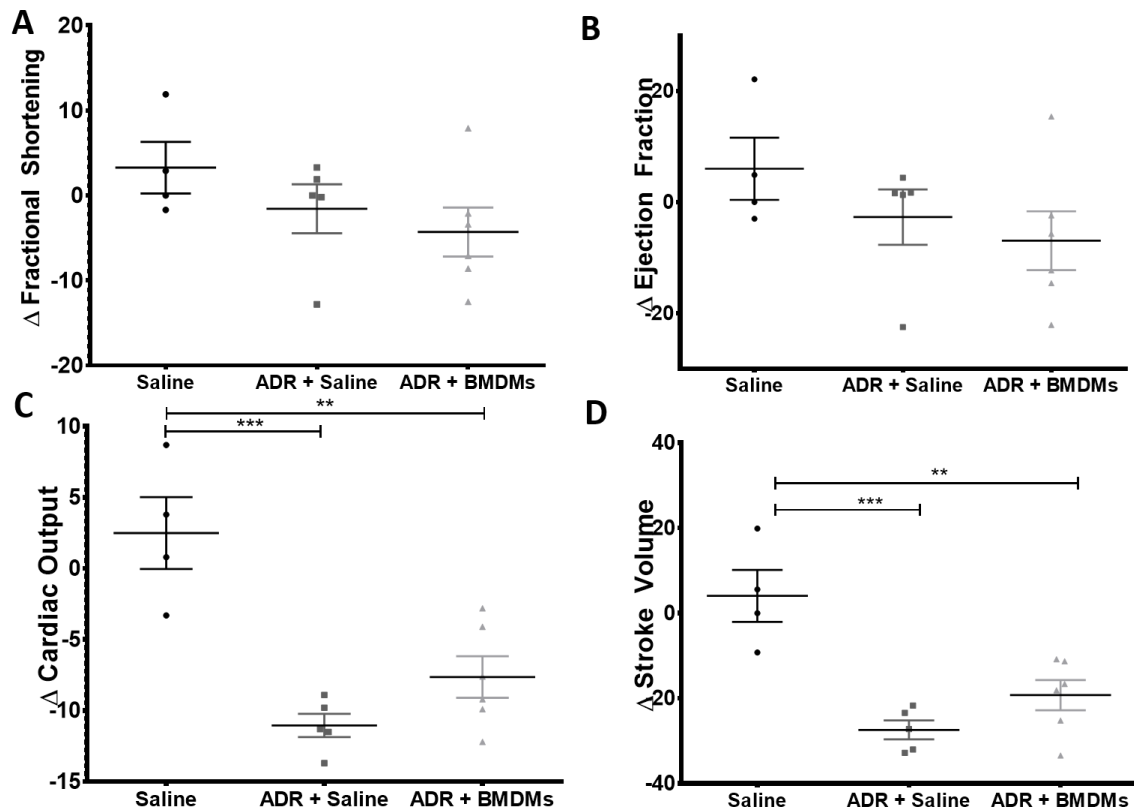
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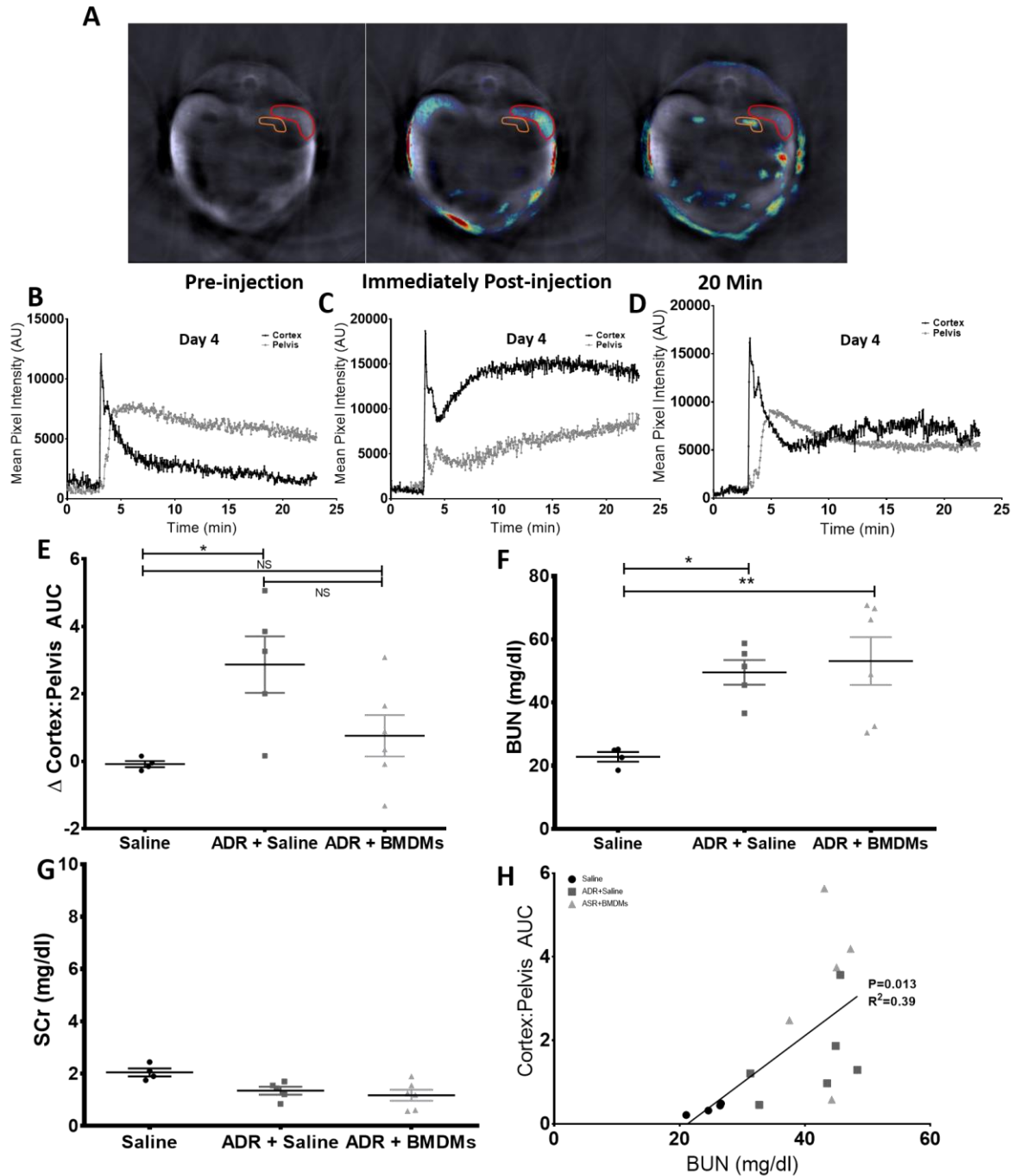
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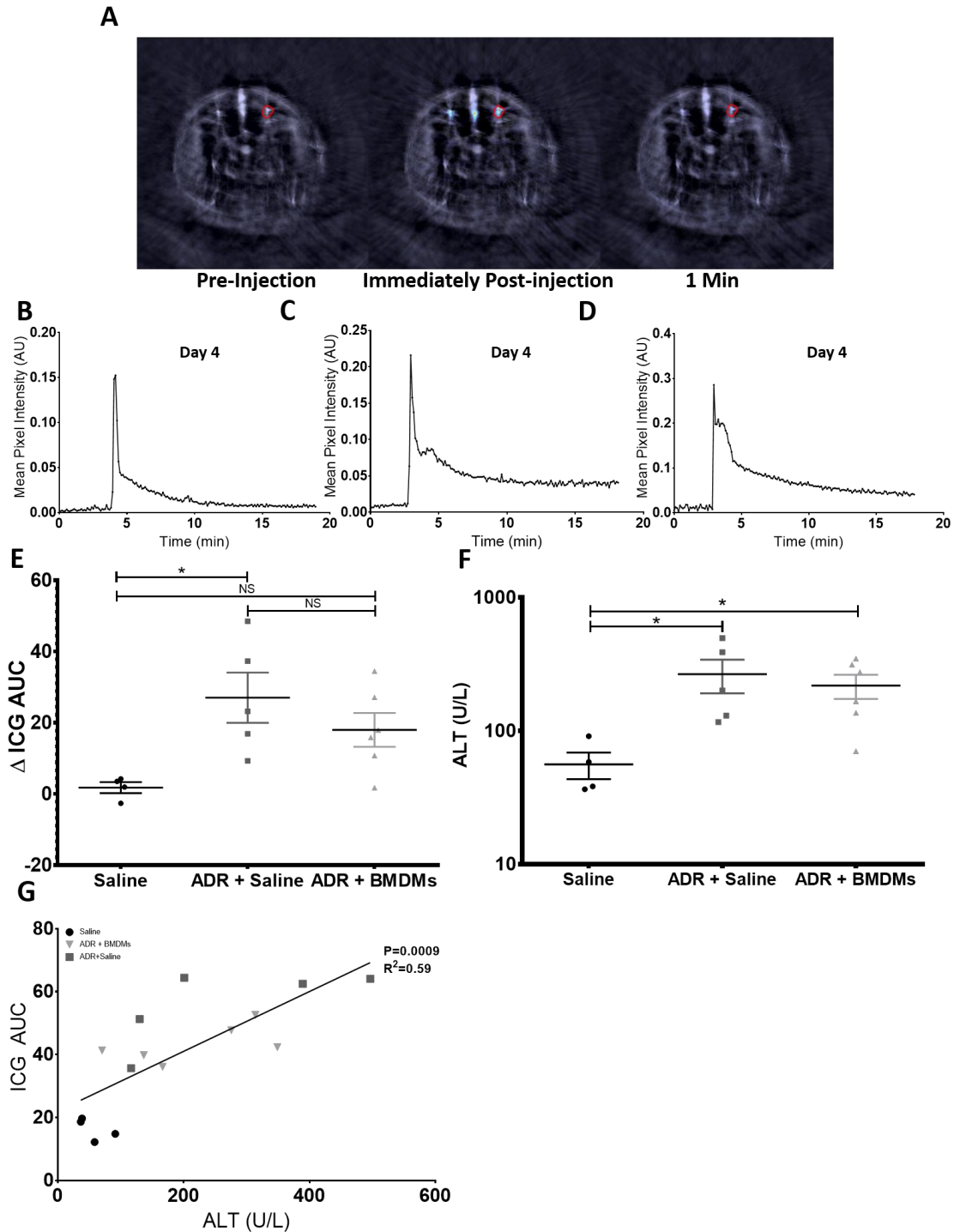
563 **Figure 2:-** Cardiac parameters as measured by ultrasound. Fractional shortening (A), ejection fraction
564 (B), cardiac output (C) and stroke volume (D) were quantified. Each parameter is represented as the
565 change in the parameter between days 1 and 4 in each mouse. Each data point represents an
566 individual mouse. ** P<0.01, *** P<0.001.



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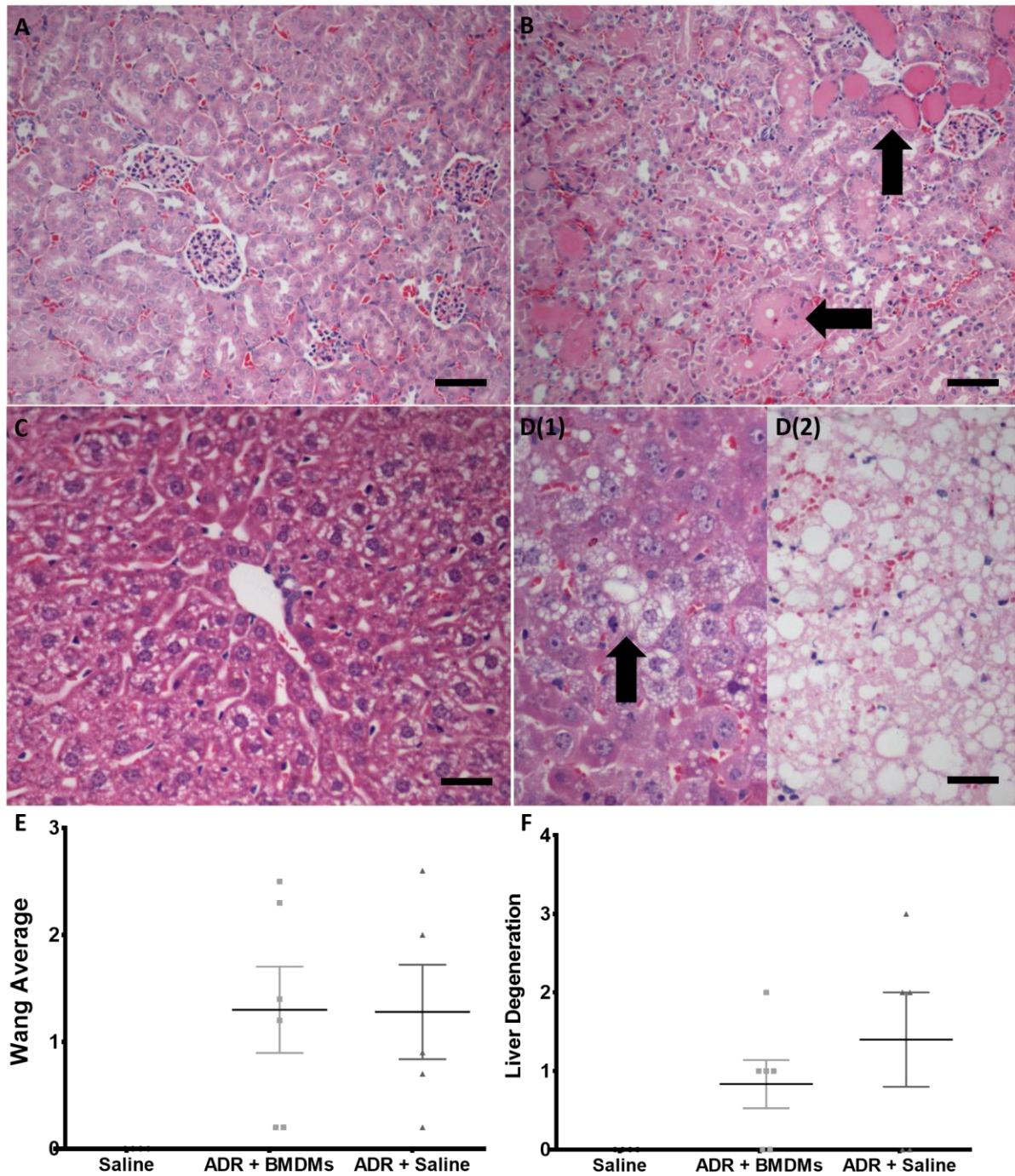
568 **Figure 3:-** Representative images showing the a typical cross section of a mouse as obtained by the
 569 MSOT prior to, immediately post and 20 minutes post IRDye administration, Cortex and medullary
 570 regions of interest are shown (A). Clearance kinetics on day 4 of IRDye 800 carboxylate from both the
 571 kidney cortex and pelvis regions of interest in a typical healthy (B), ADR treated (C) and ADR+BMDM
 572 treated mouse (D). The change in the mean cortex:pelvis AUC between days 1 and 4 in all mice is
 573 shown in (E) (Mean Δ AUC C:P -0.085, 0.755 and 2.866). Serum BUN (F) (mean 24.7, 43.4 and 41.1
 574 mg/dl) and SCr (G) levels were quantified on day 4 in each mouse. The correlation between the
 575 cortex:pelvis AUC and blood urea nitrogen on day four is shown in (H). Each data point represents an
 576 individual mouse. * P<0.05, ** P<0.01

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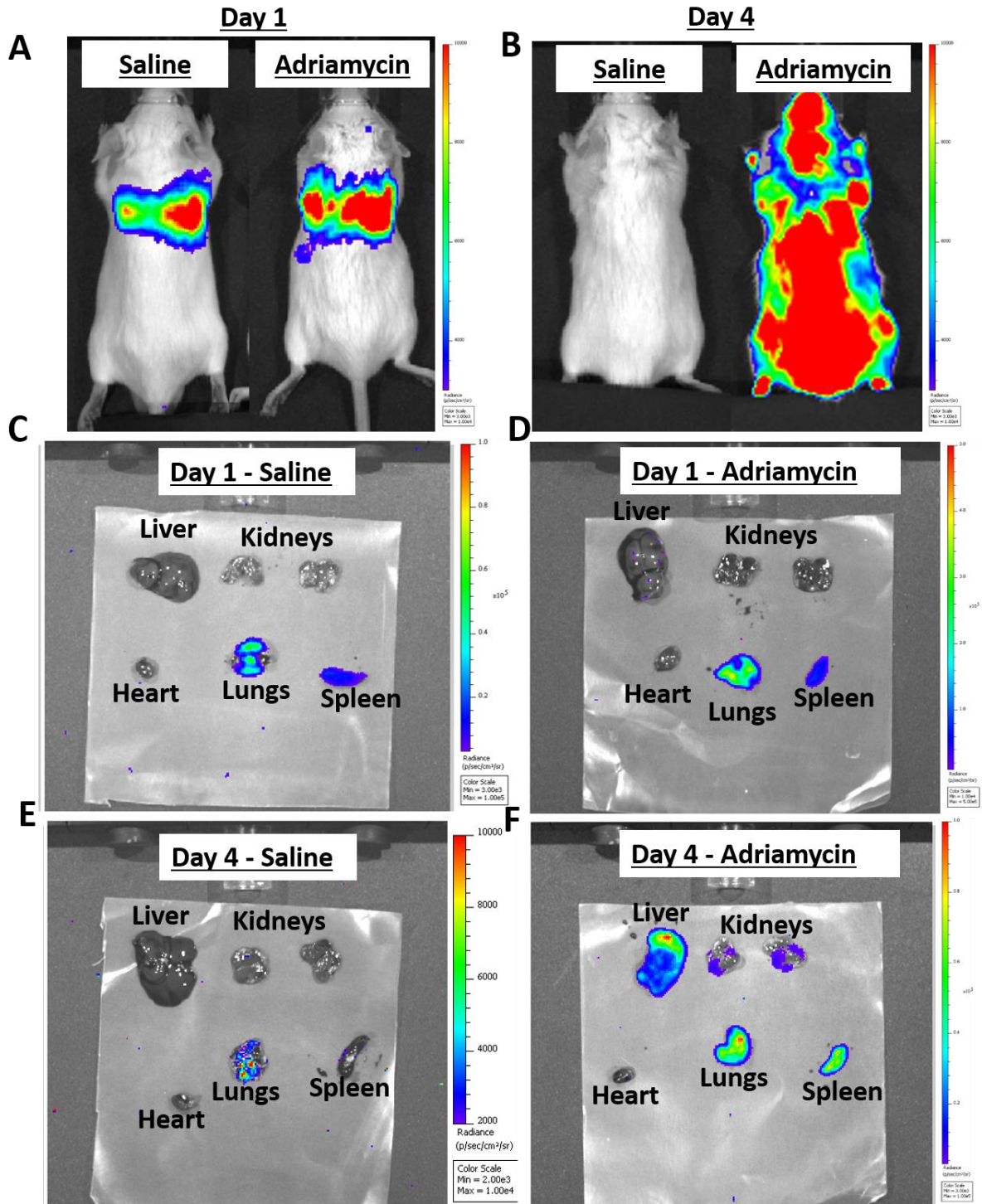
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579 **Figure 4:-** Representative images showing the a typical cross section of a mouse as obtained by the
580 MSOT both prior to, immediately post and 1 minute post ICG administration (A). Clearance kinetics on
581 day 4 of ICG from a typical healthy mouse (B), an ADR treated mouse (C) and an ADR+BMDM mouse
582 (D) from a single ischiatic vessel's region of interest. Clearance kinetics on day 4 of ICG from a mouse
583 which had received adriamycin from a single ischiatic vessel (C). The change in the mean ICG AUC
584 between days 1 and 4 in all mice is shown in (E) (Mean Δ AUC ICG 1.8, Δ AUC ICG 18). Serum ALT was
585 quantified in all mice on day 4 (F). The correlation between the ICG AUC and alanine aminotransferase
586 on day four is shown in (G) (mean 56.1, 218.6 and 266.6 U/L). Each data point represents an individual
587 mouse. * $P<0.05$.



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589 **Figure 5:-** Histological analyses from both the kidney and liver. Histological analyses show sections
590 from typical sections of a kidney from a healthy mouse (A), the kidney of a mouse which had received
591 adriamycin (B), the liver of a healthy mouse (C) and the liver of a mouse which had received adriamycin
592 (D1, 2). All organs were collected on day 4 of the study and were stained with haematoxylin and eosin.
593 (A) and (B); scale bar = 100 μ m. (C) and (D); scale bar = 50 μ m. No evidence of injury are observed in
594 (A) or (C). (B) shows evidence of intratubular protein casts and flattening of the tubular epithelium
595 (arrow). (D1) shows evidence of hepatocellular degeneration (arrow) and (D2) shows evidence of
596 necrosis with evidence of pale eosinophilic substance. Histological scoring for the kidney and liver are
597 shown (E, F respectively). Each data point represents an individual animal.

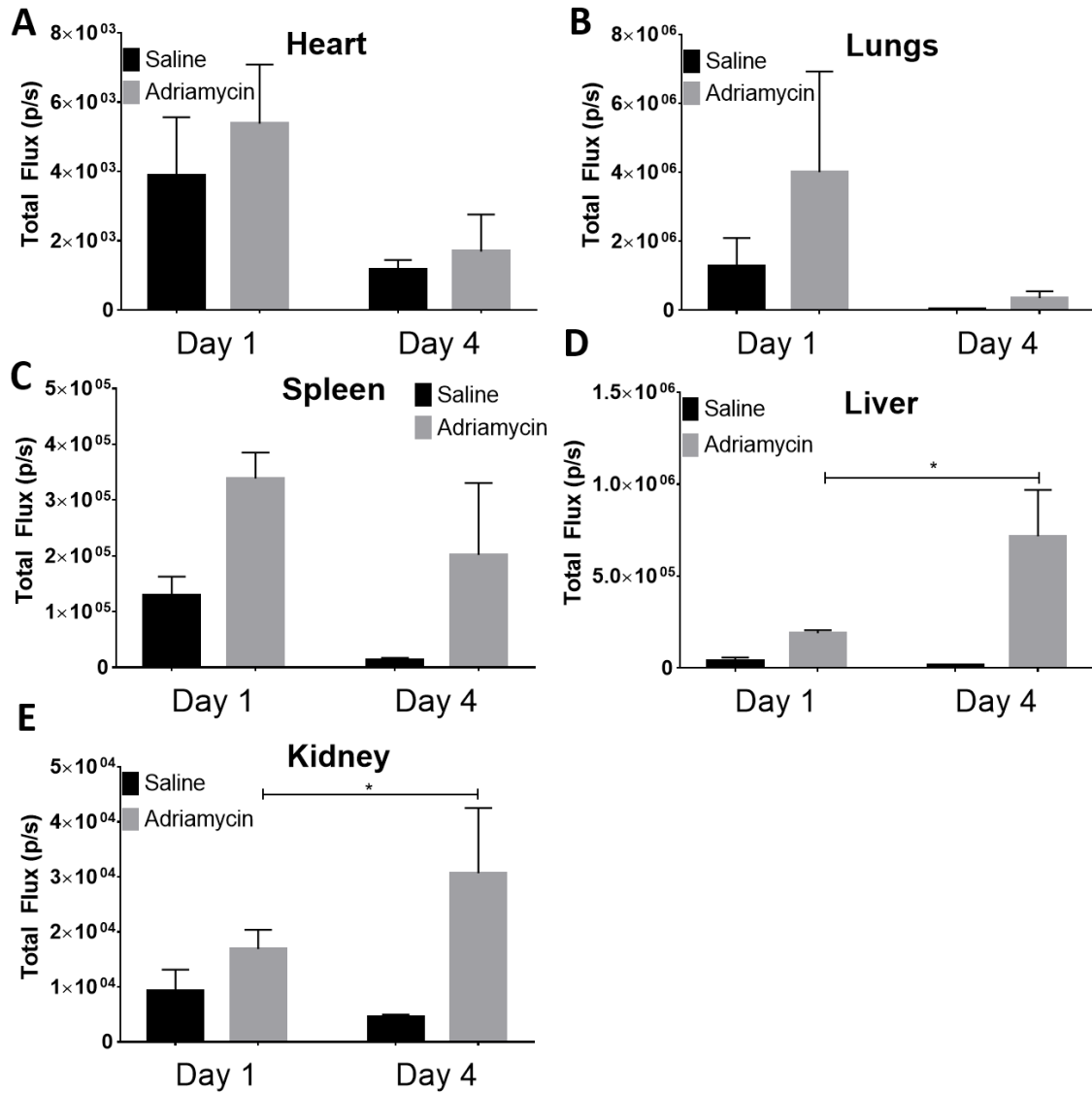


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599 **Figure 6:-** All mice received 10^7 primary bone marrow derived macrophages which expressed
600 luciferase via tail vein administration. Whole body images of typical mice treated with either saline or
601 Adriamycin on both days 1 (A) and 4 (B). Ex vivo bioluminescence images from typical saline (C, E) and
602 Adriamycin (D, F) treated mice on both days 1 (C, D) and 4 (E, F). Individual scales are shown on the
603 right of each image. Each image shows the liver, kidneys, heart, lungs and spleen from an individual
604 mouse. Scales for all ex vivo images are identical, as are scales for all whole body images.

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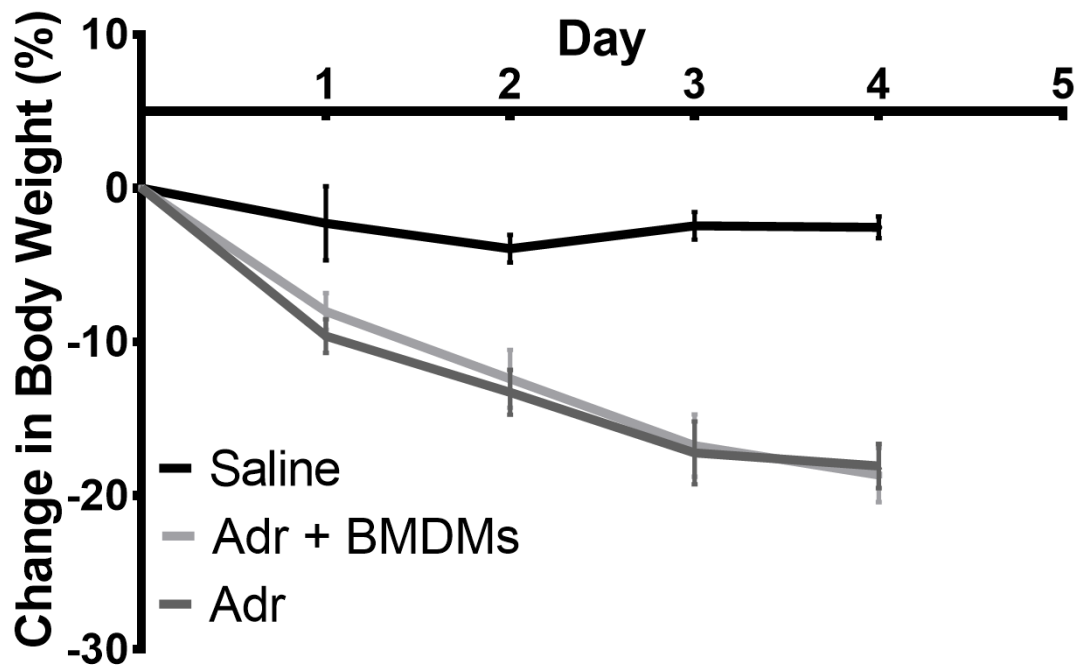
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Figure 7:- Quantified ex vivo bioluminescent results from organs of mice that received either saline on Adriamycin on both days 1 and 4. Data is shown for the heart (A), the lungs (B), the spleen (C), the liver (D) and the mean of both kidneys (E). Each bar represents the mean of 3 individual animals. * P<0.05

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629 **Supplementary figure 1:-** Change in body weight in mice which received saline, ADR+BMDMs and
630 ADR. Each data point represents the mean of mice within the group

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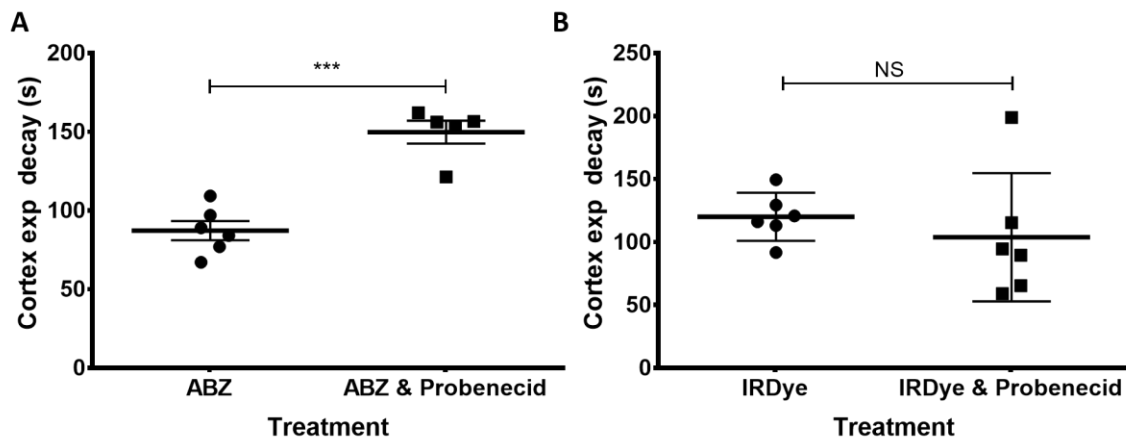
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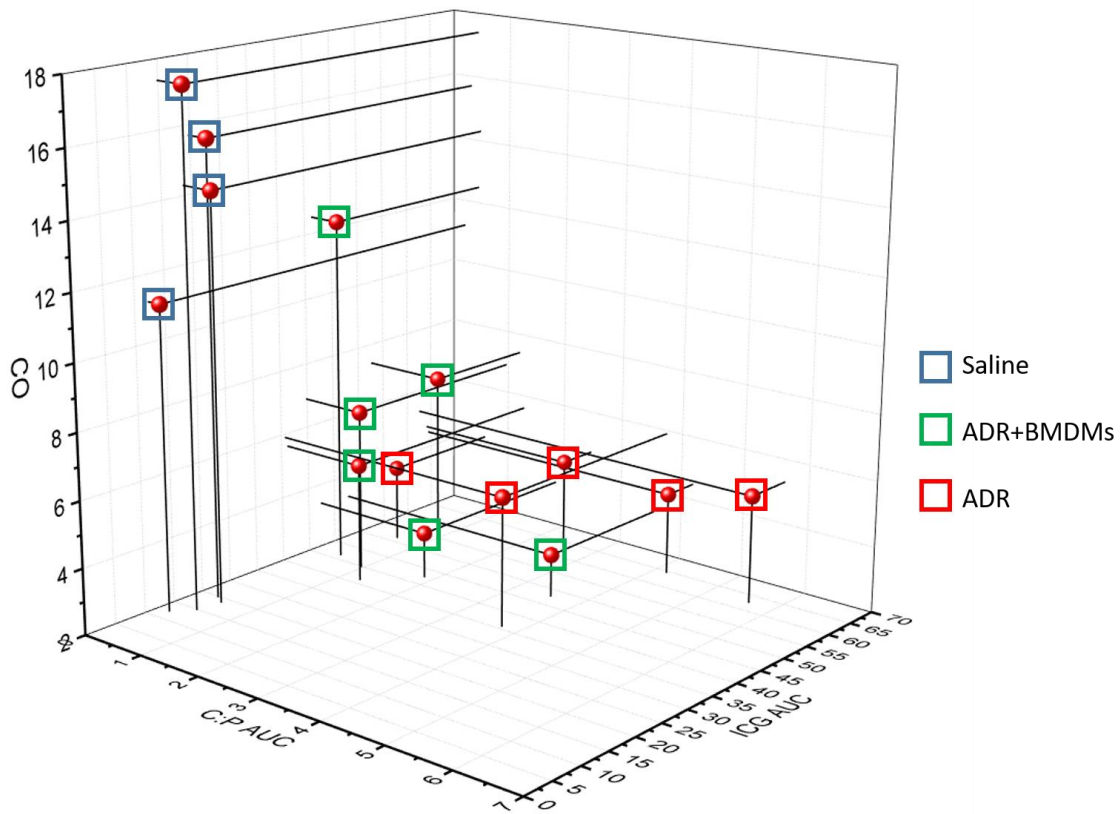
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Supplementary figure 2:- The effect of 50 mg/kg Probenecid on the clearance of two near infrared dyes through the cortex of the kidneys of mice as measured by MSOT. Results are expressed as the exponential decay time (s) of each dye from the cortex of the mice. Each data point represents an individual animal. NS = non-significant, *** P=0.001.

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666 **Supplementary Figure 3:-** 3D dot plot showing the relationship between the change in cardiac output,
667 C:P AUC and the ICG AUC between days 1 and 4 in saline treated mice (blue boxes), ADR treated mice
668 (red boxes and mice treated with ADR and BMDMs (green boxes). Each dot represents an individual
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Treatment	Animal	Day 1 Cortex: Pelvis AUC	Day 4 Cortex: Pelvis AUC	SCr (mg/dl)	BUN (mg/dl)	Day 1 ICG AUC	Day 4 ICG AUC	ALT (U/L)	Fractional Shortening Day 1	Fractional Shortening Day 4	Ejection Fraction Day 1	Ejection Fraction Day 4	Stroke Volume Day 1	Stroke Volume Day 4	Cardiac Output Day 1	Cardiac Output Day 4	Change in body weight (%) Day 1	Change in Body Weight (%) Day 4
Saline Only	1	0.3	0.4	2.1	26.5	17.4	14.8	91.2	11.1	23.0	24.1	46.2	24.1	44.0	8.7	17.4	-9.51	-3.87
	2	0.6	0.5	1.7	26.6	14.4	18.6	36.5	19.3	19.3	39.9	39.9	34.9	34.9	10.5	14.3	0.00	-3.63
	3	0.4	0.3	2.4	24.6	16.1	19.7	38.3	20.9	23.8	42.7	47.6	38.5	44.1	14.9	15.7	0.39	-1.54
	4	0.5	0.2	1.9	21.1	10.2	12.2	58.4	16.9	15.2	35.3	32.3	38.0	28.8	14.5	11.2	0.00	-1.10
ADR + BMDMs	5	0.2	1.9	1.9	44.9	24.4	42.3	348.8	17.3	25.2	36.3	51.7	31.7	15.1	11.0	3.4	-8.70	-17.00
	6	0.3	1.2	1.2	31.3	18.1	52.6	313.9	24.6	17.5	49.2	36.9	35.4	24.6	11.5	7.4	-5.70	-13.16
	7	0.5	3.6	0.6	45.6	20.6	47.7	275.6	24.3	11.8	48.4	26.3	46.2	12.8	15.5	3.3	-10.85	-22.09
	8	0.5	0.5	1.5	32.7	25.4	41.3	70.3	21.5	18.1	43.6	37.9	42.6	31.3	15.3	12.5	-6.61	-15.56
	9	2.6	1.3	0.6	48.4	34.4	36.1	166.5	24.3	15.7	48.5	33.9	42.8	17.6	15.5	5.6	-11.81	-24.89
	10	0.6	1.0	1.2	43.5	29.0	39.8	136.6	28.2	26.1	55.0	52.6	40.4	22.3	16.1	6.9	-4.37	-19.21
ADR	11	0.3	4.2	1.7	47.3	27.1	64.4	200.9	21.5	23.4	43.8	48.2	41.4	18.0	14.3	4.5	-7.05	-14.54
	12	0.5	2.5	1.2	37.5	15.6	64.1	496.6	23.4	26.7	52.1	53.7	40.0	18.3	13.6	4.7	-10.33	-16.53
	13	0.5	3.7	1.5	45.0	26.3	35.7	116.5	22.0	21.8	44.0	45.3	47.7	20.5	17.4	5.9	-13.18	-21.32
	14	0.6	5.6	0.8	43.1	45.6	62.5	389.2	22.6	22.6	45.4	47.1	47.5	14.7	19.0	5.3	-7.50	-16.25
	15	0.4	0.6	1.4	44.3	28.1	51.3	130.0	24.8	12.0	49.3	26.8	44.8	12.8	15.6	4.3	-10.00	-21.67

682

683 **Supplementary Table 1:-** Summary of all imaging and biomarker analysis for individual mice