

1 **Suppressive waves disambiguate the representation of long-range apparent**  
2 **motion in awake monkey V1.**

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## 24 **Abstract**

25 The “apparent motion” illusion is evoked when stationary stimuli are successively flashed in spatially  
26 separated positions. It depends on the precise spatial and temporal separations of the stimuli. For large  
27 spatiotemporal separation, the long-range apparent motion (lrAM), it remains unclear how the visual  
28 system computes unambiguous motion signals. Here we investigated whether intracortical interactions  
29 within retinotopic maps could shape a global motion representation at the level of V1 population in  
30 response to a lrAM. In fixating monkeys, voltage-sensitive dye imaging revealed the emergence of a  
31 spatio-temporal representation of the motion trajectory at the scale of V1 population activity, shaped by  
32 systematic backward suppressive waves. We show that these waves are the expected emergent  
33 property of a recurrent gain control fed by the horizontal intra-cortical network. Such non-linearities  
34 explain away ambiguous correspondence problems of the stimulus along the motion path, preformatting  
35 V1 population response for an optimal read-out by downstream areas.

36

## 37 **Introduction**

38 When two stationary stimuli are successively flashed in spatially separated positions, it generates the so-  
39 called “apparent motion” illusion (Wertheimer 1912). This illusion, well characterized in psychophysics  
40 (Burr and Thompson 2011), depends on the spatio-temporal characteristics of the stimulus, being called  
41 “short-range” vs “long-range” apparent motion (lrAM) for spatial separation below or above  $0.25^\circ$  and  
42 temporal separation below or above 80 ms respectively (Braddick 1980). In psychophysics, intrinsic  
43 differences were reported between these two types of apparent motion, however, there is some debate  
44 whether it is underlined by same or different process (Cavanagh and Mather 1989). In physiology, while  
45 we have a clear idea on the neuronal processing generating direction-selective neuronal response to  
46 short-range apparent motion stimuli (Mikami, Newsome, and Wurtz 1986b), we still have a poor

47 understanding of how the visual system process IrAM. This is probably because the spatial separation  
48 between individual strokes of the IrAM extend beyond the typical extent of receptive fields in the early  
49 visual system, at least in primates. In the case of the IrAM, psychophysicists have long highlighted the  
50 necessity to have a process, such as the “reviewing process” (Kahneman, Treisman, and Gibbs 1992),  
51 that will link the transient apparitions of stimuli in different spatial and temporal positions in order to  
52 generate a coherent motion percept of a single object, hereby solving the problem of “phenomenal  
53 identity” (Ternus 1926) or “correspondence” (Ullman 1978). Downstream areas with large receptive  
54 fields are a natural expected integration unit for such extended spatiotemporal input. Indeed, it has  
55 been recently shown in human that the feedback from MT to V1 plays an important role in the  
56 processing of IrAM (Wibral et al. 2009; Muckli et al. 2002; Vetter, Grosbras, and Muckli 2015), as well as  
57 evidences of downstream activation along the ventral stream (Zhuo et al. 2003). However, it is still  
58 unclear whether and how the “reviewing” process, needed to keep track of the object identity along the  
59 motion trajectory, can be achieved within these receptive fields.

60 As suggested from fMRI experiments in human, the neuronal processing within V1 could  
61 participate in formatting the representation of IrAM (Muckli et al. 2005). The extended precise  
62 retinotopic map in V1 makes it indeed an ideal platform for representing and disambiguating, at the  
63 level of the neuronal population, the trajectory of the apparent motion illusion, a representation that  
64 could be read-out by downstream areas (Mumford 1991; Lee et al. 1998). In particular, V1 has the  
65 highest resolution (Lee et al. 1998) to achieve the interactions in space and time needed to link the  
66 individual strokes of the apparent motion (Lee et al. 1998; Adelson and Bergen 1985). In such context,  
67 intra-cortical and inter-cortical connectivity would be the natural substrate to underlie the necessary  
68 spatio-temporal interactions (Deco and Roland 2010; Muller et al. 2018). Importantly, these two  
69 networks have intrinsically different spatio-temporal properties, the inter-cortical network operating  
70 over very large extent but with poor spatial and temporal resolution (Angelucci et al. 2002; Stetter

71 2002), and the intra-cortical network has a more limited extent but with high spatial and temporal  
72 resolution (Muller et al. 2014; Bringuier et al. 1999; Bullier 2001). Furthermore, they constitute the vast  
73 majority of synaptic contacts in the cortex, the feedback accounting for less than 20% and the intra-  
74 cortical connectivity contributing to 80% of the number of neuronal contacts, while the feedforward less  
75 than 1% (Markov et al. 2011). Such connectivity seems therefore like a good candidate to link transient  
76 spatio-temporal events (Muller et al. 2018). It was indeed shown, in the anesthetized cat, to shape  
77 visual information for a dynamic representations of sequences of static stimuli (Jancke et al. 2004;  
78 Gerard-Mercier et al. 2016) through non-linear gain controls of the feedforward input (Reynaud,  
79 Masson, and Chavane 2012). However, it is still unclear whether and how the cortico-cortical  
80 interactions could participate to shape the representation of IrAM within V1 retinotopic map in the  
81 awake monkey.

82         To answer this question, we used optical imaging of voltage-sensitive dyes (VSDI) in the awake  
83 fixating monkey, to measure how V1 neuronal population integrates a two-stroke IrAM that  
84 overreached individual neuronal receptive field size. In response to a single stroke, activity in V1  
85 propagates in space and time, as already documented (A. Grinvald et al. 1994; Slovlin et al. 2002; Sato,  
86 Nauhaus, and Carandini 2012; Bringuier et al. 1999; Muller et al. 2014), with spatial and temporal  
87 constants that cover about 3 mm and 80 ms. In response to the IrAM of various spatio-temporal  
88 separations, we observed that the cortical response systematically deviates from the linear prediction  
89 and generates a wave of suppression that is initiated right at the second stimulus onset and propagates  
90 to suppress the residual response to the first stimulus. A computational model was developed to  
91 understand the potential origin of such suppressive waves. The model shows that two ingredients are  
92 necessary to explain suppressive waves: the higher gain of inhibitory cells, and the shunting effect of the  
93 associated synaptic conductances. Using a spatio-temporal decoding approach, we demonstrate that  
94 such suppression waves explain away ambiguous representation of stimulus position along the apparent

95 motion trajectory. These waves thus preformat V1 population response for an unambiguous  
96 representation of the IrAM. Using an opponent motion energy approach, we demonstrate that this  
97 results in an optimal encoding of the stimulus velocity that could be easily read-out by downstream  
98 areas.

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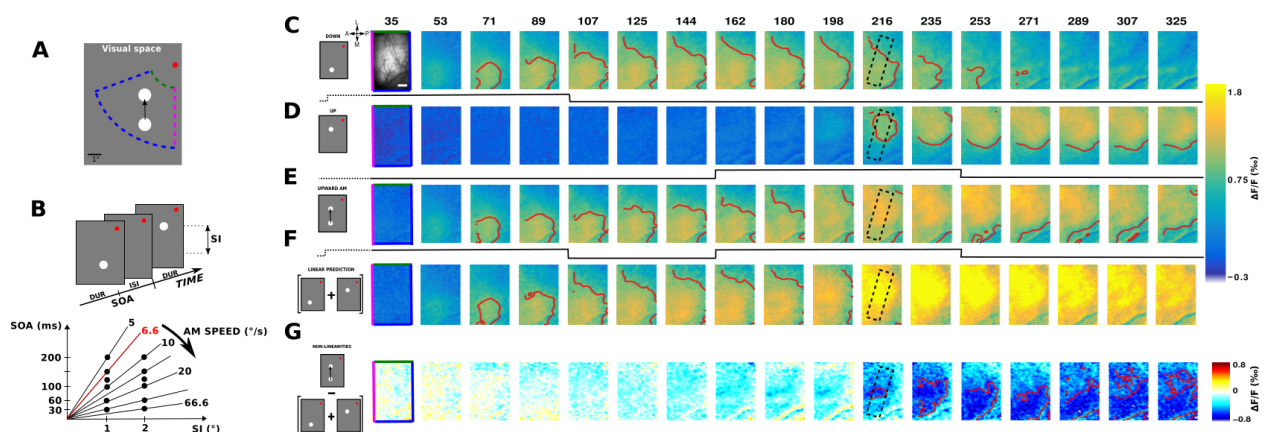
## 100 **Results**

### 101 **Characterizing the mesoscopic spatio-temporal impulse response function**

102 Two-step apparent motion sequences of various spatio-temporal characteristics (Fig 1, A and B) were  
103 presented to two behaving monkeys involved in a fixation task. The primary visual cortical response was  
104 measured at the level of the population using voltage-sensitive dye imaging (Amiram Grinvald and  
105 Hildesheim 2004; Chemla and Chavane 2010a). In response to a local stimulus ( $0.25^\circ$  in diameter)  
106 presented for 100 ms in two different visual positions (separated vertically by  $1^\circ$  or  $2^\circ$ ), activity arises at  
107 the retinotopic representation of these two positions and then spreads laterally over millimeters of  
108 cortical surface (Fig.1C: lower position, Fig. 1D: upper position) (A. Grinvald et al. 1994; Reynaud,  
109 Masson, and Chavane 2012; Muller et al. 2014). V1 activity is hereby reaching positions in space and  
110 time well beyond  $1^\circ$  and 50ms. As a consequence, the evoked spread covers a large cortical extent that  
111 can reach the representation of the other stimulus in space and beyond the inter-stimulus interval in  
112 time. The space- and time- constants of our responses were systematically quantified on the two  
113 monkeys and for the three stimulus durations we used (10, 50 and 100ms) on a 2D spatio-temporal (ST)  
114 map (Fig. 2A). To produce these ST maps, cortical activity was averaged within the apparent-motion  
115 trajectory (*dotted rectangle at frame 216 ms* in Fig. 1, C-G) to provide a unique spatial cortical dimension  
116 (ordinate in Fig. 2A). First, we extracted the space-constant of a gaussian spatial fit for all time points  
117 (see Fig. 2A, right-side of the maps). In both monkeys and across 19 sessions overall, the space-constant

118 increased from  $1.6 \pm 0.5$  mm at response onset to reach a maximum of  $3.3 \pm 0.2$  mm, independent of  
 119 the stimulus duration and monkeys (Fig. 2B, no significant difference observed between all stimuli  
 120 durations, t-test with  $p > 0.01$ ). The time-constants of the response time-course at the central  
 121 representation of the stimulus were measured using two half gaussian functions fits (see Fig. 2A,  
 122 below the maps). In both monkeys, the time-constant at response onset was on average  $23.6 \pm 17.2$   
 123 ms for all stimuli durations (except for monkey BR with a mean value of  $44.5 \pm 14.5$  ms for 100 ms  
 124 stimuli, see blue histogram in Fig. 2E), and  $80 \pm 43.6$  ms for response offset (Fig. 2F, no significant  
 125 difference observed between all stimuli durations, t-test with  $p > 0.01$ ). Lastly, we also extracted the  
 126 speed at which the response spreads across the cortical surface (see Fig. 2A, slanting lines) and obtained  
 127 a distribution with peak values of about  $0.26 \pm 0.14$  m/s, similar across monkeys and stimulus  
 128 durations (t-test with  $p > 0.01$ ), and similar to what has been observed in different species and states  
 129 (Slovin et al. 2002; Sato, Nauhaus, and Carandini 2012; Bringuier et al. 1999; Reynaud, Masson, and  
 130 Chavane 2012; Muller et al. 2014). This analysis showed that the spatio-temporal integrative properties  
 131 of the primary visual cortex are mostly independent of stimulus duration and are able to cover a large  
 132 spatial (3mm) and temporal (100ms) extent, bridging the cortical representation between our individual  
 133 stimuli in space and time.

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136 **Figure 1: Experimental protocol and time-sequence of the cortical response to the long-range apparent motion**

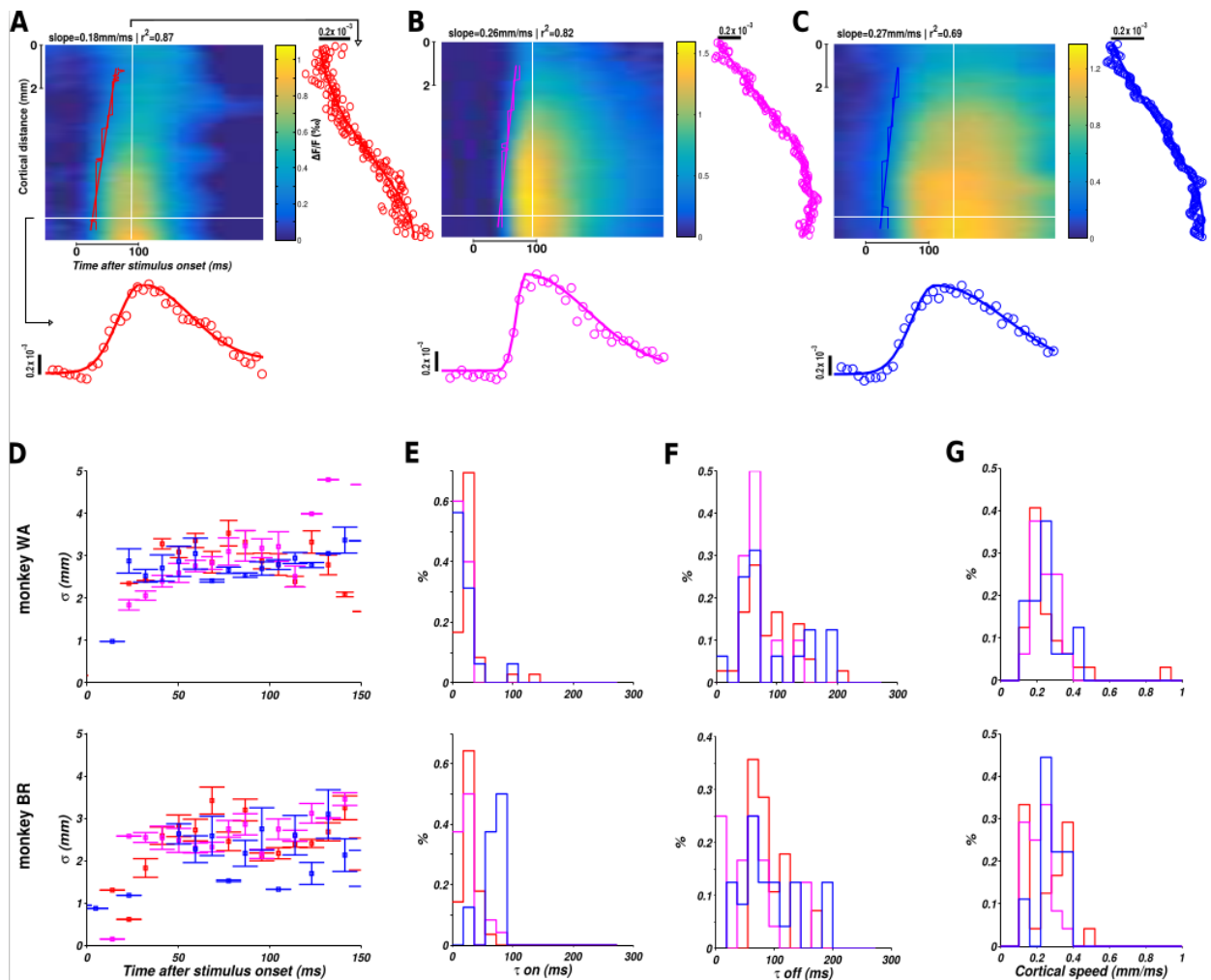
137 **(IrAM). A:** Two-step IrAM stimuli are presented to two awake fixating monkeys in their bottom left visual field,  
138 while recording in their right visual cortex using VSDI. **B:** Spatio-temporal characteristics of IrAM stimuli, i.e.  
139 duration (DUR), interstimulus interval (ISI) and spatial interval (SI), were varied to cover a [5-66.6]°/s range of  
140 speed. **C-E:** Cortical representation of evoked VSDI activity as a function of time, in response to respectively, a 100  
141 ms local stimulus in the down position, another one in the up position, and the sequence of these two stimuli (ISI =  
142 50 ms and SI = 1°). The cortical area imaged is shown at upper left. The edge of the image color codes the  
143 retinotopic borders as represented in A such as the vertical meridian (magenta), eccentricities (green and blue).  
144 Scale bar: 2 mm; A: anterior, P: posterior, M: medial, L: lateral. Time in milliseconds after stimulus onset is shown at  
145 the top, while stimulation time is drawn at the bottom of each row (black lines). **F:** Activity pattern predicted by the  
146 linear combination in space and time of the response to stimulus 1 (row C) and the response to stimulus 2 (row D).  
147 **G:** Suppression pattern obtained by subtracting the observed apparent motion response (row E) and the linear  
148 prediction (row F). Red contours delimit amplitude activity above a certain threshold: 1 % in panels C-F and -  
149 0.5% in panel G.

150

### 151 **The evoked response to the IrAM is shaped by a suppressive wave**

152 We next asked whether such lateral interactions contribute to shape the evoked population response to  
153 the temporal succession of these two stimuli. For that purpose we measured the cortical population  
154 response to a two-stroke upward apparent motion sequence (Fig. 1E). Such temporal sequence  
155 generates a propagation of activity starting at the cortical representation of the first stimulus (S1) and  
156 moving to the cortical representation of the second stimulus (S2), a cortical correlate of the illusory  
157 motion (Jancke et al. 2004). The observed pattern of activity departs from the pattern predicted by a  
158 simple linear summation of the lower and upper stimuli (Fig. 1F). If we subtract the observed (Fig. 1E)  
159 and the linear predicted responses (Fig. 1F), two deviations from non-linearities are observed. First, a  
160 suppression emerges at response onset and at the cortical representation of S2 (compare 1D and 1G at  
161 frame 216ms). The suppression then gradually propagates over the cortical surface towards the

162 representation of S1 (Fig. 1G). We can hypothesize that the evoked activities by the two stimuli  
163 composing the lrAM sequence interact together to generate this dynamic pattern of suppression. Since  
164 the suppression is observed at the onset time of the response to S2, it has to be due to the activity  
165 dynamics generated by S1 interacting with the integration of S2. However, the propagation of  
166 suppression from the representation of S2 towards the representation of S1 is probably due to the  
167 activity dynamics evoked by S2 interacting with the residual activity evoked by S1. Therefore, the  
168 suppression wave could likely be the result of multiple interactions (e.g bidirectional) between the  
169 activities evoked by the stimulus sequence.  
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**Figure 2: Spatio-temporal characteristics of cortical responses to a local stimuli. A-C: Spatio-temporal**



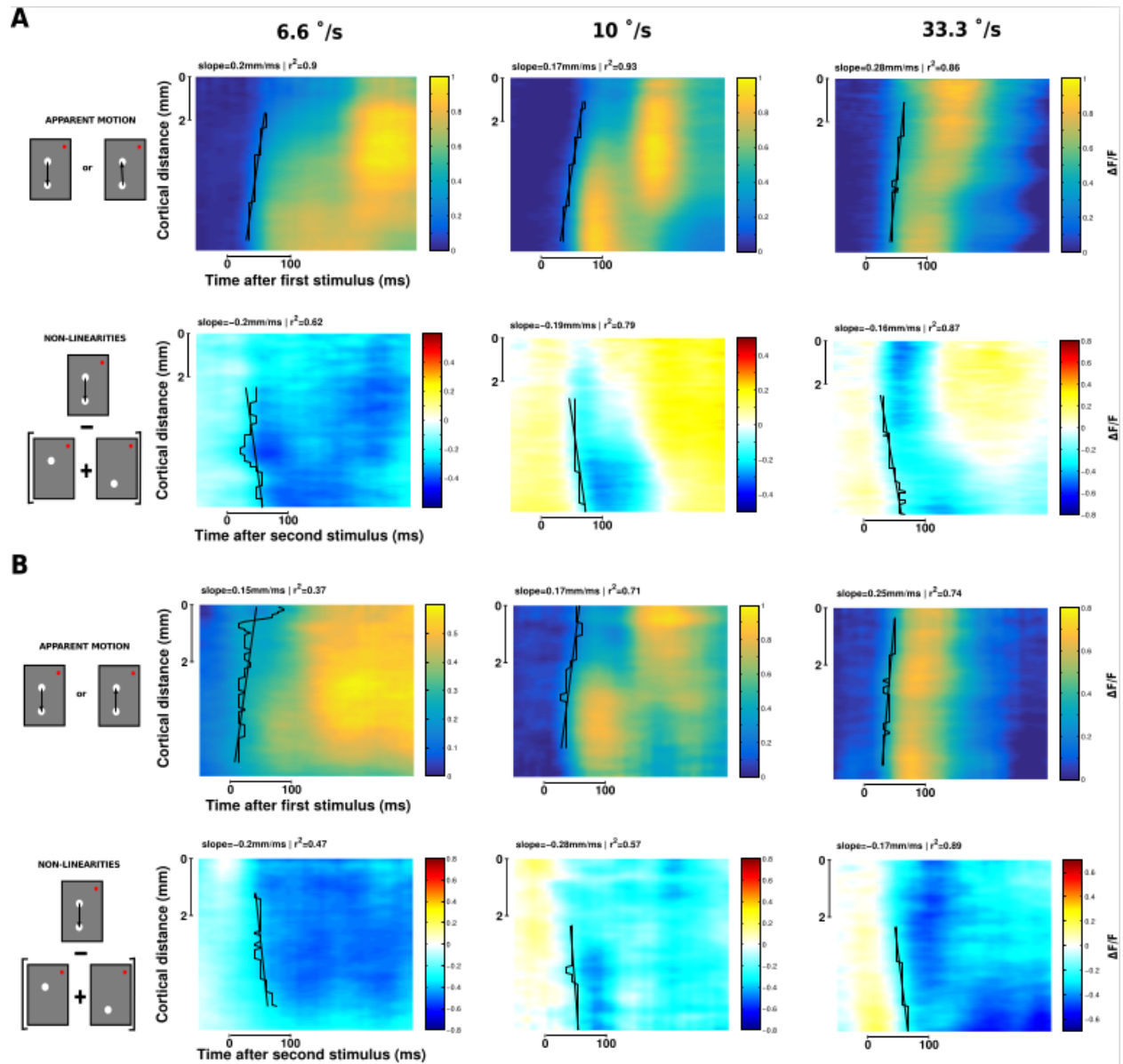
173 *representations (ST) of the evoked cortical response to, respectively, 10 ms (A, red) , 50 ms (B, purple) and 100 ms*  
174 *(C, blue) local stimuli. To produce the ST representation, we averaged spatial data along the stimulus trajectory*  
175 *(rectangle in frame 216ms, Fig1C-G). For each spatial point, the temporal data were fitted to a combination of two*  
176 *half Gaussians, as illustrated for one specific point in space (horizontal white line on the ST diagram) below the ST*  
177 *maps. Similarly, for each time frame, the spatial data were fitted to a Gaussian function as shown on the right side*  
178 *of each ST map for one specific point in time (vertical white line). D: Space-constant of the Gaussian spatial fit*  
179 *(sigma parameter) plotted as a function of time for the three considered durations (10 ms in red, 50 ms in magenta*  
180 *and 100 ms in blue) and for the two monkeys (top: monkey WA, bottom: monkey BR). E: Histograms of time-*  
181 *constant at response onset ( $\tau_{on}$ ) estimated from the temporal fit of the response for the three considered*  
182 *durations and the two monkeys. F: Histograms of time-constant at response offset ( $\tau_{off}$ ) estimated from the*  
183 *temporal fit of the response for the three considered durations and the two monkeys. G: Histograms of cortical*  
184 *speed of propagation estimated by linear regression on response latency (stairs-step contours, slanting lines and*  
185 *slope of the linear regression) for the three considered durations and the two monkeys.*

186

### 187 **The suppressive wave is systematically observed**

188 To better investigate how spreads of evoked activity and suppression shape the representation of IrAM,  
189 we first show ST representations of examples taken for both monkeys and three stimuli speeds. The  
190 example of Figure 1 is shown in Figure 3A (6.6°/s). In these ST representations, we can observe a clear  
191 propagation of activity in response to a local stimulus (slanting lines in Fig. 3, A and B) that is remarkably  
192 similar across both monkeys (Fig. 3, A and B, *first rows*) and speeds (three columns respectively for  
193 6.6°/s, 10°/s and 33.3°/s, as shown in Fig. 2F). The ST representation of non-linearities (lower rows)  
194 recentered on S2 onset, shows that suppression first appears at the cortical representation of S2 and at  
195 S2 response onset, and then propagates towards the representation of S1, at a similar speed than the  
196 one observed for the evoked activity to the first stimulus (Fig. 3, A and B, *second rows, slanting lines*). In  
197 both monkeys and the three examples shown, this suppression propagates in a direction opposite to the

198 apparent motion sequence, from S2 to S1 representations. Functionally it results in silencing the residual  
 199 activity generated by S1.



200

201 **Figure 3: The apparent motion stimulus induces a systematic suppression wave. Spatio-temporal representation**

202 *of VSDI responses to two-stroke apparent motion stimuli for three different speed (6.6°/s, 10°/s and 33.3°/s) and*

203 *two animals (A: monkey WA, B: monkey BR). The upper rows of A and B represent the observed response and the*

204 *lower rows the non-linearities of the response (observed - linear prediction). Estimates of speed propagation are*

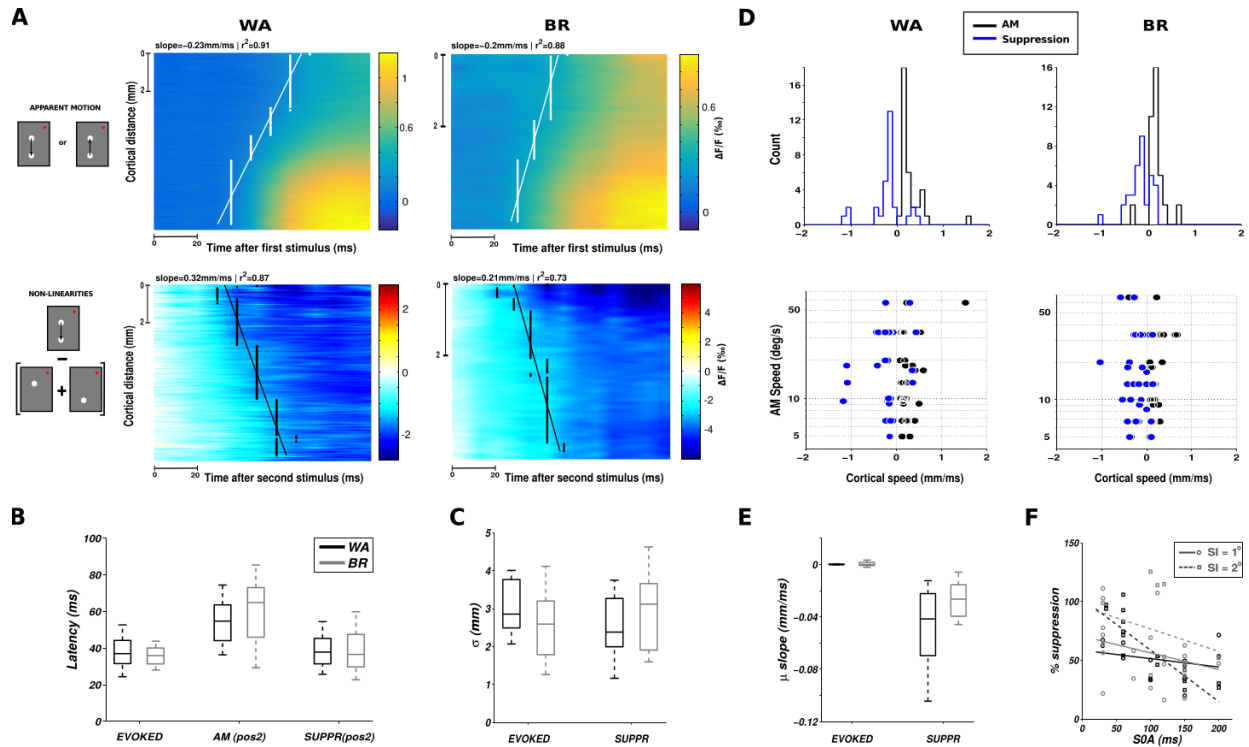
205 *reported on each ST diagram (black stairs-step are contours at threshold level, slanting lines are the slope of the*

206 *linear regression*). Similar values are observed for both the observed activity and the non-linearities.

207 **The suppressive wave propagates at the same speed and with same extent as the evoked spread**

208 This suppressive wave was systematically observed for all two-stroke IrAM conditions tested (see  
209 Fig.1B). This can be seen in the ST evoked response (centered on the onset of S1) and nonlinearities  
210 (centered on the onset of S2) averaged across all conditions and sessions for both monkeys (Fig. 4A). To  
211 better understand the origin of the suppression dynamics, and its dependence on stimulus conditions,  
212 we characterized its spatio-temporal properties. First, we measured the onset of the apparition of the  
213 suppression at S2 position. The latency of the observed suppression was the same as the latency of the  
214 activity evoked by S2 alone (Fig. 4B, respectively 39.5 +/- 2.0 ms vs. 38.6 +/- 1.6 ms for monkey WA and  
215 36.6 +/- 1.8 ms vs. 36.9 +/- 2.1 ms for monkey BR, non-significantly different, t-test with  $p = 0.77$  and  $p =$   
216  $0.35$  respectively for WA and BR). However, the suppression resulted in significantly delaying the  
217 response onset evoked by S2 when presented within the apparent motion sequence (54.2 +/- 2.0 ms  
218 and 68.3 +/- 5.3 ms for WA and BR respectively, Fig. 4B). Then, we quantified the spatial extent of the  
219 suppression ( $\sigma$  of a Gaussian fit, Fig. 4C). In all conditions, the spatial extent of the suppression was of  
220 about 2.8 mm (2.49 +/- 0.14 mm for WA and 3.08 +/- 0.18 mm for BR), similar and non significantly  
221 different than the spatial extent of the evoked response (2.99 +/- 0.11 mm and 2.41 +/- 0.17 mm for WA  
222 and BR respectively). Thus the suppressive wave starts at similar latency and covers similar spatial  
223 extent. We next characterized the speed of propagation of activity (Fig. 4D black) and suppression (Fig.  
224 4D blue), plotted as a function of stimulus speed. Remarkably, on both monkeys, the observed cortical  
225 speeds were identical for both the propagation of activity and the suppression and completely  
226 independent of the IrAM speed (0.28 +/- 0.26 m/s and 0.27 +/- 0.4 m/s respectively for WA and 0.21 +/-  
227 0.15 m/s and 0.27 +/- 0.2 m/s respectively for BR). However, from the ST plots in Figure 3, we noticed  
228 that the suppression does not seem to spread but rather propagates as a wave (Muller et al. 2014,  
229 2018). To probe for this hypothesis we thus compared the dynamics of the response peak position ( $\mu$  of

230 a Gaussian fit). In a spread, typically, the response peak will not move in space, as observed for evoked  
231 response (Fig. 4E, the peak spatial position is not changing with time, slope of  $-1.3 \times 10^{-5}$  +/-  $1.1 \times 10^{-4}$  m/s  
232 and  $1.6 \times 10^{-4}$  +/-  $3.4 \times 10^{-4}$  m/s for WA and BR respectively), whereas in a wave it will follow the onset  
233 spatial displacement, which is what we found for the suppression (Fig. 4E, the peak moves from position  
234 2 to position 1, negative slope of  $-0.05$  +/-  $0.007$  m/s and  $-0.034$  +/-  $0.005$  m/s for WA and BR  
235 respectively). Altogether, our results show that the suppression is initiated at response onset, have  
236 similar spatial extent and propagation speed as the activity evoked response. Furthermore, although  
237 evoked activity are waves hidden by spatial averaging (Muller et al. 2014), the suppression is still seen as  
238 a wave in the averaged data. This strongly suggests that the suppression is likely to be mediated by the  
239 same general process generating the propagation of evoked activity, most probably the intra-cortical  
240 horizontal network (Muller et al. 2014). If the suppression is generated along the propagation of activity,  
241 one prediction is that it should decrease in strength with spatial and temporal separation between the  
242 two stimuli composing the IrAM. This is indeed what was observed, the suppression strength decreases  
243 as a function of stimulus onset asynchrony and spatial separation (Fig. 4F, t-statistics on the slope of the  
244 linear regression gives  $t = -0.92$  with  $p=0.18$  and  $t = -6.3$  with  $p = 3.6 \times 10^{-6}$ , respectively for a spatial  
245 interval of  $1^\circ$  and  $2^\circ$  (WA);  $t = -1.2$  with  $p=0.12$  and  $t = -1.6$  with  $p = 0.05$  (BR)).  
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247

248

**Figure 4: The suppressive wave has the same properties as the evoked intra-cortical propagation.**

249

**A:** Spatio-temporal VSDI activity (top row) and non-linearities (bottom row) averaged across all IrAM speed

250

conditions and centered on stimulus 1 (S1, top row) or stimulus 2 (S2, bottom row) onset, for both monkeys

251

(columns). **B:** Boxplot of latency (ms) estimates comparing the onset of activity evoked by S2 alone (“evoked” condition),

252

the response onset evoked by S2 when embedded in the IrAM sequence (“IrAM” condition) and the onset of the

253

suppression at S2 position (“suppr” condition). Boxplots illustrate median, 25 and 75% quartiles and minimum and

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maximum of the distributions across all IrAM speed conditions, for the two monkeys (black WA, gray BR). **C:** Boxplot

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of space-constants (parameter  $\sigma$  of a Gaussian spatial fit) comparing the evoked response and the suppression, for

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the two monkeys. **D:** For each condition in both monkeys (columns), we estimated the speed of propagation of the

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VSDI (black) and the non-linearity (blue). The upper row shows frequency histograms and the lower row these

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speeds as a function of the speed of the IrAM stimulus. **E:** Boxplot of the response peak propagation speed (slope of

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the linear regression on the parameter  $\mu$  of a Gaussian spatial fit) comparing the evoked response and the

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suppression, for both monkeys. **F:** Suppression strength (normalized to the maximal response activity) as a function

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of stimulus onset asynchrony and spatial interval (open circle for  $SI = 1^\circ$ , open square for  $SI = 2^\circ$ ), for both monkeys

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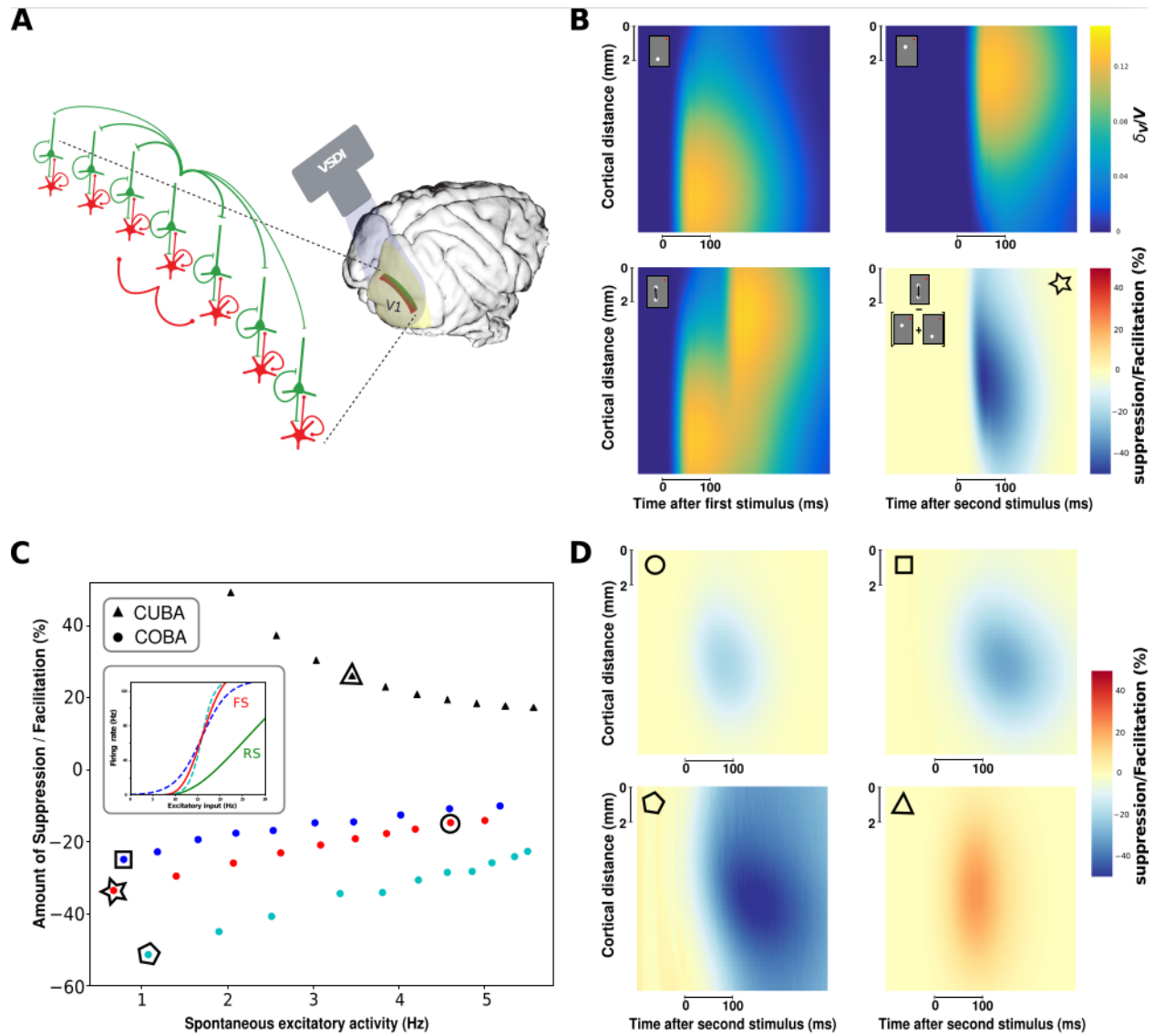
(black WA, gray for BR).

263

264 **The suppressive wave can be the result of a dynamic gain control**

265 What can be the origin of such suppressive wave? Since inhibitory intra-cortical axons have more limited  
266 spatial extent (Buzás et al. 2001), and that feedback from higher areas are excitatory (Salin and Bullier  
267 1995), we can hypothesize that it does not result from a simple net inhibition, but rather as a byproduct  
268 of the excitatory/inhibitory balance (Tsodyks et al. 1997; Ozeki et al. 2009). Indeed, as demonstrated  
269 using center-surround stimulations, the suppressive wave can be the result of a simple dynamic input  
270 normalization fed by propagation along the horizontal network (Reynaud, Masson, and Chavane 2012).  
271 To determine the possible mechanisms generating the observed suppression, we used a mean-field  
272 model designed to reproduce accurately VSDI (Zerlaut et al. 2018). In this model, it was assumed that  
273 each pixel of the VSDI represents the average  $V_m$  of two populations of interacting neurons, excitatory  
274 regular-spiking (RS) neurons, and inhibitory fast-spiking (FS) neurons (Chemla and Chavane 2010b).  
275 Arranging this model into a spatially extended interconnected populations of RS-FS cells (Fig. 5A, see  
276 Methods) allows to simulate the propagating waves observed in awake monkey under VSDI. The great  
277 advantage of such model is to explicitly take into account conductance-based interactions (COBA) as  
278 well as a different gain between excitation and inhibition. These ingredients are often neglected as they  
279 introduce difficulties in mathematical tractability of mean field models (Landau et al. 2016; Vogels,  
280 Rajan, and Abbott 2005). Nevertheless, these features are biologically relevant and, as we show here,  
281 are actually the main elements determining waves suppression. Examples of two independent waves  
282 are shown in Fig. 5B (upper row). When the two stimuli are presented in succession (see Fig. 5B lower  
283 left) the observed response shows a suppression (Fig. 5B lower right), whose values are quantitatively  
284 similar to those of experimental data (suppression of around 50% of the response max). Such  
285 suppressive effect was robustly observed across a wide range of the parameters space. The first  
286 parameter that was found to strongly affect the suppression is the ongoing spontaneous activity of the

287 system pre-stimulus. As we report in Fig. 5C (COBA model, red dots), the suppression decreases when  
288 the spontaneous activity of the system increases (see example marked by a circle, Fig 5D). Moreover,  
289 two further mechanisms were necessary to explain this suppressive effect. First, inhibitory cells need to  
290 have a higher gain than excitatory cells. When the gain of FS cells was reduced (see inset of Fig. 5C) to  
291 have a gain closer to the one of RS cells, the suppression effect was strongly affected (blue dots in Fig.  
292 5C, example marked by a square in Fig. 5D). Accordingly, increasing FS cell gain (cyan dots in Fig. 5C,  
293 example marked by a pentagon in Fig. 5D) increases the suppression strength. Second, the interaction  
294 between excitatory and inhibitory inputs needed to occur through conductances-based mechanisms.  
295 Indeed, when using a current-based (CUBA) model (see Methods), we mostly observed facilitation (black  
296 triangles in Fig. 5C) that do not appear to propagate (see example marked by a triangle, Fig. 5D). While  
297 we do not exclude that such suppression may be observed in current-based synapses, it is clear from  
298 these data that the non-linearity of voltage dependent synapses induces a strong suppression in VSDI  
299 signal. The suppression can thus be explained by the mesoscopic combination of the nonlinearity of  
300 conductance interactions and the differential gain of excitatory and inhibitory cells.  
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302

303

**Figure 5: A computational model to investigate the possible origin of the suppressive wave.**

304

**A:** Mean-field model of excitatory and inhibitory neurons distributed on the cortical trajectory of the stimulus with

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horizontal connectivity (longer for excitatory than inhibitory neurons). **B:** Model ST response to the first stimulus

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(upper left), the second (upper right), the apparent motion sequence (lower left) and the non-linearities normalized

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to the maximal response over space and time of the response to single stimuli (lower right). The input has an

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amplitude  $v_0=20$  Hz. **C:** Amount of suppression/facilitation as a function of the spontaneous excitatory firing rate.

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Colored dot stand for different interneurons gain (see inset), while black triangles stand for the Current-based

310

(CUBA) model, that shows little suppression but facilitation. The input has an amplitude  $v_0=10$  Hz. **D:**

311

Representative ST suppressive/facilitative patterns as marked in C by different geometric shapes (circle, square,



312 *pentagon, triangle). The star in C corresponds to the model parameters used for obtaining the suppressive pattern*  
313 *shown in B.*

314

### 315 **The function of the suppressive wave is to explain away ambiguous representations**

316 What can be the function of the suppressive wave? Here we propose that it will shape an unambiguous  
317 representation of motion along the apparent-motion trajectory. Indeed, silencing the cortical

318 representation of the initial stimulus when the second stimulus is being processed will have as a

319 consequence to represent only one stimulus at a time, hereby improving motion representation by

320 explaining away ambiguous position representation (problem of “phenomenal identity”) (Ternus 1926).

321 To quantify such hypothesis, we developed a simple algorithm to decode, at every instant, what is the

322 most probable stimulus position that evoked the observed cortical spatial profile out of four categories:

323 no stimulus, S1, S2, or joint S1 & S2. We used the ST representations of the evoked activity to the

324 apparent motion sequence (Fig. 6A) and used the linear prediction (Fig. 6B) as a control. The decoding

325 was computed using the joint probability that the spatial profile observed at one point in time (white

326 profile) is drawn from the spatial profile observed during blank (first row, black), S1 (second row, red),

327 S2 (third row, blue), or the joint S1 & S2 (last row, green). In the example shown in figure 6, we apply

328 this decoding method to the activity evoked by a  $6.6^\circ/s$  two stroke apparent motion stimulus (Fig.6A).

329 When S1 is presented (red), the probability that the spatial profile of the evoked response will be similar

330 to the blank distribution is quickly dropping from 1 to 0 and the probability that the evoked response

331 will be decoded as being evoked by S1 alone is jumping from 0 to 1 very rapidly (in 10ms). When S2 is

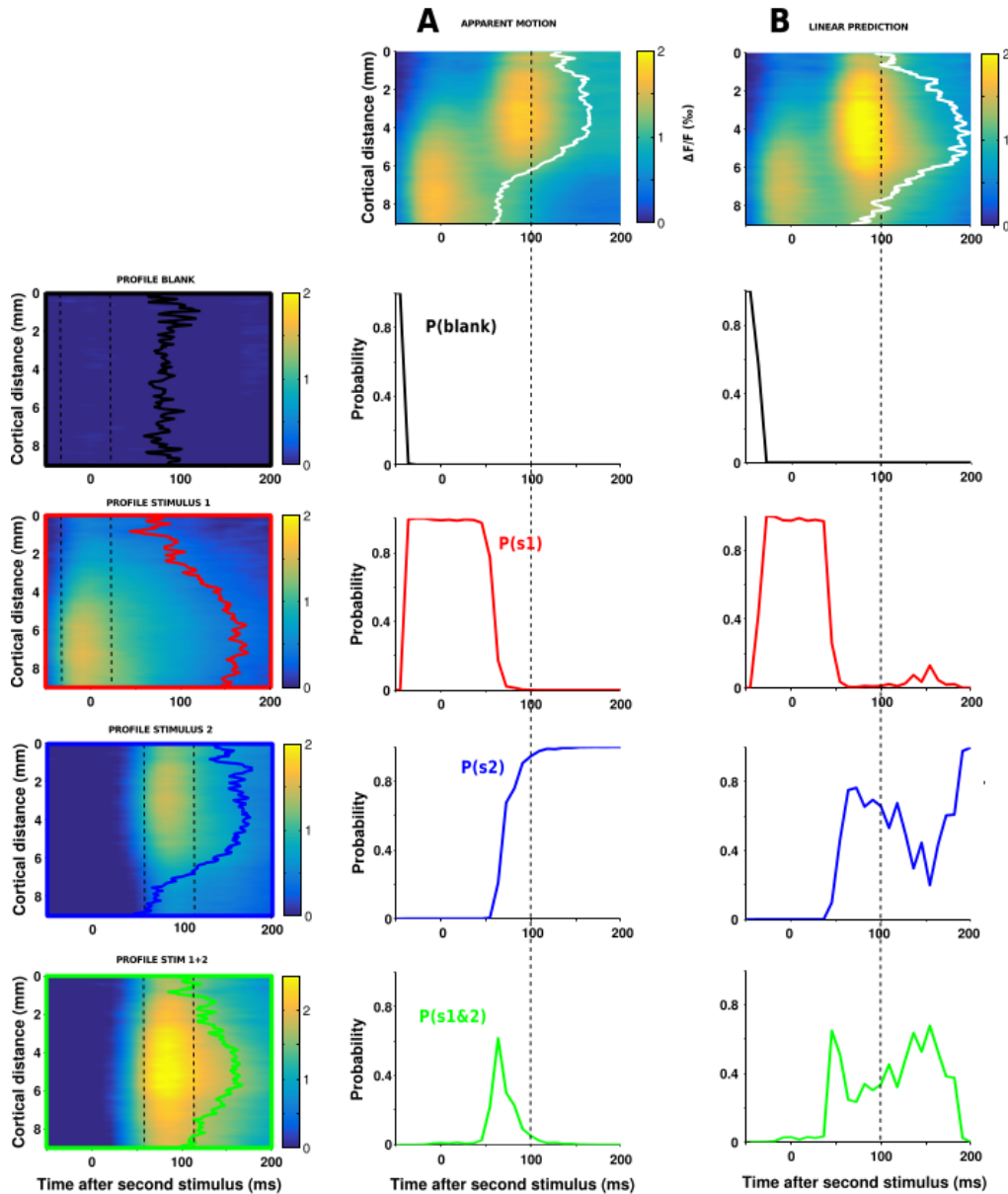
332 presented (at time 50ms) there is a sharp and rapid transition from the evoked activity being decoded as

333 S1 to S2 (blue) in about 50ms. However, the probability that the evoked activity is evoked by S1 & S2 at

334 the same time (green) is only increased moderately (peaking at 0.5) and transiently. In contrast, when

335 we apply the same approach to the linear prediction (Fig.6B), while the beginning of the decoding is the

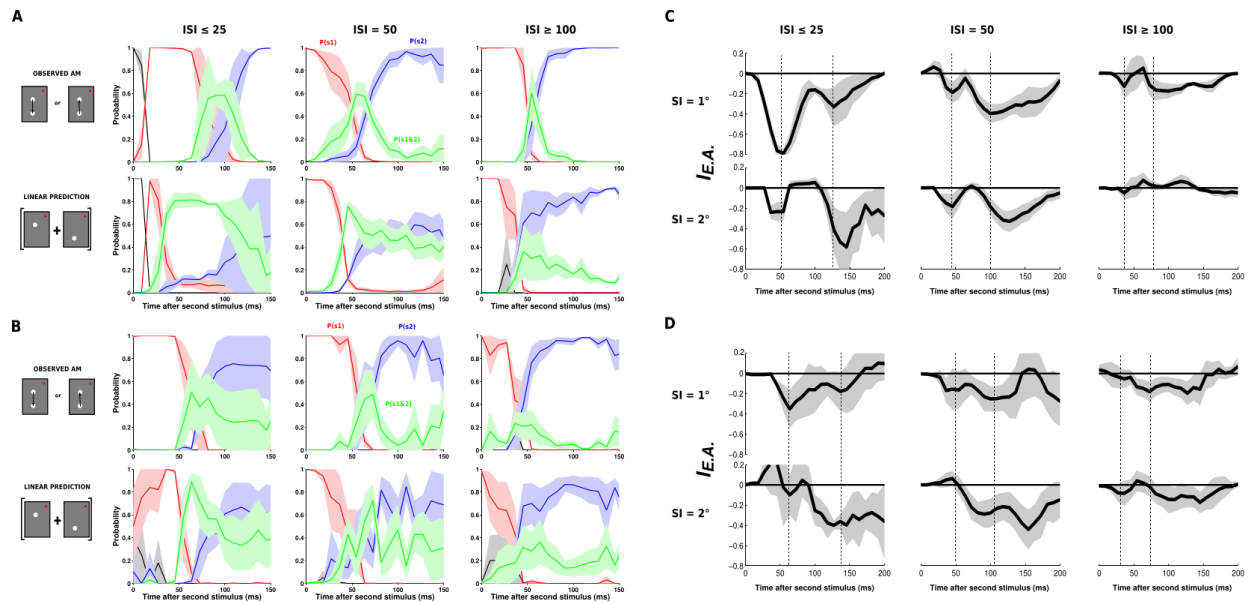
336 same (two first rows), as expected, when S2 appears, the evoked activity is ambiguously decoded as  
337 being attributed to S2 or S1 & S2 conjointly with similar probability (around 0.5).  
338



339  
340 **Figure 6: A dynamic decoding of stimulus position: Principle.** The decoding of stimulus position on ST maps, here  
341 taking the example of the activity evoked by a 6.6 %/s IrAM stimulus shown in **A** or the activity pattern predicted by  
342 the linear combination in space and time of the responses to both individual stimuli in **B**. The decoding consists in  
343 evaluating the probabilities that the spatial profile observed at each point in time (white contours in **A** and **B**) is

344 *similar to one of the four spatial profiles shown on the left column: Blank (first row, black profile), S1 (second row,*  
345 *red profile), S2 (third row, blue profile), and the joint S1 & S2 (last row, green profile). Each profile was computed by*  
346 *averaging the corresponding ST response in a 50ms-window around the time of maximum response and*  
347 *normalized. The four color-coded probabilities are respectively plotted as a function of time (time 0 corresponds to*  
348 *the onset of S2) for the IrAM response (**column A**) and for the linear prediction (**column B**). Compared to the linear*  
349 *prediction, the actual signal is more rapidly decoded, revealing a likely function of the suppressive wave:*  
350 *disambiguating stimulus position representation.*

351  
352 We applied this approach to all speeds and sessions in both monkeys (Figure 7A&B), for spatial interval  
353 of 1°, differentiated across the different inter-stimulus intervals (ISI). We separated these conditions  
354 because, when S2 appears, the residual activity in response to S1 will be less important for long ISI (the  
355 offset time constant being of the order of 80 ms). In both monkeys and for ISI ≤ 50ms, the averaged  
356 results confirm the individual example shown in Figure 6: the evoked activity results in a sharp and clear  
357 transition from the representation of S1 to the representation of S2, with only transient increase of the  
358 representation of S1 & S2 conjointly. In comparison, the linear prediction always leads to an ambiguous  
359 representation that cannot tease apart the probability that the evoked activity is coming from S2 alone  
360 or S1 & S2 together (blue and green curves merging together). For an ISI ≥ 100ms, in contrast, the  
361 evoked activity resembles more the linear prediction, as expected.



362

363

**Figure 7: A dynamic decoding of stimulus position: Application to all IrAM speeds and sessions.**

364

**A:** Color-coded probabilities (same as Figure 6) for the observed IrAM response (first row) and its corresponding

365

linear prediction (second row) for monkey WA, averaged across three ISI categories: ISI < 25 ms (left column), ISI =

366

50 (central column) and ISI > 100 ms (right column). **B:** Application of the decoding algorithm to all the data of

367

monkey BR. **C:** Explaining away index (see text and methods) computed as the probability of detecting joint S1 & S2

368

in the observed response minus the probability of detecting joint S1 & S2 in the linear prediction, from monkey WA

369

data shown in panel A. **D:** Explaining away index from monkey BR data shown in panel B.

370

371

To quantify the effect of explaining away ambiguous positional representations during IrAM

372

stimulations, we calculated an index by subtracting the probability of detecting joint S1&S2 in the

373

observed and the linear prediction for both monkeys,  $I_{E.A.} = P_{S1\&S2}^{obs} - P_{S1\&S2}^{pred}$  (Fig. 7C&D), and both

374

stimuli spatial intervals (SI) of 1 and 2° (first and second rows respectively). In all conditions but the long

375

SI and long ISI, a systematic decrease of the index was observed. This reveals a dynamic effect of

376

explaining away the ambiguous representation of S1&S2. Importantly, in both monkeys and practically

377

all conditions (ISIs and stimulus separation), we observed two peaks in the index decrease. They

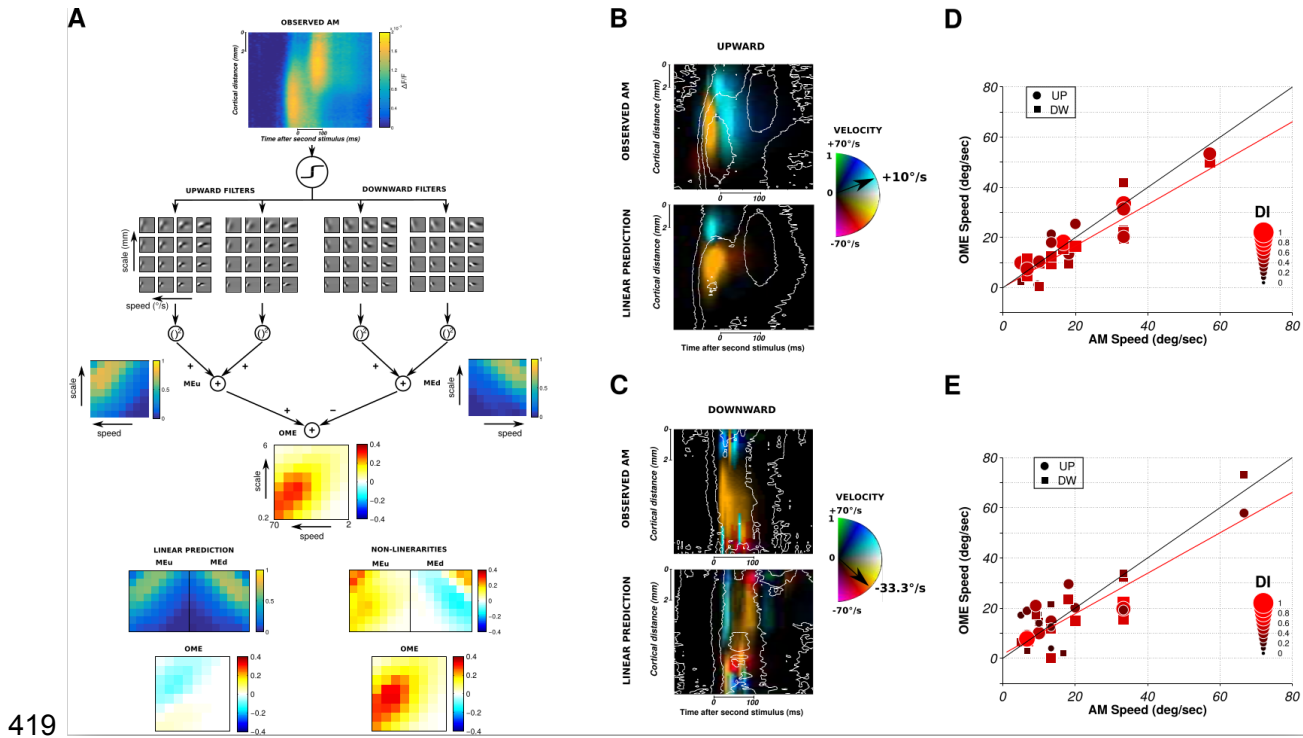
378 correspond to the bidirectional interactions occurring for each of the two evoked waves. The first peak  
379 corresponds to the effect of delaying response onset to S2 (by propagating activity from S1 to S2) , and  
380 the second peak corresponds to a shortening of the representation of S1 (by propagating activity from  
381 S2 to S1). Importantly, this calculation revealed two further phenomena that are expected because of  
382 the propagation delay and spatial extent. First, the timing of the second peak is delayed when going  
383 from 1 to 2° spatial separation. Second, the general amplitude of the decrease diminishes from short to  
384 longer ISI.

385

### 386 **Unambiguous representation for optimal encoding of velocity in V1**

387 Disambiguating the cortical population representation of the IrAM could promote an accurate  
388 encoding of direction-selective motion signals for an optimal read-out by downstream area. To test  
389 whether the measured cortical response encodes an accurate direction-selective signal, we applied  
390 opponent motion energy filters directly to V1 population responses (Adelson and Bergen 1985). Indeed,  
391 direction selectivity in MT is well described and captured by motion energy models (Adelson and Bergen  
392 1985; Rust et al. 2006). Such an approach is generally developed to model MT receptive field from a  
393 spatio-temporal input image. The rationale here is to apply the same processing directly to V1  
394 population responses that feed downstream areas such as MT or V4. This is justified by the fact that the  
395 cortical extent imaged here (~ 9mm, corresponding to 3°, see (Dow et al. 1981; Van Essen, Newsome,  
396 and Maunsell 1984)) actually corresponds to the V1 cortical extent converging to a MT or V4 neuron at  
397 our recorded eccentricity (3°, see Albright and Desimone 1987; Gattass, Sousa, and Gross 1988). Since  
398 we record VSD responses that represent both sub- and supra-thresholds activities (Chemla and Chavane  
399 2010b), we first processed our ST maps through a non-linearity to account for the VSD to spike rate  
400 transformation (Chen, Palmer, and Seidemann 2012) (Fig 8A). The resulting ST maps were convolved

401 with a set of spatio-temporal filters covering a wide range of speeds and scales. For a given value of  
402 filter speed and scale, we squared and summed the convolution from filters in quadrature, and  
403 subtracted the resulting phase-independent measure of local motion energy for opposite directions (ie.  
404 ME<sub>u</sub> - ME<sub>d</sub>) to obtain the opponent motion energy response (OME, Fig. 8A). We thereby obtained the  
405 opponent motion energy for all speeds, scales and directions. For each position on the ST map, we could  
406 hence extract the filter velocity for which the opponent motion energy is maximal, that we represented  
407 for both monkeys, and different velocities (10°/s upward in monkey1, Fig. 8B and -33°/s downward in  
408 monkey 2, Fig. 8C). In this representation, the color hue represents the velocity of the filter yielding a  
409 maximal opponent motion energy and the color intensity its amplitude (as a fraction of the maximum  
410 evoked fluorescence response). The contour of the evoked response is overlaid in white to ease  
411 comparison. The same analysis on the corresponding linear predictions serves as a control. For all the  
412 conditions we explored, we then extracted the values of the optimal velocity within a ST region of  
413 interest (between S1 and S2's centers and from 10 to 200 ms after stimulus 2 onset) and represented  
414 them as a function of the AM speed for both monkeys (Fig. 8D and 8E). Our results show that the ST  
415 response, disambiguated through the suppressive wave, is indeed generating a direction selective  
416 motion energy for a speed that is well correlated with the stimulus speed. In other words, intra-cortical  
417 non-linear interactions in V1 promote an unambiguous optimal encoding of velocity-selective motion  
418 signal along the apparent motion path.



419

420 **Figure 8: Encoding of direction-selective motion signal. A:** Application of the opponent motion energy model  
 421 (Adelson & Bergen, 1985) to the ST representation of cortical response to an upward  $10^\circ/s$  AM sequence shown at  
 422 the top. The first step consists in convolving the ST data with a set of oriented ST filters. Phase-independency is  
 423 obtained by squaring and summing the outputs of quadrature pair of filters, while motion opponency is obtained by  
 424 subtracted the two oriented motion energies ( $OME = MEu - MEd$ ). The maximal energy values for each ST filter are  
 425 plotted as a function of speed (in  $^\circ/s$ ) and scale (in mm). The energy values resulting from the same computation  
 426 applied on the linear prediction and the non-linearities for this AM sequence are respectively shown at the bottom  
 427 left and right. **B:** ST representation of the opponent motion energies computed in panel A. For each ST position, the  
 428 filter velocity for which the energy was maximal is represented as different color hue. The amplitude of the energy  
 429 is coded as color intensity. For comparison, the result for the corresponding linear prediction is shown below. **C:**  
 430 Same than B for monkey BR, for another AM sequence condition ( $33.3^\circ/s$  downward motion). **D:** Filter speed that  
 431 generated the strongest OME within a ST region of interest (see Methods) as a function of the actual IrAM speed  
 432 for monkey WA. The color and size of the dots (upward motion conditions) and squares (downward motion  
 433 conditions) code for the value of the direction-selectivity index (DI). **E:** Same than D for monkey BR.

434

## 435 **Discussion**

436 We showed that intra-cortical interactions are playing a key role in shaping the sensory representation  
437 of the long-range apparent motion within the retinotopic map of V1 in awake monkeys. Our results  
438 demonstrate that intra-cortical propagation encompasses large spatial and temporal distances allowing  
439 to link information between stimuli presented in distal spatial positions (spatial constant of about 3 mm,  
440 equivalent to  $1^\circ$ , and time constant of about 80 ms). Interestingly, above these values, the apparent  
441 motion illusion gradually fades out (Kolars 1972; Cavanagh and Mather 1989). In response to a two-  
442 stroke lRAM sequence, we observe a clear displacement of activity on the cortical surface that deviates  
443 from the linear prediction in two aspects. First, the initial stimulus suppresses and delays the response  
444 to the second stimulus. Then, a suppressive wave is evoked by the second stimulus that strongly and  
445 rapidly attenuates the residual activity evoked by the first stimulus. The spatio-temporal characteristics  
446 of the suppression showed similar spatial constant and similar propagation speed as what was observed  
447 for the evoked activity, independent of the speed of the apparent motion stimulus. However, the  
448 suppression propagated as a true wave in direction of the initial stimulus position, even at the trial-  
449 averaged level, an observation that departs from what we observed in the evoked activity (Muller et al.  
450 2014). We propose that the suppression arises from a simple gain-control mechanisms pooling  
451 feedforward and horizontal inputs (Reynaud, Masson, and Chavane 2012). To demonstrate this, we used  
452 a conductance based mean-field model developed to account for VSD dynamics (Zerlaut et al. 2018).  
453 This model shows that the observed suppression can be explained by nonlinear conductance  
454 interactions, combined with the different gain of excitatory and inhibitory cells. A decoding approach  
455 demonstrates that the suppressive wave acts as explaining away the ambiguous representation allowing  
456 to represent only one stimulus at a time in the cortex. Using opponent motion analysis applied to the



457 population response, we demonstrate that such unambiguous representation allows V1 to encode  
458 accurately the velocity signal of the IrAM that could support the read-out process from downstream  
459 areas.

460

#### 461 **Suppression and normalization as generic operations in the visual system**

462 The dynamics of the suppression is seen here as a central and key mechanism by which the input is  
463 shaped and normalized by V1 populations. When more than one stimulus is present in a visual scene,  
464 suppressive interactions between the feedforward-driven activities is what is traditionally reported,  
465 such as the well documented surround suppression (Blakemore and Tobin 1972; Angelucci et al. 2002;  
466 Cavanaugh, Bair, and Movshon 2002). This suppression is generally attributed to be an emergent  
467 property of the divisive normalization computation (Carandini and Heeger 2011). Importantly, we have  
468 shown that this normalization process is dynamic and propagate from the representation of the stimulus  
469 surround towards the representation of the center (Reynaud, Masson, and Chavane 2012). Adding a  
470 new lateral input (mostly excitatory at long-distance) is therefore resulting in a decrease from the linear  
471 prediction, a paradoxical inhibitory effect (Tsodyks et al. 1997) well captured by Stabilized Supralinear  
472 Networks (Ozeki et al. 2009). Similar suppression was also seen in response to the line-motion stimulus  
473 (Jancke et al. 2004), however, in that stimulus conditions, it was preceded by a transient facilitation. The  
474 main difference with our paradigm is that, in the line-motion condition, the second stimulus, a bar, is  
475 providing a feedforward activation all along the trajectory of the evoked wave. In the apparent motion,  
476 the interactions involve only cortical interactions at positions that do not receive any feedforward input.  
477 This may explain the differences observed with the line-motion stimulus. We believe that dynamic non-  
478 linear interactions subtended by intra-cortical network acts as a general gain control shaping the  
479 representation of visual stimulus in space and in time.

480

481 **Modeling the suppressive waves**

482 Possible mechanisms underlying the observed suppressive effects were investigated using a spatially  
483 extended computational model. We found that the model can reproduce the observed suppression,  
484 provided two mechanisms are present: excitatory and inhibitory cells have a different gain, with a  
485 higher gain for inhibition, and excitatory and inhibitory synaptic inputs must combine through  
486 conductance-based interactions. Although these two mechanisms are well known, they are usually  
487 neglected in mean-field models because they represent a mathematical difficulty. The classic mean-  
488 field models with linear (current-based) interactions and uniform gain in all cells, fail to reproduce  
489 the suppressive effect of propagating waves, and thus the present model can be considered as a step  
490 towards biologically more realistic mean-field models. Hence, by constructing a realistic mean-field  
491 model, we could demonstrate that this suppression wave is an expected byproduct of the known  
492 anatomy and does not need to be expressed solely by pure inhibition. This computational approach  
493 demonstrates how excitatory and inhibitory propagation of activity along horizontal network can  
494 dynamically change the cortical gain control resulting in the emergence of the observed suppression  
495 dynamics.

496

497 **Backward suppression to keep track of object identity along the apparent motion path**

498 This suppression can help to represent unambiguously one object at a time on the cortical surface, as  
499 our decoding model suggests. This means that the lateral interactions can link the transient spatio-  
500 temporal events while keeping track of the object moving along the trajectory. This could be a first  
501 mechanism involved in solving the correspondence problem (Ullman 1978). This problem, first  
502 introduced by Ternus as a problem of phenomenal identity (Ullman 1978; Ternus 1926), explicit the fact  
503 we need to keep track of the identity of an object in movement, and, in the case of multiple objects  
504 present at each time frame, a problem of correspondence may occur. The literature clearly show that

505 the correspondence is solved through spatio-temporal coherence more than shape or color consistency  
506 (Kahneman, Treisman, and Gibbs 1992). The correspondence, called “reviewing” by Kahneman et al.  
507 (1992) was proposed by these authors to *“operate(...) backward, (...) select(...) only a single item, and*  
508 *(...) is guided mainly by the features that control the unity and continuity of an object over time, but not*  
509 *by the shape, color, or content of the target.”* We believe that the mechanisms of backward suppression  
510 demonstrated here is an elementary and preliminary form of this reviewing process, explaining away  
511 ambiguities in the representation of the object trajectory, that will evidently necessitate further  
512 processing downstream the visual system. For instance, what we documented here could explain the  
513 ability of our visual system to detect objects based solely on the coherence of their spatio-temporal  
514 trajectory. In their seminal work, Watamaniuk and collaborators (1995) indeed showed that a single dot  
515 following a temporally coherent trajectory can be detected against a background of dots following a  
516 random walk, the only difference between signal and noise dots movement being their spatio-temporal  
517 coherence (Watamaniuk, McKee, and Grzywacz 1995). Computational studies suggested that this ability  
518 to detect coherent trajectories necessitates propagation of information in retinotopic reference frames  
519 (Perrinet and Masson 2012), in full accordance with our results.

520

### 521 **Local vs Global motion processing**

522 The processing that we describe here clearly departs from classical motion integration documented in  
523 short-range apparent motion using random-dot kinetogram (Mikami, Newsome, and Wurtz 1986b, [a]  
524 1986) In these stimuli, motion occurs and is evenly distributed within a stationary aperture typically  
525 covering a receptive field, and motion is extracted locally through motion energy detectors (Majaj,  
526 Carandini, and Movshon 2007; Pack et al. 2006). Simple L-NL hierarchical models account very well for  
527 the selective properties of neurons in V1 and MT in response to such kind of drifting or RDK stimuli (Rust  
528 et al. 2006; Carandini et al. 2005). However, there should be intrinsic differences in the processes

529 involved in integrating local drifting motion vs global trajectory motion of a single object. Indeed,  
530 Hedges and collaborators (2011) have showed that MT receptive fields are only sensitive to local motion  
531 presented within stationary aperture, totally independent of the direction of long-range trajectory  
532 simulation in which these local motion stimuli are embedded (Hedges et al. 2011). We have very limited  
533 understanding of the processing actually required to extract motion information along a trajectory. The  
534 experiments of Watamaniuk and colleagues show that this processing cannot be simply integrated from  
535 large receptive field of downstream areas (Watamaniuk, McKee, and Grzywacz 1995). Here we suggest  
536 that the visual system can simply encodes the trajectory at mesoscopic level within retinotopic map.

537

### 538 **Encoding the motion trajectory in the retinotopic map for optimal read-out**

539 The suppressive wave we documented decreases the residual activity evoked by the first stimulus,  
540 hereby shaping the dynamic response within the retinotopic map of V1 that could be read out as motion  
541 information by a downstream area. V4 or MT neurons have receptive fields whose retinotopic size  
542 encompasses the cortical region we imaged in this study. As shown by our read-out analysis (Fig. 8),  
543 those neurons will be able to simply detect this population-encoded direction selective motion  
544 information through motion energy detectors (Adelson and Bergen 1985). This signifies that V1 intra-  
545 cortical interactions would preformat the population representation of long-range apparent motion for  
546 an optimal read-out by downstream areas (Adelson and Bergen 1985; Mumford 1991, 1992). One  
547 intriguing consequence is that encoding of motion signal at the level of the population could be  
548 operated without specific extraction of motion signal at the level of local V1 neuronal receptive fields.  
549 Indeed, neurons with non-optimal direction preference or no direction selectivity could still participate  
550 into this population response by small variations of their response that would occur at the right moment  
551 depending on their position in the retinotopic space. In other words, V1 would have the possibility to  
552 encode multiple motion signals in parallel at local and global level. These results are in accordance with

553 human fMRI experiments that showed that V1 is actively involved in the network that processes and  
554 represents the perceived illusory IrAM (Muckli et al. 2005).

555

### 556 **IrAM along ventral and dorsal streams, feedback vs horizontal propagation**

557 In the visual cortex of the ferret, it was shown using VSDI, that IrAM induces feedback propagation of  
558 differential activity from area 21 down to area 17 (Roland et al. 2006). Similarly, using stimuli that could  
559 span a much large visual scale (16.5° spatial separation) and systematically larger cortical separations, it  
560 was suggested that human MT complex feedbacks on early visual cortices to process long-range  
561 apparent motion (Wibrals et al. 2009; Vetter, Grosbras, and Muckli 2015). Areas on the ventral stream  
562 (LOC) seems to be also implicated in processing such stimuli (Zhuo et al. 2003). Ventral stream areas  
563 may actually be well suited since they will process the information about object through strong  
564 feedback interactions with V1 (Poort et al. 2012) and are as well strongly involved in motion processing  
565 (Roe et al. 2012; Ferrera, Rudolph, and Maunsell 1994). The experiment from Hedges et al. (2011)  
566 indeed suggested that MT may not be the most appropriate area, at least in non-human primates, for  
567 extracting motion along a IrAM trajectory. It is important to consider though that, in all these studies,  
568 there are important difference in the spatial and a temporal scales of the IrAM has been presented that  
569 may affect the relative weight of intra-cortical and feedback mechanisms processing this information  
570 between and within the different visual areas (see Discussion in Reynaud, Masson, and Chavane 2012).

571

### 572 **Conclusion**

573 As recently proposed by Muller et al. (Muller et al. 2018), traveling waves within and between cortical  
574 areas can provide an advantageous framework for dynamic computations that will influence neuronal  
575 processing. However, in this review, it was also noted that there is a lack of evidence for a functional  
576 role of these waves. Here we show that two discrete stimuli generating the long-range apparent motion

577 illusion, will induce multiple wave interactions resulting in propagation of suppression in a direction  
578 opposite to that of the stimuli. Such suppression shapes the stimulus and helps the visual system to  
579 keep track of the stimulus position along the motion trajectory, resulting in a precise encoding of  
580 velocity information at a very early stage of processing. We believe that our work has revealed a first  
581 elementary step in processing IrAM signals that will need further integration in downstream areas and  
582 feedback controls. Further work is therefore needed to understand which areas, if any, is reading-out  
583 the population representation of motion trajectory on V1 retinotopic map and the relative role of intra-  
584 and inter-cortical interactions.

585

## 586 **Materials and Methods**

587 The experiments were conducted on two male rhesus macaque monkeys (macaca mulatta, aged 14 and  
588 11 years old respectively for monkey WA and monkey BR) over a period of three years. The  
589 experimental protocols had been previously approved by the local Ethical Committee for Animal  
590 Research (approval A10/01/13, official national registration 71-French Ministry of Research) and all  
591 procedures complied with the French and European regulations for Animal Research as well as the  
592 Guidelines from the Society for Neuroscience.

593

594 ***Surgical preparation and VSDI protocol.*** The monkeys were chronically implanted with a head-holder  
595 and a recording chamber located above the V1 and V2 cortical areas of the right hemisphere. After full  
596 recovery, the monkeys were trained to perform foveal fixation of a small red target presented over  
597 different static and moving backgrounds for up to 2-3s, with their head fixed. Once a good fixation  
598 behavior was achieved, a third surgery was performed. The dura was removed surgically over the  
599 recording aperture (18mm diameter) and a silicon-made artificial dura was inserted under aseptic  
600 conditions to allow for a good optical access to the cortex over the whole period of weekly recordings.

601 Before each recording session conducted in awake animal, the cortical surface was stained with the  
602 Voltage Sensitive Dye (VSD) RH-1691 (Optical Imaging ©) with the following procedure: The optical  
603 chamber was open, artificial dura-mater was removed and cortical surface was cleaned under strict  
604 sterile conditions. The dye solution was prepared in artificial cerebrospinal fluid (aCSF) at a  
605 concentration of 0.2 mg/ml, and filtered through a 0.2µm filter. The recording chamber was filled with  
606 this solution and closed for three hours, corresponding to the time lapse needed for a correct cortical  
607 staining. The chamber was then rinsed thoroughly with filtered aCSF to remove any supernatant dye.  
608 Before imaging, the artificial dura was placed back in position and the chamber was closed with  
609 transparent agar and cover glass. Experimental control, data collection and eye position monitoring  
610 were performed by the ReX software (NEI-NIH) running under the QNX operating system (Hays et al.,  
611 1982). During each trial, the cortex was illuminated at 630 nm using epi-illumination and we recorded  
612 optical signals high-pass filtered at 665 nm during 999ms with a Dalstar camera (512x512 pixels  
613 resolution, frame rate of 110 Hz) driven by the Imager 3001 system (Optical Imaging ©). The beginning  
614 of both online behavioral control and image acquisition were heartbeat-triggered. The surgical  
615 preparation and VSD imaging protocol have been described elsewhere (Reynaud, Masson, and Chavane  
616 2012; Muller et al. 2014).

617

618 ***Behavioral task and visual stimulation.*** Monkeys were trained for a simple fixation task. For each  
619 experimental trial, the monkeys were required to fixate a central red dot within a precision window of  
620 1°x1°. When correct fixation was achieved, the next heartbeat, detected with a pulse oximeter (Nonin  
621 8600V), triggered the beginning of the acquisition window. A visual stimulus appeared 100 ms after this  
622 trigger after which a blank screen was presented, ending the trial. Each trial ran for 700 ms. If the  
623 monkey had maintained fixation up to the end of the acquisition period, a reward (fruit compote drop)  
624 was given. Otherwise, the trial was canceled, an alert sound was delivered and the procedure was re-

625 initiated. The visual stimuli were computed on-line using VSG2/5 libraries and were displayed on a 22"  
626 CRT monitor at a resolution of 1024x768 pixels. Refresh rate was set to 100Hz. Viewing distance was of  
627 57cm. Luminance values were linearized by mean of a look-up table. We used Gaussian blobs with  
628 standard deviation (controlling the spatial width) of 0.5°. They were presented at different positions,  
629 located at 0.5° or 2° on the left of the vertical meridian respectively for monkey WA and monkey BR, and  
630 between 1.5° and 4.5° below the horizontal meridian. We used different stimulus durations, 10 ms(1  
631 frame), 50ms or 100ms and different interstimulus intervals (ISI) for the two-stroke apparent motion  
632 stimulations (from 20 to 100 ms). All stimuli (single blobs of different durations, IrAM sequences and  
633 two blank conditions i.e. where no visual stimulus) were randomly interleaved with an inter-trial interval  
634 of 8 seconds for dye bleaching prevention.

635

636 **Data analysis.** Stacks of images were stored on hard-drives for offline analysis. The analysis was carried  
637 on with Matlab R2014a (The MathWorks Inc. ©) using the Optimization, Statistics and Signal Processing  
638 Toolboxes. VSD evoked responses to each stimulus were computed in three successive basic steps. First,  
639 the recorded value at each pixel was divided by the average value before stimulus onset ("frame 0  
640 division") to remove slow stimulus-independent fluctuations in illumination and background  
641 fluorescence levels. Second, this value was subsequently subtracted by the value obtained for the blank  
642 condition ("blank subtraction") to eliminate most of the noise due to heartbeat and respiration . Third a  
643 linear detrending of the time series was applied to remove residual slow drifts induced by dye bleaching.

644

645 **Spatio-temporal representation (ST data).** For each time frame, activity was averaged across the x-  
646 dimension within the apparent-motion trajectory (e.g. *dotted rectangle at frame 216 ms* in Fig. 1, C-G)  
647 to provide a unique spatial cortical dimension as a function of time.

648



649 **Latency estimation.** Response latency was defined as the point in time at which the signal derivative  
650 crossed a threshold set a 2.57 times (99% confidence) the SD of its baseline computed during a 100-ms-  
651 long window right before stimulus onset.

652

653 **Speed estimation.** Within the ST representation, the speed of activity propagation was estimated by  
654 computing the slope of the linear regression between each latency estimate as a function of the cortical  
655 distance in the ST representation

656

657 **Data Fitting.** For extracting the space and time constants of the VSD responses, we fitted the ST data in  
658 space (for each time frame) to a Gaussian function of the form:

659 
$$F(x) = k e^{-\frac{(x-\mu)^2}{2\sigma^2}}$$

660 where  $\sigma$ ,  $k$  and  $\mu$  respectively denote the width (as the standard deviation), the amplitude and the  
661 spatial position of the Gaussian. We use the slope of the linear regression of  $\mu(t)$  for quantifying the  
662 displacement of the response peak (see Fig. 4E).

663 In time (for each spatial point), the data was fitted to the combination of two half Gaussian functions:

664 
$$F(t) = F_{11}(t) + F_{12}(t)$$

665 
$$F_{11}(t) = k_1 e^{-\frac{(t-t_c)^2}{2\tau_{on}^2}} \cdot (t \leq t_c) \text{ and } F_{12}(t) = k_2 e^{-\frac{(t-t_c)^2}{2\tau_{off}^2}} \cdot (t > t_c)$$

666 where  $\tau_{on}$  and  $\tau_{off}$  denote the time-constants of each half Gaussian, while  $k_1$ ,  $k_2$  and  $t_c$  are respectively  
667 their peak to peak amplitudes and the time of their common center.

668

669 **Statistical Procedure.** We used a two-sample t-test procedure to test whether or not the distributions of  
670 the VSD response properties (i.e. space-constant, time-constants, latencies and cortical speed) were  
671 independent of stimulus duration or lrAM speed.  $p < 0.01$  is considered significant.

672

673 **Mean-field computational model.** We consider a spatially extended ring model where every node of the  
 674 ring represents the network activity of a large population of excitatory regular spiking (RS) and inhibitory  
 675 fast spiking (FS) cells (see Fig. 5A). We consider Adaptive Exponential integrate and fire (AdExp) neurons  
 676 evolving according to the following differential equations :

$$c_m \frac{dv}{dt} = g_L(E_L - v) + \Delta e^{\frac{v-v_{th}}{\Delta}} - w + I_{syn}$$

$$\tau_w \frac{dw}{dt} = -w + b \tau_w \sum_k \delta(t - t_k) + a(v - E_L)$$

677 where  $c_m = 100\text{pF}$  is the membrane capacity,  $v$  is the voltage of the neuron and, whenever  $v > v_{th} =$   
 678  $-50\text{mV}$  at times  $t_k$ ,  $v$  is reset to its resting value  $v_{rest} = -50\text{mV}$ . The leak term has a conductance  
 679  $g_L = 10\text{nS}$  and a reversal potential  $E_L = -65\text{mV}$ . The exponential term has a different strength for RS  
 680 and FS cells, i.e.  $\Delta = 2\text{mV}$  ( $\Delta = 0.5\text{mV}$ ) for excitatory (inhibitory) cells. Inhibitory neurons do not have  
 681 adaptation ( $a=b=0$ ) while excitatory neurons have an adaptive dynamics with  $a = 4\text{nS}$ ,  $b=40\text{ nS}$  and  
 682  $\tau_w = 500\text{ms}$ . The synaptic current can be expressed as:

$$I_{syn} = Q_E(E_E - v)S_E + Q_I(E_I - v)S_I$$

683

684 where  $S_{E/I} = \sum_{pre} \theta(t - t_{pre,E/I}) e^{-\frac{t-t_{pre,E/I}}{\tau_{E,I}}}$  is the postsynaptic current due to all presynaptic  
 685 excitatory/ Inhibitory neurons spiking at time  $\tau_{pre,E/I}$  and  $\theta$  is the Heaviside function. The reversal  
 686 potentials are  $E_E = 0\text{mV}$  and  $E_I = -80\text{mV}$ , the synaptic decays are equal for excitatory and inhibitory  
 687 cells,  $\tau_{E,I} = 5\text{ms}$ . The quantal conductances are  $Q_E = 1\text{nS}$  and  $Q_I = 5\text{nS}$ . We then consider a random  
 688 network with  $p=5\%$  of connectivity and 80% of excitatory neurons.

689 The activity of the network is simulated using a mean field model, shown capable of quantitatively  
 690 predicting the stationary activity of the network and its response to an external stimuli (Zerlaut et al.  
 691 2018). All together, the dynamical equations for the spatially extended ring model read :

$$T \frac{\partial r_E(x, t)}{\partial t} = -r_E(x, t) + F_E(r_{drive} + r_{aff}(x, t) + \int_R dy G_E(x - y) r_E(y, t - \frac{|x - y|}{v_c}), r_I)$$

$$T \frac{\partial r_I(x, t)}{\partial t} = -r_I(x, t) + F_I(r_{drive} + r_{aff}(x, t) + \int_R dy G_I(x - y) r_E(y, t - \frac{|x - y|}{v_c}), r_I)$$

692 where  $r_{E/I}(x, t)$  is the population rate of excitatory/inhibitory cells at the space-time position  $(x, t)$ ,  
 693  $r_{aff}(x, t)$  is the excitatory afferent input targeting both excitatory and inhibitory populations and  $G_{E/I}$  is  
 694 the spatial connectivity in between subpopulations that we chose as Gaussian of width  $I_{exc} = 5\text{mm}$   
 695 (excitation) and  $I_{inh} = 2.5\text{mm}$  (inhibition). Moreover,  $v_c = 300\text{mm/s}$  is the axonal conduction speed,  
 696  $r_{drive}$  an external time/space constant external drive and  $T=5\text{ms}$  is the decay time of population rate.  
 697 The functions  $F_{E,I}$  are the transfer functions of excitatory/inhibitory neurons and are calculated  
 698 according to a semi-analytical tool as in Zerlaut et al. (Zerlaut et al. 2018) through an expansion in  
 699 function of the three statistics of neurons voltage, i.e. its average  $\mu_V$ , its standard deviation  $\sigma_V$  and its  
 700 autocorrelation time  $\tau_V$ :

$$F = \frac{1}{\tau_V} \text{Erfc}\left(\frac{v_{thr}^{eff} - \mu_V}{\sigma_V}\right)$$

701 where  $\text{Erfc}$  is the error function and the effective threshold  $v_{thr}^{eff}$  is expressed as a first order expansion  
 702 with some fitting coefficients in function of  $(\mu_V, \sigma_V, \tau_V)$ . More details on this procedure can be found in  
 703 Zerlaut et al. (Zerlaut et al. 2018). The values  $(\mu_V, \sigma_V, \tau_V)$  are calculated from shot-noise theory (Daley  
 704 and Vere-Jones 2007). Introducing the following quantities:

$$\mu_{G_E} = r_E K_E \tau_E Q_E$$

$$\sigma_{G_E} = Q_E \sqrt{\frac{r_E K_E \tau_E}{2}}$$

$$\mu_{G_I} = r_I K_I \tau_I Q_I$$

$$\sigma_{G_I} = Q_I \sqrt{\frac{r_I K_I \tau_I}{2}}$$

$$\mu_G = \mu_{G_E} + \mu_{G_I} + g_L$$

$$\tau_m = \frac{C_m}{\mu_G}$$

$$U_s = \frac{Q_s}{\mu_G} (E_s - \mu_V)$$

705 where  $K_{E/I}$  is the amount synapses related to pre-synaptic excitatory/inhibitory neurons (we consider a  
 706 network of  $N=10000$  neurons inside each node of the ring), we obtain the following equations for the  
 707 voltage moments:

$$\mu_V = \frac{\mu_{G_E} E_E + \mu_{G_I} E_I + g_L E_L}{\mu_G}$$

$$\sigma_V = \sqrt{\sum_s K_s r_s \frac{(U_s \tau_s)^2}{2(\tau_m + \tau_s)}}$$

$$\tau_V = \frac{\sum_s K_s r_s (U_s \tau_s)^2}{\sum_s K_s r_s (U_s \tau_s)^2 / (\tau_m + \tau_s)}$$

708 The afferent input has the following form:

$$r_{aff}(x, t) = A \cdot \frac{1}{2\sqrt{\sigma_{inp}}} e^{-\frac{(x-x_0)^2}{\sqrt{2}\sigma_{inp}}} \cdot (H(t-t_0)e^{-\frac{(t-t_0)^2}{\sqrt{2}\tau_1}} + H(t_0-t)e^{-\frac{(t-t_0)^2}{\sqrt{2}\tau_2}})$$

709 where  $A$  is the input amplitude,  $(x_0, t_0)$  the stimulus location. And  $H$  the heaviside function. The spatial  
 710 extension of the stimuli is  $\sigma_0 = 3.5\text{mm}$ , the time rise  $\tau_1 = 15\text{ms}$  and the decay time  $\tau_2 = 90\text{ms}$ .  
 711 The time delay in between stimulus 1 and stimulus 2 is  $\Delta_t = 100\text{ms}$  (if not stated differently) and the  
 712 spatial distance  $\Delta_x = 7\text{mm}$ . The VSDI signal is calculated as follows :

$$\frac{\delta_V}{V} = \frac{\mu_V - \mu_V^0}{\mu_V^0}$$

713 where  $\mu_V^0$  is the average voltage pre-stimuli.

714

715 *CUBA model :*

716 The current based model is obtained by considering the following synaptic coupling :

$$I_{syn} = Q_E^{CU} S_E + Q_I^{CU} S_I$$

717 where  $Q_E^{CU} = 0.03pA$  and  $Q_I^{CU} = -0.15pA$  are the coupling with excitatory and inhibitory neurons . The  
 718 rest of the parameters are the same. The voltage of the neurons is calculated accordingly, i.e.

$$\mu_V = \frac{r_E K_E \tau_E Q_E^{CU} + r_I K_I \tau_I Q_I^{CU} + E_L}{G_L}$$

719 Also in this case we use the same methodology to estimate the neurons transfer function as done for  
 720 the COBA model.

721

722 *Different FS gain :*

723 In order to modify the gain of FS cells we manually change the transfer function  $F_I(r_E, r_I)$ . In practice, for  
 724 any  $r_I$  we calculate the value  $r_E^*$  for which TF changes convexity. This gives us the slope

725  $\sigma_r = \frac{dF(r_E, r_I)}{dr_E}(r_E^*, r_I)$  and the maximal value  $F_{max}$  that we estimate calculating F for very high rates

726 (typically  $r_E = 200Hz$ ). We then use the following function :

$$F_I(r_E, r_I) = 2max \cdot \frac{1}{1 + e^{-\left(\frac{r_E - r_E^*}{\sigma_r}\right)}}$$

727 where we recall that  $r_E^*$  and  $\sigma_r$  change in function of  $r_I$ . This permits us to have a sigmoidal form of the  
 728 transfer function  $F$ . In order to change its slope we use a factor  $\gamma$  that scales the slope which becomes  
 729 then  $\gamma\sigma_r$ . In Fig. 4 we use  $\gamma$  equal to 1.2 or 0.8.

730

731 **Decoding Model.** The algorithm for the decoding model used in Figures 6 and 7 is detailed here. First,

732 the ST data (i.e. space-time matrix) were whitened (i.e. spatially decorrelated and scaled) by applying a

733 ZCA transformation. The whitening matrix was computed from the eigen-decomposition of the

734 covariance matrix of the blank data. Next, the four spatial profiles (blank, stimulus 1, stimulus 2 and joint

735 stimulus 1 and 2) were computed by averaging the corresponding ST response in a 50 ms-window

736 around the time of maximum response and then normalized. The decoding of any ST data (e.g. the  
737 observed activity evoked by a 6.6 °/s two stroke apparent motion stimulus “*obs*” or its linearly predicted  
738 pattern “*pred*”) thus consisted in evaluating the likelihood that the spatial profile observed at one point  
739 in time of the data  $A(x, t)$  was best correlated with one of the four spatial profiles  $S_j$  with  $j \in \{1: 4\}$ . This  
740 comes down to calculating the four probability  $P_j(t)$  of the form:

$$P_j(t) = e^{-\frac{1}{2\sigma_j} \sum_x \left( \frac{A(x,t) - S_j(x)}{\|A(x,t)\| \|S_j(x)\|} \right)^2}$$

741 where  $\sigma_j$  is the averaged standard deviation of the residual activity between  $A(x, t)$  and  $S_j(x)$ .  
742 Then, we defined the explaining away index as the probability of detecting joint S1&S2 in the observed  
743  $P_4^{obs}$  or  $P_{s1\&s2}^{obs}$  minus the probability of detecting joint S1&S2 in the linear prediction  $P_4^{pred}$  or  $P_{s1\&s2}^{pred}$  as  
744 follows:

$$I_{E.A.} = P_{s1\&s2}^{obs} - P_{s1\&s2}^{pred}$$

745  
746  
747 **Opponent motion energy model.** . To extract motion information from the population responses, we  
748 used the opponent motion energy model developed by (Adelson and Bergen 1985). Briefly, this model  
749 consists of combining quadrature pairs of spatial and temporal filters to obtain oriented spatio-temporal  
750 filters (i.e. Gabors) tuned in spatial frequency. The ranges of spatial and temporal frequencies were  
751 chosen so that the speed (i.e. FT/FS) of the resulting ST filters varies from 2 to 70 °/s and the scale (i.e.  
752 1/FS) from 0.2 to 6 mm. It resulted in 64 (FS,FT) couples representing 8 different speeds and scales. For  
753 each couple, we obtained two filters tuned for upward motion and two filters tuned for downward  
754 motion. The outputs of quadrature pairs of such filters are then squared and summed to give a phase-  
755 independent measure of local motion energy for both directions (i.e MEu and MEd values). Lastly, the  
756 opponent motion stage computes the difference between the oriented opposite energies (i.e. OME  
757 values). Note that before applying the OME model, the ST data were first normalized and passed

758 through a non-linearity to account for the VSD to spike rate transformation as proposed by (Chen,  
759 Palmer, and Seidemann 2012):

$$760 \quad R_{\text{SU}} = k(R_{\text{VSDI}})^N$$

761 where  $R_{\text{SU}}$  and  $R_{\text{VSDI}}$  are respectively the average firing rate and the average normalized VSDI response,  $k$   
762 is a constant and  $N$  is an exponent. Here we took  $k = 10$  and  $N = 3.8$ .

763 Finally, for each ST position on the map, we could extract the velocity of the filter that generated the  
764 strongest OME and provide a ST velocity map representation (Fig. 8C-D) with velocity and amplitude as  
765 color hue and color intensity respectively. We then averaged the optimal velocity within a ST region of  
766 interest, spatially between S1 and S2's center positions and in time from 10 to 200 ms after stimulus 2  
767 onset, to report a single value of filter speed for each AM speed condition (Fig. 8D-E). The direction-  
768 selectivity index is given by:

$$769 \quad DI = \frac{V_{\text{OME}} - \min(V_{\text{OME}})}{\max(V_{\text{OME}})}$$

770 where  $V_{\text{OME}}$  is to the amplitude of the OME.

771

## 772 **Acknowledgments**

773 The authors are thankful to Guillaume Masson, Andrew Meso, Eero Simoncelli, Dirk Jancke, Yves  
774 Fregnac, Cyril Monier, Lyle Muller and Tony Movshon for fruitful discussions during different phases of  
775 this work. They are also grateful to Marc Martin, Frédéric Barthélemy, Ivan Balansard and Luc Renaud  
776 for their assistance regarding experiments.

777 The authors acknowledge funding from the European Community (FET grants FACETS FP6-015879 and  
778 BrainScaleS FP7-269921), from la Fondation de l'œil (IA) and from the French National Research Agency  
779 (ANR Trajectory, ANR-15-CE37-0011-01, and ANR Horizontal V1, ANR-17-CE37-0006-02).

780

## 781 **Competing interests**

782 The authors declare no competing interests.

783

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