Vectashield quenches Alexa Fluor 647 fluorescence, but does not hinder dSTORM super-resolution
imaging

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Abstract

The right choice of mounting medium is crucial for optimal microscopy. Different techniques require

different mounting media. It was recently reported that Vectashield, one of the most commonly used

media for conventional fluorescence microscopy, can also be used for super-resolution dSTORM

(direct stochastic optical reconstruction microscopy) imaging of Alexa Fluor 647 (AF647). This is

important because dSTORM usually requires self-made imaging buffers. As self-made buffers can

introduce a lot of variation, using an off-the-shelf commercial imaging medium, such as Vectashield,

brings more reproducibility. However, while testing its compatibility with dSTORM imaging of

neurofilament light chain (NfL), we noticed an unexpected loss of AF647 fluorescence in Vectashield.

We saw almost completely dark images and we thought that our immunolabeling did not work.

However, as we discovered, dark AF647 samples have nothing to do with failed immunolabelings.

Instead, the AF647 dye molecules are simply quenched. Initial intensity measured in Phosphate

Buffered Saline (PBS) drops to about 15% in Vectashield. This loss of fluorescence means that

Vectashield is not compatible with conventional fluorescence microscopy of AF647. However,

although we can hardly recognize labeled cells in conventional microscopy, we can still perform 3D

dSTORM super-resolution microscopy in these quenched, dark cells.

Introduction

Super-resolution microscopy (SRM) requires bright, densely labeled samples. Typical experiments start with dyes in a fluorescent state. This is necessary for the identification of labeled cells. A subsequent requirement for one type of SRM, dSTORM (direct stochastic optical reconstruction microscopy), is to get dye molecules to blink. Blinking separates individual fluorescent molecules in time and space. This enables their precise localization, which is necessary to reconstruct super-resolution diffraction-unlimited images[1,2]. In order to make them blink, dye molecules are switched to a dark state from which they stochastically and spontaneously recover to a fluorescent state, multiple times before bleaching. This can be achieved by special chemicals, such as thiol-containing reducing agents with or without enzymatic oxygen scavenger systems (e.g. GLOX buffer containing glucose oxidase and catalase)[3,4]. It was recently reported that Vectashield, a commercial mounting medium, can also be used for dSTORM imaging of certain dyes, such as Alexa Fluor 647 (AF647)[5]. This finding has high practical implications since AF647 is the most widely used dye for dSTORM and Vectashield is one of the most commonly used commercial mounting media.

Results and discussion

In comparison with self-made buffers, commercially available Vectashield represents a very convenient and affordable choice for dSTORM imaging medium. The fact that it can be used off-the-shelfis especially important for demanding techniques such as dSTORM. Using the same imaging medium brings more reproducibility and allows for more comparable results within and between different laboratories. However, when we tried to use it for the imaging of neurofilament light chain (NfL), we noticed an unexpected loss of AF647 fluorescence in Vectashield compared to phosphate-buffered saline (PBS) (Fig. 1a, Supplementary Fig. 1). This is specific to AF647, as we do not see it with Alexa Fluor 488 (AF488; Fig. 1b, Supplementary Fig. 1). It is also independent of the applied microscopy technique since we see it with confocal microscopy as well (data not shown). To quantify observed fluorescence intensity changes we transfected the cells with a plasmid containing nuclear

localization sequence (NLS)-mCherry fusion protein (Fig. 2a). We chose to use NLS-mCherry for

intensity measurements for multiple reasons. Firstly, it is uniformly distributed within the nucleus,

and can be easily labeled with the same primary antibody, followed by either AF488- or AF647-

conjugated secondary antibody. Additionally, mCherry gives a bright fluorescent signal in 561

channel that is not affected by any of the imaging media. This can be used for reliable identification

of labeled regions of interest and intensity measurements of AF647 and AF488 before and after

imaging media change (Fig. 2b; Supplementary Fig. 2; see material and methods for image acquisition

and analysis details). A quantitative analysis shows there is an intensity drop to about 15 % of the

initial value for AF647, and no loss of intensity for AF488 (Fig. 2d). Albeit not quantified before, this is

in accordance with previously published work suggesting that Vectashield is not optimal for storing of

AF647-labeled samples[6]. We first thought that our immunocytochemistry labeling with primary and

secondary antibodies might not be stable. That is why we tested different types of AF647 stainings.

We observed that the loss of fluorescence is not specific to our AF647-conjugated secondary

antibody. We also see it for the cells labeled with an AF647-conjugated primary antibody (Fig. 3) or

AF647-phalloidin (Supplementary Fig. 3). However, AF647 quenching is more or less noticeable when

looking at different cellular structures, probably depending on the starting labeling intensity. For

example, tubulin immunocytochemistry still shows relatively nicely labeled cells in Vectashield (Fig.

3a). Without seeing the image in PBS (before the addition of Vectashield), one might not even realize

that there was quenching. That might be a reason why the AF647 quenching has not been reported

before. On the other hand, even when we adjusted the image display (brightness/contrast) to show

very dim pixel values (auto scale lookup table; Fig. 1c, inset), NfL shows hardly any signal and the

labeling quality seems to be very poor. However, to our surprise, even with such "dark" NfL samples,

it is still possible to do dSTORM. Although we can hardly identify positively labeled cells in

Vectashield, we can still see blinking, perform 3D dSTORM imaging and even obtain SRM images with

a resolution of less than 40 nm (Fig. 1c), as estimated by Fourier ring correlation[7]. However, this was

only made possible by identifying the labeled cell in PBS before adding Vectashield, i.e. before the

image turned dark. Otherwise, it is not possible to tell apart background from a labeled cell. In

addition to checking the cells in PBS first, and then switching to Vectashield for dSTORM, an

alternative would be to use 25% Vectashield (Fig. 2d). It was previously reported that using 25%

Vectashield in Tris-glycerol helps with reducing Vectashield's autofluorescent background[5]. Our

quantitative analysis shows that 25% Vectashield does not induce quenching of AF647, similar to

GLOX (Fig. 2d). In the context of SRM imaging, this is very important, since it not only allows us to

identify labeled cells, but also to evaluate the labeling quality, which is a prerequisite for successful

dSTORM. While trying to understand the mechanism behind the quenching, we came across reports

on Vectashield inducing cleavage of cyanine dyes and their derivatives (especially Cy2). We thought

that this might be happening with AF647. We tested this hypothesis in a recovery experiment where

we washed away Vectashield and after some time imaged the cells again in PBS. A quantitative

analysis shows that the loss of AF647 is reversible since it can be partially recovered (Fig. 2c, d; see

material and methods for analysis details). The recovery would not have been possible if the dye was

cleaved. In summary, we show that Vectashield induces quenching of AF647. On the contrary, AF488

fluorescence is increased in both pure and 25% Vectashield (respectively to 125 % and 185 % of the

initial PBS values). Our findings have important consequences for any type of fluorescence

microscopy. AF647 in Vectashield is not compatible with conventional fluorescence microscopy,

because it gets quenched. This is especially of relevance for immunohistochemical stainings since

Vectashield is used very commonly to mount tissue sections. Surprisingly, Vectashield-induced

quenching does not hinder at least one type of microscopy, i.e. dSTORM. However, without knowing

this, non-labeled and quenched cells cannot be distinguished. This would result in scientists not even

trying to perform dSTORM, which would be wrong, considering the high quality of dSTORM images

that can be achieved with Vectashield. Even though we only looked at AF647 and AF488 in this

manuscript, similar changes might be happening with other fluorophores, other mounting media or

other dSTORM imaging buffers. That is why for any type of labeling, we would recommend to always

first check the cells in buffers such as PBS. That is the only way to distinguish between failed

immunocytochemistry/immunohistochemistry stainings and unexpected fluorescence quenching

phenomena.

Figures

Figure 1. Vectashield (VS) quenches AF647 fluorescence, but does not hinder dSTORM super-resolution imaging.

ND7/23 cells were labeled with anti-NfL antibody, followed by AF647-(a,c) or AF488-conjugated secondary

antibody (b). Cells were first imaged with widefield illumination in PBS (a-b, left), then in Vectashield (a-b, right).

After replacing PBS with Vectashield, there is a significant drop in AF647 fluorescence intensity. Boxed regions

(a) show the location of the same cell. Brightness and contrast are linearly adjusted to show the same display

range, so that the effects of two imaging media can be compared. Even with 647 laser illumination and auto

scale look up table (c, inset), one can hardly recognize the original cell. However, despite AF647 being quenched,

the cell can still be successfully imaged with 3D dSTORM (c). The z positions in the 3D dSTORM image are color-

coded according to the height map shown on right. In contrast to AF647, after replacing PBS with Vectashield,

there is no change in AF488 fluorescence intensity (b). Scale bars: 20 µm (a,b), 5 µm (c).

Figure 2. Quantification of intensity changes for AF647 and AF488 in different imaging media. Quantification

was done on ND7/23 cells expressing NLS-mCherry (a) and labeled with anti-tRFP primary antibody, followed

by AF647- or AF488- conjugated secondary antibody. Example images for AF647 are shown in a-c. Cells were

first imaged in PBS, then in Vectashield (PBS→VS, b). Afterwards, Vectashield was replaced with PBS, cells were

washed and imaged 2.5 h later in PBS (VS→PBS, c). After medium change from PBS to Vectashield (AF647

after), there is a significant drop in the AF647 fluorescence intensity that is partially recovered after washing

(AF647 recovery). Additional examples for both AF647 and AF488 are shown in Supplementary Figure 2. Dot

plots in panel d show results of intensity change quantification in different imaging media (PBS, VS, 25%VS,

GLOX) for AF647 (magenta) and AF488 (cyan). In each case, cells were first imaged in PBS (before), followed by

medium change (after). Average fluorescence intensity values of all images from 3 experiments (20 images per

medium were analyzed in each experiment) are shown in the dot plot, including mean, and the standard error

of the mean. Post-hoc Bonferroni comparisons (more details in material and methods) show that in all 3

experiments there is a significant decrease of AF647 intensity after changing the medium from PBS to

Vectashield (PBS→VS; $p<0.05$), as well as significant increase after washing (VS→PBS: recovery; $p<0.05$). For

AF488, there is a significant increase of intensity in VS and 25%VS (PBS→VS, $p<0.05$; PBS→25% VS, $p<0.05$). For

135   both AF488 and AF647 there is no significant intensity change after switching the imaging medium from PBS to

136   GLOX or in control condition (PBS to PBS media change). Average intensity (X-axis) is shown on a logarithmic

137   scale. Scale bar: 20 µm (a-c).

138
Figure 3. Vectashield effect on AF647- vs. AF488-labeled microtubules. ND7/23 cells labeled with AF647- (a) or

AF488-conjugated (b) anti-Tubulin β3 (TUBB3) antibody. Cells were first imaged in PBS (upper panels).

Afterwards, PBS was replaced with Vectashield (lower panels). As shown in the panel (a), after replacing PBS

with Vectashield, there is a drop in the AF647 fluorescence intensity. Please note that left and middle panels in

(a) show the same images for which brightness and contrast levels were adjusted differently in order to make

the quenched AF647 signal in Vectashield visible. In contrast to AF647, Vectashield does not quench AF488

fluorescence (b). Scale bar: 20 μm (a,b).

  Supplementary Figures

148
Supplementary Figure 1. Control experiments with PBS to PBS media change (PBS→PBS) show no effect on

fluorescence intensity of AF647- (a) and AF488- (b) labeled neurofilaments. ND7/23 cells labeled with anti-NfL

primary antibody, followed by AF647- or AF488-conjugated secondary antibody. Cells were first imaged in PBS

(left panels). Afterwards, PBS was replaced with PBS (right panels). In both cases, medium change does not

affect fluorescence intensity. Please note that some cells get washed away during medium change – they

cannot be identified in the image after medium change, and are marked with yellow arrows. In both a and b,

brightness and contrast are linearly adjusted to show the same display range for images taken before and after

media change. Scale bar: 20 μm (a,b).

157
Supplementary Figure 2. Additional examples of images used for quantification of intensity changes for AF647

(a,b) and AF488 (c,d). As in Figure 2, cells were first imaged in PBS. Afterwards, PBS was replaced with PBS

(PBS→PBS) or Vectashield (PBS→VS). Left panels show images before medium change and middle panels show

images after medium change. In control condition (PBS→PBS, a) there is no difference in AF647 intensity, while

in Vectashield (PBS→VS, b) there is a significant drop in the AF647 signal. In contrast to AF647, Vectashield

does not quench AF488 fluorescence (c,d). Right panels show corresponding mCherry channel images after

medium change. Scale bar: 20 μm (a-d).

Supplementary Figure 3. Comparison of PBS vs. Vectashield effect on AF647-phalloidin. ND7/23 cells were labeled with AF647 phalloidin. Cells were first imaged in PBS. Afterwards, PBS was replaced with PBS (PBS→PBS, a) or Vectashield (PBS→VS, b). Left panels show images before medium change and right panels show images after medium change. In PBS (a) there is no difference in AF647 intensity, while in Vectashield (b) there is a drop in the AF647 signal. Scale bar: 20 µm (a,b).

Material and Methods

Cell culture

Mouse neuroblastoma x rat neuron hybrid ND7/23 cells (ECACC 92090903, obtained from Sigma Aldrich) were grown in high glucose Dulbecco's Modified Eagle Medium (DMEM; Thermo Fisher Scientific, cat. no. 41965062) supplemented with 10 % heat-inactivated fetal bovine serum (FBS; Thermo Fisher Scientific, cat. no. 10270106), 1 % penicillin-streptomycin (Sigma Aldrich, cat. no. P0781), 1 % sodium pyruvate (Thermo Fisher Scientific, cat. no. 11360039) and 1 % L-glutamine (Thermo Fisher Scientific, cat. no. 25030024) at 37 °C, 5 % CO_2. FBS was heat-inactivated by incubation at 56 °C for 30 minutes. Cells were passaged every 2-3 days up to passage 18-20 and were not differentiated.

For all the experiments, cells were seeded on a four-well Lab-Tek II chambered #1.5 German coverglass (Thermo Fisher Scientific, cat. no. 155382), 70,000 cells per well. Lab-Teks were coated with poly-D-lysine (Sigma Aldrich, cat. no. P6407) diluted in ddH2O at a 1 μg/ml concentration, and incubated at least 4 h at room temperature (RT). Before seeding wells were washed twice with Dulbecco's phosphate-buffered saline (DPBS; Thermo Fisher Scientific, cat. no. 14190169) or ddH$_2$O and left in the hood to dry completely.

Constructs and cloning

NLS (nuclear localization sequence)-mCherry construct was made by inserting NLS-mCherry sequence into a commercially available pcDNA^{TM}3.1/Zeo$^{(+)}$mammalian expression vector (Invitrogen). NLS sequence was added upstream of the mCherry gene (gift from Edward Lemke's laboratory, EMBL, Heidelberg) by polymerase chain reaction (PCR). The following primers were used for cloning: 5'-GCTGGCGCTAGCACCATG**CCGCCGAAAAAAAAACGCAAAGTGGAAGATAGC**GTGAGCAAGGGCGAGGAGG -3' (forward primer with NheI restriction site; NLS sequence is shown in bold) and 5'-

194 CGCGCAGCGGCCGCTCACTTGTACAGCTCGTCCATGCCG-3' (reverse primer with NotI restriction site).

195 Generated plasmid sequence was confirmed by sequencing.

Transfections (for AF647 and AF488 intensity measurements)

197 For Alexa Fluor 647 (AF647) and Alexa Fluor 488 (AF488) intensity measurement experiments,

198 ND7/23 cells were transfected with NLS-mCherry plasmid. Cells were transfected using JetPrime

199 (Polyplus-transfection, cat. no. 114-15) one day after seeding, at 80-85 % confluence, according to

200 the manufacturer´s instructions. On the following day, NLS-mCherry expression was confirmed on an

201 epifluorescent inverted microscope (Olympus CKX41) and immunostaining was started.

Immunocytochemistry stainings

For immunostaining of NLS-mCherry, cells were washed briefly with 0.01 M phosphate-buffered

saline (PBS; 137 mM NaCl, 10 mM Na_2HPO_4, 1.8 mM KH_2PO_4, 2.7 mM KCl, pH 7.4) and fixed with 2 %

paraformaldehyde (PFA; Sigma Aldrich, cat. no. 158127) in PBS for 10 min at RT. After fixation, cells

were briefly washed 3 times, blocked and permeabilized with 10 % goat serum (GS; Thermo Fisher

Scientific, cat. no. 16210064)/0.5 % Triton X-100/PBS (Sigma Aldrich, cat. no. X100) for 1 h. NLS-

mCherry was stained with rabbit anti-tRFP (turbo red fluorescent protein) antibody (Evrogene, cat.

no. AB233) diluted 1:500 in 5 % GS/0.1 % Triton X-100/PBS. The cells were incubated with primary

antibody at least 18 h at 4 °C. On the following day, cells were washed 3 times (5 minutes each wash)

and incubated with secondary goat anti-rabbit antibody conjugated with either AF647 (Thermo

Fisher Scientific, cat. no. A-21245) or AF488 (Thermo Fisher Scientific, cat. no. A-11034) for 1 h at RT.

Secondary antibodies were diluted 1:500 in 5 % GS/0.1 % Triton X-100/PBS. After incubation with the

secondary antibody, cells were washed 3 times (5 minutes each wash) and incubated in PBS until

imaging. All the washing steps were performed with PBS. Imaging was performed on the same or

following day.

For immunostaining of neurofilament light chain (NfL), cells were rinsed briefly with Tris-buffered

saline (TBS; 20 mM Tris, 150 mM NaCl, pH 7.6) and then fixed with 2 % PFA for 15 minutes at RT.

After fixation, cells were washed three times (5 minutes each wash) with TBS and blocked in

3 % GS/0.3 % Triton X-100/TBS for 40 minutes at RT. Cells were incubated with mouse anti-

neurofilament 70 kDa antibody, clone DA2 (Merck Millipore, cat. no. MAB1615) diluted 1:250 in

1 % GS/0.3 % Triton X-100/TBS for 2.5 h at RT, followed by overnight incubation at 4 °C. On the

following day, cells were washed 3 times (5 minutes each wash) with TBS, and incubated with goat

anti-mouse secondary antibodies conjugated with AF647 Plus (Thermo Fisher Scientific, cat. no.

A32728) or AF488 Plus (Thermo Fisher Scientific, cat. no. A32723) for 1 h at RT. Secondary antibodies

were diluted 1:500 in 1 % GS/0.3 % Triton X-100/TBS. Afterwards, cells were washed 3 times (5

minutes each wash) with TBS. TBS was used instead of PBS for this immunostaining because of

potential influence of PBS on phosphorylated neurofilaments. Only before imaging, TBS was replaced

with PBS. Imaging was performed on the same day.

For actin labeling with phalloidin AF647, cells were rinsed briefly with PBS and fixed with 2 % PFA, for

15 minutes at RT. After fixation, cells were washed 3 times briefly with PBS and blocked 1.5 h at RT in

5 % bovine serum albumin (BSA; Sigma Aldrich, cat. no. A9647) diluted in 0.3 % Triton X-100/PBS.

After blocking, cells were incubated with 0.25 µM AF647 phalloidin (Thermo Fisher Scientific, cat. no.

A22287) diluted in PBS, ON at 4 °C. On the following day, cells were incubated in AF647 phalloidin for

additional 4 h at RT and subsequently washed 3 times (5 minutes each wash) with PBS. Imaging was

performed on the same day.

For tubulin labeling cells were fixed as described previously[5]. Briefly, the cells were first washed with

PBS and extracted in 0.5 % Triton X-100 diluted in microtubule stabilization buffer (MTSB; 80 mM

PIPES, 1 mM $MgCl_2$, 5 mM EGTA, pH 6.8) for 10 seconds. Cells were washed once briefly with PBS,

and fixed in -20 °C methanol for 10 minutes at -20 °C. Afterwards, cells were washed 3 times (10

minutes each wash) and blocked for 1 h at RT in 5 % BSA/PBS. Cells were incubated with AF647 anti-

Tubulin β3 (TUBB3) antibody (BioLegend, cat. no. 801210) or AF488 anti-Tubulin β3 (TUBB3) antibody

(BioLegend, cat. no. 801203) diluted 1:100 in 5 % BSA/PBS, 3 h at RT. Afterwards, cells were washed

3 times (5 minutes each wash) with PBS and imaged on the same day. All washing, incubation and

blocking steps were performed on the shaker.

Microscope configuration

Widefield epifluorescence and 3D dSTORM imaging were performed on an N-STORM 4.0 microscope

from Nikon Instruments. More specifically, this is an inverted Nikon Eclipse Ti2-E microscope (Nikon

Instruments), equipped with XY-motorized stage, Perfect Focus System, an oil-immersion objective

(HP Apo TIRF 100×H, NA 1.49, Oil) and N-STORM module. Setup was controlled by NIS-Elements AR

software (Nikon Instruments). Fluorescent light was filtered through following filter cubes: 488 (AHF;

EX 482/18; DM R488; BA 525/45), 561 (AHF; EX 561/14; DM R561; BA 609/54) and Cy5 (AHF; EX

628/40; DM660; BA 692/40). Filtered emitted light was imaged with ORCA-Flash 4.0 sCMOS camera

(Hamamatsu Photonics). For epifluorescent widefield imaging, fluorescent lamp (Lumencor Sola SE II)

was used as a light source. For 3D dSTORM imaging of neurofilaments, 647 nm laser (LU-NV Series

Laser Unit) was used and cylindrical lens was introduced in the light path[8].

Imaging of tRFP labeled cells (for AF647 and AF488 intensity measurements)

tRFP labeled cells were first briefly checked in PBS using brightfield illumination. For each well in the

Lab-Tek we did following: picked randomly 30 fields of view (stage positions) using brightfield

illumination, saved xyz coordinates of each field of view in NIS-Elements AR software and acquired

images automatically by using NIS-Elements ND multipoint acquisition module, which allowed us to

go to the same position each time. The images were acquired in widefield mode, with 10 ms

exposure time, 1024x1024 pixels frame size and 16-bit image depth. To provide that the cells were

always properly focused, we used an autofocusing function of ND multipoint acquisition module.

Imaging was done first in PBS, using 561 (mCherry channel) and either 488 (AF488 channel) or Cy5

(AF647 channel) filter cube, depending on the labeling condition. Excitation light intensity for

mCherry and AF647 channels was 10 % and for AF488 channel 5 %. Afterwards, PBS was replaced

with one of the following imaging media: PBS, 100 % Vectashield (VS; Biozol, cat. no. VEC-H-1000),

25 % Vectashield or GLOX. We made 25 % Vectashield by mixing VS with Tris-Glycerol in 1:4 v/v ratio.

Tris-glycerol was obtained by adding 5 % v/v 1 M Tris, pH 8 to glycerol (Sigma Aldrich, cat.

no. G2025). For preparation of GLOX buffer, we used Buffer A (10 mM Tris, pH 8, 50 mM NaCl),

Buffer B (50 mM Tris, pH 8, 10 mM NaCl) and GLOX solution. GLOX solution was made by mixing 14

mg glucose oxidase (Sigma Aldrich, cat. no. G2133), 50 µl catalase (17 mg/ml; Sigma Aldrich, cat. no.

C3155) and 200 µl Buffer A. Aliquots of GLOX solution were kept at -20 °C. GLOX buffer was prepared

fresh, prior to use by mixing 7 µl GLOX solution with 690 µl Buffer B containing 10 % w/v glucose

(Sigma Aldrich, cat. no. D9559) on ice. For AF647 recovery experiments, 100 % Vectashield was

removed and cells were washed twice with PBS. After 2.5 h, cells were washed one more time with

PBS and imaging was repeated. To provide enough data for analysis each experiment was repeated

at least three times for AF488 labeled cells and AF647 labeled cells.

Imaging of actin (phalloidin) and tubulin labeled cells

Phalloidin AF647 labeled cells were first checked in PBS, using fluorescent light source (Lumencor

Sola SE II) and Cy5 filter cube with 10 ms exposure time and 5 % excitation light intensity. Up to 40

fields of view (positions) per well were picked and xyz coordinates of each field of view were saved in

NIS-Elements AR software. Widefield image acquisition was then performed automatically by using

NIS-Elements ND multipoint acquisition module at 30 ms exposure time and 10 % of fluorescent light

source. Both, brightfield and fluorescence images were acquired. Afterwards, PBS was replaced with

Vectashield, left 2 minutes to completely cover the sample and acquisition was repeated. Upon the

addition of Vectashield we noticed a change in focus, so before acquiring images in Vectashield,

every field of view needed to be manually refocused. During the imaging, autoscaling look-up table

(LUT) was on, which allowed us to see what would approximately be the correct focus plane, despite

the quenching of fluorescent signal.

Tubulin AF647 or AF488 labeled cells were imaged by following the same procedure as described

above, using Cy5 filter cube (AF647) or 488 filter cube (AF488).

3D dSTORM imaging of NfL

3D dSTORM (direct stochastic optical reconstruction microscopy) imaging was performed by using the N-STORM module of Nikon microscope described above. For imaging, oil-immersion objective (HP Apo TIRF 100×H, NA 1.49, Oil) and 647 nm laser (LU-NV Series Laser Unit) were used. Fluorescent light was filtered through a Cy5 filter cube. Filtered emitted light was imaged with ORCA-Flash 4.0 sCMOS camera (Hamamatsu Photonics) with cylindrical lens introduced in the light path[8].

Fluorescent and brightfield images of NfL labeled cells in PBS and Vectashield were acquired following the same procedure that was used for imaging of phalloidin AF647 labeled cells, using fluorescent light source and Cy5 filter cube. After widefield acquisition, selected fields of view were imaged with 3D dSTORM. Imaging was performed in total internal reflection fluorescence (TIRF) or highly inclined and laminated sheet microscopy (HiLo) mode with continuous 647 nm laser illumination (full power). Frame size was 256x256 pixels and image depth 16-bit. For each 3D dSTORM image, 30,000 frames were acquired at 33 Hz.

Calibration of 3D dSTORM was done previously using TetraSpeck Microspheres (Thermo Fisher Scientific, cat. no. T7279) following NIS-Elements' instructions. 3D dSTORM image processing was performed in NIS-Elements AR software. Molecule identification settings were set to defaults for 3D dSTORM analysis: minimum width 200 nm, maximum width 700 nm, initial fit width 300 nm, max axial ratio 2.5 and max displacement 1. Minimum height for peak detection was set to 200, and localization analysis was performed with overlapping peaks algorithm. Resulting molecule lists were exported as text files and analyzed by Fourier ring correlation (FRC)[7] to determine the image resolution. Based on FRC resolution estimate (35-40 nm), we reconstructed 3D dSTORM images with Gaussian rendering size of 15 nm in NIS Elements AR. Brightness and contrast were adjusted with Gaussian rendering intensity and height map with color coded molecule height (z location) was added. Final 3D dSTORM image was then exported as a tiff image. Z rejected molecules were excluded from resolution analysis and from final images.

Image analysis and intensity measurements

Intensity measurements for quantitative analysis of AF647 and AF488 were done in Fiji/ImageJ[9]. Images in ND2 format were opened using Bio-Formats plugin[10] and converted to tiff before the analysis. Original bit depth (16-bit) was used for analysis. For presentation purposes, brightness and contrast of 16-bit images were linearly adjusted in Fiji, images were converted to 8-bit and imported in Adobe Illustrator.

In all of our experiments (except recovery of AF647) each field of view was imaged two times: in 561 (mCherry) and either 647 (AF647) or 488 (AF488) channel, before and after medium change. As result, for each field of view we had four fluorescent pictures, mCherry and AF647(or AF488) before and after medium change. In AF647 fluorescence recovery experiments each field of view was imaged three times: in mCherry and AF647 channel, before medium change, after changing to Vectashield and after washing in PBS. Consequently, for each field of view in recovery experiments we had six fluorescent pictures, mCherry and AF647 before medium change, in Vectashield and after washing in PBS.

For the purpose of analysis, we made a macro that allowed us to stack and align all images of each field of view and perform the intensity measurements in same regions of interest (ROIs). Images from mCherry channel were used for alignment and thresholding, while intensity measurements were done in images from AF647 and AF488 channels, respectively.

Macro was designed to open and stack images from mCherry channel, align them using MultiStackReg (developed by Brad Busse http://bradbusse.net/sciencedownloads.html) and TurboReg plugin[11], and save the alignment information in a form of transformation matrices. After that, macro was opening and stacking images from AF647 channel. AF647 images were aligned using transformation matrices that were saved after alignment of mCherry images. This way we ensured that images from 647 channel would be properly aligned even in the case when one of them has very

low intensity (e.g. images taken in Vectashield). After alignment both mCherry and AF647 image

stacks were cropped to exclude empty space. Same procedure was done for AF488 images.

Region of interest for intensity measurements was created by thresholding in mCherry image stack,

using Otsu Dark thresholding algorithm. Thresholding was performed in the image that was taken

after medium change to exclude cells that were washed away during the change of imaging media.

Resulting ROI contained fluorescently labeled nuclei and we refer to it as nuclear ROI. At this point,

user intervention was required, to choose ROI that contains no cells, only background noise

(background ROI). Afterwards, intensity measurements (mean intensity and integrated density) of

nuclear and background ROIs were performed in AF647 and AF488 stacks, respectively.

As a result of analysis, macro saved intensity measurement results (in a form of a text file), mCherry

before/after image stacks, AF488 or AF647 before/after image stacks and nuclear ROIs.

Oversaturated images, poorly aligned images and images where all cells were washed away during

imaging media change were excluded from further analysis.

Text files with intensity measurement results were imported in Excel and corrected total cell

fluorescence (CTCF) was calculated.

CTCF = Integrated Density of nuclear ROI − (area of nuclear ROI x mean fluorescence of the

background)

In addition to CTCF, we calculated average fluorescence by dividing CTCF with the area of nuclear

ROI. Calculated values were exported to a separate Excel file for statistical analysis.

Statistical analysis

Statistical analyses (ANOVA and post-hoc analyses) were carried out with IBM SPSS Statistics Version

25, Armonk, New York, USA. The power analysis to determine the optimal sample size was carried

out with the Statistical Tree Power Calculator, QFAB (Queensland Facility for Advanced

Bioinformatics), Brisbane, Australia.

Preparation of data analysis based on pilot work

The dependent variable was the difference (delta) between the fluorescence intensities before and after media change, where the starting medium is always PBS and the change is represented by removing PBS and adding another medium (delta intensity = (intensity PBS – intensity new medium)). Based on prior assumptions, this difference will become minimal in the control condition, where PBS is first removed and the added new medium is again PBS. If another medium is added, delta will be larger and take on an either positive or negative value, depending on whether the intensity in the new medium is smaller or larger than the intensity of PBS.

The dependent variable (delta intensity) delivers continuous values and is on interval scale level, which is a prerequisite to carry out an analysis of variance (ANOVA). The independent variables (factors) were different dyes (AF647 and AF488), different imaging media (PBS, Vectashield, 25% Vectashield, GLOX) and different experiments (1, 2 and 3).

Power calculations, randomization and design

Prior to the actual experiments, it was necessary to carry out power calculations to specify the optimal sample size. These analyses needed to take into account multiple analyses, including the different experiments and post-hoc comparisons. Our main focus was to compare delta intensities between different imaging media applying ANOVA. Our defined type 1 error level was 0.05 (including two sided testing for post-hoc, planned comparisons). We aimed for a power of 0.95 (which equals a type 2 error level of 0.05). Based on pilot work, we had estimated to find at least an effect size between 0.45 and 0.5 and more realistic an effect size between 0.8 and 0.9. For the lowest effect of 0.45 we would need 23 measurements per condition, for the large effect size of 0.9 we would only need 7 measurements per group to reach the pre-specified power of 0.95. To fulfil the assumptions of ANOVA and post-hoc tests in terms of required distributions, we decided for 20 measurements per condition, which lies within the range of 7 to 23 measurements. We decided in favor of a value at the upper limit of this range because the smaller the sample size, the more likely are violations to the

assumptions of parametric tests such as ANOVA. We did not go beyond this range, though, to avoid

having over-powered statistical tests, where tiniest differences would become statistically significant.

In our pilot work, we also realized that if images are taken truly at random, a minority of the images

could not be measured because no cells appeared after changing media (they got washed away), or

some of the images were oversaturated. Because randomization was an absolute requirement for

our statistical tests, we needed to have a bigger number than 20 images randomly taken to get a

total of 20 measurements. To be safe, we decided a priori that 30 images are taken at random and

the first 20 valid images (i.e. those that contained cells before and after media change and that did

not contain oversaturated pixels) were included in the analysis. The remaining images were not

considered in the analysis. This resulted in the following design:

In each experiment, 20 delta intensities were measured for all 4 different imaging media (20 * 4 =

80). Because they were measured for both dyes, AF647 and AF488, there were 160 delta intensities

(80 * 2) per experiment. Because we carried out 3 experiments, there were 480 delta intensities in

total (160 * 3).

As a result, there was a 2 (dye) * 4 (imaging media) * 3 (experiment) ANOVA on delta intensities.

Following our a priori assumptions, we assumed the two dyes would deliver different delta

intensities. In addition, we assumed the 4 imaging media would differ in terms of their delta

intensities. Because each experiment took place on a different day with new cells (that were freshly

transfected and labeled, etc.), we also expected that the 3 experiments would differ in terms of their

delta intensities. In case the 3 experiments indeed differ, different ANOVAs are necessary for each

experiment separately, in order to show that the differences between the imaging media point in the

same direction and the same post-hoc comparisons are significant in each individual experiment. In

these individual ANOVAs, the delta intensities for all imaging media are directly compared to each

other for each experiment separately and for each dye separately. Planned post-hoc comparisons

(Bonferroni) are subsequently carried out to demonstrate that all post-hoc analyses show the same

type of significant differences between the compared imaging media. These planned comparisons

correct the significance levels for multiple tests, i.e. they avoid an accumulation of statistical error

which would otherwise occur if multiple significance tests were carried out. To give us maximum

trust in our results, we chose the strictest of all post-hoc comparisons, which is the Bonferroni

correction. Bonferroni delivers the most conservative results, i.e. the least likely to become

statistically significant.

Deriving hypotheses based on prior observations

Based on pilot experiments, our primary focus was dye AF647, because only in AF647 we noticed an

intensity drop in image medium Vectashield compared to PBS. We expected that this drop was

shown in all 3 experiments. We did not expect such a drop for dye AF488. We do, however, also

expect intensity changes on other imaging media for dye AF488. Based on pilot work, we expected

medium sized effects relating to a delta intensity increase for Vectashield and 25 % Vectashield. If

this increase is robust, it should appear in all three experiments.This also requires planned post-hoc

comparisons (Bonferroni), to demonstrate that the significant differences between the compared

imaging media are the same for all 3 experiments.

Based on pilot data, we had yet another hypothesis. We realized an intensity drop seen for dye

AF647 after adding Vectashield and found out that the intensity will recover after washing. This

would be in contrast to the previously assumed dye cleavage effect, where no recovery would be

expected. In order to test whether the AF647 intensity drop seen in Vectashield can actually recover,

we carried out a repeated measurement ANOVA. In this ANOVA, we compared 3 intensities (1. at PBS

baseline, 2. after removing PBS and adding Vectashield, 3. after replacing Vectashield with PBS and

waiting 2.5 hours in PBS imaging medium).

Data analyses

In a first step, we carried out a 2 (dye) * 4 (imaging media) * 3 (experiment) ANOVA with the

dependent variable delta intensities. There was a significant main effect for dye, $F(1, 456)=819.14$,

$p<0.001$, effect size partial $\eta^2=0.64$, Mean AF647=3596.45, Mean AF488=-2569.74,

SE(Means)=152.34. Similarly, there was a significant main effect for imaging media, $F_{(3, 456)}$=424.15,

$p<0.001$, effect size partial η^2=0.74, Mean PBS=420.74, Mean Vectashield=6239.29, Mean_25%

Vectashield=-4583.83, Mean GLOX=-22.79, SE(Means)=215.45. In addition, there was a significant

main effect for experiment, $F_{(2, 456)}$=17.58, $p<0.001$, effect size partial η^2=0.07, Mean expt

1=864.28; Mean expt 2=-383.07; Mean expt 3=1058.85, SE(Means)=186.58. Finally, all possible

combinations of interactions between the factors were significant, $p<0.001$. In summary, the delta

intensity values differ between dyes, between imaging media, between experiments and the

combination of these factors influence each other differently depending on the chosen combination.

Consequently, this analysis including all possible factors and their combinations does not permit

conclusions, calling for separate ANOVAs in each of the two dyes and separate ANOVAs in each of

the 3 experiments. From a biological point of view, it would also not make sense to carry out one

ANOVA across both dyes and all conditions.

Separate ANOVA for AF647 in each of the 3 experiments

For dye AF647, there was a main effect for imaging media in all 3 experiments, Experiment 1: $F_{(3,}$

$_{76)}$=164.46, $p<0.001$, effect size partial η^2=0.87; Experiment 2: $F_{(3, 76)}$=182.45, $p<0.001$, effect size

partial η^2=0.88; Experiment 3: $F_{(3, 76)}$=114.06, $p<0.001$, effect size partial η^2=82. Looking at the

planned, post-hoc comparisons (Bonferroni), the same result was shown in all three experiments:

there was a significant ($p<0.05$) drop of delta intensity from PBS to Vectashield (PBS→VS):

Experiment 1 mean delta intensity drop=19348.86, SE(mean intensity drop)=1150.76, Experiment 2

mean delta intensity drop=10163.16, SE(mean intensity drop)=564.35, Experiment 3 mean delta

intensity drop=13821.93, SE(mean intensity drop=975.89). The other media (25 % Vectashield and

GLOX) did not differ significantly from PBS in all 3 experiments, i.e. there was no significant intensity

drop. Consequently, the results in all 3 experiments support the notion of an intensity drop only from

PBS to Vectashield. This was the result we had expected based on our pilot data. The results are

robust because we did not rely on experiment 1 alone, but replicated the results in experiments 2

and 3. In all 3 experiments, exactly the same main effects were observed and exactly the same post-

hoc comparisons reached statistical significance.

Analysis of AF647 recovery

In addition, we carried out a repeated measures ANOVA to test whether the intensity drop seen in

Vectashield can actually recover. We had hypothesized this recovery based on earlier observations

we had made in our laboratory when running pilot experiments. Now, we could not rely on delta

intensities from 2 measurements, but were rather interested in intensities at 3 different time points.

We compared three intensities (1. at PBS baseline, 2. after removing PBS and adding Vectashield, 3.

after replacing Vectashield with PBS and waiting for 2.5 hours in PBS imaging medium). We again

performed these comparisons for all three experiments separately. In this example, we had a

repeated measurement with three consecutive measurements. In this case, the respective analysis

depends on a prerequisite for a repeated measurements ANOVA: if sphericity can be assumed based

on the Mauchly's Test of Sphericity, no corrections need to be performed. Otherwise, the

Greenhouse-Geisser Test of an overall "within subjects effect" with corrected degrees of freedom

has to be applied. Because the Mauchly's Test of Sphericity revealed a significant result for all three

experiments (p<0.001), sphericity could not be assumed and the Greenhouse-Geisser Test was

applied for all three experiments. In all three experiments, intensity differences between the 3

repeated conditions were statistically significant (1. PBS baseline, 2. after removing PBS and adding

Vectashield, 3. after replacing Vectashield with PBS and waiting for 2.5 hours in PBS imaging

medium), Experiment 1: $F(1.01, 19.26)=162.68$, $p<0.001$; effect size partial $\eta^2=0.895$; Experiment 2:

$F(1.03, 19.48)=175.17$, $p<0.001$, effect size partial $\eta^2=0.9$; Experiment 3: $F(1.18, 22.38)=104.28$,

$p<0.001$, effect size partial $\eta^2=0.85$. Given that all three experiments showed a significant overall

effect for the repeated conditions, we carried out planned, post-hoc tests with Bonferroni correction

to evaluate which of the three time points significantly differed from each other. In each of the three

experiments, there was a significant intensity drop from 1. PBS baseline to 2. after removing PBS and

adding Vectashield (PBS→VS; in each experiment, $p<0.05$). Similarly, there was a significant recovery

from 2. after removing PBS and adding Vectashield to 3. After replacing Vectashield with PBS and

waiting for 2.5 hours in PBS imaging medium (VS→PBS:recovery, in each experiment, $p<0.05$). In all

three experiments, the recovery was never as strong as to reach the original intensity (in each

experiment, $p<0.05$). Consequently, the results demonstrating the recovery effect were very robust.

The drop as well as the recovery effect was not only shown in Experiment 1, but replicated exactly in

Experiments 2 and 3. In addition, all other post-hoc tests revealed the same results in all three

experiments.

Detailed results are as follows:

Experiment 1 had a PBS baseline intensity mean=24036.37, SE(mean)=1928.87, a drop after

removing PBS and adding Vectashield with a mean=3638.06, SE(mean)=359.85, and a recovery after

replacing Vectashield with PBS and waiting for 2.5 hours with a mean=16554.7, SE(mean)=1394.89.

Experiment 2 had a PBS baseline intensity mean=12270.01, SE(mean)=921.22, a drop after removing

PBS and adding Vectashield with a mean=1855.48, SE(mean)=151.16, and a recovery after replacing

Vectashield with PBS and waiting for 2.5 hours with a mean=9834.3, SE(mean)=758.21.

Experiment 3 had a PBS baseline intensity mean=16984.29, SE(mean)=1589.18, a drop after

removing PBS and adding Vectashield with a mean=2376.21, SE(mean)=247.32, and a recovery after

replacing Vectashield with PBS and waiting for 2.5 hours with a mean=13369.76,

SE(mean)=1367.025.

Separate ANOVA for AF488 in each of the 3 experiments

For dye AF488, there was also a main effect for imaging media in all 3 experiments, Experiment 1:

$F_{(3, 76)}=144.36$, $p<0.001$, partial $\eta^2=0.85$; Experiment 2: $F_{(3, 76)}=160.66$, $p<0.001$, partial $\eta^2=0.86$;

Experiment 3: $F_{(3, 76)}=101.86$, $p<0.001$, partial $\eta^2=0.8$. Looking at the planned, post-hoc comparisons

(Bonferroni), the same result was demonstrated in all three experiments: both Vectashield (PBS→VS)

and 25 % Vectashield (PBS→25% VS) showed an increase in delta intensity, which was significantly

different from the delta intensity of PBS and GLOX (p<0.05), while the delta intensities of PBS and GLOX did not differ significantly from each other. From our pilot work, we had assumed a medium effect size. We did not expect an effect as big as it turned out in our analysis, which came as a surprise to us. The effect was already big in experiment 1 and replicated in experiments 2 and 3. In detail, the results were as follows:

In experiment 1, there were no significant delta intensity differences between both PBS imaging media and between PBS and GLOX, but delta intensity showed an increase from PBS to Vectashield with a mean=3906.7 and an increase from PBS to 25 % Vectashield with a mean=9579.34, SE(means)=400.53 (with post-hoc Bonferroni p<0.05). The increase was stronger for 25% Vectashield than for Vectashield (with post-hoc Bonferroni p<0.05)

In experiment 2, there were no significant delta intensity differences between both PBS imaging media and between PBS and GLOX, and delta intensity showed an increase from PBS to Vectashield with a mean=1781.265 and an increase from PBS to 25 % Vectashield with a mean=10930.1, SE(means)=415.99 (with post-hoc Bonferroni p<0.05). The increase was once again stronger for 25 % Vectashield than for Vectashield (with post-hoc Bonferroni p<0.05).

In experiment 3, there were once again no significant delta intensity differences between both PBS imaging media and between PBS and GLOX, and delta intensity showed an increase from PBS to Vectashield with a mean=2297.175 and an increase from PBS to 25 % Vectashield with a mean=3959.1, SE(means)=199.99 (with post-hoc Bonferroni p<0.05). The increase was again stronger for 25 % Vectashield than for Vectashield (with post-hoc Bonferroni p<0.05).

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Author Contributions

AA, NS and INS performed the experiments and analysis. AA and INS performed dSTORM imaging. RS

performed the statistical analysis with the input from INS. INS designed the experiments with

statistical advice from RS. INS wrote the manuscript with the input from AA, NS and RS. INS

supervised the project.

Competing Interests Statement

The authors declare no competing interests.

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