The effect of stimulus choice on an

EEG-based objective measure of speech

intelligibility

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1 ABSTRACT

Objectives Recently an objective measure of speech intelligibility, based on brain responses derived from the electroencephalogram (EEG), has been developed using isolated Matrix sentences as a stimulus. We investigated whether this objective measure of speech intelligibility can also be used with natural speech as a stimulus, as this would be beneficial for clinical applications.

7 **Design** We recorded the EEG in 19 normal-hearing participants while they listened to two types of stimuli: Matrix sentences and a natural story. Each stimulus was presented 8 at different levels of speech intelligibility by adding speech weighted noise. Speech 9 intelligibility was assessed in two ways for both stimuli: (1) behaviorally and (2) objectively 10 by reconstructing the speech envelope from the EEG using a linear decoder and correlating 11 it with the acoustic envelope. We also calculated temporal response functions (TRFs) 12 to investigate the temporal characteristics of the brain responses in the EEG channels 13 covering different brain areas. 14

Results For both stimulus types the correlation between the speech envelope and 15 the reconstructed envelope increased with increasing speech intelligibility. In addition, 16 correlations were higher for the natural story than for the Matrix sentences. Similar to the 17 linear decoder analysis, TRF amplitudes increased with increasing speech intelligibility for 18 both stimuli. Remarkable is that although speech intelligibility remained unchanged, neural 19 speech processing was affected by the addition of a small amount of noise: TRF amplitudes 20 across the entire scalp decreased between 0 to 150 ms, while amplitudes between 150 to 21 200 ms increased. TRF latency changes in function of speech intelligibility appeared to 22 be stimulus specific: The latency of the prominent negative peak in the early responses 23 (50-300 ms) increased with increasing speech intelligibility for the Matrix sentences, but 24 remained unchanged for the natural story. 25

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Conclusions These results show (1) the feasibility of natural speech as a stimulus for the objective measure of speech intelligibility, (2) that neural tracking of speech is enhanced using a natural story compared to Matrix sentences and (3) that noise and the stimulus type can change the temporal characteristics of the brain responses. These results might reflect the integration of incoming acoustic features and top-down information, suggesting that the choice of the stimulus has to be considered based on the intended purpose of the measurement.

1 INTRODUCTION

In current clinical practice speech intelligibility is measured behaviorally by asking the listeners to recall the words or sentences they heard. By doing so, not only the function of the auditory periphery is measured, but also working memory, language knowledge, cognition and speech production. When measuring speech intelligibility to evaluate the function of a hearing aid, it can be desirable to evaluate the auditory periphery without these extra factors. In addition, the required active participation of the patient can make these measurements challenging or even impossible because of poor attention or motivation, especially in small children.

40 To overcome these challenges an objective measure of speech intelligibility, where no input from the patient is required, would be of great benefit. Previous studies have shown that the 41 slowly varying speech envelope is essential for speech intelligibility (Shannon et al., 1995), 42 and that it can be reconstructed from brain responses using electroencephalography (EEG) or 43 magnetoencephalography (Luo and Poeppel, 2007; Aiken and Picton, 2008; Ding and Simon, 2011). 44 Correlating the reconstructed envelope from the brain response with the real acoustic envelope, 45 results in a measure of neural envelope tracking, which is related to speech intelligibility (Luo and 46 Poeppel, 2007; Ding et al., 2014; Millman et al., 2015; Molinaro and Lizarazu, 2017; Vanthornhout 47 et al., 2018; Lotzov and Parra, 2019; Lesenfants et al., 2019). 48

Vanthornhout et al. (2018) and Lesenfants et al. (2019) demonstrated the application of this 49 measure of neural envelope tracking in an objective measure of speech intelligibility using isolated 50 Matrix sentences as a stimulus. In their studies the same Matrix sentences were used during a 51 standardized behavioral recall experiment and an EEG measurement, enabling direct comparison of 52 speech intelligibility to envelope tracking. However, for the purpose of clinical applications, the 53 use of isolated sentences may be sub-optimal. Sentences do not reflect everyday communication 54 where syllable, word and sentence rate are less controlled and more semantic top-down processing 55 is involved. Therefore, an objective measure of speech intelligibility based on fully natural speech 56 would (1) overcome the patient-related challenges linked to attention and motivation (2) and allow 57

intelligibility measurements of any speech fragment, which is impossible today using behavioralmeasurements but may relate better to everyday communication.

60 In this study we investigated whether the objective measure of speech intelligibility by Vanthornhout et al. (2018) using Matrix sentences can also be conducted with natural running 61 62 speech, such as a narrated story. We hypothesized that a difference in neural envelope tracking between the two stimuli may be related to the interactive process of speech processing. Speech 63 intelligibility namely relies on the active integration of two incoming information streams (Hickok 64 and Poeppel, 2007; Anderson et al., 2018): (1) the bottom-up stream that processes the acoustic 65 features through the auditory pathway until the auditory cortex and (2) the top-down stream 66 67 originating in different brain regions. We hypothesized that if neural envelope tracking is mainly a feed-forward acoustic process, results for Matrix sentences will be enhanced compared to the story 68 because of the rigid syllable, word and sentence rate reflected in the speech envelope of the Matrix 69 sentences. If, on the other hand, neural envelope tracking captures the interaction between the 70 incoming acoustic speech stream and top-down information, results for the story will be enhanced 71 because of, e.g., increased semantic processing (Di Liberto et al., 2018; Broderick et al., 2018) and 72 attention (Kerlin et al., 2010; Ding and Simon, 2012; Mesgarani and Chang, 2012; Vanthornhout 73 et al., 2019). 74

2 MATERIAL AND METHODS

75 2.1 Participants

Nineteen participants aged between 18 and 28 years (3 men and 16 women) took part in the experiment after providing informed consent. Participants had Flemish as their mother tongue and were all normal-hearing, confirmed with pure tone audiometry (thresholds \leq 25 dB HL at all octave frequencies from 125 Hz to 8 kHz). The study was approved by the Medical Ethics Committee UZ Leuven / Research (KU Leuven) with reference S57102. All participants were unpaid volunteers.

81 2.2 Auditory stimuli

82 During the experiment participants listened to three different stimuli: (1) isolated Matrix sentences,

83 (2) a natural story and (3) another story used to train the linear decoder on.

84 2.2.1 Matrix sentences

85 Flemish Matrix sentences contain 5 words spoken by a female speaker and have a fixed syntactic structure of 'proper name-verb-numeral-adjective-object', for example, 'Sofie sees ten blue socks' 86 with a speech rate of 4.1 syllables/second, 2.5 words/second and 0.5 sentences/second. Each 87 category of words has 10 alternatives and each sentence consists of a random combination of these 88 alternatives which induces a rigid and artificial speech rate and reduces semantic context to a bare 89 minimum. These sentences are gathered into standardized lists of 20 sentences. Speech was fixed at 90 a level of 60 dBA and the noise level varied across trials. We used speech weighted noise (SWN) 91 which has the long-term-average spectrum of the stimulus and therefore results in optimal energetic 92 masking. Matrix sentences are a validated speech material to measure speech intelligibility which 93 94 allows us to directly compare EEG results with speech intelligibility, similar to Vanthornhout et al. (2018) and Lesenfants et al. (2019). However, Matrix sentences have a rigid speech rate and lack 95 semantic information, resulting in an artificial speech stimulus not representative for everyday 96 communication. 97

98 2.2.2 Natural story

99 The natural story we used is 'De Wilde Zwanen', written by Hans Christian Andersen and 100 narrated in Flemish by Katrien Devos (female speaker) with a speech rate of approximately 101 3.5 syllables/second, 2.5 words/second and 0.2 sentences/second. Speech was fixed at a level 102 of 60 dBA and the noise level of the SWN varied across trials. The main differences between the 103 Matrix sentences (2.2.1) and fully natural speech such as this narrated story are: Prosody: Matrix sentences are part of a standardized speech material where every word is
 spoken at the same intensity, while the story is naturally spoken with intensity variations as a
 consequence.

107 2. *Speech rate*: Matrix sentences have a rigid syllable, word and sentence rate, while the story has108 a naturally varying speech rate because of different word and sentence lengths.

3. *Semantic context*: Matrix sentences are a random combination of words, minimizing the use of
semantic context. The story, on the other hand, is coherent speech where the use of top-down
processing is triggered, e.g., knowledge about time, space and characters.

4. *Lexical prediction*: The permutations of the words are different in each Matrix sentence, but the
words themselves become more familiar to the participants during the experiment, in contrast
to the story.

115 2.2.3 Decoder story

A children's story, 'Milan', written and narrated in Flemish by Stijn Vranken (male speaker), was presented to the participants with a speech rate of 3.7 syllables/second, 2.6 words/second and 0.3 sentences/second. This story is 14 minutes long and was presented at a level of 60 dBA without noise. The purpose of this story was to have an independent continuous stimulus without background noise to train a linear decoder on (Vanthornhout et al., 2018) to reconstruct the speech envelope from the EEG.

122 2.3 Behavioral experiment

Speech intelligibility was measured behaviorally in order to compare envelope tracking results in terms of speech intelligibility. We need to measure speech intelligibility for both stimuli separately because they differ in content and acoustic parameters (speaker, speech rate, intonation). Adding a similar level of background noise will therefore not result in a similar level of speech intelligibility (Decruy et al., 2018). 128 Before the EEG experiment we conducted a standardized Matrix test. This standardized test 129 starts with 2 training lists followed by 3 testing lists of 20 sentences at different Signal-to-Noise Ratios (SNR): -9.5; -6.5 and -3.5 dB SNR. Participants had to recall the sentence they heard. By 130 counting the correctly recalled words, a percentage correct per presented SNR was calculated. 131 Next, a psychometric function was fitted on the data points, similar to what is done in clinical 132 practice. To measure speech intelligibility for the story, we cannot ask the participants to recall 133 every word, instead we used a rating method during the EEG experiment. Participants were asked 134 to rate their speech intelligibility with the following question: 'Which percentage of the words did 135 you understand?' at the presented SNRs (-12.5; -9.5; -6.5; -3.5; -0.5 and 2.5 dB SNR). In addition 136 to the recall procedure for the Matrix sentences before the EEG experiment, we also asked 9 of the 137 19 participants to rate their speech intelligibility for the Matrix sentences during the EEG, similar to 138 139 the story.

140 2.4 EEG experiment

141 Ten participants started the EEG experiment by listening to Matrix sentences followed by the natural story. The remaining 9 participants did this in the reversed order. The decoder story was 142 presented in between. The natural story was cut in 7 equal parts of approximately 4 minutes long, 143 which we presented in chronological order. The first part was always presented in silence to optimize 144 comprehension of the storyline. The following 6 parts were presented at 6 different SNRs in random 145 order: -12.5; -9.5; -6.5; -3.5; -0.5 and 2.5 dB SNR. The Matrix sentences were concatenated into 7 146 lists of 40 sentences with a silent gap between the sentences randomly varying between 0.8 and 1.2 147 seconds. Each 2-minute trial, containing 40 sentences at a particular SNR, was presented twice to 148 analyze test-retest reliability. The SNRs were the same SNRs as used for the story, also in random 149 order. To maximize attention and keep the participants motivated, questions were asked about each 150 SNR trial, for example, 'What happened after sunset?' (story) or 'Which colors of boats were 151 mentioned?' (Matrix sentences). The answers were not used for further analysis. After the question, 152 the participants were asked to rate their speech intelligibility with the following question: 'Which 153 percentage of the words did you understand?' as mentioned in section 2.3. 154

155 2.5 Signal processing

In this study we measured neural envelope tracking and linked this to speech intelligibility and stimulus type (natural story versus isolated Matrix sentences). Neural envelope tracking was calculated in two ways: We correlated the acoustic speech envelope (2.5.1) with the speech envelope reconstructed from the EEG respons (2.5.2) with the help of a linear decoder. Secondly, we calculated temporal response functions (TRFs) to investigate the temporal characteristics of the brain responses in the EEG channels covering the scalp (2.5.3).

162 2.5.1 Acoustic envelope

163 The acoustic speech envelope was extracted from the stimulus according to Biesmans et al. (2017), using a gammatone filterbank followed by a power law. We used a filterbank containing 28 channels 164 spaced by 1 equivalent rectangular bandwidth with center frequencies from 50 Hz until 5000 Hz. 165 The absolute value of each sample in each channel was raised to the power of 0.6. All 28 channel 166 envelopes were averaged which resulted in one single envelope. As a next step, the acoustic speech 167 envelope was band-pass filtered, similar to the EEG signal, in the delta (0.5-4 Hz) or theta (4-8 Hz) 168 frequency band with a Chebyshev filter with 80 dB attenuation at 10% outside the passband. Only 169 170 these low frequencies were further processed, because they contain the information of interest of the slowly varying speech envelope. 171

172 2.5.2 Envelope reconstruction

As a first step the EEG data was downsampled from 8192 Hz to 256 Hz to reduce processing time and referenced to an average of the electrodes. Next, EEG artefact rejection was done using a multi-channel Wiener filter (MWF) (Somers et al., 2018). the MWF was calculated on the long decoder story without noise and applied on the shorter Matrix and coherent story SNR trials. After artefact rejection, the signal was bandpass filtered, similar to the acoustic speech envelope and the sample rate was further decreased from 256 Hz to 128 Hz. A schematic overview is shown in Figure 1.

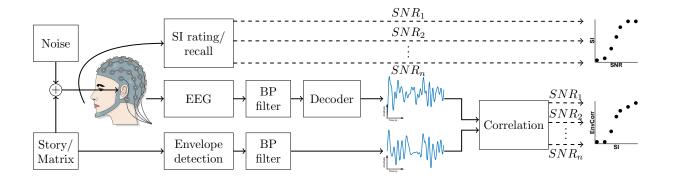


Figure 1. Overview of the experimental setup using the linear decoder analysis. We presented the Matrix sentences and a story at different Signal-to-Noise Ratio's (SNR). Participants listened to the speech while their EEG was measured. To obtain a measure of neural envelope tracking we correlated the reconstructed envelope with the acoustic envelope after band-pass filtering (BP filter). We compared the envelope tracking results with the behavioral speech intelligibility (SI) scores.

To enable reconstruction of the speech envelope from the neural data as a measure of neural 180 envelope tracking, a linear decoder was created using the mTRF toolbox (Lalor et al., 2006, 2009). 181 As speech elicits neural responses with some delay, the decoder not only attributes weights to 182 183 each EEG channel (spatial filter), but it also takes the shifted neural responses of each channel 184 into account (temporal filter), resulting in a matrix R containing the shifted neural responses of each channel. If q is the linear decoder and R the shifted neural data, the reconstruction of the 185 speech envelope $\hat{s}(t)$ was obtained by $\hat{s}(t) = \sum_n \sum_{\tau} g(n, \tau) R(t + \tau, n)$ with t the time index, n 186 ranging over the recording electrodes and τ ranging over the integration window, i.e., the number 187 of post-stimulus samples used to reconstruct the envelope. The decoder was calculated by solving 188 $g = (RR^T)^{-1}(Rs^T)$ with s the speech envelope and applying ridge regression to prevent overfitting. 189 190 We used an integration window of 250 ms post-stimulus resulting in the decoder matrix q of 64 (EEG channels) x 33 (time delays within the integration window). The decoder was created using 191 the Milan story (14 minutes) without any noise. 192

As a last step the envelope was reconstructed by applying the decoder to both test stimuli, the Matrix sentences and the natural story, at various noise levels. Each SNR trial consisted of 2 195 presentations of 80 seconds of speech (silences excluded). To measure how similar this reconstructed 196 envelope was to the acoustic envelope as a measure for neural envelope tracking, we calculated the 197 bootstrapped Spearman correlation using Monte Carlo sampling after removing the silences in the 198 stimulus and the corresponding part in the EEG. Removing the silences is necessary as the Matrix 199 sentences contain quasi-regular silent gaps between the sentences which would be a confound.

The significance level of the correlation was calculated by correlating random permutations of the real and reconstructed envelope 1000 times and taking percentile 2.5 and 97.5 to obtain a 95% confidence interval.

203 2.5.3 Temporal response function estimation

The analysis above integrates all neural activity over channels and time lags and requires a decoder trained on a separate story. To have a closer look at the spatiotemporal profile of the neural responses and remove the assumption that neural processing is similar for the decoder story and the test stimuli in different noise conditions, we calculated TRFs. A TRF is a linear filter that describes how the acoustic speech envelope of the stimulus is transformed into neural responses. This is the inverse approach of the previously mentioned envelope reconstruction where analysis is done from EEG to stimulus.

We calculated a TRF for every electrode channel in every participant. The first signal processing 211 steps are identical to the envelope reconstruction model starting with downsampling to 1024 Hz, 212 artefact rejection with MWF and filtering (0.5-8 Hz). Next, TRFs were calculated using the boosting 213 algorithm (David et al., 2007; Brodbeck et al., 2018) with an 12 error norm (using the Eelbrain 214 source code (Brodbeck, 2017)) as described in detail by David et al. (2007). After calculation, the 215 TRFs were convolved with a rotationally symmetric Gaussian kernel of 5 samples long (SD=2). To 216 analyze the TRFs in the time domain, we investigate the latency and amplitude of the negative and 217 positive peaks occurring directly after the stimulus onset (Ding and Simon, 2011; Obleser and Kotz, 218 2011; Ding and Simon, 2012; Ding et al., 2014). 219

220 2.6 Experimental setup

Recordings were made in a soundproof and electromagnetically shielded room. Speech was 221 presented bilaterally at 60 dBA and the setup was calibrated using a 2cm³ coupler of the artificial 222 ear (Brüel & Kjær 4152, Denmark) for each stimulus. The stimuli were presented using APEX 3 223 (Francart et al., 2008), an RME Multiface II sound card (Germany) and Etymotic ER-3A insert 224 225 phones (Illinois, USA). First the participants did a behavioral test to measure their speech intelligibility. Next, a 64-channel BioSemi ActiveTwo (the Netherlands) EEG recording system was 226 used for the EEG recordings at a sample rate of 8192 Hz. Participants sat in a comfortable chair and 227 228 were asked to move as little as possible during the recordings. We inserted a small break between the behavioral and the EEG part and between the Matrix sentences and the story if necessary. 229

230 2.7 Statistical Analysis

Statistical analysis was performed using MATLAB (version R2016b) and R (version 3.3.2) software. The significance level was set at α =0.05 unless otherwise stated.

For the behavioral tests and envelope reconstruction we compared dependent samples (e.g. testretest) using a nonparametric Wilcoxon signed-rank test. For every filter band and stimulus we tested the correlation between envelope reconstruction and speech intelligibility using Spearman's rank correlation. Next, we assessed the relationship between speech intelligibility, envelope reconstruction, filter band and stimulus by constructing a linear mixed effect (LME) model with the following formula:

239
$$corr \sim SI + stimulus + band + SI : band + SI : stimulus + SI : band : stimulus$$

where *corr* is defined as the Spearman correlation between the reconstructed and the acoustic envelope, with random effect of intercept of the participants and fixed and interaction effects of *SI* (speech intelligibility), *stimulus* (Matrix sentences or natural story) and *band* (the delta or theta filter band). As a control, we constructed the exact same model, but in function of SNR instead of SI. To control if every chosen fixed and random effect benefited the model the Akaike Information Criterion (AIC) was calculated. The model with the lowest AIC was selected and its residual plot was analyzed to assess the normality assumption of the LME residuals. Unstandardized regression coefficients (beta) with 95% confidence intervals and p-value are reported in the results section.

To investigate which part of the TRF was significantly different from zero, we conducted a cluster-based permutation test. To explore significant differences between stimuli we conducted a positive and negative cluster-based analysis with a post hoc Bonferroni adjustment to correct for the positive and negative test. These tests are explained in detail by Maris and Oostenveld (2007). Spearman's rank correlation was used to investigate the possible change of amplitude and latency of the temporal-occipital peaks over time.

3 RESULTS

254 3.1 Behavioral speech intelligibility

During the experiment we measured speech intelligibility behaviorally at different SNRs for every participant. Figure 2 shows that the natural story (rating method) was significantly more difficult than the Matrix sentences (recall method) (p<0.001, CI(95%) = [15.99; 23.34], n=19, Wilcoxon signed-rank test). This indicates that the same SNR does not result in the same level of speech intelligibility for the different stimuli. To be able to compare the coherent story with the Matrix sentences, we need to account for this.

To check whether the used method to measure speech intelligibility, rate (story) versus recall (Matrix sentences), did not influence the results, we asked 9 of the participants to rate their speech intelligibility for the Matrix sentences, similar to the story, in addition to the standardized recall method. Comparing their rate and recall scores for the same Matrix sentences at 3 SNRs did not reveal any significant difference (-9.5 dB SNR: p=0.19, CI(95%)=[-11.50; 22.00]; -6.5 dB SNR: p=0.06, CI(95%)=[-29.50; 1.50]; -3.5 dB SNR: p=0.41, CI(95%)=[-9.00; 2.75]; n=9, Wilcoxon signed-rank test).

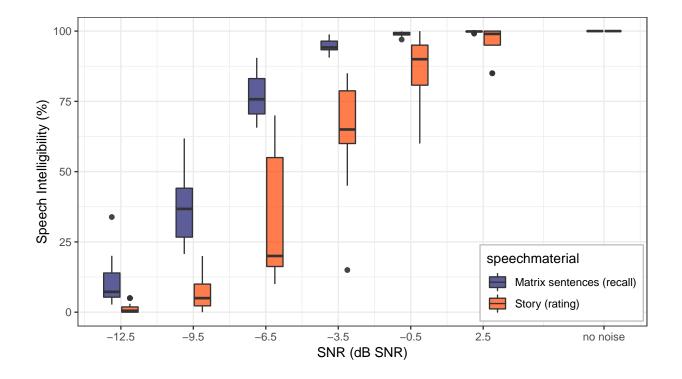


Figure 2. A comparison between the Matrix sentences and the story reveals that the story is more difficult to understand when adding background noise.

268 3.2 Envelope reconstruction

269 To measure neural envelope tracking, we calculated the Spearman correlation between the 270 reconstructed envelope and the acoustic envelope. A test-retest analysis showed no significant difference between test and retest correlations (p=0.746, CI(95%) = [-0.004; 0.006], Wilcoxon 271 signed-rank test), therefore we averaged the correlation of the test and retest conditions resulting in 272 one correlation per participant per SNR per stimulus. We also conducted a chance level analysis 273 to investigate whether there is a difference in chance level between both stimuli. A difference in 274 chance level would imply that the decoder would show a preference to one of the two stimuli. To 275 obtain the chance level we reconstructed the envelope of the story similar to the standard analysis. 276 Next we correlated the reconstructed envelope of each story trial with the acoustic envelope of all 277 trials of both the story (except for the used trial) and the Matrix sentences. No significant difference 278 was found between the chance level of the stimuli (p=0.534, CI(95%)=[-0.005; 0.003], Wilcoxon 279

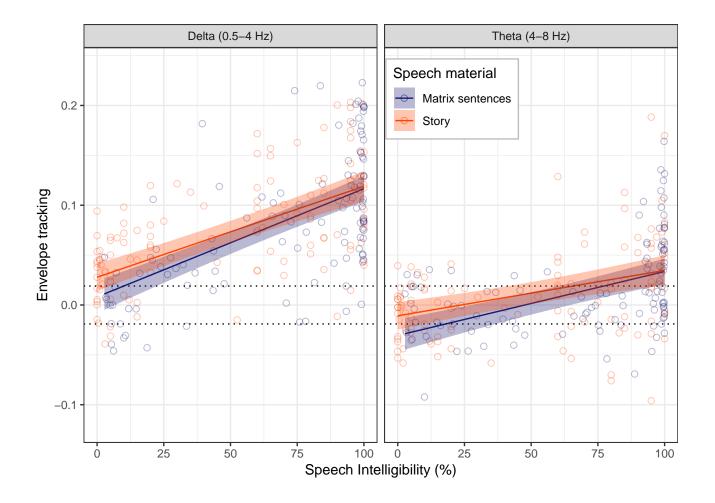


Figure 3. Neural envelope tracking increases with increasing speech intelligibility and by using natural speech as a stimulus. The shading represents two times the standard error of the fit and the dotted line is the significance level of the correlation (± 0.019).

signed-rank test). In addition, the 95% confidence interval of the difference between the chance
level of the stimuli is similar to the test-retest variability (CI(95%)=[-0.005; 0.006]), indicating that
there is no important effect.

We analyzed neural envelope tracking in the delta (0.5-4 Hz) and the theta (4-8 Hz) band for the Matrix sentences and the natural story at various levels of speech intelligibility. Figure 3 shows that when speech intelligibility increases, the correlation between the acoustic and the reconstructed envelope, i.e. neural envelope tracking, increases for every filter band and every stimulus tested (p<0.001, table 1, Spearman rank correlation).

To additionally investigate the influence of stimulus choice, we created an LME model as a 288 289 function of speech intelligibility. The analysis shows that neural envelope tracking is enhanced for the story compared to the Matrix sentences (fixed effect stimulus, p=0.010, LME, table 2). 290 291 This enhancement does not significantly depend on the level of speech intelligibility or filter band (interaction effect SI:stimulus, p=0.155; interaction effect SI:band:stimulus, p=0.912; LME, table 292 2). Further, neural envelope tracking in the delta band (0.5-4 Hz) is higher than in the theta band 293 (4-8 Hz) (fixed effect band, p<0.001, LME, table 2) with a steeper slope in the delta band (0.5-4 Hz) 294 (interaction effect SI:band, p < 0.001, LME, table 2). 295

When conducting the same analysis using SNR as a predictor for speech intelligibility, the same fixed and interaction effects were found to be significant as for the SI analysis (table 3). This shows that even at the same SNR neural envelope tracking for the natural story is enhanced compared to the Matrix sentences, making it impossible to disentangle between the effects of SNR and SI with the current data.

301 3.3 Temporal response function

The analysis above integrates all different time lags and channels to obtain an optimal 302 reconstruction of the envelope and requires a decoder trained on a separate story. In the following 303 analysis we focus on how the neural responses follow the envelope in the time and spatial domain 304 and remove the assumption that neural processing is similar for the decoder story and the test stimuli 305 by investigating TRFs. TRFs were calculated on an individual level. This resulted in 868 TRFs per 306 participant (64 channels x 2 stimuli x 7 SNRs). To visualize topographies, we averaged the TRFs 307 per stimulus per SNR over participants. To investigate the time-course of the TRFs, we averaged 308 TRFs for a temporal-occipital channel selection (Figure 4). This selection is based on the TRF 309 results shown in Figure 5. A cluster-based permutation test (Maris and Oostenveld, 2007) shows the 310 TRF samples significantly different from zero, highlighted in bold in Figure 6. 311

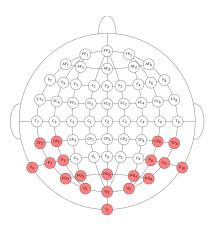


Figure 4. Electrode selection: 64 active electrodes placed according to the 10-20 electrode system. The locations of the electrodes that were selected for the calculation of the occipital-temporal TRF are indicated in red.

312 3.3.1 Effect of SNR on TRF

Figure 5 shows the spatiotemporal activation profile of respectively the Matrix sentences and the natural story. In the no-noise condition both stimuli show positive central and negative parietooccipital amplitudes over time. When a small amount of noise is added and speech intelligibility remains almost unchanged from the no-noise condition (SNR=2.5 dB SNR; Matrix sentences: median SI=99.9%, sd=0.2; Story: median SI=99.0%, sd=4.7), the amplitudes across the entire scalp decrease between 0 to 150 ms, while amplitudes between 150 to 200 ms increase in both stimuli. Between 50 and 100 ms amplitudes even swap polarities.

When more noise is added and speech intelligibility decreases positive central and negative parieto-occipital activation decreases, especially in the 150 tot 200 ms timelag (Figure 5). In the 50 to 100 ms timelag, on the other hand, the negative central activation increases with decreasing speech intelligibility and reaches a maximum at SNR=-3.5 dB SNR.

To zoom in on the amplitude changes over time, we visualized an average TRF for the temporal-occipital channels per SNR in Figure 6. When speech intelligibility is very low (SNR<-12.5 dB SNR) both stimuli have very low responses over time. When speech is understood

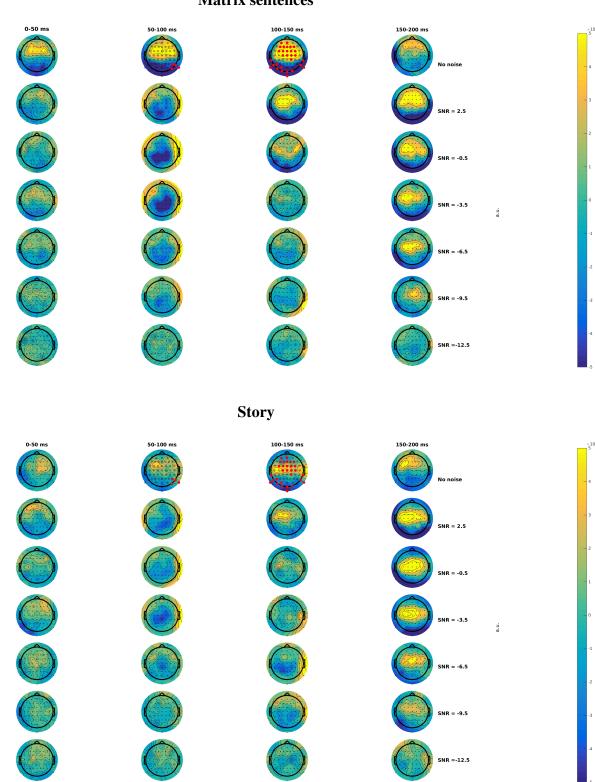
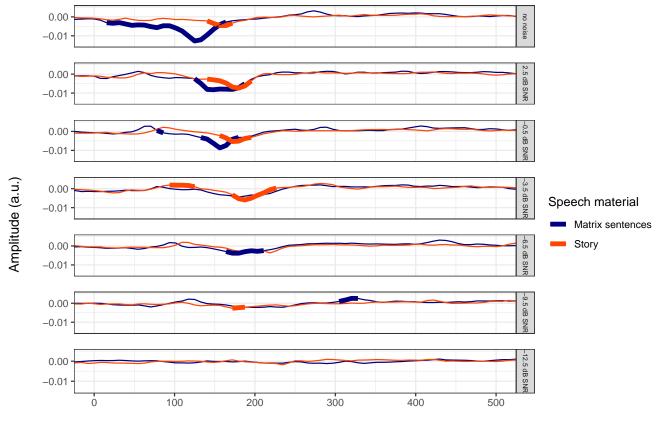


Figure 5. Topographies for the story and the Matrix sentences at different SNRs and different time lags varying from 0 until 200 ms. Significant differences between the Matrix sentences and the story are highlighted in red.

Matrix sentences



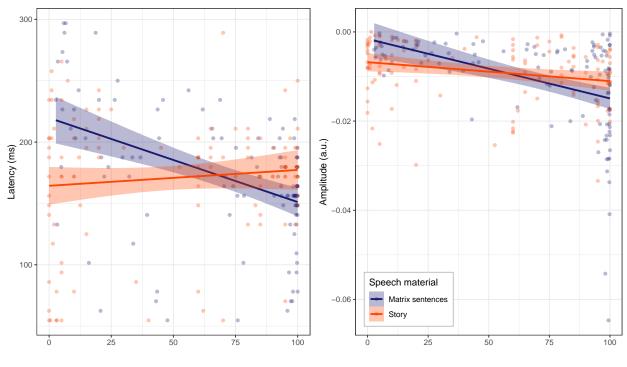
Time (seconds)

Figure 6. Time-course of the temporal-occipital TRFs over participants for the Matrix sentences and the story. TRF samples significantly different from zero are highlighted in bold.

a negative peak can be found. Figure 7 shows the latency and amplitude results of this peak on a participant level over speech intelligibility. It was determined individually by selecting the most negative amplitude of the TRF between 50 and 300 ms. With decreasing speech intelligibility the amplitude of the negative peak per participant decreases for both stimuli (Matrix sentences: Spearman rank correlation=0.49, p<0.001; Story: Spearman rank correlation=0.26, p=0.005).

332 3.3.2 Effect of stimulus type on TRF

Besides the decreasing amplitude, latency also decreases for the Matrix sentences with decreasing speech intelligibility (Spearman rank correlation=0.46, p<0.001). For the natural story, on the other hand, latency is not significantly related to speech intelligibility (Spearman rank correlation=0.02,
p=0.835)).



Speech intelligibility (%)

Figure 7. Latency and amplitude of the negative peak of the temporal-occipital TRF between 50 and 300 ms per participant over speech intelligibility.

Next to the difference between the Matrix sentences and the story concerning latency changes, 337 other stimulus dependent differences can be found. First, a positive and negative cluster analysis 338 (Maris and Oostenveld, 2007) over all participants revealed significant differences (α =0.025) 339 between both stimuli in the no-noise condition with larger amplitudes for the Matrix sentences in 340 the central and parieto-occipital channels, highlighted in red in Figure 5. In contrast to this stimuli 341 342 driven difference in the no-noise condition, no significant differences between both stimuli could be found in the presence of background noise. Second, in addition to the prominent negative peak 343 between 100 and 200 ms, a positive significant peak arises around 300 ms for the Matrix sentences 344 at -9.5 dB SNR (Figure 6), while this is not the case for the story. 345

4 DISCUSSION

In this study we investigated whether the objective measure of speech intelligibility by Vanthornhout et al. (2018) using Matrix sentences can also be conducted with natural speech as this would be beneficial for clinical applications. To that end, we tested 19 normal-hearing participants. They listened to both the Matrix sentences and a natural story at varying levels of speech intelligibility while their EEG was recorded. We found that it is feasible to use natural speech as a stimulus for the objective measure of speech intelligibility and that noise and the stimulus type can change the temporal characteristics of the brain responses over the scalp.

353 4.1 The same SNR does not result in similar speech intelligibility for different 354 stimuli

355 As a first step we measured speech intelligibility behaviorally for both stimuli at different noise 356 levels. The results show that the same SNR does not result in similar speech intelligibility for the different stimuli. The story was found to be more difficult to understand than Matrix sentences. 357 Although we controlled for the sex of the speaker and chose stimuli with similar speech rates and 358 359 spectrum, the difference could still be due to different acoustic features such as for example prosody. 360 The Matrix sentences namely are part of a standardized speech material where every word is spoken at the same intensity. The story, on the other hand, is narrated for children and has more variations. 361 An additional reason to explain this difference is lexical prediction. Even though the permutations 362 of the words are different in each Matrix sentence, the words themselves are all equally likely and 363 familiar to the participants, in contrast to the story. Perhaps drawing from a larger pool of words for 364 the Matrix sentences might have led to more similar intelligibility ratings between stimuli. Finally, 365 speech intelligibility for both stimuli was measured in a different way: rating (story) versus recall 366 (Matrix sentences). Similar to the rating and recall results for the Matrix sentences of Decruy et al. 367 (2018), we did not find a statistical difference between both measuring methods applied on the same 368 369 Matrix sentences.

370 4.2 Neural envelope tracking as an objective measure of speech intelligibility

We found that the correlation between the reconstructed and the acoustic envelope increased with speech intelligibility for both the Matrix sentences and the story. This supports the results of Luo and Poeppel (2007); Ding and Simon (2013); Ding et al. (2014); Molinaro and Lizarazu (2017); Vanthornhout et al. (2018); Lotzov and Parra (2019) where an increase in speech intelligibility was also found to accompany an increase in envelope tracking and demonstrates that the objective measure of speech intelligibility using Matrix sentences by Vanthornhout et al. (2018) can be conducted with fully natural speech.

Next, the tracking results in the delta band were significantly higher than in the theta band while the significance levels remain the same, resulting in a steeper slope of envelope tracking as a function of speech intelligibility in the delta band. This difference in correlation magnitude between the frequency bands could be explained by the fact that the modulation spectrum of both stimuli has most energy in the delta band (Luo and Poeppel, 2007; Aiken and Picton, 2008).

383 When investigating the differences between both stimuli, we found that the use of natural speech enhanced neural envelope tracking compared to Matrix sentences. This suggests that neural envelope 384 385 tracking might capture the interaction between the incoming acoustic speech stream and top-down information (Hickok and Poeppel, 2007; Gross et al., 2013) such as for example semantic processing 386 (Di Liberto et al., 2018; Broderick et al., 2018). A potential confound is that we used different SNRs 387 for the two stimulus types (to control for intelligibility). This means that the differences in envelope 388 tracking could be related simply to SNR rather than other stimulus properties. To investigate this, 389 we conducted the same analysis, but with SNR as predictor instead of intelligibility, and again found 390 significantly increased envelope tracking for the story stimulus. This shows that SNR by itself does 391 not account for the full difference between the two stimulus types. However, apart from different 392 SNRs, other confounding factors could be present where we cannot control for. First, although the 393 acoustics of the stimuli were matched in terms of sex and speech rate of the speaker and spectrum 394 of the stimulus, acoustic differences like prosody are still present, as discussed in paragraph 4.1. 395

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Second, despite the questions asked to motivate the participants, the reduced correlations for the Matrix sentences could be linked to attention. Because listening to concatenated sentences can be boring, attention loss could occur which reduces neural envelope tracking (Ding and Simon, 2012; Kong et al., 2014; Petersen et al., 2017; Vanthornhout et al., 2019). For the natural story, on the other hand, attention could be less of an issue as attending this speech is entertaining possibly resulting in higher correlations.

402 4.3 The effect of noise and stimulus type on neural envelope tracking

403 In addition to envelope reconstruction to show the feasibility of natural speech as a stimulus for the objective measure (4.2), we conducted a TRF analysis. This analysis enables us to investigate 404 the temporal characteristics of the brain responses over the entire scalp and removes the assumption 405 that neural processing is similar for the decoder story and the test stimuli. The topographies in 406 Figure 5 of both stimuli show a negative activation in the temporal-occipital channels and positive 407 activation in the central channels. This is a typical topography of auditory evoked far-field potentials 408 (Picton, 2011). The large negative peak within the 100 to 200 ms time lag (Figure 6) could be the 409 so-called N100, usually occurring at a latency between 70-150 ms (Picton, 2011). 410

411 4.3.1 Effect of SNR and speech intelligibility on TRFs

Generally we found, similar to envelope reconstruction, high TRF amplitudes over the entire scalp 412 when speech intelligibility is high (SI=100%) and reduced amplitudes when speech intelligibility 413 decreased for both stimuli, again showing feasibility of natural speech as a stimulus for the objective 414 measure of speech intelligibility. Most remarkable are the TRF amplitudes between 150 to 200 ms, 415 which consistently decrease with decreasing speech intelligibility, perhaps indicating a time window 416 sensitive to speech intelligibility. Another peculiarity are the noise induced topographic changes. 417 When a small amount of noise is added and speech intelligibility remains almost unchanged from 418 the no-noise condition (SNR=2.5 dB SNR; Matrix sentences: SI=99.9%; Story: SI=99.0%), TRF 419 amplitudes across the entire scalp decrease between 0 to 150 ms, while amplitudes between 150 to 420 200 ms increase. Moreover, TRF amplitudes between 50 and 100 ms even switch polarities in the 421

presence of noise. These results possibly reveal noise induced changes related to enhanced attention
and listening effort (Ding and Simon, 2012; Kong et al., 2014; Petersen et al., 2017; Obleser and
Kotz, 2011).

425 4.3.2 Effect of stimulus type on TRFs

426 Stimulus related differences can be found when comparing topography results between both stimuli. TRF amplitudes are larger for the Matrix sentences in the central and parieto-occipital 427 channels compared to the story in the no-noise condition. In the presence of background noise, 428 even at a very high SNR, no significant difference can be found anymore. A possible hypothesis 429 could be the interaction between the incoming acoustic speech stream and top-down information 430 (Hickok and Poeppel, 2007; Gross et al., 2013): In the no-noise condition Matrix sentences are 431 mainly processed in a feed-forward acoustical way. The enhanced TRF amplitudes could be caused 432 by the fixed syntactical 5-word structure of the Matrix sentences, resulting in a more rigid word 433 and sentence rate compared to the story. However, when noise is added, more effort has to be paid 434 to listen to the Matrix sentences. This changes listening to the Matrix sentences from a bottom-up 435 436 process to an interactive bottom-up and top-down process similar to the story, diminishing the 437 differences between both stimuli.

Another stimulus related difference is the latency pattern over speech intelligibility. The latency 438 of the N100 peak decreases with increasing speech intelligibility for the Matrix sentences, while the 439 latency remains unchanged for the story. A latency decrease with increasing speech intelligibility, 440 similar to the Matrix sentences, has been reported in literature by Petersen et al. (2017) and Kong 441 et al. (2014), but is not supported by Ding and Simon (2012). This different pattern between the 442 Matrix sentences and the story could be explained by two factors. (1) Top-down processing: This 443 is present for the story the entire time, for the Matrix sentences, on the other hand, it increases 444 with increasing noise level. Top-down processing requires more time, which could result in delayed 445 TRFs. (2) Attention: Listening to concatenated Matrix sentences might be boring, especially when 446 speech intelligibility decreases, which could result in attention loss and less listening effort known 447

to delay neural processing of speech (Ding and Simon, 2012; Kong et al., 2014; Petersen et al.,
2017; Vanthornhout et al., 2019).

A last result to point out is the positive peak around 300 ms for the Matrix sentences at -9.5 dB SNR 450 (SI=49%) (Figure 6). P300 can occur when a participant tries to detect a target stimulus (Picton, 451 1992, 2011). As the Matrix sentences do not contain semantic context, which makes content 452 453 questions not possible, counting questions were asked at every SNR trial, for example, 'Which 454 colors of boats were mentioned?'. We hypothesize that the question type, content questions for the story versus counting questions for the Matrix sentences, accounts for this P300 difference. As a 455 consequence, the type of questions to ask is also an important factor to take into account for future 456 research. 457

458 4.4 Implications for the objective measure of speech intelligibility

459 In this study we showed that the objective measure of speech intelligibility by Vanthornhout et al. (2018) using Matrix sentences can also be conducted with natural speech as a stimulus. This 460 paves the way towards intelligibility measurements of any speech fragment, which is impossible 461 today using behavioral measurements but may relate better to everyday communication and would 462 be beneficial for clinical applications. In addition, we found an enhancement in neural envelope 463 tracking when using natural speech as a stimulus instead of Matrix sentences. This suggests that 464 neural envelope tracking might reflect the integration of incoming acoustic features and top-down 465 information, which indicates that the choice of the stimulus has to be considered based on the 466 intended purpose of the measurement. To conduct research, for example, and investigate neural 467 speech processing in noise, a story could be an interesting choice as neural envelope tracking is more 468 pronounced because of better sustained attention, more listening effort and/or semantic processing. 469 However, when comparing speech intelligibility outcomes in a clinical setting, for example to fit 470 hearing aids, top-down processing effects are undesired and should be ruled out and the Matrix 471 sentences could be used instead. 472

473 **4.5 Conclusion**

We found increasing neural envelope tracking with increasing speech intelligibility for both stimuli with an additional enhancement for natural speech compared to Matrix sentences. These results show (1) the feasibility of natural speech as a stimulus for the objective measure of speech intelligibility, (2) that neural envelope tracking is enhanced using a story compared to Matrix sentences and (3) that noise and the stimulus type can change the temporal characteristics of the brain responses.

Speechmaterial	Filter band	Correlation	p-value
Matrix sentences	Delta (0.5-4 Hz)	0.62	p<0.001
Natural story	Delta (0.5-4 Hz)	0.59	p<0.001
Matrix sentences	Theta (4-8 Hz)	0.46	p<0.001
Natural story	Theta (4-8 Hz)	0.41	p<0.001

Table 1. Spearman rank correlation between neural envelope tracking and speech understanding

Table 2. Linear Mixed Effect Model of envelope reconstruction in function of SI

Linear mixed effect model (factor)	beta value	CI(95%)	p-value
Fixed effect SI	$1.08 \ge 10^{-3}$	\pm 1.90 x 10 ⁻⁴	p<0.001
Fixed effect stimulus	$1.97 \ge 10^{-2}$	\pm 1.49 x 10 ⁻²	p=0.010
Fixed effect band	-3.87 x 10 ⁻²	\pm 1.41 x 10 ⁻²	p<0.001
Interaction effect SI:stimulus	-1.74 x 10^{-4}	\pm 2.39 x 10^{-4}	p=0.155
Interaction effect SI:band	-4.43 x 10 ⁻⁴	\pm 2.14 x 10 ⁻⁴	p<0.001
Interaction effect SI:band:stimulus	-1.28 x 10 ⁻⁵	$\pm 2.25 \text{ x } 10^{-4}$	p=0.912

Speech Intelligibility (SI), Confidence Interval (CI)

Linear mixed effect model (factor)	beta value	CI(95%)	p-value
Fixed effect SNR	$7.75 \ge 10^{-3}$	$\pm 1.39 \text{ x } 10^{-3}$	p<0.001
Fixed effect stimulus	-1.25 x 10^{-2}	$\pm 1.06 \text{ x } 10^{-2}$	p=0.022
Fixed effect band	-8.10 x 10^{-2}	$\pm 1.06 \text{ x } 10^{-2}$	p<0.001
Interaction effect SNR:stimulus	$-1.01 \ge 10^{-3}$	\pm 1.83 x 10 ⁻³	p=0.284
Interaction effect SNR:band	$-3.20 \ge 10^{-3}$	\pm 1.83 x 10^{-3}	p<0.001
Interaction effect SNR:band:stimulus	-1.40 x 10 ⁻⁶	$\pm 2.13 \text{ x } 10^{-3}$	p=0.999

Table 3. Linear Mixed Effect Model of envelope reconstruction in function of SNR

Speech-to-Noise Ratio (SNR), Confidence Interval (CI)

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