Title: Thalamic state influences timing precision in the thalamocortical circuit

Abbreviated Title: Thalamic state influences thalamocortical timing

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Abstract

Sensory signals from the outside world are transduced at the periphery, passing through

thalamus before reaching cortex, ultimately giving rise to the sensory representations that

enable us to perceive the world. The thalamocortical circuit is particularly sensitive to the

temporal precision of thalamic spiking due to highly convergent synaptic connectivity.

Thalamic neurons can exhibit burst and tonic modes of firing that strongly influence timing

within the thalamus. The impact of these changes in thalamic state on sensory encoding in

the cortex, however, remains unclear. Here, we investigated the role of thalamic state on

timing in the thalamocortical circuit of the vibrissa pathway in the anesthetized rat. We

optogenetically hyperpolarized thalamus while recording single unit activity in both thalamus

and cortex. Tonic spike triggered analysis revealed temporally precise thalamic spiking that

was locked to white-noise sensory stimuli, while thalamic burst spiking was associated with a

loss in stimulus-locked temporal precision. These thalamic state dependent changes

propagated to cortex such that the cortical timing precision was diminished during the

hyperpolarized (burst biased) thalamic state. While still sensory driven, the cortical neurons

became significantly less precisely locked to the white-noise stimulus. The results here

suggest that tonic thalamic spiking is more temporally precise than burst firing, which leads to

distinct differences in sensory information representation at the level of both the thalamus and

the cortex, as assessed using spike triggered analysis. This difference in spike timing precision

enables a dynamic encoding scheme for sensory information as a function of thalamic state.

New and Noteworthy

The majority of sensory signals are transmitted through the thalamus. There is growing evidence of complex thalamic gating through coordinated firing modes that have a strong impact on cortical sensory representations. Optogenetic hyperpolarization of thalamus pushed it into burst firing that disrupted precise time-locked sensory signaling, with a direct impact on the downstream cortical encoding, setting the stage for a timing-based thalamic gate of sensory signaling.

Introduction

Sensory thalamus plays a critical role in gating information flow from sensors in the periphery to cortex, ultimately shaping how we perceive the world. Importantly, thalamic gating properties are not static, but instead vary dynamically through a range of modulatory mechanisms, including local membrane and synaptic properties (Wolfart et al., 2005), stimulus history (Whitmire et al., 2016), and neuromodulatory inputs (Castro-alamancos, 2002; Mease et al., 2014). Although arising from different mechanisms, these modulatory inputs have the net effect of altering the baseline membrane polarization level in the thalamus, referred to here as "thalamic state", which plays an important role in determining the encoding properties of the thalamic neurons that serve as primary inputs to sensory cortex. Perhaps most prominently, modulation of the baseline membrane potential in thalamic neurons enables distinct tonic and burst firing modes due to the selective engagement of low threshold calcium channels during prolonged hyperpolarization (Suzuki and Rogawski, 1989). It has long been posited that these two firing modes could dynamically control information processing (Sherman 2001), but the precise way in which this could happen has remained speculative and the way in which cortical coding properties are shaped is unknown.

Although the large majority of studies of T-type calcium channel bursts in thalamus have been focused on the underlying detailed biophysical mechanisms enabled by brain slice recordings, there have been a number of investigations of the intact circuitry in-vivo. At the thalamocortical synapse, in-vivo studies have shown that spontaneous burst spikes are more effective at driving cortical spiking (Swadlow and Gusev, 2001) and evoke larger cortical depolarizations (Bruno and Sakmann, 2006) than tonic spikes. The in-vivo properties of burst and tonic spiking have been explored perhaps most extensively in the visual pathway (Alitto et al., 2005; Denning and Reinagel, 2005; Lesica and Stanley, 2004; Reinagel et al., 1999; Wang et al., 2007), with burst firing shown to be reliably elicited across trials in response to visual stimulation (Lesica and Stanley, 2004; Martinez-Conde et al., 2002; Wang et al., 2007), associated with an "all-or-none" type of response to facilitates detection of changes in the visual scene (Lesica and Stanley, 2004) consistent with mechanisms that would serve as a

"wake-up call" to cortex (Sherman, 2001). Furthermore, although historically controversial, it

has been shown in a number of studies that thalamic bursting is not just observed in sleep

states or under anesthesia, but is present, albeit reduced, in the awake brain (Borden et al.,

2019; Guido and Weyand, 1995; Whitmire et al., 2016). However, the implication for

downstream cortical encoding remains elusive because of the complexity of the

thalamocortical circuitry. It has been estimated that 50-100 thalamic neurons converge as the

primary drivers of a single cortical neuron (Bruno and Sakmann, 2006), where the concerted

effort of a relatively large number of synaptic inputs is needed to drive suprathreshold cortical

activity. Without a mechanism to manipulate the population activity of thalamic neurons

converging on a common cortical target independent of the sensory drive, the role of

tonic/burst firing in driving downstream cortical activity remains elusive.

To address this, we used optogenetic manipulation of thalamic state to systematically

bias the thalamic population towards a burst firing regime to quantify the role of thalamic state

on precise timing of spiking activity in the thalamocortical circuit of the rodent whisker pathway

using a two-stage, linear-nonlinear framework. The first stage represents the sensory feature

selectivity, and the second stage represents the overall sensitivity of the input-output

relationship (Estebanez et al., 2012; Petersen et al., 2008; Ramirez et al., 2014). This

characterization was performed for neurons recorded extracellularly in the ventro posterior-

medial (VPm) thalamus and in primary somatosensory cortex (S1) in the fentanyl-anesthetized

rat, for both first order (spike-triggered average) and higher order (spike-triggered covariance)

selectivity. For thalamic neurons, we found that tonic spiking was associated with whisker-

stimulus feature selectivity consistent with previous findings (Petersen et al., 2008). However,

analysis of burst firing suggested that while bursting activity was clearly sensory driven, the

spike-triggered analysis revealed a lack of precise stimulus-locked spiking in response to

white-noise whisker stimulation. This was further confirmed using optogenetic

hyperpolarization of VPm to switch the thalamus into a burst mode. In the cortical neurons,

when the thalamus was dominated by tonic firing, the cortical neurons exhibited similar feature

selectivity as observed in VPm. However, when the thalamus was optogenetically

hyperpolarized, the spike-triggered analysis revealed a reduction in precise stimulus-locked

spiking in S1 units in response to the white-noise whisker stimulus, yet maintained a consistent

overall stimulus-driven firing rate. Given the sensitivity of the cortex to precise timing of

thalamic projection neurons, these results suggest that shifts in thalamic state disrupt precise

timing of thalamic inputs to cortex that are compensated for by the potency of the thalamic

bursts, setting the stage for a timing-based gating of information flow to cortex.

Methods

Experimental Procedures

Acute Surgery: All procedures were approved by the Georgia Institute of Technology Institutional Animal Care and Use Committee and were in agreement with guidelines established by the National Institutes of Health. 19 female albino rats (Sprague-Dawley, 250-300g) were anesthetized intravenously using a fentanyl cocktail (fentanyl (5 µg/kg), midazolam (2 mg/kg), dexmedetomidine (150 µg/kg)). A craniotomy was performed over VPm (2-4 mm caudal to bregma, 1.5-3.5 mm lateral to the midline), and in a subset of animals, a second craniotomy was performed over S1 (1-3 mm caudal to bregma, 4.5-6 mm lateral to the midline). At the termination of the experiment, the animal was euthanized with an overdose of sodium pentobarbital (euthasol, 0.5 mL at 390 mg/mL). All optogenetically transfected animals that underwent cortical probe recordings were perfused and their brains were imaged for verification of opsin location and cortical probe location.

Electrophysiology: Tungsten microelectrodes were lowered into the thalamus (depth: 4.5-6 mm) using a micropositioner (Kopf, Luigs-Neumann). Multielectrode probes (A1x32-10mm-50-177, NeuroNexus) were lowered perpendicular to S1 (45° relative to vertical; depth: 2 mm). The topographic location of the electrode was identified through manual stimulation of the whisker pad. Upon identification of the primary whisker for the recorded unit(s), the primary whisker was threaded into the galvo motor to permit stimulation of a single whisker.

Sensory Stimulus: Mechanical whisker stimulation was delivered using a precisely controlled galvo motor (Cambridge Technologies, custom Matlab software). The mechanical stimulus applied to the whisker in the rostral-caudal direction consisted of sensory white-noise (low pass filtered at 200 Hz, standard deviation of the noise was 0.6° or 223°/s). Feedback from the whisker stimulator were used for further spike triggered analysis across all units (down sampled to 4.88 kHz).

Optogenetics surgeries: All surgical procedures followed sterile protocol. A small craniotomy was made above VPm (3 mm lateral, 3 mm caudal to bregma). A 10 µL syringe (Neuros Syringe, Hamilton, Inc) filled with the virus (rAAV5-CamKIIa-Jaws-KGC-GFP-ER2 or rAAV5-CamKIIa-eNpHR3.0-EYFP, UNC Viral Vector Core Services) was lowered to depth of 5.2 mm before injecting 1 µL of virus at a rate of 0.2 µL/min (iSi system, Stoelting). The syringe remained in place for five minutes after the injection was complete to allow the virus to diffuse. Opsin expression was fully realized at 2-3 weeks post-surgery.

Optogenetic Stimulus: Optical manipulation was administered with a controlled pulse of light through a custom optrode consisting of an optical fiber (200µm diameter; Thorlabs) and an electrode (Tungsten microelectrode; FHC) that was lowered into the VPm. Upon identifying a whisker sensitive cell, light sensitivity was assessed by the post-inhibitory rebound spiking response using a train of 250 millisecond light pulses (λ = 590 or 617nm for Halorhodopsin and Jaws, respectively). The whisker was then stimulated without (baseline) and with (hyperpolarized) light provided directly to the thalamus (50 mW/mm^2). Optogenetic stimulus conditions (light on/hyperpolarized, light off/baseline) were interleaved to avoid long-term adaptation effects.

Analytical Methods: Spike sorting for single channel recordings was performed online and validated offline using Waveclus (Quiroga et al., 2004). Spike sorting for multichannel electrodes was performed offline using the KlustaKwik software suite (Rossant et al., 2015). Isolation of the unit was confirmed by the waveform amplitude (absolute and relative to the background noise >3) and the interspike-interval distributions (VPm: mean of 0.22%, S1: mean of 0.38% of spikes in absolute refractory period of 1ms).

Although spike-triggered analysis for exploration of feature selectivity has been utilized widely in the thalamocortical circuit of the visual (Butts et al., 2007; Jones and Palmer, 1987; Lesica and Stanley, 2004; Reid and Alonso, 1995) and auditory (Eggermont et al., 1983; Theunissen et al., 2000) pathway , the application of this approach in the somatosensory pathway has

141   been limited to a fairly small number of studies across thalamus (Petersen et al., 2008) and

142   cortex (Estebanez et al., 2012; Maravall et al., 2007; Ramirez et al., 2014).   Here we

143   implemented spike-triggered analysis across VPm thalamus and S1 cortical layer 4.

144   Specifically, feature selectivity was first estimated for each recorded unit using a simple spike

145   triggered average (STA) (Schwartz et al., 2006).

$$146 \qquad STA = \frac{1}{N} \sum_{j} s(t_j)$$

Where N is the number of spikes and s is the stimulus segment in a window surrounding each

spike (-30 to +5 ms, spike-triggered ensemble). The burst and tonic triggered averages were

computed from burst and tonic spikes, respectively. Burst spikes were classified here from the

extracellular recordings as two or more spikes with an inter-spike interval of less than four

milliseconds with the first spike in the burst preceded by 100 milliseconds of silence. The

baseline/hyperpolarized condition triggered averages were computed from all spikes in a

given stimulus condition. The bootstrap estimate of the confidence intervals on the spike

triggered average was computed as the +/- 2 standard deviation of the shuffled STA

distribution across 500 repetitions (Schwartz et al., 2006). Note that we implemented multiple

techniques of estimating the feature selectivity of the neurons including spike triggered

covariance, generalized linear models, and nonlinear-input models (McFarland et al., 2013).

The results were qualitatively consistent across all methods employed, so we chose to use

spike triggered average throughout the manuscript due to its simplicity.

The signal-to-noise ratio of the recovered STA was quantified as the peak-to-peak amplitude

of the STA within 10 milliseconds of the spike (where the significant filter activity is contained)

divided by the peak-to-peak amplitude of the STA from 30 to 20 milliseconds before the spike

(where there is no expected filter information). An SNR value of 1 means the amplitude of the

STA near the spike time is not different from the amplitude of the noise fluctuations. Therefore,

any units with an SNR value less than 2 were excluded from further analysis.

There was significant diversity in the resultant STA structure across recorded neurons.

Utilizing the approach of Estebanez et al. to make comparisons of the feature selectivity across

the population of recorded neurons, we conducted a principle components analysis of the

recovered STA (Estebanez et al., 2012). The first two principle components accounted for the

majority of the variance (71.8% VPm, 78.4% S1), and were interpreted as representative of

the primary structure in the sensory input relevant for spiking in the population.

The STA represents structure in the sensory input that is captured in the mean across spiking

activity, and cannot capture any structure that may be in higher order statistical properties of

the stimulus. Spike-triggered covariance (STC) can also be calculated as an alternative, as

an attempt to uncover high-order structure in the sensory stimulus that is associated with

neuronal firing (Estebanez et al., 2012). Note that while implemented in this analysis, STC

analysis of both VPm and S1 neurons did not reveal significantly different structure for the

neurons recorded under our experimental conditions, and are thus not shown here, and even

more importantly, this analysis did not reveal a shift in feature selectivity across thalamic

states.

The non-linearity ($P(spike|y)$) was estimated as the ratio of the probability of spike-triggered

stimuli ($P(y|spike)$) to the probability of any stimulus segment in the stimulus ($P(y)$) multiplied

by the mean firing rate of the neuron($P(spike)$) (Schwartz et al., 2006):

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$$p(spike|y) = p(spike)\frac{p(y|spike)}{p(y)}$$

Where y is defined as the stimulus (s) convolved with the feature selectivity of the unit (STA)

(Lesica et al., 2007), referred to as filtered stimulus. Because the slope of the static non-

linearity is determined by the separation between the spike triggered ensemble and the

Gaussian distributed white-noise, as the spike triggered ensemble distribution becomes more

selective (i.e. the mean moves away from the filtered stimulus distribution), the separability of

the distributions increases, and the slope of the non-linearity also increases. Intuitively, this

means that the shape of the non-linearity gives an estimate of the separability of the spike

triggered ensemble and the stimulus distribution, or how strongly tuned a neuron is for that

particular feature, given by the STA. A steeper slope in the non-linearity suggests a stronger

tuning than a shallower slope. Therefore, we also assessed the spiking nonlinearity as a

function of the spike classification. For all conditions, the best estimate of the STA was defined

as tonic spike triggered average for thalamic units and the baseline thalamic state (i.e. not

optogenetically manipulated) for the cortical units. Throughout the manuscript, we separate

the firing rate (p(spike)) from the shape of the non-linearity (p(y|spike)/p(y)) to avoid

confounding differences in firing rate with differences in tuning.

The precision in the noise evoked firing was estimated for each spike classification (tonic,

burst, baseline, hyperpolarized). The precision was defined as:

202
$$precision = \frac{\sum_{-1}^{+1} \tau_{jitter}}{\sum_{-\infty}^{\infty} \tau_{jitter}}$$

203 Or the number of spikes with τ_{jitter} values of +/- 1 ms duration normalized by the total number

204 of spikes. τ_{jitter} is defined for each spike as the temporal lag (t_{lag}) for the peak correlation

205 between the STA and the stimulus segment surrounding that spike (-30 ms to +5 ms).

206
$$\tau_{jitter} = arg \frac{max}{t_{lag}} correlation\left(STA, s(t_j)\right)$$

207 The τ_{jitter} distribution was normalized by the total number of spikes in each condition (tonic,

208 burst, baseline, hyperpolarized).

209 All pairwise statistical comparisons were computed using a Wilcoxon signed rank test unless

210 otherwise noted.

Results

Spike triggered analysis in the thalamus and cortex

We recorded thalamic and cortical extracellular spiking activity in response to sensory white-noise stimulation of a single whisker in the vibrissa pathway of the fentanyl-cocktail anesthetized rat to enable long-duration, controlled measurements needed for precise estimates of feature selectivity (Figure 1A, see Methods). We estimated the feature selectivity for each unit as the spike triggered average (STA), which captures the features of the sensory stimulus that tended to precede spiking, and the static, point nonlinearity, which captures the translation into suprathreshold spiking activity (Figure 1B; see methods). Although this quantification was performed on longer unique noise segments, we also recorded the response to short (4-10 second) frozen white-noise segments to examine the response across trials. Figure 1C shows an example recording from a simultaneously recorded pair of neurons in topographically aligned regions of the thalamus (left column, ventral posteromedial nucleus, VPm) and cortex (right column, primary somatosensory cortex, S1) in response to the repeated presentation of a single frozen white-noise segment (top of each column). Across trials, the repeatability of the response to the noise stimulus is apparent in the raster plot, with clear vertical patterns across trials. Spike-triggered analysis has been widely utilized in studying feature selectivity in the visual (Butts et al., 2007; Jones and Palmer, 1987; Lesica and Stanley, 2004; Reid and Alonso, 1995) and auditory (Eggermont et al., 1983; Theunissen et al., 2000) pathway, but has been utilized in the somatosensory pathway in only a relatively small number of studies (Estebanez et al., 2012; Maravall et al., 2007; Petersen et al., 2008; Ramirez et al., 2014). Here, to explore the feature selectivity of these recorded neurons, the spike-triggered average (STA) was computed for the thalamic and cortical unit for stimulus segments from -30 milliseconds prior to the spike to +5 milliseconds afterwards at a 0.2ms resolution (Figure 1C, bottom). The VPm STA shows clear feature selectivity in the 10-15 milliseconds prior to the thalamic spike as evidenced by the large amplitude of the STA relative to the shuffled case (grey confidence intervals). Beyond 15 milliseconds prior to the spike, the

VPm STA is essentially flat and within the confidence bounds on the shuffled process. This suggests that, on average, the thalamic unit is only sensitive to the stimulus occurring in the previous 10-15 milliseconds. The S1 unit also displays feature selectivity as evidenced by the shape and amplitude of the S1 STA immediately prior to the cortical spike relative to the shuffled case. Although the VPm STA is nearly ten times as large in amplitude as the S1 STA, the similarity in the temporal dynamics can be visualized by shifting the VPm STA by 2 milliseconds relative to the S1 STA (Figure 1C, bottom, S1 STA black, VPm STA shifted by 2 milliseconds and scaled by a factor of 0.1 as grey dashed line).

While this simple comparison provides an interesting observation for a single pair of topographically aligned neurons, we also made comparisons of the feature selectivity across the population of recorded STAs for thalamus and cortex. First, we visualized the shape of the spike triggered average for a sample of example thalamic (Figure 1D left; greyscale) and cortical (Figure 1D right; greyscale) units. These STA filters cannot be simply averaged together to give an estimate of the population filter due to differences in the phase and directionality of the recovered STA across different recorded units. Instead, utilizing an approach from Estebanez et al., we performed a principle component analysis on the set of recovered thalamic and cortical STA filters across recordings to identify salient filter properties that generalized (Figure 1E, Estebanez et al., 2012). The first two principle components for the spike triggered averages of both thalamus and cortex explain the majority of the variance for the set of recovered filters, similar to what has been seen previously for cortex (Estebanez et al., 2012). Furthermore, a simple time shift of 2.5 milliseconds for the VPm principle components relative to the S1 principle components (Figure 1F, dashed lines) demonstrates the similarity in the STA subspace spanned by these principle components. It seems that despite not necessarily being recorded simultaneously or even in the same animal, there is a high degree of overlap in the low dimensional subspace of feature selectivity for thalamocortical neurons in the whisker pathway. Note that we further analyzed the spike triggered covariance (STC) for the same data and found that the subspace spanned by the

265 recovered linear filters matched the subspace estimated using the linear filters recovered

266 using STA, thus not revealing any higher-order feature selectivity in the data.

Figure 1: Spike-triggered analysis in the thalamocortical circuit of the rat whisker pathway. A. Experimental paradigm. B. Feature selectivity is assessed from the neural response to sensory white-noise as the spike triggered average and the associated point nonlinearity. C. Top: Example noise evoked response from simultaneously recorded topographically aligned pair of neurons. Bottom: Recovered STA for the example units. The black dotted vertical line indicates the time of the spike. D. Representative example thalamic and cortical STA (grey shades indicate different units). E. First two principle components computed using principle component analysis (PCA) of all recovered STA for thalamic neurons (n = 30) and cortical neurons (n = 32). F. Overlay of cortical STA PCs and temporally shifted thalamic PCs (shift of 2.5ms).

    Tonic and burst spike triggered analysis in thalamus

Inherent in the spike triggered analysis, however, is an assumption that the average

filter is representative of the sensory stimulus preceding all spikes (Stanley, 2002). Yet

neurons in the thalamus are well known for exhibiting two fundamentally different types of

firing: tonic spiking and burst firing mediated through T-type calcium channels (Suzuki and

Rogawski, 1989). Burst spikes were classified here from the extracellular recordings as two

or more spikes with an inter-spike interval of less than four milliseconds with the first spike in

the burst preceded by 100 milliseconds of silence (Figure 2A, see methods). Using this

classification, we asked if or how the feature selectivity of an individual thalamic unit changes

as a function of the spiking mechanism in the whisker pathway.

In the thalamic recordings, tonic and burst spikes were interspersed throughout most

of the recordings. For the example thalamic unit presented in Figure 1B, we computed the

spike triggered average from all spikes (STA), the tonic spike triggered average from only tonic

spikes (tSTA), and the burst spike triggered average from only spikes that are classified as

being part of a burst (bSTA) (Figure 2B). The tSTA (grey) closely resembles the STA

computed from all spikes (black) while the bSTA (red) is significantly degraded as evidenced

by the flat shape of the filter. To compare the difference between burst and tonic feature

selectivity across thalamic units, we quantified the signal-to-noise ratio of the STA (STA_{SNR},

see methods). Across all thalamic units, the STA_{SNR} was higher for tonic spikes ($tSTA_{SNR}$) than

for burst spikes ($bSTA_{SNR}$) (Figure 2C). Note that again we calculated the STC under these

conditions and found the same result that the STC_{SNR} was higher for tonic spikes than for burst

spikes ($p = 2e-4$), and that there was not a fundamental shift in representation between tonic

and burst spiking.

If the timing of spikes within a burst is not repeatable and structured, the presence of

these additional spikes will serve to destroy the temporal structure in the feature selectivity as

revealed by the spike triggered analysis. When the bSTA was computed from only the first

spike in each burst (Figure 2B, red-dashed line), there was no apparent feature selectivity for

this example unit. This can also be visualized across units in the STA_{SNR} where the $bSTA_{SNR}$

is plotted when computed from all burst spikes (black dot) and when computed from the first

spike in each burst (red circle, Figure 2C). Therefore, including all spikes in a burst (or not)

does not strongly impact the ability to estimate the feature selectivity from the STA.

Given the estimated feature selectivity, we can compute the static non-linearity, or the

input-output function, which provides a mapping between this filtered stimulus (y) and the

spiking response of the neuron (p(spike|y)) by taking the ratio of the p(y|spike) to the p(y)

(Figure 1B, see methods). Here, we used the tSTA as the filter for all spiking conditions when

estimating the non-linearity. The probability of the filtered stimulus (p(y) remains unchanged

when the filter is held constant. Therefore, any change in the non-linearity is then only due to

changes in the probability of the filtered stimulus given that a spike occurred (p(y|spike)), or

the spike triggered ensemble. In this example unit, we found that the tonic spikes were well

tuned to the STA, as evidenced by the steep slope of the non-linearity while the burst spikes

were not well tuned to the STA, as evidenced by the relatively flat non-linearity (Figure 2D).

This trend was consistent across units where the burst spikes showed reduced tuning to the

STA as compared to tonic spikes as assessed by the slope of the spiking nonlinearity (Figure

2E). Here, we have separated the difference in the slope of the non-linearity from the

difference in the prevalence of burst and tonic spikes (p(spike) or firing rate), which is markedly

higher for tonic spikes than for burst spikes (Figure 2F). Furthermore, we tested alternative

burst spike classifications and quantified the implication for the STA (Figure 2G, top). Across

spiking classifications, increased periods of silence prior to the spike ($t_{silence}$) led to decreased

STA_{SNR} while bursts of spikes (t_{isi}<4 or <10) had consistently lower STA_{SNR} relative to tonic

spikes (t_{isi}>20) (Figure 2G, example unit in middle, population data in bottom). This suggests

that any tonic spiking incorrectly classified as part of a burst would serve to increase the

amplitude, and thus the SNR, of the burst-triggered average, but the conservative definition of

a burst pattern that we have used here likely minimizes this effect. Therefore, our data

suggests a reduction in stimulus selectivity for burst spiking perhaps not due to a true loss of

feature selectivity but instead due to the analytical framework which requires neurons having

a high temporal precision relative to the timescale of the stimulus features.

Figure 2: Spike triggered analysis of burst and tonic spikes in thalamic neurons. A. Burst definition. B. STA from thalamic unit presented in Figure 1 estimated from all spikes (black solid line, n = 44105 spikes), tonic spikes (tSTA; grey solid line, n = 36558 spikes), a subsample of tonic spikes (tSTA; dashed line, n = 2363 of 36558 spikes) all burst spikes (bSTA; red solid line, n = 7547 spikes), and the first spike in the burst (bSTA; red dashed line, n = 2363 spikes). C. STA$_{SNR}$ across recorded population (n = 30 units). Black dots depict the STA$_{SNR}$ for all bSTA computed from all burst spikes while red circles indicate the STA$_{SNR}$ for bSTA computed from only the first spike in the burst (p = 1e-6). Arrow depicts example unit in A. D. Example unit tonic and burst spike nonlinearity. E. Average non-linearity across all units. F. Burst and tonic firing rate (p(spike)) across recorded population (p = 2.6e-5). G. Spike triggered average using different spike classifications (Bottom plot: n = 30 thalamic units).

Optogenetic manipulation of thalamic state

The previous analysis was conducted by presenting sensory white-noise stimuli and

parsing measured thalamic spiking activity into tonic and burst classes, while these classes of

spiking were intermingled throughout the recordings. However, the thalamus was in tonic firing

mode, with relatively low burst firing rates (Figure 2F). Here, we used optogenetic

hyperpolarization of the thalamic neurons not to silence the thalamic neurons, but instead to

shift the thalamus into a burst firing mode during sensory white-noise stimulation (Figure 3A).

Using this optogenetic manipulation, we asked whether the optogenetically manipulated firing

mode (baseline and hyperpolarized conditions) of the thalamus impacts encoding and how

this relates to the classified burst/tonic modes.

Here, we recorded the thalamic response to sensory white-noise with and without the

presence of a light stimulus (hyperpolarized and baseline conditions, respectively). We found

no significant change in the thalamic firing rate between hyperpolarized and baseline

conditions (Figure 3B), but the firing mode of the thalamus did shift towards burst firing

(baseline burst ratio = 0.16 ± 0.15, hyperpolarized burst ratio = 0.36 ± 0.27, n = 10 units, Figure

3C). Interestingly, the mean firing rate in VPm in response to sensory white-noise was not

significantly different between the baseline and hyperpolarized conditions, reflecting a

"replacement" of tonic firing with burst firing. It is also is apparent that the bursts in the baseline

and hyperpolarized conditions are not occurring at similar times, despite a common sensory

drive, suggesting some differences in the stimulus properties to which the bursts are sensitive

across the two conditions. Bursts in the hyperpolarized condition showed a similar number of

spikes per burst (Figure 3D) with a shorter inter-spike interval within a burst (Figure 3E). For

an example unit, we have plotted the spiking response to a frozen white-noise segment without

optogenetic stimulation (Figure 3F, baseline condition) and with optogenetic stimulation

(Figure 3F, hyperpolarized condition). We have pseudo-colored the tonic spikes grey and the

burst spikes red to qualitatively visualize the thalamic firing mode (Figure 3F). In the baseline

condition, the response is primarily tonic as evidenced by the grey raster plots (Figure 3F,

Baseline, BR = 0.10). In the hyperpolarized condition (optically stimulated), the firing mode is

biased towards a burst encoding scheme, as evidenced by the prevalence of red burst spikes

(Figure 3F, Hyperpolarized, BR = 0.67). The tonic STA showed pronounced feature selectivity

for this unit while the burst STA did not (Figure 3G top), consistent with the earlier findings

reflective of the loss in timing precision for the first spike of a burst (Figure 2). In the

optogenetically manipulated states, the baseline STA has prominent feature selectivity while

the hyperpolarized condition is much smaller in amplitude (Figure 3G bottom). Qualitatively,

we can see that the STA from the hyperpolarized condition reflected the STA obtained from

the burst spiking in the previous analysis. Again, a subsequent analysis of the STC revealed

representations that were redundant with the spike-triggered average, and no apparent shift

in feature selectivity between the tonic and burst firing modes.

The similarity between the burst spike response and hyperpolarized condition can also

be seen in this example nonlinearity where the burst and hyperpolarized nonlinearities are

effectively flat while the tonic spikes and baseline condition show obvious tuning (Figure 3H).

Across units, we found an overall reduction in the STA_{SNR} for the hyperpolarized condition

relative to the baseline condition (Figure 3I, $p = 0.037$). We also found that the tuning of the

nonlinearity was lower for the hyperpolarized condition relative to the baseline condition as

reflected in the overall gain/slope (Figure 3J). Importantly, the baseline and hyperpolarized

conditions both contain burst and tonic spikes. Instead of completely separating the firing

modes into all burst spikes or all tonic spikes, we have optogenetically altered the spiking

probabilities such that the baseline condition has more tonic spikes and the hyperpolarized

condition has more burst spikes (Figure 3C) while maintaining similar numbers of spikes

(Figure 3B). The similarities between the STA and the NL properties of the burst and

hyperpolarized state as well as the tonic and baseline state suggest that there was no

discernable difference for the estimation of feature selectivity when assessed based on the

state of the thalamus at the time of the stimulus (hyperpolarized/baseline) versus the spike

type classification (burst/tonic).

Figure 3: Optogenetic Manipulation of Thalamic State. A. Experimental paradigm. Scale bar: 1 mm. YFP signal (green) shows injection site in thalamus and axonal projections in cortex. B. Baseline and hyperpolarized firing rate (p(spike)) across recorded population (n = 10 units. p>0.05). C. Characterization of the burst ratio (p = 0.021), D. the spikes per burst (p>0.05), and E. the within burst ISI (p=0.021) during baseline and hyperpolarized conditions across the population of thalamic units (n = 10 units). F. Example thalamic response to frozen white-noise segments without (baseline) and with (hyperpolarized) optogenetic stimulation. Tick marks in raster plot are pseudocolored to demonstrate classification as burst (red tick) or tonic (grey tick) spikes. G. Spike triggered average computed as a function of spike classification (burst/red, first spike in burst/red dashed, tonic/grey) or thalamic state (baseline/black, hyperpolarized/yellow). H. Example unit tonic/burst and baseline/hyperpolarized spike nonlinearity. I. STA_SNR across recorded population (n = 10 units). J. Average non-linearity across all units (n = 10 units).

<u>Temporal precision of thalamic firing modes</u>

Given the difference between the recovered estimates of burst/hyperpolarized and

tonic/baseline feature selectivity and the implications for timing precision in the thalamocortical

circuit, we implemented a series of computational controls to identify any potential

shortcomings of the methodologies that could underlie these results.

The first issue we considered was the overall difference in spike rates. Spike triggered

analyses require a large number of spikes to effectively estimate the underlying selectivity.

The proportion of spikes classified as bursts was lower than the spikes classified as tonic

(Figure 2F) as quantified by the burst and tonic firing rate. Therefore, it was possible that we

could not recover an STA for the burst spike condition due to the reduced number of burst

spikes relative to tonic spikes. In an example unit, we computed the tSTA using only a subset

of the spikes (n = 2363 of 36558 spikes corresponding to n = 2363 bursts with n = 7547 burst

spikes) and found that the linear filter was essentially identical to the tSTA (Figure 2B, grey

dashed line). We computed this for all thalamic units and again found that the burst-count

matched tSTA was also significantly larger than the bSTA. Furthermore, there was no

statistically significant difference in the firing rate between the baseline and hyperpolarized

optogenetic conditions (Figure 3G), but still the difference in the STA persisted. This suggests

that simple spike counts alone were insufficient to explain the difference in the tonic/baseline

STA and the burst/hyperpolarized STA.

The second issue we considered was the inherent assumption that the feature

selectivity for each unit could be recovered as the STA. It was possible that the burst STA was

not recoverable because the burst firing mode was better estimated by a symmetric

nonlinearity and therefore the filter could only be recovered using spike triggered covariance

(STC) techniques. The STC approach has been previously implemented in the vibrissa

pathway (Estebanez et al., 2012; Maravall et al., 2007; Petersen et al., 2008), revealing

potential feature selectivity not captured with STA in some conditions, and was therefore

important to consider here. We therefore computed the STC for all recorded thalamic units

and compared this for each spiking condition. Although the dataset was more limited because

the number of units with a significant STC filter was lower than those with a significant STA

filter (n = 13 units with STC filter compared to n = 30 units with STA filter), the same trends

regarding the reduction in the amplitude of the filter (STC_{SNR}) and the slope of the symmetric

nonlinearity persisted (as described in results). Therefore, this suggests that the method of

extracting the feature selectivity (STA compared to STC) was insufficient to explain the inability

to estimate the feature selectivity in the hyperpolarized/burst spiking conditions. However, it is

also possible that the feature selectivity for a given neuron shifts to a higher-order space as

firing modes transition from tonic to burst firing. If the burst firing could be associated with

higher-order structure in the sensory stimulus, it may only be revealed using STC analysis.

We thus conducted a STC analysis of the recorded neurons. First, we found that the tonic

STA_{SNR} was significantly larger than the burst STC_{SNR} (p = 3e-6), suggesting that the feature

selectivity did not simply shift from the first order estimate of the STA to higher order

representations captured by the STC. Then we assessed the probability that a unit with a

significant filter, as assessed using STA, also showed a significant filter, as assessed using

STC. We found that all 13 units with significant filters also showed significant STA filters. This

emphasizes the complexity of the stimulus representation, but further underscores that the

stimulus representation did not simply shift from tonic to burst firing. Therefore, this analysis

revealed that in general the high-order structure captured by STC was insignificant compared

to the first order structure revealed by STA, and that when there was a loss of structure in the

STA in the burst mode of firing, no new higher-order feature selectivity emerged through the

STC analysis.

The third assumption made throughout the analysis was that burst spikes are actually

driven by sensory stimuli such that there is a recoverable burst spike feature selectivity. The

alternative explanation would be that burst spikes are not feature selective and instead occur

randomly due to intrinsic or other non-sensory processes. To assess this, we quantified the

trial-to-trial repeatability for bursts in response to frozen white-noise segments. As can be seen

in Figure 3B, the qualitative assessment of temporally aligned bursts in response to the frozen

white-noise segment suggests that the bursts are driven by the sensory stimulus in a

repeatable way. For units with a sufficient number of repeated trials, we computed the

reliability of the burst spiking as the correlation between the peristimulus time histogram of

even and odd trials in response to the frozen white-noise segment. We found that all units

showed greater reliability than what is expected based on just the temporal correlations in the

burst spiking (shuffle control, $p = 0.002$, $n = 10$ thalamic units). This suggests that the bursts

are not randomly generated or due entirely to a non-stimulus related phenomenon.

From these controls, we propose that the difference in the spike triggered encoding

properties could not be attributed to differences in the overall spike rates, the temporal

properties of the spikes within the burst, or the mechanism of filter estimation. Instead, we

propose that the burst spikes are driven by the sensory stimulus and have an underlying

feature selectivity, but that this cannot be recovered using spike triggered techniques due to

the reduced temporal precision of burst spiking relative to tonic spikes.

Recovering feature selectivity from spike-triggered analysis relies on precise temporal

spiking relative to the sensory stimulus. To simulate degradation of the spike timing precision,

we added independent samples of normally distributed temporal jitter of varying amplitudes

(standard deviation of the jitter distribution) to each tonic spike for an example unit and

computed the STA (Figure 4A). Across units, we quantified the degradation of the STA as the

jittered-STA_{SNR} normalized by the $tSTA_{SNR}$ (0 ms jitter). The jittered-STA_{SNR} (black) is within

the band expected for the $bSTA_{SNR}$ with the addition of 4 milliseconds of jitter to the spike

times (red shaded, Figure 4A, right). We propose that the effects of temporal jitter are

particularly evident for whisker selectivity, presumably due to the short temporal duration of

the filters (approximately 10-15 milliseconds in duration, Figure 1F).

Given the marked effects of jitter on the ability to recover the STA, we investigated the

variability in the spike timing relative to the noise stimulus (Figure 4B). For this example unit,

we have identified a segment in the noise stimulus that closely resembles the tonic STA for

this unit and elicits a reliable spiking response (Figure 4B, top; stimulus – black, tSTA – grey

dashed). The vertical dashed line indicates the spike time for the spike triggered average (t_0)

with the grey bar indicating the duration of the STA. If there was no variability in the neural

spiking, the raster plots would all be perfectly aligned to t0 because the similarity between the

stimulus and the STA would predict a spiking response at that time point. However, the timing

of evoked neural responses is always variable to some extent and this can be visualized for

this example response segment as the temporal variability of the spike times surrounding this

stimulus feature in the noise stimulus (Figure 4B, as indicated by the grey stimulus bars that

extend from the first spike response to this particular sensory feature). For this example

snapshot, it is also apparent that the burst spikes in the hyperpolarized condition show greater

temporal variability than the tonic spikes in the baseline condition.

To quantify this jitter across all spikes, we developed a τ_{jitter} metric that determines the

time lag of the peak correlation between the STA and the stimulus segment ($s(t_j)$) surrounding

each spike (Figure 4C). Intuitively, this is a correlative method to identify the time lag between

when we predict a spike is most likely to occur based on the STA and the stimulus (peak

correlation) and when the spike actually occurred. For this analysis, we treated the tSTA as

the true feature selectivity of the neuron across all spiking conditions because we could not

recover a reliable estimate of the bSTA.

We computed τ_{jitter} for each spike and plotted τ_{jitter} distributions for each spike condition

(tonic, burst, baseline, hyperpolarized). If a neuron was infinitely precise such that when the

stimulus matched the spike triggered average, the neuron fired a spike without delay, this

distribution would be represented by a delta function at τ_{jitter} equals zero. As the variability of

the timing increases, the width of this distribution will also increase. For the tonic and baseline

condition spikes, we found a clear peak in τ_{jitter} values at τ_{jitter} equals zero (Figure 4C, grey,

black). For the burst and hyperpolarized condition spikes, we observe little-to-no peak in the

τ_{jitter} metric at zero (Figure 4C, red, yellow). We computed the τ_{jitter} distribution across all

thalamic units and found that the tonic and baseline spikes had higher peaks at τ_{jitter} equals

zero than the burst and hyperpolarized spike conditions (Figure 4D). We quantified this

statistically by computing a precision metric (Figure 4C) that computes the proportion of spikes

within ±1 millisecond of τ_{jitter} equals zero (Figure 4E). The tonic and baseline spike condition

were more precise than burst and hyperpolarized conditions.

These data suggest that tonic spikes showed greater temporal precision in response

to the sensory white-noise than burst spikes and that this could underlie the difference in the

recoverability of the feature selectivity in the thalamus between firing modes. It is well

established that the timing of sensory inputs is particularly important in the thalamocortical

circuit such that changes in thalamic spike timing could have large impacts on the downstream

representation of sensory information in the cortex. Next, we investigated how these changes

in temporal precision in optogenetically modulated thalamic states impact cortical encoding

properties.

Figure 4: Thalamic timing variability in the response to the sensory white-noise. A. Effect of increased jitter on thalamic STA (schematic: left, example: center). Across units (n = 30), the normalized amplitude of the jittered STA (jitteredSTA$_{SNR}$/tSTA$_{SNR}$) was plotted across jitter intensities (black, right). The normalized amplitude of the burst STA (bSTA$_{SNR}$/tSTA$_{SNR}$) is shown in red (mean ± s.d.). B. In this example, the same stimulus (black; scale bar: 0.1°) was presented with and without optogenetic hyperpolarization (data from example unit presented in Figure 3 with associated STA (grey dotted line; scale bar: 0.025°)). C. Example unit τ_{jitter} distributions for burst (n = 2107 spikes), tonic (n = 23023 spikes), baseline (n = 11361 spikes), and hyperpolarized conditions (n = 11662 spikes). D. Average τ_{jitter} distributions for burst/tonic spikes (n = 30 units) and baseline/hyperpolarized condition (n = 10 units). (mean +/- sem). E. Precision for burst/tonic spikes (n = 30 units, p = 1e-6) and baseline/hyperpolarized condition (n = 10 units). (mean +/- sem, p=1e-3).

 <u>Optogenetic modulation of thalamic firing modes directly impacts cortical representation of</u>

<u>sensory information.</u>

Cortical neurons that receive direct thalamic input are integrating information over a

population of thalamocortical neurons that can be exhibiting different firing characteristics.

This makes it difficult to determine the impact of a single burst from a single neuron on

information representation in the pathway. Instead, we used the optogenetic manipulation of

thalamic state as presented in Figure 3 to bias the activity of the thalamic population towards

burst firing (hyperpolarized condition) while recording the cortical activity extracellularly

(Figure 5A).

For an example unit, we have plotted the cortical STA in the baseline and

hyperpolarized VPm conditions (Figure 5B). Here, the amplitude of the cortical STA was

smaller when the thalamus is hyperpolarized compared to when it is not (Figure 5B). This

cortical unit also shows a reduced tuning to the STA when the thalamus was hyperpolarized

(Figure 5C). Across the population of recorded cortical neurons, the same effect seen in this

example neuron of a reduced STA_{SNR} when the VPm was hyperpolarized compared to when

it was not (Figure 5D) and a reduction in the tuning was present across all cortical units as

quantified by the spiking nonlinearity (Figure 5E). These findings mirror what was seen for

thalamic neurons when comparing the baseline and the optogenetically manipulated

conditions demonstrating that the changes in thalamic encoding properties are propagated to

cortex. Note that we again conducted the STC analysis with the S1 neurons and found the

same reduction in STC_{SNR} when the VPm was hyperpolarized compared to when it was not (p

= 9e-5), suggesting that the loss of feature selectivity in S1 with thalamic hyperpolarization

was not just due to the transfer of feature selectivity to higher-order characteristics.

Interestingly, there was no significant difference in the sensory white-noise-evoked

firing rate in the cortex as a function of the VPm condition (Figure 5F). This suggests that it

was not overall spike counts influencing the cortical feature selectivity. Instead, we propose

the temporal jitter in the thalamic spiking patterns propagated to cortex. We investigated the

temporal precision of the cortical spiking in response to the sensory white-noise using the

same methodology employed for the thalamus. As we saw for the thalamus, the cortical spikes

from this example unit also showed greater temporal precision in response to white-noise

whisker stimulation in the baseline VPm condition compared to the hyperpolarized VPm

condition (Figure 5G) as evidenced by the peak in the τ_{jitter} distribution around τ_{jitter} equals zero.

This effect was consistent across the population of recorded cortical units (Figure 5H) and

showed significant differences in the precision of the cortical firing (Figure 5I). This suggests

that the temporal jitter present in the thalamus is transmitted to the cortex where it also impacts

the representation of sensory information.

Figure 5: Optogenetic modulation of thalamic firing modes directly impacts cortical representation of sensory information. A. Experimental paradigm. Scale bar: 1 mm. YFP signal (green) shows axonal projections into cortex. DiI stain was used on the probe to confirm recording location. B. Example STA for a cortical unit recorded during optogenetic manipulation of the thalamus (black: baseline thalamic condition, yellow: hyperpolarized thalamic condition). C. Example cortical nonlinearity as a function of thalamic state. D. STA_{SNR} across cortical units (n = 32 units. p = 1e-6). E. Spiking nonlinearity across cortical units during thalamic manipulation (n = 32 units). F. Cortical firing rate during thalamic manipulation (n = 32 units, p = 0.31). G. Example cortical unit τ_{jitter} distributions for baseline (n = 12862 spikes) and hyperpolarized (n = 11848 spikes) thalamic conditions. H. Average τ_{jitter} distributions for baseline/hyperpolarized thalamic condition (n = 32 units, mean +/- sem). I. Precision for cortical spikes during baseline/hyperpolarized thalamic condition (n = 32 units, mean +/- sem, p=8e-6).

Discussion

Although there have been extensive investigations into the cortical state-dependent

processing of the thalamocortical circuit, we know surprisingly little about how information is

processed in a thalamic state-dependent manner. Here, using a combination of optogenetic

manipulation and electrophysiological recording techniques, we have performed a series of

experiments modulating the state of the thalamus (through constant optogenetic

hyperpolarization) and quantified the effects on encoding in the thalamocortical circuit. Using

this technique, we have coarse control of the firing mode in thalamus without altering the

processing occurring from the whisker to thalamus, enabling us to decouple the changes in

thalamic firing mode on thalamocortical processing from changes occurring in subthalamic

processing. We found that, unlike the visual pathway, the feature selectivity of burst spikes in

the vibrissa pathway could not be recovered using spike triggered techniques due to increased

burst spike timing variability (loss of timing precision) relative to tonic spike timing. Recordings

from barrel cortex during optogenetic manipulation of thalamic state demonstrated a loss in

the temporal precision of the cortical spiking that also led to a degradation of the recovered

feature selectivity. This suggests that bursts in the whisker pathway are less precise than tonic

spikes during ongoing weak sensory stimulation and that this loss of temporal precision is

propagated to cortex, which could have implications for the integration of complex patterns of

sensory inputs.

Although spike-triggered analysis has been widely applied in various pathways, there

have been comparatively few studies of this nature in the vibrissa pathway despite the

extensive utilization of this model system. In this study, we focused primarily on timing in the

thalamocortical circuit, and used the spike-triggered analysis as a vehicle to probe this issue

rather than uncovering novel aspects of feature selectivity related to whisker kinematics.

Nevertheless, it is important to note the similarities and differences between these studies.

Spike-triggered averaging of VPm neurons in a study from Petersen et al. revealed very similar

feature selectivity to what we report for VPm in baseline conditions here, with spiking tending

to be preceded by a very fast transient, biphasic whisker deflection (Petersen et al., 2008).

Studies in cortex, however, reveal more complex properties. Although the basic feature

selectivity that we uncovered for S1 neurons in baseline conditions using STA was very similar

to what has been observed in a subset of recorded neurons in other cortical studies

(Estebanez et al., 2012; Maravall et al., 2007), further analysis using STC as well as more

complex whisker stimulation paradigms in these studies identified more complex encoding

properties. It should be noted that we restricted analysis to cortical S1 neurons that exhibited

significant feature selectivity in the baseline condition with STA, but also observed other

cortical neurons that showed significant feature selectivity only using STC, consistent with

these previous studies. For these neurons, the filters recovered using STC analysis for tonic

spikes were lost when they were computed for burst spikes, as the STC analysis is also reliant

on precise spike-timing relative to the sensory stimulus.

Specific to our findings here related to thalamic firing modes, it is theoretically possible

that in the optogenetically induced thalamic burst mode, the feature selectivity is not lost, but

instead transformed to a type of selectivity that is not captured through the simple

characteristics of the spike-triggered averaging or a stimulus selectivity that is fundamentally

different from the tonic spike feature selectivity. As described above, previous studies have

utilized STC analysis to successfully uncover complex feature selectivity in the visual (Touryan

et al., 2005) and somatosensory (Estebanez et al., 2012; Maravall et al., 2007) pathways.

However, when we extended the analysis here to the spike-triggered covariance (STC), it was

not the case that the timing changes were captured through covariance analysis. For both the

thalamic VPm and cortical S1 recordings, there was no apparent shift in feature selectivity

from first-order structure (STA) to higher-order structure (STC) with a change in thalamic firing

mode or state. Units with significant filters in the tonic spiking condition did not show significant

filters in the burst spiking condition, even when assessed using both STA and STC. As with

the spike triggered analysis, further analysis to explore burst feature selectivity that is

fundamentally different from the tonic feature selectivity could not be pursued due to the timing

variability of the spiking. We cannot identify this selectivity without a mechanism to measure,

and compensate for, the increased spike timing jitter, as this framework is inextricably linked

to the timing precision with which neurons spike relative to the sensory input.

These results could be interpreted as consistent with the view that bursts are not

representing detailed stimulus information. However, there is evidence that bursts may convey

more information than the "all-or-none" presence or absence of a burst through inter-burst

spike timing and the number of spikes per burst (Mease et al., 2017), suggesting a role of

temporally precise burst firing in information representation. Furthermore, thalamic bursting

can be temporally precise within and across neurons in response to high intensity whisker

stimuli (Whitmire et al., 2016). Instead, we propose that the temporal precision of the thalamic

firing is a function of both the state of the thalamus and the intensity of the sensory stimulus.

It has previously been shown that the temporal precision of thalamic encoding increases with

the intensity of the sensory stimulus (Desbordes et al., 2008; Whitmire et al., 2016) while here

we have shown that the temporal precision of the thalamic firing decreases with sustained

hyperpolarization, which would naturally have implications for what signals do and do not get

conveyed through the relatively narrow cortical window of integration (Gabernet et al., 2005).

These two competing factors would enable the burst firing mode to encode high amplitude

stimuli in a temporally precise fashion while low amplitude stimuli, such as the sensory white-

noise presented here, would not be able to overcome the variability present in the burst state.

There are multiple mechanisms that could underlie the reduced temporal precision in

the burst firing mode including variability introduced by the slow dynamics of the calcium

depolarization, increased variability in the time to reach threshold due to the prolonged

hyperpolarization of the baseline polarization, as well as potential changes in the integration

properties of the thalamic neurons. Furthermore, these mechanisms could occur

independently such that the variability across neurons is uncorrelated or these mechanisms

could be coordinated in some way to enable correlated variability across the thalamic

population. Both coordinated and uncoordinated jitter would have a detrimental effect on the

ability to recover the STA because either the spike timing would no longer be locked to the

stimulus itself or the input to the cortex would be temporally imprecise. However, coordinated

jitter would maintain the information about the stimulus while uncoordinated jitter would

degrade the recoverability of the stimulus features with the spike-triggered approach. Future

work is needed to investigate the jitter in the burst spiking across the population to determine

whether or not the variability in the spike timing is coordinated across thalamic units in this

context.

While we have primarily considered thalamic state-dependent encoding as a

feedforward representation from thalamus to cortex, the highly interconnected thalamocortical

circuitry shapes coding properties in both feedforward and feedback manner. Changes in

thalamic activity impact cortical activity which then provides feedback to thalamus to further

alter activity (Crandall et al., 2015; Mease et al., 2014; Poulet et al., 2012; Reinhold et al.,

2015; Wimmer et al., 2015). It is possible for thalamus to influence cortical state and for the

cortex to influence thalamic state, but how this plays out during natural behaviors is not yet

known and must be decoupled using more sophisticated techniques such as closed-loop

control of neural activity (Bolus et al., 2018; Newman et al., 2015).

Given the importance of thalamic spike timing precision within and across neurons in

transmitting information downstream to cortex (Bruno and Sakmann, 2006; Wang et al., 2010),

alterations to thalamic state can shape multiple properties of the spiking inputs to cortex. Here,

we have shown that thalamic state directly impacts the spike timing precision in the thalamus

and cortex. Manipulation of the thalamic state can also lead to changes in the stimulus evoked

cortical dynamics (Whitmire et al., 2017) and spatiotemporal cortical activation (Borden et al.,

2019). Alterations to the state of the thalamus, or the baseline membrane potential, provides

a biophysical mechanism for the thalamus to gate information flow to cortex. Furthermore, this

mechanism could be under both feedforward and feedback control. This sets the stage for a

dynamic interaction between thalamic and cortical states to drive highly interactive patterns of

neural activity, ultimately controlling the integration of afferent signaling that underlies sensory

percepts.

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