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Rapid clearing of biological organs by using phosphoric acid, a hydrophilic solution with high refractive index

(Short title) Rapid clearing of biological organs by using phosphoric acid

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26 **Highlights**

- 27 ■ Phosphoric acid can reduce light scattering by tissue samples.
- 28 ■ Tissue clearing effect of phosphoric acid is fast and needs only 60-min incubation.
- 29 ■ Cell membrane was preserved during incubation using phosphoric acid.

30

31

32 **Abstract**

33 Tissue clearing is a fundamental challenge in biology and medicine to achieve high-resolution
34 optical imaging of tissues deep inside intact organs. The clearing methods, reported up to now,
35 require long incubation time or physical/electrical pressure to achieve tissue clearing, which is
36 done by matching the refractive indices of the whole sample and medium to that of the lipid
37 layer. Here we show that phosphoric acid increases the refractive index of the medium and can
38 increase the transparency of formalin-fixed tissue samples rapidly. Immersion of fixed tissues
39 of mice in phosphoric acid solutions increased their transparency within 60 min in the case of
40 3-mm-thick fixed tissue specimens. While phosphoric acid suppresses bright signals on the
41 boundary of cells in their phase-contrast images, it does not damage the morphology of cell
42 membrane with phospholipid bilayer. The protocol presented herein may contribute to develop
43 better and faster soaking methods for tissue clearing than previously reported protocols.

44

45 **Introduction**

46 Whole-tissue and whole-body imaging of single cells in opaque organisms like mammals has
47 been fundamental challenges in biology and medicine. Biological three-dimensional imaging
48 has been achieved by reconstructing three-dimensional structure from images taken from
49 mechanically serially sectioned tissues, for example serial block-face scanning electron
50 microscopy [1] and array tomography [2]. However, the technique is not only labor-intensive

51 and time-consuming but also error-prone [3]. The utility of rendering tissue optically
52 transparent has been well known for three-dimensional imaging of cell populations located deep
53 inside intact tissue. Optical sectioning provides a potentially fast, simple and inexpensive
54 alternative for three-dimensional reconstruction; however, its utility for deep imaging is
55 prevented by tissue opacity.

56

57 Optical imaging of thick tissues is mostly limited by scattering of imaging light through thick
58 tissues, which contain various cellular and extracellular structures with different refractive
59 indices. The imaging light traveling through different structures scatters and loses its excitation
60 and emission efficiency, resulting in a lower resolution and imaging depth [4]. The low
61 refractive index of water compared with that of cellular structures containing proteins and lipids
62 has been the major issue in this regard; in order to address this problem, the main concept of
63 tissue clearing is to adjust the difference between the refractive index of the medium and that
64 of the lipid bilayer [5, 6]. The clearing was achieved by hydrophobic solutions during the early
65 stage of technical development [7]. In this method, a fixed sample is incubated in a mixture of
66 benzyl-alcohol and benzyl benzoate after dehydration of samples with ethanol and hexane.
67 Subsequent reports have shown that the use of tetrahydrofuran (THF) or dibenzyl ether (DBE)
68 instead of alcohol for dehydration improved the clearing of entire brains of adult mice [8, 9]
69 and this method is applicable to clearing lipid-rich spinal cord [10]. Removing membrane lipids
70 by repetitive organic solvent-based dehydration-rehydration improved the permeabilization of
71 tissues [11].

72

73 To reduce the denaturation and to improve the retention of fluorescent signals in formalin-fixed
74 tissue samples, urea-based hydrophilic mixtures, *Scale*, have been developed [12]. Because this
75 technique provided a simple, inexpensive alternative to array tomography and serial section

76 electron microscopy, it contributed to promoting and devising further protocols for tissue
77 clearing. Formamide or formamide/poly(ethylene glycol), Clear^T and Clear^{T2}, were able to clear
78 mouse embryo and brain with no detergents or solvents [13]. SeeDB containing optical clearing
79 agents, fructose and α -thioglycerol, renders tissue samples transparent to allow analyses of
80 cellular morphology without removing any components of tissues during the clearing process
81 and thus with minimum deformation artifacts [14]. Adding fructose to urea can control urea-
82 mediated tissue expansion during the clearing process [15]. Sugar and sugar-alcohol solutions
83 also achieve clearing of 100- μ m-thick mouse brain slices [16]. Preparation of clearing solutions
84 to adjust the refractive index of samples to that of immersion oil (1.518) on the objective lens
85 is effective for high-resolution fluorescence imaging [17]. Electrophoresis to remove lipids
86 after embedding tissue into hydrogel polymer contributes to better tissue-clearing in a method
87 named CLARITY [18]. However, because this method was technically complex, a passive
88 tissue clearing approach using different fixative-hydrogel monomer crosslinking solutions was
89 subsequently reported for adult rodents or human postmortem brain [19, 20]. Solution of 2,2'-
90 thiodiethanol is also effective for clearing brains [21] and facilitated three-dimensional
91 observation of formalin-fixed and fluorescent-labeled whole mouse brains and 2-mm-thick
92 block of human brains in combination with CLARITY [22]. To improve the methodology to
93 deliver reagents deep inside thick tissues, rapid (4-20 h for clearing whole organs) technique of
94 active clarity, ACT-PRESTO, was reported for rendering large tissue samples such as rat and
95 rabbit brains, and even whole bodies of adult mice, optically transparent [23]. On the other hand,
96 CUBIC method achieves tissue transparency by passively clearing phospholipids and is
97 compatible with hydrogel embedding using a mixture of urea and aminoalcohol [24], which
98 decolorizes blood by efficiently eluting the heme chromophore from hemoglobin [25].
99 Optimized CUBIC protocols for whole-body transparent observation of mice [26] and organs
100 of rats [27] are also reported. To reduce tissue damage and degradation, ScaleS method was

101 developed with a mild tissue-permeant sugar-alcohol, sorbitol, and allowed optical
102 reconstructions of three-dimensional mapping of amyloid plaques, neurons and microglia by
103 successive fluorescence and electron microscopy [28]. However, one of the major issues is that
104 the protocols reported above for clearing tissues require long incubation time from several hours
105 to days or pressure that also damages the samples. Rapid and simple soaking protocols for tissue
106 clearing are thus desirable.

107

108 Many hydrophilic solvents for tissue clearing, *Scale*, FRUIT, and CUBIC, contain liquids of
109 high refractive index to increase the refractive index of the incubation medium, in some cases,
110 surfactant to delipidate [29] and potentially promote infiltration of the reagent deeper into
111 tissues, and urea [12, 15, 24, 28, 30]. The refractive index of a material is proportional to the
112 square root of the dielectric constant of that material. Therefore, we hypothesized that tissue
113 clearing is achieved by not only increasing the refractive index of the medium but also by
114 affecting polarization and dielectric coefficient of the lipid membrane, which is composed of
115 non-polarized fatty-acid chain and polarized phosphate group, due to some molecules such as
116 urea in the solutions. In particular, the research group who developed *Scale* containing urea,
117 Triton X-100, and glycerin, showed that partial tissue clearing was achieved using only urea
118 and the surfactant [12]. The mechanism underlying tissue clearing effect by urea is not known
119 but may be important to explore. In the present study, we first investigated the potential
120 contribution of urea to adjusting the refractive indices of the medium and lipid membrane. Next,
121 the tissue clearing effect of phosphoric acid, an anionic molecule that does not interact with
122 anionic lipid bilayer but increases the refractive index of medium, was investigated. We show
123 that urea does not directly contribute to decreasing the refractive index of lipid bilayer, and
124 phosphoric acid, which increases the refractive index of the medium, is able to clear the tissues.
125 Although the incubation for fixed tissue sample in phosphoric acid is only passive immersion,

126 the incubation time required for clearing whole organ samples of mice is faster (≈ 1 h) compared
127 to the case of other clearing reagents. The rapid optical clearing protocol using phosphoric acid
128 will contribute to further improvement of tissue clearing protocols and will aid in the
129 advancement of biological research.

130

131 **Materials and Methods**

132

133 Measurement of refractive index of solutions

134 Solutions of saturated concentration of 1,2-dipalmitoyl-sn-glycero-3-phosphocholine (DPPC)
135 and 4 M urea were prepared in ethanol. The refractive indices of the mixed solutions in ethanol,
136 water, and aqueous solutions of phosphoric acid (4–14.2 M), urea (4 M), sodium iodide (2 and
137 4 M), indium chloride (4 M), and ScaleA2 were measured by Abbe's refractometer (NAR-1T,
138 Atago Co., Ltd., Tokyo, Japan).

139

140 Measurement of refractive index and optical loss of liposome suspension

141 Liposome suspension was prepared by the Bangham method [31]. Briefly, a mixture of 12 μmol
142 of DPPC, 12 μmol of 1,2-dioleoyl-sn-glycero-3-phosphocholine (DOPC), 12 μmol of
143 cholesterol, and 4 μmol of *N*-(Carbonyl-methoxypolyethyleneglycol 2000)-1,2-distearoyl-sn-
144 glycero-3-phosphoethanolamine (DSPE-PEG) was prepared in 1600 μL of chloroform in an
145 eggplant-shaped glass flask, and then evaporated at 37°C to remove chloroform and to obtain a
146 thin lipid bilayer on the inner wall of the flask. 7.5-mL of either of distilled water, aqueous
147 solution of urea (4 M) or phosphoric acid (14.2 M) was added into the flask and sonicated to
148 prepare liposome suspension in each liquid. The light transparence (wavelength: 600 nm) of
149 the liposome suspensions were measured by spectrometer V-660 (JASCO Co., Tokyo, Japan)
150 and 1.5-mL disposable cuvette (Brand GmbH & Co. KG, Wertheim, Germany).

151

152 Measurement of optical loss of cell suspension of mouse brain

153 All animals were handled in accordance with the national guidelines for the care and use of
154 laboratory animals and with the approval of the Animal Care and Use Committee of the Tokyo
155 University of Science. Brain samples isolated from adult ICR mouse sacrificed under hyper-
156 anesthesia were minced by using BioMasher (Nippi Inc., Tokyo, Japan), suspended in PBS, and
157 fixed by 4 wt% formaldehyde in PBS overnight. Fixed cell suspension was collected by
158 centrifugation ($1200 \times g$, 5 min) and washed with PBS three times, and divided into different
159 tubes. The cell suspensions were then incubated in either of ScaleA2, PBS, or aqueous solution
160 of urea (4 M), indium chloride (4 M), sodium iodide (2, 4 M), Triton X-100 (10 wt%),
161 phosphoric acid (8.5, 11.4, 14.2 M), or 0.1 wt% Triton X-100 in phosphoric acid (14.2 M) for
162 24 h at room temperature. The optical loss (OD600) was measured by spectrometer V-660
163 (JASCO) and 1.5-mL disposable cuvette (Brand GmbH & Co. KG).

164

165 Observation of morphology and phase-contrast image of formalin-fixed cells

166 Cultured Colon-26 cells were maintained in Minimum Essential Medium [(+)Eagle's salt, (+)L-
167 glutamine] (Gibco, Thermo Scientific, MA, USA) supplemented with 10% fetal bovine serum
168 (Biowest, Nuaille, France) and 1% penicillin-streptomycin (Wako, Tokyo, Japan) at 37°C in
169 humidified air containing 5% CO₂. After staining of the cell membrane by CellMask Orange
170 (Thermo Fisher Scientific), the cells were fixed by 4 wt% formaldehyde in PBS for 10 min,
171 washed with PBS, and then incubated in phosphoric acid (14.2 M) for 0-48 h. Cell membrane
172 stained with CellMask was observed by fluorescence microscope through a band-pass filter
173 (cut-on wavelength: 575 nm) under excitation (540 ± 10 nm). The cells without staining were
174 also fixed with formalin, washed with PBS, incubated in ScaleA2, phosphoric acid (14.2 M),
175 or PBS for 24 h, and observed under phase-contrast microscopy.

176

177 Measurement of optical loss of mouse tissues

178 Brain, liver, kidney, and lung samples were obtained from adult ICR mouse under anesthesia.
179 The samples of liver, kidney, and lung were fixed by 4 wt% formaldehyde in PBS for 48 h,
180 washed with PBS, and cut into approximately 3-mm-thick specimens. The fixed tissue
181 specimens and brain hemispheres of mice were incubated in either of ScaleA2, PBS, or aqueous
182 solution of indium chloride (4 M), sodium iodide (4 M), Triton X-100 (10 wt%), or phosphoric
183 acid (8.5, 11.4, 14.2 M) for 60 min. The macroscopic images of the treated samples were
184 captured by a digital camera. To confirm the reversibility of tissue clearing, 450- μ m-thick
185 specimens of mouse brain were prepared, fixed by formaldehyde for 60 min, washed with PBS,
186 incubated in 14.2 M phosphoric acid or PBS for 60 min, replaced and kept in PBS for 24 h, and
187 their images were also recorded by digital camera.

188

189 **Results and Discussion**

190 Phospholipid containing both hydrophobic and hydrophilic parts is arranged in two layers on
191 the plasma membrane; the hydrophobic part is on the interior of the membrane, whereas the
192 hydrophilic part points outwards, toward either the cytoplasm or the fluid that surrounds the
193 cell. The hydrophobic and hydrophilic parts have different refractive indices due to the
194 difference in their dielectric constant. Our hypothesis was a possible contribution of decrease
195 in polarization of the phosphate group, induced by electrostatic interaction of the polarized
196 group with urea, to decrease the refractive index difference between the lipid bilayer and
197 medium. The refractive index of the solution of a representative phospholipid
198 dipalmitoylphosphatidylcholine (DPPC) in ethanol, which is able to dissolve both DPPC and
199 urea, was higher than those of ethanol and water (Fig 1a). Adding urea to ethanol and DPPC
200 solution in ethanol increased their refractive indices (Fig 1a). These results suggest that urea

201 does not decrease the refractive index of DPPC in ethanol but increases the refractive indices
202 of the solutions. The light transparency of liposome suspended in aqueous solution of urea (4
203 M), which shows higher refractive index than water, was higher than that of liposome
204 suspended in water (Fig 1b). Moreover, 14.2 M phosphoric acid, which is an anionic molecule
205 that does not interact with the anionic phosphate group of lipid bilayer, shows higher refractive
206 index than 4 M urea solution and increased transparency of the liposome (Fig 1b). We
207 concluded that urea increased the transparency of liposome not by affecting the polarization or
208 refractive index of phosphate group of the lipid bilayer, but by reducing the difference in
209 refractive indices between the medium and the lipid bilayer as well as phosphoric acid. The
210 clearing effect of phosphoric acid is greater than that of 4 M urea due to higher refractive index.
211

212 Next, we investigated the clearing effect of phosphoric acid, which decreased the light loss of
213 the liposomes, and other candidate chemical solutions on fixed cell suspensions of mouse brain
214 tissues. We targeted phosphoric acid solution, because phosphate group composes of the
215 strongly polarized part and thus contributes to high refractive index of the phospholipid bilayer.
216 Tissue-clearing effects of many kinds of solvents were evaluated by measuring the light loss
217 (OD₆₀₀) of suspension of tissue cells fixed with formaldehyde after homogenization, as shown
218 in previous studies [24]. The light loss of formalin-fixed cell suspensions of mouse brain was
219 decreased by 24-h incubation in phosphoric acid and ScaleA2 (Fig 2). On the other hand,
220 although 4 M sodium iodide (4 M) solution has a similar high refractive index to phosphoric
221 acid, sodium iodide did not decrease the light loss of the cell suspension during the 24-h
222 incubation. Indium chloride (4 M) also has a similar refractive index to urea (4 M), it did not
223 attenuate the light loss by the 24-h incubation as well as sodium iodide. This lack of clearing
224 effect of sodium iodide and indium chloride may be due to relatively poor infiltration of this
225 molecule into fixed tissues or cells. Incubation of cultured cells in tissue clearing solutions

226 (phosphoric acid and *ScaleA2*) attenuated the bright signal on the boundary of cells in the
227 phase-contrast image in a concentration-dependent manner (Fig 3). Because the bright signal
228 on the cell boundary is generated where the difference in refractive index between the sample
229 and background is large, the decrease in the signal by the clearing solutions confirms the effects
230 of the solution on the refractive index difference between the cell membrane and medium. The
231 stability of formalin-fixed cell membrane in phosphoric acid was confirmed by labeling the
232 membrane of the cultured cells, suggesting that phosphoric acid does not damage the fixed
233 membrane during incubation (Fig 4). Macroscopic images of formalin-fixed organ specimens
234 (liver, kidney, and lung) of mice demonstrated that the samples were partially cleared by 60-
235 min incubation in phosphoric acid solution (Fig 5). Phosphoric acid (8.5 M) is effective for
236 reducing scattering by the liver, while higher concentrations of 11.4 M and 14.2 M are needed
237 for the kidney and lung, respectively. On the other hand, 60-min incubation was too short to
238 clear the tissue specimens by *ScaleA2*. Rapid tissue clearing by phosphoric acid is possibly due
239 to fast infiltration of the molecule because of its small size. The molecular size (volume) of
240 phosphoric acid (PO_4^{3-}) is smaller than that of urea (CH_3COCH_3), glycerol [$\text{CH}_2(\text{OH})$ -
241 $\text{CH}(\text{OH})$ - $\text{CH}_2(\text{OH})$], and sugars and sugar alcohols. Other candidate chemicals investigated in
242 the present study, sodium iodide (4 M) and indium chloride (4 M), did not make the tissues
243 transparent but induced shrinkage of samples, especially the kidney specimen. Phosphoric acid
244 is also able to make brain hemisphere transparent as shown in Fig 6. The clearing by phosphoric
245 acid is reversible; re-incubation of transparent 450- μm -thick brain slices in PBS made the
246 sample opaque as well as the original image before phosphoric-acid treatment (Fig 6b). This
247 result indicates that phosphoric acid reduces light scattering in the tissue sample not by
248 irreversible chemical modification but by adjusting the refractive index of the sample to a value
249 close to that of the cell membrane by simple infiltration. Re-incubation of the sample in PBS
250 removed phosphoric acid from the sample and made it opaque reversibly.

251

252 **Conclusions**

253 The present study showed that phosphoric acid, a hydrophilic solvent, can clear tissues
254 including brain, liver, kidney, and lung of mice. Phosphoric acid reduces light scattering by
255 mouse tissues rapidly as it requires only 60-min incubation, while it does not damage the
256 morphology of cell membrane with phospholipid bilayer. The present study showed that
257 phosphoric acid reduced scattering by mouse tissues but did not reduce the light loss due to
258 absorption by the tissues. Combination use of decolorization reagent such as aminoalcohol [25]
259 with small molecular solutes that increase refractive index, like phosphoric acid, may achieve
260 better and rapid tissue clearing. The potential of phosphoric salts with neutral pH for tissue
261 clearing is also of future interest because acidic condition generally denatures fluorescent
262 proteins [32, 33]. The rapid reducing of scattering with the use of phosphoric acid as presented
263 here will contribute to develop better and faster soaking methods for tissue clearing that
264 previously reported protocols.

265

266 **Financial Disclosure**

267 This work was partially supported by the MEXT Grant-in-Aid for Scientific Research on
268 Innovative Areas (Resonance Bio), no. 15H05950, and the MEXT-Supported Program for the
269 Strategic Research Foundation at Private Universities, no. S1511012. The funders had no role
270 in study design, data collection and analysis, decision to publish, or preparation of the
271 manuscript.

272

273 **Competing Interests**

274 There are no conflicts of interest to declare.

275

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355

356 **Supporting Information**

357 The data required to reproduce the optical loss of suspensions of liposome and brain cells in

358 each solvent are posted as a supporting information.

359

360 Figure Captions

361

362 **Fig 1. Effects of urea and phosphoric acid on the refractive indices of solvents and on**
363 **transparency of liposome suspension.** Refractive indices of DPPC in ethanol and its mixture
364 with urea are shown in (a). An increase in the refractive index of DPPC solution in ethanol by
365 urea suggests that urea does not influence the polarization of the phosphoric acid group of lipid
366 bilayer but increases the refractive index of the medium. The effects of urea (4 M) and
367 phosphoric acid (14.2 M) on the refractive index of the medium and transparency of liposome,
368 determined by OD600, are shown in (b). The data of transmittance (%) are shown as mean \pm SD
369 (n = 3). Abbreviation: DPPC, 1,2-dipalmitoyl-sn-glycero-3-phosphocholine.

370

371 **Fig 2. Effects of candidate solutions with different refractive indices on light loss for fixed**
372 **cell suspension.** Effects of 24-h incubation in candidate chemical solutions with various
373 refractive indices on OD600 values (mean \pm SD, n = 3) of brain cell suspension fixed with
374 formaldehyde are shown. Phosphoric acid (8.5, 11.4, 14.2 M) further increases the refractive
375 indices of medium and transparency of the cell suspension than sodium iodide (4 M), urea (4
376 M), and indium chloride (4 M). Abbreviations: InCl, indium chloride; NaI, sodium iodide.

377

378 **Fig 3. Phase-contrast images of formalin-fixed cultured Colon-26 cells incubated in**
379 **phosphoric acid or ScaleA2.** Effect of ScaleA2 and phosphoric acid (14.2 M) solution on the
380 phase contrast on the edge of cultured cells is shown in the microscopic images. Scale bars
381 indicate 50 μ m. The graph shows the concentration-dependent effect of phosphoric acid
382 (8.5–14.2 M) on the gray values of background and the edge in the microscopic images.

383

384

385 **Fig 4. Images of formalin-fixed plasma membrane of cultured cells incubated in**
386 **phosphoric acid.** Cultured Colon-26 cells were stained with CellMask Orange (Thermo Fisher
387 Scientific), fixed by 4 wt% formaldehyde in PBS, washed with PBS, and then incubated in
388 phosphoric acid (14.2 M) for 0–48 h and observed under microscope. Scale bars indicate 10
389 μm . The images confirmed that formalin-fixed cell membrane was retained during incubation
390 in the solution.

391

392 **Fig 5. Effect of incubation in chemical solutions on macroscopic images of formalin-fixed**
393 **tissue specimens of mice.** The organ specimens of murine (a) liver, (b) kidney, and (c) lung
394 were fixed with 4 wt% formaldehyde for 48 h, washed with PBS, and then incubated in
395 indicated chemical solutions for 60 min. The apertures of the background lattice are 4 mm.

396

397 **Fig 6. Clearing mouse brains by phosphoric acid.** Representative images of (a) hemispheres
398 and (b) 450- μm -thick specimens of mouse brains before and after 60-min incubation in
399 phosphoric acid (8.5, 11.4, and 14.2 M) are shown. As shown in (b), the brain tissue that were
400 cleared once by phosphoric acid (14.2 M) returned to opaque state by re-incubation in PBS for
401 24 h.

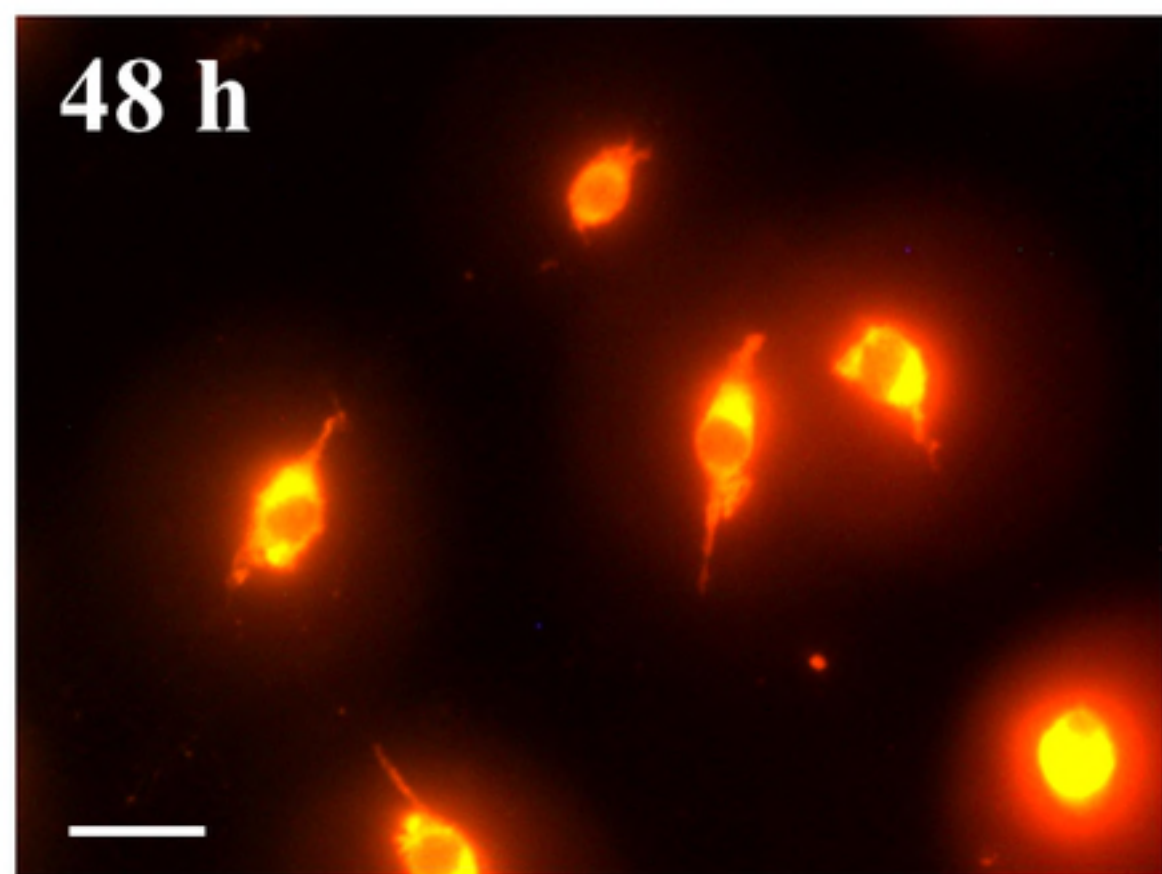
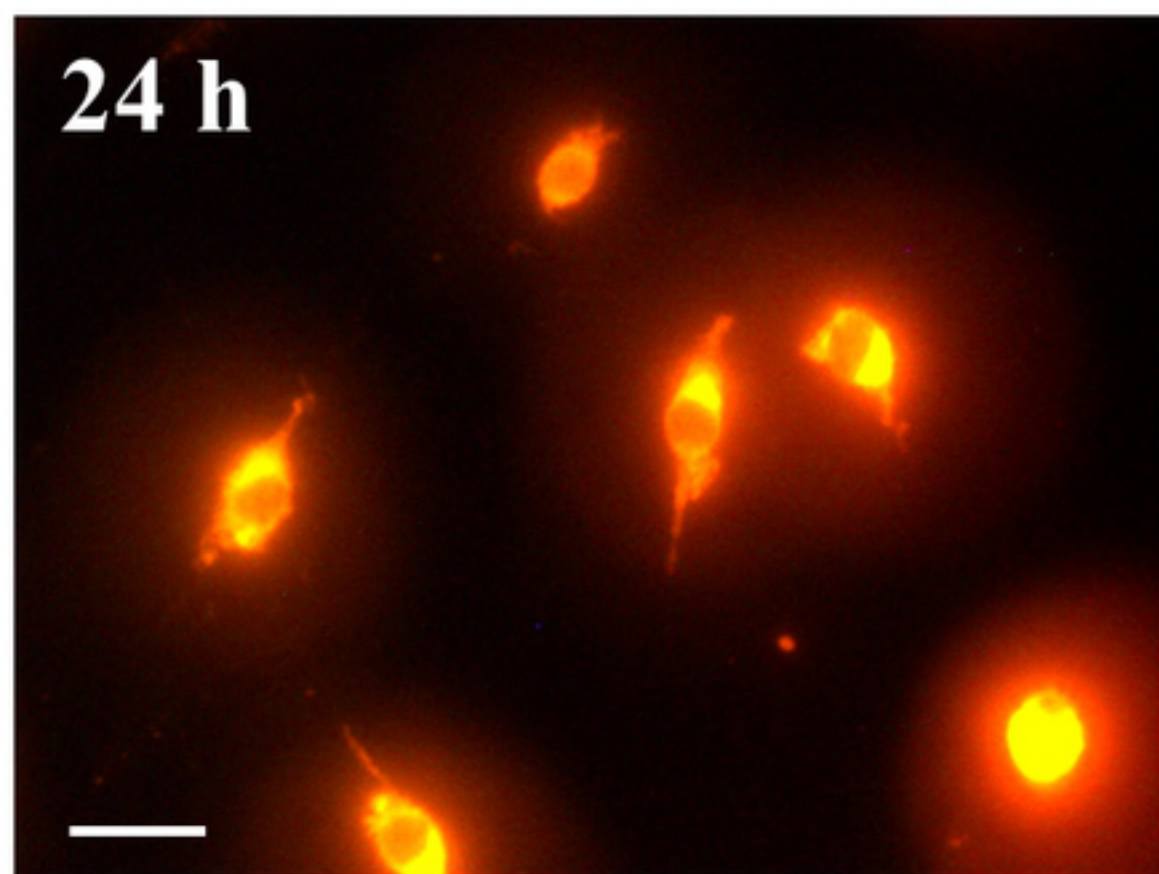
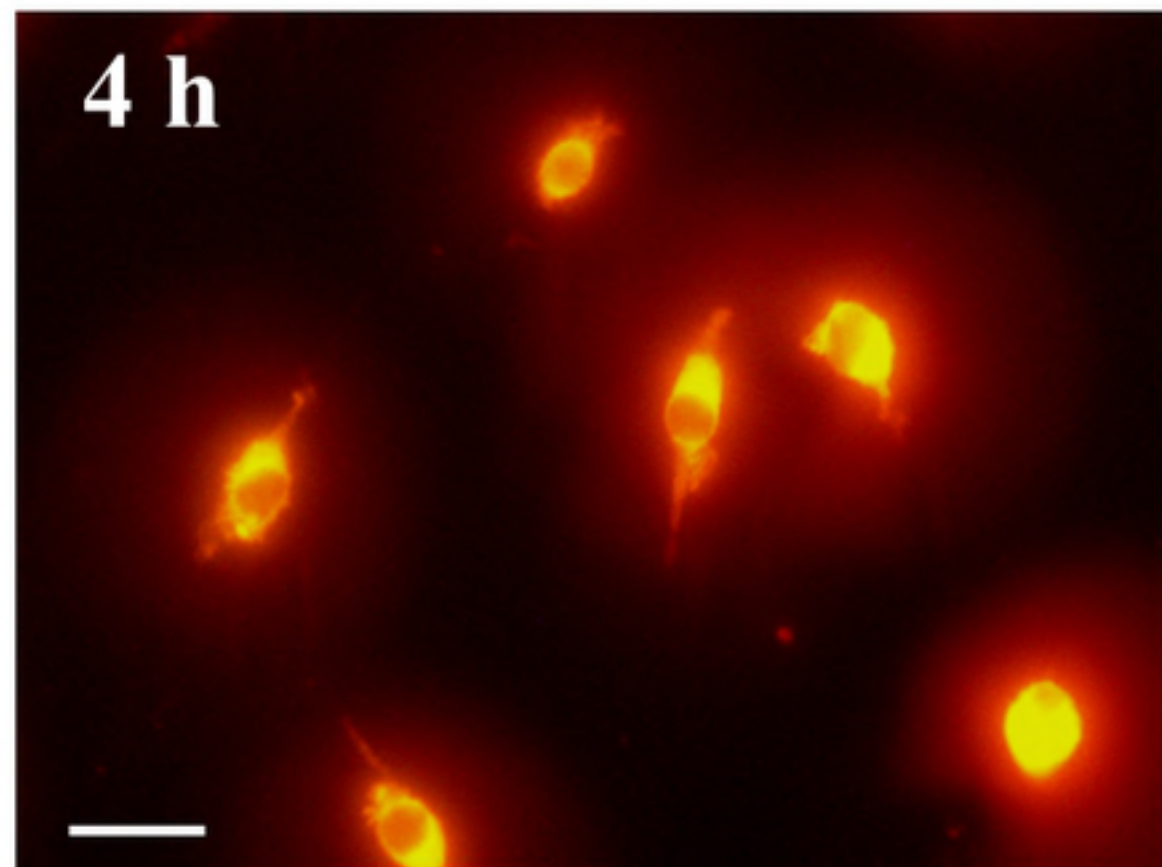
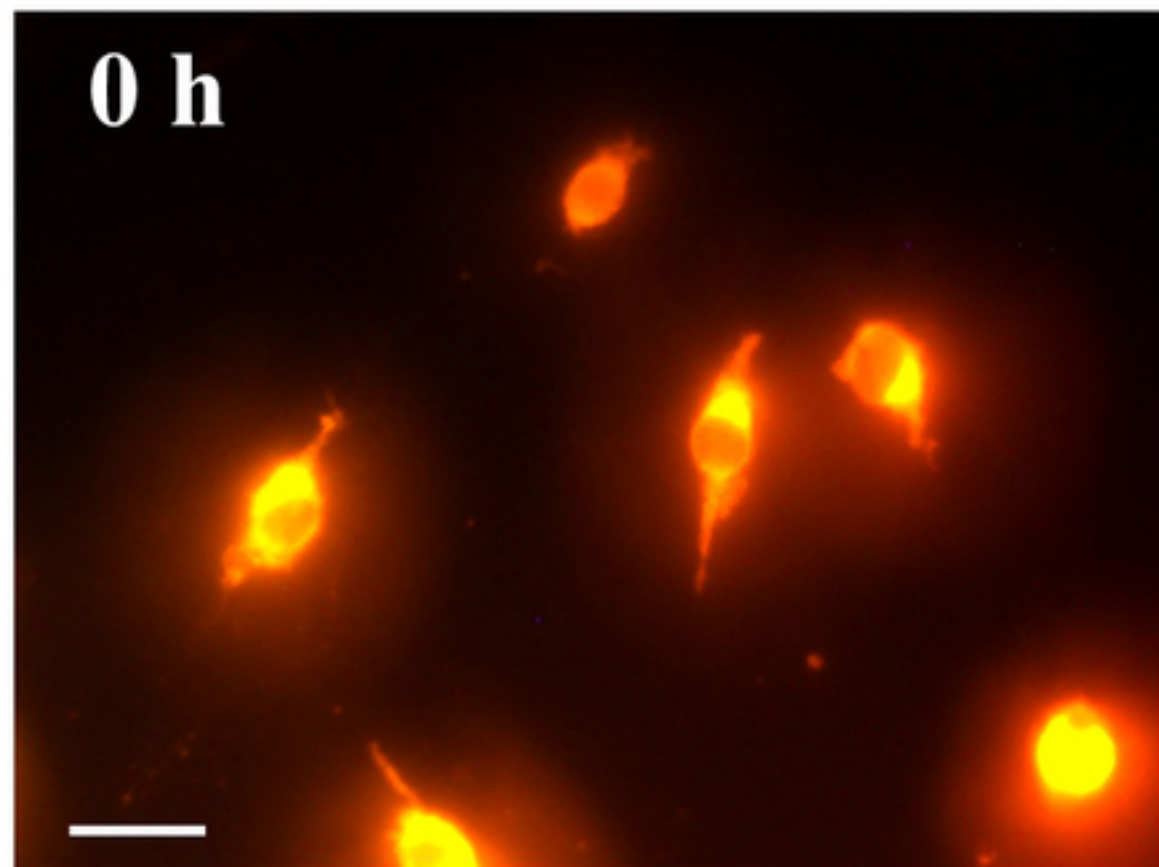


Fig. 4

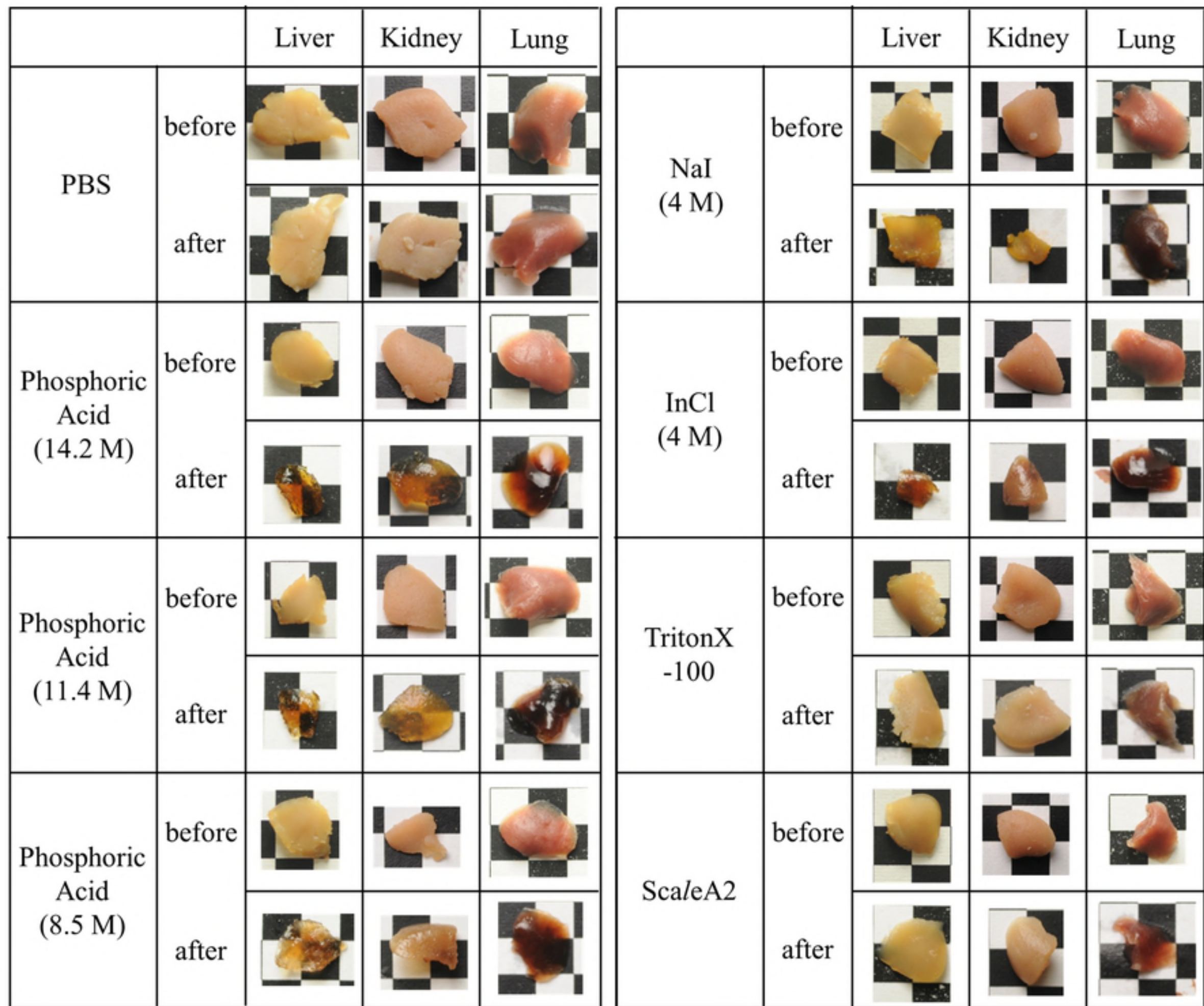


Fig. 5

(a)

Before Incubation



After Incubation



PBS

14.2 M

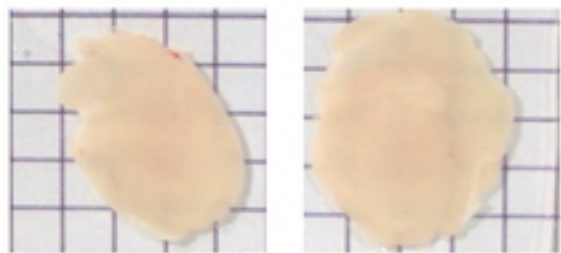
11.4 M

8.5 M

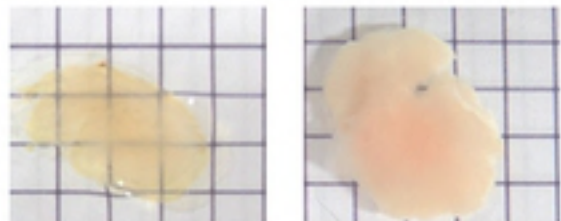
Phosphoric Acid

(b)

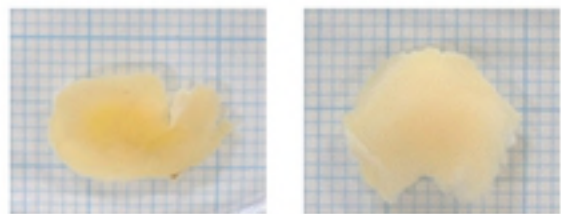
Before Incubation



After Incubation



Re-Incubation in PBS



Phosphoric Acid (14.2 M)

PBS

Fig. 6

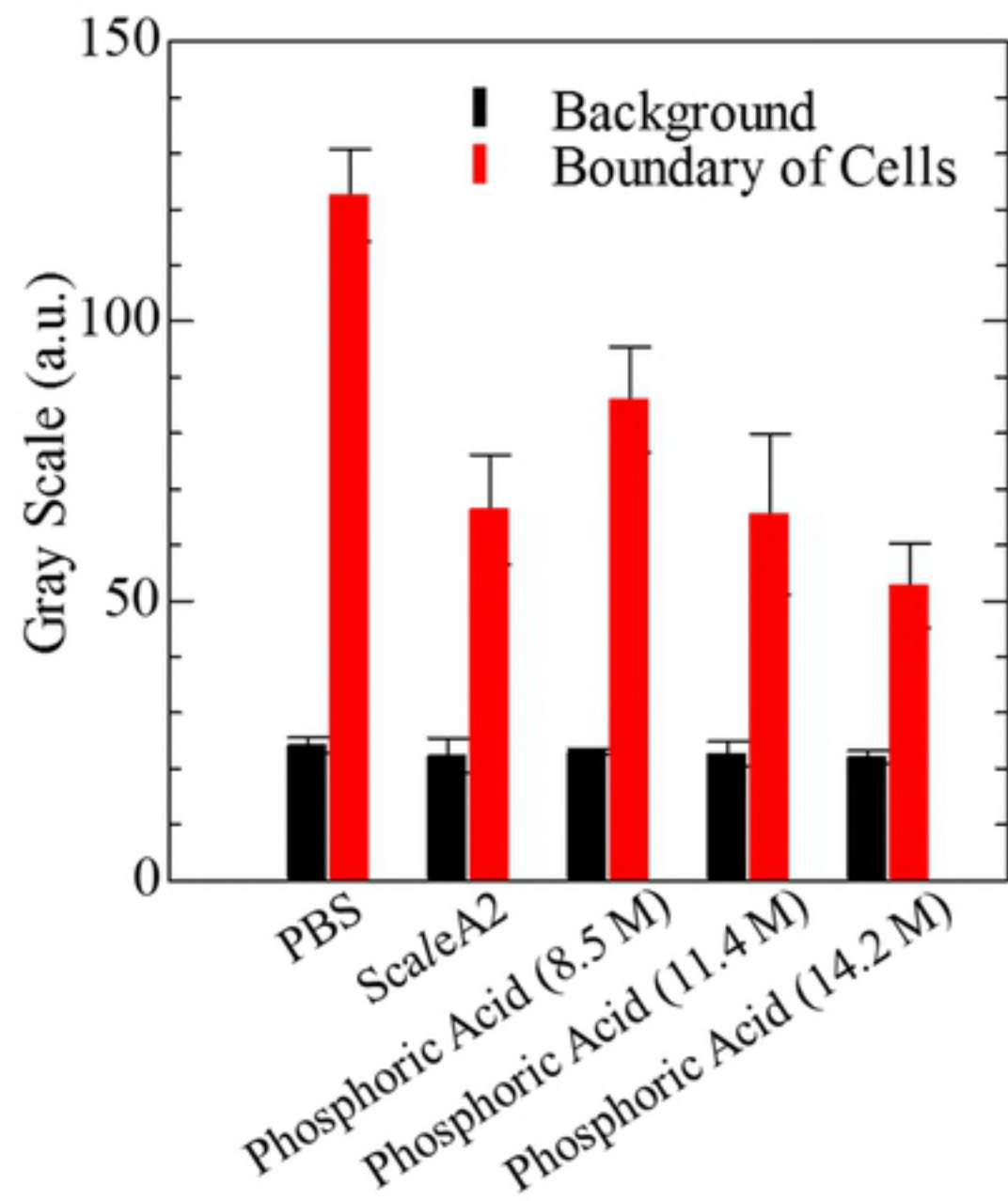
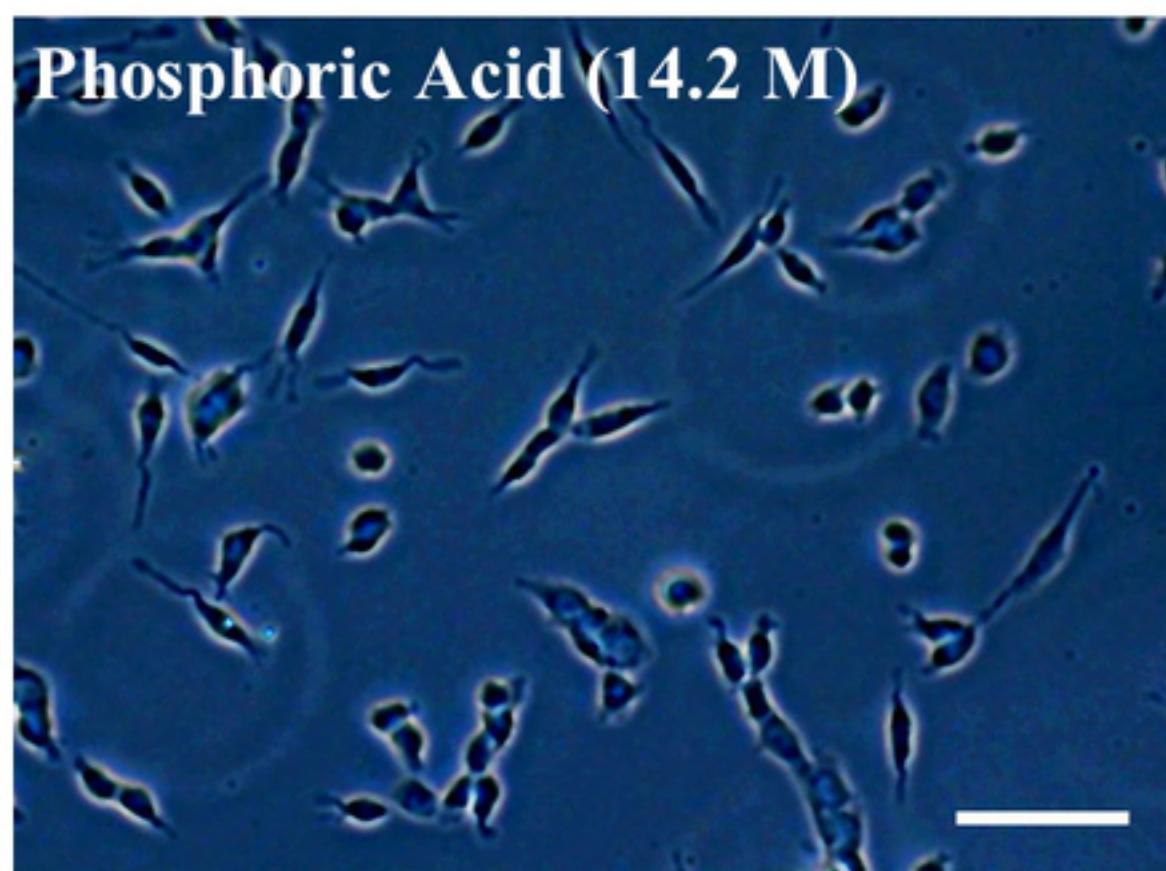
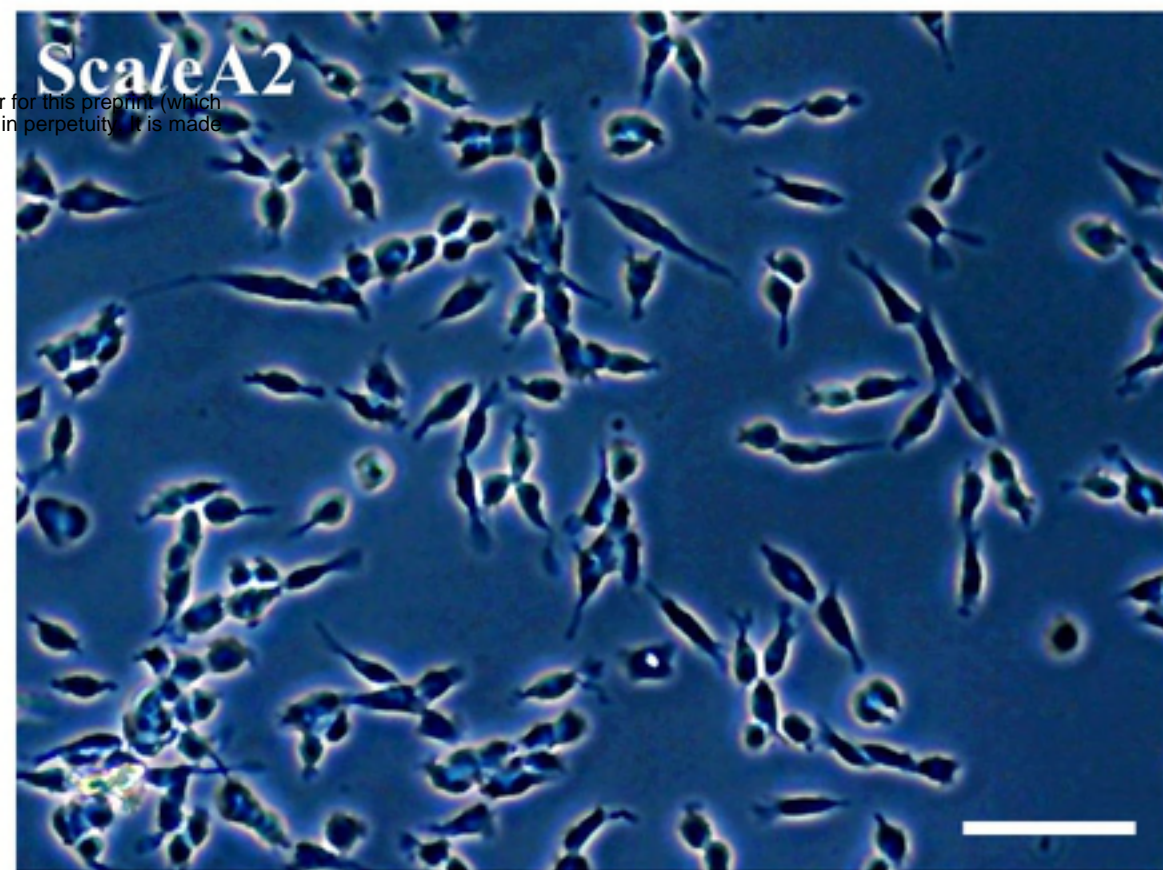
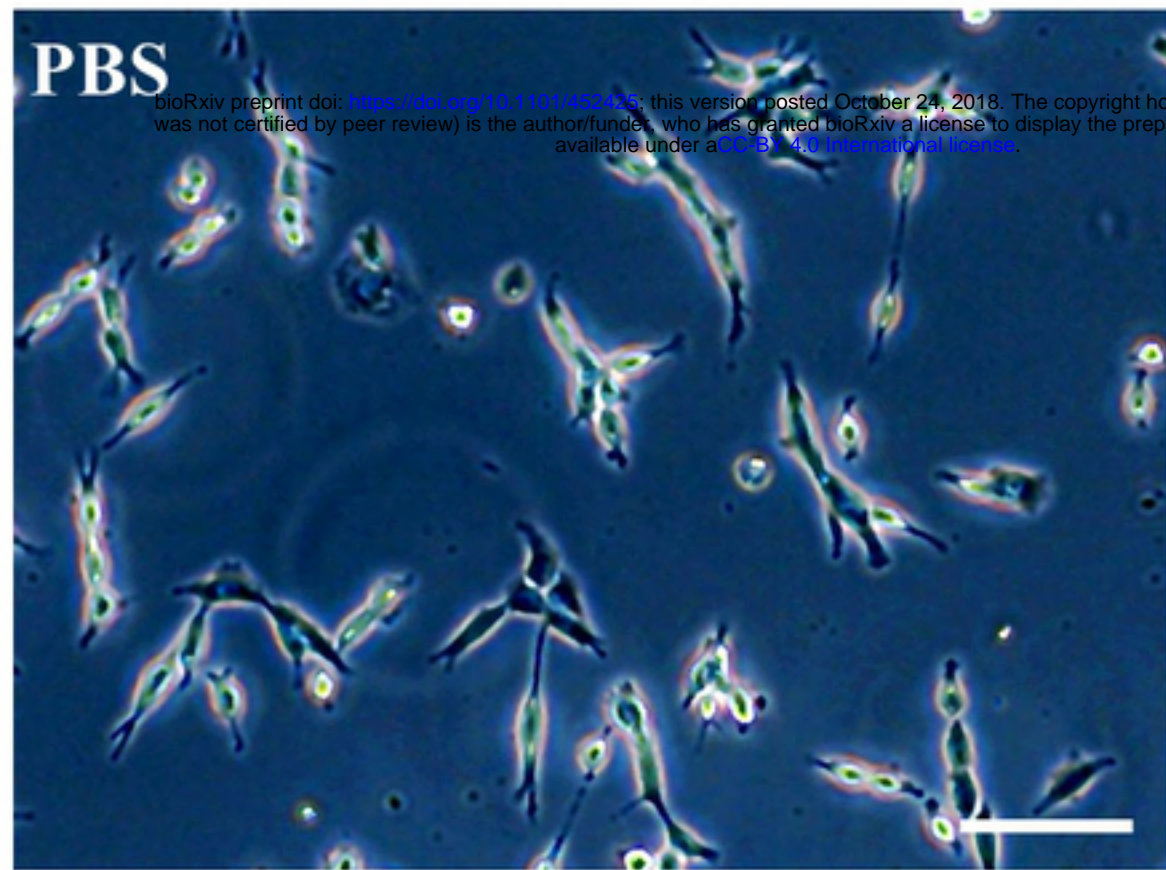


Fig. 3

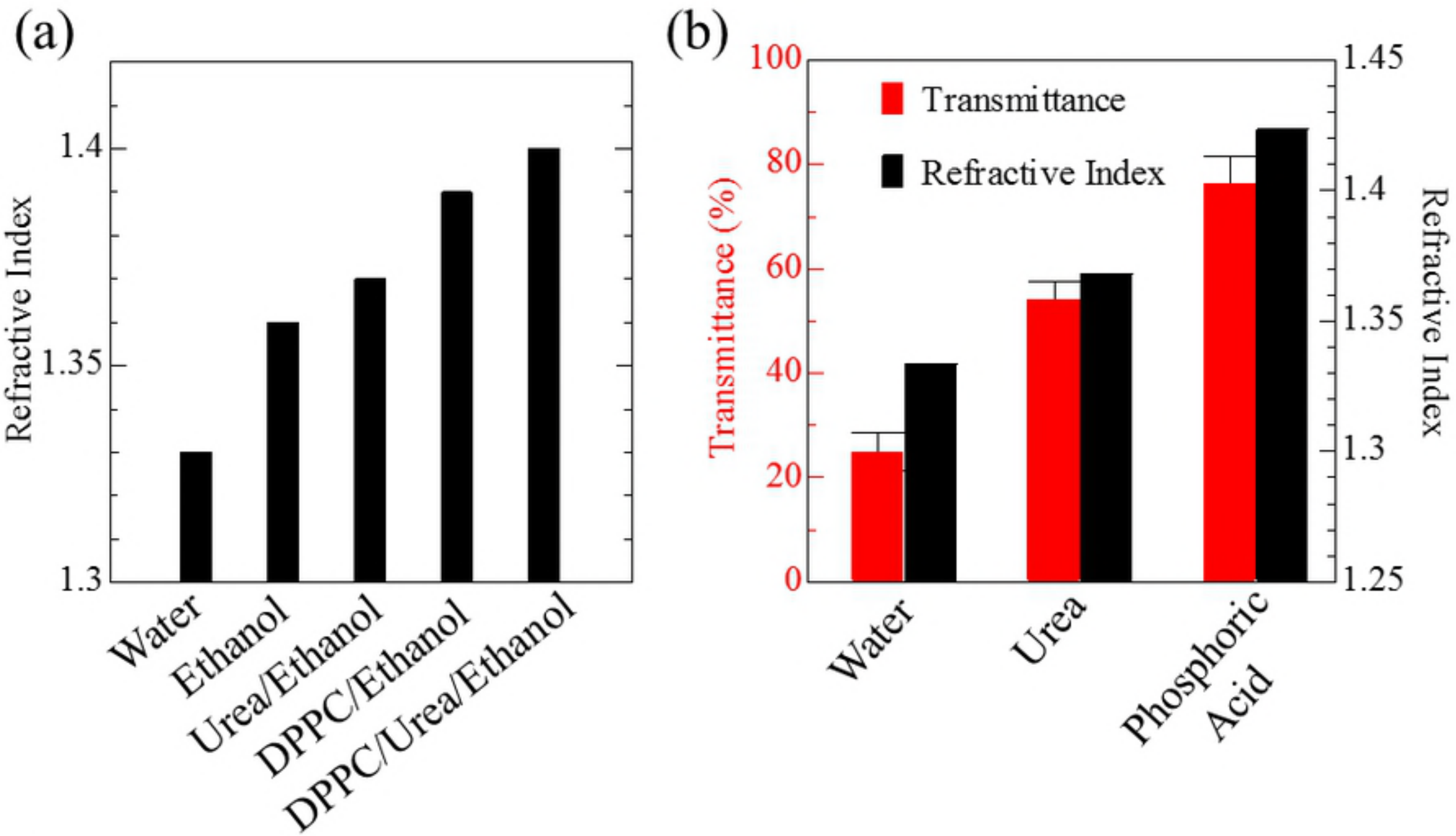


Fig. 1

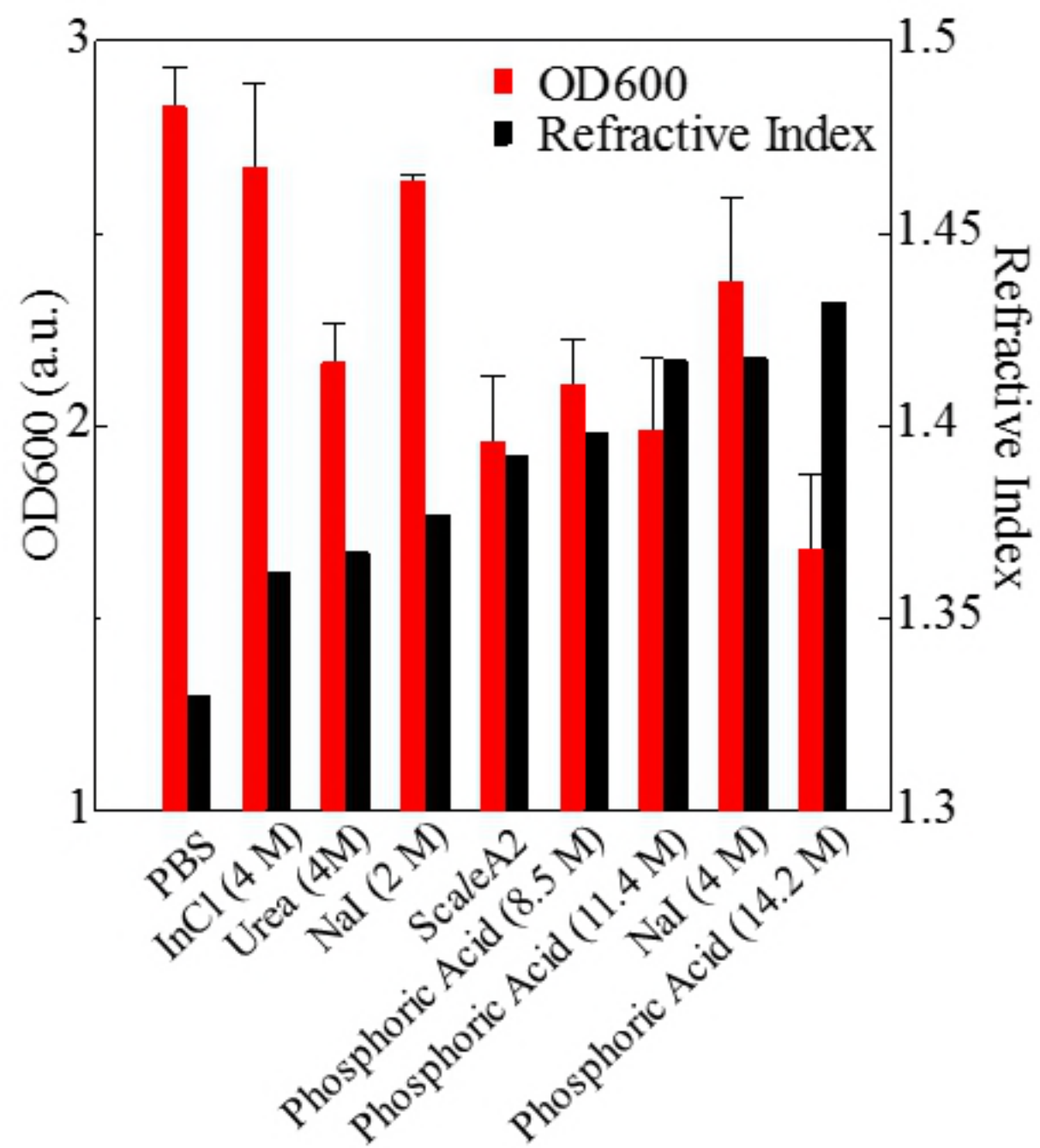


Fig. 2