Countering Cross-Individual Variance in Event Related Potentials with Functional

Profiling

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Abstract

The practical use of ERP deception detection is confounded by low signal-to-noise ratio of EEG and the high inter-participant variation in form (and even polarity) of ERP components. In this study, a simple method called the Weight Template (WT) is proposed for classifying brain responses of individuals into deceiving and non-deceiving. The performance of our method was evaluated on a number of identity deception data sets and on artificial EEG data sets. A comparison was made with a standard method used to measure P3 presence, called Peak-to-Peak. In the real experimental data, the WT showed higher performance in terms of sensitivity and specificity. In the artificial EEG data, in ERPs with low Signal-to-Noise Ratio (SNR), the WT was more resistant to noise and provided more accurate measures.

Keywords

Event Related Potentials, P300, Peak-to-Peak, ERP classification, Concealed Information Test.

Highlights

- We propose a method for classifying ERPs of the P3 Concealed Information Tests.
- The new method is based on computing a weighted template (WT) for each individual.
- The WT is used to characterize the shape of each individual's P3.
- The performance of the WT was compared with the standard Peak-to-Peak method.
- The WT showed higher performance in terms of sensitivity and specificity.

1   Introduction

In Event Related Potential (ERP) research, per-individual inference (e.g., when detecting that a single person is lying) and standard cross-individual group-level inference are made harder by the presence of considerable cross-individual variance in respect of the latency and form of ERP components. In particular, an individual's ERP pattern may be very different to the mean population pattern, as approximated by grand averages. However, most ERP research is strongly wedded to a notion of fixed-form components, e.g., that the P3b is a positive deflection in a window from 250 to 600 ms after stimulus presentation. This fixed-form is often clearly evident at the grand average-level, but much less so for some individuals' ERPs.

The emphasis on fixed-form components has been a central principle of ERP research, which has led to many clear and compelling cognitive interpretations, e.g., "working memory update occurs between 300 and 500 ms after stimulus presentation and following sensory processing (PI-NI complex), etc." However, in the presence of individual differences in ERP-form, it may sacrifice considerable statistical power.

The fixed-form components approach also reflects a wholly justified concern not to fish and thereby to prevent increase in the effective number of comparisons. The problem is that, under classical statistical inference, *tailoring* identification-parameters, such as, window placement, to the deflections in the observed ERP contrast is post hoc fishing. That is, even under the null hypothesis, i.e., when an ERP contrast really does not contain any hypothesis-distinguishing difference, there will be window placements that will isolate statistically significant differences. Moreover, such differences will be identifiable under tailoring with a

probability higher than the alpha level, potentially inflating the type one error rate considerably; see for example (Kilner 2013).

Reliance on fixed-form components resolves this issue if that form, and thus window-placement, is justified a priori, e.g., by some previous published study. This then is a statistically safe approach, in which the type one error rate is controlled. However, variability across individuals is likely to ensure a loss of statistical power, i.e., an inflation of the type two error rate. As an illustration, an individual in which the P3 is accelerated might contribute zero (or even a negative number) in a condition of a cross-participant test, because the negativity that often follows the P3 positivity also fell in the a priori fixed window (see Figure 1). However, in such situations, "real" effects may be present, even though they cannot be found under a fixed-form components assumption; and our example demonstrates this: the individual with an accelerated P3 does seem to be exhibiting a P3, it is just atypical in form.

In this paper, we explore the effectiveness of an ERP method that moves away from the fixed-form interpretation of components. Specifically, in a deception detection data set, we take advantage of a target detection condition, called the Fake in the experiment's terminology, which is independent of the conditions that detect deception: the Probe and Irrelevant conditions. The critical point is that the ERP arising from the Fake accurately characterises the temporal profile elicited by each participant's detection of a salient stimulus, i.e., it can be viewed as a *template* of such detection. This profile can then be used to test Probe vs. Irrelevant conditions for presence of such a pattern - guilt is determined by showing that the participant finds the Probe more salient than the Irrelevant. By analogy with *functional localisers* (Saxe, Brett, & Kanwisher, 2006), we call this a *functional profiler*. In fMRI, tasks are often included in experimental designs with the sole purpose of localising in space where a particular cognitive

function manifests in participants' brains, these are called functional localisers. The Fake ERP in this paper is conceptually used similarly but in respect of temporal profile, hence the term functional profiler.

Incorporation of such per-individual templating suggests adding hierarchy levels to the statistical model being applied. In typical group-level ERP analyses, a measure of interest is quantified for each participant; this might be area difference between two conditions, peak amplitude, latency, etc. A statistical test (t or ANOVA) is then run across these participant values. The quantification of error variance across participants introduces a distinct level, making this, strictly speaking, a hierarchical model with participants treated as a random effect (fixed effects would aggregate all participant single trials together for each condition, throwing away the participant distinction).

These traditional ERP models typically, though, maintain fixed-form components. That is, as previously discussed, identification parameters (such as window size and placement; and polarity) are fixed across participants, either by precedent from the literature or by inspection of the grand average (which is strictly fishing). If one is moving away from fixed-form components in order to accommodate inter-participant variance, it is natural also to consider identification parameters as a corresponding extra hierarchical level in the statistical model. For example, to accommodate inter participant variance, one might pick a different window or ERP template for each participant, which is legitimate fishing, as long as one formulates the test carefully in order to avoid type one error inflation, e.g., by using maximal statistics and/or permutation tests, as we do here.

In this context, this paper presents a methods-oriented demonstration of the increased statistical power arising from an application of a Monte Carlo permutation test, with (per-

individual) Functional Profiling. We consider a number of identity deception detection data sets, in which we seek to find a differential ERP response for a Probe stimulus, i.e., the participants' true birth date or true name. These data sets are taken from experiments demonstrating our Fringe-P3 deception detector (Bowman et al. 2014; Bowman et al. 2013) in which stimuli are presented so rapidly as to place them on the Fringe of awareness. The participant's brain then searches for salient stimuli, performing so called (sub)liminal salience search, and participant detection of a salient stimulus, particularly the guilty knowledge, elicits a P3 ERP component. In this context, our decision to assess our analysis method on two data sets allows us to test it in both low (the birthdays data) and high (the names data) signal-to-noise situations. We also use simulated data to explore how the sensitivity and specificity of our method vary with parametric manipulation of the signal-to-noise ratio. At all stages, we verify that the type one error rate is not inflated relative to the alpha level. We explore the effectiveness of our methods both at a group and individual level.

1.1   Identity Deception Detection

P3-based deception detection systems employ the P3 component (also known as the P3) to detect concealed information. Several versions of these systems have been implemented, e.g., (Abootalebi et al. 2006; Farwell et al. 2006; Meixner & Rosenfeld 2010a; Rosenfeld et al. 2004). Typically, these systems involve three main types of stimuli: Probes (**P**), which represent concealed information or crime details and can be recognized only by the guilty person; Irrelevants (**I**), which are frequent and task (crime)-irrelevant items; and Targets (**T**), which are similar to irrelevant items, but participants are asked beforehand to attend to these specific items and execute a task whenever they see one. For practical lie detection, the key comparison is

between Probe and Irrelevant ERPs, since, for the *non*-deceiver, the former would be an

Irrelevant. Importantly, the Probe for a deceiver typically generates a P3 ERP component, which

is absent for the Irrelevant. Thus, the P3 Probe serves as an index of deception. The Target

stimulus is presented for two reasons: first, it forces participants to pay attention to the presented

stimuli, as they will be asked to do a task whenever they see a Target. That is, it shows whether a

participant is cooperating or not. Second, as the Target stimuli are task-relevant items, they are

expected to evoke a typical P3, which can be used in ERP assessment methods, such as the

bootstrapped correlation difference method (Lawrence A. Farwell & Donchin 1991). Note that,

in our identity deception detectors, the term 'Target' was replaced by 'Fake', because in our

paradigms participants were asked to detect their *Fake* birthdates and names. The following

sections present the procedures of our identity deception detectors.

2   Methods

2.1   Birthday Deception Detection Experiment

2.1.1   Participants

 A total of 12 participants (7 female) took part in this experiment. All were students at the
University of Kent, right-handed, native English speakers and between 18 to 23 years of age (*M*:
21.12, *SD*: 2.4). They were paid for their participation. The participants were free from
neurological disorders and had normal or corrected-to-normal vision. No participant was dropped
from the experiment.

2.1.2   Stimulus presentation

Rapid Serial Visual Presentation (RSVP) streams were presented on a 20" LCD screen with a

refresh rate of 60 Hz and a resolution of 1600x1200, placed 60 cm from the participant's face.

Stimuli were presented using the Psychophysics toolbox version 3 running under Matlab 2010a.

Stimuli were 16 point, light grey, monospaced, and 'sans serif' characters presented on a completely black background. As a result, the visual angle for each stimulus was .95° in height and 2.2° in width, whereas the whole screen consisted of a rectangle of 28.52° by 37.56°. The rate of stimulus presentation was approximately 7.5 per second. Each RSVP trial was composed of a stream of 15 items, plus a start and stop item. The latter was either --. --- or ==.====, selected at random, and remaining on the screen for 133 ms. This last item was followed by a question ("did the last item consist of dashes or equal signs"). This task is used to maintain the participant's attention on the stream even after the critical item (Probe, Fake, or Irrelevant) has been presented, thereby avoiding muscle artefacts caused by response preparation or even initiation before the stream end. The starting item was XX.XXX, presented for 800 ms, to position the participant's focus on the stimulus presentation area. Apart from the first and last items, all stimuli were birthdays with a maximum width of 5 characters. The first 2 characters were a 2 digit number, followed by a middle dot character, and then the first 3 letters of a month's name. Distractor birthdays were chosen pseudo randomly to avoid repetition. All of the stream items were presented at the same screen location. SOA (Stimulus Onset Asynchrony, here used for the time between two stimuli) was set using a staircase test, as explained in Appendix B.

2.1.3   Stimuli

We refer to the Irrelevant, Probe, or Fake stimulus as a critical item. Thus, in the Guilty group, critical items could be the participant's real birthday (Probe), their fake birthday (Fake), or a birthday that was not known to the participant (Irrelevant). There were 3 blocks, each comprising a random sequence of Irrelevant, Probe, and Fake trials. For each trial type, there were 50 RSVP trials across the entire experiment (i.e., the three blocks); a critical item was

presented only once in each trial. The position of the critical item within the stream was selected pseudo randomly to appear in the fifth position (earliest) through to the tenth position (latest). The remaining items were (random birthday) distracters, each of which appeared rarely in the entire experiment. The participants chose one date as their Fake birthday and were instructed that their task was to respond affirmatively only to that birthday; i.e., in response to a yes/no question ('did you see your birthday?'), they were told to answer 'Yes'. They were explicitly told to answer 'No' to their real birthday (the Probe).

2.1.4 Recording apparatus

Data were recorded with a Brain Products QuickAmp recorder (Brain Products, Munich, Germany). Data were bandpass-filtered at recording, with a low-pass of 85 Hz and a high-pass of .30 Hz. Electroencephalographic data were recorded from the C_z, F_z, P_3, P_z, P_4, A_1, and A_2 electrodes from a standard 10-20 system (Jasper, 1958).

2.1.5 Analysis procedure

Data were analysed with the Brain Products Brain Vision Analyzer version 1.05. During the analysis, the data were software-filtered with a low-pass of 45 Hz and a high-pass of .5 Hz, with a slope of 12 dB. Data were re-referenced to average of the A_1 and A_2 electrodes (mastoids). In addition, eye blinks were detected using the Gratton and Coles algorithm in Analyzer (Gratton et al. 1983), and every trial that contained an eye blink marker was excluded from the remaining analysis. The number of trials remaining after artefact rejection, per condition, ranged between 41 and 50; Fake ($M = 45.6$, $SD = 3.39$); Probe ($M = 44.3$, $SD = 3.22$); Irrelevant ($M = 43.8$, $SD = 3.17$); this is out of 50 trials recorded for each condition. No participant was excluded from the study. The baseline was corrected from -100 ms to 0 ms from the onset of the critical item.

2.1.6   Innocents

To assess the empirical false alarm rate, birthday identity detection was conducted with a control group (of Innocents). The Innocent group were treated exactly as the Guilty group, except that the participants' real birthdays were never presented. The Probe item was a random birthday that was unknown to the participant. Thus, there were two Irrelevants, one of which played the (notional) Probe role and the other the Irrelevant role. We assessed our methods with the Innocent group data identically to the Guilty group. We recorded data from 10 participants (6 female) who were students at the University of Kent and 19-33 (M: 23.5, SD: 4.6) years of age. All participants were paid to participate, were native English speakers and were right-handed. The participants were free of neurological disorders and had normal or corrected-to-normal vision. No participant was excluded from the experiment.

2.2   Names-Deception Detection Experiment

The experiment presented in this section was introduced in (Bowman et al. 2013), in which the full experimental details are presented. Briefly, 15 participants were presented with 4 critical stimuli that we refer to as *Irrelevant1*, *Irrelevant2*, *Probe*, or *Fake.* These critical items could be a participant's first name (Probe), their assumed name (Fake), or one of two preselected names unknown to the participant (Irrelevant1 or Irrelevant2). The concealed information was the participant's first name (Probe). Critical items were presented in RSVP streams of name stimuli. Using a number of different P3 detection methods, e.g., our Weight Template (WT) and Peak-to-Peak, the aim was to investigate the difference in the brain responses of the participants to their first names (Probes) and to the irrelevant names (Irrelevant1 and Irrelevant2).

Innocents. As described in (Bowman et al. 2013), the Name deception detector was also conducted on a control group (of Innocents) to assess the empirical false-positive rate. This Innocent group was treated exactly as the Guilty group, except that the participant's real name was never presented. Thus, the Names identity detector was applied with 3 irrelevant names, giving 3 identical conditions: Irrelevant1, Irrelevant2, and Irrelevant3. These 3 Irrelevants yielded 6 pairwise comparisons because there are 6 permutations, e.g., (Irrelevant1, Irrelevant2), (Irrelevant1, Irrelevant3), (Irrelevant2, Irrelevant3), (Irrelevant2, Irrelevant1), and so on. We performed our statistical analysis on each such pair, with the first in the pair playing the (notional) Probe role and the second the Irrelevant role. Across the 8 participants who were assigned to the innocent group, there were 48 data sets, each comprising notional Probe and Irrelevant. We then analysed each data set with our ERP analysis methods, enabling a false alarm rate to be determined.

2.3 Methods for ERP Analyses
2.3.1 Peak-to-Peak

In most P3-based lie detection studies, the Peak-to-Peak (i.e., amplitude difference) procedure is used to measure the disparity between deception detection ERPs (Rosenfeld, Ward, Frigo, et al. 2015; Labkovsky & J. Peter Rosenfeld 2012; Bowman et al. 2013). Several P3 concealed information test studies have shown that this procedure is more accurate and sensitive for detecting P3 deception compared to other methods such as baseline-peak and correlation difference (Rosenfeld, Ward, Frigo, et al. 2015; Soskins et al. 2001; Hu et al. 2012; Meixner et al. 2013). Thus, it was chosen to be compared to our proposed method: the WT approach.

The Peak-to-Peak measurement determines whether the amplitude of the P3 response

elicited by a stimulus is greater than that elicited by another stimulus for the same individual. In

line with (Rosenfeld et al. 2004; Labkovsky & J Peter Rosenfeld 2012; Rosenfeld, Ward, Frigo,

et al. 2015), the word *peak,* in this paper*,* refers to averages across 100 ms intervals rather than

single time points. In this study, this method was applied to measure the disparity between Probe

and Irrelevant ERPs. First, subtracting the Irrelevant ERP from the Probe ERP generated a

difference wave. This difference wave will contain a P3 pattern if the Probe condition elicited a

bigger P3 response than the Irrelevant. To measure the P3, the Peak-to-Peak algorithm was used

within a (defined) time window from 300 ms to 1000 ms from stimulus onset. In that time

window, the algorithm searched for the maximal 100 ms interval (the highest peak). The

algorithm then searched from the first time point that follows this maximal 100 ms interval until

the end of the defined time window for the minimum 100 ms interval (the lowest peak). The

difference between the highest and lowest peaks was then calculated to define the Peak-to-Peak

measure. To evaluate the statistical significance of this measure, a randomisation (i.e., Monte

Carlo permutation) test was applied to generate a null hypothesis distribution. From this

distribution, a p-value can be inferred. If the p-value $< .05$, then the null hypothesis that the

Probe and Irrelevant ERPs are the same is rejected (for additional details see the Monte Carlo

permutation test section).

2.3.2   Weight Template (WT)

The new method presented here uses an individual-specific template to search for the P3

response. This template characterises an individual's P3 shape from the Fake condition, where

the largest P3 is expected; remember, the key guilt-determining comparison is between Probe

and Irrelevant, with the Fake typically being ignored. This WT approach handles situations in

which the shape of an individual's P3 is atypical. The *Template* was defined from the difference

between the Fake and Irrelevant ERPs. This template was then multiplied (point-wise) by the

difference between the Probe and Irrelevant ERPs. The result of this multiplication was used to

determine whether a participant was guilty or not. In more detail, firstly each ERP was

normalised, resulting in the mean over time being zero and the standard deviation being one (i.e.,

each ERP point becomes a Z-score) (Bandt et al. 2009).

$$norm\big(erp(t)\big) = \frac{erp(t) - mean(erp(1:T))}{std(erp(1:T))} \ , \qquad t = \in \{1, 2, \dots, T\}$$

Where $erp(t)$ is a single ERP that is a function of time (t), $std\big(erp(1:T)\big)$ is the standard

deviation and $mean\big(erp(1:T)\big)$ the mean across the ERP's time points and T is the number of

time points in the ERP. Secondly, once Probe, Irrelevant, and Fake ERPs were normalised, the

point-wise difference between the normalised Fake ERP $norm(F)$ and the normalised Irrelevant

ERP, $norm(I)$, was determined. Thirdly, the sum of the absolute values of these differences was

determined. Then, each difference calculated in the second step was divided by the sum

calculated in the third step. The result was a vector that we refer to as the *weightVector*:

$$weightVector(t) = \frac{norm(F(t)) - norm(I(t))}{\sum_{t=1}^{T} |norm(F(t)) - norm(I(t))|}$$

The *weightVector* was used as a template, with which the difference between the normalised

Probe ERP $norm(P)$ and the normalised Irrelevant ERP $norm(I)$ was multiplied:

$$V(t) = \big[norm\big(P(t)\big) - norm\big(I(t)\big)\big] \times weightVector(t)$$

Finally, the P3 weighted difference was obtained by calculating the sum of $V(t)$ over time t:

$$weighted\_Difference = \sum_{t=1}^{T} V(t)$$

The underlying principle of the WT is that the P3 weighted difference value will be large when the difference between Probe and Irrelevant (time) point-wise matches the same difference between Fake and Irrelevant. Thus, we are effectively using the Fake – Irrelevant weight as a template (or, indeed, a kernel) for an individual's characteristic P3, against which the key Probe – Irrelevant comparison is assessed. For the purpose of this study, we used the weighted difference value as a scale for the presence or absence of the P3 in the Probe ERP. The larger this value is, the more likely the P3 was elicited and the more likely a guilty decision could be made. To evaluate this value statistically, a randomisation (i.e., Monte Carlo permutation) test was applied. Thus, for each participant, a null hypothesis distribution was generated, and a p-value was then calculated. To reject the null hypothesis that Probe and Irrelevant ERPs are not different, and thereby detect a participant as guilty, the p-value should be less than 0.05.

2.4   Statistical analyses
2.4.1   Monte Carlo Permutation Test

As mentioned in the previous section, the performance of the methods was evaluated using Monte Carlo permutation resampling (randomisation test), which has been extensively used to analyse EEG (Blair & Karniski 1993; Groppe et al. 2011) and fMRI data (Brammer et al. 1997). As a central purpose of this analysis was to classify participants into guilty and innocent, the methods were applied on a per-participant basis (individual-level analysis). In general, a randomisation test involves the following two steps: (a) the computation of some statistic on the true observed data and (b) an evaluation of its p-value under the randomisation distribution. This distribution arises as a result of the random assignment of the units (in our case, *trials*) to conditions.

Because the key comparison in our ERP analysis methods is between the Probe and Irrelevant conditions, we applied the randomisation test as follows: firstly, the smallest number of trials between the Probe and Irrelevant conditions was determined and denoted by m (conditions could contain different numbers of trials due to artefact rejection). Secondly, m trials were selected (at random without replacement) from the Probe condition, and m were selected from the Irrelevant condition. Thirdly, a matrix of size (*2 × m rows, and max time point columns*) was populated with the 2 x m selected trials, with row position randomised, as justified by exchangeability.

Next, a pair of conditions was generated: the first, the surrogate Probe, was generated from the first half of the matrix rows, and the second, the surrogate Irrelevant, from the remaining half. The desired analysis (Peak-to-Peak or weight template) was then applied on the two surrogate conditions. The procedure was repeated 1000 times. In each iteration, an analysis result was obtained. The p-value was then calculated as the number of randomised results that were greater than the true observed value divided by the number of randomisations.

2.4.2 Group and Individual-Level Analysis

We assessed our methods on both a per-individual, which is required in many applications, including P3-based concealed Information Test, and on a group-level basis, as required for a population-level inference. At the individual-level, we determined whether the brain response evoked by the Probe stimulus was significantly different from that evoked by the Irrelevant within an individual. As described earlier, a randomisation was used to generate a p-value for each participant.

To determine whether there was a significant difference between the Probe and Irrelevant responses at the group level, a paired t-test was used. Each participant was assigned a pair of

Peak-to-Peak sizes, one from Probe and one from Irrelevant. A paired t-test was then applied

across participants in each experiment. Peak-to-Peak sizes of both conditions in Names and

Birthdays data sets are presented in tables 1 and 2 respectively.

In the WT method, we compared Probe and Irrelevant conditions by generating WT

values per-participant for each condition. The Fake served as a template and was applied as

described earlier except only the Fake condition was used, i.e.,

$$weightVector(t) = \frac{norm\big(F(t)\big)}{\sum_{t=1}^{T}\big|norm\big(F(t)\big)\big|}$$

Then, for example to obtain a WT value of condition X, we applied the $weightVector(t)$ to X

as,

$$WT = \sum_{t=1}^{T}\big(norm(X(t)) \times weightVector(t)\big)$$

A paired t-test was then applied to the WT values of both conditions across all participants. The

WT values of both conditions in the Names and Birthdays data sets are presented in Tables 2.

2.5   Simulated EEG Data

The aim of generating simulated data was to explore how the sensitivity and specificity of the

WT method vary with parametric manipulation of the Signal-to-Noise Ratio (SNR).

2.5.1   Intrinsic validity of the WT

To explore the validity of the WT method, we applied it to a set of artificial data for

which we already know that the null hypothesis is true (i.e., there is no significant difference

between the conditions). The aim was to assess the false-positive rate (i.e., the Type I error rate)

of the method. Statistically, false-positive errors occur when a statistical test rejects the null

hypothesis (H0) when it is in fact true (i.e., the WT indicates a significant difference between two conditions when none is present). The probability of a Type I error is always set in advance and should be equal to the alpha level of a statistical test, in our case .05.

We assessed our method in two intrinsic validity tests: the first was on pure noise data, while the second was on real human ERPs plus random noise. In the first test, we generated a set of simulated EEG data using the function *noise* that was used in (Yeung et al. 2004; Yeung et al. 2007); this contains auto-correlation statistics consistent with human EEG[1]. Specifically, we generated 1000 simulated EEG data sets. Each data set was composed of 150 random noise trials. These trials were then randomly split into three equal sets, which we refer to as simulated Fake, Probe, and Irrelevant conditions; thus, each condition comprised 50 trials. A simulated ERP was then generated for each condition by taking the average of the 50 trials. Using our Monte Carlo permutation test, we applied the WT method to each data set in an identical manner as in our analyses of the real experimental data. In this way, applying the WT to each data set will yield 1000 p-values. The Type I error rate was then defined as the proportion of p-values below .05.

In the second validity test, we assessed the Type I error of the method in a slightly different way, in which we compared between two conditions that contain a real human ERP signal. Particularly, we explore the validity of the WT approach by creating two artificial conditions (Probe and Irrelevant) that have the same signal in, where *signal* refers to an ERP containing a P3. The reason for doing such an assesment is that the Irrelevant ERP may have a similar shape to a Probe   (Bruno Verschuere, Gershon Ben-Shakhar 2011). In other words, in

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[1] The simulated EEG data was generated using the function *noise* described at
http://www.cs.bris.ac.uk/~rafal/phasereset/

some cases, an Irrelevant ERP may contain a signal (a small P3) as can be seen in (Lawrence A.

Farwell & Donchin 1991; Rosenfeld et al. 2004). Indeed in general, ERPs may contain some sort

of response to a stimulus, which is a signal, and the null hypothesis is that the form of this signal

does not change across conditions. Thus, it was vital to assess the Type I error rate of our method

when conditions have similar shapes. The procedure was as follows: we created two artifitial

conditions (Probe and Irrelevant), using the same signal (human ERP) plus pure random noise.

This signal was in fact the grand average of the Probe condition in the Names experiment (see

Figure 2). As in the first test, we again generated 1000 simulated EEG data sets, each consisting

of 50 Probe trials and 50 Irrelevant trials, in which each trial of both conditions contained the

same signal added to random noise $noise(t)$, that is,

$$X_n(t) = Signal(t) + noise_n(t), \quad n \in \{1, 2, \dots, 50\}, \quad t \in \{1, 2, \dots, 2200\}$$

where *t* is a time point and *n* a trial. An artificial ERP was then generated for each condition by

taking the average of the 50 trials. We then applied the WT method to each condition in exactly

the way we did in our analyses of the real experimental data. In particular, the *Template* for the

WT method was constructed using the grand average of the Fake condition in the Names

experiment (see Figure 2). In this way, this test will yield 1000 p-values. The Type I error rate

was then defined as the proportion of p-values below .05. In these first and second tests, the

parameters used to generate the noise time series were exactly the same; the length of a single

trial was 2200 time points and the sampling frequency was 2000 Hz.

2.5.2   Comparing method's performance at different level of SNR

The aim of generating simulated data was to evaluate the performance of the WT and

Peak-to-Peak methods with different levels of SNR (Signal-to-Noise Ratio). We varied the SNR

by adding a different amount of noise to the Probe and Irrelevant ERPs of each participant in the

Names deception detector experiment. Specifically, first, Probe and Irrelevant ERPs were generated in the normal manner. Second, we generated a set of *Surrogate* trials, each of which was the addition of a condition ERP and a single noise trial. For example, a single *surrogate* Probe trial can be defined as the following:

$$EEG\_Probe(t) = P(t) + (K \times (noise(t))), \quad t= 1, 2, 3, T, \quad K= 1, 7, 13, ... 49$$

Where *P* is the participant's Probe ERP, *noise* is a vector of (auto-correlated) random simulated noise, and *T* is the number of time points. To vary the amount of noise in a single trial, we scaled the amplitude of the *noise* by multiplying the vector that represents it by a number (a 'scalar'), which we denote as *K*. In this way, a surrogate Probe ERP was created by generating ($N =50$) *surrogate* Probe trials and then taking the average of these N *surrogate* trials. A surrogate Irrelevant was created in the same way. Third, we estimated the SNR of the surrogate Probe and Irrelevant ERPs by calculating the ratio between the root mean square of the signal (Probe/Irrelevant) and the *noise* (estimating the SNR process will be explained in the next section). Next, we applied a randomisation test with our main methods (Peak-to-Peak or WT) to both surrogate ERPs providing p-values in an identical manner as with the real experimental data (see the randomisation test section). 100 iterations of these steps will yield 100 p-values for each method and 100 SNR estimates for each condition. Next, a single average p-value (across the 100 individual p-values) was obtained for each method. In addition, for each surrogate condition, an average SNR_{avg} value was estimated (across the 100 SNRs). This procedure was repeated for every *K* value (from 1 to 49), in steps of 6.

This procedure evaluates the performance of each method in 2 different ways. First, the procedure compares the average of 100 p-values of each method at different levels of SNR; the smaller an average p-value relative to a particular alpha level (in our case .05), the greater the

statistical power of that method. Second, the procedure calculates the area under a ROC

(Receiver Operating Characteristic) curve (abbreviated AUC) for each method; see next section.

The above procedure can be summarised as follows:

    i.   For each participant, determine the Probe and Irrelevant ERPs.

    ii.   Set K=1

    iii.   For a given K, generate surrogate (noisy) Probe and Irrelevant ERPs, each of

which is composed of 50 trials.

    iv.   Estimate the SNR of the surrogate Probe and Irrelevant.

    v.   Apply a randomisation test with Peak-to-Peak and WT methods to the surrogate

ERPs, thereby generate a null hypothesis distribution and calculate a p-value for each method.

    vi.   Repeat the previous steps (iii-v) 100 times.

    vii.   For each method, calculate the average of the 100 p-values that were obtained by

the 100 iterations as well as the average SNR (SNR_{avg}) for each condition.

    viii.   For $K <= 49$, increase K by 6 and return to step iii.

    ix.

2.5.3   Statistical Analyses on the Simulated Data

Signal-to-Noise Ratio (SNR)

      In our simulated data analyses, the SNR was used to quantify the ratio between the ERPs

(Probe/Irrelevant) and the noise. For each condition, the SNR was estimated from the ratio

between the root mean square (RMS) amplitudes of an ERP (Probe/ Irrelevant) and the noise

(Drongelen 2006). First, for each single trial n, we estimated the SNR as follows:

$$SNR_n = \frac{rms(ERP)}{rms(noise)}$$

where the *rms* of time series *x* across time points *t* can be defined as (van Drongelen, 2006),

$$rms(x) = \sqrt{\frac{1}{T} \sum_{t=1}^{T} x(t)^2}$$

The *rms* of an ERP was calculated in a time window from stimulus onset to 1000 ms post-stimulus. We calculated the amount of noise in the ERP level as

$$SNR_{AVG} = A \times \frac{1}{\sqrt{N}}$$

where *A* is the average of all of the SNRs across *N* trials, i.e.,

$$A = \frac{1}{N} \sum_{n=1}^{N} SNR_n$$

ROC curve

A receiver operating characteristic (ROC) curve is a means to evaluate the performance of classifiers as their discrimination criterion (threshold) is varied. ROC graphs are used in signal detection theory to depict the trade-off between the sensitivity (hit rate) and specificity (false alarm rates) of classifiers(Egan 1975; Van Erkel & Pattynama 1998). A ROC graph is a 2-dimensional graph in which the true-positive (hit) rate is plotted on the Y axis and the false positive rate is plotted on the X axis. A single point in ROC space represents an output of a classifier in terms of the hit (true positive) rate and the false-positive rate. To quantify ROC performance, measurement of the area under the ROC curve (AUC) is used *(Fawcett, 2006).* In this study, ROC curve analysis was used to evaluate the performance of our methods with simulated data. In our simulated data, for each SNR value, 100 p-values were obtained by each method. For each method, we then calculated the true-positive rate as the number of p-values

that were less than a certain alpha level threshold divided by 100. To calculate the false-positive

rate, we created 2 data sets that were composed of (pure) noise trials and that did not contain any

signal. Specifically, we used the same noise function to generate at random 100 noisy trials; the

average of the first 50 trials played the role of a Probe and the average of the remaining trials

played the role of an Irrelevant. We then applied our methods with a randomisation test exactly

as described earlier. Here, 100 iterations of this process will yield 100 p-values. The false-

positive rate was then calculated at different alpha levels as the number of p-values that were less

than that alpha level divided by 100. The threshold (alpha level) varied from 0 to 1, with a step

of .01, to estimate both rates.

3   Results

3.1   Results of Simulated Data Analysis

As the WT method is new, we must first confirm its validity. Thus, the Type I error rate, 'the

true false-positive rate', of the method was assessed on simulated data. Statistically, the Type I

error rate of the method should be .05 (our alpha level). As described earlier, we assessed this

rate in two tests: in the first test, we generated 1,000 groups of artificial data sets (pure noise) for

all of the conditions (Fake, Probe, and Irrelevant). In the second test, we compared between two

artificial conditions (Probe and Irrelevant) with the same signal. The average p-values of 1,000

WT runs in the first and second tests were .489 and .504, respectively. The average p-value of

both tests was indeed approximately .5, as expected when there is no difference between the

Probe and the Irrelevant conditions. Importantly, the Type I error rates of the method in the first

and second tests were .039 and .0484. These results confirm that the false-positive rate of the

method is not larger than our alpha level of .05. Figure 4 shows the uniform distributions of the 1,000 p-values for both tests.

3.1.1   P-value by SNR

As noted previously, the aim of generating artificial data sets was to evaluate the WT methods on data with pre-defined settings, such as the SNR level. Specifically, we were interested in comparing the performance of the WT and Peak-to-Peak with varying SNRs.

The statistical analyses showed that the performance of both methods decreased as the SNR declined, as expected. As the amount of noise increased, the p-values increased towards .5; the p-value corresponding to identical Probe and Irrelevant. At very high SNRs, both of the methods performed successfully, with nearly equal p-values across all participants. For the participants who elicited sharp and well-defined Peaks, both methods continued to detect the peaks successfully, even at low SNR levels. For example, participant 8 (see Figure 4) has high positive P3 peaks, which yielded significant p-values ($p<.001$), even at low SNRs of .02. As SNRs dropped, the WT displayed increasingly better performance relative to Peak-to-Peak, with the p-values of the WT generally smaller than the corresponding p-value of the Peak-to-Peak. The per-individual p-values at each SNR level for both methods are presented in Table A.1 in Appendix A. At each SNR, the grand average p-values for both methods were obtained by taking the mean of all p-values across all participants. This was done at each SNR. Table 1 showed that at high SNRs, the grand mean p-values of both methods were nearly the same whereas, at low SNRs, the grand mean p-values of the WT were less than the grand mean p-values of Peak-to-Peak. Moreover, in order to obtain confidence intervals, a non-parametric bootstrap confidence interval method was used (Carpenter & Bithell 2000; Wasserman & Bockenholt 1989).

Specifically, for each SNR, 95% confidence intervals for the grand average p-value were

obtained by bootstrapping 1000 times over 1500 p-values (15 participants × 100 p-values). The

grand average p-values and 95% confidence intervals are shown in Table 1. Figure 6 shows the

grand average p-value as a function of the SNR. As can be seen in Figure 6, as SNR decreased,

the distance between confidence intervals of the two methods increased suggesting an increasing

(statistically significant) difference between methods.

3.1.2   AUC by SNR

Overall, our results also indicate that, broadly speaking, with high SNR ERPs, the two

methods are equally successful at detecting deception, i.e., the P3 component. However, at low

SNRs, the WT significantly outperforms the Peak-to-Peak. As can be noted from Table A.2, as

the K value increased, SNR decreased towards 0, and therefore the AUC of both methods

decreased towards .5. The AUC measures of both methods demonstrated that for the participants

who elicited a clear and high P3 component, the performance of the two methods were almost

equal, reaching towards AUC=1. For example, as shown in Figure 4, participant 8 has a large

positive P3 peak (amplitude>10 µv) and, although a large amount of noise was added (K <= 31)

to the Probe waveform, the P3 peak remained stable and resistant, and thus both of the classifiers

detected the component successfully with AUC>.99. However, for different levels of SNR across

all individuals, the performance of the WT was more resistant to noise. The lowest AUC for the

WT was approximately .54, for participant 1, and this result was not surprising since before noise

was added, there was already considerable noise in the Probe waveform, and there was no

evidence of P3 presence (Figure 4 depicts ERPs of participants 1 in the Names experiment).

Figure 7 shows selected ROC curves considering different levels of SNR (different K values).

The ROC curves are presented at three different K values (K=13, 31, and 49) of the WT and

Peak-to-Peak for the simulated data from participants 1, 2 and14. For each participant, as K

increases (i.e., the noise increases), the ROC curves of both methods move from the upper left

corner towards the diagonal (i.e., the performance of each classifier decreases).

The per-individual AUC scores at different levels of SNR are presented in Table A.2 in

Appendix A. Furthermore, in order to confirm the statistical difference between performances of

the two methods at a group level, a paired t-test was applied to AUC scores at each SNR level

across all 15 participants. That is, a paired t-test at each SNR level was applied to the 15 (no. of

participant) AUC pairs (one for each method) to infer whether the performance of methods are

statistically different. Table 2 shows the grand average AUC scores and the outcomes of the

paired t-tests, which show that there was no significant difference between the performances of

methods at high SNR levels. However, there was a significant (and increasing) difference as the

SNRs decreased.

3.2   Results of Experimental Data

3.2.1   ERPs of the Birthadays and Names data sets

Because the P3 amplitude is expected to be maximal over the parietal areas of the scalp

(Lawrence A. Farwell & Donchin 1991), our analysis was focused on the Pz channel. This is also

in line with (Labkovsky & Rosenfeld 2012; Rosenfeld et al. 2015).

Figure 2 shows the grand average ERPs for the 4 conditions in the Names experiment. Large P3

responses were elicited by Probe and Fake but not by Irrelevant1 or Irrelevant2. Irelevant1 and

Irrelevant2 are very similar.

Figure 3 shows the grand average ERPs (across all of the participants) of the Birthdays experiment in the Guilty group for the Fake, Probe, and Irrelevant responses. The Irrelevant and Probe patterns are similar, with the exception that, in the typical P3 time window, the Probe elicited a small P3, whereas the Fake pattern significantly differed from the other two responses, showing a large and clear P3.

We performed WT and Peak-to-Peak measurements at a single subject level for measuring the statistical significance of the brain responses elicited by the Probe and Irrelevant conditions. As noted, to diagnose guilt or innocence, the P3 responses of both conditions were compared: in a Guilty participant, Probe is expected to be larger than Irrelevant; in an Innocent participant, no difference is expected between the conditions because the Probe is just another Irrelevant. A randomisation technique was used with each analysis method, Peak-to-Peak and WT, generating a p-value for each participant. In the Names Experiment, since we have two Irrelevants (Irrelevant1 and Irrelevant2) conditions, the key comparison was between Probe and Irrelevant1. All classification results were calculated at an alpha level of .05.

3.2.2   Hit and false alarm rates

In the Names experiment, with the peak-to-peak method, 12 participants (12/15) in the Guilty group were detected as guilty (80% hit rate). The false alarm rate using Peak-to-Peak was 8% (4/48). In the Birthdays experiment, the hit rate was 17% (2/12), and the false alarm rate was 20% (2/10). The WT had a hit rate of 93% in the Names experiment; 14 participants (14/15) in the Guilty group were detected as guilty, while the false alarm rate was 2% (1/48). In the Birthdays experiment, the hit rate was slightly better than for the peak-to-peak, 33% (4/12), with a false alarm rate of 10% (1/10). Tables 3 and 4 present per-individual p-values arising from both

methods for the Birthdays and Names experiments, respectively. The false-positive test

outcomes for the Names and Birthdays data sets are shown in Tables 5 and 6 respectively.

A group-level analysis using paired t-tests of Probe against Irrelevant1 in the Names data

sets resulted in significant P-values for WT, ($M = .799$, $SD = .335$, $t(14) = 9.22$, $p = 2.5e-07$),

and Peak-to-Peak, ($M = 8.16$, $SD = 6.49$, $t(14) = 4.86$, $p = .00025$). WT and Peak-to-Peak values

of Probe and Irrelevant1 in the Names data sets are shown in Table 3. For the Birthdays data sets,

a paired t-test was applied to compare between Probe and Irrelevant at a group level. Using

Peak-to-Peak, the outcomes of the paired t-test showed no significance difference between Probe

and Irrelevant, ($M = 1.0006$, $SD = 2.215$, $t(11) = 1.56$, $p = .146$). In contrast, using the WT, a

paired t-test resulted in a significant result, ($M = .316$, $SD = .491$, $t(11) = 2.23$, $p = .047$). WT

and Peak-to-Peak values of Probe and Irrelevant in the Birthdays data sets are presented in Table

4. Figure 5 presents Pz ERPs for participants 1, 2, 8, and 14 in the Names experiment. The Probe

waveform of participant1 has no clear positivity within the critical time window (300-1000 ms),

which is, to some extent, similar to the Irrelevant1 waveform. Thus, neither method was able to

differentiate between the two waveforms; the p-values of both methods were >.25. The null

hypothesis distributions of both methods for participant 1 are shown in Figure 8. The true

observed values of both methods were small and fell around the distribution's centre, which

resulted in a large p-value. Although the Probe condition for participant 2 only elicited a weak

and narrow positivity at approximately 530 ms, which is absent in the Irrelevant1 ERP, both

methods distinguished Probe from Irelevant1. However, the p-value of the WT (p=.011) is

samller than the p-value of the Peak-to-peak measurement (p=.080). This finding arises because

Probe and Fake follow a somewhat similar pattern in the defined time window. Examination of

the participant's ERPs reveals that, from approximately 550 ms to 1000 ms, the patterns of the

Fake ERP and Probe are similar, and thus the WT can effectively detect the difference between the Probe and Irrelevant1.

The Probe ERP of participant 8 has a clear and high positive peak (i.e., a typical P3 shape) (see Figure 5). Therefore, both of the methods detected the component well with a p-value <.001. The null hypothesis distributions for participant 8 are presented in Figure 8. While the Peak-to-Peak revealed no evidence of the presence of P3, the WT was capable of detecting participant 14 as guilty. As seen from participant 14's ERPs in Figure 5, the Probe and Fake waveforms display atypical negative deflections at approximately 300 ms. These deflections were followed by slight respectively sharp positivity in the Probe respectively Fake waveforms. In other words, the two conditions, to some extent, display a similar pattern in the defined time window, which enables the WT to demonstrate deception for this participant; the p-values of the WT and Peak-to-Peak were .012 and .239, respectively. Figure 9 shows Pz ERPs for participants 6 and 7 from the Birthdays experiment. The Probe ERP of participant 6 has a positive deflection that peaks at approximately 550 ms post-stimulus onset (Figure 9, left). By contrast, the Irrelevant ERP has no such peak or evidence of a P3 pattern. Therefore, the WT and Peak-to-Peak measures identified the participant as guilty with p-values of .014 and .04, respectively. The Probe condition of participant 7 elicited a positive deflection, but its peak is late (around 650 ms) (Figure 9, right), which might be considered an atypical P3. Peak-to-Peak failed to identify that pattern significantly. By contrast, because the Probe and Fake ERPs are in the same positive direction between approximately 400 ms and 680 ms, the WT was able to detect the P3 response with a (significant) p-value (p=.02).

It is worth to note that the performance of the WT was also compared with the base-to-peak (b-p) measurement, which has been used in several P3-based concealed Information studies

(Rosenfeld, Ward, Thai, et al. 2015; Rosenfeld, Ward, Frigo, et al. 2015). The b-p was measured

by finding the maximally positive 100ms interval average within the critical time window (from

300 to 1000ms pot stimulus onset).

In the Names experiment, 11 participants (11/15) in the Guilty group were detected as guilty

(73% hit rate) using the b-p method. The false alarm rate was 12.5% (6/48). In the Birthdays

experiment, the hit rate was 17% (2/12), and the false alarm rate was 0% (0/10).

The above results showed that the WT produced more accurate classification than the Peak-to-

Peak and b-p methods. As can be noted, when applied to the Names data, the WT and Peak-to-

Peak methods had better performance than the b-p measurement. In the Birthdays experiment,

the b-p and Peak-to-Peak methods had comparable results. However, it has been found that the

Peak-to-Peak performed better than the b-p method in classifying ERPs of P3 deception

detectors (Soskins et al. 2001; Rosenfeld et al. 2004).

4 Discussion

In this paper, we have proposed a simple tool for classifying deception detection ERPs based on cross-participant templating. The most important aspect of this method is that it uses the difference between Fake and Irrelevant as a template. The WT, then, is a template for each individual's P3 pattern. In this way, the WT method moves away from the standard fixed-form interpretation of components, in order to accommodate cross-individual variability in the P3, which can be large. If this Fake - Irrelevant template matches the difference between the Probe and Irrelevant, then the weighted difference will be positive and big. Thus, the method addresses a situation in which the shape of an individual's P3 pattern is atypical. In this way, when applied as a group-level test, identification parameters can be seen as a further hierarchical level. Using a Monte Carlo permutation test, we have evaluated the performance of our method on a number of identity deception data sets in which we sought to identify a distinguishing ERP response for a participant's true birthday or true name. The performance of the WT was compared with that of Peak-to-Peak, which is typically used in ERP-based lie detection studies (Abootalebi et al. 2006; Bowman et al. 2013; Bowman et al. 2014; Rosenfeld et al. 2004; Rosenfeld, Ward, Frigo, et al. 2015), and is widely considered as an accurate measurement for diagnosing lie detection ERPs (Soskins et al. 2001).

However, our results indicate that when applied to the Names and Birthdays data sets, the WT outperformed Peak-to-Peak in terms of both sensitivity and specificity. The hit rate using the WT was 93% and 33% for the Names and Birthdays data sets, respectively. However, the hit rates using Peak-to-Peak were 80% and 17%, respectively. In terms of the false alarm rates, using the WT, they were 2% and 10%, compared to 8% and 20% with Peak-to-Peak for the

Names and Birthdays data, respectively. With the Birthdays data, both methods performed

poorly because of the low SNR ERPs that were obtained during the experiment, which can be

seen clearly in the grand average ERPs (see Figure 2)[2]. Thus, the low hit rate of this

experimental data is not due to the small alpha level (.05) that was applied in our analysis

because we re-applied our analysis at the .1 alpha level (note, a number of workers in the lie

detection domain routinely use a .1 alpha level (Hu et al. 2012; Meixner & Rosenfeld 2010b;

Rosenfeld et al. 2004). Although this value is still low, the hit rate of the WT slightly increased

to 50% (6/12), and with Peak-to-Peak, it increased to 33%. At a group level, both methods

reported significant differences between Probe and Irrelevant1 in the Names data sets. For the

Birthdays data sets, only the WT showed a significant difference between Probe and Irrelevant.

In a broader sense, the WT method is particularly likely to offer benefit at lower SNRs,

when the Probe P3 is weakened by the relative strength of noise, making it difficult for Peak-to-

Peak to detect it. This benefit of WT will particularly be the case when the Fake P3 is strong

despite a relatively weak Probe P3, as often found in the lie detection setting. In this context, the

Fake is effectively an explicit target, which yields a large P3b (Bowman et al. 2013). Clearly

though, when the Fake and Probe elicit different ERP patterns, the WT method's advantage will

weaken.

We also used simulated data to demonstrate how the sensitivity and specificity of our

methods vary at different levels of SNR. ROC curve analyses indicated that the two methods

display comparable performance when applied to ERP responses with well-defined positive

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[2] Both the Birthdays and Names experiments are examples of what we call the Fringe-P3 deception detection
(Bowman et al. 2013; Bowman et al. 2014) SNR and Birthdays so much lower. Although still to be definitively
confirmed, we believe this is because the date stimuli were presented as two parts with a fixation cross in between
and participants monitored only one of the two parts looking for, say, the Fake day. As a result the Probe date,
whose salience is due to the combination of both parts, is not ''seen''.

peaks; i.e., at high SNRs. However, Peak-to-Peak is more sensitive to noise than the WT. At all

SNR levels that were applied in our simulation, the WT was more stable and provided more

accurate measures.

Although not reported, we have also applied the cross-correlation difference (CD)

method to the Names and Birthdays data sets. This method was first introduced by (L A Farwell

& Donchin 1991) and has been used by others to assess the ERP responses of P3-based lie

detection. The CD method simply compares two cross-correlation coefficients: the cross

correlation of Probe (P) and Fake (F) (R1 (P, F)) and the cross correlation of P and Irrelevant (I)

(R2 (P, I)). The comporison is that if R1 is greater than R2, then the Probe would be more similar

to the Fake than to the Irrelevant and, therefore, the participant would be guilty. When CD was

applied to our data sets, the hit rates were 33% for the Names data and 0% for the Birthdays data

sets. However, its poor performance was not surprising because CD is much too conservative a

measure. The criterion for judging guilt is that the Probe is closer to the Fake than to the

Irrelevant, rather than being simply different from the Irrelevant (which is the difference needed

to demonstrate a lie). Indeed, Rosenfeld and colleagues have previously reported that this

method is less powerful than other methods (Rosenfeld et al. 2004). They indicated that, when

the Fake and Probe waveforms are out of phase, the result of the cross correlation would be low

even if the Probe contained a real P3 component. Thus, in this situation, CD will fail to detect the

component.

Comparing the WT with Peak-to-Peak and CD reveals that, in a sense, the WT approach

combines aspects of the other two methods. The WT shares an aspect of the Peak-to-Peak

method because it looks specifically for a difference between the Probe and Irrelevant, which is

the criterion for judging guilt. The WT also shares an aspect of the CD method because it

considers the Fake pattern. However, rather than directly comparing Probe to Fake, as CD does, it uses the form of the Fake to guide the (Probe – Irrelevant) comparison. Thus, it might be said that the WT takes the best of Peak-to-Peak and CD, which leads it to outperform both. From these findings, we conclude that either Peak-to-Peak or the WT will work effectively when applied to ERPs with a high SNR. In other words, their performances will be comparable when applied to ERPs that contain sharp or high positive peaks. By contrast, the WT will be more appropriate and more accurate than the other methods when applied to ERPs with low SNRs.

Although, the WT approach has been developed and illustrated here in the context of a specific application, ERP deception detection, we do believe the functional profiler idea is broadly applicable, In particular, in the same manner that functional localiser conditions are frequently incorporated into fMRI studies, functional profiler conditions could be incorporated into ERP experiments. These would be conditions known to elicit a particular component or ERP pattern, e.g., an N400 or P3. Then individual-specific profiles from such conditions could be used as templates to investigate presence of such components in experimental conditions targeted at the hypotheses of interest.

There has been some debate in the fMRI literature on the value of functional localisers. (Friston et al. 2006) Many of the points made can also be highlighted in the context of the ERP functional profile we consider here. For example, Friston et al. (2006) argued that running a pre experimental functional localiser was problematic. However, in the experiments presented here, our Fake condition (the profiler) is integrated into the main experiment, avoiding order and time effects. These might, for example, arise if a pre-experimental profiling condition were run, which, say, exhibited worse performance than the main experiment due to perceptual learning.

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References

Abootalebi, V., Moradi, M.H. & Khalilzadeh, M.A., 2006. A comparison of methods for ERP assessment in a P300-based GKT. *International Journal of Psychophysiology*, 62(2), pp.309–320.

Bandt, C. et al., 2009. A simple classification tool for single-trial analysis of ERP components. *Psychophysiology*, 46(4), pp.747–57. Available at: http://www.ncbi.nlm.nih.gov/pubmed/19386045 [Accessed February 4, 2013].

Blair, R.C. & Karniski, W., 1993. An alternative method for significance testing of waveform difference potentials. *Psychophysiology*, 30(5), pp.518–524. Available at: http://www.ncbi.nlm.nih.gov/pubmed/8416078.

Bowman, H. et al., 2014. Countering countermeasures: detecting identity lies by detecting conscious breakthrough. *PLoS one*, 9(3), p.e90595. Available at: http://www.pubmedcentral.nih.gov/articlerender.fcgi?artid=3946631&tool=pmcentrez&rendertype=abstract [Accessed April 6, 2014].

Bowman, H. et al., 2013. Subliminal Salience Search Illustrated: EEG Identity and Deception Detection on the Fringe of Awareness M. Sigman, ed. *PLoS ONE*, 8(1), p.e54258. Available at: http://dx.plos.org/10.1371/journal.pone.0054258 [Accessed January 28, 2013].

Brammer, M.J. et al., 1997. Generic brain activation mapping in functional magnetic resonance imaging: a nonparametric approach. *Magnetic Resonance Imaging*, 15(7), pp.763–770. Available at: http://www.ncbi.nlm.nih.gov/pubmed/17668781.

Bruno Verschuere, Gershon Ben-Shakhar, E.M., 2011. *Memory Detection: Theory and Application of the Concealed Information Test*, Cambridge University Press.

Carpenter, J. & Bithell, J., 2000. Bootstrap confidence intervals: when, which, what? A practical guide for medical statisticians. *Statistics in medicine*, 19(9), pp.1141–64. Available at: http://www.readcube.com/articles/10.1002/(SICI)1097-0258(20000515)19:9<1141::AID-SIM479>3.0.CO;2-F [Accessed November 16, 2013].

Drongelen, W. van, 2006. *Signal Processing for Neuroscientists: An Introduction to the Analysis of Physiological Signals*, Academic Press.

Egan, J.P., 1975. *Signal detection theory and ROC-analysis*, Academic Press.

Van Erkel, A.R. & Pattynama, P.M., 1998. Receiver operating characteristic (ROC) analysis: basic principles and applications in radiology. *European Journal of Radiology*, 27(2), pp.88–94. Available at: http://www.ncbi.nlm.nih.gov/pubmed/9639133.

Farwell, L.A. & Donchin, E., 1991. The Truth Will Out: Interrogative Polygraphy ("Lie Detection") With Event-Related Brain Potentials. *Psychophysiology*, 28(5), pp.531–547. Available at: http://doi.wiley.com/10.1111/j.1469-8986.1991.tb01990.x [Accessed March 27, 2012].

Farwell, L.A. & Donchin, E., 1991. The truth will out: interrogative polygraphy ("lie detection") with event-related brain potentials. *Psychophysiology*, 28(5), pp.531–547.

Farwell, L.A., Richardson, D.C. & Hernandez, R.S., 2006. Brain fingerprinting in field conditions. In *Psychophysiology*. pp. S38–S38.

Friston, K.J. et al., 2006. A critique of functional localisers. *NeuroImage*, 30(4), pp.1077–1087.

Gratton, G., Coles, M.G.. & Donchin, E., 1983. A new method for off-line removal of ocular artifact. *Electroencephalography and Clinical Neurophysiology*, 55(4), pp.468–484. Available at: http://dx.doi.org/10.1016/0013-4694(83)90135-9 [Accessed March 27, 2012].

Groppe, D.M., Urbach, T.P. & Kutas, M., 2011. Mass univariate analysis of event-related brain potentials/fields I: a critical tutorial review. *Psychophysiology*, 48(12), pp.1711–25. Available at: http://www.ncbi.nlm.nih.gov/pubmed/21895683.

Hu, X. et al., 2012. Increasing the number of irrelevant stimuli increases ability to detect countermeasures to the P300-based Complex Trial Protocol for concealed information detection. *Psychophysiology*, 49(1), pp.85–95. Available at: http://www.ncbi.nlm.nih.gov/pubmed/22091554 [Accessed August 19, 2014].

Kilner, J.M., 2013. Bias in a common EEG and MEG statistical analysis and how to avoid it. *Clinical neurophysiology : official journal of the International Federation of Clinical Neurophysiology*, 124(10), pp.2062–3. Available at: http://www.ncbi.nlm.nih.gov/pubmed/23639379 [Accessed November 15, 2013].

Labkovsky, E. & Rosenfeld, J.P., 2012. The P300-based, complex trial protocol for concealed information detection resists any number of sequential countermeasures against up to five irrelevant stimuli. *Applied Psychophysiology Biofeedback*, 37(1), pp.1–10.

Labkovsky, E. & Rosenfeld, J.P., 2012. The P300-based, complex trial protocol for concealed information detection resists any number of sequential countermeasures against up to five irrelevant stimuli. *Applied Psychophysiology and Biofeedback*, 37(1), pp.1–10. Available at: http://www.ncbi.nlm.nih.gov/pubmed/21965119.

Meixner, J.B. et al., 2013. P900: a putative novel ERP component that indexes countermeasure use in the P300-based concealed information test. *Applied psychophysiology and biofeedback*, 38(2), pp.121–32. Available at: http://www.ncbi.nlm.nih.gov/pubmed/23584620 [Accessed August 19, 2014].

Meixner, J.B. & Rosenfeld, J.P., 2010a. A mock terrorism application of the P300-based concealed information test. *Psychophysiology*, 48, pp.149–154. Available at: http://www.ncbi.nlm.nih.gov/pubmed/20579312 [Accessed December 8, 2012].

Meixner, J.B. & Rosenfeld, J.P., 2010b. Countermeasure mechanisms in a P300-based concealed information test. *Psychophysiology*, 47(1), pp.57–65. Available at: http://www.ncbi.nlm.nih.gov/pubmed/19761523 [Accessed March 27, 2012].

Rosenfeld, J.P., Ward, A., Frigo, V., et al., 2015. Evidence suggesting superiority of visual (verbal) vs. auditory test presentation modality in the P300-based, Complex Trial Protocol for concealed autobiographical memory detection. *International Journal of Psychophysiology*, 96(1), pp.16–22.

Rosenfeld, J.P. et al., 2004. Simple, effective countermeasures to P300-based tests of detection of concealed information. *Psychophysiology*, 41(2), pp.205–219.

Rosenfeld, J.P., Ward, A., Thai, M., et al., 2015. Superiority of pictorial versus verbal presentation and initial exposure in the p300-based, complex trial protocol for concealed memory detection. *Applied psychophysiology and biofeedback*, 40(2), pp.61–73. Available at: http://www.ncbi.nlm.nih.gov/pubmed/25772317 [Accessed May 20, 2015].

Soskins, M., Rosenfeld, J.P. & Niendam, T., 2001. Peak-to-peak measurement of P300 recorded at 0.3 Hz high pass filter settings in intraindividual diagnosis: complex vs. simple paradigms. *International journal of psychophysiology: official journal of the International Organization of Psychophysiology*, 40(2), pp.173–80. Available at: http://www.ncbi.nlm.nih.gov/pubmed/11165356.

Wasserman, S. & Bockenholt, U., 1989. Bootstrapping: Applications to Psychophysiology. *Psychophysiology*, 26(2), pp.208–221. Available at: http://doi.wiley.com/10.1111/j.1469-8986.1989.tb03159.x [Accessed March 27, 2012].

Yeung, N. et al., 2004. Detection of synchronized oscillations in the electroencephalogram: An evaluation of methods. *Psychophysiology*, 41(6), pp.822–832.

Yeung, N. et al., 2007. Theta phase resetting and the error-related negativity. *Psychophysiology*, 44(1), pp.39–49. Available at: http://www.ncbi.nlm.nih.gov/pubmed/17241139.

Figure 1. Measuring P3 size across participants using a fixed time window.

When a fixed time window technique is used, each participant's P3 is measured within the same time window. However, because of the expected variability across the participants, this procedure might yield false-negative cases. The Figure above, with positive plotted down, depicts an example of two individual ERPs. An a priori fixed window is placed from 400 to 600 ms. In such a situation, the P3 size of participant 1 will be measured appropriately with a large positive value because the P3 shape is almost always positive within the fixed time window. By contrast, although participant 2 has elicited a high positive P3 peak, the measure of the P3 size might result in a small positive value or even a zero or negative value due to the negative deflection that follows the positivity of the P3. In other words, within the fixed window, the classic negativity that follows the P3 positivity fell in the fixed window and cancelled that positivity. Such inter individual difference could arise for many reasons, e.g., participant alertness or variations in cortical folding.

Figure 2. Pz grand averages for Names experiment.

The grand averages at Pz for all of the conditions in the Names deception detector. Positive is

plotted downwards.

Figure 3. Pz grand averages ERPs for Birthdays experiment.

The grand averages at Pz for all of the conditions in the Birthdays deception detector. Positive is

plotted downwards.

Figure 4. P-value distributions obtained from the intrinsic validity test of the WT.

The upper and lower plots show the distributions of p-values that were generated from the first

and second intrinsic validity test. Each distribution consists of 1000 p-values. As expected, both

distributions are uniform.

Figure 5. Selection of Pz ERPs form Names Experiment.

Selections of individual ERPs at Pz for participants 1, 2, 8, and 14 in the Names experiment.

Positive is down, and the vertical dashed lines mark the region in which we search for the P3.

Figure 6. Grand average p-values at different level of SNR

The figure shows the grand average p-value as a function of the grand average SNR. At each

SNR level, the grand average p-value was obtained by taking the mean of all p-values presented

in table A.1 . For example, the grand average p-value at a certain SNR level was calculated by

taking the average of all 15 (across all participants) p-values that were obtained at that level. The

Grand average SNR was calculated in the same way by taking the average of all estimated SNRs.

As shown in the figure, the p-values of both methods increase as the amount of noise increases

(the SNR decreases). As the SNR decreased, the amount p-values of the WT were smaller than

the corresponding p-values of the Peak-to-Peak increased. Error bars indicate the 95%

confidence intervals for the means as estimated by bootstrapping over p-values at each SNR.

Figure 7. Selection of ROC curves.

The ROC curves of the WT (red) and Peak-to-Peak (green) methods, using simulated data for the

ERPs of participants 1, 2, and 14. Each column in the figure shows the performance of each

classifier for each participant at different noise levels (K), K= 13, 31, and 49. The ROC curve

depicts the relationship between the false-positive rate (FPR) (X axis) and the true-positive Rate

(TPR) (Y axis). Note the K is used as a scalar for the amplitude of noise.

Figure 8. Selection of the WT and Peak-to-Peak null hypothesis distributions.

Randomised null hypothesis distributions for the WT and Peak-to-Peak for two participants (1

and 8). The true observed value and Type I error region are marked in black. Participant 1, as

shown in Figure 5, has a noisy Probe ERP with no evidence of P3 presence. Thus, in both

methods, the true observed values were small and generated large p-values. By contrast, in both

methods, participant 8, who elicited a strong P3 component, had a large true observed value,

which fell outside the distribution, producing a significant p-value of <.001.

Figure 9. Selection of Pz ERPs from the Birthdays experiment.

ERPs at Pz for participants 6 and 7 from the Birthdays experiment. Positive is down, and the

vertical dashed lines mark the region in which we search for the P3.

Table 1. Grand average of p-values at different levels of SNR.

K	SNR	WT			Peak-to-Peak		
		Grand average P value	95% Ci		Grand average p value	95% Ci	
1	.1360	<.0001	.0000	.0000	<.0001	.0000	.0000
7	.0404	.0006	.0004	.0011	.0006	.0003	.0012
13	.0163	.0099	.0078	.0128	.0182	.0151	.0226
19	.0086	.0277	.0238	.0329	.0503	.0442	.0581
25	.0052	.0641	.0576	.0712	.1058	.0968	.1158
31	.0035	.1010	.0930	.1099	.1468	.1359	.1591
37	.0025	.1301	.1209	.1400	.1827	.1704	.1954
43	.0018	.1620	.1513	.1727	.2107	.1978	.2239
49	.0014	.1925	.1817	.2044	.2531	.2398	.2671

Table 1 presents the grand average p-values and SNRs for each method across all participants. For each K (K was used as a scalar for the amplitude of noise), the grand average values were obtained by taking the average of all p-values and SNRs that are presented in Table A.1 in Appendix A. The confidence intervals indicate the 95% confidence intervals for the means as estimated by bootstrapping over p-values (see section 3.1.1 for more details about estimating the 95% confidence interval). As *K* increases, the SNR declines, and therefore the p-value increases. The two methods performed almost equally at a high SNR. However, at low SNRs, the p-values of the WT were significantly smaller than the corresponding values for Peak-to-Peak.

Table 2. Grand average of AUC versus SNR.

K	SNR	Grand average of AUCs		Paired t-test	
		WT	Peak-to-Peak	t value	P value
1	.1360	1.000	1.000	NaN	NaN
7	.0404	.999	.999	-.5405	.5973
13	.0163	.988	.982	.9520	.3572
19	.0086	.969	.950	1.6401	.1233
25	.0052	.929	.895	2.0528	.0593
31	.0035	.889	.854	2.3244	.0357
37	.0025	.857	.818	2.7291	.0163
43	.0018	.822	.790	2.9170	.0113
49	.0014	.788	.746	3.4875	.0036

Table 2 presents the grand average AUCs and SNRs for each method across all participants in in the Names experiment. For each noise level (K), the grand average values were obtained by taking the average of all AUCs and SNRs that are presented in Table A.2 in Appendix A. It also shows results of paired t-tests (t and p values) that were applied to AUCs at each SNR level. Section 3.1.2 describes how the t-test was applied at each SNR level. As can be seen, the average performance of both methods decreased as SNR decreased. However, as the SNR dropped, the difference in average performance of the WT compared to Peak-to-Peak increased. Results of a paired t-test at each SNR level statistically confirmed this pattern.

Table 3. Per-individual analyses for the Names experiment.

Participant	WT			Peak-to-Peak		
	Probe	Irrelevant1	P value	Probe	Irrelevant1	P value
1	.4855	.4374	.342	4.2433	4.2342	.286
2	.5705	-.0925	.011	4.2141	3.8075	.080
3	.9828	.1141	<.001	11.0444	3.0311	<.001
4	.8973	-.1847	<.001	7.8579	4.2099	<.001
5	.9184	-.0159	<.001	13.6103	2.8520	<.001
6	.9921	.4822	<.001	26.224	2.8163	<.001
7	.9466	-.2069	<.001	11.629	0.9923	<.001
8	1.0784	-.4384	<.001	20.406	2.2978	<.001
9	1.0085	.3274	<.001	10.643	3.1951	<.001
10	.6516	-.1132	.001	9.957	5.3638	.001
11	.4589	-.2025	.019	6.0047	2.2418	.023
12	.9898	.3093	<.001	15.6686	2.3618	<.001
13	.6292	-.4560	<.001	11.5548	2.7867	<.001
14	.8114	.1305	.012	4.4183	2.5450	.239
15	1.0423	.3863	<.001	9.9656	2.3088	<.001

This table presents true observed values and p-values obtained from the WT and Peak-to-Peak methods for each participant in the Names experiment. The WT values of the Probe and Irrelevant1 conditions were obtained by applying the Fake as a template to each condition. The Peak-to-Peak method was applied to each condition (Probe and Irrelevant1) to obtain their Peak-to-Peak sizes. At an alpha level of .05, 14/15 of the participants were detected as guilty with the WT, whereas 12/15 of the participants were found to be guilty using Peak-to-Peak. Note that he smallest p-value we can obtain with a 1000 resamplings is 0.001. However, the exact p-values for many of the participants are likely to be significantly smaller than <0.001.

Table 4. Per-individual p-values for the Birthdays experiment.

Participant	WT			Peak-to-Peak		
	Probe	Irrelevant	P values	Probe	Irrelevant	P values
1	.9553	.6907	.0760	7.4228	4.1333	.080
2	.3772	.7839	.4780	2.6645	3.8197	.419
3	.6277	.0031	.0480	6.1961	.9474	.119
4	-.1725	.2530	.9540	3.5902	5.9752	.478
5	.5486	-.1014	.0540	4.2658	4.6447	.125
6	.6776	-.2415	.0140	4.9793	3.3458	.040
7	-.0933	-.6693	.0200	4.0758	3.1902	.086
8	.2194	-.1179	.2290	2.5920	2.7268	.536
9	.3813	.0215	.1850	2.1699	1.8156	.312
10	.3108	.5748	.8700	3.3671	4.2875	.988
11	1.0487	.9481	.5090	5.5972	3.3216	.414
12	.4629	-.6000	.0150	3.4383	.1436	.003

Table 4 shows true observed values and p-values arising from the WT and Peak-to-Peak methods

for each participant in the Birthdays experiment. At an alpha level of .05, 4/12 of the participants

were detected as guilty with the WT, whereas 2/12 of the participants were found guilty using

Peak-to-Peak.

Table 5. False-alarm rate of the WT and Peak-to-Peak methods for the Names experiment.

	P1		P2		P3		P4		P5		P6	
Participant	WT	PP	WT	PP	WT	PP	WT	PP	WT	PP	WT	PP
1	.969	.718	.324	.256	.196	.460	.466	.814	.740	.430	.963	.759
2	.265	.571	.536	.181	.114	**.012***	.056	**.013***	.401	.491	.233	.150
3	.203	.817	.789	.074	.810	.679	.783	.829	.407	.577	.115	.102
4	.773	.778	.639	.393	.880	.994	.995	.987	.240	.276	.199	.857
5	.902	.659	.545	.312	.579	.955	.776	.873	.186	.130	.272	.844
6	.137	.996	.948	.973	.435	.366	**.015***	**.004***	.627	.984	.512	.184
7	.567	.172	.211	.341	.343	.519	.503	.360	.212	**.010***	.422	.674
8	.489	.441	.535	.351	.187	.177	.262	.585	.851	.915	.704	.477

Table 5 presents the outcomes of the false-alarm test for the innocent group in the Names experiment, using both methods. Columns (**P1-P6**) refer to the six permutations that arose from changing the role between the three identical conditions of Probe, Irrelevant1, and Irrelevant2. At an alpha level of .05, only one false alarm was obtained by the WT, compared with four by the Peak-to-Peak (PP) method. The false-positive alarms are indicated with asterisks.

Table 6. False-alarm rate for Birthdays experiment using the WT and Peak-to-Peak methods.

Participant	WT	Peak-to-Peak
1	.227	.316
2	**.001***	.379
3	.525	.124
4	.877	.138
5	.755	.731
6	.991	**.023***
7	.412	.921
8	.821	.277
9	.082	**.020***
10	.440	.559

Table 6 lists the results of the false-alarm test using the WT and Peak-to-Peak methods, which were applied to the innocent group in the Birthdays experiment. At an alpha level of .05, one false alarm was obtained by the WT, compared with two by Peak-to-Peak (PP). The false-positive alarms are indicated with asterisks.