

1 **Quadriceps and hamstrings coactivation in exercises used in prevention and**  
2 **rehabilitation of hamstring strain injury in young soccer players**

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## 25 **Abstract**

26           This study aimed to study the co-activation of hamstring-quadriceps muscles  
27 during submaximal strength exercises without the use of maximum voluntary isometric  
28 contraction testing and compare (i) the inter-limb differences in muscle activation, (ii) the  
29 intra-muscular group activation pattern, and (iii) the activation during different phases of  
30 the exercise. Muscle activation was recorded by surface electromyography of 19 elite  
31 male youth players. Participants performed five repetitions of the Bulgarian squat, lunge  
32 and the squat with an external load of 10 kg. Electrical activity was recorded for the rectus  
33 femoris, vastus medialis, vastus lateralis, biceps femoris and semitendinosus. No  
34 significant inter-limb differences were found ( $F_{1, 13}=619$ ;  $p=0.82$ ; partial  $\eta^2=0.045$ ).  
35 Significant differences were found in the muscle activation between different muscles  
36 within the muscle group (quadriceps and hamstrings) for each of the exercises : Bulgarian  
37 squat ( $F_{1,18}=331$ ;  $p<0.001$ ; partial  $\eta^2=0.80$ ), lunge ( $F_{4,72}=114.5$ ;  $p<0.001$ ; partial  $\eta^2=0.86$ )  
38 and squat ( $F_{1,16}=247.31$ ;  $p<0.001$ ; partial  $\eta^2=0.93$ ).Differences were found between the  
39 concentric, isometric and eccentric phases of each of the exercises ( $F_{2, 26}=52.27$ ;  $p=0.02$ ;  
40 partial  $\eta^2=0.80$ ). The existence of an activation pattern of each of the muscles in the three  
41 proposed exercises could be used for muscle assessment and as a tool for injury recovery.

## 42 **Introduction**

43           Performance in soccer depends on psychological, physiological and  
44 biomechanical factors (1, 2). The study of these factors not only helps improve  
45 performance, but also works towards injury prevention. Performance and injury  
46 prevention are not isolated fields, and the presence of an injury can affect on-field  
47 performance. Measurement of the muscular capacity of players is an important factor in  
48 the evaluation and prediction of the functional capacity of the player (3).

49 Muscular capacity has been traditionally measured using isokinetic machines (4,  
50 5). However, recently many studies have used electromyography (EMG) (6-8). One of  
51 the major aims of such studies has been to to determine asymmetry in soccer players,  
52 which can affect both performance (9, 10) and injury (11). Such comparative studies have  
53 been carried out in youth soccer players as well (12-15) finding that there may be a  
54 neuromuscular pattern and that force work could be related to a reduction in the injury  
55 rate in football players.

56 Asymmetry in soccer players could be offset with proper exercise prescription,  
57 which facilitates improvements in musculoskeletal function by addressing the specific  
58 needs of the subject as an integral part of any rehabilitative, preventive, or maintenance  
59 program (16). Functional weight-bearing exercises have received a significant amount of  
60 attention as the preferred mode of exercise for lower extremity strengthening (17). In  
61 studies with EMG, basic strength exercises (forward lunge, bugarian squat, lateral step-  
62 ups, squat) are frequently used so that they are easily replicable. These are simple  
63 exercises used to strengthen the quadriceps and hamstrings, and their study could provide  
64 information about the activation of different muscles of the quadriceps and hamstrings  
65 and to differentiate the activation differences in the exercise phases (Caterisano, Moss  
66 (18)). Considering the muscle group that they target, these exercises can be crucial for  
67 soccer players given that recent research has shown that monitoring the electrical activity  
68 of individual muscles could help in the injury rehabilitation and prevention process (18,  
69 19).

70 Specifically, in the case of soccer players, quadriceps and hamstrings account for  
71 19% and 16% of all injuries respectively (20). The case of hamstring strain injury is of  
72 concern given that there is an increase of 4% every year in the male teams (21). Muscular  
73 imbalances have been cited as an important risk factor for hamstring strain injury (22,

74 23). This has been traditionally assessed by evaluating muscular imbalances through  
75 isokinetic machines (24-26), although recent studies have begun using surface  
76 electromyography (EMG) to evaluate muscular imbalances in different strength  
77 exercises. EMG has been used to evaluate the nordic hamstring curl (27, 28), the leg curl  
78 (29, 30), bilateral open chain (31) and unilateral closed chain exercises like forward lunge,  
79 bulgarian squat and unilateral bridge (29, 32). Research has shown, these exercises  
80 targeting the quadriceps and hamstrings have proved beneficial not only for these muscle  
81 groups, but also in rehabilitation and prevention of anterior cruciate ligament (33)  
82 patellofemoral pain syndrome (34) or groin injuries (35). However, these researches have  
83 used adult/amateur athletes, but none have specifically focused on young soccer players,  
84 which have traditionally used isokinetic machines(12).

85         Studies using EMG have required the normalization of EMG signal (36). Many  
86 normalization techniques are available being the maximal voluntary isometric contraction  
87 (MVIC) the most used standard methods (36). However some controversy exists about  
88 its reliability (37-39) leading researchers to study the agonistic-antagonist coactivation  
89 of muscles as an alternative by normalizing the electrical activity of one muscle in relation  
90 with the other (18). This can be useful because it gives information on how muscles work  
91 synergistically and permit a normalization that is not demanding for the athlete,  
92 facilitating its use at any time of the season.

93         Hence, this study aimed to study the hamstring-quadriceps muscle co-activation  
94 during submaximal strength exercises (Bulgarian squat, forward lunge and squat) without  
95 the use of voluntary maximum isometric contraction testing and compare (i) inter-limb  
96 differences in muscle activation, (ii) intra-muscular group activation pattern, and (iii)  
97 activation during different phases of the exercise. The following hypotheses were raised:  
98 1) Inter-limb differences would be noted for the different exercises.

- 99 2) Muscle activation is different according to the phases of movement.  
100 3) There is a different pattern of intra-hamstrings and intra-quadriceps muscle group co-  
101 activation for each exercise.

## 102 **Material and methods**

### 103 **Participants**

104 Nineteen soccer players participated in the study (Table 1), all of them men,  
105 belonging to the youth soccer team of a professional Spanish team.

106

107 **Table 1. Basic demographic and descriptive data of the included sample (Mean  $\pm$ SD)**

Total players	19
Sex	Male
Age (years)	19.18 $\pm$ 0.48
Height (cm)	179.68 $\pm$ 5.32
Weight (kg)	70.98 $\pm$ 5.87
Training days per week	5

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110 The players who were included in the study did not sustain leg injury in the last  
111 six months prior to the day of testing. All participants gave their written informed consent  
112 to participate in the study. The study followed the guidelines of the Declaration of  
113 Helsinki and has been approved by the ethics committee of the **\*\*blinded for peer**  
114 **review\*\***.

### 115 **Study Design**

116 A descriptive study was carried out in a sports biomechanics laboratory, where  
117 participants were required to perform the Bulgarian Squat, Squat and Lunge in a single  
118 session.

119 1. Lunge. The initial starting position was with one forward leg, straight trunk and  
120 arms to the side of the body. The lunge exercise consisted in advancing one leg in front  
121 of the other, and then flexing both knees without touching the ground while the trunk was  
122 straight. The forward knee reached a flexion angle of 90°. It was ensured that the knee of  
123 the advanced leg did not surpass the toe of the foot (6).

124 2. Bulgarian squat. The initial starting position consisted in advancing one leg  
125 while the back leg was placed on an elevated surface of 50cm. The players then had to  
126 flex the forward knee while keeping the trunk straight (40).

127 3. Squat. The participant's feet were separated such that they were apart at  
128 shoulders' length, and the players had to lower themselves until they reached a 90° knee  
129 flexion angle while the trunk was straight (41, 42).

## 130 **Procedure**

131 The players first warmed up under the guidance of a strength and conditioning  
132 coach of the club. It consisted of seven minutes of running followed by joint mobility and  
133 core activation exercises for an additional three minutes. Finally the players familiarized  
134 themselves with the three exercises at the end of the warm-up (43).

135 After warming-up, EMG sensors were placed on the rectus femoris (RF), vastus  
136 medialis (VM), vastus lateralis (VL), biceps femoris (BF) and semitendinosus (ST) with  
137 the players' skin being shaved and cleaned with alcohol prior to sensor placement. The  
138 Seniam protocol was used for sensor placement (44) and recommendations of Ramírez  
139 and Garzón (45) were followed, with the orientation for the rectus femoris being 0°, 70°

140 for the vastus medialis and  $-20^\circ$  for the vastus lateralis, taking as reference a line drawn  
141 from the origin and to the insertion.

142 EMG data was recorded using Trigno™ Wireless System (Delsys, Inc.  
143 Massachusetts, U.S.A). This system allowed players to perform the exercises with  
144 complete freedom of movement and was composed of a receiver device, a data registering  
145 software, and a series of surface wireless electrodes placed in each of the muscles, plus  
146 one placed on the back to be used as an accelerometer to discern the different phases of  
147 the exercises. The sensors measured 0.037m x 0.026m x 0.015m, with a distance between  
148 electrodes of 0.01m and weighed 0.014 kg and could record both the EMG signal and  
149 triaxial accelerometry, with an autonomy of 8 hours and a charging time of 2 hours. The  
150 input range was 0.011V, 16-bit resolution, bandwidth between 20-450Hz. Data was  
151 captured at 1500Hz. The signal gain of the electrodes was  $909V/V \pm 5\%$ . The EMGWorks  
152 Acquisition software (Delsys, Inc. Massachusetts, U.S.A) was used to visualize and  
153 record the data.

154 Once the sensors were placed, the players performed the three exercises. Each  
155 exercise had three well-differentiated phases, the first phase of descent, the second one  
156 isometric phase and finally the phase of ascent. Each exercise was repeated five times  
157 (for each leg) and the execution rhythm was externally marked by a stopwatch: two  
158 seconds of descent, two seconds of isometric and two seconds of ascent. The external  
159 load was 10kg (two 5 kg dumbbells). Between each exercise there was a complete rest of  
160 2.5 minutes.

## 161 **Data Processing**

162 The EMGWORKS® software (Delsys, Inc., Massachusetts; U.S.A.) was used to  
163 process the data. The first step of the data treatment was the filtering of the signal using  
164 a 2<sup>nd</sup> order, bandpass Butterworth filter (36) with an attenuation of 40dB and a frequency

165 cut between 20-30 Hz (46). A Root Mean Square (RMS) (47) with a window width of  
166 0.05s and a window overlap of 0.025s was later applied to the filtered signal and the signal  
167 offset was removed.

168 To identify the phases of the exercises, the accelerometer signal from a sensor  
169 placed on the back of the players in the longitudinal axis was used (48). The EMG and  
170 accelerometer signals were superimposed, and the mean RMS of the 5 repetitions was  
171 used for each of 3 exercises for analysis.

## 172 **Statistical Analysis**

173 Four independent variables were defined: preferred limb, muscle group, phases of  
174 the exercise, and exercise and two dependent variables: intragroup muscular ratio and  
175 electrical activation (V) were compared. The intragroup muscular ratio expresses the  
176 activation of each muscle with respect to the total surface muscular activity of each  
177 muscle. For example, the intragroup muscular activation for the RF = Muscular activity  
178 of RF/ (Muscular activities of RF+VL+VM).

179 The statistical analyses were carried out with SPSS 23.0 (Spss Inchicago, IL,  
180 USA). An analysis of variance was carried out study the main effects of the 4 independent  
181 variables (leg (2) x muscle (5) x phases (3) x exercise (3)). Subsequent post-hoc  
182 comparisons were done with Bonferroni corrections. The significance level was set at  
183 0.05 and effect sizes were determined using partial eta squared values (threshold values:  
184 small= 0.2, medium = 0.6 and large = 0.8, (49)).

## 185 **Results**

### 186 **Inter-limb effect**

187 Both the main effect of the leg factor ( $F_{1, 13}=619$ ;  $p=0.82$ ; partial  $\eta^2=0.045$ ) and  
188 the differences in intra-muscular group activation between dominant and non-dominant



189 leg in each phase of the movement of each muscle in the exercises analysed were not  
 190 significant. Therefore, for the successive comparisons the mean activation between the  
 191 two legs was used as the dependent variable.

## 192 **Intra-muscular group activation pattern**

193 Significant differences were found in the muscle activation between different  
 194 muscles within the muscle group (quadriceps and hamstrings) for each of the exercises  
 195 (Table 2): Bulgarian squat ( $F_{1,18}=331$ ;  $p<0.001$ ; partial  $\eta^2=0.80$ ), lunge ( $F_{4,72}=114.5$ ;  
 196  $p<0.001$ ; partial  $\eta^2=0.86$ ) and squat ( $F_{1,16}=247.31$ ;  $p<0.001$ ; partial  $\eta^2=0.93$ ). In the  
 197 quadriceps, the post-hoc comparisons showed that the vastus medialis showed the highest  
 198 activity, followed by the vastus lateralis and then the rectus femoris for all exercises  
 199 ( $p<0.001$ ). In the hamstring muscles, the semitendinosus had greater activation than the  
 200 biceps femoris ( $p<0.001$ ) for the Bulgarian squat and lunge exercises. However, in the  
 201 squat no significant differences were obtained between the two muscles ( $p=0.175$ ).  
 202 Comparisons between each muscle in the different exercises showed significant  
 203 differences in the activation pattern ( $F_{8,128}=2$ ;  $p=0.03$ ; partial  $\eta^2=0.93$ ) (Fig 1).

204

205

206 **Table 2. Intra-muscular group activation (Mean± ST) in percentage**

Muscle	Bulgarian Squat (N=19)			Lunge (N=19)			Squat (N=19)		
		CI 95%			CI 95%			CI 95%	
<b>RF(RF/RF+VM+VL)</b>	14.83±4.50 %**	12.66	17.00	16.56±5.70 %**	13.81	19.31	18.69±6.54%**	15.54	21.84
<b>VM(VM/RF+VM+VL)</b>	56.35±6.71 %**	53.12	59.58	58.85±8.02 %**	54.98	62.72	53.41±8.03%**	49.54	57.28
<b>VL(VL/RF+VM+VL)</b>	29.17±5.19 %**	26.67	31.67	25.71±6.10%**	22.77	28.65	28.67±6.90%**	25.34	32.00
<b>BF(BF/BF+ST)</b>	47.50±10 %**	42.68	52.32	44.35±6.93%**	41.01	47.69	49.37±9.50%	44.79	53.95
<b>ST(ST/BF+ST)</b>	51.43±11.22 %**	46.02	56.84	55.65±6.94%**	52.31	58.99	50.63±9.50%	46.05	55.21

207 RF: Rectus Femoris, VM: Vastus Medialis, VL: Vastus Lateralis, BF: Biceps femoris, ST: Semitendinosus

208 \*\*  $p < 0.001$ ,

209 \*  $p < 0.05$ ,

210

211 **Fig 1. Intra-muscular group activation (mean± standard deviation) in percentage**

212 **Electrical activation during the movement phases**

213 Significant differences were found in the electrical activity (RMS) between the  
214 phases and in the three exercises ( $F_{2,26}=52.27$ ;  $p=0.02$ ; partial  $\eta^2=0.80$ ).

215 In the Bulgarian squat exercise (Fig 2), significant differences were found between  
216 phases ( $F_{10,58}=12.18$ ;  $p<0.001$ ; partial  $\eta^2=0.68$ ). In all quadriceps muscles, the isometric  
217 phase was the one that registered the greatest electrical activity ( $p=0.01$ ). The ascent  
218 phase had greater activation than the descent phase ( $p=0.03$ ). In the hamstrings, the ascent  
219 phase was greater than the other two ( $p=0.02$ ) in both biceps femoris and semitendinosus.

220

221 **Fig 2. Mean activation ( $V \times 10^{-5}$ ) of all the muscles in each phase in Bulgarian squat**

222

223 In the lunge exercise (Fig 3), significant differences were found between the 3  
224 phases ( $F_{10,54}=16.85$ ;  $p<0.001$ ; partial  $\eta^2=0.76$ ). In the rectus femoris, vastus medialis and  
225 vastus lateralis, the isometric phase had greater activation than the descent and ascent  
226 phase ( $p<0.001$ ), the ascent phase had greater activation than the descent phase ( $p<0.001$ ).

227 In the biceps femoris, the ascent phase had greater activation than the isometric phase and  
228 the descent phase ( $p<0.001$ ); the descent phase had greater activation than the isometric  
229 phase ( $p<0.001$ ). In the semitendinosus, descent and ascent phase had similar activation  
230 ( $p=0.07$ ).

231 **Fig 3. Mean activation ( $V \times 10^{-5}$ ) of all the muscles in each phase in lunge**

232

233 In the squat exercise (Fig 4) there were significant differences between the phases  
234 ( $F_{10,46}=8.04$ ;  $p<0.001$ ; partial  $\eta^2=0.64$ ). In the rectus femoris, the isometric phase had

235 greater activation than the descent and ascent phase ( $p=0.04$ ), there were no significant  
236 differences between ascent phase and descent phase ( $p=0.09$ ). In the vastus medialis the  
237 isometric phase had greater activation than the descent phase ( $p<0.001$ ), there were no  
238 significant differences between the isometric phase and the ascent phase ( $p=0.25$ ), the  
239 ascent phase had greater activation than the descent phase ( $p=0.04$ ). In the vastus lateralis,  
240 the isometric phase had greater activation than the descent phase ( $p= 0.02$ ), the ascent  
241 phase had greater activation than the descent phase ( $p=0.03$ ), there was no difference  
242 between the isometric and ascent phase ( $p=0.87$ ). In biceps femoris and in the  
243 semitendinosus, the ascent phase had the highest activation ( $p<0.001$ ).

244

245 **Fig 4. Mean activation ( $V \times 10^{-5}$ ) of all the muscles in each phase in squat**

246

## 247 **Discussion and implications**

248 In this paper, the surface muscular activation of two important muscular groups,  
249 hamstrings and quadriceps, was measured in strength exercises in elite youth soccer  
250 players. These exercises, namely the Bulgarian squat, the lunge and the squat, are  
251 frequently used and easily replicable. No significant inter-limb differences were  
252 observed, rejecting hypothesis 1. Muscle activation patterns showed differences across  
253 the intra-muscular group to which they belonged, confirming hypothesis 2. Also, muscle  
254 activation differed across the concentric, isometric and eccentric phases of each exercise,  
255 confirming hypothesis 3. This is one of the first investigations to study the muscle  
256 activation pattern in elite youth soccer players and has important applications where  
257 differences in the muscle activation pattern could indicate muscular deficiencies leading  
258 to other muscles assuming part of that deficiency.

### 259 **Inter-limb effect**

260           The results show that no significant differences were found between dominant and  
261 non-dominant leg in electrical activity, other previous studies obtained similar results  
262 with professional or semi-professional samples (50-52). Although soccer is an  
263 asymmetric sport, the modern demands of the sport lay an emphasis on training both limbs  
264 equally. Another important factor to consider is that the participants in this study were  
265 elite youth players, playing in national and European competition, and studies have  
266 suggested that inter-limb differences in strength decrease with an increase in level of play  
267 (53). Inter-limb differences could be a precursor to injuries (54) hence the monitoring of  
268 inter limb differences could be important in injury prevention programs.

### 269 **Intra-muscular group activation**

270           In all exercises, the muscular activation patterns of the quadriceps muscles were  
271 repeated, with the vastus medialis being predominant, followed by the vastus lateralis and  
272 finally the rectus femoris (Fig 1). These results were similar to those obtained with  
273 amateur athletes previously for the lunge (55) and squat exercises (18, 56). The similar  
274 pattern of activation of quadriceps and hamstrings could indicate a synergy of work in the  
275 proposed exercises (57). The results showed that there is a very similar activation pattern  
276 in the three exercises and in all the muscles (Fig 1), this pattern can be used for the  
277 rehabilitation process of an injury or to find deficiencies in the coactivation inside each  
278 muscle. This can be applied in the case of the patellofemoral pain syndrome, where vastus  
279 medialis activation is the primary goal in the early stages of recovery (58).

280

281           In the hamstrings, the greater intra-muscular activation (Fig 1) of the  
282 semitendinosus muscle compared to that of the biceps femoris account for its  
283 predominance (59, 60). A balance in the synergy of the hamstring muscles is important  
284 in the reduction of risk of a potential injury (60). This synergy helps to reduce the tension

285 on the biceps femoris (19, 61), which plays a fundamental role in the hamstring injury  
286 since biceps femoris is affected in 80% of all hamstring lesions (62). A low hamstring to  
287 quadriceps ratio is believed to be a risk factor for injuries (63) and many rehabilitation  
288 and prevention programs focus on strengthening the hamstrings. The heterogeneity of  
289 activation pattern of different exercises must be taken into consideration when developing  
290 hamstring strength (30), and these exercises help in the coactivation of the hamstring and  
291 quadriceps muscle groups.

## 292 **Activation during the movement phases**

293 Differences were found between the different phases of the 3 exercises (Fig 2-4),  
294 for quadriceps muscles, the greatest activation was recorded in the isometric phase, while  
295 in the hamstrings the greatest activation was in the ascent phase, or knee extension phase.

296 In the quadriceps, in all the muscles and exercises (Fig 2-4) greater activation was  
297 found in the ascent phase (concentric) than in the descent phase (eccentric), coinciding  
298 with previous studies (64-66) . In the concentric phase, there is a greater activation  
299 generated as there is a greater recruitment of fibres (67); while in the eccentric phase, a  
300 greater proportion of rapid contraction motor units were active at the expense of less  
301 recruitment of other motor units for load reduction (68). This finding illustrates the  
302 contribution of the hamstrings to effective force production in the concentric phase of the  
303 squat. There are two major theories to justify less activation in the eccentric phase than  
304 in the concentric phase. It is believed that the lower amplitude of EMG during eccentric  
305 phases may be due to the greater predominance of muscle-tendon strength produced by  
306 elongation in the eccentric phase (69). Other authors, however, have proposed that  
307 differences in EMG amplitude may be due to different neuronal pathways for each  
308 activation (68).

309           The isometric phase showed that rectus femoris presented the least activation in  
310 the quadriceps in all exercises, giving predominance in the stabilization of movement to  
311 the vastus medialis and vastus lateralis (67).

312           For hamstrings muscles, there was greater activation in all phases in the Bulgarian  
313 squat (Fig 2) than in the normal squat (Fig 4), which may be due to a greater demand for  
314 co-activation of the posterior leg musculature to keep joints and the body stable (70).  
315 Wright, Delong (60) emphasized the importance of the posterior muscles in exercises  
316 such as the Bulgarian squat, where the knee joint was fixed, thereby increasing the  
317 activation of the hamstrings.

318           These results can help sports scientists and strength and conditioning coaches,  
319 especially those working with youth players, when they want to influence a greater  
320 muscle activation for hypertrophy or implement these exercises in processes of strength  
321 development and rehabilitation.

## 322 **Choice of exercises**

323           The proposed exercises have been considered suitable for muscle evaluation and  
324 rehabilitation (6, 71, 72) and have therefore been implemented in most soccer club  
325 training programmes by physical trainers. The in-depth study of such exercises with a  
326 specific high-performance sample may allow soccer clubs to implement specific  
327 protocols for the development of lower train strength in players. An ineffective recovery  
328 of the thigh injury could cause a relapse in the soccer (73), so it is vital to be able to  
329 correctly quantify the recovery process where EMG can be used as a reliable method.  
330 Hence, the monitoring of such exercises could be used by sports scientists and strength  
331 and conditioning coaches. Specific leg exercises can be graded by exercise intensity  
332 providing athletes and therapists to select appropriate exercises during different phases of  
333 prevention.

334

## 335 **Conclusion**

336           EMG activation patterns in different muscles differed across the muscle group to  
337 which they belonged. Comparing the different phases of the exercises, in the quadriceps  
338 the isometric phase had the greatest activation followed by the concentric and eccentric  
339 phases; while in the hamstrings the concentric phase was the one with the greatest  
340 activation. A monitoring of the 3 proposed exercises, using EMG, can be used to find  
341 activity deficits in the muscles or for assessing muscles activation during injury  
342 rehabilitation. This procedure could be used in the future as a tool for researching about  
343 the risk of hamstrings strain injury in soccer.

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347 study.

## 348 **References**

- 349 1. Philippaerts RM, Vaeyens R, Janssens M, Van Renterghem B, Matthys D,  
350 Craen R, et al. The relationship between peak height velocity and physical  
351 performance in youth soccer players. *Journal of Sports Sciences*.  
352 2006;24(3):221-30.
- 353 2. Di Salvo V, Baron R, Tschan H, Montero FC, Bachl N, Pigozzi F.  
354 Performance characteristics according to playing position in elite soccer.  
355 *International journal of sports medicine*. 2007;28(03):222-7.
- 356 3. Daneshjoo A, Rahnama N, Mokhtar AH, Yusof A. Effectiveness of injury  
357 prevention programs on developing quadriceps and hamstrings strength of young  
358 male professional soccer players. *Journal of human kinetics*. 2013;39(1):115-25.
- 359 4. Evangelidis PE, Pain MT, Folland J. Angle-specific hamstring-to-  
360 quadriceps ratio: a comparison of football players and recreationally active males.  
361 *J Sports Sci*. 2015;33(3):309-19.
- 362 5. Houweling TA, Head A, Hamzeh MA. Validity of isokinetic testing for  
363 previous hamstring injury detection in soccer players. *Isokinetics and Exercise  
364 Science*. 2009;17(4):213-20.

- 365 6. Begalle RL, DiStefano LJ, Blackburn T, Padua DA. Quadriceps and  
366 Hamstrings Coactivation During Common Therapeutic Exercises. *Journal of*  
367 *Athletic Training* (Allen Press). 2012;47(4):396-405.
- 368 7. Dedinsky R, Baker L, Imbus S, Bowman M, Murray L. EXERCISES THAT  
369 FACILITATE OPTIMAL HAMSTRING AND QUADRICEPS CO-ACTIVATION TO  
370 HELP DECREASE ACL INJURY RISK IN HEALTHY FEMALES: A  
371 SYSTEMATIC REVIEW OF THE LITERATURE. *International journal of sports*  
372 *physical therapy*. 2017;12(1):3.
- 373 8. Ebben W. Hamstring activation during lower body resistance training  
374 exercises. *International journal of sports physiology and performance*.  
375 2009;4(1):84-96.
- 376 9. Rouissi M, Chtara M, Owen A, Chaalali A, Chaouachi A, Gabbett T, et al.  
377 Effect of leg dominance on change of direction ability amongst young elite soccer  
378 players. *Journal of sports sciences*. 2016;34(6):542-8.
- 379 10. Cortis C, Tessitore A, Perroni F, Lupo C, Pesce C, Ammendolia A, et al.  
380 Interlimb coordination, strength, and power in soccer players across the lifespan.  
381 *The Journal of Strength & Conditioning Research*. 2009;23(9):2458-66.
- 382 11. Navandar A, Veiga S, Torres G, Chorro D, Navarro E. A previous  
383 hamstring injury affects kicking mechanics in soccer players. *The Journal of*  
384 *sports medicine and physical fitness*. 2018.
- 385 12. Iga J, George K, Lees A, Reilly T. Cross-sectional investigation of indices  
386 of isokinetic leg strength in youth soccer players and untrained individuals.  
387 *Scandinavian journal of medicine & science in sports*. 2009;19(5):714-9.
- 388 13. Daneshjoo A, Rahnema N, Mokhtar AH, Yusof A. Bilateral and unilateral  
389 asymmetries of isokinetic strength and flexibility in male young professional  
390 soccer players. *Journal of human kinetics*. 2013;36(1):45-53.
- 391 14. Thorlund JB, Aagaard P, Madsen K. Rapid muscle force capacity changes  
392 after soccer match play. *International journal of sports medicine*.  
393 2009;30(04):273-8.
- 394 15. Montini M, Felici F, Nicolo A, Sacchetti M, Bazzucchi I. Neuromuscular  
395 demand in a soccer match assessed by a continuous electromyographic  
396 recording. *The Journal of sports medicine and physical fitness*. 2017;57(4):345-  
397 52.
- 398 16. LaPrade RF, Surowiec RK, Sochanska AN, Hentkowski BS, Martin BM,  
399 Engebretsen L, et al. Epidemiology, identification, treatment and return to play of  
400 musculoskeletal-based ice hockey injuries. *Br J Sports Med*. 2014;48(1):4-10.
- 401 17. Farrokhi S, Pollard CD, Souza RB, Chen Y-J, Reischl S, Powers CM.  
402 Trunk position influences the kinematics, kinetics, and muscle activity of the lead  
403 lower extremity during the forward lunge exercise. *journal of orthopaedic & sports*  
404 *physical therapy*. 2008;38(7):403-9.
- 405 18. Caterisano A, Moss RE, Pellingier TK, Woodruff K, Lewis VC, Booth W, et  
406 al. The effect of back squat depth on the EMG activity of 4 superficial hip and  
407 thigh muscles. *The Journal of Strength & Conditioning Research*.  
408 2002;16(3):428-32.
- 409 19. McCurdy K, O'Kelley E, Kutz M, Langford G, Ernest J, Torres M.  
410 Comparison of lower extremity EMG between the 2-leg squat and modified  
411 single-leg squat in female athletes. *Journal of sport rehabilitation*. 2010;19(1):57-  
412 70.
- 413 20. Ekstrand J, Hagglund, Walden. Injury incidence and injury patterns in  
414 professional football: the UEFA injury study. *Br J Sports Med*. 2011;45(7):553-8.



- 415 21. Ekstrand J, Waldén M, Hägglund M. Hamstring injuries have increased by  
416 4% annually in men's professional football, since 2001: a 13-year longitudinal  
417 analysis of the UEFA Elite Club injury study. *British journal of sports medicine*.  
418 2016;50(12):731-7.
- 419 22. Croisier J-L. Factors associated with recurrent hamstring injuries. *Sports*  
420 *medicine*. 2004;34(10):681-95.
- 421 23. Fousekis K, Tsepis E, Poulmedis P, Athanasopoulos S, Vagenas G.  
422 Intrinsic risk factors of non-contact quadriceps and hamstring strains in soccer: a  
423 prospective study of 100 professional players. *British journal of sports medicine*.  
424 2011;45(9):709-14.
- 425 24. Aagaard P, Simonsen EB, Andersen JL, Magnusson SP, Bojsen-Moller F,  
426 Dyhre-Poulsen P. Antagonist muscle coactivation during isokinetic knee  
427 extension. *Scandinavian Journal of Medicine & Science in Sports*. 2000;10(2):58.
- 428 25. Ayala F, De Ste Croix M, Sainz De Baranda P, Santonja F. Acute effects  
429 of static and dynamic stretching on hamstring eccentric isokinetic strength and  
430 unilateral hamstring to quadriceps strength ratios. *Journal of Sports Sciences*.  
431 2013;31(8):831-9.
- 432 26. Beyer KS, Fukuda DH, Miramonti AM, Church DD, Tanigawa S, Stout JR,  
433 et al. Strength ratios are affected by years of experience in American collegiate  
434 rugby athletes: A preliminary study. *Isokinetics and Exercise Science*.  
435 2016;24(3):257-62.
- 436 27. Shield AJ, Bourne MN. Hamstring injury prevention practices in elite sport:  
437 Evidence for eccentric strength vs. Lumbo-pelvic training. *Sports Medicine*.  
438 2018:1-12.
- 439 28. Van der Horst N, Smits D-W, Petersen J, Goedhart EA, Backx FJ. The  
440 preventive effect of the Nordic hamstring exercise on hamstring injuries in  
441 amateur soccer players: a randomized controlled trial. *The American journal of*  
442 *sports medicine*. 2015;43(6):1316-23.
- 443 29. Brukner P. Hamstring injuries: prevention and treatment—an update.  
444 *British journal of sports medicine*. 2015;49(19):1241-4.
- 445 30. Bourne MN, Williams MD, Opar DA, Al Najjar A, Kerr GK, Shield AJ.  
446 Impact of exercise selection on hamstring muscle activation. *Br J Sports Med*.  
447 2017;51(13):1021-8.
- 448 31. Guex K, Millet GP. Conceptual framework for strengthening exercises to  
449 prevent hamstring strains. *Sports Medicine*. 2013;43(12):1207-15.
- 450 32. Tsaklis P, Malliaropoulos N, Mendiguchia J, Korakakis V, Tsapralis K,  
451 Pyne D, et al. Muscle and intensity based hamstring exercise classification in elite  
452 female track and field athletes: implications for exercise selection during  
453 rehabilitation. *Open access journal of sports medicine*. 2015;6:209.
- 454 33. Heckmann TP, Noyes FR, Barber-Westin S. Rehabilitation after ACL  
455 reconstruction. *ACL Injuries in the Female Athlete*: Springer; 2018. p. 505-35.
- 456 34. Irish SE, Millward AJ, Wride J, Haas BM, Shum GL. The effect of closed-  
457 kinetic chain exercises and open-kinetic chain exercise on the muscle activity of  
458 vastus medialis oblique and vastus lateralis. *The Journal of Strength &*  
459 *Conditioning Research*. 2010;24(5):1256-62.
- 460 35. Charlton PC, Drew MK, Mentiplay BF, Grimaldi A, Clark RA. Exercise  
461 interventions for the prevention and treatment of groin pain and injury in athletes:  
462 a critical and systematic review. *Sports Medicine*. 2017;47(10):2011-26.

- 463 36. Robertson DG, Dowling JJ. Design and responses of Butterworth and  
464 critically damped digital filters. *Journal of Electromyography and Kinesiology*.  
465 2003;13(6):569-73.
- 466 37. Marras WS, Davis KG. A non-MVC EMG normalization technique for the  
467 trunk musculature: Part 1. Method development. *Journal of Electromyography*  
468 *and Kinesiology*. 2001;11(1):1-9.
- 469 38. Suydam SM, Manal K, Buchanan TS. The advantages of normalizing  
470 electromyography to ballistic rather than isometric or isokinetic tasks. *Journal of*  
471 *applied biomechanics*. 2017;33(3):189-96.
- 472 39. Mirka GA. The quantification of EMG normalization error. *Ergonomics*.  
473 1991;34(3):343-52.
- 474 40. Andersen V, Fimland M, Brennsset Ø, Haslestad L, Lundteigen M,  
475 Skalleberg K, et al. Muscle activation and strength in squat and bulgarian squat  
476 on stable and unstable surface. *International journal of sports medicine*.  
477 2014;35(14):1196-202.
- 478 41. Chiu LZ, Burkhardt E. A teaching progression for squatting exercises.  
479 *Strength & Conditioning Journal*. 2011;33(2):46-54.
- 480 42. Comfort P, Kasim P. Optimizing squat technique. *Strength and*  
481 *Conditioning Journal*. 2007;29(6):10.
- 482 43. Van den Tillaar R, Lerberg E, Von Heimburg E. Comparison of three types  
483 of warm-up upon sprint ability in experienced soccer players. *Journal of Sport*  
484 *and Health Science*. 2016.
- 485 44. Hermens HJ, Freriks B, Disselhorst-Klug C, Rau G. Development of  
486 recommendations for SEMG sensors and sensor placement procedures. *Journal*  
487 *of Electromyography and Kinesiology*. 2000;10(5):361-74.
- 488 45. Ramírez A, Garzón DA. Análisis de sensibilidad por la colocación de los  
489 electrodos en la electromiografía de superficie (semg). *Revista Facultad de*  
490 *Ingeniería*. 2013(46):70-9.
- 491 46. De Luca CJ, Gilmore LD, Kuznetsov M, Roy SH. Filtering the surface EMG  
492 signal: Movement artifact and baseline noise contamination. *Journal of*  
493 *biomechanics*. 2010;43(8):1573-9.
- 494 47. Fukuda TY, Echeimberg JO, Pompeu JE, Lucareli PRG, Garbelotti S,  
495 Gimenes RO, et al. Root mean square value of the electromyographic signal in  
496 the isometric torque of the quadriceps, hamstrings and brachial biceps muscles  
497 in female subjects. *J Appl Res*. 2010;10(1):32-9.
- 498 48. Yoo W. Comparison of hamstring-to-quadriceps ratio between  
499 accelerating and decelerating sections during squat exercise. *Journal of Physical*  
500 *Therapy Science*. 2016;28(9):2468-9.
- 501 49. Cohen J. A power primer. *Psychological bulletin*. 1992;112(1):155.
- 502 50. Hoshikawa Y, Iida T, Muramatsu M, Nakajima Y, Fukunaga T, Kanehisa  
503 H. Differences in thigh muscularity and dynamic torque between junior and senior  
504 soccer players. *Journal of sports sciences*. 2009;27(2):129-38.
- 505 51. Zakas A. Bilateral isokinetic peak torque of quadriceps and hamstring  
506 muscles in professional soccer players with dominance on one or both two sides.  
507 *Journal of Sports Medicine and Physical Fitness*. 2006;46(1):28.
- 508 52. Gstöttner M, Neher A, Scholtz A, Millonig M, Lember S, Raschner C.  
509 Balance ability and muscle response of the preferred and nonpreferred leg in  
510 soccer players. *Motor Control*. 2009;13(2):218-31.

- 511 53. Fousekis K, Tsepis E, Vagenas G. Lower limb strength in professional  
512 soccer players: profile, asymmetry, and training age. *Journal of Sports Science*  
513 *and Medicine*. 2010;9(3):364-73.
- 514 54. Daneshjoo A, Rahnema N, Mokhtar AH, Yusof A. Bilateral and Unilateral  
515 Asymmetries of Isokinetic Strength and Flexibility in Male Young Professional  
516 Soccer Players. 2013;36(1):45.
- 517 55. Pincivero DM, Aldworth C, Dickerson T, Petry C, Shultz T. Quadriceps-  
518 hamstring EMG activity during functional, closed kinetic chain exercise to fatigue.  
519 *European journal of applied physiology*. 2000;81(6):504-9.
- 520 56. Schwanbeck S, Chilibeck PD, Binsted G. A comparison of free weight  
521 squat to Smith machine squat using electromyography. *The Journal of Strength*  
522 *& Conditioning Research*. 2009;23(9):2588-91.
- 523 57. Housh TJ, deVries HA, Johnson GO, Housh DJ, Evans SA, Stout JR, et  
524 al. Electromyographic fatigue thresholds of the superficial muscles of the  
525 quadriceps femoris. *European journal of applied physiology and occupational*  
526 *physiology*. 1995;71(2):131-6.
- 527 58. Crossley K, Bennell K, Green S, McConnell J. A systematic review of  
528 physical interventions for patellofemoral pain syndrome. *Clinical Journal of Sport*  
529 *Medicine*. 2001;11(2):103-10.
- 530 59. Ninos JC, Irrgang JJ, Burdett R, Weiss JR. Electromyographic analysis of  
531 the squat performed in self-selected lower extremity neutral rotation and 30 of  
532 lower extremity turn-out from the self-selected neutral position. *Journal of*  
533 *Orthopaedic & Sports Physical Therapy*. 1997;25(5):307-15.
- 534 60. Wright GA, DeLong TH, Gehlsen G. Electromyographic Activity of the  
535 Hamstrings During Performance of the Leg Curl, Stiff-Leg Deadlift, and Back  
536 Squat Movements. *The Journal of Strength & Conditioning Research*.  
537 1999;13(2):168-74.
- 538 61. Schuermans J, Van Tiggelen D, Danneels L, Witvrouw E. Biceps femoris  
539 and semitendinosus—teammates or competitors? New insights into hamstring  
540 injury mechanisms in male football players: a muscle functional MRI study. *British*  
541 *journal of sports medicine*. 2014;48(22):1599-606.
- 542 62. Thelen DG, Chumanov ES, Sherry MA, Heiderscheit BC.  
543 Neuromusculoskeletal models provide insights into the mechanisms and  
544 rehabilitation of hamstring strains. *Exercise and sport sciences reviews*.  
545 2006;34(3):135-41.
- 546 63. Coombs R, Garbutt G. Developments in the use of the  
547 hamstring/quadriceps ratio for the assessment of muscle balance. *J Sports Sci*  
548 *Med*. 2002;1(3):56-62.
- 549 64. Ebben W, Jensen. Electromyographic and kinetic analysis of traditional,  
550 chain, and elastic band squats. *The Journal of Strength & Conditioning Research*.  
551 2002;16(4):547-50.
- 552 65. Selseth A, Dayton M, Cordova ML, Ingersoll CD, Merrick MA. Quadriceps  
553 concentric EMG activity is greater than eccentric EMG activity during the lateral  
554 step-up exercise. *Journal of Sport Rehabilitation*. 2000;9(2):124-34.
- 555 66. Yavuz HU, Erdağ D, Amca AM, Arıtan S. Kinematic and EMG activities  
556 during front and back squat variations in maximum loads. *Journal of Sports*  
557 *Sciences*. 2015;33(10):1058-66.
- 558 67. Pincivero DM, Gandhi V, Timmons MK, Coelho AJ. Quadriceps femoris  
559 electromyogram during concentric, isometric and eccentric phases of fatiguing  
560 dynamic knee extensions. *Journal of Biomechanics*. 2006;39(2):246-54.

- 561 68. Nardone A, Romano C, Schieppati M. Selective recruitment of  
562 high-threshold human motor units during voluntary isotonic lengthening of active  
563 muscles. *The Journal of physiology*. 1989;409(1):451-71.
- 564 69. Laidlaw DH, Bilodeau M, Enoka RM. Steadiness is reduced and motor unit  
565 discharge is more variable in old adults. *Muscle & Nerve: Official Journal of the*  
566 *American Association of Electrodiagnostic Medicine*. 2000;23(4):600-12.
- 567 70. Behm DG, Anderson K, Curnew RS. Muscle force and activation under  
568 stable and unstable conditions. *The Journal of Strength & Conditioning Research*.  
569 2002;16(3):416-22.
- 570 71. Jönhagen S, Halvorsen K, Benoit DL. Muscle activation and length  
571 changes during two lunge exercises: implications for rehabilitation. *Scandinavian*  
572 *journal of medicine & science in sports*. 2009;19(4):561-8.
- 573 72. Richards J, Thewlis D, Selfe J, Cunningham A, Hayes C. A biomechanical  
574 investigation of a single-limb squat: implications for lower extremity rehabilitation  
575 exercise. *Journal of athletic training*. 2008;43(5):477-82.
- 576 73. Heiderscheit BC, Sherry MA, Silder A, Chumanov ES, Thelen DG.  
577 Hamstring strain injuries: recommendations for diagnosis, rehabilitation, and  
578 injury prevention. *journal of orthopaedic & sports physical therapy*.  
579 2010;40(2):67-81.
- 580

# Activation Pattern

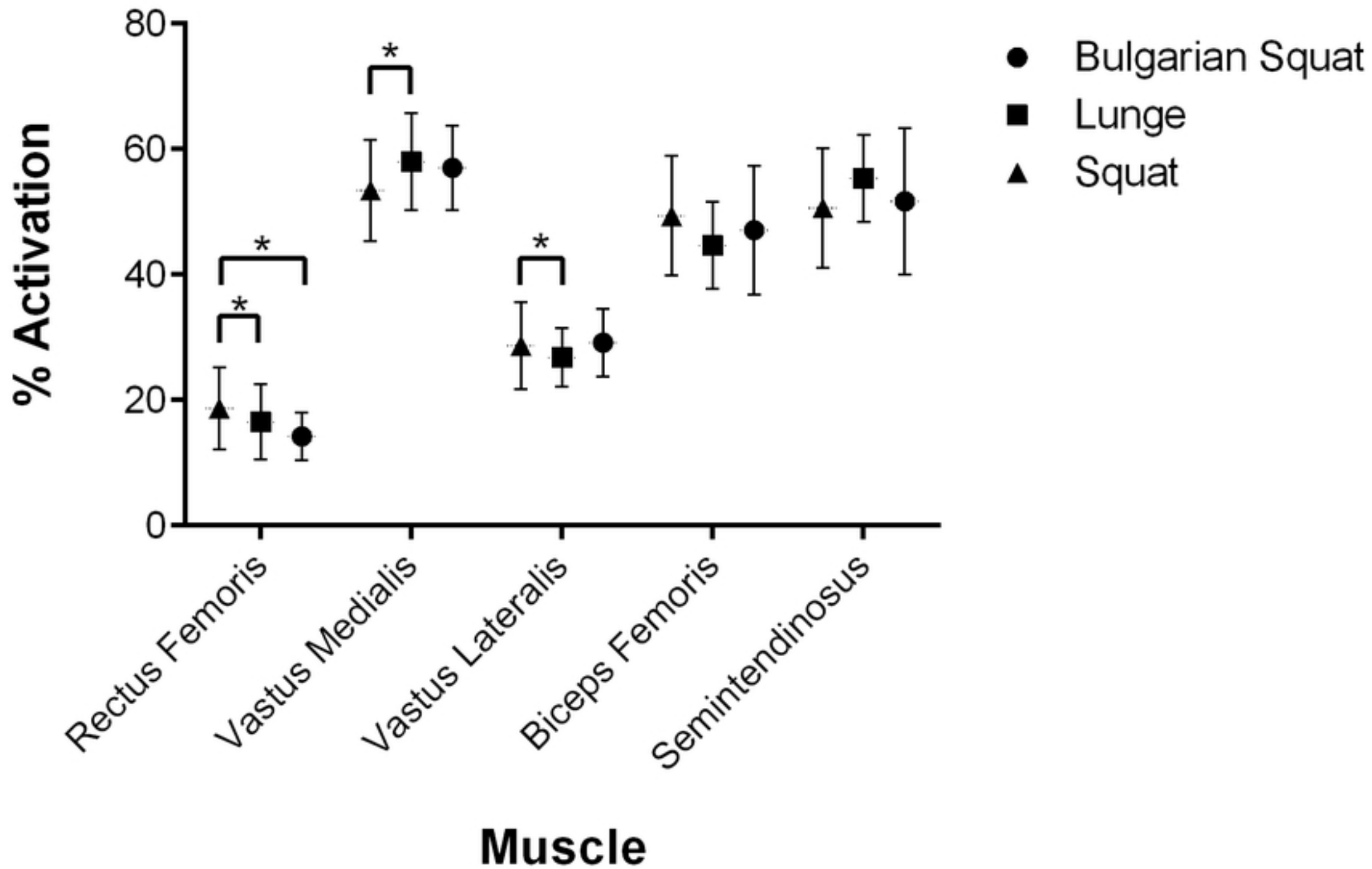


Figure 1

# Bulgarian Squat

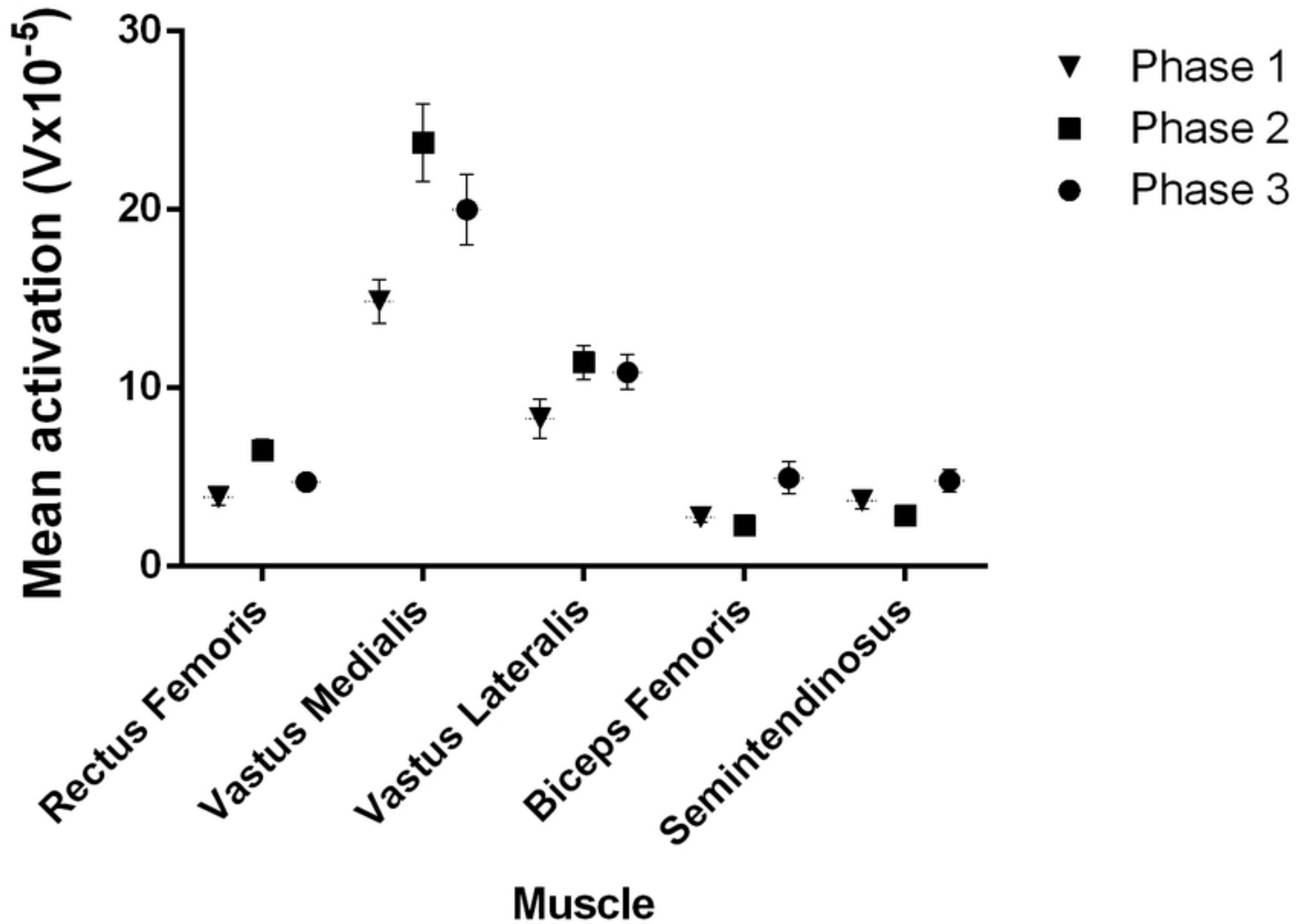


Figure2

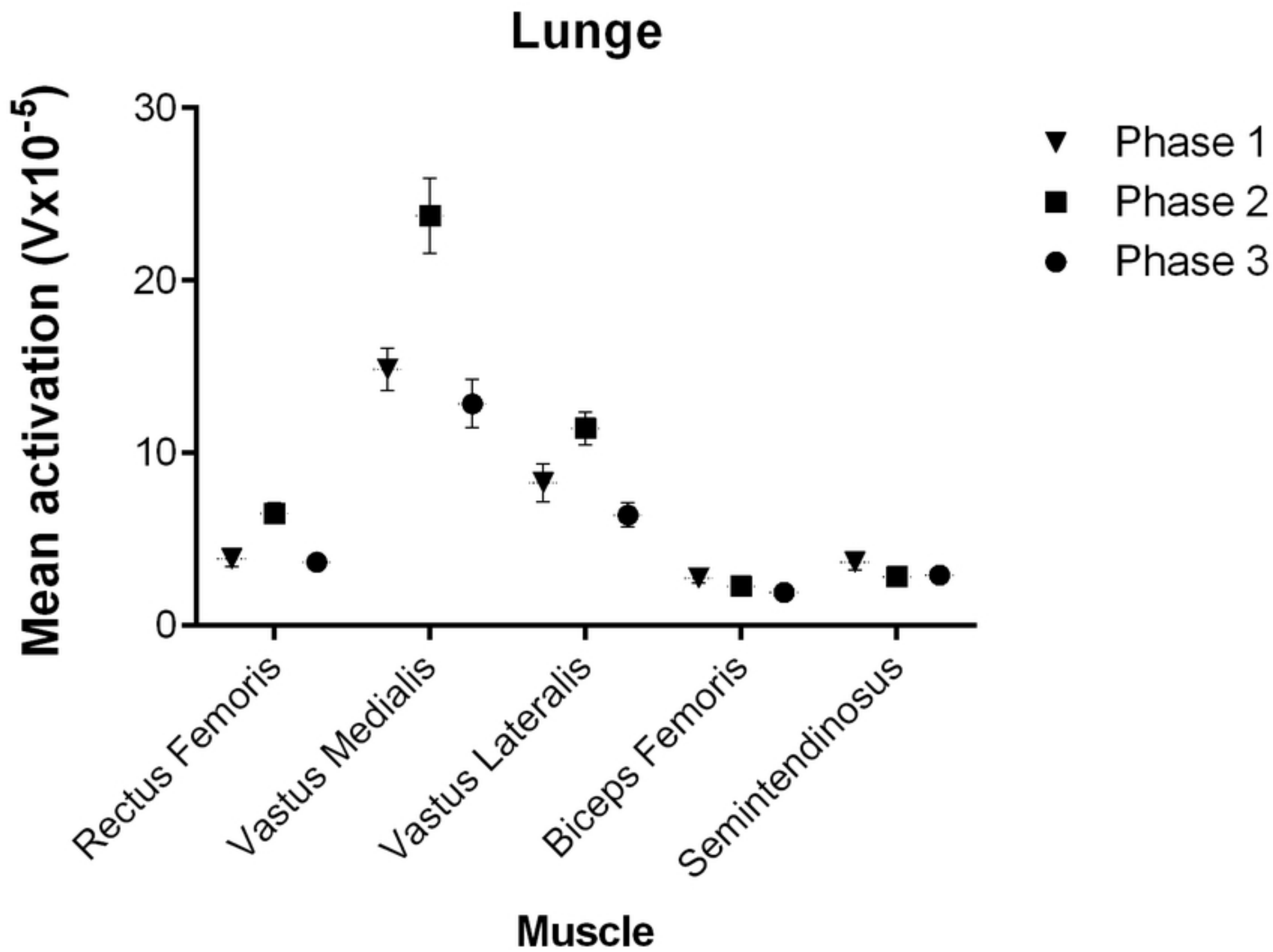


Figure3

# Squat

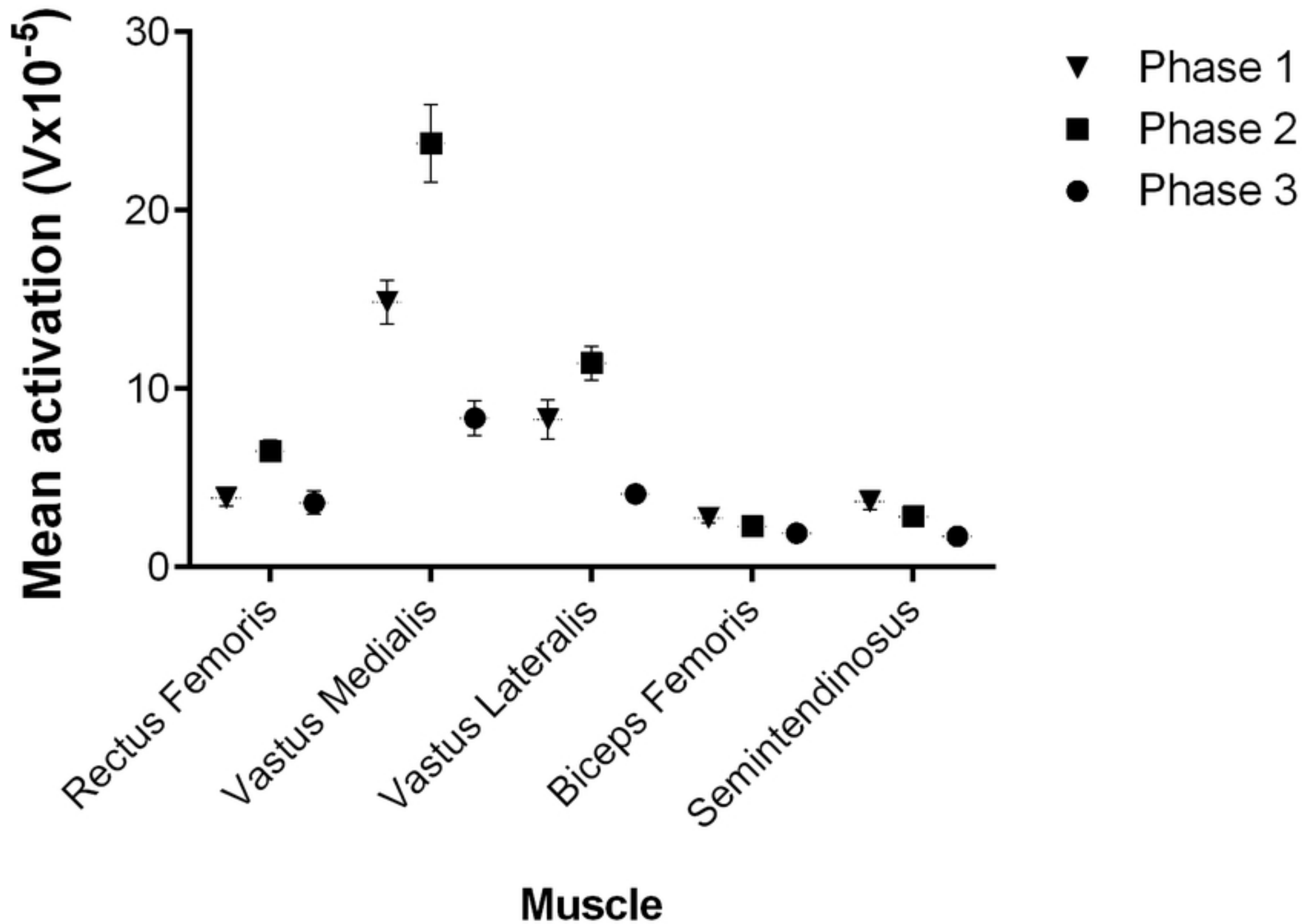


Figure4