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Forward modelling reveals dynamics of neural orientation tuning to unconscious visual stimuli during binocular rivalry

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Abstract

When different visual stimuli are presented to the two eyes, they typically compete for

access to conscious perception, a phenomenon known as *binocular rivalry*. Previous

studies of binocular rivalry have shown that neural responses to consciously

suppressed stimuli are markedly diminished in magnitude, though they may still be

encoded to some extent. Here we employed multivariate forward modelling of human

electroencephalography (EEG) data to quantify orientation-selective responses to

visual gratings during binocular rivalry. We found robust orientation tuning to both

conscious and unconscious gratings. This tuning was enhanced for the suppressed

stimulus well before it was available for conscious report. The same pattern was

evident in the overall magnitude of neural responses, and it emerged even earlier than

the changes in neural tuning. Taken together, our findings suggest that rivalry

suppression affects broadband, non-orientation selective aspects of neural activity

before refining fine-grained feature-selective information.

There is considerable evidence that the human brain can encode sensory events

that elude conscious detection, either following acquired lesions of the sensory or

association areas (Cowey & Stoerig, 1995; Mattingley, Davis, & Driver, 1997), or due to

masking (Enns & Di Lollo, 2000) or attentional manipulations of relevant stimuli (D. E.

Broadbent & Broadbent, 1987; Raymond, Shapiro, & Arnell, 1992). A particularly

striking example occurs during binocular rivalry, in which the presentation of different

images to the two eyes leads to alternating periods during which the image to one eye

is clearly perceived while the other is suppressed from awareness. One reason for the

continued interest in binocular rivalry is that it provides a window onto the neural bases

of consciousness (Ling & Blake, 2009; Rees, Kreiman, & Koch, 2002; Tong, Nakayama,

Vaughan, & Kanwisher, 1998) by allowing investigators to compare patterns of brain

activity elicited by pairs of stimuli that are held constant while conscious perceptual

reports alternate stochastically over time. Although previous research has shown that

neural responses to suppressed stimuli are reduced in overall amplitude, no study to

date has determined how the basic features that define such stimuli, such as their

colour or orientation, are affected under conditions of binocular suppression. Here we

addressed this question directly by recording neural activity with

electroencephalography (EEG) while observers viewed rivalrous displays in which

differently coloured and oriented gratings were projected to each eye. We used

frequency tagging to track neural activity to each grating over time, and applied

multivariate forward encoding modelling to recover orientation tuning profiles for the

two stimuli as they alternated between conscious and unconscious perception.

A persistent question in the literature on binocular rivalry concerns the extent to

which the brain represents stimuli that are currently suppressed from awareness.

Invasive recordings in macaques (Leopold & Logothetis, 1996; Logothetis & Schall,

1989) have shown that neurons in early cortical areas continue to respond to stimuli

that are under binocular suppression. For some neurons, firing rates appear to track

the animal's perceptual reports, becoming lower when the stimulus is suppressed and

higher when it is perceived. Likewise, human neuroimaging studies (Brown & Norcia,

1997; Lansing, 1964; Polonsky, Blake, Braun, & Heeger, 2000; Srinivasan, Russell,

Edelman, & Tononi, 1999; Tong et al., 1998; Tononi, Srinivasan, Russell, & Edelman,

1998) have shown that the overall magnitude of neural responses in early cortical areas

is modulated according to observers' subjective perceptual report. For example,

studies using EEG to track the time course of neural activity during binocular rivalry

have revealed that response profiles to perceived and suppressed stimuli are anti-

correlated, and that perceived stimuli elicit a larger neural response overall (Brown &

Norcia, 1997; Haynes, Deichmann, & Rees, 2005; Tononi et al., 1998; Zhang, Jamison,

Engel, He, & He, 2011). Studies using functional magnetic resonance imaging (fMRI)

have localised these effects to relatively early cortical areas (Polonsky et al., 2000;

Tong et al., 1998; Tong & Engel, 2001). In higher areas, activity induced by suppressed

inputs may still be present, if for example the stimuli carry biologically salient

information (e.g., fearful faces(Pasley, Mayes, & Schultz, 2004; Williams, Morris,

McGlone, Abbott, & Mattingley, 2004), while it can be completely absent in other brain

regions (Pasley et al., 2004; Tong et al., 1998) This work suggests that any neural

activity elicited by the suppressed stimulus is simply too weak to cross the threshold

for conscious report.

All previous studies in humans have focused exclusively on the overall *level* of

neural activity during binocular rivalry, rather than on the time-varying patterns of

activity associated with changes in the features of suppressed visual inputs. However,

other aspects of the stimulus' representation, in addition to the overall magnitude of

response, are known to be critical for conscious detection of targets (Kullback &

Leibler, 1951). Here we asked whether orientation selectivity, which can be defined

along several dimensions, including the amplitude or gain of stimulus evoked activity

as well as the fidelity or sharpness of neural tuning, is modulated for a fixed stimulus as

it alternates between periods of conscious perception and suppression. Behavioural

work in humans has suggested that stimulus selectivity is affected during rivalry (Ling &

Blake, 2009; Lunghi & Alais, 2013), but no study to date has examined how rivalry

affects neural representations of specific stimulus features.

To address this question we used multivariate forward modelling (Brouwer &

Heeger, 2009; Garcia, Srinivasan, & Serences, 2013; Smout, Tang, Garrido, &

Mattingley, 2019; Sprague & Serences, 2013; Tang, Smout, Arabzadeh, & Mattingley,

2018) of human electroencephalography (EEG) data to quantify orientation-selective

responses to visual gratings that were undergoing changes in awareness during

binocular rivalry. To anticipate the results, we observed robust orientation tuning to

both conscious and unconscious gratings. Strikingly, orientation tuning began to

increase for the currently suppressed stimulus more than 300 ms before observers

were aware of it, while at the same time orientation tuning began to decline for the

currently perceived grating that was about to be suppressed from awareness. The

same pattern was evident for the overall magnitude of neural responses, and this effect

emerged even earlier than the changes in neural tuning (~800 ms before observers'

button press indicating a switch in percept). Taken together, our findings suggest that

rivalry suppression first affects the broadband, and non-orientation selective aspects of

the neural information, before refining the fine-grained feature selective information.

111   **Results**

To quantify the time-course and extent of neural information processing of

conscious and unconscious stimuli, we presented spatially overlapping red and green

gratings dichoptically to the left and right eyes. (Figure 1A; Movie 1). Dichoptic

presentation causes interocular suppression, such that observers perceive a single

coherent image that oscillates stochastically between the two stimuli over time, with

occasional mixed percepts in between (Figure 1B; (Alais & Blake, 2005; Levelt, 1965).

To measure time-resolved neural responses to the stimuli, we recorded neural activity

using EEG, while the two orthogonally oriented gratings counter-phase flickered at two

different frequencies (20 and 24 Hz). The two gratings generated distinct steady-state

visual evoked potentials (SSVEPs) that were tracked continuously over each 30 s trial.

As described in detail below, the orientations of the two gratings varied from 0° to 160°

(in 20° steps) across the trials to enable modelling of orientation-selective responses as

a function of perceptual awareness. Participants (N = 22) reported whether they

perceived the red or green grating, or a mixed percept, while we measured SSVEP

responses. The magnitude of SSVEPs generated by rivalrous gratings are typically anti-

correlated, exhibiting a larger response to the grating that is consciously perceived

than to the grating that is suppressed from awareness (Zhang et al., 2011).

Figure 1. The SSVEP paradigm used to measure neural activity elicited by conscious and unconscious grating stimuli during binocular rivalry. **(A)** A red and green grating were presented on a computer screen while neural activity was recorded using EEG. A mirror stereoscope and a dividing board ensured that each eye received visual information exclusively from one of the two gratings, yielding binocular rivalry. **(B)** Under binocular rivalry observers typically perceive a slowly alternating percept in which one of the two gratings dominates in perception and the other is suppressed. Here observers occasionally reported a combination of either colour or orientation information (i.e., a mixed percept). **(C)** To separately track the brain's response to the gratings, the two stimuli counter-phase flickered at 20 and 24 Hz, producing unique frequency tags in the EEG. An illustrative segment from a typical trial of the rivalry task showing neural responses to the gratings (i.e. the power at the tagged frequencies) as a function of the participant's percept. **(D)** Mean frequency response for all participants across the entire 30 s trial (averaged over electrodes Oz, O1, O2, POz). Grey shading indicates ∓1 standard error of the mean. **(E)** Distribution of SSVEP responses for the 20 and 24 Hz gratings across the scalp for all participants.

Binocular rivalry affects the overall strength of neural responses

The median duration of perceptual dominance, during which one grating was

perceived while the other was suppressed, lasted for 1390 ms (interquartile range =

1024 to 2349 ms; Figure 2A). To determine the effect of binocular rivalry on neural

responses to the two gratings, SSVEP responses were epoched into bins that

extended from 2s before the participant indicated a change in percept to 2 s after this

response. The data were then combined across the flicker frequencies of the two

presented gratings to produce 'aware' and 'unaware' epochs (see Methods for further

details). The label of the response (i.e., aware versus unaware) was defined relative to

the percept reported at the time of the button press (0 ms). As shown in Figure 2B, the

SSVEP elicited by the currently suppressed grating began to increase around 1500 ms

before the stimulus was consciously perceived. At the same time, the SSVEP elicited

by the currently perceived stimulus began to decline sharply after it had been reported,

and the response to the suppressed stimulus began to rise. Thus, around 1000 ms

after the observers' button press, the neural response to the unaware stimulus was

now larger than the response to the stimulus that was currently perceived. This timing

fits with the behavioural observation that periods of stimulus dominance lasted on

average around 1390 ms. As shown in Figure 2C, SSVEPs elicited by the grating

stimuli were most pronounced over occipital-parietal electrode sites, as expected for

such square-wave grating stimuli (Tong et al., 1998; Zhang et al., 2011).

Figure 2. Behavioural and neural results associated with changes in awareness during binocular rivalry. **(A)** Distribution of durations of perceptual dominance across the 22 participants. **(B)** Time series of relative EEG power elicited by the grating stimuli, plotted separately for aware and unaware periods of the trial, averaged across three occipital electrodes (Oz, POz, Pz). The 'aware' response corresponds to the grating reported as the dominant percept at the time of the button press (0 ms), and the 'unaware' response corresponds to the suppressed stimulus at the same time point. The black horizontal lines indicate periods of significant difference between the conditions (two-tailed cluster-permutation, alpha $p < .05$, cluster alpha $p < .05$, N permutations = 20,000). **(C)** Headmaps of EEG data showing changes in relative power for periods in which gratings were consciously perceived (Aware, top row) and suppressed (Unaware, middle row), and the difference between these states (bottom row). Circles indicate clusters of electrodes with significantly lower activity, and crosses indicate clusters with significantly greater activity in the Aware vs. Unaware conditions (alpha $p < .05$, cluster $p < .025$, N permutations = 1500). **(D)** Accuracy of linear discriminant analysis used to predict observers' grating perception at time 0 ms (corresponding to the participants' button press). Coloured horizontal bars indicate times during which classification accuracy was significantly better than chance for Aware and Unaware epochs. Coloured shading in C and D represents ∓1 standard error of the mean.

Stimulus-evoked SSVEPs predict perceptual reports prior to awareness

We next sought to determine whether SSVEPs could be used to predict which

percept the participant would report on a single-trial basis. To do this, we used a

multivariate linear discriminant analysis to determine whether there were patterns of

activity distributed across the scalp that predicted which grating was about to be

consciously perceived. Separately, for each SSVEP frequency and at each time point

across the epoch around when the percept changed, the classifier was trained on the

percept reported at time zero, which coincided with the participants' indicated

perceptual report. Again, the results were combined across frequencies to produce

unaware and unaware responses. Neural responses to consciously perceived gratings

predicted observers' perceptual reports around 800 ms before the report occurred

(Figure 2D), whereas neural responses to the unaware gratings did not reliably predict

observers' reports at this same time point. By contrast, at around 1000 ms after

observers made their response, SSVEP power was able to predict observers'

perceptual reports for both the aware and unaware stimuli.

Binocular rivalry affects visual orientation selectivity

Next, we sought to answer the critical question of whether orientation selectivity

for the rivalrous gratings was influenced by observers' awareness of the frequency-

tagged stimulus. To do this, we applied forward encoding modelling, which has

previously been used to recover orientation selectivity from both EEG and MEG activity

(Brouwer & Heeger, 2009; Garcia et al., 2013; Smout et al., 2019; Sprague & Serences,

2013; Tang et al., 2018) Broadly, this technique identifies multivariate patterns of EEG

activity that are selective for defined stimulus features, in this case orientation (see

Figure 3 for an example). We convolved grating orientation in each epoch against a

bank of nine canonical, orientation-selective tuning functions, each maximally sensitive

to a different orientation, to produce regression coefficients for that trial (Figure 3B).

Then at each time point in the epoch, multivariate regression was used to estimate the

spatial map (or *weight matrix*) sensitive to orientation in a training set of data. This

weight matrix (Figure 3C) was inverted and multiplied against a test set of data (Figure

3D) to determine orientation selectivity (Figure 3E) in the test data. The procedure was

iterated over all time points in the epoch, and a cross-validation procedure was used

such that all epochs served in both training and test data.

Figure 3. Overview of the forward encoding modelling procedure used to measure orientation selectivity in the binocular rivalry paradigm. **(A)** Patterns of SSVEP activity (here separated into real and imaginary components) are measured in response to a range of orientations. **(B)** Regression coefficients for the orientations are estimated for each trial from orientation selective functions. **(C)** Least-squares regression is used to estimate weights for all EEG electrodes for each of the channels in the orientation model. The channel weights are shown here for three example occipital-parietal electrodes. **(D)** The channel weights are inverted and multiplied against a set of independent training data. **(E)** The model will reconstruct the presented orientation if there is an orientation selective response. In this case, the stimulus reconstruction shows a tuned response to a presented grating of 20° orientation. **(F)** Average orientation reconstructions over time for the two SSVEP frequencies (collapsed across aware and unaware conditions) for all participants for each of the nine presented orientations, indicated by the black dotted line. These reconstructions were realigned so we could combine the representations of the different orientations.

Figure 3F shows the results of the forward encoding modelling for each of the

presented orientations (20° to 180° in 20° steps) for the two SSVEP frequencies of 20

and 24 Hz. As shown, the forward encoding model successfully recovered the

presented orientation across all time points in the epoch. Because we were not

interested in any specific orientation, but rather in orientation selectivity in general, and

to increase the signal to noise ratio, we re-centred all the representations to the

presented orientation (0° for consistency) in that trial. To quantify orientation selectivity

between different conditions, these outputs were fit with a Gaussian function, with the

amplitude providing an index of orientation selectivity (see Methods for details).

The forward encoding model revealed a strong orientation-selective neural

response that was tuned to the presented orientation (Figure 4A). Strikingly, we found

orientation-selective response to both the currently perceived grating and to the

grating that was suppressed due to binocular rivalry. Critically, this result suggests that

the visual system encodes feature-selective information about the presented stimulus

even when that stimulus is not consciously perceived. Moreover, just prior to the

observers' button press indicating a switch in percept, the grating that was currently

suppressed but was about to be consciously reported was associated with

significantly greater orientation selectivity than the grating that was perceived (but was

about to be suppressed).

Figure 4. Results of forward encoding modelling for orientation selectivity under binocular rivalry. **(A)** Orientation decoding (given by height of tuning curves) over time for SSVEP responses elicited by aware and unaware gratings. The 'aware' response corresponds to the grating reported as the dominant percept at the time of the button press (0 ms), and the 'unaware' response corresponds to the suppressed stimulus at the same time point. The horizontal black bars indicate significant differences between the aware and unaware conditions (two-tailed cluster-permutation, alpha $p < .05$, cluster alpha $p < .05$, N permutations = 20,000). Coloured shadings show ∓1 standard error of the mean. **(B)** Orientation tuning curves collapsed across significant time points shown in A. Error bars show ∓1 standard error of the mean. The lines are fitted Gaussians (Equation 4) to data averaged across observers.

To further determine how orientation selectivity was affected by awareness, we

averaged the time-resolved tuning curves over the significant time points (black lines in

Figure 4A) to recover the tuning curve, and fitted Gaussian functions to quantify the

change in neural representations (Figure 4B). This again revealed robust orientation-

selective responses to both aware and unaware stimuli, shown by the tuned response

at the presented orientation (0°). The analysis also confirmed that the amplitude of the

orientation-tuning functions was reliably larger for grating stimuli when they were aware

than when they were unaware ($p = .01$), suggesting that conscious perception is

associated with a boost in the gain of orientation selectivity (or a suppression in the

gain for suppressed stimuli). Crucially, however, at the same time points relative to

observers' perceptual reports, there was no change in the width of the tuning functions

($p = .37$), suggesting that awareness does not alter the fidelity or tuning of the

underlying neural representation (aware $M = 33.70$, $SE = 2.97$; unaware $M = 31.58$, SE

$= 1.25$).

288   **Discussion**

We investigated how binocular rivalry affects the neural representation of visual

orientation information in human observers. Previous work in non-human primates has

shown that the selectivity of neurons in visual areas tracks changes in awareness, such

that suppressed stimuli evoke a smaller selective response than dominant (perceived)

stimuli. It has remained unclear whether the same changes in feature-selectivity occur

in humans because conventional neuroimaging approaches focus on overall levels of

activity, rather than tracking the time-varying changes in selectivity for elementary

stimulus features. Here we used forward encoding modelling to determine how

orientation selectivity was influenced under conditions in which orthogonally oriented

pairs of gratings were presented dichoptically to induce binocular rivalry.

We found significant orientation selectivity in neural activity associated with both

aware and unaware gratings, and this response increased just before the reported

change in awareness. Forward encoding modelling allowed us to quantify orientation

tuning curves. These analyses revealed that while the gain (amplitude) of orientation

tuning was affected by rivalry, the fidelity (or sharpness) was not. We also found that

the overall neural response to the gratings, as indexed by the power of the frequency-

tagged SSVEP, began to increase ~1000 ms before orientation-selectivity changed. On

a single trial basis, from the power of the SSVEP response alone, it was possible to

predict an observer's choice ~800 ms before the individual reported the change. As

with most previous investigations of binocular rivalry (Alais, Cass, O'Shea, & Blake,

2010; Brown & Norcia, 1997; Tong et al., 1998; Zhang et al., 2011), we used observers'

button-press responses to demarcate changes in awareness, and these perceptual

switches typically precede overt responses by 300 to 400 ms (Alais et al., 2010). Such

response time delays cannot account for the current findings, however, as SSVEP

power predicted observers' percepts ~800 ms before their responses. This observation

suggests that during rivalry, alternations in awareness of rivalrous stimuli are initially

signalled by broadband changes which are not selective for orientation in neural

activity, followed by a change in fine-grained stimulus selectivity immediately prior to a

change in conscious report.

Our results are broadly consistent with findings from invasive recordings in

macaque visual cortex during binocular rivalry (Leopold & Logothetis, 1996; Logothetis,

Leopold, & Sheinberg, 1996). Around 300 ms before the currently suppressed stimulus

broke into awareness, we found that orientation selectivity for the grating began to

increase. This anticipatory neural response in humans is consistent with findings from

neuronal recordings in macaque area V4, which have shown that the firing rate of

neurons during binocular rivalry increases around 300-500 ms before the animal

reports a change in the perceived stimulus. Our work goes beyond these findings by

showing that, in humans, orientation-selective information is reliably available to the

system even when a rivalrous stimulus is not consciously perceived.

More broadly, our findings are consistent with the influential global workspace

theory of consciousness (Dehaene & Naccache, 2001; Salti et al., 2015), which

proposes that while all stimulus information is represented by early sensory regions,

only those that get fed through to higher cortical regions activate a global brain

network and thus reach awareness. On this account, stimuli reach awareness because

they induce high synchrony within a global network of more local networks. Once an

item has activated the global network, it can inhibit alternative and competing stimuli.

Our results potentially add to this account, as we found that during rivalry broadband

neural responses first change with awareness, and are followed several hundred

milliseconds later by more fine-grained (feature-specific) changes in stimulus

representations. One way this might occur is via feedback connections from higher

brain areas, which are predicted to have access to the global workspace, to lower-level

sensory regions which represent stimulus-selective information such as visual

orientation. This idea could be tested by disrupting higher cortical areas – for example

using transcranial magnetic stimulation – and measuring changes in orientation tuning

to rivalrous stimuli. Future studies could also apply the forward encoding approach

used here to assess feature-specific neural responses in different experimental

paradigms in which conscious reports are altered, such as visual masking (Enns & Di

Lollo, 2000), or in cases of neural pathologies such as blindsight (Cowey & Stoerig,

1995) or unilateral spatial neglect (Driver & Mattingley, 1998; Mattingley et al., 1997).

348   **Methods**

Participants

A group of 26 healthy adult observers (age range = 18 to 37 yr) participated in

exchange for partial course credit or financial reimbursement (AUD$20/hr). All

participants provided written informed consent, and all reported normal or corrected-

to-normal vision and normal colour perception. We based the sample size on previous

studies using SSVEPs to investigate binocular rivalry (Jamison, Roy, He, Engel, & He,

2015; Zhang et al., 2011), forward encoding modelling (Garcia et al., 2013; Myers et

al., 2015; Smout et al., 2019; Tang et al., 2018; Wolff, Jochim, Akyürek, & Stokes,

2017) and from initial pilot testing. The study was approved by The University of

Queensland Human Research Ethics Committee and was conducted in accordance

with the Declaration of Helsinki.

Experimental setup

The experiment was conducted inside a dimly illuminated room with participants

seated in a comfortable chair. The stimuli were displayed on a 22-inch LED monitor

(resolution 1920 x 1080 pixels, refresh rate 120 Hz) using PsychToolbox presentation

software (Brainard, 1997; Pelli, 1997) for MATLAB (v7.3). Viewing distance was

maintained at 54 cm using a chinrest, meaning each pixel subtended 1.8' x 1.8'.

Task

Task

Prior to the start of the experiment, participants aligned the mirror stereoscope

(Fig 1A) so images presented to the left and right eyes appeared overlapping. Identical

circular checkerboards were placed around the stimulus in both eyes to encourage

fusion of the images. Each trial began with presentation of these checkerboards and a

central Gaussian fixation dot. After 1500 ms, green and red square-wave gratings were

presented to the left and right eyes, so that they appeared within the centre of the

surrounding checkerboards. The colours were presented at 100% luminance intensity.

To generate SSVEPs, the gratings counter-phase flickered at 20 and 24 Hz for 30 s.

Counter-phase flickering square-wave gratings were used because these produce

large SSVEP responses (Brown & Norcia, 1997; Norcia, Appelbaum, Ales, Cottereau, &

Rossion, 2015) and produce orientation-selective neural activity that can be tracked

with EEG (Garcia et al., 2013). Participants indicated whenever the percept (red, green

or mixed) changed during the trial using separate keys on a standard keyboard. For

half the participants, the red gratings flickered at 20 Hz and the green gratings flickered

at 24 Hz; for the remaining participants these contingencies were reversed.

Across trials the orientations of the gratings were varied between 0° and 160° (in

20° steps) so that forward encoding modelling could be employed to determine

orientation selectivity contained with the EEG data. The orientations of the pairs of

gratings presented in each trial were always perpendicular to ensure strong rivalry

between the stimuli (Haynes & Rees, 2005; Logothetis et al., 1996; O'Shea, 1998).

There were 90, 30 s trials in total across the experiment, meaning that each orientation

was repeated 10 times.

EEG acquisition and pre-processing

Continuous EEG data were recorded using a BioSemi Active Two system

(BioSemi, Amsterdam, Netherlands). The signal was digitised at 1024 Hz sampling rate

with a 24-bit A/D conversion. The 64 active scalp Ag/AgCl electrodes were arranged

according to the international standard 10–20 system for electrode placement [26]

using a nylon head cap. As per BioSemi system design, the common mode sense and

driven right leg electrodes served as the ground, and all scalp electrodes were

referenced to the common mode sense during recording.

Offline EEG pre-processing was performed using EEGLAB in accordance with

best practice procedures (Bigdely-Shamlo, Mullen, Kothe, Su, & Robbins, 2015; Keil et

al., 2014). The data were initially down sampled to 256 Hz and subjected to a 0.5 Hz

high-pass filter to remove slow baseline drifts. Electrical line noise was removed using

the *clean_line.m,* and *clean_rawdata.m* in EEGLAB [29] was used remove bad channels

(identified using Artifact Subspace Reconstruction), which were then interpolated from

the neighbouring electrodes. Data were then re-referenced to the common average

before being epoched into trials (-1 to 31 s). Systematic artefacts from eye blinks,

movements and muscle activity were identified and regressed out of the signal using

semi-automated procedures in the SASICA toolbox (Chaumon, Bishop, & Busch,

2015). After this stage, any trial with a peak voltage exceeding ±100 *uV* was excluded

from the analysis.

Data analysis

A wavelet transform (150 ms time-domain standard deviation) was applied to

the recorded EEG data in each trial to extract the neural response to the two gratings.

The data were then epoched into 4 s time periods symmetrically around each button

press (-2 s to + 2 s), which observers used to indicate a change in the perceived

grating. Epochs were only included if the preceding epoch was not a mixed percept, so

we were certain the preceding epoch was the previously aware stimulus. We did not

include periods with mixed percepts because these are by definition ambiguous with

respect to stimulus awareness (i.e., both stimuli are perceived to some extent). Epochs

were also only included if the button press occurred between 2 and 28 s into the trial

(thus ensuring a robust frequency tagged signal). To ensure the encoding reflected

periods of stable perception, only dominance periods lasting longer than 500 ms were

included. Two participants were excluded because most responses were between one

colour and mixed. Two further participants were excluded because they reported

significantly fewer switch (<100, SD < 2 SD below average). This produced a mean of

1276 epochs for the remaining (N = 22) participants (range = 445 to 1963 across the

participants). For each participant the periods of dominance were relatively evenly split

between the two colors; there were relatively fewer periods in which the percept was

mixed, and these tended to be shorter-lived in duration (Figure 2A). To maintain

consistent phase information in the SSVEPs, we aligned the nearest counter-phase

flicker within the epoch to the participants' button press, separately for the 20 and 24

Hz frequencies.

Forward encoding modelling

We used forward encoding modelling to extract the orientation selective

response from the patterns of EEG activity. This technique transforms sensor-level

activity distributed across the scalp into tuned 'feature-channels' that are selective for

a specific feature dimension, in this case orientation (Brouwer & Heeger, 2009; Garcia

et al., 2013; Smout et al., 2019; Sprague & Serences, 2013; Tang et al., 2018) To do

this, we used the orientations of the epoched data segments (4 s each) to construct a

regression matrix with 9 regression coefficients for each of the orientations. This

regression matrix was convolved with a tuned set of nine basis functions (half cosine

functions raised to the eighth power) cantered from 0° and 160° (in 20° steps). This

tuned regression matrix was used to measure orientation at each time point in the 4 s

epoched segments. This was done by solving the linear equation (1):

$$B_1 = WC_1 \tag{1}$$

Where B_1 (64 sensors x N training trials) is the electrode data for the training set, C_1 (9

channels x N training trials) is the tuned channel response across the training trials, and

W is the weight matrix for the sensors to be estimated (64 sensors x 9 channels).

Following an approach recently introduced for the analysis of MEG data, we separately

estimated the weights associated with each channel individually (Kok, Mostert, & de

Lange, 2017; Smout et al., 2019). W was estimated using least square regression to

solve equation (2):

$$W = (C_1\ C_1^T)^{-1}\ C_1^T\ B_1 \tag{2}$$

Following this previous work (Kok et al., 2017; Wolff et al., 2017) we also sought to

remove the correlation between the sensors which hinders finding the true solution to

the linear equation. To do this, we first estimated the noise correlation between

electrodes and removed this component through regularisation (Blankertz, Lemm,

Treder, Haufe, & Müller, 2011). The channel response in the test set C_2 (9 channels x N

test trials) was estimated using the weights in (2), and was applied to activity in B_2 (64

sensors x N test trials).

$$C^2 = (W\ W^T)\ W^T\ B^2 \qquad\qquad (3)$$

To avoid overfitting, we used a five-fold cross validation procedure in which 80% of

epochs were used to train the model, and the remaining 20% of epochs were used for

testing. This procedure was repeated until all epochs had served as both training and

test trials. We repeated this procedure for both of the SSVEP frequencies and at each

time-point in the epoch to produce a time-resolved orientation-selectivity function. We

then shifted all trials to a common orientation, so that 0º corresponded to the

orientation presented on each trial. These reconstructions were smoothed with a

Gaussian temporal kernel to increase signal-to-noise (Myers et al., 2015).

To quantify orientation selectivity, we fit the results of the forward encoding

model with a Gaussian function (4) using least square regression to quantify the

amount of orientation selective activity.

$$G(x) =\ A\ exp(-\frac{(x-\phi)^2}{2\sigma^2}) + C \qquad\qquad (4)$$

Where *A* is the amplitude representing the amount of orientation selective activity, ϕ is

the orientation the function is centred on (in degrees), σ is the width (degrees) and *C* is

a constant used to account for non-orientation selective baseline shifts.

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