Altered hypothalamic microstructure in human obesity

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Abstract

Animal studies suggest that obesity-related diets induce structural changes in the hypothalamus, a key brain area involved in energy homeostasis. Whether this translates to humans is largely unknown, as non-invasive brain imaging of the hypothalamus remains challenging. Using a novel multimodal approach with manual segmentation, we here show that body mass index (BMI) selectively predicted higher proton diffusivity within the hypothalamus, indicative of compromised microstructure, in a well-characterized population-based cohort ($n_1 = 338$, 48% females, age 21-78 years, BMI 18-43 kg/m²). Results were independent from confounders and replicated in another independent sample ($n_2 = 236$) which was processed with a tailored automated segmentation procedure. In addition, while hypothalamic volume was not associated with obesity, we identified a sexual dimorphism and larger hypothalamic volumes in the left compared to the right hemisphere. Our findings underpin the relevance of population neuroimaging to discover structural brain changes in subcortical areas that are crucial for understanding obesity and other eating-related disorders.

Introduction

Obesity is associated with dysfunctions in central homeostatic regulation, which might also play a pivotal role in its pathogenesis (Guillemot-Legris & Muccioli, 2017; Waterson & Horvath, 2015). Energy homeostasis (i.e. the balance between food intake and energy expenditure) depends on signaling pathways in the hypothalamus, a small diencephalic brain region comprised of different sub-nuclei (Horvath, 2005; Timper & Brüning, 2017). Here, distinct subpopulations of neurons integrate circulating hormones that signal satiety (e.g. leptin, insulin) and hunger (e.g. ghrelin) (Schwartz, Woods, Porte, Seeley, & Baskin, 2000).

Animal models support the hypothesis that a high-fat diet (HFD) triggers an inflammation-like response in the hypothalamus, which in turn impairs the sensing of anorexigenic signals, thereby contributing to continuous food intake and weight gain (Dorfman & Thaler, 2015; Thaler & Schwartz, 2010). For example, rodents fed a HFD showed increasing levels of proinflammatory cytokines such as interleukin-6 (IL-6) and tumor necrosis factor alpha (TNF α) in the hypothalamus (De Souza et al., 2005), even prior to substantial weight gain (Thaler et al., 2011). This immunologic response was also accompanied by a rapid accumulation of microglia and recruitment of astrocytes (Douglass, Dorfman, & Thaler, 2017; Thaler & Schwartz, 2010). Additionally, hypothalamic neurons showed signs of toxic stress and underwent apoptosis after HFD (Moraes et al., 2009). While some studies reported that this inflammation-like response declined after several days of overnutrition, suggesting a compensatory mechanism to prevent neurons from damage (Baufeld, Osterloh, Prokop, Miller, & Heppner, 2016), others showed that gliosis and astrocytosis reoccurred after several weeks, pointing to prolonged changes in hypothalamic tissue and microstructural properties in obese animals (Thaler et al., 2011).

Whether these neurobiological alterations shown in animal models of obesity also contribute to the pathophysiology of obesity in humans is however largely unknown. A post mortem analysis of obese and non-obese individuals reported that a higher BMI correlated with alterations in hypothalamic glia cells, which exhibited increased levels of dystrophy according to histological stainings (Baufeld et al., 2016). Studies using in vivo magnetic resonance imaging (MRI) linked volumetric changes in the hypothalamus to altered eating behavior within neurodegenerative and psychiatric disorders such as frontotemporal dementia or schizophrenia (Bocchetta et al., 2015; Goldstein et al., 2007; Koolschijn, van Haren, Hulshoff Pol, & Kahn, 2008). However, the direction of effects was partly contradictory and results barely replicated.

Although the assessment of microstructural properties with conventional spin echo or fluid-attenuated inversion recovery in vivo MRI may be limited, two studies provided initial evidence for changes in hypothalamus T2-weighted signals: Thaler et al. showed increased signal ratio in a circular region-of-interest (ROI) in the left hypothalamus referenced to an amygdala-ROI in 12 obese compared to 11 non-obese participants (Thaler et al., 2011). Another study including 67 participants reported higher T2-relaxation times in obesity within a ROI in the left mediobasal hypothalamus, and both studies proposed these measures as a marker of hypothalamic gliosis in diet-induced obesity (Schur et al., 2015; Thaler et al., 2011). Still, applying fixed ROIs could be misleading due to partial volume effects and the heterogenous appearance of the hypothalamus.

In sum, animal experiments and first, but not all, human studies support the hypothesis that central homeostatic changes reflected in compromised (micro)structure of the hypothalamus are present in obesity. However, there is currently no convincing methodology to detect these changes in the living human brain (Alkan et al., 2008; Berkseth et al., 2014; Lizarbe, Benítez, et al., 2013; Puig et al., 2015), and limited

resolution, multiple sources of image artifacts, as well as blurry non-hypothalamic grey

and white matter structures adjacent to the hypothalamus make it difficult to apply

unified landmarks (Baroncini et al., 2012; Goldstein et al., 2007; Koolschijn et al., 2008;

Lizarbe, Benítez, et al., 2013; Schönknecht et al., 2013).

To overcome these methodological constraints, we here combined a novel fine-graded

voxel-wise hypothalamus segmentation algorithm (Schindler et al., 2013; Wolff et al.,

2018) with advanced microstructural measures based on diffusion-weighted-imaging

(DWI) (Alexander, Lee, Lazar, & Field, 2007; Assaf, 2018) in a well-characterized large

population-based sample. We aimed to determine whether larger hypothalamic

volume and higher hypothalamic mean diffusivity (MD), commonly interpreted as less

intact cellular microstructure, are positively associated with obesity measured using

BMI. We also explored whether hypothalamic MD was linked to higher visceral adipose

tissue volume (VAT), given the elevated inflammatory risk profile of this body fat depot

(Shuster, Patlas, Pinthus, & Mourtzakis, 2012). We additionally implemented a

multiatlas-based label segmentation to validate our results in another independent

sample.

Results

Hypothalamic volume

In a sample of 338 participants (48% females, aged 21-78 years, BMI range of 18-43)

kg/m²), we delineated the left and right hypothalamus on T1-weighted anatomical MRI

using a state-of-the-art semi-automated segmentation algorithm resulting in individual

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hypothalamic masks at the voxel-level (Fig. 1A, see Methods for details).

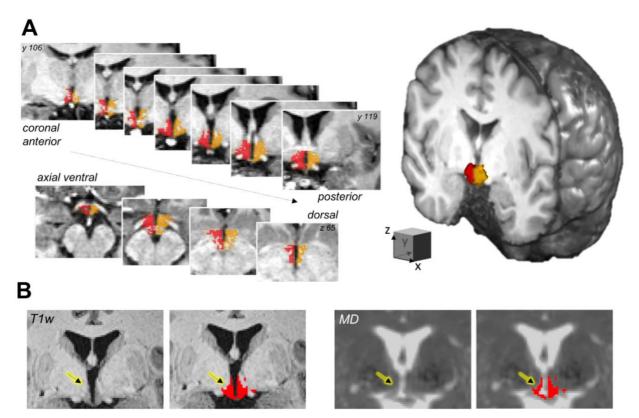


Figure 1: The hypothalamus on multimodal MRI. A: The bilateral hypothalamus (right: red, left: orange) of a representative participant according to semi-automated segmentation on anatomical images. **B**: Coregistration of the T1-weighted (T1w)-derived hypothalamus mask to the mean diffusivity (MD) image derived by diffusion-weighted imaging. Note the sparing of hypothalamus voxels which are affected by partial volume effects on the MD image (arrows). Images are shown in radiological convention.

On average, men showed 12.8% larger head-size adjusted whole hypothalamic volumes than women (**Fig. 2**), statistically significant (β =-0.18, p < 0.001) in a multiple regression model which explained 21.8% of the variance (F_{3,333} = 26.9, p < 0.001) and controlled for potential effects of age (no significant contribution, p = 0.96), and rater (β _{0,1}=-0.56, p < 0.001, β _{0,2}=-0.33, p=0.001). Adding BMI as additional predictor to the model did not improve the model fit (p = 0.58) indicating that BMI was not associated with hypothalamic volume.

When investigating the hemispheres separately, we observed higher volume for the left than for the right hypothalamus, an effect which was slightly less pronounced in women and independent of age and rater (linear mixed effect model, side: β =-40.9;

sex: β =-26.5; side-by-sex interaction: β =1.98; p = 0.048; rater: β _{0,1}=-52.6/ β _{0,2}=-39.3, p<0.001; age:p = 0.48).

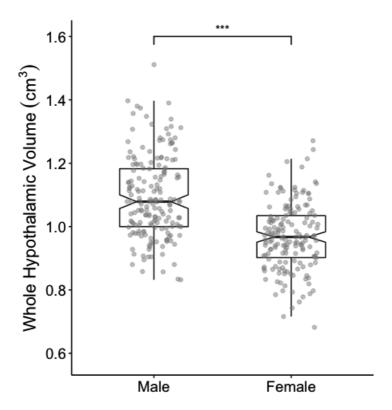


Figure 2: Sex differences in hypothalamic volume. Analysis of hypothalamic volume reveals bigger values for male than for female participants (p < 0.001).

Obesity and hypothalamic microstructure

Next, we examined average MD within the individual's hypothalamus using DWI as a sensitive measure of microstructural properties (Alexander et al., 2007; Den Heijer et al., 2012). A carefully designed processing pipeline ensured that DWI-related distortions adjacent to the hypothalamus region did not bias hypothalamic MD estimates (**Fig. 1B**, see **Methods** for details). This led to exclusion of 27 images not passing quality control resulting in a sample of 311 participants with average MD within the hypothalamus. According to linear regression, BMI significantly predicted hypothalamic MD (β = 0.14, p = 0.008), showing that higher BMI was related to higher MD (**Fig. 3A**). The regression model ($F_{4,306}$ = 24.5, p < .001, R^2 = 0.23) adjusted for

potential effects of sex (β = -0.19, p < 0.001), age (β = 0.38, p < 0.001), and rater (n.s., p = 0.67). Men had larger MD than women and higher age was linked to higher MD. Adding BMI as predictor explained 1.5% more variance in hypothalamic MD than a model without BMI ($F_{1,306}$ = 7.1, p = 0.008). To test the specificity of our findings, we added MD within the hippocampus as another heterogenous subcortical structure to the model, which did not attenuate the predictive association of BMI and hypothalamic MD. The same was true when adding the volume of the 3rd ventricle as covariate to the model, to account for partial volume effects.

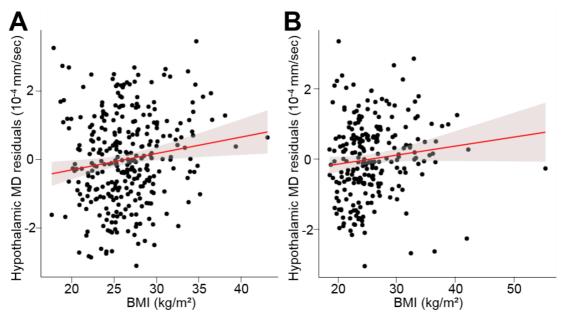


Figure 3: Obesity and hypothalamic microstructure. Higher body mass index (BMI) significantly predicts higher hypothalamic mean diffusivity (MD), commonly interpreted as less intact cellular microstructure, in a first ($\bf A$, n = 311, comparison to age, sexcorrected model, $F_{1,306}$ = 7.1, p = 0.008) and a second independent sample ($\bf B$, n = 236, comparison to age, sex-corrected model, $F_{1,232}$ = 4.2, p = 0.041). Line indicates regression fit with 95% confidence interval.

Replication analyses

To validate our findings in an independent sample, we developed a novel multi-label fusion atlas based on the initial segmentations that automatically generates individual hypothalamic segmentations (**Fig. 4**). Evaluation of this fully automated atlas-approach revealed acceptable reliability (see **Methods** for details).

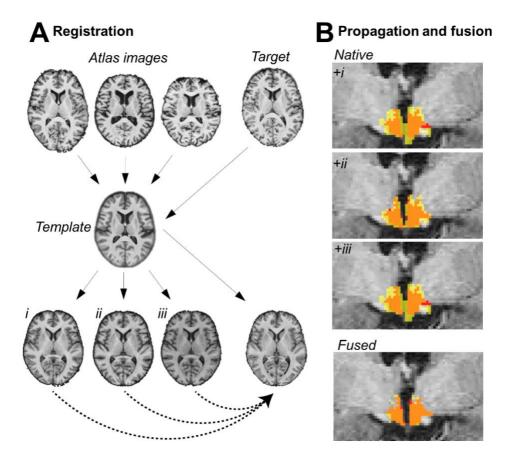


Figure 4: Multi-atlas fusion segmentation for automated hypothalamus segmentation. A: In the registration step both atlas and target images were nonlinearly registered to a template image. In this common space another non-linear registration of atlas images to the target image was performed. **B**: In the label propagation step all transformations were concatenated and the atlas hypothalami were brought into the native space of the target image (upper images). Fusion of the region of interest was performed using STEPS (lower image, see **Methods** for details).

Using this atlas approach in a second group of 236 participants confirmed a significant association between higher BMI and higher hypothalamus MD in similar magnitude (β = 0.14, p = 0.04, **Fig. 3B**; regression model: F_{3,232} = 15.5, p < .001, R² = 0.41), adjusted for age (β = 0.37, p < 0.001) and sex (β = -0.12, p = 0.04). Changes in F-values confirmed that adding BMI increased the explained variance of hypothalamic MD significantly by 1.5% (F_{1,232} = 4.2 p = 0.04). Similar to the initial sample, when adding hippocampal MD and ventricular volume to the model, BMI remained a significant predictor of hypothalamic MD. Furthermore, consideration of obesity-associated biomarkers (systolic blood pressure and HOMA-IR) as possible

confounders did also not attenuate the positive association between BMI and

hypothalamic MD.

Exploratory analysis of visceral fat

To explore whether visceral obesity explained additional variance in hypothalamic MD,

we added log-transformed height-corrected VAT as an additional predictor into the

regression model ($F_{5,300} = 19.8$, p < .001, $R^2 = 0.24$). VAT was estimated from T1-

weighted abdominal MRI in a subset of the initial sample (n = 306, see **Methods** for

details). Controlling for the impact of age ($\beta = 0.37$, p < 0.001), sex ($\beta = -0.17$, p <

0.001), rater (p = 0.658) and BMI (p = 0.132), we did not find significant associations

for VAT ($F_{1,300} = 0.5$, p = 0.5) and average hypothalamic MD.

Discussion

Using multimodal neuroimaging in two large samples of healthy adults, we showed

that higher BMI is associated with higher proton diffusivity in the hypothalamus,

indicating hypothalamic microstructural alterations in obesity. In parallel, while men

had higher hypothalamus volumes than women and the volume of the left hemispheric

hypothalamus was larger than the right, BMI was not associated with hypothalamic

volume.

Hypothalamic microstructure and obesity

Our findings provide first evidence that higher BMI is associated with higher MD in the

hypothalamus, based on a novel, tailored approach to assess advanced DWI-derived

markers of microstructure in this small diencephalic brain region in a large human

cohort. While the effect size is to be considered small explaining 1.5% of the variance

in hypothalamus MD, we replicated our findings in another large independent sample.

Further arguments for the robustness and specificity of our findings stem from

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covariate adjustments for age, sex and other potential confounders. Particularly, considering hippocampal MD, HOMA-IR and systolic blood pressure in our statistical analysis did not attenuate the association between obesity and hypothalamic MD in our validation sample. Therefore, we conclude that changes in hypothalamic diffusion metrics are likely to specifically relate to obesity itself rather than to associated comorbidities such as insulin resistance and hypertension, and that the effects are region-specific.

Our result is in line with and extends previous animal and human studies reporting obesity-related alterations in hypothalamic microstructure assessed with DWI (animals) or T2*-weighted imaging (humans), though previous human studies were based on limited sample sizes and less established markers of microstructure(Kreutzer et al., 2017; Lee et al., 2013; Puig et al., 2015; Thaler et al., 2011). In contrast, MD in grey matter regions is thought to reflect the amount, density or integrity of neuronal membranes, dendrites, axons, or glial compartments, that restrict water diffusion in the tissue in both animals and humans (Alexander et al., 2007; Assaf, 2018; Kreutzer et al., 2017), and previous work showed that higher MD for example in the hippocampus correlated with poorer memory function (Den Heijer et al., 2012). This might indicate that obesity-associated higher MD in the hypothalamus goes along with microstructural changes that could lead to dysfunctional outcomes. We also found higher values of hypothalamic MD in men than in women as well as an age-related increase in MD. The latter is supported by a broad range of studies that consistently found positive associations between diffusion metrics (such as MD and FA) and age in various GM structures, often in line with worse cognitive performance (Kerti et al., 2013; Pfefferbaum, Adalsteinsson, Rohlfing, & Sullivan, 2010).

Yet, despite of being able to detect alterations on a cellular level, DTI metrics such as MD suffer from non-specificity and are confounded by tissue geometry. Accordingly,

MD has been linked to various neurological disorders as well as to unspecific cerebral

abnormalities such as edema, necrosis, demyelination or augmented cellularity

(Alexander et al., 2007). Therefore, various underlying mechanisms might explain the

obesity-associated increases in hypothalamic MD in our study.

First, as discussed in the concept of hypothalamic inflammation, changes in MD might

be attributed to a sustained gliosis as a consequence of diet-induced obesity. This is

supported by findings in mice showing that microgliosis and astrocytosis returned

permanently in mice fed a HFD, although temporarily subsiding (Thaler et al., 2011).

In addition, another study suggested microglial responses due to ongoing malnutrition

in humans as they also detected signs of gliosis and microglial dystrophy in human

hypothalamus assessed by post mortem stereology (Baufeld et al., 2016).

Second, hypothalamic inflammation in mice is also linked to a loss of hypothalamic

neurons that underwent apoptosis as a consequence of the HFD (Moraes et al., 2009).

Therefore, the observed diffusion alteration might also be due to an enhanced amount

of extracellular fluid that is accompanied by the neuronal loss or the neuroinflammation

in general (Pasternak, Kubicki, & Shenton, 2016).

Another possible explanation for the increase in MD addresses vessel integrity, as it

has been shown that HFD triggers hypothalamic angiopathy in mice with increased

vessel density and length (Yi et al., 2012). Currently, new approaches are underway

that aim to disentangle the changes in diffusion metrics driven by blood perfusion from

them originating from the extracellular space (Rydhög et al., 2017).

Taken together, MD was positively associated with BMI in two large samples. While

this suggests small, but reliable alterations in the hypothalamic microstructure in obese

humans, the underlying histological mechanisms remain elusive. We encourage future

studies to link our neuroimaging findings with advanced analysis at the cellular level

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(e.g. post-mortem stereology) to further explore the underlying mechanisms.

Hypothalamic volume and its associations with obesity

asymmetry in hypothalamic volume.

Our bilateral estimations of hypothalamic volume yielded comparable results with previous manual or semi-manual protocols in smaller samples, indicating that whole hypothalamic volume assessed by neuroimaging techniques is around 1 cm³ (Schindler et al., 2013). Results of our regression analysis suggested that hypothalamic volumes are higher for males compared to females, irrespective of age and BMI. This finding might be attributable to known sex differences in metabolic dysregulation (Ha, Cohen, Tirsi, & Convit, 2013) and the neuroendocrine regulation system (Chowen, Argente-Arizón, Freire-Regatillo, & Argente, 2018). Furthermore, we found a significant left-right asymmetry in hypothalamic volume with higher volumes for the left than for the right hypothalamus, which is in line with a previous publication that described a trend in the same direction in a sample of 84 subjects (Wolff et al., 2018). Along these lines, some hypothalamic functions have been described as lateralized to the left (Toth et al., 2014). Recent studies also suggest the lateral hypothalamus to be involved in a lateralized brain circuit that mediates feeding behavior and homeostatic regulation (Castro, Cole, & Berridge, 2015). Future studies need to explore whether these processes might also contribute to volumetric

We did not find a significant relationship between hypothalamic volume and BMI, controlling for the impact of age, sex and the different raters. Although a wide range of literature demonstrate that higher BMI is associated with lower GM volumes in various brain regions (García-García et al., 2018), to date there is no evidence for significant changes in hypothalamic volumes associated with obesity. Nevertheless, BMI has been shown to be related to functional alterations in several brain circuits that involve the hypothalamus (Stephanie Kullmann et al., 2014). Interestingly, while age-related

atrophy in various subcortical structures is commonly observed (Raz & Rodrigue, 2006), age was not related to hypothalamic volume in the present cohort..

Methodological considerations

Results of previous protocols using MRI to reveal alterations in hypothalamic volume consistently stress the difficulty to judge its boundaries, especially with regard to the lateral and superior border (Gabery et al., 2015; Schindler et al., 2013). Likewise, it has been argued that the hypothalamic edges applied in histological approaches such as post mortem stereology do not necessarily need to be appropriate landmarks for neuroimaging approaches (Gabery et al., 2015). Additionally, the applicability of neuroanatomical landmarks for the segmentation of subcortical structures also strongly depends on the spatial resolution (this is, the magnetic field strength) and the quality of the MRI images (Keuken, Isaacs, Trampel, van der Zwaag, & Forstmann, 2018). Especially image artifacts (e.g. due to head motion) impact the quality of neuroimaging data from small brain structures such as the hypothalamus (Goldstein et al., 2007; Stephanie Kullmann et al., 2014; Schönknecht et al., 2013). Given that hypothalamic volumetry is challenging, we decided to carefully implement a combination of manually setting landmarks with grey matter probability-based thresholding (Wolff et al., 2018). This approach enabled us to successfully determine whole hypothalamic volume on 3T MRI in a total of 338 participants, which is the largest sample of hypothalamic volumes obtained by semi-automated segmentation to date. Reliability analysis in 20 subjects revealed acceptable to excellent intra-rater and interrater reliabilities of hypothalamus volume and spatial overlap of resulting masks, ranging from 93% to 96% within each rater and from 88% to 89% between the two raters (Supplementary Table 1). These encouraging results highlight the sensitivity and specificity of our procedure and compare to previous high-quality segmentation

protocols implemented in smaller sample sizes (Bocchetta et al., 2015; Gabery et al.,

2015; Schönknecht et al., 2013). However, due to its small size and the

aforementioned methodological constraints, absolute hypothalamic volume should be

interpreted with caution. As a consequence, subsequent analysis should consistently

consider potential bias introduced by diverging judgements of the different raters as a

possible confounder.

Evaluation of the multi-atlas label segmentation

We showed that multi-atlas label segmentation could reliably estimate hypothalamic

MD in an automated fashion, leading to a confirmation of our results in an independent

sample with a different measurement technique. For hypothalamus MD, we saw good

to excellent reliability (ICC > 0.87) between the semi-automated and the fully-

automated segmentation procedures. This suggests that the accuracy of the

automated segmentation, combined with a carefully designed co-registration, is

sufficient to reliably assess hypothalamus MD. Regarding the anatomical images, we

found high spatial overlap (DSC > 0.8), but only moderate reliability for the volume

estimates (ICC $\sim 0.55 - 0.73$). This result was similar to the inter-rater comparison in

the semi-automated segmentation and underline that absolute volumetric measures of

small structures such as the hypothalamus should be interpreted with caution.

Limitations and strengths

Some further limitations need to be taken into consideration. As our dataset is cross-

sectional, we cannot infer causality. Altered hypothalamic microstructure might be

attributable to both, prerequisite or consequence, of obesity. Furthermore, even if

referring to established concepts such as hypothalamic inflammation, knowledge

about the temporal dynamics of this inflammatory process is scarce or inconsistent

(Baufeld et al., 2016).

Also, hypothalamus physiological function is not restricted to energy metabolism and

homeostasis. There are further nuclei serving as main hubs in the control of fluid

balance, circadian rhythms or thermoregulation (Lizarbe, Benitez, et al., 2013), which

might have contributed to the MD signal. In addition, the usage of BMI to characterize

obesity might be too simplistic (Shuster et al., 2012). However, our results

incorporating MRI-based measures of VAT, indicative of visceral obesity, strongly

indicate that VAT did not improve the model fit with regard to microstructural changes

within the hypothalamus. Strengths of our study include the large, well-characterized

population-based sample size, a thorough methodological design combining a semi-

automated segmentation algorithm with sensitive DWI metrics, along with replication

analysis in an independent sample.

Conclusion

Using a novel multimodal MRI approach in two large samples of healthy adults of the

general population, we were able to demonstrate that a higher BMI specifically relates

to higher MD in the hypothalamus, independent from confounders such as age, sex

and obesity-associated co-morbidities. This finding thus points to persisting

microstructural alterations in a key regulatory area of energy homeostasis occurring

with excessive weight. The underlying mechanisms might include inflammatory

activity, neuronal degeneration or angiopathy in the hypothalamus due to obesity-

related overnutrition and metabolic alterations. Future studies need to test the

functional relevance of these microstructural changes, and if interventions aiming to

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reduce obesity can effectively reverse the observed changes in hypothalamic MD.

Materials and Methods

Participants

Participants were recruited randomly as part of the MRI-subsample within the "Health Study for the Leipzig Research Centre for Civilization Diseases" (LIFE-Adult) study (Loeffler et al., 2015). The study was approved by the Ethics Committee of the University of Leipzig and all participants gave informed written consent. In total, 2637 adults received brain MRI. We selected participants without history of stroke, cancer, epilepsy, multiple sclerosis and Parkinson's disease, neuroradiological findings of brain pathology or intake of centrally active medication (n = 2095). Further, only a well-characterized subgroup with abdominal MRI was considered (n = 993).

Two raters begun the segmentation and continued until rater 1/2 had segmented the hypothalamus of 166/152 participants, respectively. For test-retest and interrater-reliability both raters additionally segmented 20 participants twice. In total, bilateral hypothalami were segmented in n = 338 participants (for demographic characteristics, see Table 1). 27 participants had to be removed from further analysis due to incomplete or deficient diffusion imaging data (**Supplementary Figure 1**).

Table 1: Demographic characteristics of the segmentation sample. Data is given as mean \pm standard deviation (SD) and range (minimum – maximum).

n (females/males)	338 (162/176)
Age (years)	$55.03 \pm 12.36 (21 - 78)$
BMI (kg/m²)	$26.41 \pm 3.92 (17.68 - 43.09)$
VAT ¹ (cm ³)	2355.92 ± 1421.42 (232.76 – 7584.29)

 $^{^{1}}$ n = 331 due to missing values of VAT.

BMI: body mass index, VAT: visceral adipose tissue

Anthropometry

Body weight was measured with a scale with a precision of 0.01kg and body height

was assessed using the means of a stadiometer to the nearest 0.1cm. BMI was

calculated as body weight [kg] divided by squared body height [m].

Waist and hip circumference were taken with an ergonomic measuring tape (SECA

201) to the nearest 0.1cm. Waist-to-hip ratio was then calculated.

Obesity-related biomarkers

We collected additional obesity-related biomarkers in a subset of participants.

Laboratory indicators of glucose metabolism (glucose and insulin) were obtained after

overnight fasting according to standard procedures (Loeffler et al., 2015) and used to

calculate insulin resistance with the homeostatic model assessment (HOMA-IR)

(Matthews et al., 1985). Blood pressure was measured with an automatic oscillometric

blood pressure monitor (OMRON 705IT, OMRON Medizintechnik Handelsgesellschaft

mbH).

Magnetic Resonance Imaging

Magnetic resonance imaging (MRI) was performed on a 3T Magnetom Verio scanner

(Siemens, Erlangen, Germany, equipped with a 32-channel head array coil and syngo

MR B17 software).

Abdominal MRI acquisition and preprocessing:

MRI of the abdomen was performed using an axial T1-weighted fast spin-echo

technique with the following parameters: repetition time, 520 ms; echo time, 18 ms;; 5-

mm gap between slicefield of view, 500 mm \times 375 mm; final voxel size 1.6 \times 1.6 \times 5.0

mm³. Beginning 10 cm below the umbilicus, 5 slices were recorded from feet-to-head

direction with 5 cm table shift after each acquisition and finishing in the liver region(Loeffler et al., 2015). Using a semi-automated segmentation algorithm implemented in ImageJ (https://imagej.nih.gov/ij/download/), visceral adipose tissue (VAT) was obtained from 20 slices centered around the participant's umbilicus (Raschpichler et al., 2013). For subsequent analysis, the VAT volume was log-

Head MRI acquisition and preprocessing:

transformed and normalized by height.

Anatomical MRI was acquired using a T1-weighted Magnetization prepared rapid gradient echo (MPRAGE) pulse sequence with the following parameters: inversion time, 900 ms; repetition time, 2.3 ms; echo time, 2.98 ms; flip angle, 98;; image matrix, $256 \times 176 \times 240$; voxel size, $1 \times 1 \times 1$ mm³.

Preprocessing of the anatomical T1-weighted data included skullstripping and realignment to anterior and posterior commissure in Lipsia (https://www.cbs.mpg.de/institute/software/lipsia/download). Then, tissue segmentation was performed with the default settings using SPM12's New Segment based on Matlab version 2017b.

Diffusion weighted imaging was acquired with a double-spin echo planar imaging sequence (EPI) with the following parameters: repetition time, 13800 ms; echo time, 100 ms;; image matrix 128 \times 128; 72 slices; voxel size 1.7 \times 1.7 \times 1.7 mm³; maximum b-value 1000 s/mm², and 7 volumes with b-value 0s/ mm².

Preprocessing included denoising (MRtrix v3.0) of the raw data removal of gibbs-ringing artifact from all b0 images using the local subvoxel-shift method and outlier replacement using the eddy tool in FSL 5.0.10 (Andersson, Graham, Zsoldos, & Sotiropoulos, 2016a, 2016b; Kellner, Dhital, Kiselev, & Reisert, 2016; Veraart et al., 2016). Subsequently, data was corrected for head motion and linearly coregistered to theT1 image with Lipsia tools. Finally, we applied tensor model fitting and generated

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MD and FA images.

Segmentation of the Hypothalamus

Based on previous protocols for 3T MRI data, we performed semi-automated

segmentation of the hypothalamus in MeVisLab 4.1. (Wolff et al., 2018).

We predefined four different regions of interest (ROI) to evaluate hypothalamic volume.

Due to some false-positive segmentation results of intraventricular voxels with the

original approach, we adapted the medial landmarks according to Mai, Majtanik &

Paxinos (2015).

First, semi-automated segmentation comprised a manual delineation of each ROI

based on the neuroanatomical landmarks in the T1-weighted anatomical scans (Fig.

1A). Grey matter tissue probability masks were overlaid to facilitate a proper and

comparable segmentation. Having defined the boundaries of each ROI, MeVisLab

computed three-dimensional volume of the hypothalamus taking into account

predefined grey matter thresholds. Subsequently, each rater checked the results

carefully in a triplanar view with regard to plausibility and coherence to the predefined

anatomical edges.

The segmentation procedure was conducted separately for left and right hypothalamus

and took between 30 and 45 minutes per brain. After six months of segmentation we

finished the volumetry. Hypothalamic volumes were assessed by extracting the

number of voxels for each side. Whole hypothalamic volume was calculated by

summing up volumes of left and right hypothalamus. As subcortical volumes are

trivially linked to total intracranial volume, hypothalamic volume was adjusted using the

following formula (Voevodskaya, 2014):

 $Hypothalamus\ volume_{adjusted,i} = Hypothalamus\ volume_{raw,i} - \beta(ICV_{raw,i} - ICV_{mean})$

where ICV is the total intracranial volume and β is the unstandardized slope of the

regression model between ICV and the whole hypothalamic volume across

participants. As nonparametric Shapiro-Wilk test indicated a non-normal distribution of

the adjusted hypothalamic volumes, we log-transformed volumetric data.

Reliability analysis of the segmentation algorithm

Two different raters applied the semi-automated segmentation algorithm. 20 additional

subjects were chosen to perform intra- and interrater reliability analysis. We ensured

that reliability subjects were comparable to the whole segmentation sample with

respect to age, sex and BMI. Each rater segmented each of these subjects twice.

According to Shrout & Fleiss (1979), intraclass correlation coefficients (ICC) were

calculated using model 1,1 and 3,1. We considered an ICC ≥ 0.9 excellent,

 $0.9 > ICC \ge 0.8$ good and $0.8 > ICC \ge 0.7$ acceptable (Perlaki et al., 2017). Additionally,

percentage of relative overlap between the two raters was assessed using Dice

similarity coefficient (DSC)(Dice, 1945). An overlap of 70, 80 or 90% (DSC = 0.7, 0.8,

0.9) was regarded acceptable, good and excellent, respectively.

For the statistical analysis, we considered rater as a variable with three levels: rater 1,

rater 2 and "rater1/2". For these 20 reliability subjects, we used the average of the two

measurements by the two raters.

Extraction of the hypothalamus mean diffusivity

To gain insights into hypothalamic microstructure, we used MD which reflects the

overall amount of diffusion in a certain voxel and averaged this measure in the

hypothalamic volume. FA images of all subjects with hypothalamic volumetry were

coregistered to the respective anatomical images with FSL's FLIRT using 6 degrees

of freedom. Then, the registration matrix was used to coregister the MD images to the

anatomical space (Fig. 1B). 24 participants did not receive diffusion weighted imaging

or had incomplete data. Furthermore, coregistration failed in 3 subjects (see Fig. 4).

Due to its small size, minor shifts or artifacts within the overlay of hypothalamus and

the MD mask might be detrimental for analysis, especially for hypothalamic and non-

hypothalamic voxels adjacent to the third ventricle (Fig. 1B). In order to avoid that

intraventricular voxels were regarded as hypothalamic tissue, further processing was

required to distinguish these voxels from those in hypothalamic tissue with regard to

MD. Consequently, we derived the average MD in the third ventricle based on the

automatic segmentation in FreeSurfer version 5.3.0. Suggesting that grey matter

(hypothalamus) MD is smaller than MD in CSF (third ventricle)(S. Kullmann,

Schweizer, Veit, Fritsche, & Preissl, 2015), average MD of the whole third ventricle

was chosen as a threshold for the hypothalamic MD. Specifically, the MD value of

each putative hypothalamic voxel was compared to the average MD of the whole third

ventricle. Unless MD of each voxel was higher than the average MD of the third

ventricle, this voxel was considered hypothalamic. Results were manually

crosschecked. Finally, average MD of all voxels that were likely to be hypothalamic

tissue was extracted.

Statistical analysis of hypothalamic volume and diffusion

R version 3.2.3 was used to perform statistical analysis.

BMI-related differences in whole hypothalamic volume and MD were assessed by two

groups of regression models. For both hypothalamic volume and MD, we compared

the null model (including age, sex and rater as predictors) against a regression model

including BMI as an additional predictor. The difference between the model was

assessed using a F-test and a p-value < .05 was regarded as statistically significant.

To test the specificity of the finding and exclude confounding of ventricular volume, we

additionally tested a model including the MD of the hippocampus and the ventricular

volume as predictors (Den Heijer et al., 2012).

Hemispheric and sex differences of hypothalamic volume were evaluated in a linear

mixed model which included a side-by-sex interaction, rater and age as predictors and

subject as a random factor. We report β estimates and p-values based on likelihood

ratio tests-based for the fixed main and interaction effects.

Multi-atlas fusion segmentation

For the automated multi-label fusion segmentation procedure, we first created a study-

specific template. We used n = 150 randomly selected participants with manual

segmentations of the hypothalamus. This sub-sample did not differ from the final

sample (n = 338) in age, sex, BMI or rater distribution (all p > 0.05) (Supplementary

Table 4).

To create the template, we applied the function buildtemplateparallel.sh implemented

in ANTS version 2.2.0 (Avants et al., 2011). For more details on the code see publicly

available scripts (https://edmond.mpdl.mpg.de/imeji/collection/wLm6DPKVY7 ylzyz).

We then implemented a multi-atlas label fusion based on an intermediate template in

nipype (for details, see Supplementary information) (Dewey, Carass, Blitz, & Prince,

2017; Gorgolewski et al., 2011; Jorge Cardoso et al., 2013).

Finally, we extracted the volume of the resulting hypothalamus segmentation and the

ventricle-thresholded average MD values. We validated this approach in two samples.

First, we performed the multi-label fusion segmentation for each of the 44 participants

from the template sample. We compared estimated hypothalamic volumes and MD

with the values derived from the manual segmentation using ICC (model 3,1) and DSC.

In this sample, three participants could not be included for the analysis of MD due to

deficient DWI preprocessing.

In the second validation, we aimed to test whether the automated segmentation would

perform equally well in participants who were not included into the template. Therefore,

we randomly selected 24 participants with manual segmentations who were not part

of the n = 150 template sample. The 44 participants from the first sample were used

as atlas inputs, and we again calculated DSC and ICC to compare the manual and

automated segmentation approaches.

After validation, we moved on to perform automated multi-atlas based segmentation

of the hypothalamus in another n = 236 participants from our cohort with complete

information on primary covariates, laboratory parameters, diffusion-weighted MRI etc.

Again, the 44 participants were used as atlas inputs.

We extracted mean MD from the automatically segmented hypothalami and repeated

the multiple regression analysis with age, sex and BMI as predictors. Likewise, we

considered hippocampal MD and third ventricular volume as possible confounders.

Additionally, since this sample had complete measures of blood pressure, glucose and

insulin, we included HOMA-IR and systolic blood pressure into the regression model.

Validation of the multi-label fusion segmentation

For both the template and the validation sample, we received low to acceptable ICCs

(model 3,1) for the volumetric agreement between automatically segmented and

manually segmented hypothalamus. Similar to the inter-rater comparison, the DSC

between the automatically and manually segmented hypothalami were good with

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average values across participants of > 0.8 (Supplementary Table 2).

Regarding the MD, we reported good to excellent ICC between the values based on automatically segmented and manually segmented hypothalamic (Supplementary Table 3). In the validation sample 2 the ICC dropped slightly in the left compared to the right hemisphere but remained in the good range (ICC = 0.87).

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Supplementary information

Details about the multi-atlas fusion segmentation:

The algorithm included three main steps: First, the atlas images were non-linearly

coregistered to the study-specific template using antsRegistration. The registration

included a rigid-body transform, an affine transform and the non-linear 'SyN'

registration step with four resolution levels. For exact settings of the parameters, see

publicly available scripts. With the same command, the target image was non-linearly

registered to the study-specific template. In a third step, an additional quick registration

between the atlas images and the target image in the template space was performed.

The quick registration used the same parameters as the full registration, but it excluded

the fourth resolution level (Fig. 4).

All transforms were concatenated and applied in a single registration step to the

hypothalami of the atlas images using antsApplyTransforms. This step yielded multiple

labels of the hypothalamus in the target native space.

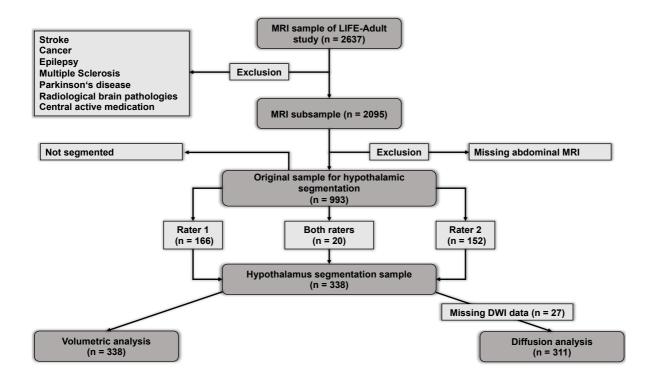
To fuse these labels, we applied STEPS (Similarity and Truth Estimation for

Propagated Segmentations) implemented in NiftySeg (https://github.com/KCL-

BMEIS/NiftySegSTEPS) which generated one multi-atlas based hypothalamic

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segmentation per target image.



Supplementary Figure 1: Flowchart of the study illustrating the exclusion criteria, the subsample sizes and the different approaches of data analysis.

Supplementary Table 1: Measures of intra-rater, inter-rater reliability and spatial overlap for left and right hypothalamus (n = 20)

	Left Hypothalamus		Right Hypothalamus	
	ICC ^a	<u>DSC</u>	ICC ^a	<u>DSC</u>
Rater				
Rater 1	.73	.93	.82	.94
Rater 2	.95	.96	.89	.96
Rater 1 – Rater 2	.83	.88	.88	.89

ICC: Intra-class correlation coefficient, DSC: Dice similarity coefficient

^a ICC (1,1) was used to assess agreement within each rater, whereas ICC (3,1) was used to assess agreement between both raters

Supplementary Table 2: Inter-rater reliability and percentage of overlap for left and right hypothalamic volume between the semi-automated segmentation sample and the two different multi-label fusion segmentation samples.

	Left Hypothalamus		Right Hypothalamus	
	ICC ^a	<u>DSC</u>	ICC ^a	DSC
Rater				
Validation 1 (atlas) (n = 44)	.62	.85	.55	.86
Validation 2 (n = 24)	.67	.85	.73	.85

ICC: Intra-class correlation coefficient, DSC: Dice similarity coefficient ^a ICC (3,1) was used to assess agreement between both approaches

Supplementary Table 3: Inter-rater reliability and percentage of overlap for left and right hypothalamic MD between the semi-automated segmentation sample and the two different multi-label fusion segmentation samples.

	Left Hypothalamus	Right Hypothalamus	
	<u>ICC</u> ^a	ICC ^a	
Rater			
Validation 1 (atlas) (n = 44)	0.97	0.98	
Validation 2 (n = 24)	0.87	0.97	

ICC: Intra-class correlation coefficient, DSC: Dice similarity coefficient

^a ICC (3,1) was used to assess agreement between both approaches

Supplementary Table 4: Group characteristics of the samples used for multi-atlas fusion segmentation. Data is given as mean ± standard deviation and range (minimum – maximum).

	Semi-	Study-	Validation 1	Validation 2
	automated	specific	(atlas)	
		template		
	n = 338	n = 150	n = 44	n = 24
Age (years)	55.0 ± 12.4	55.1 ± 12.4	56.3 ± 10.8	59.2 ± 10.9
	(21 – 78)	(21 – 78)	(34 – 76)	(40 – 78)
Sex (males/females)	176/162	76/74	24/20	15/9
Rater (1/2/both)	166/152/20	73/69/8	21/19/4	11/9/4
BMI (kg/m²)	26.4 ± 3.9	26.6 ± 3.8	26.8 ± 3.8	25.9 ± 2.8
	(18 – 43)	(18-37)	(20 – 37)	(20 – 30)
RMI: hody mass index				

BMI: body mass index