

Nuclear deformation and anchorage defect induced by DCM mutants in lamin A

Manindra Bera^{1,3¶}, Rinku Kumar^{2¶}, Bidisha Sinha² and Kaushik Sengupta^{1,4*}

2 Department of Biological Sciences, Indian Institute of Science Education and Research Kolkata, Mohanpur-741246, India

1. Biophysics & Structural Genomics Division, Saha Institute of Nuclear physics, Kolkata-700064, India

3 Present address: Department of Cell Biology, Yale School of Medicine, New Haven, CT, USA 06510

4 Homi Bhabha National Institute, Mumbai-400094, India

¶ These authors contributed equally and the first author was selected on alphabetical order.

Running title: Nuclear deformations in cardiomyopathic nuclei

Keywords: Deformation; Stress; Cardiomyopathic; Nuclei

*To whom correspondence may be addressed

Kaushik Sengupta

Biophysics & Structural Genomics Division, Saha Institute of Nuclear Physics, 1/AF, Bidhannagar, Kolkata-700064, India,

Phone- 033 2337 5345 (Ext. 3504)

kaushik.sengupta@saha.ac.in

Nuclear deformations in cardiomyopathic nuclei

1 **ABSTRACT**

2 Dilated Cardiomyopathy (DCM) is one of the different types of laminopathies caused by the
3 mutations in A-type lamins in somatic cells. The involuntary cyclic stretching of cardiac
4 muscle cells, as observed in normal physiological conditions is perturbed in DCM which
5 afflict patients globally. As A-type lamins are principal components in nuclear mechanics, we
6 have investigated the effect of the DCM causing mutants- K97E, E161K and R190W on
7 nuclear stretching and deformation by static and dynamic strain inducing experiments. All
8 the mutants exhibited differential nuclear structural aberrations along with a tilt in the
9 nuclear axis compared to the direction of the cell axis and a significant decrease in the lamina
10 thickness which reflected the lower mechanical rigidity. These phenotypes could potentially
11 lead to defects in nuclear anchorage to the actin filaments thereby resulting in the misshapen
12 and misaligned nucleus.

13

14

15 **INTRODUCTION**

16 Nuclear lamins which are type V intermediate filament proteins were first visualized
17 to form ~50 nm meshwork underlying the inner nuclear membrane (1). It was considered
18 that lamin A forms 10-nm filaments inside the cell (2-5) until recently when this notion has
19 been revised by the cryo-ET structure of vimentin null mouse embryonic fibroblast
20 suggesting that both A- and B-type lamins form tetrameric 3.5 nm thick filaments inside the
21 nucleus (6). Earlier, it was also reported by the structured illumination microscopy that both
22 lamins form distinct meshwork in the nucleoplasm (7). Lamin A is a principal regulator of
23 nuclear mechanics and the relative abundance of the lamin A is dependent on the tissue types
24 and matrix elasticity (8,9). More than 450 mutations have been discovered in the *LMNA* gene
25 (<http://www.umd.be/LMNA/>) which produces almost 16 different types of diseases like
26 Dilated Cardiomyopathy (DCM), Emery-Dreifuss Muscular Dystrophy (EDMD) etc. that are
27 collectively coined as laminopathies (10-12). These are tissue-specific in nature
28 predominantly affecting muscle and adipose tissues. The hallmark of laminopathies is the
29 formation of misshapen and even fragile nuclei (13). Two hypotheses are in vogue to explain
30 the role of mutant lamin A protein in the pathogenesis of laminopathies. The gene regulation

Nuclear deformations in cardiomyopathic nuclei

31 hypothesis correlated the occurrence of aberrant gene expression due to differential
32 transcriptional regulation by lamin A while the structural hypothesis focuses on the
33 perturbation effect of mutant lamin A on higher order assembly of the nuclear lamina leading
34 to fragile nuclei (14,15). Previously, several reports based on AFM indentation, micropipette
35 aspiration and microrheological experiments showed altered nuclear elasticity for lamin A
36 null MEF or cells containing lamin A mutations (16-18). The rapidly growing area of
37 nucleus-cytoskeleton interactions has led to numerous studies involving the
38 transduction of external mechanical cues to the nucleus. Earlier studies revealed that
39 cytoskeleton maintains the nucleus in a pre-stressed state by aligned actin filaments forming
40 a perinuclear actin cap (19-21). Recently, it has been shown for endothelial cells that central
41 and apical stress fibers play distinct mechanical roles in maintaining coordination between
42 the cell and nuclear shapes (20).

43 In this report, we studied the effect of nuclear morphology due to dilated cardiomyopathic
44 mutations (K97E, E161K, and R910W) under different physiological strains. These
45 mutations were selected based on their severities of phenotypes in patients. The phenotype
46 of this disease is characterized by the cardiac arrhythmia with acute conduction defects and
47 myocardial infarction that can lead to sudden death (22). We took two different approaches
48 to observe the effect of the laminopathic mutations (human origin) in the mouse myoblast
49 C2C12. Cells were stretched by applying cyclic strain (dynamic strain) on the PDMS
50 membrane to mimic the physiological state of extension and relaxation of muscle and cardiac
51 cells. Secondly, cells were grown on the different micropatterned surfaces which exert static
52 deformation force (static strain) on the cytoskeleton via cell adhesion molecules (23,24) and
53 ultimately perturbs the lamin A network assembly. In both the cases, we observed
54 differential nuclear deformations, anchorage defect characterized by a tilt in nuclear axis
55 about actin axis and variation in the lamina thickness which suggested a reduction in nuclear
56 rigidity and integrity. These results also suggest a probable explanation behind the
57 formation of elongated and misshapen nuclei in cardiomyopathy caused due to the *LMNA*
58 mutations.

59

60

Nuclear deformations in cardiomyopathic nuclei

61 **RESULTS AND DISCUSSION**

62 **Differential impairment of the nucleo-actin axis on the micropatterned substrate**

63 The actin cytoskeleton is known to mechanically couple with the nuclear lamins through
64 **Linker of Nucleoskeleton and Cytoskeleton (LINC)** complexes (25). We measured the
65 alignment of the nucleus with the cell's orientation vector in cells expressing WT and mutant
66 Lamins A/C. Usually, the orientation vector of the cell reflects closely the orientation of actin
67 stress fibers (26). However, well-spread cells often had random orientations of stress fibers
68 as is evident from cells on non-patterned glass (Fig. 1 A, left). To be able to control this
69 variation, we used substrates in which the adhesion area was patterned by photomasks (Fig.
70 1 A, right). Two rectangular patterns denoted by RA and RB with aspect ratios 3, 2 and spread
71 areas 1200, 450 μm^2 respectively, were chosen. These aspect ratios were chosen based on a
72 similar ratio (1:3) (27) of hPSC-derived monolayers of cardiomyocytes. To quantify the
73 alignment of the nucleus with the cell, the cell and nucleus outlines were fitted with ellipses
74 and the absolute angle between their major axes noted as orientation angle (Fig. 1 B) for cells
75 expressing the GFP tagged versions of lamin A (Fig. 1 C). For perfect alignment of the nucleus
76 with the cell axis, the expected orientation angle is 0° , while for randomly oriented nuclei,
77 the angles are expected to vary from 0° to 90° , therefore averaging at 45° (dashed line, Fig.
78 1 D). As suspected, the non-uniform shapes in non-patterned cells resulted in angles ($\sim 21^\circ$)
79 implying low alignment (Fig. 1 D). There was also no difference in orientation angles in
80 mutant lamins compared to wild type lamin A (denoted by WT) (Fig1 D). However, using
81 micropatterns, we first observed lowered angles ($\sim 10^\circ$) for WT as expected from the
82 uniformity of the shape (Fig. 1 D). Secondly, we found that all mutants exhibited the
83 alignment of nucleus axis to cell axis within the range $24^\circ - 37^\circ$ (Fig. 1 D, Supporting Table1)
84 rendering it closer to the value expected from random orientation (45° , Fig. 1 D, dashed line).
85 However, no particular parameter of nuclear shape (eccentricity, aspect ratio, circularity, -
86 Fig. 1 D) was significantly affected by the mutations. This strongly suggested the lack of
87 nuclear alignment to cell-axis presumably due to a loss of mechanical coupling between the
88 nucleus and cytoplasmic actin network (Fig. 1 D, *top*). Furthermore, we observed the lamin
89 A aggregation inside the nucleoplasm and quantified the size in terms of area. K97E and
90 R190W transfected nuclei showed significantly larger aggregates, ~ 14 and $12 \mu\text{m}^2$

Nuclear deformations in cardiomyopathic nuclei

91 respectively. WT and E161K nuclei showed smaller aggregates compared, ~ 2.5 and $8.3 \mu\text{m}^2$
92 respectively on the RB micropatterned surface. But on the RA pattern, E161K and R190W
93 nuclei produced smaller aggregates compared to RB, ~ 4.6 and $5.5 \mu\text{m}^2$ respectively (shown
94 in Supplementary Fig1). The size of aggregates for WT and K97E were unchanged, ~ 2 and
95 $15 \mu\text{m}^2$ respectively. The aggregate may constitute other subtypes of endogenous lamin also
96 because of its homo- and hetero-polymerization nature but we only monitored GFP-
97 fluorescence of the exogenous lamin A. Since all these experiments were performed by
98 transient transfection, that enhance the possibility of overexpression of protein lead to
99 misfolded protein and aggregation. We ruled out this possibility by measuring the non-
100 significant change in the amount of lamin upon transfection through western blotting
101 (shown in Supplementary Fig 3).

Nuclear deformations after the cell stretching

103 In cardiac muscle tissues, the cells continuously experience the cyclic and uniaxial stretching.
104 Hence, the cells also reorient themselves towards the stretching axis (28,29). Zimmermann
105 et al. stretched neonatal rat heart cells up to 10% at 2 Hz frequency to generate engineered
106 heart tissue (30) and Yu et al. showed that 10% static stretching can insert new sarcomere
107 in the neonatal rat (31). The normal resting heart rate in infant and in the case of tachycardia
108 in adult heart rate can be more than 2 Hz (32,33). We intended to test the impact of chronic
109 mechanical perturbation (cyclic stretching) on lamin A-dependent nuclear morphology by
110 mimicking physiological frequency of extension and relaxation of muscles and cardiac cells. We
111 performed the mechanical stretching experiments on the wild-type (WT) and DCM-causing
112 mutant lamin A transfected C2C12 cells. The cells were grown on the PDMS membrane and
113 the membrane was stretched cyclically up to 10% for 2.5 hr. at a frequency of 2 Hz. We
114 measured how the mutants differed from the WT in shape parameters and orientation of
115 nucleus with and without cyclic stretching. In the absence of cyclic stretch, WT and mutant
116 cells grown on PDMS displayed non-significant differences in most (8/12) parameters
117 except for the observations that R190W was less aligned than WT while E161K resulted in
118 nuclei with higher eccentricity and aspect ratio and lower circularity. However, after cyclic
119 stretch was imparted most (10/12) parameters were found to be different – especially the
120 ones quantifying nuclei shape changes. Eccentricity and aspect ratio of all three mutants
121 increased on stretching in contrast to E161K which showed an increase even in the absence

Nuclear deformations in cardiomyopathic nuclei

122 of stretching. Correspondingly, the circularity of all three mutants decreased on cyclic
123 stretching in contrast to only E161K showing a decrease in the absence of stretching. It must
124 be emphasized that, K97E showed a tendency to deviate from the WT in mechanically
125 unperturbed condition (Fig. 2). On cyclic stretching nuclear deformation of K97E was seen to
126 largest among all mutants. Thus, we quantified alignment of the nucleus with the cell body
127 (orientation angle difference) by employing micropatterning to reduce the initial
128 heterogeneity of cell shape in the population (reduced standard deviation of θ , Supporting
129 Table 1). Here, we could elucidate that lamin A mutations may lead to weaker coupling of the
130 nucleus shape to the cell's shape (Supporting Table 2). Next, we demonstrated that when
131 these mutants undergo mechanical perturbation, they are less resistant to shape changes
132 and therefore underwent deformations, unlike WT nuclei that did not show any significant
133 alteration in nucleus-to-cell alignment or shape on cyclic stretching (Supporting Table 3).
134 We have calculated the meshwork size of lamin A for WT and R190W (Supplementary Fig 2).
135 R190W nuclei dilated lamin A meshwork compared to the WT-nuclei which reflected the
136 lower mechanical rigidity of the nuclei. K97E and E161K nuclei produced lamin A aggregates
137 only.

Reduction in the lamina thickness due to laminopathic mutation

138 Nuclear stiffness is primarily determined by nuclear lamina meshwork. We measured lamina
139 thickness which could be the direct readout of stiffness as reported earlier as well (34). We
140 assessed the impact of laminopathic mutations on nuclear lamina thickening behavior. We
141 also included the effect of spreading as reported earlier that lowering in the spread area
142 reduces the stress fiber driven compression of the nucleus and nuclear volume which in turn
143 reduces physical strain on the nucleus (35). We chose two spread area (RA, 1200 μm^2 and
144 RB, 450 μm^2) which has ~ 3 -fold spread area difference. We measured the lamina thickness
145 by structured illumination microscopy (SIM) whose lateral resolution was calculated to be
146 ~ 120 nm (shown in Supplementary Figure 3). We measured average thickness 0.35 ± 0.03
147 μm of the WT lamina on the RA patterned that reduces to 0.30 ± 0.03 μm on RB surface
148 (shown in Fig. 3 A-D, left) suggesting thickening of the lamina on highly spread cells. We
149 believed that lamina in the low spread area cells is less stiff thereby resulting in the less
150 aligned network and showed lamina softening behavior. On comparing lamina thickness of
151

Nuclear deformations in cardiomyopathic nuclei

152 WT with R190W and E161K transfected nuclei, we observed that the lamina thickness did
153 not alter for wild-type ($\sim 0.3 \pm 0.05 \mu\text{m}$) and R190W ($\sim 0.29 \pm 0.02 \mu\text{m}$), however, E161K
154 mutant lamina ($\sim 0.23 \pm 0.03 \mu\text{m}$) showed significant softening behavior compared to WT on
155 the RB surface (Figure 3D). But on RA, the lamina for both E161K and K97E were not clearly
156 visible and both the nuclei showed a significantly large number of aggregates. All the values
157 are tabulated in the supporting table 3. The effect of the geometrical constraint on the K97E-
158 lamin A transfected nuclei were similar. In both cases (RA & RB) for K97E nuclei, the lamina
159 was not clearly visible and nuclei showed larger aggregates. On the spread cell area (RA), the
160 mechanical strain perturbed the lamin A assembly for the mutant nuclei, hence, lamina
161 thickness was significantly decreased or abolished. This lamina softening behavior might
162 explain the lower mechanical rigidity of the nuclei among the cardiomyopathic patients.

163 **CONCLUSION**

164 In this article, we studied the nuclear deformation and misalignments of the nuclear axis
165 compared to the cell axis under different physiological strain. We chose different DCM
166 causing *LMNA* mutants (K97E, E161K, and R190W) and applied external mechanical strain
167 to mimic the physiological condition. In addition, we measured the variation in lamina
168 thickness which plausibly explained the origin of DCM disease and its severity. We observed
169 all the mutations produced significant nuclear deformations and showed significant
170 misalignments of nuclear axes when cyclic stretching was applied. On different
171 micropatterned surfaces, K97E and E161K nuclei produced significantly large lamin A
172 aggregates. Previously, it was reported that no apparent changes in the nuclear lamina
173 occurred for E161K mutation in heart tissue (36). As similarly overexpressed WT nuclei
174 showed less or no visible aggregates, hence the aggregation in the mutant nuclei was due to
175 the overexpression of the improperly assembled mutants lamin A. Previously, it has also
176 been reported that the perinuclear actin and TAN lines anchor the nucleus in pre-stressed
177 condition and help to maintain its orientation (37) and nesprin-1 (an important LINC
178 partner) also helps in tethering the nucleus to actin in C2C12 cells (38). A plausible
179 explanation for impairment of nucleo-actin axis might be the progressive weakening of
180 lamina at points such that the contact nodes with the actin filaments are abrogated thereby
181 resulting in impairment about the axis of the TAN lines. It is important to note that we had

Nuclear deformations in cardiomyopathic nuclei

182 previously observed bundling behavior in E161K & R190W which lead to misshapen nuclei
183 with reduced viscoelastic properties. But in the case of the K97E, the lamin A network
184 formation was significantly altered which was reflected on the nuclear elasticity (39,40).
185 Therefore, the cell might not respond to the external mechanical cues effectively which in
186 turn can lead to altered cell response. This might be the reason behind significant nuclear
187 deformations under cyclic stretching. Furthermore, we studied the variation in lamina
188 thickness by SIM. The thickness of the lamina is in the range of ~20-50 nm and electron
189 microscopic study revealed that lamina thickness can vary from ~18 nm to 100 nm in human
190 cartilage due to injury(41). Earlier, Schermmelleh et al. showed by 3D-SIM that thickness of
191 the lamin B1 thread is ~100 nm laterally and ~300 nm axially in C2C12 cells (because of its
192 resolution limit) (42). But in our experiments, lamina thickness was detected around ~0.3
193 μm which could be due to both overexpression of lamin A and response to mechanical stress.
194 But within the resolution limits (~120 nm) of our experiments, we confirmed the thickening
195 behavior of lamina. We observed that WT lamina thickness slightly increased on the
196 geometrically constrained surface area. But the mutant nuclei showed drastic effect. We
197 could not detect any rim staining of lamin A on the RA surface for the E161K mutant, instead,
198 they formed larger aggregates in the nucleoplasm. The lamina thickness for the R190W
199 mutant nuclei also decreased when cells were grown on the RB surface. We also observed
200 that the total lamin A expression did not change because of the mutation (Supplementary Fig
201 3). These results suggested that soluble lamin A might get recruited to the lamina in response
202 to an increase in the mechanical strain, but mutant lamin A showed the defect in the lamina
203 assembly. Therefore, R190W nuclei showed less thick lamina and E161K nuclei showed
204 larger lamin A aggregates in the nucleoplasm. Due to mechanical stress, changes in the lamin
205 A structure and the phosphorylation status may lead to a change in the lamina organization
206 (43,44). It is already established that at higher mechanical stress, lamin A accumulates at the
207 nuclear periphery that leads to the increment in nuclear stiffness and at low strain, changes
208 in the phosphorylation status produce more soluble lamin A. Hence, lamin A follows a
209 'mechanostat equilibrium' in the nucleoplasm (45). The change in lamina thickness could be
210 due to the accumulation of the lamin A in the aggregates and the change in the
211 phosphorylation pattern. The increase in WT lamina thickness due to the increase in

Nuclear deformations in cardiomyopathic nuclei

212 mechanical stress suggested that changes in the phosphorylation profiles led to the
213 accumulation of the insoluble lamin A to the envelope. But the mutant nuclei lack this ability
214 leading to improper self-assembly and aggregate formation. Ectopic expression of lamin A in
215 the background of the endogenous lamins can significantly contribute to the nuclear stiffness
216 (46). But the background lamin expression was not sufficient to resist the lamina
217 deformation due to different mechanical strain. The aspect ratio of the micropattern was like
218 the hPSC-derived monolayer of the immature cardiomyocytes. The change in the nuclear
219 organization due to the geometrical constraint might be irreversible in the case of
220 cardiomyocytes which might lead to laminopathies. Based on our experimental findings
221 which we have summarized all the results in Supporting Table 1, 2 and 3. We hereby propose
222 that external mechanical cue can alter lamin A meshwork density significantly in presence
223 of laminopathic mutations; lamina shows stress induced thinning behavior and soluble lamin
224 A forms large insoluble aggregates inside the nucleoplasm. These factors cumulatively affect
225 the nuclear rigidity which alters the nuclear shape and mechanics. A plausible model for
226 occurring of laminopathy diseases due to single-point mutation is shown in **Fig 4**. In all
227 cases, we noticed differential alterations in the nuclear shape and the lamin A meshwork for
228 the DCM mutations. The mutant nuclei produced a severe deformation when exposed to the
229 external mechanical strain. In the physiological state also, we can predict that mutation of
230 lamin A in the tissues which are continuously exposed to the external strain can produce
231 significant damage to the nuclear shape and lamin meshwork. Eventually, that can lead to
232 differential gene expression programme and thereby produce the disease.

233

234

235

236

237

238

239

240

Nuclear deformations in cardiomyopathic nuclei

241 **METHODS**

242 **Site-directed mutagenesis**

243 All the mutations were generated using site-directed mutagenesis methods in EGFP-LA plasmid and
244 the details of the primer are reported in Bhattacharjee et al. (40). The mutations were confirmed by
245 the Sanger sequencing method(47).

246 **Micropatterning glass coverslip**

247 22 x 22 mm glass coverslips were etched in ethanol: acetic acid (19:1) mixture for 30 min, following
248 by ethanol washing and air drying. Dried coverslips were treated with UV Ozone cleaner (Jelight
249 Company, USA) for 5 min and incubated with 0.2 mg/ml PLL-g-PEG (SuSos, Switzerland) solution
250 (prepared in 10 mM HEPES buffer, pH 8.3) for 1 h. Photo-masks (JD, Photo Data, UK) is cleaned with
251 acetone and isopropanol followed by 5 min UV Ozone cleaning. PEG-coated coverslips are attached
252 on the chrome side of already cleaned photo-masks with the help of a drop of water. Excess water
253 was soaked with tissue paper for firm adherence of coverslip to mask. Coverslips attached with
254 photo-mask were illuminated with deep UV for 5 min by placing non-chrome side facing UV lamp.
255 Patterned coverslips were detached by floating into water followed by 45 min incubation in 20 μ l
256 fibronectin solution (Sigma) (25 μ g/ml solution in NaHCO₃, pH 8.6). Finally, patterned coverslips
257 were used for cells seeding.

258 **Transfection and cells seeding**

259 70 % of confluence C2C12 cells were transfected with 3 μ g GFP lamin mutants by lipofection
260 (Lipofectamine 3000, Life Technologies) following manufacturer instructions. Post 16 h of
261 transfection, cells were detached from culture dish using 0.02 % EDTA solution (Calbiochem, USA)
262 prepared in cell culture grade PBS (Sigma). 2 X 10⁵ cells were seeded on each patterned coverslips
263 and unattached cells washed off after 30 using warm media. For cell stretching, 10⁵ cells per 500 μ l
264 culture media on each PDMS sheet were seeded. After transfection, Lamin A expression was checked
265 mouse monoclonal anti-lamin A/C antibody at 1:1000 dilution.

266 **Cell Stretching**

267 Custom made cells stretching device was employed for cell stretching as used earlier (ref). Briefly,
268 Silicon elastomer (SYLGRAD 184, Dow Corning) and the curing agent was mixed in 10:1 proportion,
269 an air bubble was removed by centrifuging 5 min at 3000 rpm. 3 ml mixture was spread over each
270 90 mm dish. Placed vertically to get excess mixture flow away. The dish at this configuration was

Nuclear deformations in cardiomyopathic nuclei

271 baked at 60° C to get 100 µm thick PDMS sheet. PDMS sheet was treated 0.5 mg/ml Sulfo-SANAPAH
272 (Pierce chemicals) under deep UV for 5 min (UVO cleaner, Jelight, Inc., USA), functionalized with
273 fibronectin (25 µg/ml solution in NaHCO₃, pH 8.6 Sigma). Fibronectin functionalized coverslips were
274 mounted and custom builds stretchers, GFP Lamin transfected cells were seeded on 25 x 25 mm area
275 encircled with silicon grease. Cells were grown for 24 h on PDMS loaded stretcher inside the
276 incubator. For cyclic cell stretching, PDMS sheet containing C2C12 cells grown in a well was attached
277 to two motors (Physik Instrumente (PI), GmbH and Co KG) using custom-designed adapters. Cyclic
278 stretching at 2 Hz frequency and 10% amplitude was performed with MATLAB for 2.5 h. Stretching
279 was performed inside the cell-culture incubator.

280 **Cell fixation and microscopy**

281 C2C12 cells either grown on glass or PDMS sheet were fixed using 4% PFA on their respective
282 surfaces for 12 min, following PBS wash. Cells were permeabilization by 0.2 % Triton X-100 solution
283 (Sigma) in PBS, stained with DAPI (2.8 µM, Sigma) and Phalloidin Alexa Fluor 568 (0.35 µM,
284 Molecular probe, Life Technologies) for 2 h at room temperature. Finally, coverslips were mounted
285 on with slides (Sigma) for imaging. In case of cells grown on a PDMS sheet, a number one glass
286 coverslips were first attached on top of the PDS sheet with mounting media (Mowiol, Sigma). The
287 entire stretching device was flipped upside down and captured images using oil objective through
288 the glass. Z-stack (0.5 µm step size) images were captured by Olympus epi-fluorescence microscope
289 (Olympus Corporation Japan) with 100X, 1.49NA objective and sCMOS camera (Orca-Flash 4.0,
290 Hamamatsu Photonics Japan) with pixel size 65 nm.

291 **Nucleus to cell orientation angle difference and nucleus shape parameter extraction**

292 Image analysis was done using software ImageJ/Fiji (<https://imagej.net/Fiji>). Nucleus (GFP lamin)
293 to cell (actin) orientation angle difference was measured in two-parts, first drawing ROI manually on
294 maximum intensity projection image to outline object, second fitting ROI to an ellipse for measuring
295 orientation angle. Major (D1) and minor (D2) axis of the fitted ellipse on the nucleus was used for
296 eccentricity ($\sqrt{1 - \frac{D2^2}{D1^2}}$) and aspect ratio (D1/D2) measurement. Perimeter and area of object
297 (nucleus) outline on maximum intensity projection image were used for circularity ($4\pi \times \frac{Area}{Perimeter^2}$)
298 measurement.

299 **Mesh size and width of the peripheral lamin measurements**

Nuclear deformations in cardiomyopathic nuclei

300 Cells were washed three times with ice-cold 1X PBS (pH 7.4) and fixed with 4% paraformaldehyde.
301 Actin was stained with Alexa-561 conjugated phalloidin (Thermo Fisher Scientific) with 1:1000
302 dilutions. After proper washing with PBS, the coverslips were stained with Vectashield that contained
303 DAPI (Vector Laboratories). The coverslips were sealed with watercolor nail polish. The slides were
304 visualized with NIKON Inverted Research Microscope ECLIPSE TiE with Plan Apo VC 100X oil DIC N2
305 objective/1.40 NA/1.515 RI with a digital 4X zoom. Images were analyzed using Ni Elements AR Ver
306 4.13 and Image J (Fiji). The X-Y resolution of N-SIM was calibrated to 120-150 nm using 20 nm
307 FluoSphere beads (Thermo Scientific, F887) in 580 nm laser. We measured the mesh sizes using the
308 area selection tool of Ni-Elements software, but the lines were drawn considering the FWHM method
309 where lower values were considered as the limit of the sides. To measure the lamina thickness, first
310 nuclear rim staining of lamin A were straightened using Image J and then lines were drawn across
311 the linearized lamina and intensity profiles were plotted. From the intensity profile, FWHM was
312 considered to be the thickness or width of the lamina. The thickness of each nucleus was calculated
313 by averaging 10 randomly chosen line profiles and more than 15 separate nuclei were considered for
314 each condition. Sizes of aggregates were measured using an area selection tool of Ni-Elements. The
315 statistics were generated using Origin Pro 8.5 software.

316 **ACKNOWLEDGMENTS**

317 Authors thank Arikta Biswas for her generous help in the instrument set up.

318 **FUNDING**

319 The authors thank the Department of Atomic Energy and SERB, Department of Science & Technology,
320 India for research Grant and fellowship. B. S. acknowledges the Wellcome Trust DBT-India Alliance
321 (IA/I/13/1/500885) for financial support.

322 **AUTHORS CONTRIBUTION**

323 KSG, BS, MB & RK designed all the experiments. RK & MB performed all the experiments. KSG, MB,
324 RK & BS analyzed the data and wrote the paper. KSG conceived the entire project and responsible for
325 finances related to the project.

326 **COMPETING FINANCIAL INTERESTS**

327 The authors declare no competing financial interests.

328

329

Nuclear deformations in cardiomyopathic nuclei

330 **REFERENCES**

- 331 1. Fawcett, D. W. (1966) On the occurrence of a fibrous lamina on the inner aspect of the nuclear envelope
332 in certain cells of vertebrates. *The American journal of anatomy* **119**, 129-145
- 333 2. Heitlinger, E., Peter, M., Haner, M., Lustig, A., Aebi, U., and Nigg, E. A. (1991) Expression of chicken lamin
334 B2 in *Escherichia coli*: characterization of its structure, assembly, and molecular interactions. *The*
335 *Journal of cell biology* **113**, 485-495
- 336 3. Strelkov, S. V., Kreplak, L., Herrmann, H., and Aebi, U. (2004) Intermediate filament protein structure
337 determination. *Methods in cell biology* **78**, 25-43
- 338 4. Stuurman, N., Heins, S., and Aebi, U. (1998) Nuclear lamins: their structure, assembly, and interactions.
339 *Journal of structural biology* **122**, 42-66
- 340 5. Dechat, T., Pflieger, K., Sengupta, K., Shimi, T., Shumaker, D. K., Solimando, L., and Goldman, R. D.
341 (2008) Nuclear lamins: major factors in the structural organization and function of the nucleus and
342 chromatin. *Genes & development* **22**, 832-853
- 343 6. Turgay, Y., Eibauer, M., Goldman, A. E., Shimi, T., Khayat, M., Ben-Harush, K., Dubrovsky-Gaup, A.,
344 Sapra, K. T., Goldman, R. D., and Medalia, O. (2017) The molecular architecture of lamins in somatic
345 cells. *Nature* **543**, 261-264
- 346 7. Shimi, T., Kittisopikul, M., Tran, J., Goldman, A. E., Adam, S. A., Zheng, Y., Jaqaman, K., and Goldman, R.
347 D. (2015) Structural organization of nuclear lamins A, C, B1, and B2 revealed by superresolution
348 microscopy. *Molecular biology of the cell* **26**, 4075-4086
- 349 8. Swift, J., Ivanovska, I. L., Buxboim, A., Harada, T., Dingal, P. C., Pinter, J., Pajerowski, J. D., Spinler, K. R.,
350 Shin, J. W., Tewari, M., Rehfeldt, F., Speicher, D. W., and Discher, D. E. (2013) Nuclear lamin-A scales
351 with tissue stiffness and enhances matrix-directed differentiation. *Science* **341**, 1240104
- 352 9. Harada, T., Swift, J., Irianto, J., Shin, J. W., Spinler, K. R., Athirasala, A., Diegmiller, R., Dingal, P. C.,
353 Ivanovska, I. L., and Discher, D. E. (2014) Nuclear lamin stiffness is a barrier to 3D migration, but
354 softness can limit survival. *The Journal of cell biology* **204**, 669-682
- 355 10. Capell, B. C., and Collins, F. S. (2006) Human laminopathies: nuclei gone genetically awry. *Nature*
356 *reviews. Genetics* **7**, 940-952
- 357 11. Bonne, G., Mercuri, E., Muchir, A., Urtizberea, A., Becane, H. M., Recan, D., Merlini, L., Wehnert, M., Boor,
358 R., Reuner, U., Vorgerd, M., Wicklein, E. M., Eymard, B., Duboc, D., Penisson-Besnier, I., Cuisset, J. M.,
359 Ferrer, X., Desguerre, I., Lacombe, D., Bushby, K., Pollitt, C., Toniolo, D., Fardeau, M., Schwartz, K., and
360 Muntoni, F. (2000) Clinical and molecular genetic spectrum of autosomal dominant Emery-Dreifuss
361 muscular dystrophy due to mutations of the lamin A/C gene. *Annals of neurology* **48**, 170-180
- 362 12. Raffaele Di Barletta, M., Ricci, E., Galluzzi, G., Tonali, P., Mora, M., Morandi, L., Romorini, A., Voit, T.,
363 Orstavik, K. H., Merlini, L., Trevisan, C., Biancalana, V., Housmanowa-Petrusewicz, I., Bione, S., Ricotti,
364 R., Schwartz, K., Bonne, G., and Toniolo, D. (2000) Different mutations in the LMNA gene cause

Nuclear deformations in cardiomyopathic nuclei

- 365 autosomal dominant and autosomal recessive Emery-Dreifuss muscular dystrophy. *American journal*
366 *of human genetics* **66**, 1407-1412
- 367 13. Ho, C. Y., Jaalouk, D. E., and Lammerding, J. (2013) Novel insights into the disease etiology of
368 laminopathies. *Rare diseases* **1**, e27002
- 369 14. Bertrand, A. T., Chikhaoui, K., Yaou, R. B., and Bonne, G. (2011) Clinical and genetic heterogeneity in
370 laminopathies. *Biochemical Society transactions* **39**, 1687-1692
- 371 15. Worman, H. J., and Bonne, G. (2007) "Laminopathies": a wide spectrum of human diseases.
372 *Experimental cell research* **313**, 2121-2133
- 373 16. Radmacher, M. (2007) Studying the mechanics of cellular processes by atomic force microscopy.
374 *Methods in cell biology* **83**, 347-372
- 375 17. Lammerding, J., Dahl, K. N., Discher, D. E., and Kamm, R. D. (2007) Nuclear mechanics and methods.
376 *Methods in cell biology* **83**, 269-294
- 377 18. Rowat, A. C., Lammerding, J., Herrmann, H., and Aebi, U. (2008) Towards an integrated understanding
378 of the structure and mechanics of the cell nucleus. *BioEssays : news and reviews in molecular, cellular*
379 *and developmental biology* **30**, 226-236
- 380 19. Khatau, S. B., Hale, C. M., Stewart-Hutchinson, P. J., Patel, M. S., Stewart, C. L., Searson, P. C., Hodzic, D.,
381 and Wirtz, D. (2009) A perinuclear actin cap regulates nuclear shape. *Proceedings of the National*
382 *Academy of Sciences of the United States of America* **106**, 19017-19022
- 383 20. Versaevel, M., Grevesse, T., and Gabriele, S. (2012) Spatial coordination between cell and nuclear shape
384 within micropatterned endothelial cells. *Nature communications* **3**, 671
- 385 21. Mazumder, A., Roopa, T., Basu, A., Mahadevan, L., and Shivashankar, G. V. (2008) Dynamics of
386 chromatin decondensation reveals the structural integrity of a mechanically prestressed nucleus.
387 *Biophysical journal* **95**, 3028-3035
- 388 22. Taylor, M. R., Fain, P. R., Sinagra, G., Robinson, M. L., Robertson, A. D., Carniel, E., Di Lenarda, A.,
389 Bohlmeier, T. J., Ferguson, D. A., Brodsky, G. L., Boucek, M. M., Lascor, J., Moss, A. C., Li, W. L., Stetler, G.
390 L., Muntoni, F., Bristow, M. R., Mestroni, L., and Familial Dilated Cardiomyopathy Registry Research, G.
391 (2003) Natural history of dilated cardiomyopathy due to lamin A/C gene mutations. *Journal of the*
392 *American College of Cardiology* **41**, 771-780
- 393 23. Garrison, M. D., McDevitt, T. C., Luginbuhl, R., Giachelli, C. M., Stayton, P., and Ratner, B. D. (2000)
394 Quantitative interrogation of micropatterned biomolecules by surface force microscopy.
395 *Ultramicroscopy* **82**, 193-202
- 396 24. Lehnert, D., Wehrle-Haller, B., David, C., Weiland, U., Ballestrem, C., Imhof, B. A., and Bastmeyer, M.
397 (2004) Cell behaviour on micropatterned substrata: limits of extracellular matrix geometry for
398 spreading and adhesion. *Journal of cell science* **117**, 41-52
- 399 25. Wang, N., Tytell, J. D., and Ingber, D. E. (2009) Mechanotransduction at a distance: mechanically
400 coupling the extracellular matrix with the nucleus. *Nat Rev Mol Cell Biol* **10**, 75-82

Nuclear deformations in cardiomyopathic nuclei

- 401 26. Hatch, E. M., and Hetzer, M. W. (2016) Nuclear envelope rupture is induced by actin-based nucleus
402 confinement. *The Journal of cell biology* **215**, 27-36
- 403 27. Lundy, S. D., Zhu, W. Z., Regnier, M., and Laflamme, M. A. (2013) Structural and functional maturation
404 of cardiomyocytes derived from human pluripotent stem cells. *Stem cells and development* **22**, 1991-
405 2002
- 406 28. Liau, B., Zhang, D., and Bursac, N. (2012) Functional cardiac tissue engineering. *Regenerative medicine*
407 **7**, 187-206
- 408 29. Hirt, M. N., Hansen, A., and Eschenhagen, T. (2014) Cardiac tissue engineering: state of the art.
409 *Circulation research* **114**, 354-367
- 410 30. Zimmermann, W. H., Melnychenko, I., Wasmeier, G., Didie, M., Naito, H., Nixdorff, U., Hess, A., Budinsky,
411 L., Brune, K., Michaelis, B., Dhein, S., Schwoerer, A., Ehmke, H., and Eschenhagen, T. (2006) Engineered
412 heart tissue grafts improve systolic and diastolic function in infarcted rat hearts. *Nature medicine* **12**,
413 452-458
- 414 31. Yu, J. G., and Russell, B. (2005) Cardiomyocyte remodeling and sarcomere addition after uniaxial static
415 strain in vitro. *The journal of histochemistry and cytochemistry : official journal of the Histochemistry*
416 *Society* **53**, 839-844
- 417 32. Fleming, S., Thompson, M., Stevens, R., Heneghan, C., Pluddemann, A., Maconochie, I., Tarassenko, L.,
418 and Mant, D. (2011) Normal ranges of heart rate and respiratory rate in children from birth to 18 years
419 of age: a systematic review of observational studies. *Lancet* **377**, 1011-1018
- 420 33. Pinto, D. S., Ho, K. K., Zimetbaum, P. J., Pedan, A., and Goldberger, A. L. (2003) Sinus versus nonsinus
421 tachycardia in the emergency department: importance of age and heart rate. *BMC cardiovascular*
422 *disorders* **3**, 7
- 423 34. Buxboim, A., Irianto, J., Swift, J., Athirasala, A., Shin, J. W., Rehfeldt, F., and Discher, D. E. (2017)
424 Coordinated increase of nuclear tension and lamin-A with matrix stiffness outcompetes lamin-B
425 receptor that favors soft tissue phenotypes. *Molecular biology of the cell* **28**, 3333-3348
- 426 35. Kim, D. H., Li, B., Si, F., Phillip, J. M., Wirtz, D., and Sun, S. X. (2015) Volume regulation and shape
427 bifurcation in the cell nucleus. *J Cell Sci* **128**, 3375-3385
- 428 36. Mewborn, S. K., Puckelwartz, M. J., Abuisneineh, F., Fahrenbach, J. P., Zhang, Y., MacLeod, H., Dellefave,
429 L., Pytel, P., Selig, S., Labno, C. M., Reddy, K., Singh, H., and McNally, E. (2010) Altered chromosomal
430 positioning, compaction, and gene expression with a lamin A/C gene mutation. *PLoS one* **5**, e14342
- 431 37. Maninova, M., Iwanicki, M. P., and Vomastek, T. (2014) Emerging role for nuclear rotation and
432 orientation in cell migration. *Cell adhesion & migration* **8**, 42-48
- 433 38. Espigat-Georger, A., Dyachuk, V., Chemin, C., Emorine, L., and Merdes, A. (2016) Nuclear alignment in
434 myotubes requires centrosome proteins recruited by nesprin-1. *Journal of cell science* **129**, 4227-4237
- 435 39. Banerjee, A., Rathee, V., Krishnaswamy, R., Bhattacharjee, P., Ray, P., Sood, A. K., and Sengupta, K. (2013)
436 Viscoelastic behavior of human lamin A proteins in the context of dilated cardiomyopathy. *PLoS one* **8**,
437 e83410

Nuclear deformations in cardiomyopathic nuclei

- 438 40. Bhattacharjee, P., Banerjee, A., Banerjee, A., Dasgupta, D., and Sengupta, K. (2013) Structural alterations
439 of Lamin A protein in dilated cardiomyopathy. *Biochemistry* **52**, 4229-4241
- 440 41. Ghadially, F. N., Dick, C. E., and Lalonde, J. M. (1980) Thickening of the nuclear fibrous lamina in injured
441 human semilunar cartilages. *Journal of anatomy* **131**, 717-722
- 442 42. Schermelleh, L., Carlton, P. M., Haase, S., Shao, L., Winoto, L., Kner, P., Burke, B., Cardoso, M. C., Agard,
443 D. A., Gustafsson, M. G., Leonhardt, H., and Sedat, J. W. (2008) Subdiffraction multicolor imaging of the
444 nuclear periphery with 3D structured illumination microscopy. *Science* **320**, 1332-1336
- 445 43. Bera, M., Kotamarthi, H. C., Dutta, S., Ray, A., Ghosh, S., Bhattacharyya, D., Ainaravapu, S. R., and
446 Sengupta, K. (2014) Characterization of unfolding mechanism of human lamin A Ig fold by single-
447 molecule force spectroscopy-implications in EDMD. *Biochemistry* **53**, 7247-7258
- 448 44. Buxboim, A., Swift, J., Irianto, J., Spinler, K. R., Dingal, P. C., Athirasala, A., Kao, Y. R., Cho, S., Harada, T.,
449 Shin, J. W., and Discher, D. E. (2014) Matrix elasticity regulates lamin-A,C phosphorylation and
450 turnover with feedback to actomyosin. *Current biology : CB* **24**, 1909-1917
- 451 45. Osmanagic-Myers, S., Dechat, T., and Foisner, R. (2015) Lamins at the crossroads of mechanosignaling.
452 *Genes & development* **29**, 225-237
- 453 46. Zwerger, M., Jaalouk, D. E., Lombardi, M. L., Isermann, P., Mauermann, M., Dialynas, G., Herrmann, H.,
454 Wallrath, L. L., and Lammerding, J. (2013) Myopathic lamin mutations impair nuclear stability in cells
455 and tissue and disrupt nucleo-cytoskeletal coupling. *Human molecular genetics* **22**, 2335-2349
- 456 47. Sanger, F., and Coulson, A. R. (1975) A rapid method for determining sequences in DNA by primed
457 synthesis with DNA polymerase. *Journal of molecular biology* **94**, 441-448

458

459

460

Nuclear deformations in cardiomyopathic nuclei

FIGURE LEGEND

Figure 1. Lamin A mutations lead to the altered alignment of the nucleus with the cell axis. (A) Schematic representations depicting variations possible in the nucleus and cell shape along with nucleus alignment with cell axis in non-patterned (grown on glass) (left) and patterned cells (right). Ellipses are fits to cell-outline and nucleus-outline; the corresponding major axes represented as dashed lines. Wide-field transmission images of patterns on photomasks used to create micropatterns – RA (60 μm x 20 μm) and RB (30 μm x 15 μm) are shown here. Scale bar, 50 μm . (B) Schematic representation of cell to nuclear orientation angle (θ) and major (D1) and minor (D2) diameters of nucleus used for calculating nuclear eccentricity and aspect ratio. (C) Representative images of cells expressing GFP-Lamin A/C (green) mutants stained with DAPI (blue, DNA) and Phalloidin Alexa Fluor 568 (red, F-actin). Images show basal plane for actin and the maximum intensity projection for DAPI and GFP-Lamin A/C. Scale, 10 μm . (D) Orientation angle difference (θ), eccentricity, aspect ratio, and circularity of nucleus measured from three different conditions Glass (*left column*), RA pattern (*middle column*), RB pattern (*right column*). The asterisk marks significance ($p < 0.001$) difference when compared with WT cells grown on the glass. $n = 27, 32, 52, 21$ cells for glass from one experiment, $n = 70, 41, 48, 55$ cells for RA in three independent experiment, $n = 41, 37, 52, 36$ cells for RB in two independent experiment. * $p < 0.05$, ** $p < 0.01$, *** $p < 0.001$, Wilcoxon based Mann-Whitney U test were performed for statistical testing.

Figure 2. Nuclei of cells with lamin mutations are less resistant to cyclic stretch. Blue, green and red channels in images denote DAPI, GFP-Lamin A transfection and Phalloidin staining in C2C12 cells with wild type (WT) and mutant Lamin A/C (WT, K97E, E161K, R190W). Cells were either (A) grown on PDMS and fixed – without imparting cyclic stretch or (B) grown, imparted cyclic stretch (10% cyclic stretched with 2 Hz frequency for 2.5 h.) and subsequently fixed. Scale, 10 μm . The arrow shows the direction of stretching. (C) Orientation angle difference (θ), eccentricity, aspect ratio, and circularity of nucleus measured from unstretched and stretched conditions. $n = 26, 80, 72, 119$ cells for unstretched and $n = 77, 55, 77, 123$ cells for stretched condition in three independent experiment. * $p < 0.05$ * $p < 0.01$, ** $p < 0.001$, Wilcoxon based Mann-Whitney U test were performed for statistical testing.

Figure 3. Reduction in the lamina thickness due to laminopathic mutation. eGFP-lamin A (containing wild-type and R190W, E161K & K97E mutations) transfected cells were grown on RA (A) and RB (C) patterned surface. The lower panels of A and C are representing linearization of the nuclear lamina for wild-type and mutant nuclei. The representative FWHMs of the intensity profiles

Nuclear deformations in cardiomyopathic nuclei

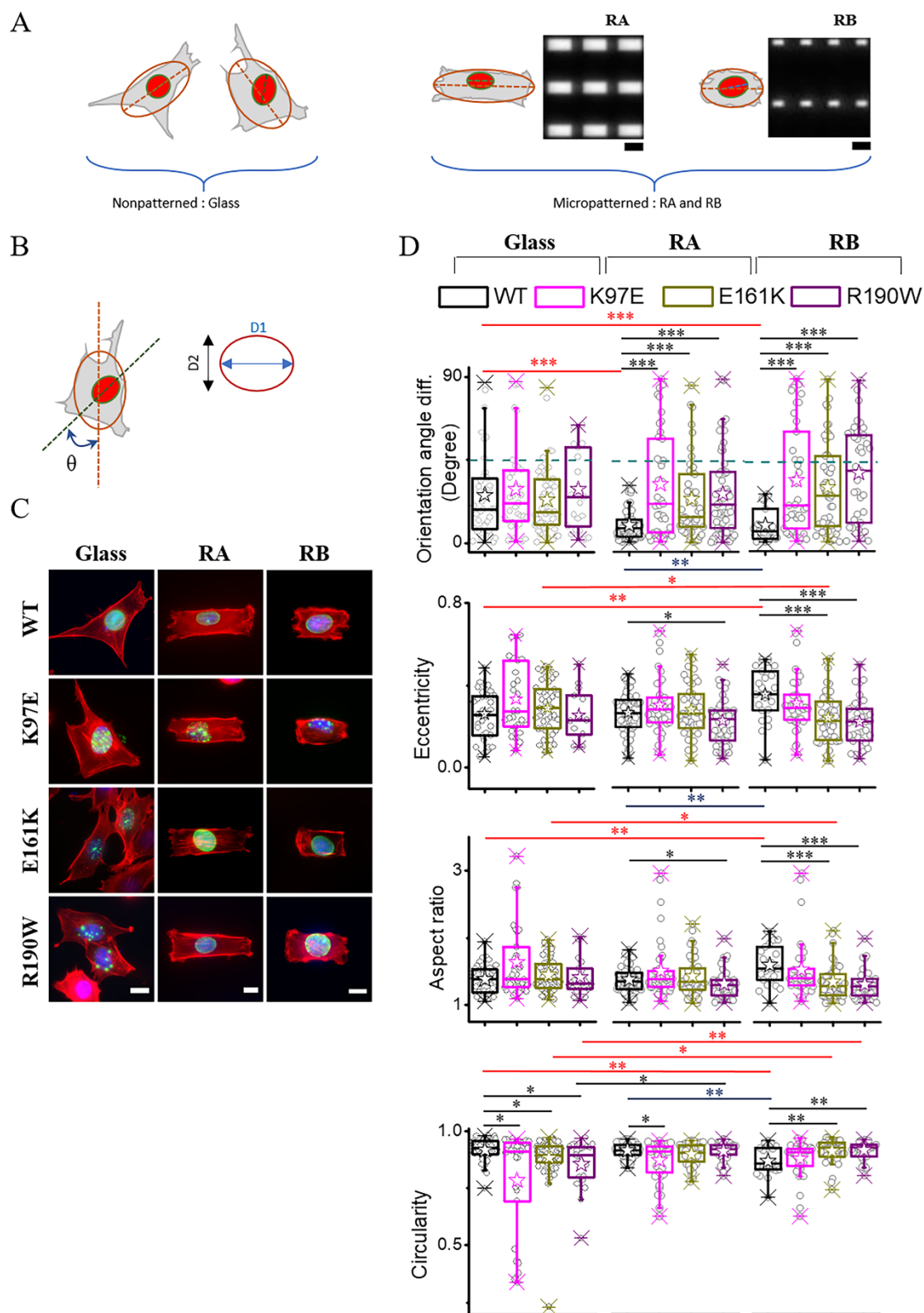
of white the line across the linearized lamina (after Gaussian Fittings) are shown in panel B for RA and in panel D for RB surface. The box plots in the panel B and D represent the FWHM (thickness) of the lamina for RA and RB micropatterned surface respectively. Each dot in the box plot denotes the raw data obtained from each nucleus. The scale bar is 5 μm . *** $p < 0.001$, ** $p < 0.05$, ns= not significant.

Figure 4. Model for lamin meshwork in the presence of mechanical cue in laminopathic cells.

In presence of the external mechanical cue, wild-type lamin A form dense meshwork inside the nucleoplasm and width of the lamina also increases. In the case of laminopathic nuclei, lamin A meshwork density decreases and the lamina also shows thinning behavior in the presence of the same external mechanical force. The nuclear axis also shows large impairment along the acting stress fiber compared to the wild-type nucleus.

Nuclear deformations in cardiomyopathic nuclei

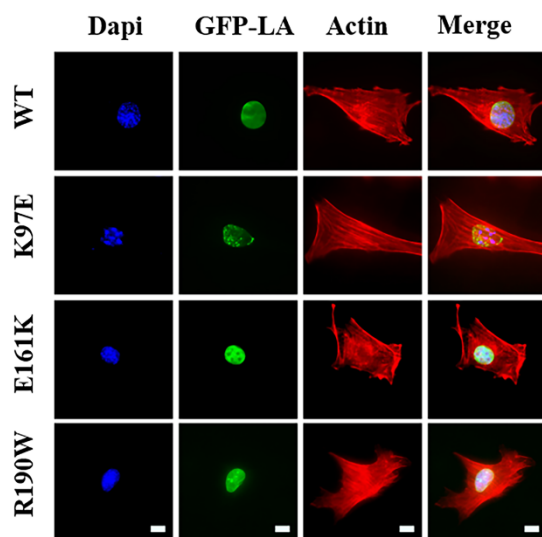
Figure 1



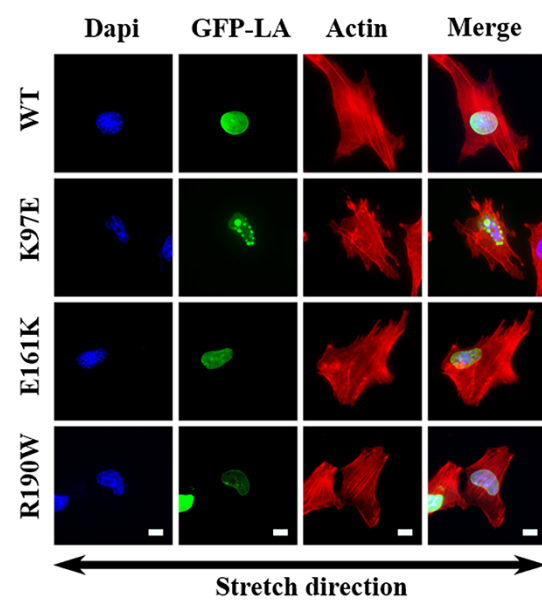
Nuclear deformations in cardiomyopathic nuclei

Figure 2

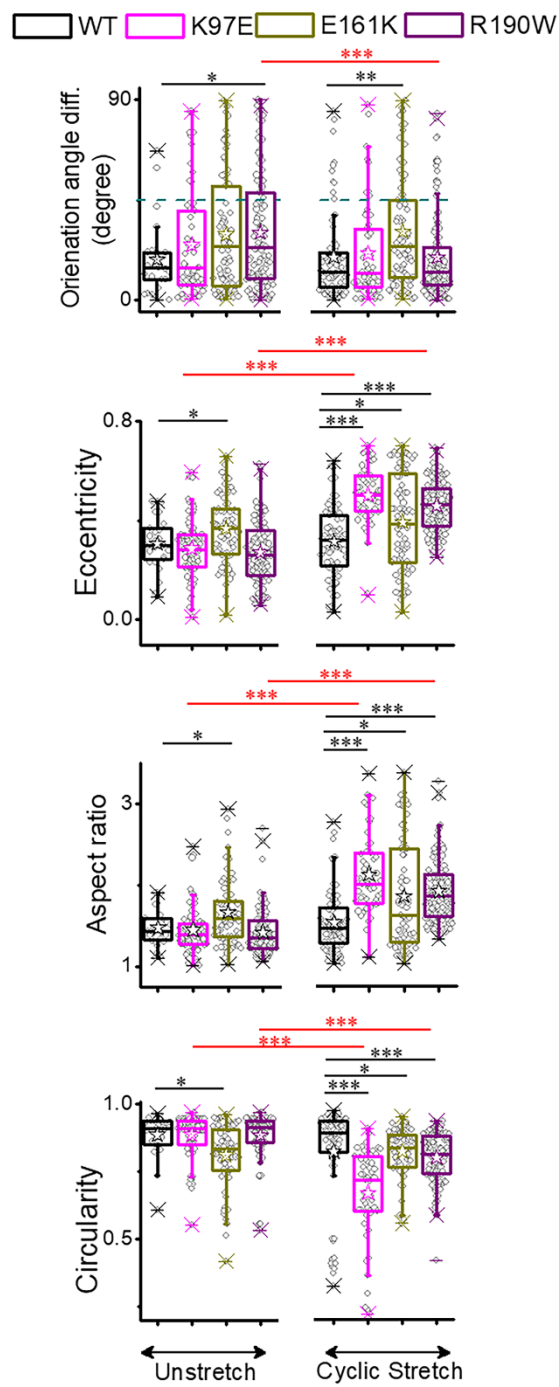
A



B

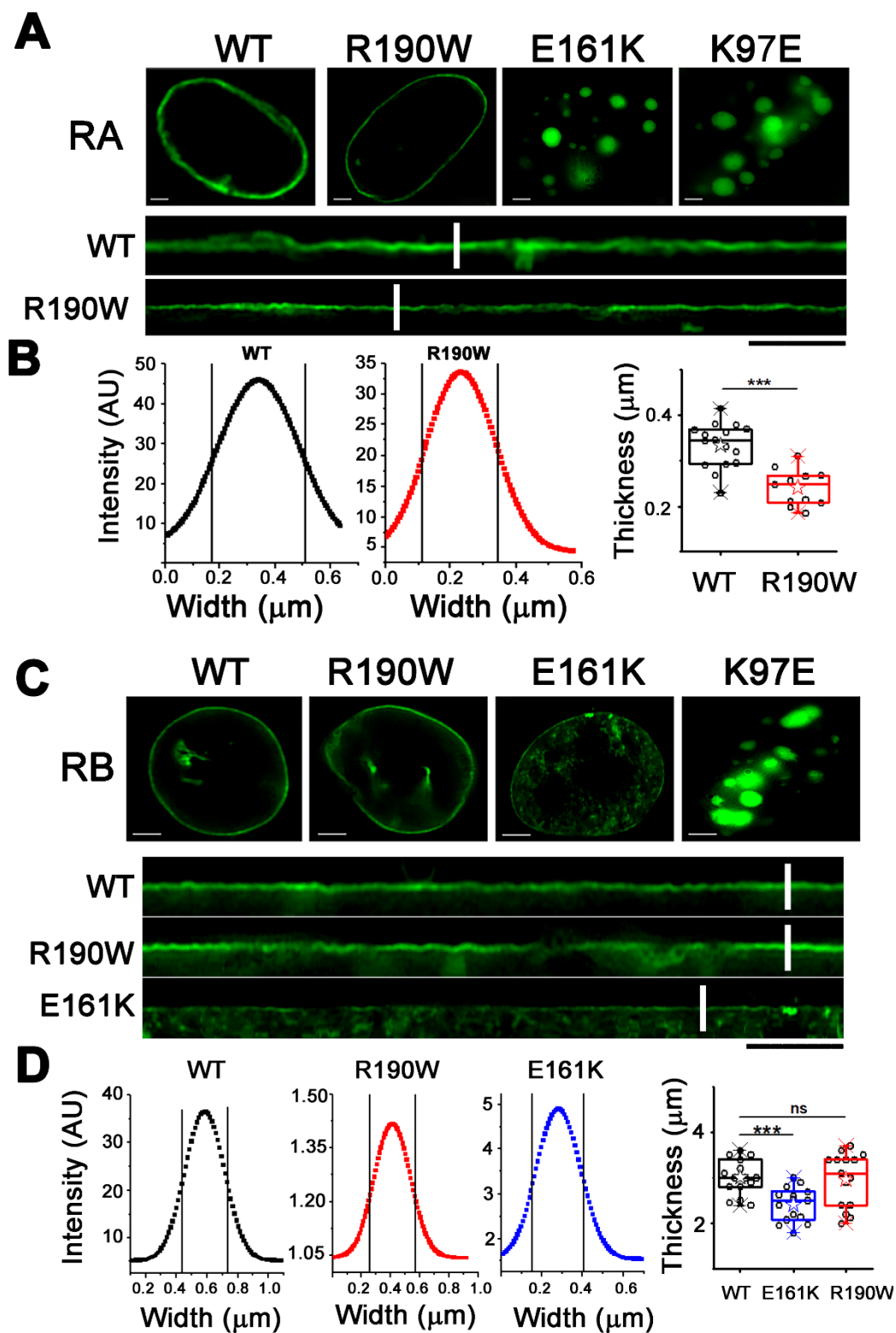


C



Nuclear deformations in cardiomyopathic nuclei

Figure 3



Nuclear deformations in cardiomyopathic nuclei

Figure 4

