

Investigating the physical effects in bacterial therapies for avascular tumors

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Abstract

Tumor-targeting bacteria elicit anticancer effects by infiltrating hypoxic regions, releasing toxic agents and inducing immune responses. Although current research has largely focused on the influence of chemical and immunological aspects on the mechanisms of bacterial therapy, the impact of physical effects is still elusive. Here, we propose a mathematical model for the anti-tumor activity of bacteria in avascular tumors that takes into account the relevant chemo-mechanical effects. We consider a time-dependent administration of bacteria and analyze the impact of bacterial chemotaxis and killing rate. We show that active bacterial migration towards tumor hypoxic regions provides optimal infiltration and that high killing rates combined with high chemotactic values provide the smallest tumor volumes at the end of the treatment. We highlight the emergence of steady states in which a small population of bacteria is able to constrain tumor growth. Finally, we show that bacteria treatment works best in the case of tumors with high cellular proliferation and low oxygen consumption.

Keywords: Cancer, Bacterial therapy, Mathematical modeling,
Chemotaxis, Space competition

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1 **1. Introduction**

2 Cancers display huge variability between different patients and even in
3 the same patient. Nonetheless, cancer cells share a finite set of hallmarks
4 such as sustained proliferation, invasion and metabolic reprogramming, which
5 shape their behavior in solid tumors (Hanahan and Weinberg, 2011). Among
6 other hallmarks, tumor cells are known to recruit new blood vessels to sus-
7 tain their proliferation, in a process known as *tumor angiogenesis* (Folkman,
8 1971). This neovasculature is generally altered in terms of architecture and
9 morphology of the vessels, leading to poor perfusion of certain areas of the
10 tumor (Carmeliet and Jain, 2000). Hypoxic regions are thus created and
11 maintained during tumor development, concurring to the progression of can-
12 cer cells towards malignant phenotypes (Vaupel and Mayer, 2007). More-
13 over, low nutrient levels can lead to cell quiescence, a situation in which
14 tumor cells delay metabolic activities and become less sensitive to standard
15 chemotherapies (Challapalli et al., 2017). Such hypo-perfused areas are gen-
16 erally associated with poor patient outcome but, on the other hand, could
17 be exploited for tumor targeting (Wilson and Hay, 2011). The same hypoxic
18 areas provide indeed a niche for bacteria to colonize the tumor and exert a
19 therapeutic action (Forbes, 2010; Zhou et al., 2018). The use of bacteria for
20 cancer therapy dates back hundreds of years, with doctors reporting tumor
21 regression in several patients (Kramer et al., 2018). However, such treatments
22 also caused some fatalities and the limited understanding of the therapeutic
23 mechanisms of action shifted research efforts towards other strategies - es-
24 pecially radiotherapy (Kramer et al., 2018). In the last few years the use of
25 live bacteria for cancer treatment has regained interest, and several bacterial
26 strains have been tested in animal models and even advanced to clinical tri-
27 als (Torres et al., 2018). Nevertheless, clinical development of such therapies
28 is still facing significant issues due to infection-associated toxicities and in-
29 complete knowledge of infection dynamics (Kramer et al., 2018; Zhou et al.,
30 2018). As much research was focused on the immune responses after bac-
31 teria administration, a clear picture of the interaction between cancer and
32 bacterial cells is still lacking.

33 Mathematical modeling emerges as a promising candidate to assist the
34 understanding of bacterial therapy mechanism of action in cancer. Mathe-
35 matical models have been applied in the context of cancer to elucidate its
36 progression and treatment (Byrne, 2010; Altrock et al., 2015). Recent exam-
37 ples combining experimental and modeling work in bacterial therapies are

38 given in (Kasinskas and Forbes, 2006; Jean et al., 2014; Hatzikirou et al.,
39 2017; Suh et al., 2018), featuring *in vitro* as well *in vivo* experiments.

40 Here we describe a mathematical model for bacteria-based cancer ther-
41 apy within avascular tumors, focusing on the influence of physical effects on
42 therapy outcomes. Such effects are present in every biological system but are
43 often concealed by the complexity of the interactions between molecular and
44 cellular players. Here we show through a simple mathematical model that
45 these effects take an important part in bacterial therapies and are able to
46 influence their outcomes. The model is formulated in the context of mixture
47 theory, a framework with a long history of applications to biological prob-
48 lems - see for example Ambrosi and Preziosi (2002); Breward et al. (2001,
49 2002, 2003); Byrne and Preziosi (2003); Chaplain et al. (2006); Preziosi and
50 Tosin (2009) and the recent reviews of Siddique et al. (2017); Pesavento
51 et al. (2017). Our aim is to evaluate the impact of bacterial chemotaxis
52 and anti-tumor activity on cancer cells, using spheroids as a prototype of
53 avascular tumors. We consider bacterial administration after full formation
54 of the spheroid, when hypoxic areas are present. We describe the effects of
55 the treatment on the behavior of the spheroid constituents, e.g. tumor cells
56 and bacteria volume fractions, at different time points and over the spheroid
57 radius.

58 The remainder of the paper is organized as follows. In Section 2 we
59 describe the mathematical model and its derivation. In Section 3 we present
60 model results, analyzing the impact of different model parameters. Finally,
61 in Section 4 we discuss the biological implications of the results and suggest
62 new research directions.

63 2. Materials and Methods

64 We propose a mathematical model describing the impact of bacterial
65 cells on tumor spheroid growth. The model is based on mixture theory, a
66 continuum theory that allows to describe the chemo-mechanical interactions
67 between different tissue components. We follow the approach discussed in
68 Preziosi (2003); Byrne (2012) and, specifically, adapt the derivation in Boemo
69 and Byrne (2019) to our problem. In the following we present the final form of
70 the equations, leaving the full derivation in the Supplementary Information.

71 We describe the tumor as being composed of three main constituents
72 (or *phases* in the language of mixture theory): tumor cells (TCs), bacteria
73 and extracellular material. The variables referring to these quantities will

74 be identified by the indexes c, b and f, respectively. We also consider the
 75 presence of a nutrient, i.e. oxygen, diffusing over the spheroid domain. The
 76 model equations are derived by applying conservation of mass and linear
 77 momentum to each phase, and enforcing the saturation constraint (i.e. all
 78 the space in the spheroid is occupied by the phases, there are no voids). Then,
 79 we close the model by imposing suitable constitutive assumptions regarding
 80 the material properties of the phases and their interaction terms.

81 2.1. Model equations

82 In the following we will be interested in the case of tumor spheroids, for
 83 which the assumption of spherical symmetry applies. The problem reduces
 84 to the set of Partial Differential Equations (PDEs):

$$\frac{\partial \phi_c}{\partial t} = \frac{1}{r^2} \frac{\partial}{\partial r} \left\{ r^2 \left[D_c (1 - \phi_c) \frac{\partial \phi_c}{\partial r} - D_b \phi_c \frac{\partial \phi_b}{\partial r} - \chi \phi_c \phi_b \frac{\partial n}{\partial r} \right] \right\} + S_c, \quad (1)$$

$$\frac{\partial \phi_b}{\partial t} = \frac{1}{r^2} \frac{\partial}{\partial r} \left\{ r^2 \left[D_b (1 - \phi_b) \frac{\partial \phi_b}{\partial r} - D_c \phi_b \frac{\partial \phi_c}{\partial r} + \chi \phi_b (1 - \phi_b) \frac{\partial n}{\partial r} \right] \right\} + S_b, \quad (2)$$

$$\frac{\partial n}{\partial t} = \frac{1}{r^2} \frac{\partial}{\partial r} \left(r^2 D_n \frac{\partial n}{\partial r} \right) + S_n. \quad (3)$$

85 Here, ϕ_c , ϕ_b and n are the tumor cell and bacteria volume fractions and
 86 normalized nutrient concentration, respectively. These quantities depend on
 87 the radial coordinate $r \in [0, R]$ and time $t \in [0, t_f]$. In addition, D_i are
 88 the phases motility coefficients (i=c,b), D_n the nutrient diffusion coefficient,
 89 and χ the bacterial chemotactic coefficient. The mass exchange terms S_i
 90 (i=c,b,n), regulating the transfer of mass between the different components,
 91 will be detailed in the next subsection. Note that we do not solve explicitly
 92 for ϕ_f (i.e. the volume fraction of extracellular material) since this quantity
 93 can be obtained as $\phi_f = 1 - \phi_c - \phi_b$ due to the saturation constraint (see
 94 the Supplementary Information). We model growth of the spheroid as a free-
 95 boundary problem, in which the outer tumor radius $r = R(t)$ moves with the
 96 same velocity as the TC phase,

$$\frac{dR}{dt} = v_c(R, t) = D_b \frac{\partial \phi_b}{\partial r} + D_c \left(1 - \frac{1}{\phi_c} \right) \frac{\partial \phi_c}{\partial r} + \chi \phi_b \frac{\partial n}{\partial r} \Big|_{r=R}. \quad (4)$$

Finally, we define a set of boundary and initial conditions to close the differ-
 ential problem in equations (1)-(3). Due to the problem symmetry no-flow

boundary conditions are enforced at the spheroid center, whereas we fix the values of TC volume fraction, bacterial volume fraction and normalized nutrient concentration on the spheroid boundary:

$$\partial_r \phi_c = \partial_r \phi_b = \partial_r n = 0, \quad r = 0 \quad (5)$$

$$\phi_c = \phi_{c0}, \quad \phi_b = \phi_{b0}, \quad n = 1, \quad r = R(t). \quad (6)$$

97 We assume a uniform initial tumor volume fraction $\phi_{c0} = 0.8$ across the
98 spheroid (Byrne and Preziosi, 2003) and, to model bacteria administration,
99 we consider a time dependent value for the bacterial volume fraction at the
100 spheroid outer radius:

$$\phi_b = \begin{cases} 0, & \text{for } 0 \leq t < t_0 \\ \phi_{b0}, & \text{for } t_0 \leq t < t_a \\ 0, & \text{for } t_a \leq t \leq t_f, \end{cases} \quad (7)$$

101 where ϕ_{b0} is the administered volume fraction of bacteria, t_0 is the time
102 of administration and t_a its duration. Regarding the initial conditions, we
103 consider a spheroid devoid of bacteria and displaying a uniform TC volume
104 fraction and nutrient concentration over its radius:

$$\phi_c(r, 0) = \phi_{c0}, \quad \phi_b = 0, \quad n = 1. \quad (8)$$

105 Finally, we prescribe an initial spheroid radius, i.e. $R(0) = 90 \mu\text{m}$. The
106 equations of the model are discretized through the Finite Element Method
107 and solved using the commercial software COMSOL Multiphysics (COMSOL
108 AB).

109 2.2. Choice of mass exchange terms

110 To formulate the mass exchange terms in equations (1)-(3) we assume the
111 following assumptions (see Figure 1):

112 **A1** TCs proliferate when oxygen is available. As soon as the latter de-
113 creases below a critical threshold, they stop proliferating and start
114 necrosis (Chaplain et al., 2006; Gerlee and Anderson, 2007; Agosti
115 et al., 2018).

116 **A2** Bacteria compete with TCs for space and exert an anti-tumor effect
117 by a variety of mechanisms (e.g. by realising toxins and therapeutic
118 agents, or stimulating an immune response). (Forbes, 2010; Osswald
119 et al., 2015; Torres et al., 2018; Zhou et al., 2018).

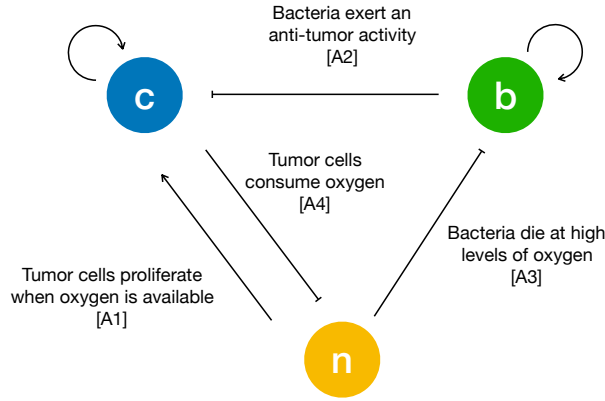


Figure 1: Schematic of the interactions between tumor cells (c), bacteria (b) and oxygen (n). The arrows are drawn according to the biological hypotheses detailed in the main text.

120 **A3** Bacteria die when oxygen is above a critical threshold and thrive in
 121 hypoxic conditions (*anaerobic* bacteria) (Toley and Forbes, 2011; Phai-
 122 boun et al., 2015; Osswald et al., 2015).

123 **A4** TCs consume oxygen provided by the culture medium (Matzavinos
 124 et al., 2009; Grimes et al., 2014).

The resulting mass exchange terms read:

$$S_c = \gamma_c \phi_c \frac{\phi_f}{\phi_{f0}} \mathcal{H} \left(\frac{n}{n_{cr}} - 1 \right) - \delta_c \phi_c \mathcal{H} \left(1 - \frac{n}{n_{cr}} \right) - \kappa \phi_c \phi_b, \quad (9)$$

$$S_b = \gamma_b \phi_b \frac{\phi_f}{\phi_{f0}} \mathcal{H} \left(1 - \frac{n}{n_{cr}} \right) - \delta_b \phi_b \mathcal{H} \left(\frac{n}{n_{cr}} - 1 \right), \quad (10)$$

$$S_n = -\delta_n \phi_c n. \quad (11)$$

125 Here γ_i and δ_i are the proliferation and death rate of the i -th phase respec-
 126 tively ($i = c, b$), whereas δ_n is the oxygen consumption rate. In addition, ϕ_{f0}
 127 is the initial volume fraction of extracellular material and we indicate with
 128 $\mathcal{H}(\cdot)$ a smooth version of the step function, and with n_{cr} the critical oxygen
 129 value below which hypoxic conditions develop. Finally, we do not consider a
 130 specific form for the anti-tumor effect of bacteria and introduce an effective
 131 TC killing rate κ in the equation for S_c .

Parameter	Value	Description	Reference
D_c	$0.5 \text{ mm}^2\text{d}^{-1}$	TC motility coefficient	(Colombo et al., 2015)
γ_c	0.48 d^{-1}	TC proliferation rate	(PBCF, 2012)
δ_c	0.5 d^{-1}	TC death rate	(Martínez-González et al., 2012)
D_b	$0.05 \text{ mm}^2\text{d}^{-1}$	Bacterial motility coefficient	(Toley and Forbes, 2011)
γ_b	15 d^{-1}	Bacterial proliferation rate	(Gibson et al., 2018)
δ_b	0.24 d^{-1}	Bacterial death rate	(Phaiboun et al., 2015)
D_n	$100 \text{ mm}^2\text{d}^{-1}$	Oxygen diffusion coefficient	(Matzavinos et al., 2009)
δ_n	8640 d^{-1}	Oxygen consumption rate	(Colombo et al., 2015)
χ	$[0, 0.864] \text{ mm}^2\text{d}^{-1}$	Bacterial chemotactic coefficient	estimated
κ	$[0, 5] \text{ d}^{-1}$	Bacterial killing rate	model specific
n_{cr}	0.58	Critical oxygen concentration	calibrated

Table 1: Summary of the parameter values considered in the model simulations.

132 2.3. Model parametrization

133 The parameters used in the model simulations are reported in Table 1. In
134 the following we will compare model results with a set of published experi-
135 ments on the U87 glioma cell line. We take the TC proliferation rate from the
136 available data provided from the Bioresource Core Facility of the Physical
137 Sciences-Oncology Center (PBCF, 2012), whereas we select the TC death
138 rate in accordance to the estimate in (Kolokotroni et al., 2011; Martínez-
139 González et al., 2012). The work in (Toley and Forbes, 2011) provides a
140 value for the bacterial motility coefficient and proliferation rate in *in vitro*
141 cellular aggregates. Regarding bacterial proliferation, (Gibson et al., 2018)
142 supply a similar value through an analysis of bacterial doubling times. We
143 estimate the bacterial death rate from (Phaiboun et al., 2015), in which cel-
144 lular death dynamics are quantified under starvation at different bacteria
145 densities. Finally, we use the values in (Schaller and Meyer-Hermann, 2005;
146 Matzavinos et al., 2009; Grimes et al., 2014; Colombo et al., 2015; Alfonso
147 et al., 2016) for the oxygen diffusion coefficient and consumption rate in tu-
148 mor tissues. When carrying out the simulations, we vary the chemotactic
149 coefficient in the interval $[0, 8.64 \times 10^{-1}] \text{ mm}^2\text{d}^{-1}$. Since it was not possible
150 to find in the literature an estimate for the chemotactic coefficient of bacteria
151 in tissues, we considered the value of χ in bacterial solutions (Ford et al.,
152 1991; Lewus and Ford, 2001) and divided it for the ratio between the motil-
153 ity coefficient in solution and in tissue - about 100, (Ford et al., 1991; Lewus
154 and Ford, 2001). Since we do not consider a specific mechanism for the anti-
155 tumor activity of bacteria, we select the killing rate κ to be in the interval
156 $[0, 5] \text{ d}^{-1}$, i.e. spanning characteristic times between several days and a few

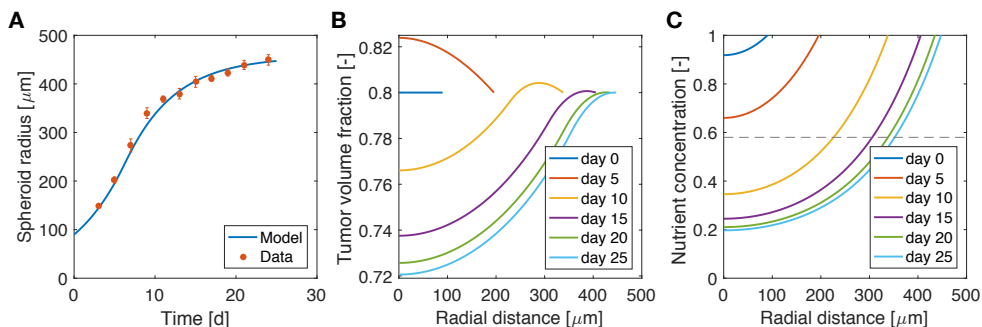


Figure 2: Calibration of the model on tumor spheroid data. **A** Comparison between model results and experimental data for the spheroid growth curve. The experimental points are taken from (Mascheroni et al., 2016) and represent the growth of U87 spheroids. Dots are mean values and bars standard deviation of the measurements. Tumor volume fraction (**B**) and oxygen concentration (**C**) at different times of spheroid growth. The dashed line in the last plot displays the critical oxygen concentration.

157 hours. Finally, we fit the parameter for the critical oxygen concentration
 158 from the above mentioned experiments. The value that we found is similar
 159 to the one reported in (Gerlee and Anderson, 2007; Agosti et al., 2018).

160 3. Results

161 3.1. Model calibration on spheroid experiments

162 We start the analysis by considering the growth of a spheroid suspended
 163 in culture medium, in the absence of bacteria. We compare the results of the
 164 model with the data for radial growth of U87 tumor spheroids available from
 165 Mascheroni et al. (2016). We use the model to fit the critical oxygen concen-
 166 tration parameter n_{cr} , keeping all the other quantities as defined in Table 1.
 167 Figure 2 shows a good agreement between the model and the experiments,
 168 over all the growth curve. The model is able to reproduce the two phases
 169 of spheroid growth usually described in the literature (Conger and Ziskin,
 170 1983; Sutherland, 1988; Vinci et al., 2012). The spheroid radius (see Figure
 171 2A) displays a first stage of rapid increase, followed by a saturation phase.
 172 This behavior is detailed in Figures 2B,C, showing the evolution of the tu-
 173 mor volume fraction and oxygen concentration over the spheroid radius at
 174 different time points. The tumor volume fraction, i.e. ϕ_c , increases over the
 175 spheroid at early time points (Figure 2B). Then, as TCs consume oxygen to
 176 proliferate, its concentration decreases in the centre of the aggregate (Figure

177 **2C**). When the oxygen level drops below the critical threshold n_{cr} (dashed
178 line in Figure **2C**), TCs stop proliferating and die. This results in a decrease
179 of ϕ_c in the spheroid core, displayed at longer times in Figure **2B**. Close to
180 saturation, the amount of cells that proliferate is balanced by the number
181 of cells that die, turning into extracellular material. Therefore, even if cell
182 growth continues to take place in the outer rim of the spheroid, it is not
183 enough to advance the spheroid front, which reaches a steady state. These
184 results match qualitatively what is observed in the experimental (Landry
185 et al., 1982; Montel et al., 2011; Grimes et al., 2014; Sarkar et al., 2018)
186 and modeling (Ward and King, 1999; Byrne and Preziosi, 2003; Ambrosi and
187 Mollica, 2004; Schaller and Meyer-Hermann, 2005; Mascheroni et al., 2016;
188 Boemo and Byrne, 2019) literature for tumor spheroids and will serve as a
189 basis for the discussion in the next sections.

190 *3.2. Administration of bacteria leads to tumor remission but not eradication*

191 Figure 3 shows the influence of bacterial therapy on tumor spheroid com-
192 position for an example case. We evaluate the effects of adding bacteria to
193 the culture medium after the spheroid is fully formed, i.e. when hypoxic
194 regions have developed. In particular, we select an administration time of
195 $t_0 = 26\text{d}$ and a treatment duration of $t_a = 2\text{d}$. We consider an interme-
196 diate value for both the bacterial chemotactic coefficient and killing rate
197 ($\chi = 0.432\text{mm}^2\text{d}^{-1}$, $\kappa = 2.5\text{d}^{-1}$). As shown by the low TC volume fraction
198 in Figure **3A** at later times, bacteria administration leads to spheroids less
199 populated by TCs. This space is occupied by bacteria (Figure **3B**), which
200 thrive in the hypoxic region located in the spheroid core. After bacterial ther-
201 apy the spheroid shrinks and is less populated by cancer cells. This leads
202 to higher values of oxygen concentration at the center of the aggregate, as
203 displayed in Figure **3C**. Finally, Figure **3D** shows the evolution of TC (V_c)
204 and bacteria (V_b) volumes over time. These quantities are calculated as

$$V_i = \int_{V_{sf}} \phi_i dV, \quad (12)$$

205 where the integral is performed over the spheroid volume V_{sf} ($i=c,b$). At early
206 time points, V_c is in a phase of fast growth, since the nutrient is available
207 throughout the spheroid and no bacteria are present. After administration,
208 there is a fast increase of bacteria volume together with a rapid decrease of
209 TC volume. At later time points the system evolves toward a steady state in

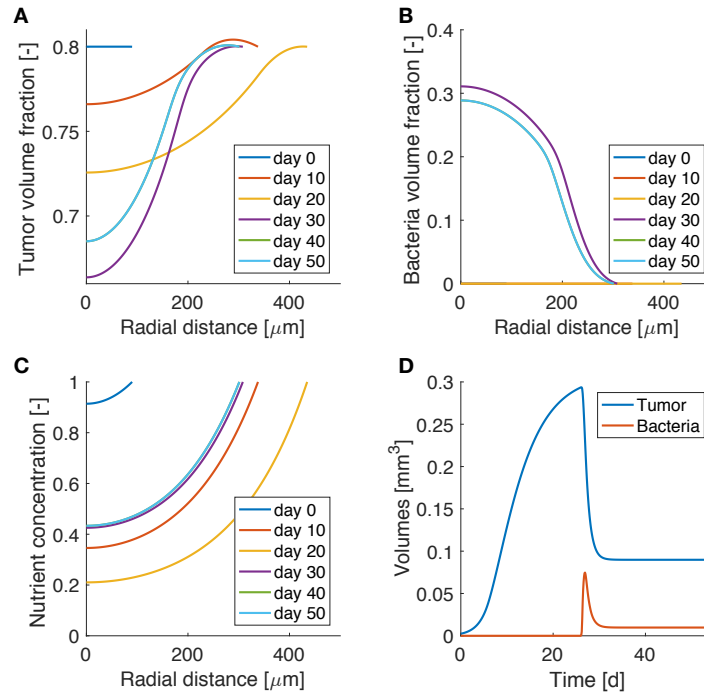


Figure 3: Model results for bacteria administration to tumor spheroids. Spatio-temporal evolution of tumor (A) and bacteria (B) volume fractions and oxygen concentration (C). D Temporal evolution of tumor and bacteria volumes in the spheroid.

210 which both bacteria and TCs coexist in the tumor aggregate. Even though
211 the TCs are not completely removed, the spheroid persists in an equilibrium
212 state, where an asymptotic size is kept for long times.

213 3.3. High chemotaxis allows for maximal reduction of tumor size

214 We investigated the impact of different bacterial chemotactic and anti-
215 tumor strengths on spheroid composition at the end of the simulations, i.e.
216 at day 50 (Figure 4). We found that the highest reduction in tumor volume is
217 obtained for the highest values of the chemotactic coefficient and killing rate,
218 as shown in Figure 4A. On the other hand, highly chemotactic bacteria with-
219 out an anti-tumor activity lead to the highest tumor volume. Interestingly,
220 the tumor is never completely eradicated over all the explored parameter
221 sequence. A similar result is obtained for the bacteria volume at the end of
222 the simulations (Figure 4). Here, no matter the strength of chemotaxis or
223 anti-tumor activity, bacterial cells are always present in the final spheroid

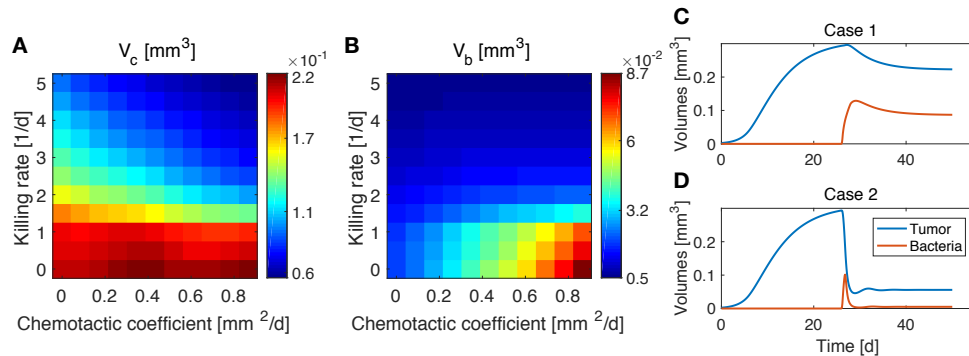


Figure 4: Influence of bacteria chemotactic coefficient and anti-tumor activity on tumor (A) and bacteria (B) volumes at the end of the simulations (day 50). Temporal evolution of tumor and bacteria volumes for a high chemotactic coefficient and a low (Case 1, C) and high (Case 2, D) killing rate.

224 volume. High bacterial volumes are present for high chemotactic coefficients,
 225 whereas high killing rates lead to small bacterial volumes independent of the
 226 chemotactic strength. Indeed, even though the tumor volume considerably
 227 varies over the chemotactic space for high killing rates, the bacterial volume
 228 is almost independent of this quantity (see Figure S1 in the Supplementary).
 229 Finally, Figures 4C and 4D show the temporal variation of tumor and bacte-
 230 rial volumes for two extreme cases occurring for high chemotaxis and low
 231 (Case 1) or high (Case 2) killing rate. The first plot shows that after the
 232 administration of bacteria the tumor volume is reduced, even in the absence
 233 of anti-tumor activity. The two populations in the spheroid reach an equi-
 234 librium at later times, with bacteria representing a significant portion of the
 235 spheroid. In the second case, the high anti-tumor activity of the bacteria
 236 is responsible for a sharp decrease of the tumor population, leading also to
 237 oscillations in the TC volume. Although bacteria now constitute a small
 238 part of the overall spheroid volume, they are still able to keep the tumor size
 239 under control.

240 3.4. Highly proliferating and low oxygen consuming tumors are mostly bene- 241 fited from bacterial therapy

242 The results obtained in the previous subsection are insensitive of the
 243 administration time t_0 , the duration of the administration t_a and the ad-
 244 ministered bacteria volume fraction ϕ_{b0} , even for large variations of these
 245 parameters (see Supplementary Figures S2-S4). This made us investigate

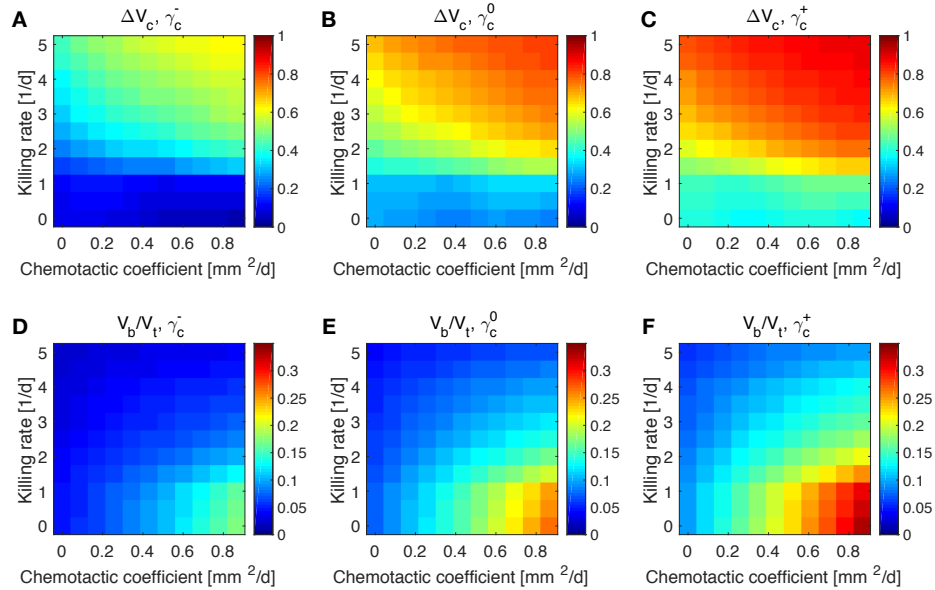


Figure 5: Impact of tumor proliferation rate on tumor and bacteria volumes at the end of the simulations (day 50). Relative tumor volume change and relative bacteria volume for low (**A**, **D**), nominal (**B**, **E**) and high (**C**, **F**) tumor cell proliferation rate.

246 whether the steady states reached at the end of the simulations and dis-
 247 played in Figure 4 were therefore a function of the mechanisms regulating
 248 the tumor/bacteria dynamics. To check this hypothesis we simulated the be-
 249 havior of TCs with a lower or higher proliferation and oxygen consumption
 250 rates with respect of the one shown in Figure 4. We report our findings in
 251 Figures 5 and 6. We considered a variation of $\pm 50\%$ with respect to the
 252 nominal value of the parameters in Table 1, and labeled the cases using the
 253 plus or minus in the superscript accordingly. All the other parameters keep
 254 the nominal values. We evaluated the spheroid response in terms of relative
 255 tumor reduction by introducing the quantity:

$$\Delta V_c = \frac{V_0 - V_c}{V_0}, \quad (13)$$

256 where V_c is the final tumor volume and V_0 the tumor volume at the time of
 257 bacteria administration. We also analyzed the relative bacteria volume at
 258 the end of the simulation, plotting the ratio of bacteria volume V_b to the
 259 total spheroid volume V_t .

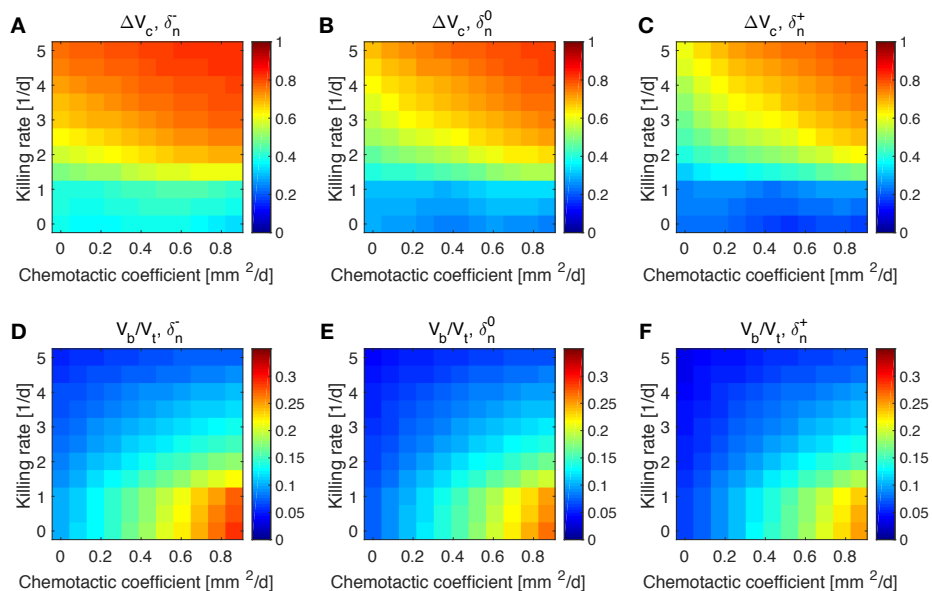


Figure 6: Impact of tumor oxygen consumption rate on tumor and bacteria volumes at the end of the simulations (day 50). Relative tumor volume change and relative bacteria volume for low (**A**, **D**), nominal (**B**, **E**) and high (**C**, **F**) tumor cell proliferation rate.

260 Tumors in which cells proliferate at a higher rate display the highest tu-
 261 mor reductions (Figure 5**A-C**). This is particularly true for the treatment
 262 with bacteria characterized by high chemotaxis and killing rate. Highly pro-
 263 liferative tumors are the ones that also show higher colonization by bacteria,
 264 as displayed in Figures 5**D-F**. Treatments with high chemotactic bacteria
 265 with low killing rates provide the highest relative bacteria volumes. Low
 266 oxygen consumption by TCs leads to results similar to highly proliferative
 267 tumors (6). Again, treatment using bacteria with high chemotaxis and high
 268 killing rate produces the best results in terms of tumor reduction. Regard-
 269 ing the final bacterial content, both high and low oxygen consuming tumors
 270 show considerable bacteria colonization. As before, the relative bacteria vol-
 271 ume is higher for highly chemotactic bacteria with low anti-tumor activity.
 272 Even though highly proliferative and low oxygen consuming TCs originate
 273 the highest final spheroid volumes (Figure S5), they benefit the most from
 274 bacteria treatment and display the higher final bacteria content.

275 4. Discussion

276 We proposed a mathematical model to study the influence of bacteria
277 treatment on avascular tumor growth. We considered anaerobic bacteria
278 which thrive in hypoxic environments and actively migrate towards nutrient
279 deprived regions in solid tumors. The model was calibrated to reproduce
280 published tumor spheroid data and then used to evaluate the impact of bac-
281 teria chemotaxis and killing rate on spheroid response.

282 Model results show preferential bacteria accumulation in the hypoxic
283 spheroid core, with tumor cells more localized towards the external spheroid
284 surface. In general, highly chemotactic bacteria possessing increased anti-
285 tumor activity provide the highest tumor reduction after treatment. On the
286 other hand, high chemotaxis but low anti-tumor activity lead to smaller tu-
287 mor reduction but higher bacteria colonization at the end of the simulations.
288 When varying the tumor parameters, we found that bacteria treatment works
289 best for highly proliferative and low oxygen consuming tumors.

290 For simplicity, we considered a general effective anti-tumor activity of
291 TCs by bacteria without focusing on specific mechanisms, e.g. cytotoxic
292 agents, prodrug-converting enzymes, etc. (Torres et al., 2018; Zhou et al.,
293 2018; Kramer et al., 2018). Such treatment modalities could be incorpo-
294 rated by extending the model, to provide a more accurate description of the
295 therapeutic action. Moreover, we focused on tumor spheroids, an *in vitro*
296 approximation of avascular tumors. As such, they lack all the interactions
297 between the tumor and its immune environment. On the one hand, this ap-
298 proach allows to investigate the mutual dynamics of bacteria and tumor cells
299 without external influences, but on the other including the cross-talk between
300 bacteria and the components of the immune system would be a fundamental
301 step to address questions coming from *in vivo* tumors. Following (Boemo
302 and Byrne, 2019), we modeled the mechanical response of cells and bacte-
303 ria in the simplest way considering the phases as inviscid fluids. Although
304 this description is still able to qualitatively describe the experimental re-
305 sults, more detailed constitutive assumptions for the mechanical behavior of
306 the phases would lead to new insights into the interactions between bacteria
307 and TCs in the aggregate (Sciumè et al., 2013; Giverso et al., 2015; Ambrosi
308 et al., 2017; Mascheroni et al., 2018; Fraldi and Carotenuto, 2018; Giverso
309 and Preziosi, 2019). We also considered ideal spherical spheroids to reduce
310 the mathematical problem to one dimension. Even if the qualitative results
311 will be maintained in a three-dimensional geometry, adopting the latter will

312 be crucial to translate the model to *in vivo* situations.

313 In this modeling approach, space competition between bacteria and tumor
314 cells arises naturally from the conservation of mass and momentum imposed
315 by the governing equations. As no void regions are allowed into the spheroid,
316 when cells move or die one of the model components automatically fills the
317 space. Bacteria and TCs compete for space in the spheroid and the expansion
318 of the tumor becomes limited, especially when the anti-tumor activity
319 of bacteria is strong. However, for increasing values of the chemotactic coefficient
320 and low values of the killing rate, bacteria localize predominantly
321 in the spheroid core and displace TCs to the outer region of the spheroid.
322 Both types of cell can proliferate in each of the two spheroid areas (hypoxic
323 for spheroids, well-oxygenated for TCs), giving rise to high spheroid volumes
324 and considerable bacteria colonization.

325 As a matter of fact, chemotaxis could be a target for bacteria-based anticancer
326 therapies and diagnostic tools. For example, TCs that become restricted to outer
327 spheroid areas after administration of highly chemotactic bacteria are more oxygenated
328 and could benefit from standard chemotherapeutic or radiation treatments in the context
329 of synergistic treatments (Zhou et al., 2018). We highlight that this is an example
330 showing that mathematical models could help to identify situations when TC sensitization
331 to therapies might be possible - see also (Owen et al., 2004; Kim et al., 2013;
332 Michor and Beal, 2015; Mascheroni et al., 2017). On the other hand, highly
333 chemotactic bacteria could be used as tracers to identify necrotic regions
334 in spheroid, exploiting their targeting efficiency. Moreover, the simulations
335 show the existence of steady states in which a small population of bacteria
336 is in dynamical equilibrium with cancer cells, leading to tumor size control
337 over time. All these mechanisms arise as a pure physical effect from the competition
338 for space between cancer and bacteria cells and could be optimized
339 to obtain the highest tumor volume reduction or bacteria colonization. Currently,
340 even though researchers are aware of the benefits coming from active bacteria
341 migration towards hypoxic regions in tumors (Forbes, 2010; Kramer et al., 2018),
342 this knowledge has not been efficiently exploited in the clinical trials carried out
343 so far (Torres et al., 2018).

345 Finally, we point out three straightforward developments that emerge
346 from the findings of this work. Firstly, our theoretical results advocate for experiments
347 with tumor spheroids. With such a simplified experimental setup, several bacterial
348 strains could be tested on different cancer cell lines to validate model findings.
349 Secondly, one could think about extending the model to

350 consider different bacterial administration schedules. The duration of bacte-
351 ria administration, the time of administration and single vs. multiple dosing
352 could be investigated to determine the optimal conditions for this kind of
353 treatment. Lastly, the tight coupling between the dynamics of TCs and bacte-
354 ria in terms of regulating their reciprocal environment could be addressed
355 via mathematical models, in order to control the bacterial infection or iden-
356 tify the optimal timing of the therapy.

357 **Conflict of Interest Statement**

358 The authors declare that the research was conducted in the absence of any
359 commercial or financial relationships that could be construed as a potential
360 conflict of interest.

361 **Author Contributions**

362 PM, HH and MMH contributed conception and design of the study; PM
363 derived the model and performed the computational analysis; PM wrote the
364 first draft of the manuscript; HH and MMH wrote sections of the manuscript.
365 All authors contributed to manuscript revision, read and approved the sub-
366 mitted version.

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376 **References**

- 377 Agosti, A., Cattaneo, C., Giverso, C., Ambrosi, D., Ciarletta, P., 2018.
378 A computational framework for the personalized clinical treatment of
379 glioblastoma multiforme. *ZAMM-Journal of Applied Mathematics and Me-*
380 *chanics/Zeitschrift für Angewandte Mathematik und Mechanik* 98, 2307–
381 2327.
- 382 Alfonso, J., Köhn-Luque, A., Stylianopoulos, T., Feuerhake, F., Deutsch, A.,
383 Hatzikirou, H., 2016. Why one-size-fits-all vaso-modulatory interventions
384 fail to control glioma invasion: in silico insights. *Scientific reports* 6, 37283.
- 385 Altrock, P.M., Liu, L.L., Michor, F., 2015. The mathematics of cancer:
386 integrating quantitative models. *Nature Reviews Cancer* 15, 730.
- 387 Ambrosi, D., Mollica, F., 2004. The role of stress in the growth of a multicell
388 spheroid. *Journal of mathematical biology* 48, 477–499.
- 389 Ambrosi, D., Pezzuto, S., Riccobelli, D., Stylianopoulos, T., Ciarletta, P.,
390 2017. Solid tumors are poroelastic solids with a chemo-mechanical feedback
391 on growth. *Journal of Elasticity* 129, 107–124.
- 392 Ambrosi, D., Preziosi, L., 2002. On the closure of mass balance models for
393 tumor growth. *Mathematical Models and Methods in Applied Sciences* 12,
394 737–754.
- 395 Boemo, M.A., Byrne, H.M., 2019. Mathematical modelling of a hypoxia-
396 regulated oncolytic virus delivered by tumour-associated macrophages.
397 *Journal of Theoretical Biology* 461, 102–116.
- 398 Breward, C., Byrne, H., Lewis, C., 2001. Modelling the interactions between
399 tumour cells and a blood vessel in a microenvironment within a vascular
400 tumour. *European Journal of Applied Mathematics* 12, 529–556.
- 401 Breward, C., Byrne, H., Lewis, C., 2002. The role of cell-cell interactions in
402 a two-phase model for avascular tumour growth. *Journal of Mathematical*
403 *Biology* 45, 125–152.
- 404 Breward, C.J., Byrne, H.M., Lewis, C.E., 2003. A multiphase model de-
405 scribing vascular tumour growth. *Bulletin of mathematical biology* 65,
406 609–640.

- 407 Byrne, H., 2012. Mathematics and life sciences.
- 408 Byrne, H., Preziosi, L., 2003. Modelling solid tumour growth using the theory
409 of mixtures. *Mathematical medicine and biology: a journal of the IMA* 20,
410 341–366.
- 411 Byrne, H.M., 2010. Dissecting cancer through mathematics: from the cell to
412 the animal model. *Nature Reviews Cancer* 10, 221.
- 413 Carmeliet, P., Jain, R.K., 2000. Angiogenesis in cancer and other diseases.
414 *nature* 407, 249.
- 415 Challapalli, A., Carroll, L., Aboagye, E.O., 2017. Molecular mechanisms of
416 hypoxia in cancer. *Clinical and translational imaging* 5, 225–253.
- 417 Chaplain, M.A., Graziano, L., Preziosi, L., 2006. Mathematical modelling of
418 the loss of tissue compression responsiveness and its role in solid tumour
419 development. *Mathematical medicine and biology: a journal of the IMA*
420 23, 197–229.
- 421 Colombo, M.C., Giverso, C., Faggiano, E., Boffano, C., Acerbi, F., Ciarletta,
422 P., 2015. Towards the personalized treatment of glioblastoma: integrating
423 patient-specific clinical data in a continuous mechanical model. *PLoS One*
424 10, e0132887.
- 425 COMSOL AB, . Comsol multiphysics, stockholm, sweden. URL: <https://comsol.com>.
- 427 Conger, A.D., Ziskin, M.C., 1983. Growth of mammalian multicellular tumor
428 spheroids. *Cancer Research* 43, 556–560.
- 429 Folkman, J., 1971. Tumor angiogenesis: therapeutic implications. *New eng-
430 land journal of medicine* 285, 1182–1186.
- 431 Forbes, N.S., 2010. Engineering the perfect (bacterial) cancer therapy. *Nature
432 Reviews Cancer* 10, 785.
- 433 Ford, R.M., Phillips, B.R., Quinn, J.A., Lauffenburger, D.A., 1991. Measure-
434 ment of bacterial random motility and chemotaxis coefficients: I. stopped-
435 flow diffusion chamber assay. *Biotechnology and bioengineering* 37, 647–
436 660.

- 437 Fraldi, M., Carotenuto, A.R., 2018. Cells competition in tumor growth poroe-
438 lasticity. *Journal of the Mechanics and Physics of Solids* 112, 345–367.
- 439 Gerlee, P., Anderson, A.R., 2007. An evolutionary hybrid cellular automaton
440 model of solid tumour growth. *Journal of theoretical biology* 246, 583–603.
- 441 Gibson, B., Wilson, D.J., Feil, E., Eyre-Walker, A., 2018. The distribution
442 of bacterial doubling times in the wild. *Proceedings of the Royal Society*
443 *B: Biological Sciences* 285, 20180789.
- 444 Giverso, C., Preziosi, L., 2019. Influence of the mechanical properties of the
445 necrotic core on the growth and remodelling of tumour spheroids. *Inter-*
446 *national Journal of Non-Linear Mechanics* 108, 20–32.
- 447 Giverso, C., Scianna, M., Grillo, A., 2015. Growing avascular tumours as
448 elasto-plastic bodies by the theory of evolving natural configurations. *Mechanics Research Communications* 68, 31–39.
- 450 Grimes, D.R., Kelly, C., Bloch, K., Partridge, M., 2014. A method for
451 estimating the oxygen consumption rate in multicellular tumour spheroids.
452 *Journal of The Royal Society Interface* 11, 20131124.
- 453 Hanahan, D., Weinberg, R.A., 2011. Hallmarks of cancer: the next genera-
454 tion. *cell* 144, 646–674.
- 455 Hatzikirou, H., Alfonso, J.C.L., Leschner, S., Weiss, S., Meyer-Hermann,
456 M., 2017. Therapeutic potential of bacteria against solid tumors. *Cancer*
457 *research* 77, 1553–1563.
- 458 Jean, A.T.S., Swofford, C.A., Panteli, J.T., Brentzel, Z.J., Forbes, N.S., 2014.
459 Bacterial delivery of staphylococcus aureus α -hemolysin causes regression
460 and necrosis in murine tumors. *Molecular Therapy* 22, 1266–1274.
- 461 Kasinskas, R.W., Forbes, N.S., 2006. Salmonella typhimurium specifically
462 chemotax and proliferate in heterogeneous tumor tissue in vitro. *Biotech-*
463 *nology and bioengineering* 94, 710–721.
- 464 Kim, M., Gillies, R.J., Rejniak, K.A., 2013. Current advances in mathemat-
465 ical modeling of anti-cancer drug penetration into tumor tissues. *Frontiers*
466 *in oncology* 3, 278.

- 467 Kolokotroni, E.A., Dionysiou, D.D., Uzunoglu, N.K., Stamatakos, G.S.,
468 2011. Studying the growth kinetics of untreated clinical tumors by us-
469 ing an advanced discrete simulation model. *Mathematical and Computer*
470 *Modelling* 54, 1989–2006.
- 471 Kramer, M.G., Masner, M., Ferreira, F.A., Hoffman, R.M., 2018. Bacterial
472 therapy of cancer: Promises, limitations, and insights for future directions.
473 *Frontiers in Microbiology* 9, 16.
- 474 Landry, J., Freyer, J., Sutherland, R., 1982. A model for the growth of
475 multicellular spheroids. *Cell Proliferation* 15, 585–594.
- 476 Lewus, P., Ford, R.M., 2001. Quantification of random motility and chemo-
477 taxis bacterial transport coefficients using individual-cell and population-
478 scale assays. *Biotechnology and bioengineering* 75, 292–304.
- 479 Martínez-González, A., Calvo, G.F., Romasanta, L.A.P., Pérez-García,
480 V.M., 2012. Hypoxic cell waves around necrotic cores in glioblastoma:
481 a biomathematical model and its therapeutic implications. *Bulletin of*
482 *mathematical biology* 74, 2875–2896.
- 483 Mascheroni, P., Boso, D., Preziosi, L., Schrefler, B.A., 2017. Evaluating the
484 influence of mechanical stress on anticancer treatments through a multi-
485 phase porous media model. *Journal of theoretical biology* 421, 179–188.
- 486 Mascheroni, P., Carfagna, M., Grillo, A., Boso, D., Schrefler, B., 2018.
487 An avascular tumor growth model based on porous media mechanics and
488 evolving natural states. *Mathematics and Mechanics of Solids* 23, 686–712.
- 489 Mascheroni, P., Stigliano, C., Carfagna, M., Boso, D.P., Preziosi, L., Decuzzi,
490 P., Schrefler, B.A., 2016. Predicting the growth of glioblastoma multiforme
491 spheroids using a multiphase porous media model. *Biomechanics and mod-
492 eling in mechanobiology* 15, 1215–1228.
- 493 Matzavinos, A., Kao, C.Y., Green, J.E.F., Sutradhar, A., Miller, M., Fried-
494 man, A., 2009. Modeling oxygen transport in surgical tissue transfer.
495 *Proceedings of the National Academy of Sciences* 106, 12091–12096.
- 496 Michor, F., Beal, K., 2015. Improving cancer treatment via mathematical
497 modeling: surmounting the challenges is worth the effort. *Cell* 163, 1059–
498 1063.

- 499 Montel, F., Delarue, M., Elgeti, J., Malaquin, L., Basan, M., Risler, T., Ca-
500 bane, B., Vignjevic, D., Prost, J., Cappello, G., et al., 2011. Stress clamp
501 experiments on multicellular tumor spheroids. *Physical review letters* 107,
502 188102.
- 503 Osswald, A., Sun, Z., Grimm, V., Ampem, G., Riegel, K., Westendorf,
504 A.M., Sommergruber, W., Otte, K., Dürre, P., Riedel, C.U., 2015. Three-
505 dimensional tumor spheroids for in vitro analysis of bacteria as gene de-
506 livery vectors in tumor therapy. *Microbial cell factories* 14, 199.
- 507 Owen, M.R., Byrne, H.M., Lewis, C.E., 2004. Mathematical modelling of the
508 use of macrophages as vehicles for drug delivery to hypoxic tumour sites.
509 *Journal of theoretical biology* 226, 377–391.
- 510 PBCF, 2012. PBCF product guide. URL: [https://physics.cancer.gov/
511 docs/bioresource/brain/NCI-PBCF-HTB14_U-87_MG_SOP-508.pdf](https://physics.cancer.gov/docs/bioresource/brain/NCI-PBCF-HTB14_U-87_MG_SOP-508.pdf).
- 512 Pesavento, F., Schrefler, B.A., Sciumè, G., 2017. Multiphase flow in de-
513 forming porous media: a review. *Archives of Computational Methods in
514 Engineering* 24, 423–448.
- 515 Phaiboun, A., Zhang, Y., Park, B., Kim, M., 2015. Survival kinetics of
516 starving bacteria is biphasic and density-dependent. *PLoS computational
517 biology* 11, e1004198.
- 518 Preziosi, L., 2003. *Cancer modelling and simulation*. CRC Press.
- 519 Preziosi, L., Tosin, A., 2009. Multiphase modelling of tumour growth and ex-
520 tracellular matrix interaction: mathematical tools and applications. *Jour-
521 nal of mathematical biology* 58, 625.
- 522 Sarkar, S., Peng, C.C., Kuo, C.W., Chueh, D.Y., Wu, H.M., Liu, Y.H.,
523 Chen, P., Tung, Y.C., 2018. Study of oxygen tension variation within live
524 tumor spheroids using microfluidic devices and multi-photon laser scanning
525 microscopy. *RSC Advances* 8, 30320–30329.
- 526 Schaller, G., Meyer-Hermann, M., 2005. Multicellular tumor spheroid in an
527 off-lattice voronoi-delaunay cell model. *Physical Review E* 71, 051910.
- 528 Sciumè, G., Shelton, S., Gray, W.G., Miller, C.T., Hussain, F., Ferrari, M.,
529 Decuzzi, P., Schrefler, B., 2013. A multiphase model for three-dimensional
530 tumor growth. *New journal of physics* 15, 015005.

- 531 Siddique, J., Ahmed, A., Aziz, A., Khalique, C., 2017. A review of mixture
532 theory for deformable porous media and applications. *Applied Sciences* 7,
533 917.
- 534 Suh, S., Leaman, E., Zhan, Y., Behkam, B., 2018. Mathematical modeling of
535 bacteria-enabled drug delivery system penetration into multicellular tumor
536 spheroids, in: 2018 40th Annual International Conference of the IEEE
537 Engineering in Medicine and Biology Society (EMBC), IEEE. pp. 6162–
538 6165.
- 539 Sutherland, R.M., 1988. Cell and environment interactions in tumor microre-
540 gions: the multicell spheroid model. *Science* 240, 177–184.
- 541 Toley, B.J., Forbes, N.S., 2011. Motility is critical for effective distribution
542 and accumulation of bacteria in tumor tissue. *Integrative Biology* 4, 165–
543 176.
- 544 Torres, W., Lamed, V., Olivares, L.C., Navarro, C., Fuenmayor, J., Pérez, A.,
545 Mendiola, A., Rojas, M., Martínez, M.S., Velasco, M., et al., 2018. Bacteria
546 in cancer therapy: beyond immunostimulation. *J Cancer Metastasis Treat*
547 4, 4.
- 548 Vaupel, P., Mayer, A., 2007. Hypoxia in cancer: significance and impact on
549 clinical outcome. *Cancer and Metastasis Reviews* 26, 225–239.
- 550 Vinci, M., Gowan, S., Boxall, F., Patterson, L., Zimmermann, M., Lomas,
551 C., Mendiola, M., Hardisson, D., Eccles, S.A., et al., 2012. Advances
552 in establishment and analysis of three-dimensional tumor spheroid-based
553 functional assays for target validation and drug evaluation. *BMC biology*
554 10, 29.
- 555 Ward, J., King, J., 1999. Mathematical modelling of avascular-tumour
556 growth ii: modelling growth saturation. *Mathematical Medicine and Biol-*
557 *ogy: A Journal of the IMA* 16, 171–211.
- 558 Wilson, W.R., Hay, M.P., 2011. Targeting hypoxia in cancer therapy. *Nature*
559 *Reviews Cancer* 11, 393.
- 560 Zhou, S., Gravekamp, C., Bermudes, D., Liu, K., 2018. Tumour-targeting
561 bacteria engineered to fight cancer. *Nature Reviews Cancer* , 1.