Validating Minimally Invasive Laser Doppler Flowmetry for Serial Bone Perfusion Measurements in Mice

Nicholas J. Hanne^{a,1}, Elizabeth D. Easter^{b,1}, Jacqueline H. Cole^{a,*}

¹ These authors contributed equally to this work.

^a Joint Department of Biomedical Engineering, University of North Carolina, Chapel Hill, NC, and North Carolina State University, Raleigh, NC, USA

^b Materials Science and Engineering, North Carolina State University, Raleigh, NC, USA

*Corresponding Author:

Jacqueline H. Cole Joint Department of Biomedical Engineering University of North Carolina and North Carolina State University 911 Oval Drive Campus Box 7115 Raleigh, NC 27695-7115 Tel: 919-515-5955 Fax: 919-513-3814 jacquecole@ncsu.edu

Highlights

- Modified, minimally invasive laser Doppler flowmetry (LDF) technique was validated for serial measures of tibial perfusion in mice.
- Weekly LDF procedures did not induce inflammation or alter gait patterns that could confound metrics of interest in bone studies.
- Ligation of the femoral artery confirmed the LDF technique measures functional perfusion within the bone.

Abstract

In vivo laser Doppler flowmetry (LDF) has previously been used to quantify blood perfusion accurately at a single timepoint in the murine tibial metaphysis. However, this procedure entailed substantial disruption to soft tissues overlying the bone and caused notable localized inflammation for several weeks after the procedure, impeding serial measurements in the same mouse. In this study, we tested a less invasive technique to measure perfusion in the tibia with LDF and validated that it can be used serially in the same mouse without causing inflammation or gait perturbations. Twenty 14-week-old C57Bl/6J mice were evenly divided into groups that either had daily treadmill exercise or remained sedentary. Within these activity groups, mice were evenly subdivided into groups that received LDF measurements either weekly or only once at the study endpoint. Bone perfusion was measured with LDF in the anteromedial region of the right tibial metaphysis. Serum concentrations of interleukin 6, incision site wound area, and interlimb coordination during gait were measured weekly for four weeks. Tibial perfusion did not differ significantly between exercise and sedentary groups within the weekly or endpoint-only LDF groups at any timepoint. Perfusion was significantly increased in the third week in the weekly LDF group relative to measurements in the second and fourth weeks. Ligation of the femoral artery caused consistent, rapid reductions in tibial perfusion, validating that LDF is sensitive to changes in tibial blood supply. Weekly LDF procedures did not adversely affect gait, as interlimb coordination during treadmill locomotion was similar between weekly and endpoint-only LDF groups at every timepoint. Images of the incision site show wound closure within one week, and serum concentrations of interleukin 6 were not significantly different between weekly and endpoint-only groups. Together, these findings demonstrate that our minimally invasive LDF technique can be

used for serial *in vivo* measurements of intraosseous blood perfusion without inducing localized inflammation or negatively affecting gait patterns in mice.

Keywords:

laser Doppler flowmetry, bone blood perfusion, vascular supply, minimally invasive, serial measurement, in vivo

Abbreviations:

LDF – laser Doppler flowmetry

1 1. Introduction

2 Vasculature within bone (osteovasculature) is an essential contributor to bone health, providing nutrients, oxygen, cells, and chemical signals and removing waste products [1,2]. 3 Adequate vascular perfusion is required for bone development, adaptation in response to loading, 4 and healing after fracture [2–4]. Evidence that vascular pathologies are associated with bone loss 5 6 is growing. Aortic calcification is associated with decreased lumbar spine bone mineral density (BMD) and increased fracture risk in men and women within four years [5], and the incidence of 7 cardiovascular disease increases with reduced BMD in the spine in white men, and hip, trochanter, 8 9 and femoral neck in black women [6]. Osteoporosis is associated with reduced perfusion in the vertebrae for men [7] and in the femoral head for women [8], although the mechanisms responsible 10 for bone loss in these individuals is unknown and needs further examination using animal studies. 11 Although murine models are commonly used to determine the effect of pathologies on bone 12 properties, measuring blood perfusion within mouse bone is complicated due to their small size. 13 Current methods are either experimentally difficult (e.g., hydrogen washout [9]) or require the 14 animal to be sacrificed (e.g., microspheres, radiolabels, polyoxometalates, barium sulfate, or 15 Microfil[®] [10–16]). Some methods can be performed *in vivo* but provide poor resolution not 16 17 suitable for small bones: laser speckle imaging [17], laser Doppler perfusion imaging [18], contrast-enhanced magnetic resonance imaging (MRI) [19], contrast-enhanced positron emission 18 19 tomography (PET) [19], and contrast-enhanced micro-computed tomography [20,21]. Endpoint 20 and ex vivo measurements only provide a snapshot of vascular network function, missing the timing of vascular changes and any transient changes to vascular supply. A technique that could 21 22 be used for longitudinal studies of bone perfusion in vivo would enable us to capture temporal

changes in bone perfusion for individual subjects, thereby improving understanding of disease
progression and intervention effectiveness.

First proposed as a tool to measure intraosseous perfusion by Nilsson *et al.* in 1980 [22], 25 laser Doppler flowmetry (LDF) directs a monochromatic light source over a perfused tissue and 26 measures backscattered light from fluid movement with a photodetector to provide a relative 27 28 measure of blood perfusion. Perfusion is a functional measure of blood flow that is affected not only by the amount and velocity of red blood cells but also capillary density, vascular permeability, 29 and flow direction [23,24]. LDF was first used to measure blood perfusion in the cancellous bone 30 31 of pig mandibles by Hellem et al. in 1983 [25] and thereafter was rapidly adopted in orthopaedic clinics as an intraoperative tool to aid surgeons in identifying non-viable bone for debridement in 32 patients with osteomyelitis, osteonecrosis of the femoral head, and lower limb traumatic injury 33 [23]. LDF has also been used as an endpoint measure to compare relative intraosseous perfusion 34 between groups in murine research studies [26,27]. Recently, it was validated as a tool to quantify 35 perfusion in the mouse tibia, but the technique used in that study involved a relatively large incision 36 that resulted in inflammation at the incision site up to three months after the procedure [28]. To 37 monitor longitudinal changes in murine bone perfusion, a less invasive LDF procedure is needed 38 39 that will not induce significant localized inflammation or limping during gait, which could have both biological and mechanical confounding effects on bone. 40

We developed a minimally invasive LDF procedure and have used it to measure changes in tibial perfusion in mice in response to diet-induced obesity, ischemic stroke, and treadmill exercise [29,30]. The objective of this study was to determine if this modified LDF procedure could be performed repeatedly in a longitudinal study without affecting bone perfusion, inducing inflammation, or altering limb coordination during locomotion, which could confound bone 46 metrics of interest and perfusion changes associated with interventions. Developing new *in vivo* 47 techniques to measure bone blood perfusion is a critical step needed to understand longitudinal 48 changes to osteovasculature, which may contribute to bone loss occurring during progression of 49 various clinical pathologies.

50

51 **2. Materials and Methods**

52 2.1 Study design

The protocol for this study was approved by the Institutional Animal Care and Use 53 54 Committee at North Carolina State University. Eighteen 14-week-old male C57Bl/6J mice (The Jackson Laboratory, Bar Harbor, ME) were acclimated to the animal facility for one week. They 55 were group-housed (4 per cage) on a 12-hour light/12-hour dark diurnal cycle and provided chow 56 and water ad libitum. The mice were randomly assigned to four groups (Fig. 1) based on LDF 57 procedure frequency (weekly, endpoint) and exercise regimen (sedentary, exercise): weekly 58 sedentary (n = 5), weekly exercise (n = 5), endpoint sedentary (n = 4), and endpoint exercise (n = 5)59 4). Exercise groups were acclimated to treadmill exercise (Exer-3/6, Columbus Instruments, 60 Columbus, OH) by increasing exercise intensity for 2 days prior to the start of the study (Day 1: 5 61 m/min for 10 min, 9 m/min for 10 min, and 12 m/min for 10 min; Day 2: 5 m/min for 5 min, 9 62 m/min for 5 min, and 12 m/min for 20 min). During the study, exercise groups performed daily 63 exercise for 4 weeks (30 min/day, 5 days/week, 12 m/min, 5° incline), while sedentary groups 64 65 were placed on a stationary treadmill for the same amount of time to equalize handling among the 66 groups.

Laser Doppler flowmetry was used to measure intraosseous blood perfusion in the right tibial
metaphysis, performed either weekly for 4 weeks (weekly groups) or at a single timepoint at the

end of the study (endpoint groups). For the weekly LDF groups, starting in Week 2, images of the 69 incision site were taken during the LDF procedure prior to making an incision to assess the wound 70 from the previous week. Blood samples were collected from the submandibular vein of all mice 71 under anesthesia (at the end of the LDF procedure for the weekly groups). Blood samples were 72 centrifuged at 2,000 x g for 10 min, and the isolated serum was stored at -80°C until analysis with 73 74 an enzyme-linked immunosorbent assay (ELISA). At five days after each of the first three LDF procedures, gait patterns were assessed using high-speed video. Immediately following the last 75 LDF procedure and serum collection, mice were euthanized using CO₂ asphyxiation followed by 76 77 cervical dislocation.

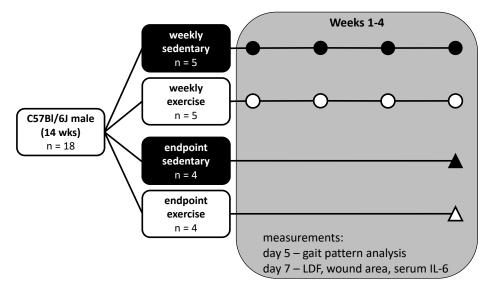


Figure 1. Experimental design. Symbols indicate weeks in which tibial perfusion was measured with LDF. Wound area, serum interleukin 6 (IL-6), and gait patterns were assessed weekly.

- 78
- 79
- 80 2.2 Tibial perfusion

All mice were fasted for 6-8 hours before each LDF procedure. Anesthesia was induced and maintained with isoflurane (2%) in pure oxygen throughout the procedure (about 15 minutes). After anesthesia induction, the fur over the right knee was shaved, mice were placed supine on a

heated pad, and the right leg was taped to the surgical platform. A 2-5-mm long incision was made 84 over the anteromedial surface of the right proximal tibial metaphysis, the bone was exposed, and 85 a small region of the periosteum was scraped away. LDF measurements were recorded using an 86 LDF monitor with a 785-nm light source (MoorVMS-LDF, Moor Instruments Ltd, Axminster, 87 UK), and a 3 kHz lowpass filter selected. A VP4 Needle Probe (0.8 mm outer diameter, 0.25 mm 88 89 fiber separation) was placed directly on the exposed bone surface (Fig. 2) and held in place using a micromanipulator (MM3-ALL, World Precision Instruments, Sarasota, FL) to reduce signal 90 noise from probe movement. Each weekly measurement was composed of the weighted mean and 91 standard deviation of three 30-second readings, with repositioning of the probe between readings. 92 The incisions were closed using VetBond™ tissue glue (3M Company, St. Paul, MN) and covered 93 with triple antibiotic cream. 94

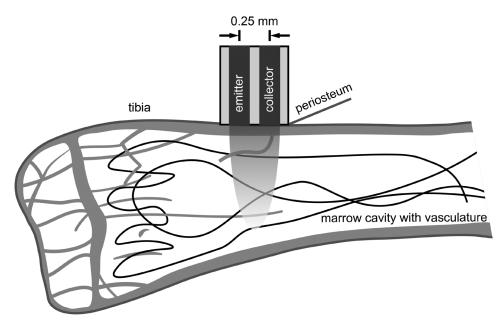


Figure 2. Schematic of LDF setup for bone perfusion measurements in the proximal tibia. The probe, placed on the tibial surface, emitted 785-nm light that scattered through a region of underlying tissue (represented by parabolic shading) and experienced Doppler shifts, some of which was scattered back to the collection probe, where it was measured.

96

97 2.3 Femoral ligation validation

At the end of the study, just prior to euthanasia, additional LDF measurements were 98 performed in a subset of mice (n=12) during arterial ligation to confirm the association of LDF 99 perfusion measurements with changes in blood supply to the bone. While still anesthetized during 100 the final LDF procedure, the skin incision over the proximal tibia was extended to expose the entire 101 102 inner thigh and the femoral artery. The LDF probe was again positioned over the tibial metaphysis, and a suture was tied around the femoral artery but not tightened. A 30-second baseline 103 measurement was taken, the suture was tightened to ligate the artery, and another 30-second 104 105 measurement was recorded. The reduction in tibial perfusion was calculated as the ratio of the ligated measurement to the baseline measurement, expressed as a percent. 106

107

108 2.4 Wound area

As mentioned above, for the weekly LDF groups, pictures were taken of the incision wounds immediately prior to each LDF procedure to assess localized inflammation and healing at the wound site from the procedure performed in the preceding week. Wound area was calculated by tracing the edge of the wound in ImageJ (version 1.51k, National Institutes of Health, Bethesda, MD). The wound was considered closed if no moist granulation tissue was visible and the wound was covered with new epithelium [31].

115

116 2.5 Serum concentration of interleukin 6

Systemic inflammation was examined by quantifying serum concentrations of the
proinflammatory marker interleukin 6 (IL-6) with an ELISA (IL-6 Mouse ELISA kit, KMC0061,
Invitrogen, Carlsbad, CA). Samples were prepared according to the manufacturer's instructions

and measured using a plate reader (Synergy H1, BioTek Instruments, Inc., Winooski, VT). Due to
limited serum, some samples were diluted 2-4 times to allow samples to be run in duplicate.

122

123 2.6 Gait pattern analysis

The effect of the LDF procedures on interlimb coordination was examined weekly in all 124 125 mice, five days after each procedure day, because limping or other gait asymmetries could alter the strain experienced by hindlimb bones and confound bone outcome measures [32]. During a 126 short treadmill session (12 m/min for 60 sec), high-speed video was collected in the sagittal plane 127 at 240 frames per second (HERO4, GoPro, Inc., San Mateo, CA). Gait was analyzed using Kinovea 128 (version 0.8, Kinovea Open Source Project) to quantify duty cycle for both hindlimbs and phase 129 dispersions for ipsilateral, diagonal, and contralateral limbs with relation to the LDF limb (right 130 hindlimb) (Fig. 3) [33–35]. Duty cycle for a given limb is the ratio of the time that limb is on the 131 ground (measured from paw strike to lift off) to the total time of an entire gait cycle (measured 132 from paw strike to paw strike). Phase dispersion between two limbs is a measure of the time 133 between paw strikes for those two limbs within a gait cycle. Five consecutive gait cycles were 134 analyzed for each treadmill session. Duty cycle and phase dispersion were averaged over the five 135 136 gait cycles at each timepoint.

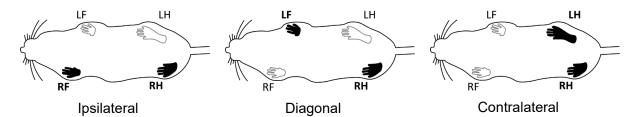


Figure 3. Schematic of the ipsilateral (RF-RH), diagonal (LF-RH), and contralateral (LH-RH) phase dispersions used for gait analysis. Relevant limbs relative to the LDF limb (RH) shaded in black. L=left, R=right, F=forelimb, H=hindlimb.

137

139 2.7 Statistical analysis

All data analyses were performed using SAS (SAS University Edition v. 9.4, SAS Institute 140 Inc., Cary, NC) with a significance level of 0.05. Models were chosen to answer five questions: 1) 141 Does performing weekly LDF procedures affect bone perfusion? To answer this question, LDF 142 data from the final timepoint (Week 4) were compared across LDF frequency (weekly, endpoint) 143 144 and exercise regimen (sedentary, exercise) using a two-way ANOVA with interaction. Tukey's post-hoc tests were used to compare group means. 2) Does exercise affect bone perfusion? For this 145 question, LDF data for the weekly group were compared across exercise regimen and timepoint 146 147 (Weeks 1-4) to examine differences between exercise groups within each timepoint (i.e., sedentary vs. exercise at Week 1). A mixed effects general linear model (procedure MIXED) with interaction 148 149 was used, with exercise group as a fixed factor and timepoint as a repeated factor. The covariance 150 matrix was modeled using compound symmetry. Exercise effect differences were calculated based on least squares means (LSM) with Tukey-Kramer adjustments for multiple comparisons. For the 151 endpoint-only group (Week 4 data), the effect of exercise was examined with one-way ANOVA. 152 3) Do weekly LDF procedures alter exercise effects on bone perfusion? Effect differences between 153 timepoints (i.e., Week 1 vs. Week 2) were evaluated in the same mixed effects model using LSM 154 155 with Tukey-Kramer adjustments for multiple comparisons. 4) Do LDF readings directly correspond to changes in blood supply, assessed by femoral artery ligation? LDF data before and 156 after the femoral artery was ligated were compared using a paired t-test. 5) Do weekly LDF 157 158 procedures alter gait and interlimb coordination? This question was addressed by comparing gait parameters between LDF groups within exercise groups and timepoints (i.e., weekly sedentary vs. 159 endpoint sedentary at Week 1). Four gait parameters were compared across LDF groups, exercise 160 161 groups, and timepoints (Weeks 2-4) with mixed effects linear models (procedure MIXED) with

interaction, where LDF frequency and exercise regimen were fixed factors and timepoint was a repeated measure. The covariance matrices were modeled using either compound symmetry (duty cycle, contralateral phase dispersion) or a first-order autoregressive (diagonal and ipsilateral phase dispersion), based on which covariance matrix yielded a lower corrected Akaike's Information Criterion. Effect differences were calculated based on LSM with Tukey-Kramer adjustments for multiple comparisons. All data are presented as mean \pm standard deviation, except LDF and gait data, which are presented as LSM \pm 95% confidence interval.

169

170 **3. Results**

171 3.1 Tibial perfusion

At Week 4, bone perfusion was similar between the weekly and endpoint-only groups (p = 172 173 0.92), showing that our modified LDF procedure can be performed weekly without affecting perfusion, the primary outcome of interest (Fig. 4). With weekly LDF procedures, treadmill 174 exercise did not affect perfusion measurements, compared to the sedentary group, at any timepoint 175 (p = 0.11 Week 1, p = 0.64 Week 2, p = 0.76 Week 3, and p = 0.78 Week 4). Similarly, with 176 endpoint-only LDF procedures, perfusion also did not differ significantly between exercise and 177 sedentary groups at Week 4 (p = 0.49), suggesting weekly LDF procedures did not mask an 178 exercise effect on perfusion. Perfusion was higher in Week 3 compared to Weeks 2 and 4, 179 180 indicating that the technique is sensitive to transient perfusion changes regardless of exercise.

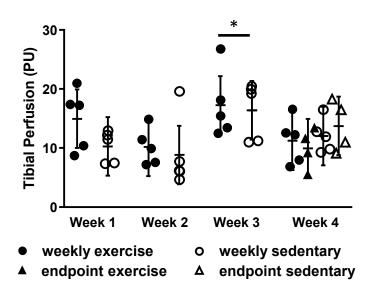


Figure 4. At Week 4, tibial perfusion was similar between weekly and endpoint-only groups. Sedentary and exercise groups had similar perfusion at every timepoint. LDF was sensitive to transient perfusion changes, measuring higher in Week 3 compared to Week 2 and Week 4. PU = perfusion units. Data presented as least squares mean \pm 95% confidence interval. *p < 0.05 vs. Weeks 2 and 4.

181

- 183 3.2 Femoral ligation validation
- After the femoral artery was ligated, perfusion in the tibia dropped rapidly from 15.3 ± 9.2
- perfusion units (PU) to 3.8 ± 1.4 PU within 30 seconds ($31 \pm 19\%$ of the baseline perfusion, p =
- 186 0.004) (Fig. 5), validating that the LDF perfusion measurements are directly associated with blood
- 187 supply within the bone. Two measurements were not included in the analysis, because the LDF
- 188 probe slipped off the tibia when the ligature was tightened.

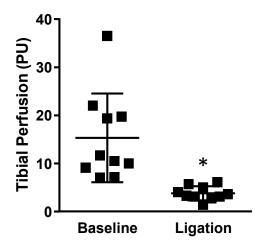


Figure 5. After ligation of the femoral artery, tibial perfusion dropped to $31 \pm 19\%$ of the baseline value. PU = perfusion units. *p < 0.05 vs. baseline.

190

189

191 3.3 Wound area

Wound images taken one week after each weekly LDF procedure showed minimal signs of inflammation for all but one incision for both exercise and sedentary mice, with either full closure (Fig. 6A) or a small, dry scab (Fig. 6B) resulting in zero wound area recorded. Wet granulation tissue was observed in only one incision site, for a sedentary mouse in Week 2 (Fig. 6C, wound area = 0.39 mm^2), and the wound was healed within the subsequent week.

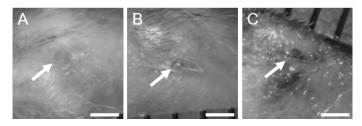
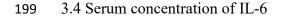


Figure 6. Example images of the incision wound site (arrows) from the weekly LDF group taken one week following the procedure. Incisions were either A) fully closed or B) closed with small, dry granulation tissue. C) Only one incision did not fully heal, but it was healed by the following week. Scale bars are 1 mm.

197



200 Circulating levels of proinflammatory marker IL-6 were below the detectable limit for all animals at each timepoint, except one mouse in the endpoint sedentary group at Week 4 (52.1 pg/mL). 201 Since the lower threshold of the test is 7.8 pg/mL, and serum samples were diluted up to four times 202 to allow for duplicate measurements, serum levels of IL-6 were below 31.2 pg/mL. These levels 203 204 agree with normal physiologic concentrations of IL-6, which are below 100 pg/mL in C57Bl/6J 205 mice [36,37], suggesting the mice in our study experienced little to no systemic inflammation in response to the weekly LDF procedures. Pathologic inflammation can increase IL-6 levels up to 206 200-1,000 pg/mL [36,37] 207

208

209 3.5 Gait pattern analysis

Weekly LDF procedures did not affect gait parameters during treadmill locomotion. Limb coordination did not differ between weekly and endpoint-only groups at any timepoint for either sedentary or exercise groups (Fig. 7). Sedentary groups did have small alterations in gait parameters in Week 2 compared to exercise groups (hindlimb duty cycle and diagonal and contralateral phase dispersion), possibly indicating slight discomfort or unfamiliarity with treadmill locomotion. Diagonal phase dispersion was lower in exercise mice compared to sedentary during Week 4 (8.6% lower, p = 0.012).

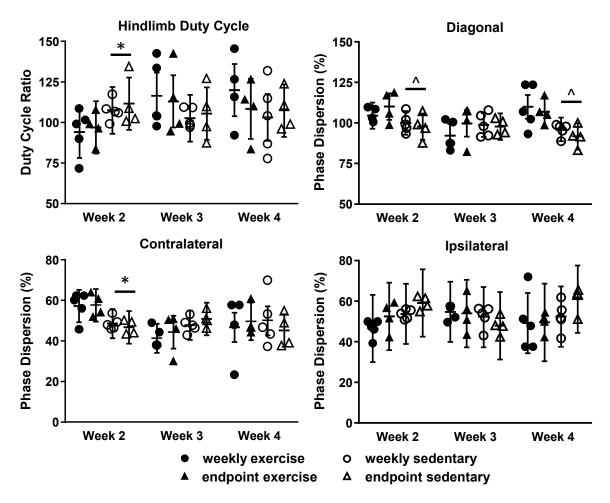


Figure 7. Treadmill locomotion patterns involving the LDF affected limb (right hindlimb). Gait patterns were not significantly different between weekly and endpoint-only groups at any timepoint for hindlimb duty cycle ratio (A), diagonal phase dispersion (B), contralateral phase dispersion (C), or ipsilateral phase dispersion (D). Diagonal and contralateral phase dispersion were lower in exercise than sedentary groups at some timepoints. Data are presented as least squares mean \pm 95% confidence interval. *p < 0.05 vs. sedentary. ^ p = 0.066 vs. sedentary.

218

219

220 **4. Discussion**

Our minimally invasive laser Doppler flowmetry technique measured *in vivo* intraosseous perfusion in the tibia weekly without inducing localized or systemic inflammation. LDF measures of tibial perfusion were similar between groups that received weekly procedures and groups that received only an endpoint procedure, indicating that the procedure itself did not impact measurements of intraosseous perfusion. A previous study demonstrated that LDF could be used

to quantify blood perfusion in murine tibiae but noted that signs of inflammation were observed at 226 the incision site up to three months following the procedure and suggested that it be used as an 227 endpoint-only measure to avoid influencing bone outcomes [28]. In this study, we limited the 228 invasiveness of the procedure by reducing the incision size and preserving muscle tissue, thereby 229 enabling repeated measurements to be performed without causing chronic increases in 230 231 proinflammatory marker IL-6. Furthermore, all but one incision from the procedures were fully closed within the one-week period before the next procedure, and no visual signs of inflammation 232 were observed throughout the study. The fast healing times observed in the small incisions from 233 234 this procedure (approximately 1 mm) are consistent with wound closure studies, where even large (9-28 mm²), unclosed dermal biopsies heal in 7-14 days [38]. 235

The femoral ligation test confirmed that LDF measures are sensitive to changes in blood 236 supply and thus are directly related to perfusion within the underlying cortical bone and marrow 237 space. We demonstrated that femoral artery ligation reliably decreased the measured perfusion to 238 about 3.8 PU (31% of baseline) within 30 seconds in all mice. Cortical thickness in the tibia affects 239 the depth into the marrow space that LDF can measure. Another study quantified this relationship 240 in the murine tibia and found that small variations in cortical thickness had minimal effect on LDF 241 242 perfusion measurements [28], suggesting that LDF can be used to track longitudinal changes in bone perfusion. Because cortical thickness in the tibial diaphysis changes by ~10% from skeletal 243 maturity at 16 weeks of age to 52 weeks of age [39], and can differ by sex [40], longitudinal LDF 244 245 measurements should only be performed in age- and sex-matched subjects. Finally, we found no interaction effect of daily treadmill exercise on LDF readings. Taken together, these results suggest 246 247 that the minimally invasive LDF procedure validated in our study can be used to monitor and 248 compare blood perfusion longitudinally in murine studies involving exercise therapy. This

procedure can be used to track changes to osteovascular function, which is known to play animportant role in bone development, remodeling, and repair [41,42], yet remains under-studied.

In addition to providing aerobic exercise, treadmill activity also mechanically loads the bones 251 and increases the functional strain experienced by the bones [43-45]. Even slight changes to 252 functional strain can affect osteogenesis [32,46] and angiogenesis [15,47]. Since other studies have 253 254 shown that changes to gait kinematics and limb patterning affect bone strain [44,48], we were concerned the LDF procedure could affect locomotion patterns and confound exercise effects by 255 altering functional strain. We found no differences in duty cycle or interlimb coordination between 256 257 weekly and endpoint-only groups at any timepoint, indicating that weekly LDF measurements do not alter gait patterns (and thus functional strain) during treadmill exercise. 258

Although not the main focus of this study, aerobic treadmill exercise was anticipated to cause 259 260 increased tibial perfusion over time due to vascular growth and adaptation, as we have previously found in studies using the same exercise regimen and LDF technique [29,30]. Perfusion is a 261 functional measure of not only the amount and direction of blood flow but also vascular 262 permeability and capillary density [24]. Treadmill exercise may be affecting the size, number, or 263 cellular makeup of the vasculature without causing changes in perfusion. Rats that performed a 264 similar treadmill routine for two weeks had a 19% increase in the number but not total area of 265 blood vessels in the proximal tibial metaphysis compared to the sedentary group [15]. A more 266 rigorous aerobic exercise intervention, such as free access to running wheels where mice will run 267 268 4-10 km daily [49,50], may have a larger and more detectible effect on perfusion. Nevertheless, our study confirmed that weekly LDF procedures will not confound perfusion measurements in 269 future exercise studies. 270

271 Stress, like inflammation and aerobic exercise, can also affect vascular function. Neuropeptide Y, which is expressed during stress response, has been shown to be both angiogenic 272 and vasoconstrictive, which could increase blood pressure and the amount of vasculature in bone 273 [51]. Although we found no detectible increases in IL-6 or visible signs of inflammation at the 274 incision site, both sedentary and exercise mice had a significant increase in tibial perfusion in the 275 276 third week that was resolved by the fourth week. Stress may have played a role in increasing perfusion in the third week; all mice were handled daily for either treadmill exercise or the 277 sedentary treadmill activity and had blood drawn weekly which could induce a stress response. 278 279 The increased perfusion lasted only one week and was present in both exercise and sedentary mice. This study had several limitations that warrant attention in future studies. A primary 280 concern of this technique is the removal of a small area of the periosteum, a highly vascularized 281 282 tissue that contains osteoblast precursor cells [52]. LDF measures of intracortical perfusion in the tibiae of juvenile ewes dropped by 25% immediately following the removal of the periosteum from 283 the medial aspect [53]. Although the amount of periosteum removed in our procedure is small 284 (about the size of our probe, 0.5 mm² area), the effects of periosteal removal were not examined 285 and may affect bone tissue function. The effects of weekly LDF procedures on bone remodeling 286 and homeostasis were not examined in this study. This study did not compare LDF results to other 287 promising emerging techniques for examining osteovasculature in vivo. Several new higher 288 resolution PET scans can be used in rodent bones [54], and emerging MRI techniques (e.g., blood 289 290 oxygen level-dependent MRI and intravoxel incoherent motion MRI [24]) greatly improve resolution and do not require contrast agents, but these techniques remain prohibitively expensive. 291 292

293 5. Conclusions

Weekly LDF procedures performed over four weeks did not induce measurable signs of inflammation or significantly alter gait patterns during treadmill exercise. Unlike other existing methods used for measuring the vascular network in bone, this procedure can be performed *in vivo*, is repeatable without confounding study controls, is relatively simple to perform, and is inexpensive. Monitoring intraosseous perfusion serially with LDF provides a functional measure of blood flow, enabling researchers to track changes to the osteovasculature noninvasively during disease progression and interventions.

301

302 Acknowledgments

This work was supported by the Eunice Kennedy Shriver National Institute of Child Health and Human Development (NICHD) of the National Institutes of Health (NIH) under award number K12HD073945. Additional support was provided by the Office of Undergraduate Research at North Carolina State University.

307

308 Declaration of interest

309 None

310

311 Role of the funding source

The funding sources had no involvement in study design; in the collection, analysis, and interpretation of data; in the writing of the report; or in the decision to submit the article for publication. The content is solely the responsibility of the authors and does not necessarily represent the official views of the National Institutes of Health.

316 **References**

317 [1] A.M. Parfitt, The mechanism of coupling: a role for the vasculature, Bone. 26 (2000) 319–

318 323. doi:10.1016/S8756-3282(00)80937-0.

- 319 [2] J. Trueta, The Role of the Vessels in Osteogenesis, Bone Joint J. 45-B (1963) 402–418.
- 320 [3] R.E. Tomlinson, J.A. McKenzie, A.H. Schmieder, G.R. Wohl, G.M. Lanza, M.J. Silva,
- Angiogenesis is Required for Stress Fracture Healing in Rats, Bone. 52 (2013) 212–219.
 doi:10.1016/j.bone.2012.09.035.
- 323 [4] A.L. Wallace, E.R.C. Draper, R.K. Strachan, I.D. Mccarthy, S.P.F. Hughes, The effect of
- devascularisation upon early bone healing in dynamic external fixation, Bone Joint J. 73
 (1991) 819–825.
- M. Naves, M. Rodríguez-García, J.B. Díaz-López, C. Gómez-Alonso, J.B. Cannata-Andía,
 Progression of vascular calcifications is associated with greater bone loss and increased
- bone fractures, Osteoporos Int. 19 (2008) 1161–1166. doi:10.1007/s00198-007-0539-1.
- 329 [6] G.N. Farhat, A.B. Newman, K. Sutton-Tyrrell, K.A. Matthews, R. Boudreau, A.V.
- 330 Schwartz, T. Harris, F. Tylavsky, M. Visser, J.A. Cauley, for the H.A. Study, The
- association of bone mineral density measures with incident cardiovascular disease in older
- adults, Osteoporos Int. 18 (2007) 999–1008. doi:10.1007/s00198-007-0338-8.
- 333 [7] J.F. Griffith, D.K.W. Yeung, G.E. Antonio, F.K.H. Lee, A.W.L. Hong, S.Y.S. Wong,
- E.M.C. Lau, P.C. Leung, Vertebral Bone Mineral Density, Marrow Perfusion, and Fat
- 335 Content in Healthy Men and Men with Osteoporosis: Dynamic Contrast-enhanced MR
- Imaging and MR Spectroscopy, Radiology. 236 (2005) 945–951.
- doi:10.1148/radiol.2363041425.

- 338 [8] J.F. Griffith, D.K. Yeung, P.H. Tsang, K.C. Choi, T.C. Kwok, A.T. Ahuja, K.S. Leung,
- 339P.C. Leung, Compromised Bone Marrow Perfusion in Osteoporosis, J Bone Miner Res. 23
- 340 (2008) 1068–1075. doi:10.1359/jbmr.080233.
- 341 [9] L.A. Whiteside, P.A. Lesker, D.J. Simmons, Measurement of Regional Bone and Bone
- 342 Marrow Blood Flow in the Rabbit Using the Hydrogen Washout Technique, Clin. Orthop.
- 343 Relat. Res. 122 (1977) 340–346.
- [10] M.A. Serrat, Measuring bone blood supply in mice using fluorescent microspheres, Nat.
 Protoc. 4 (2009) 1779–58. doi:http://dx.doi.org/10.1038/nprot.2009.190.
- [11] O. Grundnes, O. Reikerås, Blood flow and mechanical properties of healing bone, Acta
- 347 Orthop. Scand. 63 (1992) 487–491. doi:10.3109/17453679209154720.
- 348 [12] J. Reeve, M. Arlot, R. Wootton, C. Edouard, M. Tellez, R. Hesp, J.R. Green, P.J. Meunier,
- 349 Skeletal Blood Flow, Iliac Histomorphometry, and Strontium Kinetics in Osteoporosis: A
- 350 Relationship Between Blood Flow and Corrected Apposition Rate, J. Clin. Endocrin. &
- 351 Metab. 66 (1988) 1124–1131. doi:10.1210/jcem-66-6-1124.
- 352 [13] G. Kerckhofs, S. Stegen, N. van Gastel, A. Sap, G. Falgayrac, G. Penel, M. Durand, F.P.
- 353 Luyten, L. Geris, K. Vandamme, T. Parac-Vogt, G. Carmeliet, Simultaneous three-
- dimensional visualization of mineralized and soft skeletal tissues by a novel microCT
- contrast agent with polyoxometalate structure, BIomater. 159 (2018) 1–12.
- doi:10.1016/j.biomaterials.2017.12.016.
- 357 [14] O. Barou, S. Mekraldi, L. Vico, G. Boivin, C. Alexandre, M.H. Lafage-Proust,
- 358 Relationships between trabecular bone remodeling and bone vascularization: a quantitative
- study, Bone. 30 (2002) 604–612. doi:10.1016/S8756-3282(02)00677-4.

- 360 [15] Z. Yao, M.-H. Lafage-Proust, J. Plouët, S. Bloomfield, C. Alexandre, L. Vico, Increase of
- 361 Both Angiogenesis and Bone Mass in Response to Exercise Depends on VEGF, J Bone

362 Miner Res. 19 (2004) 1471–1480. doi:10.1359/JBMR.040517.

- 363 [16] J.D. Boerckel, B.A. Uhrig, N.J. Willett, N. Huebsch, R.E. Guldberg, Mechanical regulation
- of vascular growth and tissue regeneration in vivo, Proc. Natl. Acad. Sci. USA. 108 (2011)
- 365 E674–E680. doi:10.1073/pnas.1107019108.
- 366 [17] D. Briers, D.D. Duncan, E.R. Hirst, S.J. Kirkpatrick, M. Larsson, W. Steenbergen, T.
- 367 Stromberg, O.B. Thompson, Laser speckle contrast imaging: theoretical and practical
- 368 limitations, J. Biomed. Opt. 18 (2013) 066018. doi:10.1117/1.JBO.18.6.066018.
- 369 [18] B. Roche, V. David, A. Vanden-Bossche, F. Peyrin, L. Malaval, L. Vico, M.-H. Lafage-
- Proust, Structure and quantification of microvascularisation within mouse long bones: What
 and how should we measure?, Bone. 50 (2012) 390–399. doi:10.1016/j.bone.2011.09.051.
- [19] J.P. Dyke, R.K. Aaron, Noninvasive methods of measuring bone blood perfusion, Ann.
- 373 N.Y. Acad. Sci. 1192 (2009) 95–102. doi:10.1111/j.1749-6632.2009.05376.x.
- 374 [20] J.T. Au, G. Craig, V. Longo, P. Zanzonico, M. Mason, Y. Fong, P.J. Allen, Gold
- 375 Nanoparticles Provide Bright Long-Lasting Vascular Contrast for CT Imaging, Am. J.

376 Roentgenol. 200 (2013) 1347–1351. doi:10.2214/AJR.12.8933.

- 377 [21] D.P. Clark, K. Ghaghada, E.J. Moding, D.G. Kirsch, C.T. Badea, In vivo characterization
- of tumor vasculature using iodine and gold nanoparticles and dual energy micro-CT, Phys.
- 379 Med. Biol. 58 (2013) 1683. doi:10.1088/0031-9155/58/6/1683.
- 380 [22] G.E. Nilsson, T. Tenland, P.A. Oberg, Evaluation of a Laser Doppler Flowmeter for
- 381 Measurement of Tissue Blood Flow, IEEE T. Biomed. Eng. BME-27 (1980) 597–604.
- doi:10.1109/TBME.1980.326582.

- [23] M.F. Swiontkowski, Laser Doppler Flowmetry—Development and Clinical Application,
 Iowa Orthop. J. 11 (1991) 119–126.
- 385 [24] J.F. Griffith, Imaging vasculature of bone, Journal of Orthopaedic Translation. 4 (2014)
- 386 192. doi:10.1016/j.jot.2014.07.106.
- 387 [25] S. Hellem, L.S. Jacobsson, G.E. Nilsson, D.H. Lewis, Measurement of microvascular blood
- flow in cancellous bone using laser Doppler flowmetry and 133Xe-clearance, Int. J. Oral
- 389 Surg. 12 (1983) 165–177. doi:10.1016/S0300-9785(83)80063-5.
- 390 [26] P. Okunieff, X. Wang, P. Rubin, J.N. Finkelstein, L.S. Constine, I. Ding, Radiation-induced
- changes in bone perfusion and angiogenesis, Int. J. Radiat. Oncol. 42 (1998) 885–889.
- doi:10.1016/S0360-3016(98)00339-3.
- 393 [27] M. Melnyk, T. Henke, L. Claes, P. Augat, Revascularisation during fracture healing with
 394 soft tissue injury, Arch Orthop Trauma Surg. 128 (2008) 1159–1165. doi:10.1007/s00402395 007-0543-0.
- 396 [28] B. Roche, A. Vanden-Bossche, M. Normand, L. Malaval, L. Vico, M.-H. Lafage-Proust,
- 397 Validated Laser Doppler protocol for measurement of mouse bone blood perfusion —
- Response to age or ovariectomy differs with genetic background, Bone. 55 (2013) 418–426.
- doi:10.1016/j.bone.2013.03.022.
- 400 [29] N.J. Hanne, A.J. Steward, E.D. Easter, S.V. Pinnamaraju, J.H. Jacqueline H, Diet-Induced
- 401 Obesity Deteriorates Cancellous Bone Structure Despite Increased Blood Perfusion,
- 402 Orthopaedic Research Society Annual Meeting, San Diego, CA, March 19-22, 2017. Poster
- 403 #1699.

- 404 [30] N.J. Hanne, A.J. Steward, S.V. Pinnamaraju, S.D. Teeter, J.H. Cole, Exercise Therapy
- 405 Mitigates Reductions in Tibial Blood Flow during Acute Stroke Recovery, Orthopaedic
- 406 Research Society Annual Meeting, San Diego, CA, March 19-22, 2017. Paper #0337.
- 407 [31] M.T. Goova, J. Li, T. Kislinger, W. Qu, et al, Blockade of receptor for advanced blycation
- 408 end-products restores effective wound healing in diabetic mice, Am. J. Pathol. 159 (2001)
- 409 513–25.
- 410 [32] H.M. Frost, Bone's Mechanostat: A 2003 Update, Anat. Rec. 275A (2003) 1081–1101.
 411 doi:10.1002/ar.a.10119.
- 412 [33] H. Leblond, M. L'Espérance, D. Orsal, S. Rossignol, Treadmill Locomotion in the Intact
- 413 and Spinal Mouse, J. Neurosci. 23 (2003) 11411–11419.
- 414 [34] A.D. Kloos, L.C. Fisher, M.R. Detloff, D.L. Hassenzahl, D.M. Basso, Stepwise motor and
- 415 all-or-none sensory recovery is associated with nonlinear sparing after incremental spinal
- 416 cord injury in rats, Experimental Neurology. 191 (2005) 251–265.
- 417 doi:10.1016/j.expneurol.2004.09.016.
- 418 [35] E. Redondo-Castro, A. Torres-Espín, G. García-Alías, X. Navarro, Quantitative assessment
- 419 of locomotion and interlimb coordination in rats after different spinal cord injuries, J.

420 Neurosci. Methods. 213 (2013) 165–178. doi:10.1016/j.jneumeth.2012.12.024.

- 421 [36] S. Amar, Q. Zhou, Y. Shaik-Dasthagirisaheb, S. Leeman, Diet-Induced Obesity in Mice
- 422 Causes Changes in Immune Responses and Bone Loss Manifested by Bacterial Challenge,
- 423 Proceedings of the National Academy of Sciences of the United States of America. 104
- 424 (2007) 20466–20471.
- 425 [37] M. da S. Krause, A. Bittencourt, P.I.H. de Bittencourt, N.H. McClenaghan, P.R. Flatt, C.
- 426 Murphy, P. Newsholme, Physiological concentrations of interleukin-6 directly promote

427		insulin secretion, signal transduction, nitric oxide release, and redox status in a clonal
428		pancreatic β -cell line and mouse islets, Journal of Endocrinology. 214 (2012) 301–311.
429		doi:10.1530/JOE-12-0223.
430	[38]	K.T. Keylock, V.J. Vieira, M.A. Wallig, L.A. DiPietro, M. Schrementi, J.A. Woods,
431		Exercise accelerates cutaneous wound healing and decreases wound inflammation in aged
432		mice, A. J. PhysiolReg. I. 294 (2008) R179–R184. doi:10.1152/ajpregu.00177.2007.
433	[39]	V.L. Ferguson, R.A. Ayers, T.A. Bateman, S.J. Simske, Bone development and age-related
434		bone loss in male C57BL/6J mice, Bone. 33 (2003) 387-398. doi:10.1016/S8756-
435		3282(03)00199-6.
436	[40]	J.M. Somerville, R.M. Aspden, K.E. Armour, K.J. Armour, D.M. Reid, Growth of
437		C57BL/6 mice and the material and mechanical properties of cortical bone from the tibia,
438		Calcif. Tissue Int. 74 (2004) 469–475. doi:10.1007/s00223-003-0101-x.
439	[41]	S.C. Marks, P.R. Odgren, Chapter 1 - Structure and Development of the Skeleton, in: J.P.
440		Bilezikian, L.G. Raisz, G.A. Rodan (Eds.), Principles of Bone Biology (Second Edition),
441		Academic Press, San Diego, 2002: pp. 3–15. doi:10.1016/B978-012098652-1.50103-7.
442	[42]	HP. Gerber, T.H. Vu, A.M. Ryan, J. Kowalski, Z. Werb, N. Ferrara, VEGF couples
443		hypertrophic cartilage remodeling, ossification and angiogenesis during endochondral bone
444		formation, Nat Med. 5 (1999) 623-628. doi:10.1038/9467.
445	[43]	J.M. Wallace, R.M. Rajachar, M.R. Allen, S.A. Bloomfield, P.G. Robey, M.F. Young, D.H.
446		Kohn, Exercise-induced changes in the cortical bone of growing mice are bone- and
447		gender-specific, Bone. 40 (2007) 1120-1127. doi:10.1016/j.bone.2006.12.002.

- 448 [44] J. Prasad, B.P. Wiater, S.E. Nork, S.D. Bain, T.S. Gross, Characterizing gait induced
- 449 normal strains in a murine tibia cortical bone defect model, J. Biomech. 43 (2010) 2765–
- 450 2770. doi:10.1016/j.jbiomech.2010.06.030.
- 451 [45] A.G. Berman, M.J. Hinton, J.M. Wallace, Treadmill running and targeted tibial loading
- differentially improve bone mass in mice, Bone Rep. 10 (2019).
- 453 doi:10.1016/j.bonr.2019.100195.
- 454 [46] R. Ellman, J. Spatz, A. Cloutier, R. Palme, B.A. Christiansen, M.L. Bouxsein, Partial
- 455 reductions in mechanical loading yield proportional changes in bone density, bone
- 456 architecture, and muscle mass, J. Bone. Miner. Res. 28 (2013) 875–885.
- 457 doi:10.1002/jbmr.1814.
- 458 [47] A.J. Steward, J.H. Cole, F.S. Ligler, E. Loboa, Mechanical and Vascular Cues
- 459 Synergistically Enhance Osteogenesis in Human Mesenchymal Stem Cells, Tissue Eng.
- 460 Part A. (2016). doi:10.1089/ten.TEA.2015.0533.
- 461 [48] D.E. Hurwitz, D.R. Sumner, T.P. Andriacchi, D.A. Sugar, Dynamic knee loads during gait
- 462 predict proximal tibial bone distribution, J. Biomech. 31 (1998) 423–430.
- 463 doi:10.1016/S0021-9290(98)00028-1.
- 464 [49] K. Gertz, J. Priller, G. Kronenberg, K.B. Fink, B. Winter, H. Schröck, S. Ji, M. Milosevic,
- 465 C. Harms, M. Böhm, U. Dirnagl, U. Laufs, M. Endres, Physical Activity Improves Long-
- 466 Term Stroke Outcome via Endothelial Nitric Oxide Synthase–Dependent Augmentation of
- 467 Neovascularization and Cerebral Blood Flow, Circ. Res. 99 (2006) 1132–1140.
- 468 doi:10.1161/01.RES.0000250175.14861.77.
- 469 [50] M. Styner, G.M. Pagnotti, C. McGrath, X. Wu, B. Sen, G. Uzer, Z. Xie, X. Zong, M.A.
- 470 Styner, C.T. Rubin, J. Rubin, Exercise Decreases Marrow Adipose Tissue Through β-

- 471 Oxidation in Obese Running Mice, J Bone Miner Res. 32 (2017) 1692–1702.
- 472 doi:10.1002/jbmr.3159.
- 473 [51] L.E. Kuo, Z. Zukowska, Stress, NPY and vascular remodeling: Implications for stress-
- 474 related diseases, Peptides. 28 (2007) 435–440. doi:10.1016/j.peptides.2006.08.035.
- 475 [52] C. Colnot, X. Zhang, M.L.K. Tate, Current insights on the regenerative potential of the
- 476 periosteum: Molecular, cellular, and endogenous engineering approaches, J. Orthop. Res.
- 477 30 (2012) 1869–1878. doi:10.1002/jor.22181.
- 478 [53] M.J. Kowalski, E.H. Schemitsch, P.J. Kregor, D. Senft, M.F. Swiontkowski, Effect of
- 479 periosteal stripping on cortical bone perfusion: A laser doppler study in sheep, Calcif.
- 480 Tissue Int. 59 (1996) 24–26. doi:10.1007/s002239900080.
- 481 [54] R.E. Tomlinson, M.J. Silva, K.I. Shoghi, Quantification of Skeletal Blood Flow and
- Fluoride Metabolism in Rats using PET in a Pre-Clinical Stress Fracture Model, Mol.
- 483 Imaging Biol. 14 (2012) 348–354. doi:10.1007/s11307-011-0505-3.