

1 Growing old too early, automated 2 assessment of skeletal muscle single 3 fiber biomechanics in ageing R349P 4 desmin knock-in mice using the 5 *MyoRobot* technology

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27
28 **Abstract** Muscle biomechanics is determined by active motor-protein assembly and passive
29 strain transmission through cytoskeletal structures. The extrasarcomeric desmin filament network
30 aligns myofibrils at the z-discs, provides nuclear-sarcolemmal anchorage and may also serve as
31 memory for muscle repositioning following large strains. Our previous analyses of R349P desmin
32 knock-in mice, an animal model for the human R350P desminopathy, already depicted pre-clinical
33 changes in myofibrillar arrangement and increased fiber bundle stiffness compatible with a
34 pre-aged phenotype in the disease. Since the specific effect of R349P desmin on axial
35 biomechanics in fully differentiated muscle fibers is unknown, we used our automated *MyoRobot*
36 biomechatronics platform to compare passive and active biomechanics in single fibers derived
37 from fast- and slow-twitch muscles from adult to senile mice hetero- or homozygous for this
38 desmin mutation with wild-type littermates. Experimental protocols involved caffeine-induced

39 Ca²⁺-mediated force transients, pCa-force curves, resting length-tension curves, visco-elasticity and
40 'slack-tests'. We demonstrate that the presence of R349P desmin predominantly increased single
41 fiber axial stiffness in both muscle types with a pre-aged phenotype over wild-type fibers. Axial
42 viscosity was unaffected. Likewise, no systematic changes in Ca²⁺-mediated force properties were
43 found. Notably, mutant single fibers showed faster unloaded shortening over wild-type fibers.
44 Effects of ageing seen in the wild-type always appeared earlier in the mutant desmin fibers.
45 Impaired R349P desmin muscle biomechanics is clearly an effect of a compromised intermediate
46 filament network rather than secondary to fibrosis.

47

48 Introduction

49 Skeletal muscle is the largest organ system of the body and under constant mechanical stress, either
50 due to passive strain or through active contraction producing axial and lateral stresses. While lateral
51 forces are distributed between single fibers across anchorage points in the extracellular matrix
52 (ECM) to the intracellular cytoskeleton via the dystrophin-glycoprotein complex (DGC) *Ramaswamy*
53 *et al. (2011)* and focal adhesion complexes *Ra et al. (1999)*, axial forces are distributed through
54 contractile (active) and non-contractile (passive) elements. Apart from the giant, roughly 1.5 μm
55 long elastomeric protein titin, being responsible for the visco-elastic properties of single muscle
56 fibers through unfolding of globular domains under strain *Mártonfalvi and Kellermayer (2014)*;
57 *Powers et al. (2018)*, connecting proteins of the extra-sarcomeric intermediate filament (IF) family
58 may also be a vital determinant of axial elasticity. An important member of the IFs is the type
59 III filament protein desmin, transversely linking adjacent myofibrils at the level of the z-disc and
60 thus, being responsible for myofibrillar register *Waterman-Storer (1991)*; *Anderson et al. (2001)*;
61 *Meyer et al. (2010)*. In humans, desmin is encoded on chromosome 2q35 by a single copy gene.
62 The 53 kDa desmin presents a tripartite structure with a central-helical coiled-coil domain flanked
63 by non-helical tail and head domains. Due to its intrinsic self-assembling properties, it builds
64 three-dimensional networks, starting with supercoil formation via dimerization of two desmin
65 molecules. Two such dimers then associate into tetramers that represent the repetitive add-on
66 units for spontaneous assembly of 60 nm long filaments, the so-called unit-length filaments (ULFs,
67 *Clemen et al. (2013)*). Serial longitudinal annealing of ULFs consequently builds short filaments,
68 extending the IF network. In the end, long filaments reduce their diameter by spontaneous radial
69 compaction to form the mature IF network. The network connects to multiple intracellular adhesion
70 sites by cross-bridging proteins from the spectrin superfamily, i.e. plectin and nesprins *Liem (2016)*.
71 In skeletal muscle, IFs form a huge stress-transmitting and stress-signalling network, and desmin
72 in particular, is required for the maintenance of myofibrillar alignment, nuclear positioning and
73 shape, stress production and sensing *Palmisano et al. (2015)*; *Meyer et al. (2010)*. Due to the low
74 turn-over rates of IF proteins, the IF network remains largely intact even when exposed to large
75 physical strains, e.g. surviving at least 350% strains before rupture *Block et al. (2017)*; *Kreplak*
76 *et al. (2008)*. This led to their proposed role of acting as a cytoskeletal 'position-memory' to ensure
77 the proper re-assembly of cytoskeletal components following recovery from large strains *Gan*
78 *et al. (2016)*. The deleterious effects of abnormal desmin IF networks, due to either the additional
79 presence of mutant or the complete lack of wild-type desmin protein, are emphasized by the
80 group of human desminopathies that comprise autosomal-dominantly and recessively inherited
81 myopathies and cardiomyopathies *Clemen et al. (2013)*. Human desminopathies are clinically
82 characterized by a broad phenotypic variability ranging from primary distal myopathies, limb girdle
83 muscular dystrophies and scapulo-peroneal syndromes to generalized myopathies *Walter et al.*
84 *(2007)*; *Baer (2005)*; *Clemen et al. (2009)*; *Durmuş et al. (2016)*. The major problem with elucidating
85 pathophysiological mechanisms of the human phenotypes is that knowledge about early and
86 intermediate stages of the disease is usually elusive, since muscle tissue specimens for research
87 are not available from patients at pre-clinical stages. Therefore, a patient-mimicking knock-in

88 mouse strain carrying the R349P desmin mutation, the murine orthologous of the human R350P
89 mutation, was generated *Clemen et al. (2015)*. This model already allowed detailed systematic
90 studies of clinical and myopathological phenotypes as well as age-dependent effects on the disease
91 progression in heterozygous (het) and homozygous (hom) desminopathy mice over their wild-type
92 (wt) littermates *Diermeier et al. (2017a)*. In particular, our previous work demonstrated that the
93 expression of R349P mutated desmin compromised the three-dimensional arrangement and the
94 order of the myofibrillar lattice already starting in young mice before presenting muscle. The
95 latter findings were interpreted as a pre-aged phenotype of muscle structural ageing in the R349P
96 environment *Diermeier et al. (2017b)*. Moreover, biomechanical analyses of small fiber bundles,
97 initially in slow-twitch, load-bearing *M. soleus* (SOL) from young het and hom R349P desmin mice,
98 showed a marked increase in passive bundle stiffness compared to wt bundles *Clemen et al. (2015)*;
99 *Diermeier et al. (2017a)*. Since robust biomechanical experiments in small muscle fiber bundle
100 preparations are difficult to carry out and require precise actuation to record steady-state resting
101 length tension curves at slow strain speeds, we engineered a novel automated biomechanics
102 system that also contains a sensitive force transducer technology for recordings of active and
103 passive axial muscle forces *Haug et al. (2018)*. Alongside with the ongoing engineering progress,
104 our system was also systematically validated extending our previous recordings in SOL bundles from
105 R349P desmin mice not only to the fast-twitch extensor digitorum longus (EDL) muscle, but also to a
106 wide age range from young (17 - 23 weeks) to aged (60 - 80 weeks) animals *Haug et al. (2019)*. Again,
107 our findings in young animals of increased tissue stiffness were confirmed in both muscle entities
108 with a pre-aged phenotype in the desminopathy model. However, since also ECM re-modeling has
109 been shown with increased levels of tissue fibrosis with age in the R349P background *Diermeier*
110 *et al. (2017a)*, an unambiguous explanation towards the link of increased axial stiffness to the
111 disrupted desmin network could not be drawn. This is because in small fiber bundles, both the
112 ECM and the intracellular cytoskeleton still contribute to the overall axial compliance. To tackle this
113 constraint, the present study was designed to revisit biomechanical tests in EDL and SOL R349P
114 desminopathy muscles using pure mechanically dissected single fiber segments with a refined
115 version of our *MyoRobot* suitable to record single fiber forces. Our results provide novel insights
116 into (i) the connection of mutated desmin to axial active / passive biomechanics in single fibers and
117 (ii) the age-dependent progression of altered fiber mechanics in this desminopathy model.

118 Results

119 **Ca²⁺-mediated active isometric force and contractile apparatus Ca²⁺-sensitivity au-** 120 **tomatically assessed in single fibers from R349P desminopathy SOL and EDL mus-** 121 **cles during ageing**

122 Fig. 1A shows representative *MyoRobot*-executed force transient recordings of a caffeine-triggered
123 Ca²⁺-mediated force response to empty the SR of its releasable Ca²⁺, followed by a maximum
124 Ca²⁺-saturated activation of the contractile apparatus in HA solution. Finally, exposure to EGTA-rich
125 HR solution buffered any remaining excess Ca²⁺ ions. Consistent with the characteristics of fast-
126 vs. slow-twitch muscle, EDL and SOL fibers showed faster or slower transient kinetics, respectively.
127 Caffeine-induced peak force (Fig. 1B), maximum Ca²⁺-saturated force amplitudes (Fig. 1C) and
128 their ratio (Fig. 1D) were evaluated for all single fibers from all genotypes over all ages in both
129 muscles. In EDL, caffeine-induced force developed differentially with age in the three genotypes. In
130 wt single fibers, force amplitudes initially increased with age to significantly drop again in senile
131 animals. In contrast, in the R349P desmin knock-in background, force developed oppositely in het
132 fibers (decrease in the aged group and recovery to adult levels in the senile group) or did not vary
133 significantly within the hom group. Within age groups, we discovered isolated, genotype-specific
134 significant differences that were however, not systematic (Fig. 1B). Unlike caffeine-induced force,
135 maximum Ca²⁺-saturated force was unchanged in EDL single fibers, regardless of age or genotype
136 (Fig. 1C). The ratio of caffeine-induced to maximum force amplitudes serves as an indicator of SR

137 Ca^{2+} filling and thus, showed a similar behaviour as the former (Fig. 1D). While maximum force
138 amplitudes in SOL single fibers were generally similar to those in EDL fibers (Fig. 1C), caffeine-
139 induced force levels were roughly two-times smaller (Fig. 1B). Within SOL fibers, no difference
140 among genotypes was seen while age had a strong negative effect on force amplitudes, which were
141 significantly reduced in wt preparations for all progressing ages, and in het/hom fibers between
142 the adult and the senile age group. Maximum attainable force levels were also impeded by age and
143 displayed a significant decline during ageing within each genotype. Particularly hom fibers were
144 already significantly reduced in the adult age cohort, while the still better performing wt and het
145 fibers gradually declined to the level of hom fibers with age. This suggests a pre-aged phenotype in
146 hom fibers regarding maximum contractile forces. The combined differences regarding force ratios
147 were restricted to a significant age-related, genotype-specific decline (Fig. 1D).

148 To elaborate on the Ca^{2+} -sensitivity of the contractile apparatus in single fibers carrying the
149 desmin R349P mutation, pCa-force recordings were performed in single fibers across the three
150 age groups in EDL and SOL muscles, as shown in representative single fiber data traces from
151 each genotype in aged animals (Fig 2A). The top left panels show how force quickly rises to a new
152 steady-state level in response to increasing Ca^{2+} (decreasing pCa) steps. The right panels show the
153 respective average pCa-force of this age group for EDL (left) and SOL (right) muscle along with the
154 average reconstructed Hill fits (Fig. 2B). The curves in Fig. 2A already suggest a marked left-shift of
155 the sensor-curve in R349P desmin knock-in single fibers over wt, indicative of a myofibrillar Ca^{2+}
156 sensitization in presence of mutant desmin. This was also confirmed in the group analysis, where
157 adult hom R349P desmin knock-in EDL single fibers were initially less Ca^{2+} sensitive but became
158 more sensitive than the wt in aged animals. Since in senile mice, an age-related Ca^{2+} -sensitization
159 was also observed in wt animals, the behaviour of hom fibers can be considered as a pre-aged
160 phenotype towards higher Ca^{2+} -sensitivity of the contractile apparatus. This also agrees with wt
161 single EDL fibers reaching their largest pCa_{50} value one age bin later than hom fibers. Within the
162 oldest age cohort (senile), all pCa_{50} values had finally reached similar levels among genotypes.
163 Unlike EDL, SOL only displayed age-related effects in the wt, with an initial Ca^{2+} -desensitization
164 (from the adult to aged animals) that was later revoked in senile animals. Similar to the EDL, adult
165 hom SOL fibers showed yet significantly depressed pCa_{50} values, which however, strongly increased
166 in the aged age cohort while wt fibers only matched those high levels in the senile age group (Fig.
167 2B). Het fibers showed similar trends as hom fibers, yet, did not reach statistical significance. The
168 Hill coefficients in EDL single fibers showed no significant differences regarding genotypes while
169 age had a significant influence on het fibers between aged and senile animals. In SOL single fibers,
170 differences were present among genotypes, with lower coefficients values for fibers expressing the
171 R349P mutation (except het adult), while age had a significant influence on wt fibers, leading to
172 a significant increase in Hill coefficients in aged and senile fibers over adult fibers, indicative of a
173 higher dynamic range of the myofibrillar Ca^{2+} -biosensor complex.

174 **Steady-state resting length-tension curves demonstrate a markedly decreased axial** 175 **compliance and a pre-aged passive stiffness increase in R349P desmin knock-in** 176 **single fibers**

177 Our previous work in small fiber bundles from SOL muscles demonstrated an increased axial
178 stiffness in R349P desmin knock-in mice *Diermeier et al. (2017a)*; *Haug et al. (2019)*. However,
179 since we also documented increased fibrosis in these muscles *Diermeier et al. (2017a)*, it cannot
180 be ruled out to which extent the observed fibrosis would impact on the increased axial stiffness. To
181 eliminate the influence of ECM components on biomechanics recordings, a preparation of single
182 fibers represented the best possible experimental solution. Fig. 3A shows a series of example RLT
183 curves of single fibers of each genotype and age group from EDL and SOL muscles. The example
184 traces already suggest that the RLT slope strongly increased with age in single fibers with mutation
185 background, the more so in EDL over SOL muscle. This increase occurred in wt EDL single fibers
186 in a less-pronounced fashion, while it was absent in wt SOL samples, which remained at similar

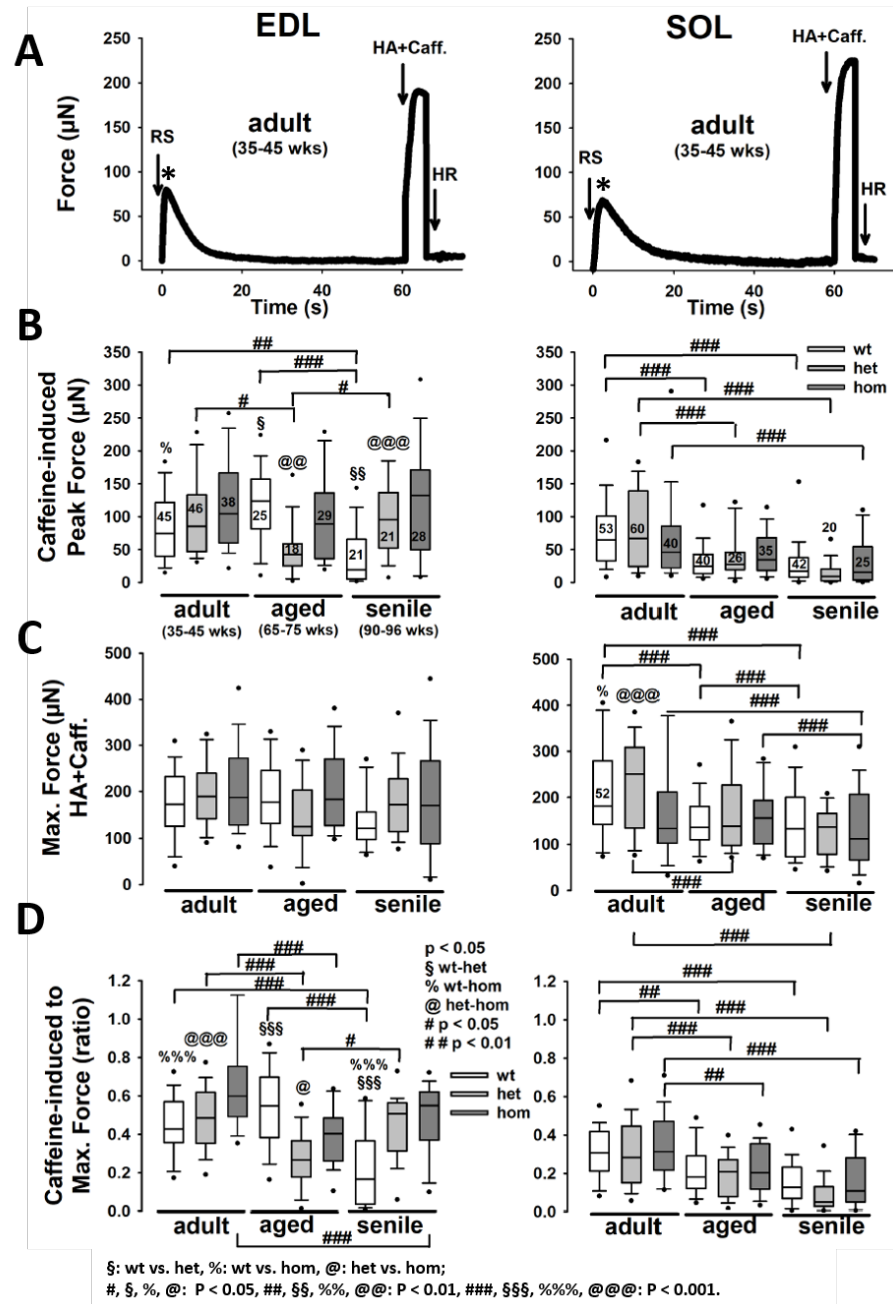


Figure 1. Caffeine-induced force and maximum Ca^{2+} -saturated force recorded in permeabilized single EDL and SOL fibers from adult, aged and senile R349P desmin mice. **A**, representative force recordings in a single EDL (left) and SOL (right) fiber. Group analysis of peak force amplitude during caffeine-release (RS) (**B**), steady-state maximum force (HA) (**C**) and respective RS:HA force ratios (**D**) indicate an overall decrease in SR Ca^{2+} -release force during ageing in EDL and SOL, regardless of genotype. Within age groups, RS peak force was significantly larger in hom EDL fibers for the adult and senile groups, while they were similar in SOL. In EDL, there was no difference in maximum attainable force among genotypes regardless of age. Thus, RS:HA force ratios in EDL reflect the pattern-differences of RS peaks, while in SOL fibres, relative force during SR Ca^{2+} release over maximum Ca^{2+} -saturated force were similar among genotypes and showed a significant decrease with ageing. Significance tested with two-way ANOVA followed by post-hoc analysis (Bonferroni). Numbers in box plots: number of single fibers analysed; also valid for (**C**) & (**D**).

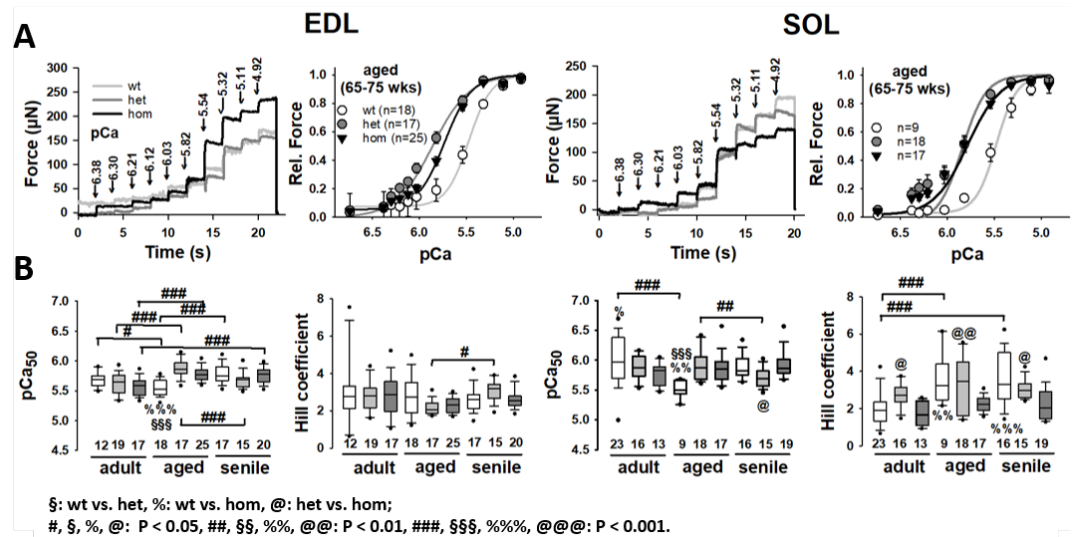


Figure 2. Ca^{2+} -sensitivity of the contractile apparatus in permeabilized single EDL and SOL fibers from adult, aged and senile R349P desmin mice. **A**, representative force recordings in an aged single EDL (left) and SOL (right) fiber for each genotype showing increasing force for each indicated step change in pCa. The mean pCa-force curves alongside with the mean reconstructed Hill fit to the data are shown to the right. The curves display a marked left-shift in the R349P desmin knock-in background. Group analysis of pCa₅₀ values and Hill coefficients in **(B)** show a significantly increased Ca^{2+} -sensitivity in aged R349P desmin knock-in animals over the wt which is caught up in the senile group. Likewise, in the adult age group, Ca^{2+} -sensitivity is similar between genotypes. In EDL, there was a significant trend towards increasing Ca^{2+} -sensitivity in the R349P desmin knock-in background with age, while in SOL, significant age-related changes were only observed in the wt. Overall, differences between wt and hom preparations became more distinct with age. Numbers in box plots: number of single fibers analysed.

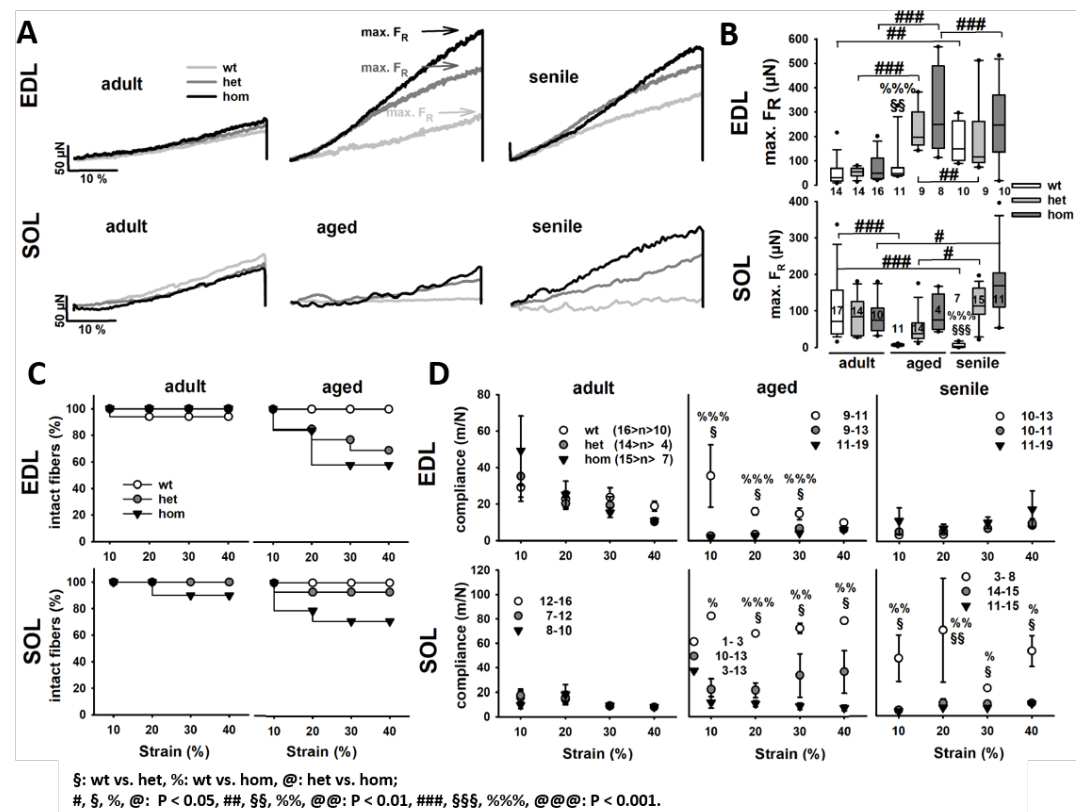
187 levels independent of age. This is in accordance with a pre-aged phenotype in the R349P mutants
188 regarding axial fiber stiffness. As a measure for steady-state stiffness at the end of the stretch to the
189 140% L_0 length, the maximum restoration force (FR) was analysed in Fig. 3B, statistically confirming
190 the behaviour seen in the examples. In the adult age group, max. FR values were all similar between
191 genotypes. In the EDL fibers, while they all increased with age, they did so more strongly and earlier
192 in the R349P knock-in background, significantly exceeding the wt in the aged group. By the very old
193 senile age, the wt had then caught up with the mutants. Although not significant, the het fibers
194 had smaller max. FR values than the hom fibers. This trend was also seen in the SOL fibers except
195 for the wt fibers showing significantly decreased max. FR values with age in comparison to the
196 adult group. The higher max. FR values in the R349P knock-in background also impacted on a lower
197 survival of single fibers during stretch. Both, in EDL and SOL muscles, mutant single fibers already
198 broke at lower strains compared to the wt, while fibers het for R349P displayed a better survival
199 than hom fibers (Fig. 3C). Since these results indicate an increased axial stiffness or elasticity, the
200 10% strain-wise compliance was computed by linear fits to the RLT curve at the indicated strain
201 bins, as described in *Haug et al. (2019)*, and plotted for all genotypes, ages and strains in Fig. 3D.
202 The compliance plots confirm similar mechanical axial compliance for all genotypes in the adult age
203 group while compliance was significantly reduced in mutant fibers of the aged age group. The wt
204 then declined to similar low compliances as the mutants in the senile age group for EDL muscle
205 fibers, whereas for SOL, compliance remained at high levels.

206 **Axial viscosity is unaltered by the R349P mutation in single EDL and SOL fibers**

207 While the R349P mutation clearly affects axial elasticity, RLT curves did not provide insights into the
208 biomechanical axial viscosity. Therefore, we used the *MyoRobot* to perform ultra-fast stretch-jumps
209 such as shown in Fig. 4A for wt adult single fibers from EDL and SOL muscle. Each new stretch
210 jump was answered by an instantaneous restoration force (F_R) increase to a maximum, followed
211 by viscous relaxation (F_{relax}) to a new steady-state during the 5 s holding phase. Confirming the
212 findings from the slow RLT curves, mutant single fibers had a much higher chance of rupture during
213 these strenuous sudden stretches as compared with wt fibers (Fig. 4B). The analysis of maximum
214 F_R amplitudes with stretch bin, reflecting axial elasticity, confirmed the findings from the RLT curves,
215 i.e. higher restoration forces in the mutant background (Fig. 4C). However, relaxation force F_{relax} ,
216 representing the difference between maximum F_R and steady-state F_R within the same stretch
217 jump, was not significantly different between either genotype or ages (Fig. 4D), arguing against any
218 involvement of the R349P mutant desmin in viscous relaxation.

219 **Unloaded speed of shortening in R349P desmin single fibers is increased rather 220 than compromised**

221 The observed increased passive elasticity in R349P mutant desmin single fibers suggests a negative
222 influence on muscle contraction kinetics, e.g. unloaded speed of shortening. To address this
223 question, we performed so-called 'slack-tests' using our automated *MyoRobot* system *Haug et al.*
224 (2018). Fig. 5A shows representative example recordings of a senile EDL (left) and an aged SOL
225 (right) single fiber. After reaching steady-state maximum isometric contraction in HA solution, the
226 VCA quickly introduced a slack of defined length dL. Consequently, force dropped to zero and
227 redeveloped over time (dt). The relation dL vs. dt is plotted to the right in Fig. 5A. Also shown
228 are the linearly derived fast and slow velocities v_{fast} and v_{slow} from the respective section of the
229 double exponential fit. Fig. 5B shows the dL-dt plots for all age groups and genotypes for both
230 muscles and Fig. 5C the statistical analysis of v_{fast} and v_{slow} . v_{fast} reflects the initial, unloaded phase,
231 whereas v_{slow} represents the internally loaded phase that occurs while taking up larger 'slacks
232 lengths' *Haug et al. (2018)*. Notably, v_{fast} increased with age in all genotypes, while it decreased
233 again in senile mutation-bearing fibers, except for hom SOL fibers. In this context it was even
234 more compelling that mutant fibers performed significantly faster than wt fibers in aged animals.
235 Although v_{slow} qualitatively showed a similar trend, there were no statistical significances regarding



236 age or genotype.

237 Discussion

238 Desminopathies comprise a heterogeneous group of inherited and sporadic myopathies which, in
239 the vast majority of cases, share a common morphological picture comprising sarcoplasmic and
240 subsarcolemmal desmin-positive protein aggregates and signs of myofibrillar degeneration *Jurcu*
241 *et al. (2017)*; *Clemen et al. (2009)*; *Walter et al. (2007)*. In general, analyses of the pathophysiology
242 of human desminopathies are hampered by the very limited amount of available human muscle
243 tissue specimens and the fact that the alterations noticed in diagnostic muscle biopsies nearly
244 always reflect late stages of the disease. In addition, these specimens are highly heterogeneous with
245 regard to sex, age, type of muscle and disease severity. To overcome these limitations, we generated
246 the patient-mimicking R349P desmin knock-in desminopathy mouse model, which harbours the
247 orthologous of the most frequent human desmin mutation R350P *Clemen et al. (2015)*. The
248 availability of this mouse line has already served invaluable to perform age-related morphometric

249 analysis of cytoarchitectural changes in early disease stages in single fibers from slow- and fast-
250 twitch muscles using multiphoton Second Harmonic Generation (SHG) microscopy *Diermeier et al.*
251 (2017a). In that study, we could show a pre-aged morphological phenotype depicting sarcomeric
252 lattice disorder and myofibrillar angular distribution in both EDL and SOL single fibers *Diermeier*
253 *et al. (2017a)*. On a single fiber level, such distorted myofibrillar cytoarchitecture would already be
254 a structural determinant of muscle weakness 'per se' since the resulting force vector of the parallel
255 myofibrillar lattice in single fibers would be expected to be smaller compared to if all myofibrils
256 were perfectly aligned *Friedrich et al. (2010)*; *Buttgereit et al. (2013)*; *Schneidereit et al. (submitted*
257 *2018)*. For human R350P desminopathy, apart from clinical assessment of overall force in proximal
258 and distal muscle groups according to MRC grades *Walter et al. (2007)*, no information on active
259 force production on the sub-organ level (single fibers, fiber bundles) is available. For the murine
260 R349P desmin knock-in model, initial characterization of small SOL fiber bundles at preclinical
261 stages in young mice *Clemen et al. (2015)* as well as very recently, a whole age-dependent study of
262 ours on small EDL and SOL fiber bundles in mice from 17 wks to >60 wks of age, documented a
263 pre-aged phenotype regarding increased passive axial stiffness, using our novel high-end *MyoRobot*
264 biomechanics system *Haug et al. (2018)*. Together with the finding of also increased extracellular
265 fibrosis in aged R349P desmin knock-in muscles *Diermeier et al. (2017a)*, this still leaves the
266 possibility of series-elastic elements of increased stiffness in parallel to the cytoskeletal visco-elastic
267 elements to be responsible for the reduced axial compliance in small EDL and SOL fiber bundles
268 seen before. In order to close this gap, we refined our previous study to determine the active
269 and passive biomechanics properties in het and hom R349P desmin knock-in mice as well as
270 their wt littermates extending the age range from adult (35 - 45 wks) to very old (90 - 96 wks), as
271 well as to mechanically dissected single fibers, for the very first time. The advantage of dissected
272 single fibers not containing ECM connections to surrounding elements any more, i.e. being void
273 of neighbouring fibers, provides a pure preparation to exclusively focus on the effect of mutated
274 desmin on cytoskeletal axial fiber biomechanics.

275 **Age is the more predominant determinant of compromised active axial biome-**
276 **chanics in single fibers from slow- and fast-twitch muscle compared to the pres-**
277 **ence of R349P mutant desmin protein**

278 The most important finding in our age-related study in single EDL and SOL fibers from adult to
279 senile mice was that age had a strong negative influence on active force production, with significant
280 declines during ageing within each genotype regarding the caffeine-induced Ca^{2+} -mediated force
281 transients. This effect was more prominent in slow SOL fibers but also, to a lesser extent, in
282 fast-twitch EDL fibers. Among the genotypes, the presence of R349P mutated desmin was much
283 less of a systematic determinant of caffeine-induced active force, in particular in SOL fibers, while
284 in EDL fibers, some inconsistent significances were present. Detailed systematic age-related studies
285 on contractile properties in fast- and slow-twitch muscle are rare with most studies having been
286 carried out on whole muscle. In 2 yr-old versus 6 mo-old rats, twitch and tetanic force were lower in
287 old over young animals, but accounting for an age-related atrophy of fibers, no differences were
288 found in the maximum force-generating capacity in either slow- or fast-twitch muscles at either
289 age *Larsson and Edström (1986)*. In the respective mouse muscles however, a decline in absolute
290 isometric tetanic force production to ~75% of the values in young (2 - 3 mo) and adult (9 - 10 mo)
291 was reported in aged (26 - 27 mo) mice for both EDL and SOL muscle. This difference prevailed after
292 normalization to specific force for fast-twitch EDL, but for SOL specific tetanic force no more age
293 dependence was seen *Brooks and Faulkner (1988)*. In a comparative study on maximum isometric
294 tension, comparing both fiber bundles and single skinned fibers from rat SOL and EDL muscle
295 with age, maximum tension was increased by roughly 35% in senescent rats (30 mo) over control
296 adults (9 mo) for both SOL bundles and single fibers. The same only applied for single EDL fibers
297 whereas in EDL bundles, force almost dropped ~20% with age *Eddinger et al. (1986)*. Lastly, in
298 an age-related study in dystrophic mdx mice, single skinned SOL and EDL fibers displayed no

299 differences comparing young (3 - 6 wks) and adult (17 - 23 wks) animal *Williams et al. (1993)*. The
300 recognition of considerable variability in specific isometric force values between study groups has
301 been stated to render comparisons between whole muscles, fiber bundles and single fibers with
302 respect to ageing difficult *Brooks and Faulkner (1988)*.

303 The important strength of our approach lies in the age-dependent assessment of R349P mutant
304 desmin effects in an age-dependent background which was not available before. One limitation
305 of our *MyoRobot* system at the time this study was initiated was still the lack of in-built optics
306 to measure the fiber diameter for conversion of absolute force to specific, cross-sectional area
307 (CSA)-normalized force. Towards the completion of data collection for the age-related biomechanics
308 assessment here, ongoing optical engineering in our labs resulted in a more advanced version of
309 the *MyoRobot* that now contains in-built optics and a CCD camera to capture fiber diameter online.
310 Although this system will be presented elsewhere, the absolute single fiber force levels presented
311 here are well in the range of those reported by Stelzer & Widrick (2003) *Stelzer and Widrick (2003)*
312 in SOL fibers from adult (8 - 12 wks) mice, around 150 μ N per fiber at maximum Ca^{2+} activation.
313 Inversely, when measured with our current setup, single mouse fibers from animals unrelated to
314 this study, fiber diameter values of mostly between 30 μ m and 40 μ m were found which translates
315 specific forces to roughly 15 N/cm² or 150 kPa, in perfect agreement with single fiber specific force
316 values from literature *Williams et al. (1993)*; *Stelzer and Widrick (2003)*.

317 Regarding the Ca^{2+} sensitivity of the contractile apparatus, a pre-aged phenotype in the R349P
318 background was observed. Particularly mutation-bearing EDL fibers displayed a myofibrillar Ca^{2+} -
319 sensitization already within the aged age group, while in wt littermates, this became only apparent in
320 the senile group. This corroborates well with results from our very recent age-related biomechanical
321 assessment of R349P desmin small fiber bundles, where a very similar desensitization of about
322 0.2 - 0.3 pCa units was seen from the adult to the aged age group in EDL bundles, both the het
323 and the hom *Haug et al. (2019)*. For SOL, the single fiber data here do not seem to show a firm
324 consistent trend among the genotypes with age, apart from a large scattering between individual
325 SOL fibers. This could be due to marked differences of pCa₅₀ values between fast- and slow-twitch
326 fibers being present in the SOL muscle as it contains an almost equal proportions of either fiber
327 type *Edgerton et al. (1975)*; *Lynch et al. (1993)*. Unlike in previous studies using single fiber Ca^{2+}
328 sensitivity assessment (e.g. Lynch et al. (1993) *Lynch et al. (1993)*), we did not attempt to type fibers
329 for myosin heavy chain (MHC) isoforms due to technical reasons and thus, this may at least partially
330 explain the observed scatter. However, from our previous work assessing the MHC composition
331 in SOL muscle homogenates in the three genotypes, we are confident that in particular the hom
332 fibers shall present with a higher slow-type MHC I proportion over wt and het fibers *Diermeier*
333 *et al. (2017a)*. Therefore, the large scatter towards higher pCa₅₀ values in aged and senile single
334 SOL fibers (Fig. 2B) is in good agreement with the fact of higher pCa₅₀ values in type I over type II
335 fibers *Lynch et al. (1993)*. Also, our absolute pCa₅₀ values presented here are in good agreement
336 with the aforementioned study *Lynch et al. (1993)*.

337 **Passive axial biomechanics is shifted towards a pre-aged stiffer phenotype in sin-** 338 **gle fibers by R349P desmin**

339 Similar to our previous assessment in small fiber bundles *Clemen et al. (2015)*; *Diermeier et al.*
340 *(2017a)*; *Haug et al. (2019)*, single fibers showed a marked increase in passive restoration forces in
341 RLT experiments, which was at least three-times larger in aged animals with R349P background.
342 Restoration forces were significantly increased and axial compliance accordingly decreased, al-
343 ready in single EDL fibers from aged R349P desmin knock-in animals compared to the equivalent
344 observations found in wt animals in the senile group, only. This clearly points to a pre-aged pheno-
345 type in fast-twitch muscle in the mutant desmin background. Notably, the increase in restoration
346 force (decrease in compliance) in EDL bundles already happened in young animals and was more
347 pronounced in hom R349P desmin knock-in mice, albeit not statistically significant *Haug et al.*
348 *(2019)*. Also, from the adult age, the differences were blunted among genotypes in bundles in

349 the EDL, arguing in favour of an important difference compared to single fibers. This can only be
350 explained by the abolishment of ECM components in the pure single fibers blunting the effects
351 of an additional parallel series elastic element contributing to the axial steady-state compliance.
352 In our SOL single fibers, a similar increase in passive axial stiffness in het and more pronounced
353 in hom R349P desmin knock-in single fibers was seen. This is also much more clear-cut here
354 compared to the presentation in SOL bundles. In the latter, the increase in stiffness with age was
355 mostly seen in hom bundles only, but those being highly statistically stiffer over het R349P and
356 wt bundles in aged mice *Haug et al. (2019)*. The direct comparison of bundles *Haug et al. (2019)*
357 and single fibers now being available suggests that ECM components likely introduce an additional
358 compliance to the bundles, e.g. through elastic fibers, that would reduce the overall stiffness.
359 Alternatively, the over-proportionally larger cross-sectional area in bundles carrying the R349P
360 mutation may be dissipating restoration forces between both, intracellular (i.e. mutated desmin)
361 and extracellular non-contractile elements. Although an increase in ECM collagen was detected
362 in our previous study in R349P SOL bundles that was larger in hom over het bundles *Diermeier*
363 *et al. (2017a)*, the involvement of other, more compliant ECM components to be increased in
364 the R349P desmin knock-in background cannot be ruled out and deserves further investigation.
365 Nevertheless, our *MyoRobot* approach was able to extend our previous knowledge on R349P axial
366 muscle stiffness to single fibers and also including a larger age range extending to the senile stage,
367 not only with regard to the R349P desmin knock-in background, but also in particular including
368 ageing effects in normal muscle. For instance, in both our EDL and SOL single fiber preparations
369 from wt mice, axial compliance increased from the adult to the aged age groups to then remain
370 mostly stationary in the EDL, or they declined again in the SOL within the senile groups (Fig. 3D).
371 This is in good agreement with a comparative study on *tibialis anterior* mouse muscle single fibers
372 and small fiber bundles, where single fibers from old mice showed a tendency for reduced elasticity
373 moduli (reflecting smaller stiffness, larger compliance values, respectively, kPa, n.s.) *Wood et al.*
374 *(2014)*. More strikingly, the researchers showed that intrinsic stiffness of ECM increased with age as
375 indicated by larger Young moduli in fiber bundles over single fibers, and in particular, a two-fold
376 increased bundle stiffness in old versus adult *tibialis anterior* fiber bundles *Wood et al. (2014)*. The
377 same behaviour of increased modulus (quadratic modulus, $\text{kPa}/\mu\text{m}^2$) values was shown in EDL fiber
378 bundles over single fibers from young (7 - 9 wks) wt mice *Meyer and Lieber (2011)*. When comparing
379 our axial single fiber compliance values to the corresponding values in small fiber bundles given
380 in our associated study in adult and aged mice (Haug et al. (2019a) *Haug et al. (2019)*), i.e. for
381 SOL $\sim 1 - 4 \text{ m/N}$ and for EDL bundles $\sim 1 - 6 \text{ m/N}$), one can see that our single fibers consistently
382 show higher compliance values, reflecting higher stiffness in bundles over single fibers. Meyer &
383 Lieber (2011) *Meyer and Lieber (2011)* also provide an elegant experimental explanation for the
384 increased stiffness in fiber bundles over single fibers and grouped single fibers, in that the ECM
385 contribution to non-linear bundle elasticity is set out by spreading the sarcomere length distribution
386 of individual fibers within the bundle. This superposes different RLT-curves from single fibers in a
387 bundle to a non-linear resultant elasticity behaviour. This is most probably due to different lateral
388 and axial forces acting on adjacent single fibers through ECM-mediated focal adhesion connections,
389 i.e. integrins *Gershlak and Black (2015)*. It is of note that the absolute values for axial stiffness
390 (compliance) in our study and those aforementioned ones cannot be directly compared, as different
391 methods were employed, and our system during that time of experiments in single fibers could
392 not yet assess single fiber CSA and sarcomere lengths. When focusing on the influence of mutant
393 R349P on passive axial compliance / stiffness, our current results support those obtained in fiber
394 bundles *Haug et al. (2019)* in showing significantly reduced axial compliance indicative of stiffer
395 phenotype with the important difference that in the bundles, this effect seemed less systematic in
396 the respective age groups in both EDL and SOL muscles. In single fibers, compliance was clearly at
397 least two-fold reduced in the R349P background over wt animals, starting from the aged age group
398 in both muscles and staying diminished in SOL muscles while alleviating in the EDL muscle from
399 senile animals. Thus, revealing the higher stiffness in single fibers in a more robust way over the

400 respective fiber bundle preparations *Haug et al. (2019)* again points to the crucial involvement of
401 ECM components which introduce additional non-linear elasticities to the axial compliance that
402 are difficult to predict in the R349P desmin knock-in background. The larger presence of fibrosis in
403 muscle tissue from aged mice hom for the R349P desmin allele clearly points towards the presence
404 of such non-linear elasticities over het and wt muscles *Diermeier et al. (2017a)*. The larger stiffness
405 in pure single fibers in the R349P desmin knock-in background is also confirmed by their lower
406 resistance to stretch and thus, lower survival upon stretch, either quasi-static (Fig. 3C) or dynamic
407 (Fig. 4B). Similar to our findings in bundles *Haug et al. (2019)*, visco-elastic properties were not
408 significantly altered in R349P desmin knock-in single fibers. It should be noted that apart from our
409 detailed study here, nothing is known about the influence of intermediate-filament mutations on
410 the visco-elastic properties of fully differentiated muscle fibers.

411 **Unloaded speed of shortening in ageing: faster contractions of R349P desmin knock-** 412 **in single fibers**

413 With our recent implementation of a VCA within the *MyoRobot* *Haug et al. (2018)*, it was now possible
414 to address whether the markedly increased axial stiffness in single fibers in the R349P desmin
415 knock-in background would impact on unloaded shortening, given the fact that the isometric
416 maximum force development was only marginally affected. The absolute values of velocities for
417 the fast component with mean values between 4 mm/s and 12 mm/s for EDL single fibers and
418 2 – 6 mm/s for SOL fibers are well in the range of velocities reported for single EDL fibers from wt
419 mice unrelated to this study *Haug et al. (2018)*. This demonstrates the robustness of our automated
420 biomechatronics system to assess active biomechanical properties in single fibers across studies
421 and organ scales. Similar to our previous study in small fiber bundles, fast velocities increased
422 with age in het mice while in the wt, they remained stationary *Haug et al. (2019)*. However, in
423 the aforementioned mentioned study of ours, only few numbers of observations were available
424 for EDL muscle bundles, which complicates a robust comparison. Rather, for SOL bundles with
425 higher numbers of observations, fast velocities showed a tendency for slowed shortening in the
426 R349P knock-in background in young animals that was mostly abrogated in the adult and aged
427 age group, except for a tendency of a faster shortening in the mutants *Haug et al. (2019)*. Thus, it
428 was intriguing to find that both, fast and slow components of shortening in single muscle fibers
429 increased with age, the more so for the R349P knock-in background over the wt for adult and
430 aged mice for both EDL and SOL fibers, while values again merged to similar levels in senile mice.
431 Age-related values for unloaded shortening in single fibers are scarce in the literature. A study
432 on rat EDL single fibers found an unchanged maximum shortening velocity was in adult (9 mo)
433 versus senescent (30 mo) animals, whereas SOL fibers from old rats *Eddinger et al. (1986)* were
434 slower. In human *vastus lateralis* single skinned fibers, shortening velocities were reduced in type
435 IIA fibers but not type I fibers in older man, while the opposite was found for women *Krivickas*
436 *et al. (2001)*. For murine muscles, a detailed sex and age-related study is not available, to our
437 knowledge. The reason for the increased speed of shortening in R349P desminopathy muscle
438 fibers cannot unambiguously be explained at current, in particular in view of our recent finding that
439 slow-type MHC I isoforms were upregulated in R349P desmin knock-in muscles while fast-twitch
440 MHC II isoforms were downregulated *Diermeier et al. (2017a)*. Thus, the R349P mutated desmin
441 must have some influence on the kinetics of weak cross-bridge attachment that has been found to
442 predominantly determine unloaded speed of shortening *Stehle, R. & Brenner, B. (2000)*. Whether
443 this may be an explanation for the increased shortening velocity in desminopathy single fibers
444 deserves future investigation.

445 **Summary and outlook**

446 Our results prove the increased passive steady-state elasticity found in R349P desminopathy skeletal
447 muscle to be an inherent factor related to the mutant desmin inflicted damage of the cytoskeleton
448 and not the ECM. This results in a pre-aged, stiffer phenotype of affected muscle fibers. Apart

449 from a yet unexplained acceleration of speed of shortening in fibers expressing R349P desmin,
450 Ca^{2+} -mediated active force was only mildly affected, if at all. Our *MyoRobot* system allows a highly
451 versatile and modular design of automated execution of various additional muscle test protocols,
452 e.g. eccentric contractions, that shall be of use to the community to ease future myopathy and
453 mechanistic studies related to skeletal muscle and ageing.

454 **Methods and Materials**

455 **Mouse model - R349P Desmin knock-in mouse**

456 Heterozygous (het) and homozygous (hom) littermates of the R349P desmin knock-in mouse model
457 B6J.129Sv-Des^{tm1.1Ccrs} (<http://www.informatics.jax.org/allele/MGI:5708562>) *Clemen et al. (2015)*;
458 *Winter et al. (2016)* were used. Littermates not carrying the R349P desmin mutation served as
459 wild-type (wt) control. We here extended our previous biomechanics study on small fiber bundles
460 from only young mutant mice *Diermeier et al. (2017a)* towards three older age groups, spanning
461 35 - 45 weeks (adult), 65 - 75 weeks (aged) and 90 - 96 weeks (senile). All animal-related work was
462 performed in accordance with the German Animal Welfare Act (Tierschutzgesetz), as well as the
463 German Regulations for the protection of animals used for experimental purposes or other scientific
464 purposes (Tierschutz-Versuchstierverordnung). The governmental Office for Animal Care and Use
465 (Regierung von Mittelfranken, 91511 Ansbach, Germany; reference number TS-14/2015) approved
466 the investigations. All applicable international, national, and institutional guidelines for the care
467 and use of animals were followed.

468 **Chemical solutions**

469 All muscle dissection was performed in Krebs-solution containing (mM): 120 NaCl, 4.7 KCl, 1.2
470 KH_2PO_4 , 1.2 $\text{MgSO}_4 \cdot 7\text{H}_2\text{O}$, 24.8 NaHCO_3 , 0.1 M glucose, 0.1% FCS (FBS), pH 7.3. A Ca^{2+} -free, high K^+ -
471 solution (HKS) was used to permanently depolarize the muscle cell membrane to abolish excitability
472 during manual tethering of fascicles and isolation of single fiber segments. HKS ('high- K^+ -solution')
473 contained 140 K-glutamate, 10 Hepes, 10 glucose, 10 MgCl_2 , 1 EGTA (ethylene glycol-bis(β -aminoethyl
474 ether)-N,N,N',N'-tetraacetic acid, pH 7.0. To maximally Ca^{2+} -activate single fibers, a Ca^{2+} -saturated
475 high activating internal solution (HA) was used containing: 30 Hepes, 6.05 $\text{Mg}(\text{OH})_2$, 30 EGTA, 29
476 CaCO_3 , 8 Na_2ATP , 10 Na_2CP , pH 7.2. Free Ca^{2+} of HA was calculated to $\sim 12.5 \mu\text{M}$ using the chelator-
477 ligand binding software React (developed by Geoffrey Lee, University of Glasgow). To maximally
478 relax single fibers and to completely buffer Ca^{2+} ions each time a fiber was exposed to Ca^{2+} , high
479 relaxing solution (HR) was used that had the same composition as HA except for not containing
480 any Ca^{2+} (for practical reasons of pCa calculations, a pCa of 9 is assumed in HR). Mixtures of HA
481 and HR were calculated to obtain a given pCa of the internal solution for graded Ca^{2+} -activation in
482 pCa-force response curves using React and consisted of HA:HR ratios of 0.3:0.7, 0.5:0.5, 0.55:0.45,
483 0.6:0.4, 0.65:0.35, 0.7:0.3, 0.8:0.2, 0.9:0.1, 0.95:0.05, 0.98:0.02, 1:0, converting to pCa values of
484 6.74, 6.38, 6.30, 6.21, 6.12, 6.03, 5.82, 5.54, 5.32, 5.11, 4.92, respectively. Low relaxing solution (LR)
485 served as an intermediate step after HR or loading solution (LS, see below) to replace the high
486 affinity Ca^{2+} chelator EGTA for low affinity HDTA (1,6-diaminohexane-N,N,N',N'-tetraacetic acid). LR
487 contained: 30 Hepes, 7.86 $\text{Mg}(\text{OH})_2$, 87.8 K-glutamate, 6.6 HDTA, 0.4 EGTA, 8 Na_2ATP , 10 Na_2CP
488 (creatine phosphate), pH 7.2. LS was a mixture of HA and HR titrated to a free Ca^{2+} of $\sim 300 \text{ nM}$
489 to reload the sarcoplasmic reticulum (SR) for defined incubation times. RS served as release solution
490 for Ca^{2+} ions from the SR and was LR supplemented with 30 mM caffeine. All solutions were
491 thawed from stocks at the day of experiments and freshly supplemented with creatine kinase (CK,
492 Sigma/Roche, Germany) to $\sim 300 \text{ U/ml}$ or $\sim 3 \text{ U/well}$ and sodium azide (0.1 M NaN_3), the latter to
493 prevent mitochondrial Ca^{2+} uptake *Fry et al. (1989)*. To initially chemically permeabilize a single
494 fiber, saponin was added to HR in a separate well of the *MyoRobot* rack to a concentration of 0.1%
495 (w/v).

496 **Preparation of single muscle fibers**

497 Mice were anaesthetized via isoflurane inhalation and sacrificed by cervical dislocation. The hind
498 limbs were cut off and transferred to Krebs-solution. SOL and EDL muscles were dissected under a
499 stereo-microscope (Olympus SZX7, Olympus, Hamburg, Germany), while being pinned under slight
500 stretch into a Sylgard (Dow Corning, Wiesbaden, Germany) coated petri dish. Upon completing the
501 dissection, Krebs-Solution was exchanged for HKS, allowing for 15 min equilibration, before single
502 fibers were manually dissected with fine forceps.

503 **Assessment of active and passive biomechanics in single muscle fibers in an auto-** 504 **mated MyoRobot environment**

505 Biomechanics recordings were conducted using the *MyoRobot*, a novel automated biomechanics
506 system combining high precision voice coil actuation (VCA) with force sensor technology *Haug*
507 *et al. (2018)*. After isolation, the single fiber segment (length at least 2 mm) was transferred to the
508 *MyoRobot* multi-well rack in a custom-made Perspex chamber while submerged in HKS solution,
509 placed below the pins of the force transducer and VCA and fixed to both pins via a tweezer
510 mechanism. For details on the biomechanics system and sensor, and actuation implementation,
511 refer to *Haug et al. (2018)*. Every protocol started with a chemical permeabilization of single fibers in
512 HR supplemented with saponin for 20 s. An automated set of biomechanical recordings on the same
513 preparation was then executed, consisting of sequential runs of (i) caffeine-induced, Ca^{2+} -mediated
514 force generation, (ii) pCa-force curves, (iii) speed of shortening (slack-test), (iv) passive elasticity –
515 resting length-tension curve (RLT) and (v) assessment of visco-elastic passive behaviour:

- 516 • **Caffeine-induced, Ca^{2+} -mediated force generation:** After fiber permeabilization, the fiber
517 was shortly dipped into HR to wash off remaining saponin and to buffer internal Ca^{2+} . Subse-
518 quently, it was translocated to LR for 60 s, after which the SR was loaded in LS for 60 s. The
519 caffeine-induced force transient was triggered by exposure to RS for 60 s, while maximum
520 force was induced via HA solution for 5 s (Fig. 1).
- 521 • **Ca^{2+} sensitivity of the contractile apparatus, pCa-force curves:** The fiber was sequen-
522 tially exposed to solutions of increasing Ca^{2+} ion concentrations (decreasing pCa values
523 $(-\log_{10}[\text{Ca}^{2+}])$) for a duration of 20 s (Fig. 2).
- 524 • **Unloaded speed of shortening ('slack-test'):** The muscle fiber was held at resting length L_0
525 and transferred to HA solution, resulting in maximum isometric contraction. Upon achieving
526 steady-state force, the VCA pin moved at maximum speed towards the force transducer,
527 slacking the fiber by a defined percentage of L_0 (5%, 10%, 20%, 30%, 40%, 50% or 55%) as
528 force dropped to 0 mN. While taking up the slack, force re-established in the presence of
529 saturating Ca^{2+} . Once the next force-plateau was reached, the fiber was washed in HR to
530 remove excessive Ca^{2+} and to relax the myofibrils before moving on to the consecutive 'slack
531 length'. For this recording, sampling rate was set to 2 kHz (Fig. 3).
- 532 • **Passive elasticity – RLT curves:** To assess passive axial elasticity, the muscle fiber was kept
533 in LR solution to avoid active contraction. The fiber was continuously stretched at a slow
534 speed ($0.44 \mu\text{m/s}$) to 140% of L_0 ($L_0 \sim 1,950 \mu\text{m}$) by moving the actuator pin away from the
535 force transducer pin. Restoration force was continuously recorded. To every 10% stretch bin,
536 a linear fit was applied to calculate the fiber's compliance, reflected by the inverse of that
537 slope and thus, the inverse of stiffness (Fig. 4).
- 538 • **Visco-elastic passive behaviour:** To assess the visco-elastic passive behaviour, the fiber was
539 stretched in a sudden staircase-like pattern in 10% L_0 steps to 160% L_0 with a holding time
540 of 10 s. To prevent any active contraction, the fiber was kept in LR during the recording. The
541 force response of the fiber comprised of an instantaneous passive restoration force and a
542 force relaxation, with an exponential decay of force back to a steady-state level (Fig. 5).

543 **Data analysis and statistics**

544 *MyoRobot* data were processed with analysis protocols in RStudio (RStudio Inc., rstudio.com) while
545 plotted and statistically evaluated with SigmaPlot (Systat Software Inc., sigmaplot.co.uk). All data
546 traces were smoothed with a moving average filter. For pCa-curves, the plateau force close to the
547 end of each pCa step was determined by the software and plotted against the corresponding pCa
548 value. The scatter plot of normalized force (normalized to max. force at pCa 4.92) was fitted to a
549 four-parameter Hill-equation ($y = y_0 + \frac{a \cdot 10^{-bx}}{c^b + 10^{-bx}}$) utilizing least-square methods with the physiological
550 constraints $y_0 = 0$ and $a = 1$. The steepness (b , Hill-coefficient) and the deflection point ($-\log_{10}([Ca^{2+}]_i)$,
551 pCa_{50}) of every individual curve fit were used to reconstruct a mean fit to the averaged data points
552 (Fig. 2). For speed of shortening (slack-tests), a 5% threshold criterion was established from the
553 maximum isometric force of the first slack. This threshold defined significant 'force redevelopment'
554 for this and all consecutive 'slack lengths' (dL). The time needed to cross this force-threshold
555 was called 'slack time' (dt) and was plotted against the respective 'slack length' dL . The resulting
556 dt - dL -scatter plot was fitted with a bi-exponential function ($y = a(1 - e^{k_1 dt}) + c(1 - e^{k_2 dt})$). Its
557 derivative represented the non-linear slack-length dependent shortening velocity $v(dL)$. The dL - dt
558 range was divided in a fast (unloaded phase, <45% 'slack length') and a slow phase (internally
559 loaded phase, >45% 'slack length') as described in Haug et al. (2018) **Haug et al. (2018)**. Passive
560 elasticity - RLT curves: To every 10% L_0 stretch bin, a linear fit was applied and the respective
561 increase / steepness computed to obtain axial elasticity and compliance (inverse increase). Visco-
562 elastic behaviour: The force baseline (F_0) was determined as the last 5 s before the first step while
563 absolute restoration force ($F_{abs} = \max_{n \cdot 10\%} - F_0$) of each 10% stretch-step was calculated as the
564 difference of maximum recorded force of the corresponding step to the baseline. Force relaxation
565 was obtained from the difference between maximum and minimum force recorded within the
566 same step ($F_{relax} = \max_{n \cdot 10\%} - \min_{n \cdot 10\%}$). Statistical significance was assessed by applying two-way
567 ANOVA tests (age bins and genotypes as variables), following post-hoc analysis (Tukey, Bonferroni) in
568 SigmaPlot. Significance levels of $P < 0.05$ were considered significant, < 0.01 and < 0.001 considered
569 strongly and highly significant, respectively. Significance levels involving age effects were depicted
570 as #, while genotype differences were depicted as \bar{S} : wt vs. het, %: wt vs. hom, and @: het vs. hom,
571 respectively.

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577 **Conflict of interest**

578 The authors declare that they have no competing or financial interests.

579 **Author contributions statement**

580 C.M., M.H. and B.R. conducted the experiments. C.M. analyzed the results. G.P. and M.H. engineered
581 the *MyoRobot* biomechatronics system. R.S. and C.S.C. provided the animal model and expertise
582 on the pathophysiology of desminopathies, and O.F. conceived the project and supervised the
583 whole research. C.M., M.H., R.S., C.S.C and O.F. wrote the manuscript. All authors approved the
584 manuscript. This paper is part of the doctoral thesis of C.M.

585 **Additional information**

586 O.F. discloses relationship to the SME comoto through the aforementioned ZIM grant as an R&D
587 project to translate the *MyoRobot* technology into commercialization.

References

- 588
589 **Anderson J**, Li Z, Gouble F. Passive stiffness is increased in soleus muscle of desmin knockout mouse. *Muscle &*
590 *Nerve*. 2001; 24(42):1090–1092.
- 591 **Baer H**. Pathogenic effects of a novel heterozygous R350P desmin mutation on the assembly of desmin
592 intermediate filaments in vivo and in vitro. *Human Molecular Genetics*. 2005; 14(10):1251–1260. doi:
593 10.1093/hmg/ddi136.
- 594 **Block J**, Witt H, Candelli A, Peterman EJG, Wuite GJL, Janshoff A, Köster S. Nonlinear Loading-Rate-Dependent
595 Force Response of Individual Vimentin Intermediate Filaments to Applied Strain. *Physical Review Letters*.
596 2017; 118(4):048101. doi: 10.1103/PhysRevLett.118.048101.
- 597 **Brooks SV**, Faulkner JA. Contractile properties of skeletal muscles from young, adult and aged mice. *Journal of*
598 *Physiology*. 1988; 404:71–82.
- 599 **Buttgereit A**, Weber C, Garbe CS, Friedrich O. From chaos to split-ups—SHG microscopy reveals a specific
600 remodelling mechanism in ageing dystrophic muscle. *Journal of Pathology*. 2013; 229(3):477–485. doi:
601 10.1002/path.4136.
- 602 **Clemen CS**, Fischer D, Reimann J, Eichinger L, Mueller CR, Mueller HD, Goebel HH, Schroeder R. How much
603 mutant protein is needed to cause a protein aggregate myopathy in vivo? Lessons from an exceptional
604 desminopathy. *Human Mutation*. 2009; 30(3):E490–E499. doi: 10.1002/humu.20941.
- 605 **Clemen CS**, Herrmann H, Strelkov SV, Schroeder R. Desminopathies: pathology and mechanisms. *Acta*
606 *Neuropathologica*. 2013; 125(1):47–75. doi: 10.1007/s00401-012-1057-6.
- 607 **Clemen CS**, Stöckigt F, Strucksberg KH, Chevessier F, Winter L, Schütz J, Bauer R, Thorweihe JM, Wenzel D,
608 Schlötzer-Schrehardt U, Rasche V, Krsmanovic P, Katus HA, Rottbauer W, Just S, Müller OJ, Friedrich O, Meyer
609 R, Herrmann H, Schrickel JW, et al. The toxic effect of R350P mutant desmin in striated muscle of man and
610 mouse. *Acta Neuropathologica*. 2015; 129(2):297–315. doi: 10.1007/s00401-014-1363-2.
- 611 **Diermeier S**, Buttgereit A, Schürmann S, Winter L, Xu H, Murphy RM, Clemen CS, Schröder R, Friedrich O.
612 Preaged remodeling of myofibrillar cytoarchitecture in skeletal muscle expressing R349P mutant desmin.
613 *Neurobiology of Aging*. 2017; 58:77–87. doi: 10.1016/j.neurobiolaging.2017.06.001.
- 614 **Diermeier S**, Iberl J, Vetter K, Haug M, Pollmann C, Reischl B, Buttgereit A, Schürmann S, Spörrer M, Goldmann
615 WH, Fabry B, Elhamine F, Stehle R, Pfitzer G, Winter L, Clemen CS, Herrmann H, Schröder R, Friedrich O. Early
616 signs of architectural and biomechanical failure in isolated myofibers and immortalized myoblasts from
617 desmin-mutant knock-in mice. *Scientific Reports*. 2017; 7(1):1391. doi: 10.1038/s41598-017-01485-x.
- 618 **Durmuş H**, Ayhan Ö, Çırak S, Deymeer F, Parman Y, Franke A, Eiber N, Chevessier F, Schlötzer-Schrehardt U,
619 Clemen CS, Hashemolhosseini S, Schröder R, Hemmrich-Stanisak G, Tolun A, Serdaroğlu-Oflazer P. Neuro-
620 muscular endplate pathology in recessive desminopathies: Lessons from man and mice. *Neurology*. 2016;
621 87(8):799–805. doi: 10.1212/WNL.0000000000003004.
- 622 **Eddinger TJ**, Cassens RG, Moss RL. Mechanical and histochemical characterization of skeletal muscles
623 from senescent rats. *American Journal of Physiology*. 1986; 251(3 Pt 1):C421–30. doi: 10.1152/ajp-
624 cell.1986.251.3.C421.
- 625 **Edgerton VR**, Smith JL, Simpson DR. Muscle fibre type populations of human leg muscles. *Histochemical Journal*.
626 1975; 7(3):259–266.
- 627 **Friedrich O**, Hund E, von Wegner F. Enhanced muscle shortening and impaired Ca²⁺ channel function in an
628 acute septic myopathy model. *Journal of Neurology*. 2010; 257(4):546–555. doi: 10.1007/s00415-009-5362-5.
- 629 **Fry CH**, Harding DP, Miller DJ. Non-mitochondrial calcium ion regulation in rat ventricular myocytes. *Pro-*
630 *ceedings of the Royal Society of London Series B, Biological sciences*. 1989; 236(1282):53–77. doi:
631 10.1098/rspb.1989.0012.
- 632 **Gan Z**, Ding L, Burckhardt CJ, Lowery J, Zaritsky A, Sitterley K, Mota A, Costigliola N, Starker CG, Voytas DF,
633 Tytell J, Goldman RD, Danuser G. Vimentin Intermediate Filaments Template Microtubule Networks to
634 Enhance Persistence in Cell Polarity and Directed Migration. *Cell Systems*. 2016; 3(3):252–263.e8. doi:
635 10.1016/j.cels.2016.08.007.
- 636 **Gershlak JR**, Black LD. Beta 1 integrin binding plays a role in the constant traction force generation in response
637 to varying stiffness for cells grown on mature cardiac extracellular matrix. *Experimental Cell Research*. 2015;
638 330(2):311–324. doi: 10.1016/j.yexcr.2014.09.007.

- 639 **Haug M**, Reischl B, Pröls G, Pollmann C, Buckert T, Keidel C, Schürmann S, Hock M, Rupitsch S, Heckel M, Pöschel
640 T, Scheibel T, Haynl C, Kiriaev L, Head SI, Friedrich O. The MyoRobot: A novel automated biomechatronics
641 system to assess voltage/Ca²⁺ biosensors and active/passive biomechanics in muscle and biomaterials.
642 *Biosensors & Bioelectronics*. 2018; 102:589–599. doi: [10.1016/j.bios.2017.12.003](https://doi.org/10.1016/j.bios.2017.12.003).
- 643 **Haug M**, Meyer C, Reischl B, Pröls G, Vetter K, Iberl J, Nübler S, Schürmann S, Rupitsch SJ, Heckel M, Pöschel T,
644 Winter L, Herrmann H, Clemen CS, Schröder R, Friedrich O. The MyoRobot technology discloses a premature
645 biomechanical decay of skeletal muscle fiber bundles derived from R349P desminopathy mice. *Scientific*
646 *Reports*. 2019; 9(1):108. doi: [10.1038/s41598-019-46723-6](https://doi.org/10.1038/s41598-019-46723-6).
- 647 **JurcuȚ RO**, Bastian AE, Militaru S, Popa A, Manole E, Popescu BA, Tallila J, Popescu BO, Ginghină CD. Discovery
648 of a new mutation in the desmin gene in a young patient with cardiomyopathy and muscular weakness.
649 *Romanian Journal of Morphology and Embryology = Revue Roumaine de Morphologie et Embryologie*. 2017;
650 58(1):225–230.
- 651 **Kreplak L**, Herrmann H, Aebi U. Tensile properties of single desmin intermediate filaments. *Biophysical Journal*.
652 2008; 94(7):2790–2799. doi: [10.1529/biophysj.107.119826](https://doi.org/10.1529/biophysj.107.119826).
- 653 **Krivickas LS**, Suh D, Wilkins J, Hughes VA, Roubenoff R, Frontera WR. Age- and gender-related differences in
654 maximum shortening velocity of skeletal muscle fibers. *American Journal of Physical Medicine & Rehabilitation*.
655 2001; 80(6):447–455; quiz 456–7.
- 656 **Larsson L**, Edström L. Effects of age on enzyme-histochemical fibre spectra and contractile properties of fast-
657 and slow-twitch skeletal muscles in the rat. *Journal of the Neurological Sciences*. 1986; 76(1):69–89.
- 658 **Liem RKH**. Cytoskeletal Integrators: The Spectrin Superfamily. *Cold Spring Harbor Perspectives in Biology*.
659 2016; 8(10). doi: [10.1101/cshperspect.a018259](https://doi.org/10.1101/cshperspect.a018259).
- 660 **Lynch GS**, Rodgers BJ, Williams DA. The effects of age and low-intensity endurance exercise on the contractile
661 properties of single skinned fast- and slow-twitch skeletal muscle fibres. *Growth, Development, and Aging :*
662 *GDA*. 1993; 57(3):147–161.
- 663 **Mártonfalvi Z**, Kellermayer M. Individual globular domains and domain unfolding visualized in overstretched
664 titin molecules with atomic force microscopy. *PloS one*. 2014; 9(1):e85847. doi: [10.1371/journal.pone.0085847](https://doi.org/10.1371/journal.pone.0085847).
- 665 **Meyer GA**, Kiss B, Ward SR, Morgan DL, Kellermayer MSZ, Lieber RL. Theoretical predictions of the effects of
666 force transmission by desmin on intersarcomere dynamics. *Biophysical Journal*. 2010; 98(2):258–266. doi:
667 [10.1016/j.bpj.2009.10.014](https://doi.org/10.1016/j.bpj.2009.10.014).
- 668 **Meyer GA**, Lieber RL. Elucidation of extracellular matrix mechanics from muscle fibers and fiber bundles.
669 *Journal of Biomechanics*. 2011; 44(4):771–773. doi: [10.1016/j.jbiomech.2010.10.044](https://doi.org/10.1016/j.jbiomech.2010.10.044).
- 670 **Palmisano MG**, Bremner SN, Hornberger TA, Meyer GA, Domenighetti AA, Shah SB, Kiss B, Kellermayer M, Ryan
671 AF, Lieber RL. Skeletal muscle intermediate filaments form a stress-transmitting and stress-signaling network.
672 *Journal of Cell Science*. 2015; 128(2):219–224. doi: [10.1242/jcs.142463](https://doi.org/10.1242/jcs.142463).
- 673 **Powers JD**, Williams CD, Regnier M, Daniel TL. A Spatially Explicit Model Shows How Titin Stiffness Modu-
674 lates Muscle Mechanics and Energetics. *Integrative and comparative biology*. 2018; 58(2):186–193. doi:
675 [10.1093/icb/icy055](https://doi.org/10.1093/icb/icy055).
- 676 **Ra HJ**, Picart C, Feng H, Sweeney HL, Discher DE. Muscle cell peeling from micropatterned collagen: direct probing
677 of focal and molecular properties of matrix adhesion. *Journal of Cell Science*. 1999; 112 (Pt 10):1425–1436.
- 678 **Ramaswamy KS**, Palmer ML, van der Meulen JH, Renoux A, Kostrominova TY, Michele DE, Faulkner JA. Lateral
679 transmission of force is impaired in skeletal muscles of dystrophic mice and very old rats. *Journal of Physiology*.
680 2011; 589(Pt 5):1195–1208. doi: [10.1113/jphysiol.2010.201921](https://doi.org/10.1113/jphysiol.2010.201921).
- 681 **Schneidereit D**, Nübler S, Pröls G, Reischl B, Schürmann S, Müller OJ, Friedrich O. Optical prediction of single
682 muscle fibre force production using a combined biomechatronics-Second Harmonic Generation Imaging
683 approach. *Light: Science & Applications*. submitted 2018; .
- 684 **Stehle, R & Brenner, B** . Cross-Bridge Attachment during High-Speed Active Shortening of Skinned Fibers of
685 the Rabbit Psoas Muscle: Implications for Cross-Bridge Action during Maximum Velocity of Filament Sliding.
686 *Biophysical Journal*. 2000; 78(3):1458–1473. doi: [10.1016/S0006-3495\(00\)76699-9](https://doi.org/10.1016/S0006-3495(00)76699-9).

- 687 **Stelzer JE**, Widrick JJ. Effect of hindlimb suspension on the functional properties of slow and fast soleus fibers
688 from three strains of mice. *Journal of Applied Physiology* (Bethesda, Md : 1985). 2003; 95(6):2425–2433. doi:
689 [10.1152/jappphysiol.01091.2002](https://doi.org/10.1152/jappphysiol.01091.2002).
- 690 **Walter MC**, Reilich P, Huebner A, Fischer D, Schroder R, Vorgerd M, Kress W, Born C, Schoser BG, Krause KH,
691 Klutzny U, Bulst S, Frey JR, Lochmuller H. Scapulooperoneal syndrome type Kaeser and a wide phenotypic
692 spectrum of adult-onset, dominant myopathies are associated with the desmin mutation R350P. *Brain*. 2007;
693 130(6):1485–1496. doi: [10.1093/brain/awm039](https://doi.org/10.1093/brain/awm039).
- 694 **Waterman-Storer CM**. The cytoskeleton of skeletal muscle: is it affected by exercise? A brief review. *Medicine*
695 *and Science in Sports and Exercise*. 1991; 23(11):1240–1249.
- 696 **Williams DA**, Head SI, Lynch GS, Stephenson DG. Contractile properties of skinned muscle fibres from young
697 and adult normal and dystrophic (mdx) mice. *Journal of Physiology*. 1993; 460(1):51–67. doi: [10.1113/jphys-](https://doi.org/10.1113/jphysiol.1993.sp019458)
698 [iol.1993.sp019458](https://doi.org/10.1113/jphysiol.1993.sp019458).
- 699 **Winter L**, Wittig I, Peeva V, Eggers B, Heidler J, Chevessier F, Kley RA, Barkovits K, Strecker V, Berwanger C,
700 Herrmann H, Marcus K, Kornblum C, Kunz WS, Schröder R, Clemen CS. Mutant desmin substantially perturbs
701 mitochondrial morphology, function and maintenance in skeletal muscle tissue. *Acta Neuropathologica*. 2016;
702 132(3):453–473. doi: [10.1007/s00401-016-1592-7](https://doi.org/10.1007/s00401-016-1592-7).
- 703 **Wood LK**, Kayupov E, Gumucio JP, Mendias CL, Claflin DR, Brooks SV. Intrinsic stiffness of extracellular matrix
704 increases with age in skeletal muscles of mice. *Journal of Applied Physiology*. 2014; 117(4):363–369. doi:
705 [10.1152/jappphysiol.00256.2014](https://doi.org/10.1152/jappphysiol.00256.2014).

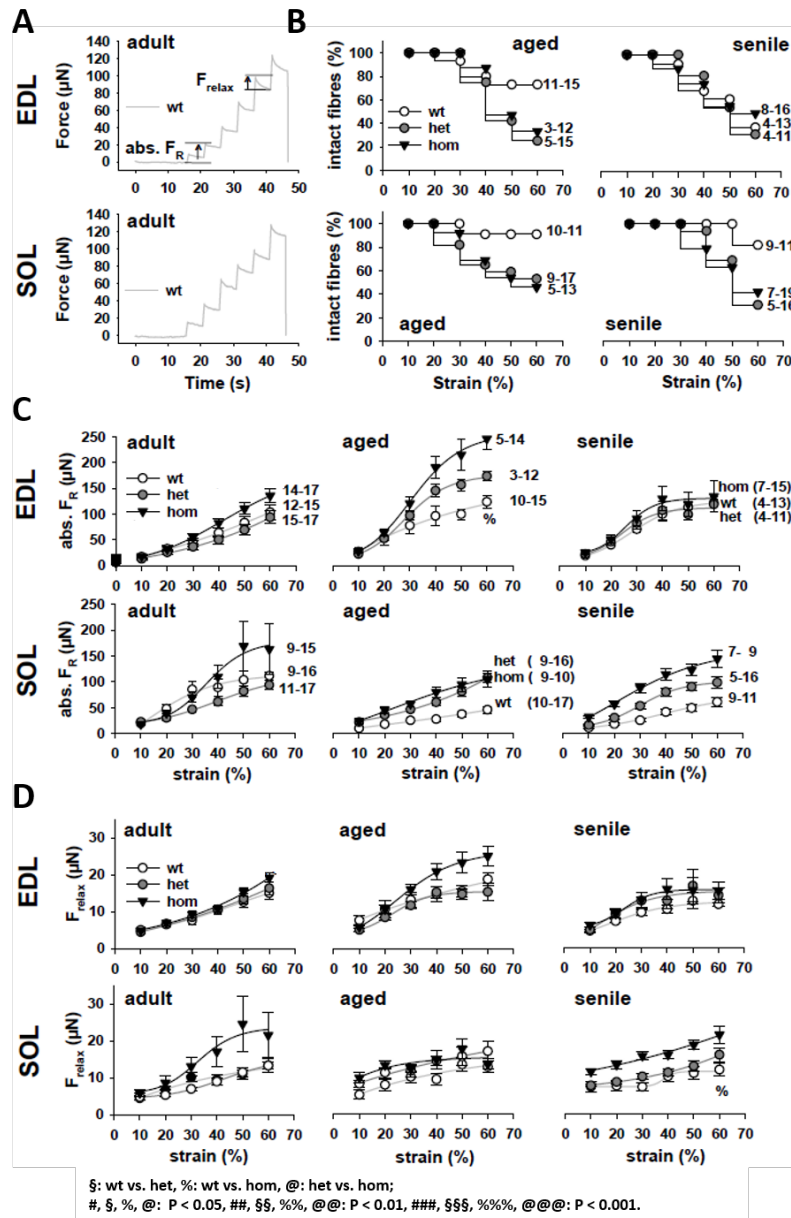


Figure 4. Visco-elastic behaviour of single muscle fibers from EDL and SOL muscle carrying the R349P desmin mutation during ageing. **A**, representative examples of quick step-stretch experiment protocols stretching adult EDL and SOL fibers in 10% bins to 160% L_0 . **B**, Kaplan-Meier curves displaying the percentage of intact fibers during the protocol demonstrate a worsened stretch-resistance of mutant fibers. **C**, group analysis of F_R across ages in EDL (top) and SOL (bottom) fibers showing overall increased absolute restoration force levels in the mutants over the wt for almost all ages and in both muscles. **D**, force relaxation amplitudes with stretch suggest almost similar viscous relaxation with a tendency for higher viscous relaxation in mutant fibers over the wt. Error bars: standard error.

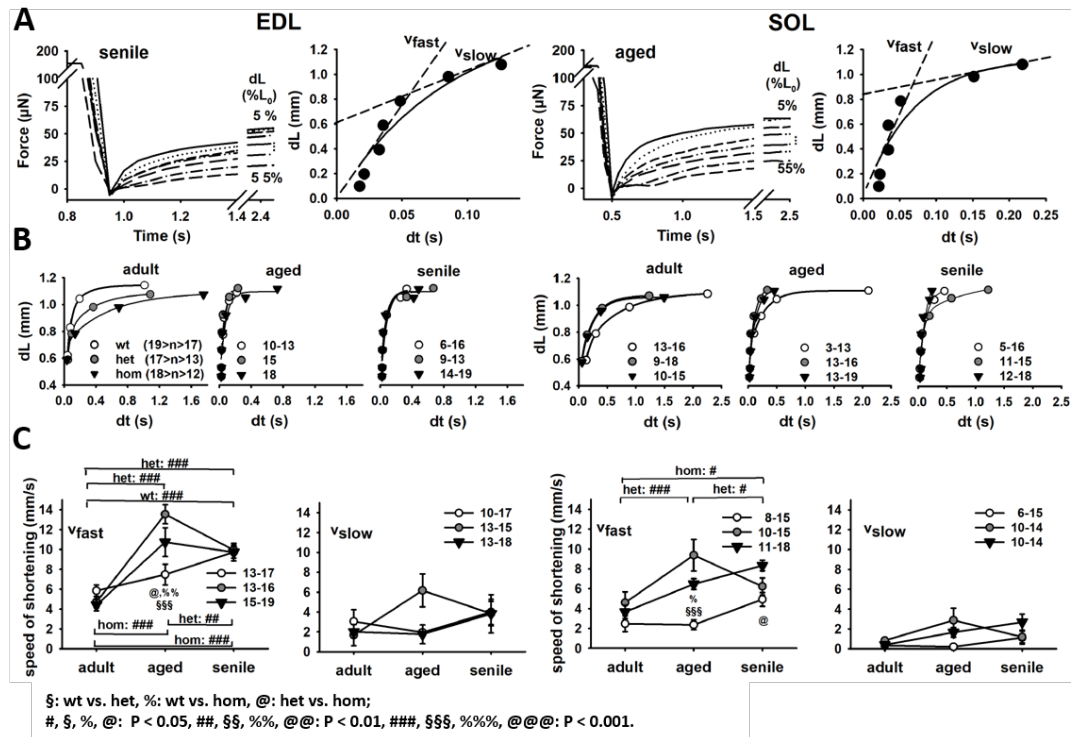
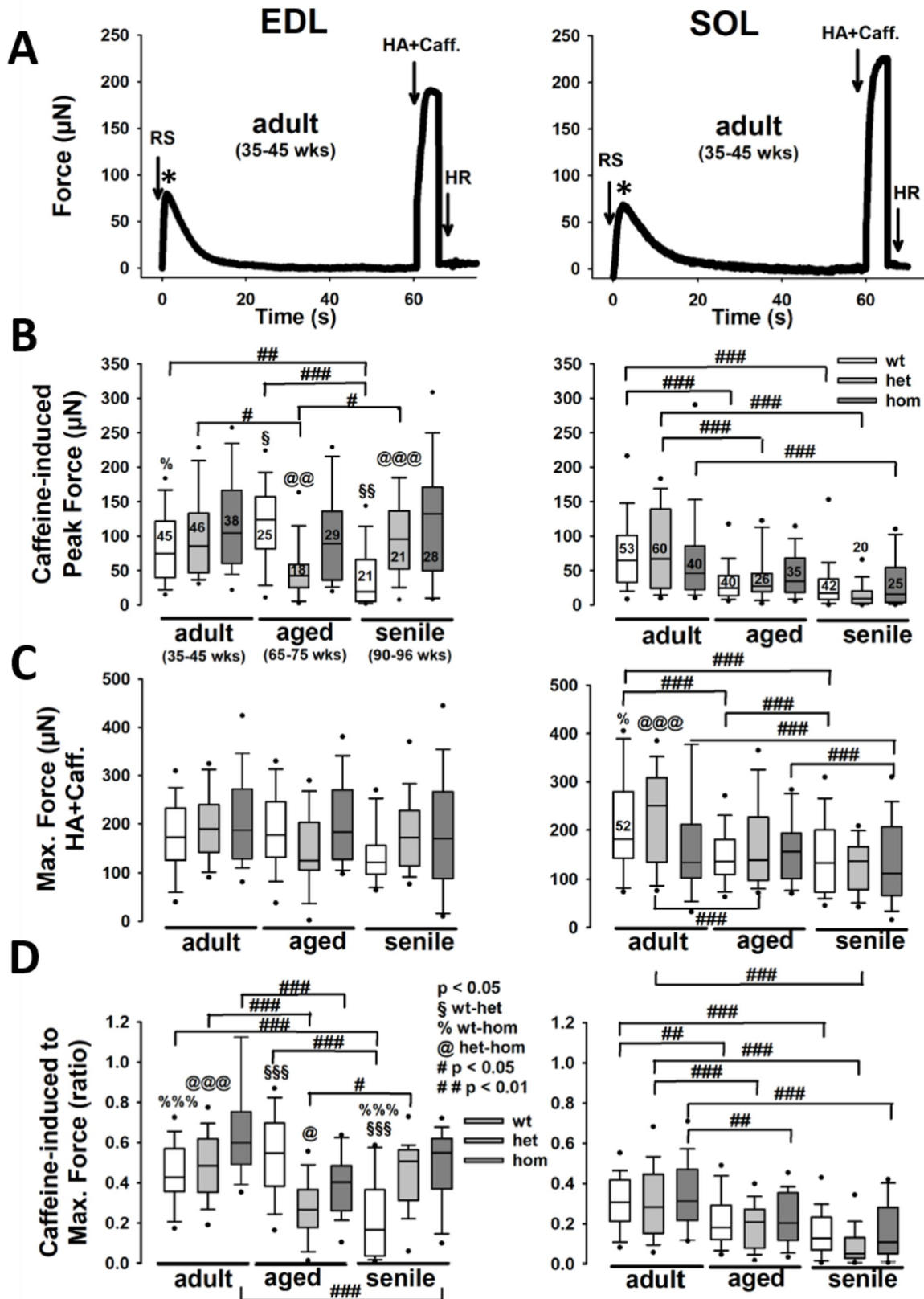
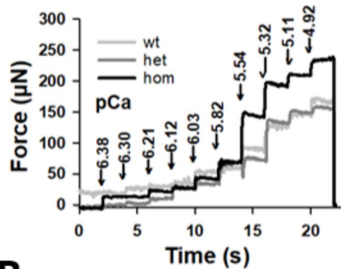
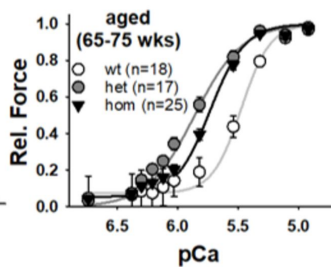
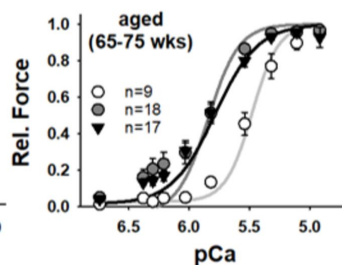
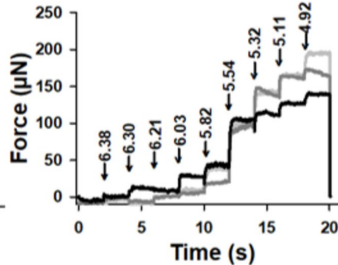
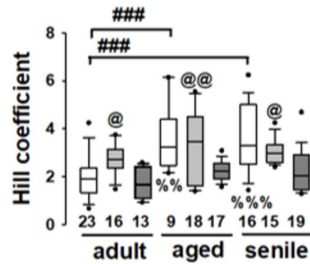
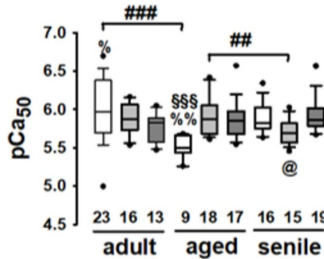
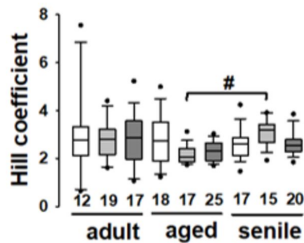
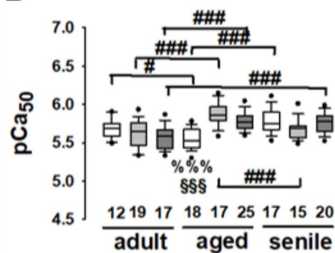


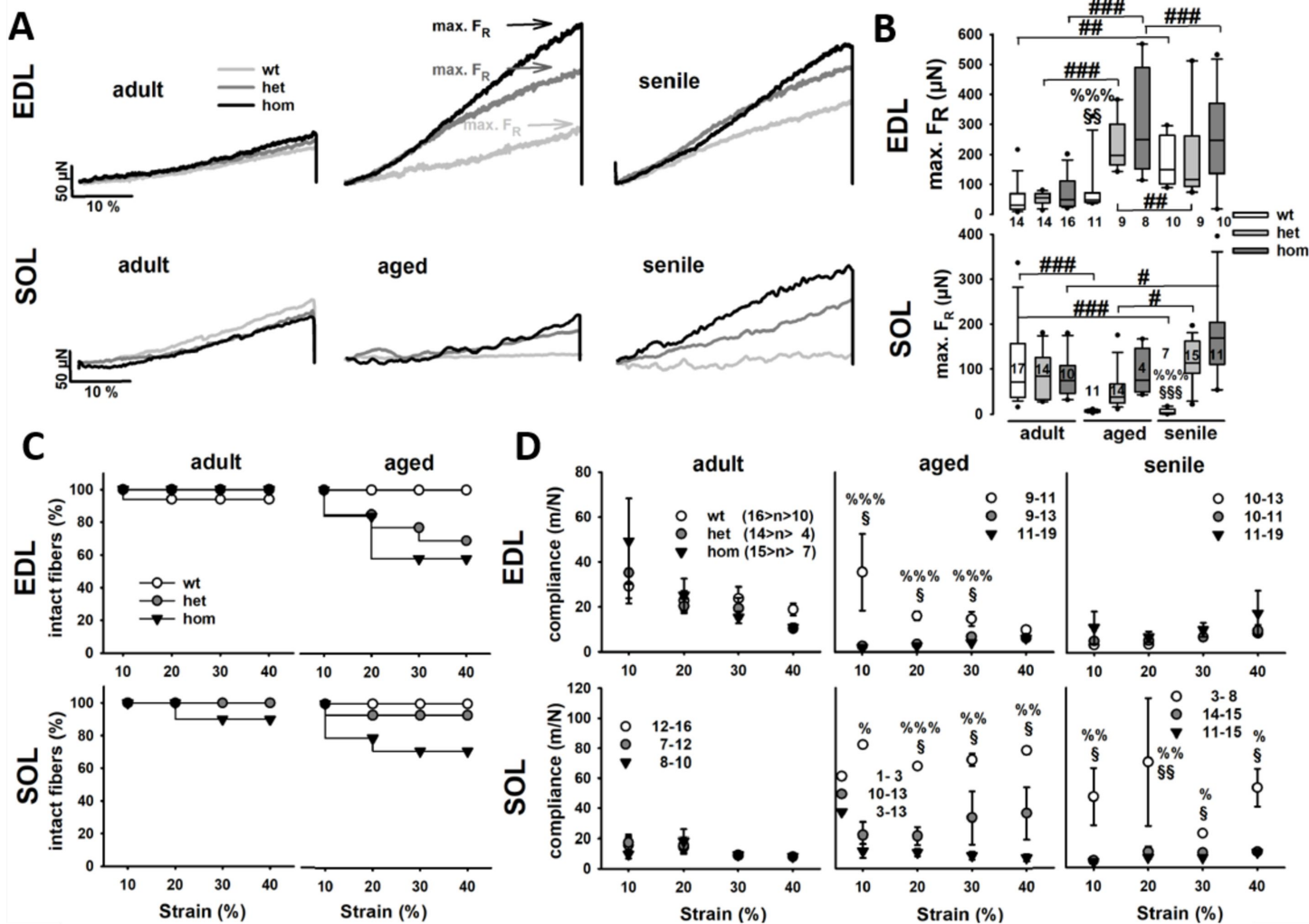
Figure 5. The fast phase of unloaded speed of shortening in single EDL and SOL fiber segments from adult, aged and senile R349P desmin mice is markedly increased in aged mutation-bearing fibers. A, representative 'slack-test' recordings of a single senile EDL (left) and aged SOL (right) fiber. The 'slack time' was extracted for each 'slack length' and the dL-dt relationship plotted in the right subpanels along with a biexponential fit and a linear velocity approximation in the lower dL (fast) and upper dL (slow) regime. **B,** group analyses of all single fibers from each genotype and age described by biexponential fit curves. The group analysis of the linear fast (v_{fast}) and slow (v_{slow}) phase for all fibers of each genotype and muscle is shown in **(C)**. Shortening speed consistently increased in wt fibers with age, while particularly het samples reveal a maximum shortening velocity for aged fibers. In hom fibers, shortening speeds also increased with age and only displayed a single decline for senile EDL muscle. Numbers next to symbol legends: number of single fibers analysed.



A**EDL****SOL****B**

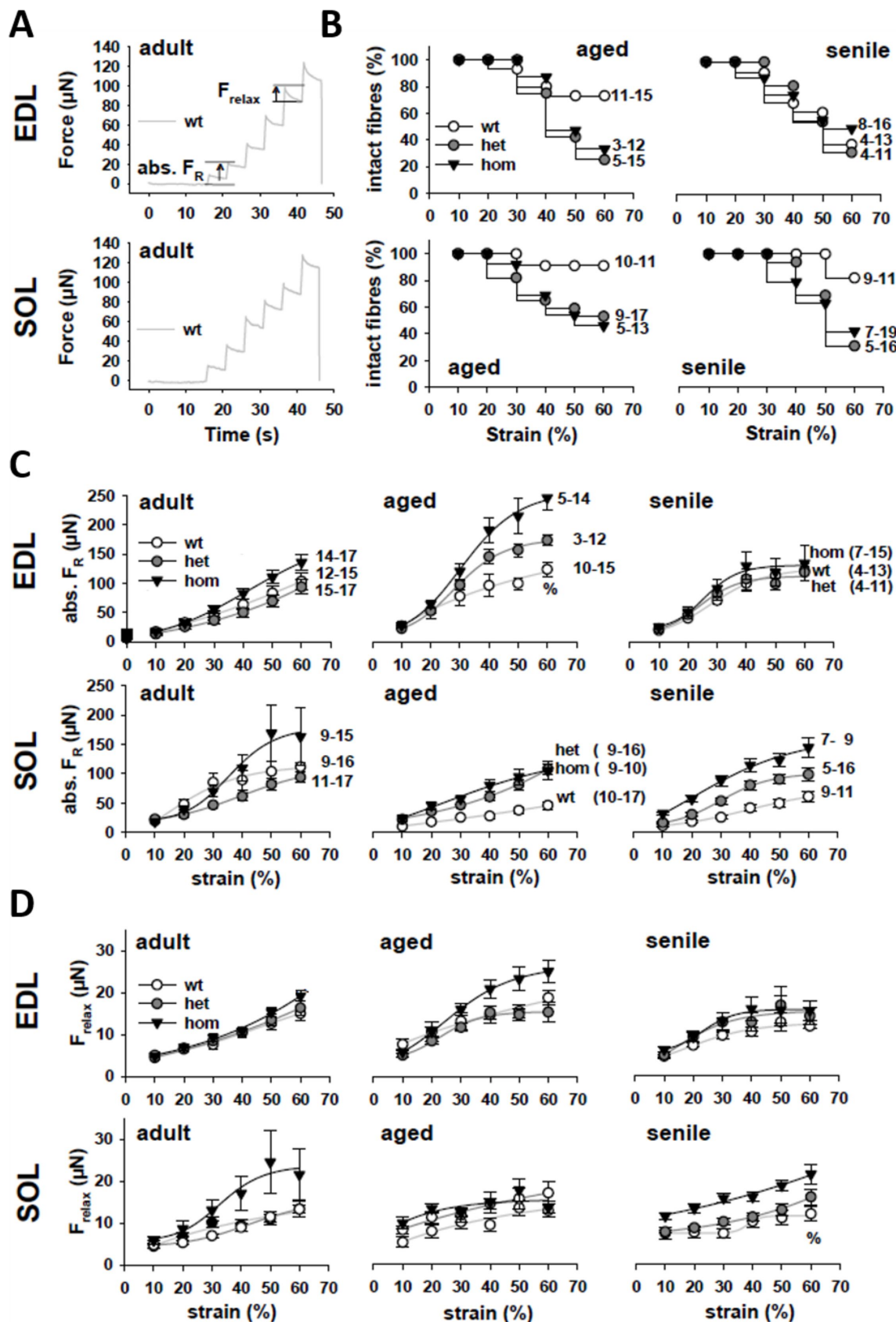
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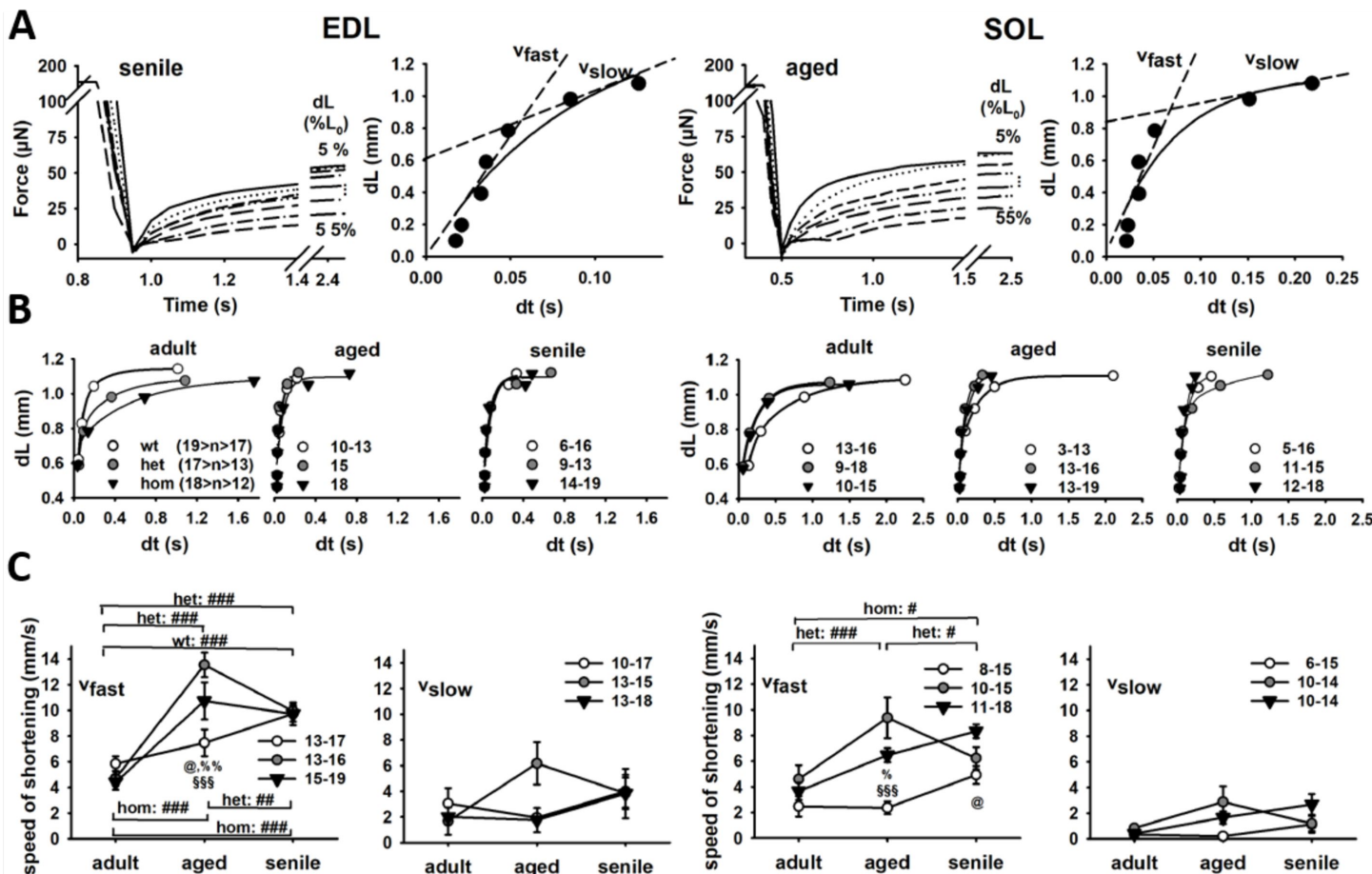
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§: wt vs. het, %: wt vs. hom, @: het vs. hom;

#, §, %, @: $P < 0.05$, ##, §§, %%, @@: $P < 0.01$, ###, §§§, %%%, @@@: $P < 0.001$.



§: wt vs. het, %: wt vs. hom, @: het vs. hom;

#, §, %, @: $P < 0.05$, ##, §§, %%, @@: $P < 0.01$, ###, §§§, %%%, @@@: $P < 0.001$.