Pectin methylesterase selectively softens the onion epidermal wall

yet reduces acid-induced creep

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Running title: Effects of pectin methylesterase on cell wall mechanics

Highlight

After enzymatic de-esterification without added calcium, the onion epidermal wall swells and

becomes softer, as assessed by nanoindentation and tensile plasticity tests, yet exhibits reduced

expansin-mediated creep.

Abstract

De-esterification of homogalacturonan (HG) is thought to stiffen pectin gels and primary cell walls by increasing calcium crosslinking between HG chains. Contrary to this idea, recent studies found that HG de-esterification correlated with reduced stiffness of living tissues, measured by surface indentation. The physical basis of such apparent wall softening is unclear, but possibly involves complex biological responses to HG modification. To assess the direct physical consequences of HG de-esterification on wall mechanics without such complications, we treated isolated onion (*Allium cepa*) epidermal walls with pectin methylesterase (PME) and assessed wall biomechanics with indentation and tensile tests. In nanoindentation assays, PME softened the wall (reduced the indentation modulus). In tensile force/extension assays, PME increased plasticity (but not elasticity). These softening effects are attributed to increased electrostatic repulsion and swelling of the wall after PME treatment. Despite softening and swelling upon HG de-esterification, PME treatment alone failed to induce cell wall creep. Instead, acid-induced creep, mediated by endogenous α-expansin, was reduced. We conclude that HG de-esterification physically softens the onion wall, but reduces expansin-mediated wall extensibility.

Key words

Atomic force microscopy, biomechanics, expansin, homogalacturonan, nano-indentation, onion (*Allium cepa*) epidermis, pectin methylesterase, plant cell wall mechanics, tensile testing, wall hydration.

Abbreviations

AFM: atomic force microscopy; HG: homogalacturonan, PME: pectin methylesterase, AFM: atomic force microscope, PG: endo-polygalacturonase, PL: pectate lyase, CMF: cellulose microfibril

Introduction

This study attempts to resolve some perplexing and apparently contradictory results concerning the influence of pectin de-esterification on the mechanics and extensibility of growing cell walls. Pectins are acidic polysaccharides that constitute a large proportion of the cell wall in primary cells of many plant species and are particularly dominant in cell walls of some Charophycean algae (Domozych *et al.*, 2014) and the tips of pollen tubes (Chebli *et al.*, 2012). Homogalacturonan (HG) constitutes the most abundant pectic component of the primary wall (Atmodjo *et al.*, 2013). It is synthesized in methyl esterified form in the Golgi system, deposited to the cell wall, and subsequently de-esterified *in muro* by pectin methylesterases (PMEs) (Wolf *et al.*, 2009). Methyl esters block the charged carboxylates of galacturonic acid residues that make up the HG backbone; methyl esters influence the physico-chemical properties of HG, particularly its net charge and charge distribution, its gelling ability and its interactions with cations, notably calcium (Jarvis, 1984; John *et al.*, 2019; MacDougall *et al.*, 1996; Willats *et al.*, 2001).

In vivo, HG de-esterification by PME has often been associated with wall stiffening and growth cessation (Goldberg *et al.*, 1989; Goldberg *et al.*, 1996; Hongo *et al.*, 2012; Siedlecka *et al.*, 2008). Calcium crosslinking of de-esterified regions of HG is presumed to stiffen the wall, e.g. Bou Daher *et al.* (2018), but quantification of calcium crosslinking is challenging (Hocq *et al.*, 2017) and the idea that calcium-mediated wall stiffening limits cell wall growth is not well supported, e.g. (Coartney and Morre, 1980; Virk and Cleland, 1990). Moreover, the concept of wall stiffness is not as simple as it once seemed, as indentation stiffness (normal to the plane of the cell wall) can vary independently of tensile stiffness (in the plane of the cell wall), e.g. Zhang *et al.* (2019). There is evidence that HG may limit the loosening action of expansins as cells cease growth (Wei *et al.*, 2010; Zhao *et al.*, 2008), but whether this results from wall stiffening or from interference with expansin action by another means is uncertain. In the special case of pollen tubes, regions of low HG esterification on the flanks of the tip coincide with cell wall regions of high stiffness and reduced surface enlargement, potentially connected with calcium crosslinking of HG (Chebli *et al.*, 2012; Zerzour *et al.*, 2009).

Contrary to these ideas, other studies reported an opposite pattern in which regions of low HG esterification at the surface of *Arabidopsis thaliana* shoot apical meristems coincided with

regions of cell expansion or low mechanical stiffness, as measured by surface micro-indentation

with a 5-μm bead driven by an AFM (atomic force microscope) (Braybrook and Peaucelle, 2013;

Peaucelle *et al.*, 2011; Peaucelle *et al.*, 2008). Another study assessing the effect of PME activity

on Arabidopsis hypocotyls reported a similar trend (Peaucelle *et al.*, 2015). The basis for reduced

stiffness in regions of reduced esterification, where high stiffness would generally be expected, is

uncertain. Various speculative possibilities have been proposed, but not yet tested: (a) with

limited Ca^{2+} supply, de-esterified HGs may not become ionically crosslinked, instead resulting in

a more fluid HG; (b) de-esterified HGs may be degraded by endogenous endo-polygalacturonase

(PG) or pectate lyase (PL); and (c) PME activity may acidify the wall, potentially activating

expansins or weakening physical interactions between pectin and cellulose, e.g. Phyo *et al.*

(2019). In addition to these biochemical possibilities, HG modifications *in vivo* may trigger

complex biological responses involving wall integrity sensors, brassinosteroids , auxin and other

signaling pathways, with undefined consequences for cell wall properties (Braybrook and

Peaucelle, 2013; Wolf *et al.*, 2012). Reviews of this topic point out the many complications

involved in relating growth and wall mechanics to HG methylesterification (Levesque-Tremblay

et al., 2015; Peaucelle *et al.*, 2012). These considerations highlight the difficulty and uncertainty

in ascribing a direct causal relationship between pectin esterification and wall mechanics in

growing organs.

With these points in mind, we designed an *in-vitro* experimental approach to identify the

direct consequences of PME action on wall mechanics and extensibility, without the

complications and secondary responses likely in living cells. Although *in-vitro* experiments have

demonstrated Ca^{2+}-mediated stiffening of pectic gels by PME (Willats *et al.*, 2001), there

appears to be scant information about the direct (physical) consequences of PME action on cell

wall biomechanics.

For this study we used the cell-free outer periclinal wall from the onion scale epidermis,

because it lends itself to nano-scale indentation and macro-scale tensile tests (Zhang *et al.*, 2019;

Zhang *et al.*, 2017). The outer epidermal wall represents a major structural restraint to growth of

many organs (Cosgrove, 2018b; Galletti *et al.*, 2016; Kutschera, 1992; Kutschera and Niklas,

2007) and epidermal wall stresses may participate in feedback loops that modulate microtubule

patterns and morphogenesis, e.g. Verger *et al.* (2018). Because cell walls are inherently

anisotropic, we probed PME effects on wall biomechanics with both tensile and indentation
assays.

As described elsewhere (Cosgrove, 2018a; Zhang *et al.*, 2019), we make a distinction
between wall softening and wall loosening: 'softening' makes the wall more deformable to
mechanical force (a purely mechanical concept) whereas 'loosening' induces wall stress
relaxation, leading to irreversible wall enlargement, an essential aspect of cell growth and
morphogenesis. Loosening is conveniently measured by creep of a cell wall (slow, irreversible
extension that depends on wall modifying agents such as expansin) whereas softening is
measured with force/extension assays that assess wall stiffness. In their simplest forms,
indentation assays measure out-of-plane wall stiffness while tensile assays measure in-plane
stiffness. As shown below, PME does soften the wall in some (but not all) respects, yet does not
display loosening activity and in fact diminishes the loosening action of endogenous expansins.

Materials and methods

Cell wall preparation

White onion bulbs (*Allium cepa*), ~15 cm in diameter, were purchased from local grocery stores.
The 5th scale, with the 1st being the outermost fleshy scale, was used to make epidermal peels.
Abaxial epidermal cells were torn open by peeling 3-mm or 5-mm wide strips midway along the
apical-to-basal gradient of the scale, as described previously (Zhang *et al.*, 2014; Zhang *et al.*,
2019). The epidermal peels were washed with 20 mM HEPES (4-(2-hydroxyethyl)-1-
piperazineethanesulfonic acid), pH 7.5, with 0.01% (v/v) Tween 20 for 15 min to eliminate the
residual cytoplasmic debris, then dipped in boiling methanol for 30 s to deactivate endogenous
wall enzymes while retaining α-expansin activity (Cosgrove and Durachko, 1994).

Pectin methylesterase

Recombinant PME from *Streptomyces avermitilis* (Cat NO.: PRO-E0233, 27.5 units/mg),
characterized as a processive enzyme by the supplier (PROZOMIX, Haltwhistle, UK), was
desalted with 3 kDa centrifugal filters (Merck Millipore, Tullagreen, IRL) and diluted to 50
μg/mL in 20 mM HEPES, pH 7.5, for all experiments except where noted.

Antibody labeling

A strip of onion epidermal wall (10 mm × 10 mm) was placed onto a glass slide with the inner

surface facing upward and affixed by sealing the edges with nail polish. The exposed epidermal

wall inner surface was submerged in 20 mM HEPES pH 7.5 ± 50 μg/mL PME for 2 h. The

samples were then washed with 1× PBS (phosphate-buffered saline) three times. To block the

wall, 1× TBS (tris-buffered saline) based blocking agent containing 10% (w/v) horse serum, 2

mM sodium azide, and 0.01% (v/v) Tween 20 was dropped onto the exposed wall surface for 1

h. JIM7 or LM19 antibodies (PlantProbes, Leeds, UK), diluted 10×, were bound to the wall

surface for 1 h, followed by addition of 100× diluted secondary antibody: FITC-linked anti-rat

IgG (Thermo Fisher Scientific, Rockford, IL) for an additional 1 h. Samples were washed

extensively with 1× PBS three times at the end of each antibody labeling step. Labeled wall

samples were imaged under an Olympus BX63 microscope using the FITC channel (λex = 490

nm, λem = 525 nm).

Methanol release quantification of saponification and PME activity

Methanol quantification was based on the alcohol oxidase method (Klavons and Bennett, 1986).

Onion wall strips (3 mm × 10 mm) were peeled, washed with 20 mM HEPES pH 7.5 with 0.01%

(v/v) Tween 20 for 15 min, and boiled in water for 10 s to inactivate endogenous PME and other

wall enzymes. Three wall strips were incubated in 500 μL 20 mM HEPES pH 7.5 for 0.5, 1, 1.5,

3, 6, and 16 hours in the presence of 50 μg/mL PME. A negative control was prepared by

incubating heat-inactivated wall strips in buffer for 16 h. For quantifying the total saponifiable

methyl esters in the wall, three wall strips were placed in 500 µL 1 M NaOH for 1 h. The

supernatant was collected from each sample and filtered through a 0.4 µm centrifugation filter.

For the NaOH saponified samples, 10 M HCl was used to adjust the pH to 7.5. Alcohol oxidase

(# A2404, Sigma Aldrich, Saint Louis, MO) was added in the amount of 0.03 U to the filtered

supernatant and the volume was adjusted to 1 mL with 20 mM HEPES pH 7.5. The mixture was

incubated at 26°C for 15 min. A total of 500 µL assay solution (20 mM acetyl acetone, 50 mM

acetic acid, and 2 M ammonium acetate) was then added to the reaction followed by incubation

at 60°C for 15 min. The reaction was cooled to room temperature before the absorbance was

assessed at 412 nm. A standard curve was generated using 1, 2, 4, 8, and 16 µg methanol.

AFM imaging and nanoindentation

Onion epidermal walls were fixed onto a glass slide by nail polish and the exposed wall surface

was immersed in 20 mM HEPES pH 7.5. AFM topography images were captured with a

Dimension Icon AFM (Bruker, CA, USA) with a ScanAsyst-Fluid+ probe (nominal spring

constant: 0.7 N/m). The silicon tip of the probe has a triangular pyramid shape, 2.5 – 8.0 µm in

height with a 15 ± 2.5^o front angle, 25 ± 2.5^o back angle and 2 nm tip radius. The AFM was

operated in PeakForce Tapping mode with ScanAsyst and quantitative nanomechanical mapping.

For nanoindentation, wall samples were affixed by double-sided tape on a glass slide and the

edges were sealed with nail polish (Zhang *et al.*, 2014). Walls were incubated in 20 mM HEPES

pH 7.5 buffer and a series of nanoindentations were carried out using a Bruker Dimension Icon

AFM equipped with a ScanAsyst-Fluid+ tip. The deflection sensitivity of the AFM tip was

obtained by tapping onto the glass slide (Butt *et al.*, 2005). The spring constant of the tip was

then calibrated using a thermal tune method (Hutter and Bechhoefer, 1993). A target force of 4

nN was used for the nanoindentation experiments with the ramp size set at 500 nm and ramp

speed of 3 µm/s. Five spots (100 nm apart on a straight line parallel to the cell long axis) per cell

were chosen for indentation measurements using the Autoramp function in the Nanoscope

software (Bruker). For each wall sample, 10 cells at random locations were used. Wall samples

were then incubated in HEPES buffer ± PME on the AFM stage for 3 h and indentations were

conducted again for the same X-Y coordinates. The indentation modulus was calculated using

the 10% – 90% region of the force curve and the Sneddon model (Sneddon, 1965) in the

Nanoscope Analysis program (Bruker).

Tensile test (force/extension)

Onion wall strips (3 mm × 10 mm) were prepared the same way as in the methanol release

experiment. Three strips were placed in a 2 mL centrifuge tube with addition of 500 µL 20 mM

HEPES pH 7.5 buffer. For PME treatment, walls were treated with 50 µg/mL PME in HEPES

buffer. The incubation was done on a shaking block at 26^oC, 500 rpm. Tensile tests were

conducted on a custom extensometer (Durachko *et al.*, 2017). Preliminary assays showed that

walls given a 16-h PME pretreatment showed more consistent results than shorter incubations,

therefore the 16-h treatment was used. To assess cation effects on wall tensile compliances, 100

mM $CaCl_2$ or $MgCl_2$ was added to the PME-treated and control walls followed by an additional

2-h incubation.

Wall strips were clamped on both ends with two clamps that were 3 mm apart, then extended

at 3 mm/min until a load of 10 g (0.1 N) was reached. Subsequently, two clamps were returned

to the original position. Wall samples were extended again with the same load to assess the

elastic properties of wall samples. A least-squares fit to the last 10% of each recorded

force/extension curve was used to calculate the total compliance and elastic compliances, with

the plastic compliance calculated as the difference (Durachko *et al.*, 2017). Compliance is the

reciprocal of stiffness or modulus.

Creep and stress relaxation

Creep experiments were carried out at 26°C by clamping wall strips (3×10 mm; 5 mm between

clamps) in a cuvette filled with buffer, applying a constant tensile force with a 10 g weight (=0.1

N force) and monitoring specimen length (Durachko *et al.*, 2017). To assess PME's effects on

endogenous acid-induced creep, methanol-boiled wall samples were pre-incubated in HEPES pH

7.5 ± 50 µg/mL PME for 16 h at 26°C. Methanol boiling inactivates endogenous enzymes but not

expansins. To measure acid-induced extension, walls were clamped in neutral buffer [20 mM

MES (2-(N-morpholino) ethanesulfonic acid), pH 6.8, with 2 mM dithiothreitol (DTT)]. When

the extension rate became constant, the buffer was replaced with acidic buffer (20 mM NaOAC,

pH 4.5, containing 2 mM DTT) to induce expansin-mediated extension. DTT is added to

stabilize expansin activity.

To test the ability of PME alone to induce cell wall extension, methanol-boiled walls were

clamped in the extensometer in 20 mM HEPES pH 7.5 buffer, as described above. After

stabilization of the creep rate, the buffer was exchanged for the same buffer containing 100

µg/mL PME.

To test the effect of buffer pH on wall stress relaxation, 5 mm $\times$ 10 mm wall strips were

briefly pre-incubated in 20 mM MES pH 6.8 or NaOAC pH 4.5 buffers, with 2 mM DTT, then

clamped a custom extensometer with 5 mm between clamps and extended to 120% of their

original length, corresponding to a 30 g (294 mN) load. The decay in holding force was then

monitored for 5 min. A small droplet of buffer was positioned at the base of the wall sample to

maintain hydration of the sample during the measurement, which was carried out at 26°C. The

force decay curves were smoothed using Origin 9.1 (OriginLab, Northampton, MA) and the

relaxation rate was calculated by taking the derivative of stress decay as a function of $\log_{10}$ time.

To test the effect of PME on stress relaxation, wall samples were pre-incubated in 20 mM

HEPES buffer pH 7.5 ± 50 µg/mL PME for 3 h at 26°C, then clamped and stretched as detailed

above.

Onion scale cross-section

A tissue piece (3 mm × 3 mm × 10 mm) was cut from the 5th scale with the longer edge parallel

to the cell long axis. The onion piece was then placed under a dissecting microscope with the

abaxial side facing upward. A razor blade was aligned parallel with the shorter edge in order to

make 0.4-mm-thick cross sections by hand. Sections were boiled in methanol for 30 s and

stained with 0.1 % toluidine blue (in 20 mM HEPES pH 7.5) for 1 min followed by water washes

until the water appeared colorless. One section was placed on a glass slide and an O-ring shaped

piece of double-sided tape was used for spacing between the glass slide and cover slip. Images of

wall cross sections were acquired after 0 h and 3 h incubation in HEPES buffer ± PME at 26°C

using a 20× objective by an Olympus X63 microscope equipped with a color camera

Zeta potential measurements

Onion epidermal walls were pulverized at 30 Hz shaking for 10 min (Retsch Cryomill) to

produce wall fragments (~10 µm in diameter) suitable for zeta-potential measurements. Cell

walls were as alcohol-insoluble residues following the protocol of Pettolino *et al.* (2012). In

brief, wall fragments were incubated in 70% ethanol for 30 min followed by two washes in

chloroform : methanol (1:1) for 5 min and one wash in absolute acetone (5 min). Wall fragments

were then extensively washed with water; fragments that remained in the suspension after 15 min

of settling were collected by filtration and freeze dried. One mg of wall was resuspended in 1 mL

buffer and incubated for 16 h at 26°C with 50 µg/mL PME or with 50 µg/mL bovine serum

albumin (BSA), a basic protein without wall-specific activity (=negative control). A Zetasizer

(Malvern, UK) was used to assess cell wall zeta-potential.

Image analysis for surface roughness measurement

AFM height images of onion wall surface were flattened using the Nanoscope Analysis program

(Bruker) to correct for image tilting. Surface roughness was estimated using the built-in

measurement of Nanoscope Analysis program with the zero crossing enabled under peak

characterization (Longuet-Higgins, 1957). Since the PME treatment masked the edge detection

of cellulose microfibril, it is anticipated that the peak density (density of detected edges of

cellulose microfibril) would decrease upon PME treatment.

Results

Experimental design

To assess the effect of HG esterification on cell wall mechanics, outer periclinal walls of onion

scale epidermis were prepared as cell-free strips suitable for tensile and indentation assays

(Zhang *et al.*, 2019). This pectin-rich wall has a cross-lamellate structure (Zhang *et al.*, 2016),

typical of many outer epidermal walls. Endogenous enzymes were inactivated with a brief

pretreatment of the walls in hot methanol, which minimizes pectin degradation (Merrill and

Weeks, 1945) and retains endogenous α-expansin activity (Cosgrove, 1989; McQueen-Mason *et*

al., 1992). This pretreatment enabled us to measure both expansin-mediated cell wall creep (to

assess wall loosening) and wall stiffness by indentation and tensile tests (to assess wall

softening) in samples treated ± PME.

De-esterification by PME

Wall strips were incubated for 2 h in 20 mM HEPES buffer, pH 7.5, ± 50 µg/mL PME, which

hydrolyzes methyl esters of HG. PME effectiveness was assessed qualitatively by

immunofluorescence microscopy with monoclonal antibodies JIM7 and LM19 to detect HG of

high and low degree of methylesterification, respectively (Verhertbruggen *et al.*, 2009). For

buffer-treated walls, labeling by JIM7 and LM19 was most intense for the torn anticlinal walls

and the cell borders, with signs of weaker, diffuse labeling of the cell wall proper (Fig. 1A). The

labeling pattern indicates the epidermal wall contains a mixture of HG of high and low

esterification. After PME treatment, the JIM7 signals were reduced whereas LM19 signals

increased, confirming HG de-esterification by PME.

To quantitatively assess the rate and extend of de-esterification, PME-catalyzed release of

methanol was measured as a function of time (Fig. 1B). PME acted rapidly and approximately

linearly for the first three hours, after which the rate slowed down and approached a plateau after

the sixth hour. Approximately 42% of the total saponifiable methyl ester was released during

PME treatment for 16 h. Based on this time course, the effect of a 3-h PME treatment, releasing

~27% of the total saponifiable methyl ester in the wall, was tested in wall biomechanical assays.

PME softens the wall in nanoindentation assays

Wall strips were placed cuticle side down on the AFM stage, submerged in buffer, and the upper

surface was indented with a sharp pyramidal AFM probe (nominal tip radius 2 nm). This

procedure indented the most recently-deposited cell wall surface. The tip pressed ~120-150 nm

into the wall, corresponding to the depth of 3-4 lamellae (Zhang *et al.*, 2016), before reaching the

target force of 4 nN (Fig. 2A). There was little hysteresis between the extend and retract curves,

indicating predominantly elastic indentation with little viscoelastic dissipation.

After 3-h incubation in buffer ± PME, a second set of indentations were made (Fig. 2A, B).

The force/extension curves showed the PME-treated walls to be substantially softer than buffer

controls. Wall stiffness was quantified as an indentation modulus calculated by the Sneddon

model, as appropriate for a sharp pyramid-shaped probe. Because of uncertainties in the shape of

wall deformation during indentation, we view the calculated modulus as an ad-hoc estimate of

wall indentation stiffness rather than an accurate estimate of the wall modulus. Buffer-treated

walls became slightly stiffer after 3 h, but the difference was not statistically significant (Fig.

2C). In contrast, stiffness of the PME-treated walls was reduced by 65%. These results revealed a

wall-softening action by PME that reduced the nano-indentation stiffness of this wall. Note that

external calcium was not included in the buffer, so this represents the direct effect of PME in a

calcium-limited situation. This result supports previous speculation that PME action might

increase the fluidity of HG when calcium was limiting (Peaucelle *et al.*, 2008). Previous work

showed that calcium addition or removal increases or decreases the indentation stiffness of onion

epidermal walls, respectively (Xi *et al.*, 2015; Zhang *et al.*, 2014; Zhang *et al.*, 2019), so external

calcium availability was not varied in these specific experiments.

PME potentiates macro-scale plastic deformation in tensile testing

A custom extensometer was used to assess PME's effect on wall tensile stiffness. Following a

conventional protocol (Durachko *et al.*, 2017), onion wall strips were stretched and relaxed twice

in succession. The second extension is reversible and the slope of the last 10% of the curve is

used to calculate an elastic compliance (=slope of the line). Compliance is inversely related to

stiffness and modulus. Because the shape of the force/extension curve is nonlinear, compliance

values vary with strain. The first extension combines elastic and plastic extensions and is used to

calculate a total compliance. A plastic compliance is obtained as the difference between total and

elastic compliances. With 0.1 N tensile force, buffer-treated wall strips extended ~9.5% whereas

after PME treatment the extension was ~12% (Fig. 3A). The additional extension of the PME-

treated walls resulted from an increased plastic compliance, whereas the elastic compliance was

not significantly affected (Fig. 3B). These results show that PME softens the onion wall in a

selective manner, increasing plastic but not elastic deformation.

In these experiments, exogenous calcium was not added to the walls, so enhanced calcium

crosslinking of HG after PME treatment was unlikely. We found that addition of 100 mM $CaCl_2$

had little effect on the elastic or plastic compliances of buffer-treated walls (Fig. 4), whereas

with PME pretreatment the plastic compliance was reduced by 32% (Fig. 4). Thus, HG de-

esterification reduced wall plasticity in the presence of abundant Ca^{2+}, increased plasticity

without added Ca^{2+}, and had no effect on the elastic compliance in either case.

We also tested the effect of 100 mM $MgCl_2$ because Mg^{2+} does not form strong ionic

crosslinks with HG, yet can shield negative charges on the HG backbone (Thibault and Rinaudo,

1986). Mg^{2+} slightly reduced the plastic compliance of buffer-treated walls (not statistically

significant) and completely negated PME-mediated softening (Fig. 4). These results suggest that

PME-mediated plastic softening depends on the increased negative electrostatic charge of de-

esterified HG. Consistent with this interpretation, zeta potential measurements confirmed that

PME-treated walls have a more negative zeta potential than control walls (-23.3 $\pm$ 0.41 mV for

PME treated versus -17.0 $\pm$ 0.35 mV for BSA control, Fig. 5). Thus, PME treatment had two

opposing effects: by itself it increased the plastic compliance, an effect nullified by electrostatic

shielding of Mg^{2+}, and it enabled greater interaction with exogenous Ca^{2+}, reducing plasticity.

Cell wall swelling upon de-esterification

Electrostatic repulsion between pectin carboxylates generated by PME action could lead to

increased hydration and swelling of the cell wall. In light of this idea, we tested whether PME

treatment caused onion wall swelling, assessed microscopically as epidermal wall thickness (Fig.

6A). The average thickness of onion epidermal wall increased from 6.2 $\pm$ 0.3 µm in buffer to 7.3

$\pm$ 0.2 µm after 3-h incubation with PME (Fig. 6B), whereas incubation in buffer alone did not

alter wall thickness significantly. Thus, we conclude that HG de-esterification indeed enhanced

wall hydration.

PME treatment reduces cellulose microfibril resolution by AFM imaging

To assess the PME effect on the arrangement of cellulose microfibrils, we used the AFM to image the same wall surface before and after PME treatment. Distinct microfibril features can usually be resolved by AFM on the surface of native onion epidermal walls (Zhang *et al.*, 2014; Zhang *et al.*, 2016). After PME treatment, microfibril features appeared blurred (Fig. 7). The blurring effect may be the result of swollen HG chains near and between individual and bundled microfibrils, causing the AFM tip to glide over the surface without dropping into the spaces between microfibrils. To test this idea we measured surface roughness of AFM height maps before and after PME treatment. Surface roughness, as measured by peak density, was reduced by 47% as a result of PME treatment (Supplementary Fig. S1).

PME does not induce cell wall loosening

Creep and stress relaxation assays were used to assess PME's ability to induce cell wall loosening. The stress relaxation assay measures the time-dependent decay in wall stress after the wall is extended and then held at constant length, whereas the creep assay measures the time-dependent increase in length when the wall is clamped at constant tensile force (Cosgrove, 2016). In stress relaxation assays of onion epidermal walls, acidic pH, which activates the endogenous α-expansins, enabled faster stress relaxation (Fig. 8A), whereas PME treatment resulted in a negligible change in stress relaxation (Fig. 8B).

For the creep experiments, wall strips were clamped at 0.1 N tension in neutral buffer and after the length stabilized the buffer was swapped for one containing PME. Length remained nearly constant for the duration of the experiment (90 min) and was not increased by PME addition (Fig. 9A). Thus we did not find evidence of PME-mediated wall loosening in either creep or stress relaxation assays.

We also tested whether PME pretreatment affected acid-induced extension, mediated by endogenous α-expansins. Wall strips, which were treated with hot methanol to inactivate endogenous PME and other enzymes but not endogenous α-expansins (McQueen-Mason *et al.*, 1992), were pre-incubated in neutral buffer ± PME, then clamped at neutral pH in the constant-force extensometer, and tested for acid-induced extension by exchanging the neutral buffer for pH 4.5 buffer. The walls extended rapidly in acidic buffer. Sustained creep was diminished by

~50% in the PME-treated walls compared with buffer-treated controls (Fig. 9B). Thus, despite

the increase of wall hydration, tensile plasticity, and nanoindentation by PME, expansin-

mediated creep was reduced. We conclude that PME may selectively soften the epidermal wall

under calcium-limited conditions, but we found no evidence for wall loosening by PME.

Discussion

As detailed in the introduction, this study was initiated to resolve some of the confusion and

speculation surrounding the action of PME on cell wall stiffness and extensibility (Levesque-

Tremblay *et al.*, 2015; Peaucelle *et al.*, 2008). Our results show that – even in our simplified,

cell-free system (isolated outer epidermal walls from onion) - a more nuanced appreciation of the

complexity of wall biomechanics and the action of PME is needed to unpack this issue. Thus,

measured by nanoindentation (Fig. 2) or by tensile plasticity (Fig. 3), PME softened the onion

cell wall, yet it did not change tensile elasticity nor did it loosen the wall, assayed as the ability

to induce cell wall creep (Fig. 9). Indeed, despite its selective softening and hydrating actions,

PME treatment actually hindered the wall loosening activity of endogenous α-expansins to

induce acid-dependent extension. The wall became less extensible despite its increase in plastic

compliance. Thus, in this case plasticity is not a good predictor of the ability of the cell wall to

undergo chemorheological creep – a conclusion similar to that of another recent study that

employed other enzyme treatments (Zhang *et al.*, 2019). These PME effects occurred without

addition of calcium to the wall, so we conclude they were direct physico-chemical effects of HG

de-esterification within the cell wall. Because endogenous wall enzymes were inactivated by

pretreatment in hot methanol, the softening action did not involve HG degradation by

endogenous pectinases or pectolyases. Hence, our answer to the question "How does PME affect

wall biomechanical properties?" depends on the specific assay and requires the clarification that

wall stiffness and wall creep are not tightly coupled (Cosgrove, 2018a; Zhang *et al.*, 2019).

The results of the current study are relevant to understanding: (1) PME effects on wall

mechanics, (2) the relationships of different biomechanical assays to each other and to growth,

and (3) the relationships between wall structure and various biomechanical properties. These

three points are discussed below.

PME effects on wall mechanics

After PME treatment, the electrostatic potential of the onion wall (measured as zeta potential)

became more negative, as expected for an enzyme that unmasks carboxylate groups of

methylesterified HG (Moustacas *et al.*, 1986). It is likely that cell wall swelling, hence greater

wall hydration, after PME treatment resulted from increased electrostatic repulsion of negatively-

charged HG chains (MacDougall *et al.*, 2001; Ryden *et al.*, 2000) and these effects in turn

contributed to increases in wall plasticity in the tensile test. This later point is supported by the

fact that $MgCl_2$, which was used to reduce electrostatic fields within the wall, negated the PME

effect on plasticity (Fig. 4). This scenario is consistent with previous work showing charge-

dependent swelling of isolated pectins and tomato cell walls (MacDougall *et al.*, 2001; Ryden *et*

al., 2000; Zsivanovits *et al.*, 2004), and supports the concept that pectin hydration influences

wall thickness (Jarvis, 1992).

Hydration also influences wall extensibility in some conditions. For instance, wall

dehydration by polyethylene glycol reduced wall extensibility in two studies (Edelmann, 1995;

Evered *et al.*, 2007). However, in the current study PME-mediated increase in wall hydration

was associated with reduced cell wall creep, not higher creep, despite an increase in wall

plasticity. Perhaps the increased electrostatic charge in the wall interferes with expansin-

mediated creep (Wang *et al.*, 2013), despite higher hydration. There are many potential

mechanisms for such interference (Ricard, 1987). A more detailed look at the effects of

electrostatic charge on cell wall rheology might be give insights into the basis of this charge

effect.

The greater electrostatic charge after PME treatment amplified the sensitivity of the cell wall

to exogenous calcium. For instance, calcium addition had little effect on either elastic or plastic

compliances of buffer-treated walls, whereas after PME-treatment calcium addition substantially

reduced wall plasticity (but not elasticity) (Fig. 4). These observations suggest the possibility that

newly unmasked carboxylate groups participated in calcium crosslinking of HG, e.g. via the 'egg

box' model (John *et al.*, 2019; Morris *et al.*, 1982), stiffening the matrix and thereby reducing

wall plasticity. However, the lack of effect on elasticity runs counter to this simple explanation,

as more crosslinking of HG might be expected to reduce the elastic compliance too. Other

physical mechanisms may contribute to the reduced plasticity: approximately half of the calcium

effect may due to electrostatic shielding, judging from the effect of $MgCl_2$ (Fig. 4) and assuming

that Mg^{2+} does not form HG crosslinks (Thibault and Rinaudo, 1986); calcium-HG interactions

may also reduce HG-cellulose interactions (Lopez-Sanchez *et al.*, 2020; Phyo *et al.*, 2017; Wang

et al., 2015). Such interactions may be extensive, but their significance for wall mechanics is

uncertain. A molecular understanding of the nature of cell wall plasticity and the physical

interactions between cell wall polymers is required to assess the relative contributions of these

different biophysical mechanisms to wall plasticity.

Because the experiments in the current study imposed large changes in HG methyl

esterification and used high calcium concentrations, these results should be considered the

extremes of possible PME-dependent changes in wall biomechanics. Whether similar changes

occur *in vivo* is uncertain at this time. Nevertheless, the nanoindentation results do offer a

potential explanation for correlations between HG de-esterification and reduced indentation

stiffness on Arabidopsis surfaces (Peaucelle *et al.*, 2011; Peaucelle *et al.*, 2015). How indentation

stiffness relates to other wall properties is considered next.

Relating different biomechanical assays to each other and to growth

One striking conclusion from this study is that different measures of wall biomechanics are not

closely coupled to one another. Thus, PME action softened the wall, as measured by indentation,

yet it did not result in wall loosening, as measured by cell wall creep. Wall creep is considered a

fundamental mechanism of cell wall growth (Cosgrove, 2018a). Consequently our *in-vitro*

results thus do not support the concept that PME has direct wall loosening activity. Various

indirect mechanisms for PME-mediated wall loosening have been suggested (Moustacas *et al.*,

1986; Moustacas *et al.*, 1991; Peaucelle *et al.*, 2008) and our results do not speak to these

speculations.

These results with PME are consistent with another recent study likewise showing that wall

softening and loosening are not tightly coupled in the onion epidermal wall (Zhang *et al.*, 2019).

For instance, treatment with pectate lyase reduced wall stiffness as measured by nanoindentation,

yet did not change the tensile properties of wall (elastic and plastic compliances and cell wall

creep). In the case of onion epidermal walls, nanoindentation evidently does not serve as a

reliable indication of tensile properties. Whether this is also true for other epidermal walls needs

to be examined. Theory predicts that indentations with larger probes (1 μm or larger) and at

greater depths may be sensitive to wall tensile properties (Milani *et al.*, 2013), but this prediction

requires experimental validation.

Relating wall structure to various biomechanical properties

Many conceptual models of primary cell wall structure have been proposed since the 1970s,

based largely on biochemistry and microscopy. These models make implicit statements about

wall mechanics, yet rarely has biomechanics been used to test the validity of these models, which

can be viewed as graphical hypotheses in need of experimental testing. One such test by Park

and Cosgrove (2012) rejected the concept that cellulose microfibrils were mechanically linked

into a load-bearing network by long xyloglucan tethers. A recent study using onion epidermal

wall concluded that tensile (in-plane) properties (elastic compliance, plastic compliance, and

creep) were largely determined by the network of cellulose microfibrils within individual

lamellae of this polylamellate wall, whereas the indentation (out-of-plane) properties were

largely controlled by pectins, along with some contributions from the cellulose microfibril

networks (Zhang *et al.*, 2019). Such results need to be incorporated into quantitative cell wall

models with both explanatory and predictive value (Smithers *et al.*, 2019).

The current study of PME action indicates that electrostatics and hydration affect selective

aspects of wall mechanics. Because PME does not cut the HG backbone, its biomechanical

effects are likely the result of physical changes resulting from the increased negative charge on

HG. This leads to charge repulsion of HG chains and swelling of the wall, which in turn affects

the indentation properties. The increase in tensile plasticity may result from increased hydration,

but higher electrostatic charge density within the wall may also contribute more directly. Despite

PME-induced changes in nano-indentation, tensile elasticity was insensitive to HG esterification

and to calcium cross linking. This is a remarkable result and suggests that static tensile forces are

transmitted predominantly via the interconnected network of cellulose microfibrils with little

mechanical contribution from HG networks. A similar conclusion was recently reached in a

study that used pectate lyase to cleave HG chains in onion epidermal walls (Zhang *et al.*, 2019).

Concluding remarks

By use of isolated epidermal wall strips to explore the physical consequences of PME action, we

avoided the complexity of living tissues, where cell anatomy and turgor pressure can complicate

the interpretation of mechanical assays (Forouzesh *et al.*, 2013; Weber *et al.*, 2015) and where

biological responses to pectin modifications can elicit far-ranging responses involving auxin,

brassinosteroids , wall integrity sensors, and changes in transcription of thousands of genes

(Braybrook and Peaucelle, 2013; Wolf *et al.*, 2012). Our results show that, in the absence of

added calcium, PME softened the wall in the nanoindentation assay, potentially accounting for

some previous AFM-based reports of wall softening associated with regions of HG de-

esterification (Peaucelle *et al.*, 2011; Peaucelle *et al.*, 2015). A concomitant increase in onion

wall plasticity, however, did not translate into a more extensible cell wall, as measured by cell

wall creep, and so does not account for increased growth associated with regions of de-esterified

HG. The multidimensionality of wall biomechanics offers a rich path for gaining greater insights

into cell wall structure.

Supplementary data

Fig. S1. PME effects on onion wall surface roughness.

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Figure legends

Fig. 1. PME de-esterifies HG in onion epidermal walls. (A) Immunolabelling of the inner surface
of onion epidermal cell walls after 2 h in HEPES buffer ± PME. JIM7 and LM19 antibodies
detect HG of high and low degree of methylesterification, respectively. Scale bar = 100 µm.
Representative results from two independent replicates. (B) Methanol release from onion
epidermal wall as a function of PME treatment time. Mean ± SEM of two independent replicates.

Fig. 2. PME effect on AFM nano-indentation. Force/extension measurements performed on
onion epidermal walls submerged in 20 mM pH 7.5 HEPES buffer alone (A) and in the presence
of 50 µg/mL PME (B) at time 0 h (black) and 3 h (gray). The representative extend (solid) and
retract (dashed) curves have modulus values close to the average value of each treatment. (C)
Modulus calculated by the Sneddon model using retract curves. Values are mean ± SEM (23 ≤ n
≤ 24). Letters indicate statistical significance based on one-way ANOVA with *post hoc* Tukey
test ($p < 0.01$).

Fig. 3. PME effect on tensile mechanics of onion epidermal walls. (A) Force/extension curves of
control (solid) and PME treated (dashed) walls. For each data set, the first stretch is the upper
curve which contains both plastic and elastic components while the second stretch is the bottom
curve containing only the elastic component. These are representative curves with compliance
values close to the average. (B) Statistical summary of elastic and plastic compliances (mean ±
SEM; n = 15). Student's t-test (paired, two-tail) was used to assess statistical significance (* $p <$
0.05). Experiment was repeated four times with similar results.

Fig. 4. Effect of $CaCl_2$ and $MgCl_2$ on elastic and plastic compliances of walls pretreated with
buffer ± PME. Values are means ± SEM (9 ≤ n ≤ 17). Letters indicate statistical difference in
one-way ANOVA with *post hoc* Tukey test ($p < 0.05$). Replicated three times for $MgCl_2$ and
twice for $CaCl_2$.

Fig. 5. Zeta potential of onion wall fragments treated with PME or BSA (box and whiskers plot).

Wall fragments were suspended in 20 mM HEPES pH 7.0. Three biological samples with

analysis by Student's t-test.

Fig. 6. Cell wall swelling caused by PME treatment. (A) Onion scale cross-sections stained with

toluidine blue; the wall thickness is marked by black arrows (top). Scale bar = 20 μm. Binary

image was generated using ImageJ, red line shows the selection for wall thickness measurement

(bottom). (B) Wall thickness comparisons at 0 h and 3 h, ± PME treatment. Values are means ±

SEM (n = 20). Student's t-test (paired, two-tail) was used to assess statistical significance (**-p

< 0.01).

Fig. 7. PME treatment reduces cellulose microfibril resolution by AFM imaging. (A) Peak force

error image of onion epidermal wall surface in HEPES buffer. Scale bar = 20 nm. Distinct

cellulose microfibrils and bundles well resolved by AFM. (B) Same area scanned after PME

treatment. The resolution of cellulose microfibrils is reduced while fibrils in the underlying

lamella were obscured. Similar results observed with six biological replicates.

Fig. 8. Effect of acid pH and PME pretreatment on stress relaxation spectra of onion epidermal

walls. Each curve is the average of 7-8 data sets. Boxed regions show statistically significant

difference in relaxation rate. Student's t-test was used to evaluate statistical significance (* boxed

region different at $p < 0.05$). (A) Walls in acidic (pH 4.5) buffer have greater stress relaxation

than walls in neutral (pH 6.8) buffer. (B) Stress relaxation spectra of walls after 3 h incubation in

20 mM HEPES pH 7.5 ± PME.

Fig. 9. Influence of PME treatment on cell wall creep. (A) Addition of 100 μg/mL PME in pH

7.5 HEPES buffer does not induce creep. Walls were incubated in pH 7.5 buffer while clamped

on the constant force extensometer. At the time indicated by the arrow, the buffer was exchanged

with fresh buffer containing PME. (B) Acid-induced creep of walls pretreated for 16 h with

buffer (solid) is substantially greater than creep of walls pretreated for 16 h with PME (dash).

Curves are averages of 6 (PME) and 9 (buffer- and PME- pretreated) replicates.

A

	Buffer	PME treated
JIM 7		
LM 19		

B

Methanol release (µmol) per mg wall

0.25
0.2
0.15
0.1
0.05
0

Time of incubation (h)
0 2 4 6 8 10 12 14 16

Fig. 1. PME de-esterifies HG in onion epidermal walls. **(A)** Immunolabelling of the inner surface of onion epidermal cell walls after 2 h in HEPES buffer ± PME. JIM7 and LM19 antibodies detect HG of high and low degree of methylesterifcation, respectively,. Scale bar = 100 µm. Representative results from two independent replicates. (**B**) Methanol release from onion epidermal wall as a function of PME treatment time. Mean ± SEM of two independent replicates).

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Fig. 9. Influence of PME treatment on cell wall creep. (A) Addition of 100 µg/mL PME in pH 7.5 HEPES buffer does not induce creep. Walls were incubated in pH 7.5 buffer while clamped on the constant force extensometer. At the time indicated by the arrow, the buffer was exchanged with fresh buffer containing PME. (B) Acid-induced creep of walls pretreated for 16 h with buffer (solid) is substantially greater than creep of walls pretreated for 16 h with PME (dash). Curves are averages of 6 (PME) and 9 (buffer- and PME- pretreated) replicates.