How brain reacts to attack at a local region

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Abstract

The brain function is a network phenomenon. The architecture of brain networks has been extensively studied in multiple species. However, exactly how the brain network reconfigures when a local brain region stops functioning is virtually unknown. By combining chemogenetic and resting-state functional magnetic resonance imaging (rsfMRI) methods in an awake rodent model, we investigated the causal impact of inactivating a hub region (i.e. dorsal anterior cingulate cortex) on brain network properties. We found that disrupting hub activity profoundly changed the function and organization of the default-mode network (DMN), as well as DMN-related behavior (i.e. quiet restfulness). It also altered the topological architecture of the whole-brain network in network resilience, segregation and small worldness, but not network integration. These data provide direct evidence supporting the hypothesis that acute dysfunction of a brain hub can cause large-scale network changes. They also comprehensively document the differential impact of inactivating a hub versus a non-hub on network dynamics.

Introduction

The mammalian brain is a highly inter-connected network system with distributed brain regions orchestrating to support normal function and mediate complex behavior (Bullmore and Bassett, 2011). The brain network is organized to maintain an optimal balance of information segregation and integration, which simultaneously maximizes the efficiency of distal communication via long-range connections and minimizes the wiring cost through clustered local processing (Bullmore and Sporns, 2009, 2012). Such organization is well conserved in multiple species including rodents, primates and humans (Liang et al., 2011; Vincent et al., 2007; Wang et al., 2010).

It is becoming increasingly clear that altered brain network organization is tightly linked to brain disorders (Bassett and Bullmore, 2009; Fornito et al., 2015; Liu et al., 2008). However, the neural substrates causing these large-scale network changes remain unknown. A key hypothesis is the dysfunction of brain hub regions. Hubs are brain regions that have high degrees of connections with the rest of the brain (Rubinov and Sporns, 2010; van den Heuvel and Sporns, 2013). Because of their central roles, dysfunction of hub nodes can change global integrative process, and has been hypothesized to be a direct cause of altered brain network properties and pathophysiology of brain disorders (Alstott et al., 2009; Crossley et al., 2014). For instance, brain network analysis in patients with Alzheimer's Disease showed that amyloid-beta deposition mainly accumulated in functional hubs (Buckner et al., 2009). Therefore, comprehensively understanding the causal relationship between hub activity and brain network organization is critical. However, directly testing this hypothesis in humans is challenging, as selectively altering activity in a hub and dissecting its causal impact on brain networks are difficult.

This obstacle can be overcome in experimental animals using neuroscience tools

like Designer Receptors Exclusively Activated by Designer Drugs (DREADDs) and resting

state functional magnetic resonance imaging (rsfMRI). DREADDs introduce genetically

encoded modified muscarinic G-protein-coupled receptors into living neurons, which

allow reversible *in vivo* manipulation of neuronal activity of a defined brain region for hours

(Armbruster et al., 2007). rsfMRI measures brain-wide resting-state functional

connectivity (RSFC), and provides comprehensive assessment of brain network

properties (Biswal et al., 1995; Liang et al., 2011). Thus, combining these two techniques

offers a system that allows us to characterize the reconfiguration of the brain network as

the neural activity of a network node is selectively perturbed. In addition, given the highly

conserved brain network architecture in the mammalian brain (Liang et al., 2011; Vincent

et al., 2007; Wang et al., 2010), the results are translatable to humans.

Here we investigate the causal impact of manipulating a hub region, dorsal anterior

cingulate cortex (dACC), on brain network function and organization, as well as behavior

using an awake rodent model established in our lab (Dopfel et al., 2019; Ma et al., 2018;

Ma and Zhang, 2018; Zhang et al., 2010). Imaging awake rodents avoids the confounding

effects of anesthesia (Gao et al., 2016; Hamilton et al., 2017; Liang et al., 2012b; Ma et

al., 2017), and permits linking imaging and behavioral data (Dopfel et al., 2019; Liang et

al., 2014). dACC is selected because it is a known functional and anatomical hub in both

human and rat brain (Ma et al., 2018; van den Heuvel et al., 2016; van den Heuvel and

Sporns, 2013)ʼ(Bush et al., 2000). We first examine the impact of suppressing the dACC

on the default mode network (DMN), which is composed of a group of distributed brain

regions exhibiting higher activity at rest (Gusnard et al., 2001; Raichle et al., 2001). DMN

function is tightly linked to self-referential mental activity in humans, and its abnormality

has been linked to numerous brain disorders (Whitfield-Gabrieli and Ford, 2012; Zhang

and Raichle, 2010). DMN has also been reported in rodents and primates (Hsu et al.,

2016; Lu et al., 2012; Stafford et al., 2014; Vincent et al., 2007; Zhou et al., 2016),

although our understanding of DMN in animals is mostly limited to its anatomical

resemblance to the DMN in humans (Lu et al., 2012; Vincent et al., 2007). Since dACC

is a hub node in the rodent DMN (Hsu et al., 2016), manipulating dACC activity provides

an avenue for understanding the rodent DMN at the functional level. Our data show that

suppressing the dACC disrupts activity and connectivity across the whole DMN, and

changes DMN-related behaviors. These data suggest that, like humans, DMN in rodents

is a functional network with coordinated activity to mediate behavior. Furthermore, we

demonstrate that suppressing the dACC impacts the organization of the whole-brain

network including network resilience, segregation and small worldness, but not network

integration. All these changes are absent in sham rats or when a non-hub region is

suppressed. Taken together, this study provides direct measurement of the brain's

response to local attack, and presents a comprehensive framework demonstrating the

pivotal role of hubs in the brain network.

Results

Animals were stereotactically injected with adeno-associated viruses (AAVs)

expressing inhibitory G-protein coupled hM4Di receptor with a pan-neuronal synapsin

promoter (AAV8.hSyn.hM4Di.mCherry, Addgene). After 4-6 weeks of recovery and

protein expression (Fig. S1), animals received either Clozapine-N-Oxide (CNO) or saline

30 min before electrophysiology recording, rsfMRI scanning or behavioral tests. Saline

and CNO sessions were separated by at least 3 days in a random order. The experimental

procedure is summarized in Fig. 1.

DREADD suppressed both evoked and spontaneous neural activities in the injected site.

We first validated the inhibitory effect of the DREADD using a visual stimulation

paradigm (Fig.2). AAVs expressing inhibitory DREADD (AAV8.hSyn.hM4Di.mCherry,

Addgene) were injected into the superior colliculus (SC). After recovery and DREADD

expression, neural activity in the SC was activated by visual stimuli (Figs. 2A-D, 1

flash/trial and 5 flashes/trial, 100ms per flash, 10 sec per trial, 15 trials per animal) and

measured by electrophysiology. SC firing rates were significantly reduced 30 min after

CNO injection (1 flash/trial: two-sample tests, t = 10.30, p = 8.8 ×10^{-17}, Figs. 2B & D; 5

flash/trial, t = 13.48, p = 4.1×10^{-23}, Fig. 2C & D). In addition, spontaneous neural activities

including spiking activity and local field potential (LFP), quantified by the

electrophysiology data 5s before the onset of visual stimulation in each trial, were

significantly dampened in CNO-injected rats (MUA: t = 16.15, p = 1.041×10^{-36}; LFP: t =

5.84, p = 8.6 × 10^{-8}; Figs. 2E, F & G). The LFP spectrograms after saline and CNO

injections in a representative rat were also shown in Fig. S2. These data collectively

confirmed the inhibitory effect of the DREADD on evoked and spontaneous neural

activities in rats.

Suppressing the dACC reduced its rsfMRI signal, RSFC and local network organization.

The bilateral dACC was transfected by inhibitory DREADDs under a pan-neuronal

synapsin promoter (AAV8.hSyn.hM4Di.mCherry, Addgene). Sham rats received a control

virus (AAV8-hsy-GFP, Addgene). Animals were scanned using rsfMRI twice in the awake

state, with each session starting 30 min after either CNO or saline injections. The two

imaging sessions were separated by at least 3 days with a randomized order. There was

no difference in motion level during rsfMRI scanning between CNO and saline injection

conditions in both DREADD and sham groups (Fig. S3).

Fig. 3A shows that DREADD suppression of the dACC reduced its resting-state

blood-oxygenation-level dependent (BOLD) amplitude (std divided by mean, $t = 2.00$, $p =$

0.048), again confirming the inhibitory effect of the DREADD on spontaneous neural

activity. Suppressing the dACC also affected its functional connectivity, reflected by

generally reduced RSFC in the dACC seedmaps (one sample t test, $p<0.0005$, linear

mixed model, false discovery rate (FDR) corrected) after CNO injection relative to saline

injection (Fig. 3B). We further examined the impact of suppressing the dACC on its local

information processing, assessed using the modular structure, which is defined as a

group of nodes with significantly greater within-module connections than between-module

connections (Newman, 2006). The dACC-related module shrunk in size in DREADD rats

after CNO injection relative to saline injection at high graph densities ($p < 0.05$, linear

mixed model, Fig. 3E), suggesting that suppressing the dACC mainly dropped relatively

weaker connections in the dACC module.

In addition to dACC-related circuits, RSFC in distributed connections was altered

(two-sample t-tests, $p < 0.05$, linear mixed model, FDR corrected) with lower RSFC in the

majority of these connections (i.e. blue elements in the T map, Figs. 3C & 3D), indicating

that the impact of suppressing neural activity in a hub can go beyond the hub itself and

propagate to neural circuits across the whole brain. This ripple effect is consistent with

the report in human patients with focal brain lesions to critical locations (Gratton et al.,

2012).

None of these changes (i.e. resting-state BOLD amplitude, dACC-related RSFC

and community size) were observed in sham rats when comparing CNO- to saline-

injection conditions (Fig. S4), which suggests that CNO had minimal off-target effects in

our system, ruling out its potential confounding effects on rsfMRI data (Gomez et al.,

2017).

Suppressing dACC altered activity and connectivity in the DMN.

Given that dACC is a major hub node in the functional network of DMN, we

examined the impact of inactivating the dACC on the DMN organization in awake rodents.

We first constructed the DMN using *fractional amplitude of low-frequency fluctuations*

(fALFF), defined by voxel-wise low-frequency spectrum power (0.01–0.08 Hz) normalized

by the full-spectrum power (Zou et al., 2008) of the rsfMRI signal. This well-established

method measures the amplitude of regional spontaneous brain activity. As a result, it can

reliably identify brain regions with higher activity at rest, and map the spatial pattern of

the DMN (Zou et al., 2008).

Fig. 4 displays the DMN spatial maps in DREADD and sham rats after saline and

CNO injections, respectively. Brain regions highlighted in the network included the ACC,

posterior cingulate cortex (PCC), prelimbic cortex (PL), retrosplenial cortex (RSC), orbital

cortex (ORB), posterior parietal cortex (PPC), as well as subcortical regions of the basal

forebrain (BF) and hypothalamus (Hypo). This DMN pattern was reproduced with a

completely different method (i.e. independent component analysis, Fig. S5) previously used by other groups, and well agreed with the rodent DMN pattern reported in the literature (Hsu et al., 2016; Lu et al., 2012; Stafford et al., 2014). Notably, we found that the BF was a prominent node in the rodent DMN, which was not observed in other rodent DMN mapping studies, but was reported in an electrophysiology study that demonstrated that the BF is a key DMN node and critical in regulating DMN-related behaviors in rats (Nair et al., 2018).

Intriguingly, suppressing one node in the DMN (i.e. dACC) dampened the activity of virtually the entire network (Fig. 4A, top row), reflected by reduced BOLD fALFF in the ACC, PL, ORB, PPC, BF and Hypo after CNO injection in DREADD-suppressed rats (Fig. 4B, two row, $p < 0.05$, Family-wise error corrected). Again, no regions displayed reduced spontaneous activity in sham rats after CNO injection (Figs. 4A & 4B, bottom row). We also calculated RSFC between every pair of nodes in the DMN including the dorsal and ventral ACC, dorsal and ventral PCC, RSC, ORB, PL, PPC, as well as BF and Hypo (Hsu et al., 2016) in both DREADD and sham rats after saline and CNO injections, respectively (Fig. 4C). Cortical nodes generally displayed significantly reduced RSFC ($p < 0.05$, FDR corrected, Figs. 4D & 4E), except that the RSC exhibited increased RSFC with the PPC, BF and Hypo. This result is consistent with our observation that RSC emerged as a new hub in the whole-brain network when the dACC was suppressed (Fig. 7). In contrast, both subcortical nodes (BF and Hypo) showed increased RSFC after dACC suppression (Figs. 4D & 4E). Taken together, these data revealed that the DMN was significantly reorganized when dACC activity was suppressed, suggesting that the rodent DMN is a functional network with coordinated activity, and the dACC is a pivotal node in this network.

Suppressing dACC altered DMN-related behaviors in animals.

Considering that suppressing dACC significantly altered DMN activity in awake rodents, we hypothesize that it also changes DMN-related behavior, measured by quiet restfulness in rodents. Nair and colleagues demonstrated that quiet restfulness in home-cage is characteristic behavior to DMN activity, evidenced by elevated neural activity in the DMN, including ACC and BF, during this behavioral state (Nair et al., 2018). Robust DMN activation during quiet restfulness was also reported in chimpanzees (Barks et al., 2015). Therefore, we evaluated quiet restfulness, defined by continuous immobility for at least 2s, in our animals. After either CNO or saline injection, the rat was put in the home cage for 45min and was video-recorded. The animal's behavior was analyzed using behavioral tracking software (ANY-maze, Stoelting Co., Wood Dale, IL). After CNO injection, quiet restfulness was significantly reduced in the rat (Fig. 5), reflected by significantly lower immobile time for at least 2s ($t = 3.991$, $p = 0.0009$), but higher distance travelled ($t = 4.294$, $p = 0.0004$), mean speed ($t = 4.811$, $p = 0.0001$) and total mobile time ($t = 3.991$, $p = 0.0009$). Rats also displayed significantly higher rearing after CNO injection ($t = 2.80$, $p = 0.01$), likely reflecting an increase in vigilance and/or exploratory behavior. Reduced quiet restfulness remained consistent during the last 15 min of testing, suggesting that these behavioral changes were not due to the environmental changes at the beginning of the test (Fig. S6). These data demonstrate that dACC suppression reduced DMN-related behaviors in rats, echoing their dampened DMN activity.

Suppressing a hub node changed whole-brain network organization

We further investigated the effect of suppressing the dACC on the organization of

the whole-brain network architecture in four aspects: network resilience, functional

segregation, functional integration, and small-worldness. The whole rat brain was

parcellated into 68 bilateral regions of interest (ROIs) based on the Swanson atlas

(Swanson, 2004). The whole-brain network was constructed by calculating RSFC

between every two ROIs, generating a RSFC matrix for each animal at each condition.

This RSFC matrix was then binarized based on graph density. Graph topological

parameters including assortativity, modularity, global efficiency, and small-worldness

were respectively calculated as a function of graph density.

Assortativity measures network resilience. Brain networks with high assortativity

are more resistant to local attack such as lesion and neurological degeneration (Newman,

2002; Rubinov and Sporns, 2010). Fig. 6 shows that suppressing the dACC considerably

reduced the network assortativity, and as a consequence, the whole-brain network

became more vulnerable (Fig. 6A). Functional segregation, quantified by modularity,

measures the network's ability of specialized processing. We observed that dACC

suppression decreased the modularity of the global brain network, indicating reduced

functional segregation (Fig. 6C). Global efficiency measures functional integration, which

assesses the ability to integrate specialized information from distributed brain regions.

Interestingly, suppressing the dACC did not seem to affect the global efficiency (Fig. 6D).

Small-worldness reflects the ability to balance functional segregation and integration.

Suppressing the dACC reduced small-worldness of the whole-brain network (Fig. 6B). In

summary, we observed that suppression of the dACC affected global brain topology

including network resilience, network segregation and small-worldness, but not network

integration.

As expected, DREADD suppression of the dACC significantly lowered its degree

(Fig. 7), suggesting that dACC lost its hubness in the network. Interestingly, the degree

of the ventral RSC was significantly increased after dACC suppression, consistent with

our data that some RSC connections increased their RSFC within the DMN (Fig. 4D).

Again, no changes in the degree of dACC or RSC were observed in sham rats (Fig. S7).

These results indicate that a new hub can emerge when an existing hub stops functioning,

likely due to the compensatory mechanism.

Suppression of a non-hub region did not change whole-brain network properties

To determine whether aforementioned network changes depended on the specific

role of the node (i.e. hub versus non-hub), we also suppressed the activity in a non-hub

region—primary visual cortex (V1, bilateral) (Ma et al., 2018) using the same pan-

neuronal inhibitory DREADD. After CNO injection, significantly reduced BOLD amplitude

in V1 was observed (Fig. 8A), which confirmed the inhibitory effect of DREADD in V1.

However, suppression of V1 did not affect fALFF in the DMN (Fig. S8), nor did it cause

any whole-brain topological changes including network resilience, functional segregation,

functional integration, or small-worldness (Figs. 8B-8E). Taken together, these data

suggest that attack on separate brain regions can have differential impact on brain

network properties, and hub nodes are particularly vulnerable to such attacks.

Discussion

For over a century, the neuroscience field has been tremendously moved forward

by the effort of examining the relationship between damage of specific brain regions and

loss of certain brain function. Classical examples are the discovery of the inferior frontal

gyrus in speech production by Paul Broca, and the left posterior temporal cortex in

language comprehension by Carl Wernicke. Despite this vital advancement, converging

evidence suggests that a large number of complex tasks involve numerous cognitive

processes and require integrated activity from multiple brain regions (Liegeois et al.,

2019). Therefore, brain function should be viewed as a network phenomenon.

By combining DREADDs and rsfMRI in an awake rodent model, we established a

system that allowed us to manipulate the activity in any brain region, and measure the

corresponding changes in brain-wide networks. This system makes it possible to

mechanistically dissect the causal relationship between a (or multiple) local brain region(s)

and brain network properties. In this study we specifically investigated the role of a hub

region (i.e. dACC) in brain networks. We found that disrupting hub activity profoundly

changed the function and organization of the DMN (Figs 4), as well as DMN-related

behavior (Fig. 5). It also altered the topological architecture of the whole-brain network in

terms of network resilience, segregation and small worldness, but not network integration

(Fig. 6). These data offer direct evidence supporting the hypothesis that acute dysfunction

of a brain hub can cause large-scale network and behavioral changes. They also provide

a comprehensive framework documenting the differential impact of inactivating a hub

versus a non-hub node on network dynamics.

Tight relationship between local regions and brain networks

The activity in local brain regions can be manipulated using tools like

chemogenetic, optogenetic, pharmacological and lesion methods. Such perturbations are

often used to study the role of a specific brain region in behavior (Whissell et al., 2016).

Meanwhile, the capacity of manipulating local brain regions can be tremendously

expanded when combined with neuroimaging approaches with a global field of view (e.g.

fMRI), as the causal impact of local region dysfunction on the rest of the interconnected

network can be monitored across the whole brain (Lee et al., 2010). For instance, using

DREADDs and rsfMRI, Grayson and colleagues showed that inactivating the amygdala

disrupted communication throughout the cortex and altered the topology of the global

brain network in anesthetized monkeys (Grayson et al., 2016). This observation echoes

human patient studies in which lesions of critical focal brain locations caused widespread

disruption of the brain modular structure and behavior (Gratton et al., 2012; Warren et al.,

2014). These results collectively suggest tight links among regional activity, large-scale

network properties and behavior, and highlight the importance of combining local

perturbations and global network measurement. Uniquely, our study was conducted in

awake animals, which avoids the confounding effects of anesthesia on brain network

function, and permits direct association of network features and behavioral changes

resulting from hub inactivation. This nature also makes the findings translatable to

humans, considering numerous reports of large-scale brain network changes in human

brain disorders.

DREADDs vs lesion

There are several advantages choosing the DREADD over the lesion method for

our research purpose. First, DREADDs allow us to specifically and reversibly inhibit a

brain region with minimal damage. On the other hand, long-term damage in brain tissue

can decrease metabolism and alter local vascular structure. In addition, there can be

excessive blood flow in surrounding regions (Rorden and Karnath, 2004). All these factors

will impact fMRI data measurement and can confound RSFC results. Long-term lesion

studies can also be compounded by post-lesion neural plasticity changes resulting from

the compensatory mechanism (i.e. secondary effects). Furthermore, most psychiatric

disorders are linked to loss of function without tissue damage, making the DREADD

method a better translatable model.

DMN in rodents – beyond anatomical resemblance with other species

We observed significant reconfiguration of the DMN after transiently inactivating

one of its hub nodes (i.e. dACC) in awake rodents. This finding was corroborated by

altered DMN-related behaviors after dACC suppression. Although the DMN has been

extensively studied in humans including its network structure, function and clinical

implications, our understanding of the DMN in rodents is limited. The discovery of rodent

DMN was mainly based on the anatomical resemblance of the network structure with the

DMN in humans and primates (Lu et al., 2012; Stafford et al., 2014), but its functional role

in behavior remains unclear. Nair and colleagues showed that the rat BF exhibited

pronounced gamma oscillations during DMN-related behaviors and this activity was

suppressed during active exploration of an unfamiliar environment (Nair et al., 2018),

suggesting that the BF might be a key DMN node that regulates DMN activity. They further

demonstrated that the BF controls DMN-related behaviors by affecting neural activity in

the ACC. These results are in remarkable consistency with our findings. First, we also

observed prominent involvement of the BF in the rat DMN at baseline, which was missing

in previous rodent DMN mapping studies (Hsu et al., 2016; Lu et al., 2012). Notably, the

BF has strong connections with the cortex and subcortical regions like Hypo, and these

connected regions substantially overlapped with the DMN revealed in our study

(Agostinelli et al., 2019; Gielow and Zaborszky, 2017). Second, suppressing the dACC

considerably dampened the DMN activity, including that involving the BF. Third,

suppressing dACC reduced DMN-related behaviors. Taken together, these results

support the concept that, like humans and primates, the DMN in rodents is a functional

network with coordinated neural activity from distributed brain regions, and this network

might support behavior related to internally oriented brain states.

Hubs and brain network topology

The topological changes resulting from hub inactivation, including reduced network

resilience, segregation and small worldness, are important for our understanding of the

role of individual regions in the global brain network organization. A brain network can be

modeled as a graph composed of spatially distributed neuronal components as nodes

and anatomical or functional associations between components as edges (Bullmore and

Sporns, 2009, 2012). Topological features of the brain graph are critical in understanding

inter-areal information exchange in health and disease. Although the architecture of brain

networks has been extensively studied in multiple species (Bassett and Bullmore, 2006;

Belcher et al., 2013; Liang et al., 2011; Liska et al., 2015), it remains elusive whether

different types of nodes, such as hubs versus non-hubs, play distinct or similar roles in

the topology of the global brain network. Our data revealed that changes in a hub, but not

a non-hub, can significantly alter brain network topology. These results provide critical

insight into understanding the pathogenesis of neurological and psychiatric disorders,

which indicate that altered brain topological properties reported in these brain disorders

might start from dysfunction of certain hub nodes (Seeley et al., 2009). Interestingly, our

data showed that network integration was intact after dACC inactivation, likely due to the

compensatory effect of the so-called 'rich club organization' in the rat brain (Ma et al.,

2018). Another possible explanation is that although the dACC has high centrality, it

functions as a provincial hub as opposed to a connector hub (Guimera and Nunes Amaral,

2005). These two types of hubs were demonstrated to have differential impact on brain

network properties (Gratton et al., 2012), with connector hubs more affecting network

integration, and provincial hubs more affecting network segregation. Our result is

consistent with the notion that the ACC belongs to the "segregation effect" class, which

agrees with the report in human lesion studies (Yuan et al., 2017).

Methods and Materials

Animals.

44 adult male Long-Evans rats (300-500g) were used in the present study. Animals

were housed in Plexiglas cages. Food and water were provided *ad libitum*. The housing

room was maintained at an ambient temperature (22-24 ˚C) with a 12h light:12h dark

cycle. All experiments were approved by the Pennsylvania State University Institutional

Animal Care and Use Committee.

Surgery.

Aseptic stereotaxic surgery was conducted to infuse the virus to the brain. Rats

were anesthetized by intramuscular (IM) injections of ketamine (40 mg/kg) and xylazine

(12 mg/kg). Dexamethasone (0.5 mg/kg) and Baytril (2.5 mg/kg) were injected SQ to

prevent tissue inflammation and bacterial infections. During the surgery, respiration was

controlled by a ventilator with artificial oxygen. The heart rate was monitored by a pulse

oximetry (MouseSTAT® Jr., Kent Scientific Corporation), and the body temperature was

maintained at 37 ˚C with a warming pad (PhysioSuite, Kent Scientific Corporation). The

DREADD virus (AAV8-hSyn-hM4Di-mCherry, 1 μL at titer ≥ 3×10^{12} vg/mL, Addgene,

Watertown, MA) was bilaterally injected into the dACC (coordinates: AP +2, ML +/-0.5,

DV -1) and the primary visual cortex (coordinates: AP -6.5, ML +/-3.5, DV -1) for the hub

(n = 25) and non-hub (n = 8) groups, respectively [24]. Sham rats were injected with a

control virus (AAV8-hsy-GFP, 1 μL at titer ≥ 3×10^{12} vg/mL, Addgene, Watertown, MA, n

= 8)[24] into the dACC. In addition, separate animals used in the visual stimulation

experiment were unilaterally injected with AAV8-hSyn-hM4Di-mCherry (1 μL at titer ≥

3×10^{12} vg/mL, Addgene, Watertown, MA, n = 3) in the SC (coordinates: AP -7, ML +1.5,

DV -3). Rats were allowed to recover for at least four weeks.

fMRI experiments:

Before imaging, animals were acclimated to the MRI environment for 7 days in

order to minimize stress and motion during imaging. To better adapt the animal to the

restrainer and scanning environment, the acclimation period was gradually increased

from 15 min on Day 1 to 30 min on Day 2, 45 min on Day 3, and maintained at 60 min/day

for Days 4-7. Detailed procedures for acclimation can be found from our previous

publications (Dopfel and Zhang, 2018; Liang et al., 2012a). A similar approach to imaging

awake animals has also been adopted by other research groups in multiple species

(Bergmann et al., 2016; Chang et al., 2016; Yoshida et al., 2016). CNO (1mg/kg in saline,

dissolved in DMSO, Sigma-Aldrich, St. Louis, MO) or saline (with DMSO) was IP injected

30 min before rsfMRI data acquisition, at a random order with at least three days apart.

All imaging sections were conducted at the High Field MRI Facility at the

Pennsylvania State University on a 7T Bruker 70/30 BioSpec running ParaVision 6.0.1

(Bruker, Billerica, MA). rsfMRI data were acquired at the awake state using T2*-weighted

gradient-echo rsfMRI images using the echo-planar-imaging (EPI) sequence with the

following parameters: repetition time = 1000ms; echo time = 15ms; matrix size = 64×64;

field of view = 3.2×3.2 cm^2; slice number = 20; slice thickness = 1mm; flip angle = 60;

600 volume each run. Three runs were acquired each rsfMRI session. Raw EPI images

were shown in Fig. S9.

Data analysis:

All acquired image data were aligned to a defined atlas using Medical Image

Visualization and Analysis software (MIVA, http://ccni.wpi.edu/), and then subjected to

motion correlation (SPM12), spatial smoothing (Gaussian kernel, full-width at half-

maximum = 1 mm), voxel-wise nuisance regression of motion parameters, as well as the

signals from the white matter and ventricles, and bandpass filtering (0.01-0.1Hz). Before

these steps, rsfMRI volumes with relative framewise displacement (FD) > 0.25 mm and

the preceding and following volumes were removed. In addition, the first 10 volumes of

each rsfMRI scan were discarded to ensure steady state of magnetization. rsfMRI scans

with > 15% volumes discarded were removed from further analysis.

fALFF was determined by calculating the ratio of the power in the low-frequency

range (0.01–0.08 Hz) to that of the full spectrum (0–0.25 Hz). For each voxel, the time

course was detrended without a band-pass filtering, and then transformed to the

frequency domain using FFT. We calculated the ratio between the square root of power

in the range of 0.01–0.08 Hz and that across the entire frequency range. fALFF changes

after DREADD inhibition were obtained using voxel-wise two-sample t-tests with family

wise error correction (P<0.05, FWE corrected) between data acquired after CNO injection

versus saline injection.

Seed RSFC maps were generated using seed-based correlation analysis. Pearson

cross-correlation coefficients between the regionally averaged time course from all voxels

inside the seed and time courses of individual voxels were calculated. The corresponding

correlation coefficients were Fisher transformed, averaged across all scans and animals

in each group, and transformed back to r values.

The whole-brain RSFC network was constructed by parcellating the rat brain into

68 anatomical ROIs based on the Swanson Atlas (Swanson, 2004), which were also

grouped into 10 functional systems including amygdala complex, striatum, hypothalamus,

hippocampus, thalamus, sensory-motor cortex, polymodal association cortex, brainstem,

pallidum, and retro-hippocampal regions. RSFC between each pair of ROIs was

calculated by Pearson correlation of regionally averaged time series of the ROIs.

A hub score of each node ranged from 0-4 was determined by the number of the

following four criteria the node met: (1) 20% highest degree; (2) 20% highest

betweenness centrality; (3) 20% lowest characteristic path length; (4) 20% lowest local

clustering coefficient.

Topological parameters of the whole-brain network including the modularity, global

efficiency, small-worldness, and assortativity were calculated on binarized network

across the graph density ranging from 0.15 to 0.45 with a step of 0.05 using the brain

connectivity toolbox (BCT) [30] based on the following equations:

Assortativity (Newman, 2002):

457
$$r = \frac{l^{-1}\sum_{(x,y\in L)} k_x k_y - [l^{-1}\sum_{(x,y\in L)}\frac{1}{2}(k_x + k_y)]^2}{l^{-1}\sum_{(x,y\in L)}\frac{1}{2}(k_x^2 + k_y^2) - [l^{-1}\sum_{(x,y\in L)}\frac{1}{2}(k_x + k_y)]^2}$$

458 where k_x, k_y is the degree of node x and y on two opposite ends of an edge; L is the set

459 of all edges within the network, and l is total number of edges.

460
461 *Modularity (Newman, 2004):*
462
463
$$Q = \sum_{i\in M}[e_{ii} - (\sum_{j\in M} e_{ij})^2]$$

464 where M represents a set of non-overlapping modules, and e_{ij} is the proportion of

465 between-modules connections of module i and j; e_{ii} is the proportion of within-modules

466 connections of module i.

467 *Global efficiency (Latora and Marchiori, 2001):*

468
$$E = \frac{1}{n}\sum_{i\in N}\frac{\sum_{y\in N, y\neq x} d_{xy}^{-1}}{n-1}$$

469 where n is the total number of nodes; N is the set of all nodes. d_{xy} is the shortest path

470 length between nodes x and y,

471 *Small-worldness (Humphries and Gurney, 2008):*

472
$$S = \frac{C/C_{rand}}{L/L_{rand}}$$

where C and C_{rand} are the clustering coefficients of the testing network and a random

network, respectively; L and L_{rand} are the characteristic path lengths of the testing

network and a random network.

At each graph density, all topological parameters were determined for each scan.

Changes in each parameter was determined by two-sample t-tests (linear mixed model)

between the CNO injection and saline injection conditions.

Behavioral Test

Animals underwent two behavioral sessions with either CNO or saline injection

with a random sequence separated by at least 7 days. Each session was composed of a

45 min home-cage test. Before the test, the animal was acclimated to the behavioral room

for 15 min, followed by either CNO (1mg/kg) or saline injection. The animal was then put

back to its home-cage in the behavioral room for 45 min. Behaviors including the total

distance traveled, mean speed, time of mobility and time of immobility for at least 2s were

recorded by an infrared camera and analyzed by behavioral tracking software (ANY-maze,

Stoelting Co., Wood Dale, IL).

Electrophysiology.

Electrophysiology recordings were conducted in animals with inhibitory DREADD

expressed in the SC. Rats were initially anesthetized by IM injections of ketamine (40

mg/kg) and xylazine (12 mg/kg). An electrode (Neuronexus, Ann Arbor, MI) was then

inserted into the SC to measure visually-evoked neuronal response to light stimulation

produced by a blue laser source (100 mW, 473 nm, Opto Engine) coupled with an optic

fiber, which was placed 5 cm away from the contralateral eye. Before recording, rats were

injected with either saline or CNO in each session. During recording, light anesthesia was

maintained using isoflurane (~0.75%). Each session included 15 trials of visual

stimulation, presented as a single light flash (100 ms per flash) or five flashes (100 ms

each flash, 100 ms inter-flash interval) every 10 s. Light stimulation was controlled by a

custom Labview program. The electrophysiological signal was amplified and sampled at

25 kHz using a Neuronexus recording system (Neuronexus, Ann Arbor, MI). Raw data

were bandpass filtered (MUA: 300-3000 Hz, LFP: 3-300 Hz). Spikes larger than three

times of the standard deviation of electrophysiological signal were detected and clustered

at a bin size of 50 ms in peristimulus-timed histograms (PSTHs).

Histology.

After electrophysiology, animal was perfused with saline followed by 4% PFA

solution. The brain was taken out carefully and stored in solution with 4%

paraformaldehyde and 20% sucrose. After fixation, the brain was sliced into 60 μm slices.

Fluorescent expression in the injection site was examined under microscopy.

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paper.

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Data availability: Data supporting the findings of this manuscript are available from

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Figure Captions.

Figure 1. *Schematic diagram of the experimental paradigm.*

Figure 2. *Validation of the inhibitory effect of DREADDs.* **A**) Visual stimulation paradigm; Examples of spiking activity in the SC in response to **B**) 1 flash (100ms/flash) and **C**) 5 flashes (100ms/flash) of light stimulation after saline and CNO injections; **D**) DREADD suppressed evoked firing rate ($p < 0.005$ for both 1 flash and 5 flash stimuli, 15 trials per animal, per condition, n=3); **E**) DREADD suppressed spontaneous firing rates during 5s before visual stimulation ($p < 0.005$); **F**) Averaged spectrograms after saline (left) and CNO (right) injections; **G**) Chemogenetic inhibition reduced local field potential power (3-300Hz) in the SC. ***: $p < 0.005$.

Figure 3. *Suppressing dACC reduced its spontaneous BOLD signal, RSFC, and local network structure.* **A**) Amplitude of spontaneous BOLD activity in the DREADD (19 animals, 78 scans) and sham groups (8 animals, 41scans); **B**) Averaged seedmaps after saline and CNO injections (one-sample t-test, linear mixed model, $p < 0.0005$, FDR corrected); **C**) Left: averaged RSFC matrices after saline and CNO injections in the DREADD group. Right: connections exhibiting significant RSFC change (two-sample t-test, linear mixed model, $p < 0.05$, FDR corrected). **D**) These connections were grouped into multiple brain systems. Line thickness represents the total number of connections with significant RSFC changes between the two systems; **E**) The size of the dACC-associated community structure as a function of graph density in the DREADD group after saline and CNO injections (two-sample t-test, linear mixed model). *: $p < 0.05$; **: $p < 0.01$.

Figure 4. *Suppressing dACC disrupted activity across the DMN.* A) DMN constructed using fractional amplitude of low-frequency fluctuations (fALFF) after saline and CNO injections; B) Voxel-wise fALFF changes after DREADD inhibition ($p < 0.05$, linear mixed model, family-wise error corrected); C) RSFC between DMN regions in the DREADD and sham groups after saline and CNO injections, respectively; D) RSFC changes within the DMN after dACC inhibition ($p < 0.05$, linear mixed model, FDR corrected); E) Negative and positive RSFC changes after dACC inhibition ($p < 0.05$, linear mixed model, FDR corrected).

Figure 5. *Suppressing dACC changed DMN-related behavior (n=10).* **A**) Total distance traveled in homecage (45 min); **B**) Mean speed; **C**) Total mobile time; **D**) Total immobile time for at least 2s. **E**) Total rearing behavior. *: $p < 0.05$; ***: $p < 0.005$.

Figure 6. *Suppressing a hub node changed whole-brain network topology.* **A**) Network resilience; **B**) Small-worldness; **C**) Network segregation; **D**) Network integration. Linear mixed model; DREADD: n = 19, 78 scans; sham: n = 8, 41 scans. *: $p < 0.05$; **: $p < 0.01$.

Figure 7. *New hub emerged after the inactivation of an old hub*. **A**) Hub scores without and with dACC inactivation, respectively; **B**) The degree of dACC and ventral RSC without and with dACC inactivation (linear mixed model; n = 19, 78 scans). *: $p < 0.05$; **: $p < 0.01$; ***: $p < 0.005$.

Figure 8. *Suppressing a non-hub node did not change whole-brain network topology.* A) Amplitude of spontaneous BOLD activity in the primary visual cortex after CNO and saline injections ($p < 0.05$, n=8, 66 scans); B) Network resilience; C) Small-worldness; D) Network segregation; E) Network integration.

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How brain reacts to attack at a local region

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Supplementary Information

Figure S1. *Representative Histology.* **A**) DREADD dACC; **B**) Sham dACC; **C**) DREADD Superior colliculus. Anatomical definition of the regions are shown in the left hemisphere.

Figure S2. *LFP spectrograms after saline and CNO injections in a representative rat with DREADDs infused in the SC.*

Figure S3. *Motion levels in all groups.* **A**. dACC DREADD (n=19, 78 scans); **B**. dACC sham (n=8, 41 scans); **C**. V1 DREADD (n=8, 66 scans). Left column: translational movement (in μm). Right column: rotational movement (in rad) (linear mixed model, p > 0.05 for all 6 parameters in all groups).

Figure S4. *Sham group did not show reduced RSFC or dACC community size.* **A**) Averaged seedmaps after CNO and saline injections in the sham group (one sample t test, linear mixed model, p<0.0005, FDR corrected; n=8, 41scans); **B**) Averaged ROI-wise RSFC matrices after saline and CNO injections in the sham group. No connections exhibit RSFC changes (two-sample t-tests, linear mixed model, p < 0.05, FDR corrected, n=8, 41scans). **C**) The size of the dACC-associated community as a function graph density after saline and CNO injections in the sham group (two-sample t-tests, linear mixed model, p > 0.05 for all densities tested, n=8, 41 scans).

Figure S5. *DMN pattern revealed by independent component analysis.*

Figure S6. *Suppressing dACC changed DMN-related behavior.* **A**) Total distance traveled; **B**) Mean speed; **C**) Total mobile time; **D**) Total time when animal was immobile for at least 2s; **E**) total number of rears in home-cage in the last 15 min of tests (i.e. 30 min after injection of CNO or Saline). n=10; #: p = 0.07.

Figure S7. *Sham group did not show changed degree of the dACC or RSC.* Degree changes of the dorsal anterior cingulate area and ventral retrosplenial area in the dACC sham group (two-sample t-tests, linear mixed model, p > 0.05 for all densities tested, n=8, 41 scans).

Figure S8. *Suppressing V1 did not affect DMN activity*. DMN constructed using fALFF in the V1 DREADD group after saline and CNO injections (n=8, 66 scans).

Figure S9. *Raw EPI data.* A. Averaged EPI image for each group and condition (dACC DREADD: n=19, 78 scans; dACC Sham: n=8, 41 scans; V1 DREADD: n=8, 66 scans); B. Example of a single EPI volume.