Pulmonary acini exhibit complex changes during postnatal rat lung development

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Abstract

Pulmonary acini represent the functional gas-exchanging units of the lung and are defined as the airways distal of the terminal bronchioles. Due to technical limitations, it was not possible to identify individual acini on microscopic lung sections. Recently, X-ray tomographic microscopy has been adapted to lung imaging to overcome these limitations. This study aimed to follow the acinar development and to gain insight into changes of the acinar structures during postnatal development. Rat lungs were fixed by instillation at postnatal days P4, P10, P21, and P60. Right lower lobes were imaged at the TOMCAT beamline of the Swiss Light Source synchrotron facility at a voxel size of 1.48 μm. Individual acini were segmented out of the obtained 3D data sets by closing the airways at the acinar entrance which is the transition point from conducting to gas exchanging airways happens. Acinar development was followed by estimating the individual acinar volume, complexity, and number of alveoli (N=268). We observed that the mean volume of the acini increases 10 times between days 4 and 60 which corresponds to a 10 times increase of the total lung volume. During the same time, the coefficients of variation dropped from 1.26 to 0.49 and the difference between the mean volumes of the fraction of the 20 % smallest and 20 % largest acini decreased from a factor of 27.26 (day 4) to a factor of 4.07 (day 60). This indicates that the dispersion of the value is based on an entirely different pattern of distribution of acinar sizes. Methodologically, we conclude that our approach is well suited to follow acinar development and to acquire large amounts of data comparable to classical stereology in a time-efficient manner. Biologically, we conclude that the newly formed acini show a large size distribution which is reduced by a factor of 7 until adulthood. Most likely the latter leads to a more homogeneous ventilation of the lung.

1 Introduction

1.1 Lung development

Lung development starts with the formation of the two lung buds. During the embryonic stage (prenatal days E11-E13 in rats) the major airways and the pleura are formed. During the pseudoglandular stage (E13-E18.5) most of the remaining airway generations are formed by branching morphogenesis. Few additional branches are added during the canalicular (E18.5 - E20) and maybe the saccular stage (E20 to postnatal day P4). Epithelial differentiation becomes morphologically visible during the canalicular stage. Together with angiogenetic activation of the capillaries, this process leads to the first functional air-blood barriers in the lung.

The saccular stage represents an intermediate stage where branching morphogenesis ceases and the developmental program switches to the phase of alveolarization. During alveolarization, 90 % of the adult gas-exchange area is formed by the lifting off of new septa from the existing gas-exchange surface (Schittny 2017). The alveolarization itself is divided into two distinct phases, the so-called classical (P4-P21) and continued alveolarization (P14 to approximately P60).

During classical alveolarization, new septa are formed starting from preexisting immature septa which contain a double-layered capillary network. During alveolarization, the structure of the alveolar septa is changed to increase the efficiency of the lung. It includes the transformation of the double-layered capillary network into a single-layered one. As a consequence angiogenesis is necessary at the basis of newly forming septa. To distinguish these modes of the formation of new alveolar septa and to specify that alveolarization continues after classical alveolarization ceased, the second phase of alveolarization is called *continued alveolarization* (Schittny 2017; Schittny 2018; Schittny et al. 2008).

1.2 The functional lung units

Pulmonary acini represent the functional gas-exchanging units of the bronchial tree and are defined as the airways distal of the terminal bronchioles. The latter do represent the most distal purely conducting airways. In humans, the acini are followed by approximately four generations of respiratory bronchioles before reaching the alveolar ducts. The alveolar duct starts at the transition region between the terminal bronchioles and the alveoli, at the so-called bronchioalveolar duct junction (BADJ). The small tree of airways distal of the BADJ is called *ventilatory unit (Storey and Staub 1962)*. Since murine lungs do not possess respiratory bronchioles, the murine acini consist of one single ventilatory unit (Storey and Staub 1962). In this study we used rat lungs; hence we speak of acini. To translate our results to humans, monkeys, or dogs, one rat acinus would correspond to a single ventilatory unit in these species.

Developmentally the BADJ is of particular interest. The junction is formed during the canalicular stage when the epithelia are differentiating. Ciliated epithelia containing goblet or club cells form proximal and type I and II alveolar epithelia form distal of the BADJ. The BADJ is home to various stem cells (Storey and Staub 1962). The generation of the airway in which an individual murine acinus starts is defined during the canalicular stage and remains constant once it is formed. As a consequence, the number of formed acini also remains constant during the phase of alveolarization and thereafter (Barré et al. 2016; Barré et al. 2014). The latter was somehow surprising because the total lung volume increases by roughly a factor of 10 during alveolarization (Tschanz et al. 2014). Therefore, the mean volume of the acini has to increase by approximately the same factor. Since we can extract the acinus volume relatively easy with our method, we can test if an how the acinus volume increases during lung development.

However, besides the global numbers little is known about the range of the volume of individual acini throughout lung development. The latter represents a physiological significant value, because it has been shown by pulmonary particle deposition (Semmler-Behnke et al. 2012; Kreyling et al. 2018; Tschanz et al. 2014) and by computational fluid dynamics simulations of airflow (Fishler et al. 2015; Hasler et al. 2019; Hofemeier and Sznitman 2014) that the acinar architecture is important for ventilation and particle deposition. Therefore, in the presented study we determined the volume and number of alveoli in individual acini throughout lung development. We observed a very wide range of acinar sizes at the beginning of alveolarization at postnatal day 4 which decreased significantly until adulthood.

1.3 Acinus detection and delineation

To detect and delineate individual acini, three-dimensional information is needed. On single two-dimensional (histological) sections it is not possible to unambiguously detect which parts of the airways and alveoli in the lung parenchyma are connected three-dimensionally. Historically, single or very few acini were delineated and extracted from manually traced serial sections (Mercer and Crapo 1987; Woodward and Maina 2005) or sectioned silicone casts (Rodriguez et al. 1987), both with considerable manual work. Non-destructive three-dimensional imaging is best suited to acquire data sets that can be used to easily detect, delineate and study large amounts of single acini. This has been shown by Vasilescu et al. (Vasilescu et al. 2012). In their study, they reconstructed 22 mouse acini from tomographic data sets and compared those with scanning electron microscope images of acinar silicone rubber casts. Similarly, Kizhakke Puliyakote et al. (Puliyakote et al. 2016) analyzed the volume of 32 mouse acini, as well as the branching pattern of their internal airways. All prior work known to us has analyzed considerably fewer acini than what is presented in this manuscript.

The hereby presented method is well adapted to thoroughly analyze large amounts of acini in a time-efficient manner, where the largest part of the work is spent on the detailed stereological analysis of the extracted acini.

2 Materials & Methods

2.1 Rat lung samples

In the present study, a superset of the animals described by Haberthür et al. (Haberthür et al. 2013) were used. Tschanz et al. (Tschanz et al. 2014) described a biphasic formation of new alveoli on the same set of animals as described here. The stereological analysis presented here represents a part of the 3R-initiative (replacement, reduction, and refinement) (Flecknell 2002) for the ethical use and the reduction of the number of animals sacrificed for science.

Briefly, we extracted the lungs of Sprague-Dawley rats after having deeply anesthetized them with a mixture of medetomidine, midazolam, and fentanyl (Erhardt et al. 2012). The rats were euthanized by exsanguination during the removal of the lung. The lungs were fixed with 2.5 % glutaraldehyde by intratracheal instillation and kept under constant pressure (20 cm H_2O) during fixation to prevent recoiling of the tissue. The samples were prepared for tomographic imaging by post-fixation with 1 % osmium tetroxide and staining with 4 % uranyl acetate (to increase the X-ray absorption contrast), as well as by dehydration in a graded series of ethanol and embedding in paraffin. In total we assessed 12 animals, on postnatal days P4, P10, P21, and P60 (N=3 per day. From now on, we will omit the postnatal prefix and only list the day.).

The animals were housed in the central animal facility of the University of Bern. They received food and water ad libitum at a 12/12 hours day/night cycle. The experiments themselves, as well as the handling of the animals before and during the experiments, were approved and supervised by the Federal Food Safety and Veterinary Office of Switzerland and the Department of Agriculture and Nature of the Kanton of Bern in Switzerland.

2.2 Tomographic imaging

Tomographic imaging was performed at the TOMCAT beamline (Marone et al. 2009; Marone et al. 2011) of the Swiss Light Source at the Paul Scherrer Institute in Villigen, Switzerland. The samples were scanned at an X-ray energy of 20.0 keV. After penetrating the sample, the X-rays were converted into visible light by either a 20-μm-thick LuAG:Ce or 18-μm-thick YAG:Ce scintillator screen (both from Crytur, Turnov, Czech Republic), depending on the date of experiments. The resulting visible light was magnified using a 10-times magnifying, diffraction-limited microscope lens and recorded with a 2048×2048 pixel CCD camera (pco.2000, PCO, Kelheim, Germany) with 14 bits dynamic range operated in 2 by 2 binning mode. As a result, in a single field of view, we were able to image a sample volume of a cube of 1.5 mm side length with a voxel side length of 1.48 μm, with the exposure time of the single projections varying between 160 and 200 ms.

Since our samples were substantially larger than the field of view of the detector, we applied the so-called wide-field scanning method (Haberthür et al. 2010) to increase the field of view horizontally. Additionally, several such wide-field scans were stacked vertically to match the height of the samples.

The resulting data sets for each of the lung samples covered a field of view of a cube with approximately 4.5 mm side length which corresponds to an image stack with approximately 3000×3000×3000 pixels at 1.48 μm side length each.

The total size of all tomographic reconstructions, which is the raw data of all samples, is around 350 GB.

2.3 Extraction of acini

For the present manuscript, we extracted single acini from three-dimensional data, acquired without destroying the samples. Details of this semi-automatic extraction of the rat acini are described by Haberthür et al. (Haberthür et al. 2013). We applied this protocol to extract 701 randomly selected acini throughout lung development, at postnatal days 4, 10, 21 and 60. Individual acini were extracted from the tomographic data with a custom image processing network established in MeVisLab (version 2.1, 2010-07-26 release, MeVis Medical Solutions and Fraunhofer MEVIS-Institute for Medical Image Computing, Bremen, Germany).

This extraction was performed by segmenting the acinus volume with a gray-level threshold-based region growing algorithm using manually placed seed points. To isolate individual acini in the data set we placed disk-shaped segmentation stoppers at the acinus entrances. Each individual acinus was then exported as a single DICOM file for portability. For each acinus, its exported DICOM file contained the segmented acinus overlaid with the original background for further analysis. Example images from the DICOM files are shown in the bottom row of Fig 1.

2.4 Stereological analysis of alveolar characteristics

The stereological estimation of the alveolar number was performed according to the standards for quantitative assessment of lung structure from the American Thoracic Society (Hsia et al. 2010) to guarantee accurate and unbiased results. To perform the stereological analysis, each DICOM file from the isolated acini was sampled into a systematic random set of single images using a MATLAB script (missing citation).

The stereological assessment was performed with the STEPanizer (TSCHANZ et al. 2011), an easy-to-use software tool for the stereological assessment of digital images. Details of the stereological assessment have previously been described (Haberthur et al. 2013). Briefly, we counted the appearance or disappearance of alveolar entrance rings (Hyde et al. 2004) on paired images spanning the whole acinus volume by using the disector method (Sterio 1984) in the STEPanizer to estimate the number of alveoli in 267 of the 701 exported acini. The acini were subsampled in a systematic random way.

Previously, we have shown that the stereological assessment of the acinar volume (according to the Cavalieri principle (Cruz-Orive 1999)) gives comparable results to an automated volume extraction by counting the segmented pixels in the tomographic data sets (Haberthur et al. 2013). Due to variations in the gray value, the automatic segmentation underestimates the volume of the single acini. The best-suited approach to obtain valid and unbiased results is to asses the volume manually (according to the Cavalieri principle), which is what we did for the 267 acini presented in this manuscript. The sets of JPG slices and the raw results from the stereological analysis with the STEPanizer are available on request.

2.5 Data analysis and display

All the stereologically assessed data was processed in a Jupyter (Kluyver et al. 2016) notebook, producing all the results and plots shown below. The notebook with all its history is freely available (Haberthür 2019), the final version is available in the supplementary materials of this manuscript. The performed calculations are described in detail in section 3. In the plots, semitransparent circles mark the single observations. The box shows the 25-75 % quartiles range of the data. The whiskers extend to the rest of the distribution. Outliers are determined as a function of the inter-quartile range and are shown outside the whiskers. Numerical values in the text are given as averages±standard deviation. P-values in the text and figure legends are given as precise numbers, as suggested by Amhrein et al. (Amrhein et al. 2019).

3 Results

The number of alveoli per acinus was assessed for 267 individual acini throughout postnatal lung development at days 4, 10, 21 and 60. For day 4, we analyzed 124 acini, for day 10 we analyzed 58 acini, for

day 21 we analyzed 42 acini, and for day 60 we analyzed 43 acini.

To get started, we show an overview of our process in figure 1. The top row shows a representative light microscopy image for each assessed time point. The middle row of figure 1 shows one slice of the tomographic data sets acquired at TOMCAT. The bottom row of figure 1 is composed of one detail image from one of the extracted acini. The extracted acinus is shown in light gray as an overlay on the tomographic data.

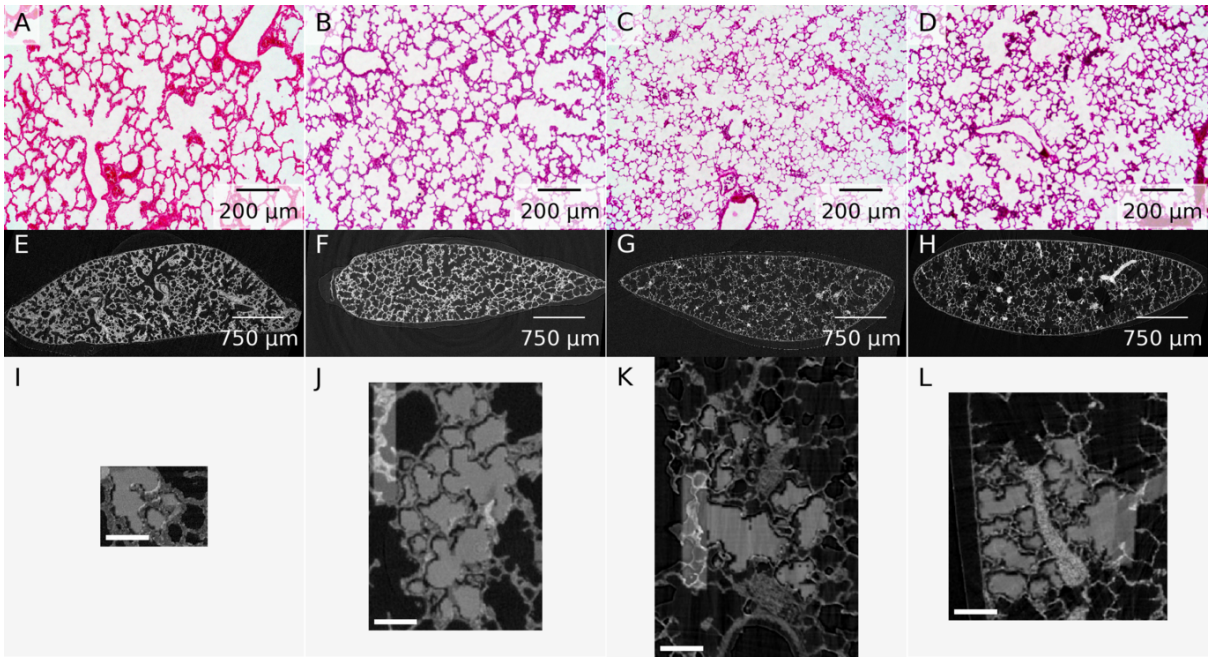

Figure 1: Example images for each of the assessed time points. A-D: Representative light microscopy images. E-H: One slice of the tomographic data sets. I-L: Middle slice of one of the extracted acini. The images correspond to the middle slice of the data sets used for the stereological analysis. The scale bar was burnt in during preparation of the data sets and is 100 μm long.. A, E, I: Day 4. B, F, J: Day 10. C, G, K: Day 21. D, H, L: Day 60. I-L:

3.1 Alveoli per acinus

The average entrance ring count, which corresponds to the number of alveoli per acinus for the 124 acini at day 4 is 48±41 alveoli. For the 58 acini at day 10 it is 89±84 alveoli, for the 42 acini at day 21 it is 233±164 alveoli. At day 60 we assessed 43 acini in total, on average they have 702±219 alveoli.

The values for the single animal are given in table 1 and plotted in figure 2.

The alveolar number shows highly significant differences (Šidák-corrected p-value < 0.00167 (Šidák 1967)) between all possible combination of days. The full statistical analysis can be found in the analysis notebook (Haberthür 2019). Briefly, we performed a Shapiro-Wilk test for normality (SHAPIRO and WILK 1965) showing us that the volumes of animals 21D, 21E and all animals of day 60 are non-normally distributed. Since at least one sample is non-normally distributed, we can use an U-test for assessing the differences, namely a two-sided Mann-Whitney rank test (Mann and Whitney 1947). This test tells us that all possible combinations of entrance ring counts per day are significantly different (all p-values are better than p=2.5e-5, which is the p-value of the difference between days 4 and 10). An additional Kruskal-Wallis H-test for independent samples (Kruskal and Wallis 1952) shows that the entrance ring counts for all animals are independent (p=2.2e-34).

Animal	Assessed acini	Average	STD	Minimum	Maximum
04A	50	27.04	23.69	4	111
04B	23	65.04	43.85	15	171
04C	51	60.51	45.42	10	249
10A	27	77.85	56.31	18	245
10B	14	84.57	65.75	23	199
10C	17	108.76	125.45	15	505
21B	14	208.14	197.71	35	781
21D	17	196.0	128.56	50	493
21E	11	323.09	145.94	108	572
60B	24	701.75	230.95	322	1296
60D	10	668.3	121.67	444	810
60E	9	739.11	281.22	272	1204

Table 1: Detailed alveolar numbers for each animal.

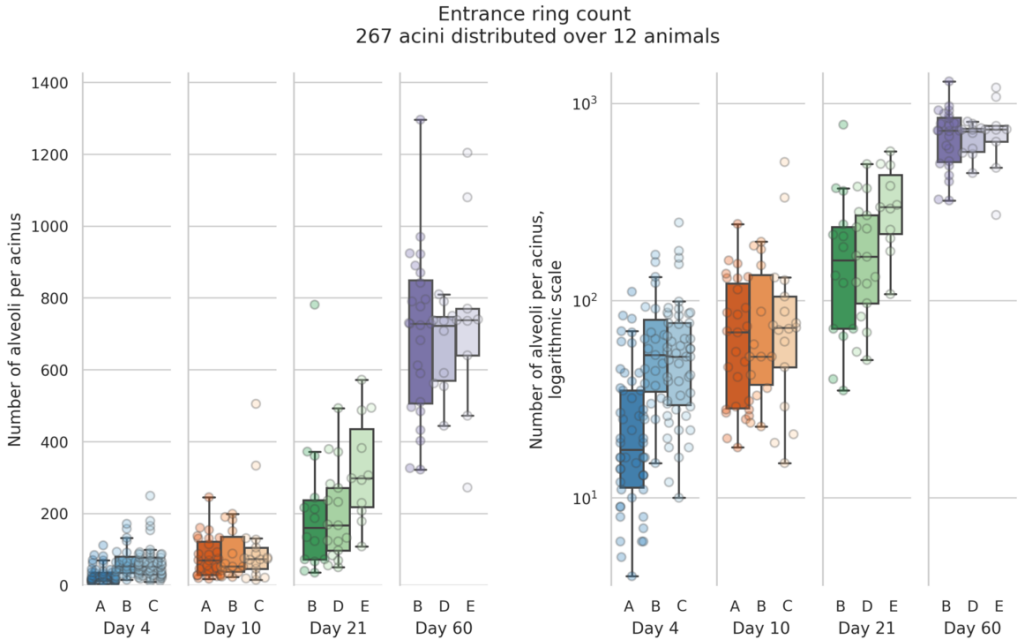

Figure 2: Distribution of the number of alveoli per acinus (entrance ring count per acinus) for each animal. Left: linear scale, right: logarithmic scale. The entrance ring counts per day are all significantly different (all p-values better than 2.5e-5, which is the one between days 4 and 10).

3.2 Acinus volume

The stereological assessment resulted in a mean acinar volume of 0.03±0.04 mm^3 for the 124 acini at day 4. For the 58 acini at day 10 we get a volume of 0.04±0.05 mm^3. For the 42 acini at day 21 a volume of 0.10±0.09 mm^3 and for the 43 acini at day 60 a volume of 0.74±0.37 mm^3.

The values for the single animals are shown in table 2 and displayed in figure 3. The mean volume of the 20 % smallest acini to the 20 % largest acini at day 4 increases 27.26 times (from 0.0035 μl to 0.095 μl, N=25). At day 10, this increase is 15.28 times (from 0.0071 μl to 0.11 μl, N=12). At day 21, this increase is 14.42 times (from 0.018 μl to 0.26 μl, N=8). At day 60, we saw an increase of 4.07 times (from 0.33 μl to 1.3 μl, N=9).

The acinar volumes show highly significant differences between all possible combinations of days except

Animal	N	Average	STD	Minimum	Maximum
04A	50	0.01	0.01	0.0	0.04
04B	23	0.06	0.05	0.01	0.19
04C	51	0.04	0.04	0.01	0.28
10A	27	0.03	0.03	0.0	0.11
10B	14	0.03	0.03	0.0	0.1
10C	17	0.06	0.08	0.0	0.33
21B	14	0.09	0.09	0.01	0.32
21D	17	0.11	0.11	0.01	0.38
21E	11	0.12	0.07	0.03	0.24
60B	24	0.59	0.22	0.23	1.1
60D	10	0.89	0.35	0.36	1.58
60E	9	0.98	0.53	0.19	1.88

Table 2: Detailed volume data for each animal.

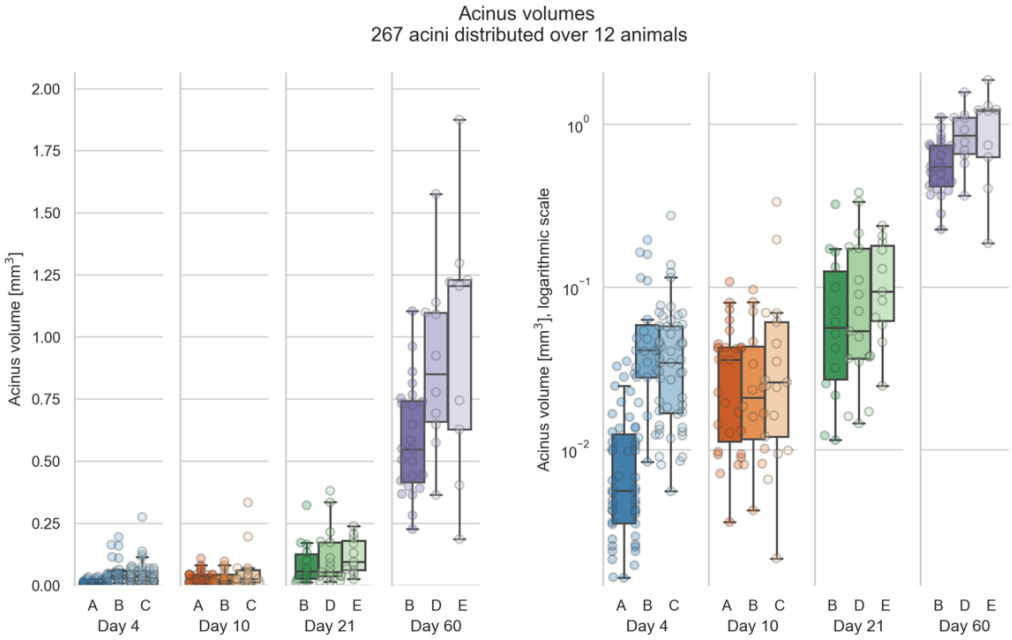

Figure 3: Distribution of the acinar volumes for each animal. Left: linear scale, right: logarithmic scale. The acinar volumes are all significantly different (all p-values better than 4.5e-6, which is the one between days 10 and 21) for each combination of days except between days 4 and 10 (p=0.092).

between days 4 and 10 (p=0.092). All other p-values are better than p=4.5e-6, which is the p-value for the difference between days 10 and 21. The statistical analysis is equal to what is briefly described for the entrance ring count above. The acinar volumes for animals 21E and all animals of day 60 are non-normally distributed, but all acinar volumes per animal are independent (p=6.4e-29).

3.3 Alveoli per volume

The mean number of alveoli for the 124 acini at day 4 is 2165±1137 alveoli per mm^3. For the 58 acini at day 10 we counted 2831±1189 alveoli per mm^3, for the 42 acini at day 21 2723±771 alveoli per mm^3 and for the 43 acini at day 60 1080±349 alveoli per mm^3. These numbers were found by dividing the counted entrance rings by the acinus volumes.

The numbers for the single animals are shown in table 3 and displayed in figure 4.

Animal	Assessed acini	Average	STD	Minimum	Maximum
04A	50	3142	1157	1618	8208
04B	23	1363	499	679	2704
04C	51	1569	380	799	2775
10A	27	2685	1022	1246	5582
10B	14	3091	1166	1890	5422
10C	17	2848	1462	1182	7009
21B	14	2642	493	1625	3344
21D	17	2534	895	1111	4032
21E	11	3119	775	1604	4379
60B	24	1249	297	530	1912
60D	10	838	271	476	1221
60E	9	898	323	411	1463

Table 3: Details of entrance ring count per acinus volume for each animal.

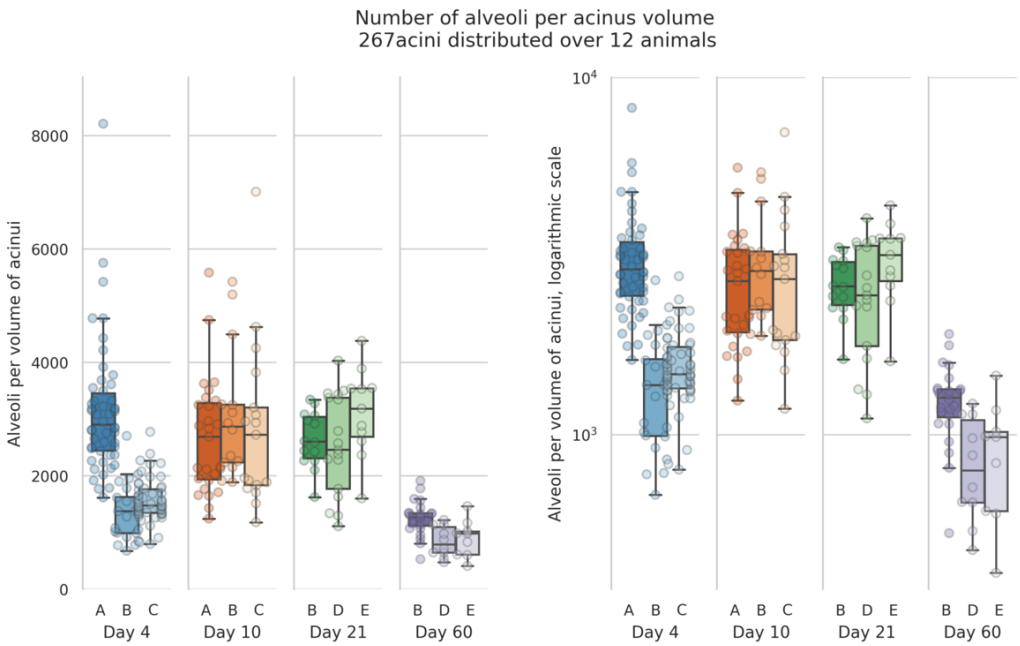

Figure 4: Number of alveoli per acinus volume. Left: linear scale, right: logarithmic scale. The number of alveoli per acinus volume are all significantly different (all p-values are better than 5.4e-5, which is the one between days 4 and 21) for each combination of days except between days 10 and 21 (p=0.7).

The counts per volume, which correspond to the number of alveoli per acinus volume are a value for estimating the complexity of the single acini. This acinus complexity shows highly significant differences between all possible combinations of days except between days 10 and 21 (p=0.7). All other days have a p-value better than p=5.4e-5, this being the one between days 4 and 21. The statistical analysis is equal to what is briefly described for the entrance ring count above. The counts per volume for all animals except 04A are non-normally distributed, but all are independent (p=3.2e-21).

3.4 Number of acini

The number of acini for day 4 was 18129±16370 acini, for day 10 14359±5611 acini, for day 21 11203±2681 acini and for day 60 4277±777 acini. These numbers were obtained by dividing the parenchymal volume of the lungs (Tschanz et al. 2014) with the Cavalieri-estimated volume of the acini.

3.5 Total number of alveoli per lung

The total alveolar number for day 4 was found to be 0.64±0.34 million alveoli, for day 10 1.23±0.39 million alveoli, for day 21 2.65±0.57 million alveoli, and for day 60 3.01±0.58 million alveoli. The total number of acini was estimated by dividing the mean parenchymal volume of the lungs (Tschanz et al. 2014), by the shrinkage-corrected stereologically estimated acinar volume. The number of alveoli is then simply the multiplication of the average entrance ring count with the estimated number of acini.

3.6 Volume of individual alveoli

The alveolar volume for day 4 was 686604 μm^3, for day 10 452285 μm^3, for day 21 445373 μm^3 and for day 60 1053526 μm^3. This corresponds to an average diameter per alveolus of 109 μm, 95 μm, 95 μm, and 126 μm for days 4, 10, 21 and 60, respectively. The average volume of one alveolus was estimated by dividing the mean acinar volume by the mean count of alveoli for each day separately.

4 Discussion

To our best knowledge, the present manuscript is the first to quantitatively describe the changes in the volumes of single rat lung acini based on stereological data obtained from all those single acini. In addition, we can easily estimate the number of acini during lung development from our data and compare this to prior work. There are some limitations to our results though. The main one is that we only assessed the acini in the lower medial tip of the right lower lung lobe.

We have assessed the same lungs as Tschanz et al. (Tschanz et al. 2014). Nonetheless, our results are not equal to what was found by Tschanz et al., but they are closely comparable. This is also because the morphometric data obtained by stereological analysis from different labs or persons can show a large variation in the final results. Osmanagic et al. have compiled results from different studies (Osmanagic et al. 2010); for example the estimated number of alveoli per unit lung volume varied by a factor of 5.2 for three studies (2.7e3-14.1e3 mm^{-3}). The measured lung volume varied by a factor of 3, which could also stem from different sample preparation, namely from different pressure levels during fixation.

4.1 Acinus volumes

The mean acinar volume significantly increases during lung development from postnatal days 10 to 60 with all p-values better than 4.5e-6. No significant difference was observed between postnatal days 4 and 10 (1.2×increase, p=0.092). A large part of the acinus volume increase happens after day 21 (compare Fig. 3).

As mentioned in the introduction, Barré et al. (Barré et al. 2016) have shown that the number of acini remains constant during lung development. This is somewhat surprising since the total lung volume increases by roughly a factor of 10 during alveolarization. Therefore, we expect the mean volume of the acini to increase by at least the same factor (Barré et al. 2016; Tschanz et al. 2014).

We observed that the mean volume of acini increases 23 times between days 4 and 60 which corresponds to a 23 times increase of the total lung volume (Increases: day 4 to day 21: 3.16×, day 10 to day 21: 2.6×, day 10 to day 60: 18.46×, day 21 to day 60: 7.11×).

During the same time, the coefficients of variation of the acinus volumes dropped from 1.26 to 0.49 but the difference between the mean volumes of the fraction of the 20 % smallest and 20 % largest acini

decreased from a factor of 27.26 (day 4) to a factor of 4.07 (day 60). This indicates that the dispersion of the value is based on an entirely different pattern of distribution of acinar sizes.

The difference of the mean acinus volumes from the smallest to the largest fraction per day becomes smaller and smaller during postnatal lung development. When we normalize the acinus volumes to the largest volume per day (data shown in supplementary materials or analysis notebook (missing citation)), we see that the spread at day 4 is smaller than at the other days. Additionally, at days 4, 10 and 21 the distribution of the normalized volumes is skewed towards less than the average (median of normalized volumes at day 4: 0.16, at day 10: 0.18 and at day 21: 0.23), which means that we have more smaller than larger acini early in the development. At day 60, the distribution is more homogeneous, with the median of the normalized acinus volumes at exactly 0.50. This result might also stem from the difficulty of locating the acinus entrance early in the lung development because the bronchioalveolar duct junction is more difficult to localize unambiguously in the three-dimensional data sets.

By dividing the individual lung volumes estimated by Tschanz et al. (Table 1, (Tschanz et al. 2014)) by the mean number of acini estimated by Barré et al. (Barré et al. 2014) we can globally estimate the mean acinar volume. The values we get from the direct Cavalieri estimation of the volumes are on average 8.31 times lower but show a similar increase over the studied period. While the estimation based on Tschanz et al. is from the entire right middle lobe and on Barré et al. globally for the whole organ, our estimation is solely based on the stereological analysis of the acini in the lower medial tip of the right lower lung lobe.

We thus suspect differences in the acinar characteristics related to their position in the organ. This has been shown before, where Kizhakke Puliyakote et al. (Puliyakote et al. 2016) found significant heterogeneities of the acini in relation to the location in the lungs. We thus expect differences in resulting absolute numbers while the general trend is expected to be comparable, which is the case here.

4.2 Acinus complexity, alveoli per volume

The volume and shape of the alveoli, alveolar ducts, and the acini are critical parameters for ventilation and particle deposition (Sznitman et al. 2010; Henry et al. 2012; Tsuda et al. 2008). Particle deposition, for example, is relatively low during the first two weeks of a rats' life, high at postnatal day P21 and medium at days P36-P90 (Kreyling et al. 2018; Semmler-Behnke et al. 2012). This correlates well with our results, where we found a significantly larger acinus complexity (number of alveoli per acinus volume) at days 10 and 21 compared to days 4 and 60 (p-values all better than 5.4e-5, which is the one for day 4 vs. day 21). Kreyling et al. (Kreyling et al. 2018) report a maximal retention of gold nanoparticles at this time point (see their Fig. 1).

Tschanz et al. (Tschanz et al. 2014) stereologically estimated the mean total acinar volume as the sum of ductal and alveolar air spaces. The mean volume of the individual alveoli was found to be smallest around postnatal day 21 (see their Fig. 4). We thus postulate a high acinar complexity at days 10 and 21 while early and late in the lung development, the acinar complexity is relatively low. This also correlates with structural changes. In rats, the alveolar air spaces are large during the first two weeks of life, small at day P21 and medium afterward (Tschanz et al. 2014).

4.3 Number of acini

Previously, it was postulated that the number of acini remains constant during postnatal lung development from day 4 to 60 (Barré et al. 2016), with a mean of 5612±547 acini per lung. Our data shows a decrease from an estimated 18100 acini at day 4 to 4300 acini at day 60. At day 60 we estimate 4277±777 acini per lung, which corresponds well to the data shown by Barré et al.

As the acini are small at days 4-21, the biological variability between the single animals has a larger impact on the results than at day 60. We thus expect a pronounced influence of minor inaccuracies of the entrance ring counts on the estimation of the number of acini. For sample 04A the Cavalieri method estimated a significantly smaller volume (p=0.025) of the acini than samples 04B and 04C. This leads

to a much larger number of acini estimated for this animal than the other animals on this day, possibly skewing the results. One also has to keep in mind that the number of acini has been calculated by dividing the parenchymal volume of the whole lungs estimated by Tschanz et al. (Tschanz et al. 2014) with our estimation of the mean acinus volumes for each day. Due to technical limitations during the imaging for this study, the mean acinus volumes were only analyzed for a small part of the entire lungs, which might be a reason for the observed differences here.

If we were to remove animal 04A from our analysis, we would estimate 6588 acini at day 4, bringing us much closer to the estimate by Barré et al. While the values at days 10 and 21 are closer to the data shown by Barré et al., they are still larger and just about do not include the Barré range in their mean±standard deviation. Again, an additional reason for the observed difference may be owned by the fact that in this study we analyzed only a small part of the entire lungs due to technical limitations during the imaging.

4.4 Total alveolar number

In this study, we assessed the number of alveoli per acinus. The alveolar number we get (0.64±0.34, 1.23±0.39, 2.65±0.57, 3.01±0.58 million alveoli for days 4, 10, 21 and 60, respectively) have to be seen in the context of the results shown by Tschanz et al. (0.823±0.01, 3.538±1.26, 14.303±3.08 and 19.297±3.06 million alveoli, (Tschanz et al. 2014), Table 1). On average, our results are five times smaller but show the same trend when linearly corrected with a factor of 5.04. The values from Tschanz et al. with their standard deviation overlap our linearly scaled values with their standard deviation, as seen in Fig. 5.

The estimation of our results is based on only one region of the lung while Tschanz et al. stereologically estimated the alveolar number over the entire right middle lobe. As with the acinar volume above, we think that the fact that the characteristics of single acini are heterogeneous in relation to the location in the lungs (Puliyakote et al. 2016) plays a major role in the differences in absolute numbers we see; nonetheless, the trend is closely comparable.

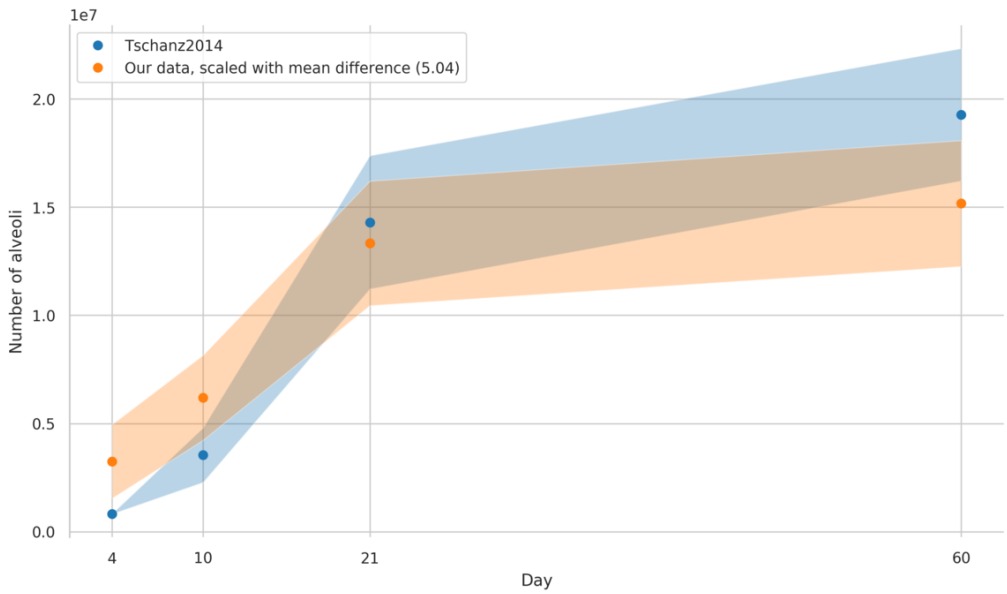

Figure 5: Number of alveoli based on data from Tschanz et al. (Tschanz et al. 2014) plotted together with our linearly scaled data (our data multiplied by 5.04). Values are plotted with a band of the width of their standard deviation.

4.5 Volumes of individual alveoli

As for the alveolar number discussed above, the mean volumes of the alveoli we assessed differs to the volumes of the single alveoli as calculated from data shown in Table 1 of Tschanz et al. (Tschanz et al. 2014). By dividing the alveolar air space by the number of alveoli we can estimate a mean alveolar volume of 5.91e5 μm^3 for day 4, of 2.49e5 μm^3 for day 10, of 1.34e5 μm^3 for day 21, and 2.93e5 μm^3 for day 60. On average, our values are 2.48 times larger (day 4: 6.87e5 μm^3, day 10: 4.52e5 μm^3, day 21 4.45e5 μm^3 and day 60 1.05e6 μm^3), but scale equally during postnatal lung development. Tschanz et al. estimated the total alveolar volume without the alveolar ducts.

Since we directly estimated the volume fraction of the alveoli per acinus our number is expected to be larger. Additionally, as specified above; the data presented here is from one region of the lung while the data we compare with has been estimated for the entire right middle lobe. The volumes do differ more than the alveolar number, though, so the volumes convey the impression of being more sensitive to regional differences than the alveolar number.

4.6 Physiological relevance of the acinar size

It has been predicted by computational fluid dynamics simulations and by to scale experiments that the amount and location of massless particle deposition, as well as ventilation, are depending on the size of the acini. The predictions could be confirmed at least in one case, where mice received fluorescent particles during mechanical ventilation. In 3D-visualizations the particles were predominately detected in the proximal half of the acini (Yang et al. 2019).

Based on the above-mentioned knowledge and the data of this study, we propose the following. In very small acini as the smallest ones we observed at postnatal day 4 acinar flows are mainly characterized by radial streamlines. Massless particle deposition is governed by diffusion(Sznitman et al. 2006). As the acini increase in size convective transport becomes more and more dominant in the proximal regions of the acini. In larger acini, the proximal region shows a much higher particle retention than the distal once. The proximal regions may even be viewed as a kind of filter capturing the particles whereas the distal regions do not receive significant amounts (Fishler et al. 2015; Hofemeier and Sznitman 2014; Sznitman 2009).

Multi-breach gas-washout is also dependent on the size of the acini. Based on computational simulations of nitrogen multi-breath gas-washout it has been shown that small acini washout faster at the beginning and slower at the end of the washout as compared to larger acini (Hasler et al. 2019). Not surprisingly, the distribution of the acinar sizes in terms of their range has also an influence on the gas-washout. Furthermore, a clustering versus an even distribution of the locations of acinar similar sizes effects gas-washout. Therefore, the question where an acinus of which size is located in the lungs has a significant influence on pulmonary ventilation and particle deposition.

The consideration of the location is not only a theoretical consideration, because it has been shown in adult mice that the acini close to the pleura are larger than central ones (Puliyakote et al. 2016). Therefore, acini of different size are not evenly distributed in the lungs.

To our best knowledge, very few data characterizing acinar properties was available up to now. This is especially true for lung development. Therefore, the data of the hereby presented study can contribute to the improvements of computational simulations of pulmonary ventilation and particle deposition.

5 Conclusion

We conclude that our method is well suited to efficiently extract precise qualitative and quantitative values of large amounts of single acini from non-destructive three-dimensional tomographic data sets. The underlying stereological analysis can be efficiently performed on tomographic data sets, the further analysis of the data was performed in a reproducible manner. Besides, our method enabled us to maximize the number of investigations per sample, thus reducing the number of sacrificed animals. The

results align with previous studies, the right middle lobe of the lung is a good estimator for assessing the quantitative data for the entire lung. Furthermore, we conclude that the newly formed acini show a large size distribution which is reduced by a factor of 7 until adulthood. Most likely the latter leads to a more homogeneous ventilation of the lung and an increase of gas-washout equal to a decrease in number of breaths needed for gas-washout.

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7 Contributions

JS conceived the project. DH, SB and JS performed the tomographic data acquisition. DH segmented the acini. EY and DH analyzed the acini stereologically. DH, ST, TC and JS analyzed the data. DH wrote the manuscript and generated all figures. ST and JS contributed to writing, all authors proof-read the manuscript.

8 Disclosures

No conflicts of interest, financial or otherwise, are declared by the authors.

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