Title

Effective mechanical potential of cell–cell interaction explains basic structures of three-

dimensional morphogenesis

Short title

Effective potential of cell–cell interaction for morphogenesis

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Author contribution

H.K. designed the work, H.K., A.M.I., and H.O. contributed to the conception. H.K. and

T.F. designed experiments, T.O. provided experimental materials, and H.K. performed

experiments and image processing. H.K. and H.O. designed models, H.K. developed

computational algorithms, and H.K. and K.N. statistically analyzed the data. H.K., T.O.,

H.O., A.M.I., K.N., K.K., and T.F. wrote the manuscript, and all authors contributed to

the interpretation of the results.

Conflicts of interest

The authors declare no competing financial interests.

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61   Main text

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Abstract

Mechanical forces of cell–cell interactions are critical for the emergence of diverse three-

dimensional morphologies of multicellular organisms. Live measurements of the forces

have been difficult due to technical limitations. Here, we developed a framework for

inferring and modeling mechanical forces of cell–cell interactions. First, by analogy to

coarse-grained models in molecular and colloidal sciences, cells were approximated as

spherical particles, where the mean forces (i.e. effective forces) of pairwise cell–cell

interactions were considered. Then, the forces were statistically inferred from cell

tracking data, and subsequently, we successfully detected effective mechanical potentials

of cell–cell interactions as a function of the cell–cell distances in epithelial cells,

blastomeres, etc. Through perturbation experiments, we found that quantitative

differences in the potentials reproduce morphological features in the mouse and *C.*

elegans early embryos, including compaction and cavitation. In conclusion, effective

potential is a measurable approximated parameter describing three-dimensional

morphogenesis.

Introduction

In multicellular living systems, various three-dimensional morphologies are

emerged, which is thought to be primarily dependent on the mechanical properties of the

constituent cells (1–5). To understand the mechanisms of morphogenesis in large tissues

including embryos, organoids, etc., predictable mathematical models are required to be

developed. Multicellular systems are of many degrees of freedom. For instance,

mechanical interactions among cells are provided from adhesive forces and cell surface

tensions (Fig. 1A-i) (4), while there are non-cellular structures such as extracellular

matrices and liquid cavities, all of which contributes to cell behaviors. Quantitative and

spatiotemporal measurements of their related mechanical forces are required for

developing predictable models, but are still highly challenging. Another possible solution

is to develop approximated models with low degrees of freedom. This idea is analogous

to molecular sciences where models used for molecular dynamics simulations are

approximation of models based on quantum mechanics.

Here we explain typical examples of approximation and then present our strategy

later. In two isolated cells as a simplest situation (Fig. 1A-i), because cell–cell adhesive

forces reduce cell–cell distances (Fig. 1A-ii, "Attractive"), the adhesive forces may be

approximated as distance-dependent attractive forces (Fig. 1A-iii, "attractive force")(6–

8). Conversely, excluded volume effect of cells increases cell-cell distances (Fig. 1A-ii,

"Repulsive"), corresponding to repulsive forces (Fig. 1A-iii, "repulsive force"). In

consequence, the summation of these attractive and repulsive forces provides a distance–

force curve (Fig. 1A-iii), which can be written as a distance–potential energy curve (Fig.

1A-iv). From the profiles of these curves, we can speculate various properties of the

particles and of the interactions (e.g. the distance at the potential minimum corresponds

to the mean diameter of the particles.) (Fig. 1A-iii and -iv). Such pairwise potential of

cell-cell interactions is conceptually well recognized (6–15), and various profiles of the

potentials have been assumed in theoretical studies for multicellular systems (e.g. hard-

or soft-core potentials etc.) (8, 12, 16). In experiments, adhesive forces between two

isolated cells have been measured (i.e. forces required to dissociate one cell from the

other) (4, 17). However, quantitative profiles of the potentials have neither been measured

nor inferred, though such profiles would be critical for cell behaviors. In addition, this

approximation is analogous to non-living matters such as atoms, molecules, and colloids:

although the interactions among these matters are determined by electron clouds (i.e.

quantum state) which have complex shapes, approximation as pairwise potentials is

succeeded and is very useful for simulating large systems (18).

In real tissues, the situations are more complicated. For instance, cell shapes can

be far from spherical shapes in contrast to isolated cells (Fig. 1B-i). Apico-basal polarity

is linked to biased localization of cell–cell adhesion proteins such as cadherins, leading

to directional differences in cell–cell interaction forces (1, 2, 19). Moreover, the apico-

basal polarity cannot be defined in isolated cells but can be in epithelial cell sheets in the

relationship among surrounding cells (i.e. many-body effect), resulting in no adhesive

capabilities on the apical and basal surfaces. However, whether pairwise potentials can

be defined and experimentally measurable in real tissues remains to be addressed (Fig.

1B-ii). By contrast, modeling of polarized or non-spherical objects have been performed

in atomic and molecular sciences (Fig. 1B-iii); even in the case of polarized or non-

spherical molecules including water and amino acids, pairwise potentials have been

sometimes defined, and these approximation models (i.e. coarse-grained models) have

been succeeded to explain overall behaviors of the systems with a trade-off of

microscopic accuracy (18).

To measure or infer pairwise potentials in real tissues, we were inspired by

atomic and molecular sciences where inferences of potentials among these matters are a

central issue. In the fields, one strategy is usage of potential energy of a whole system

calculated on the basis of quantum chemistry. Then, pairwise potentials of the matters are

searched for so as to satisfy the value of the above potential energy. In other words, the

information based on quantum chemistry is used as data to be referred during inference

(i.e. reference data) (20). Another simpler strategy is a usage of radial distribution

functions (i.e. spatial information of matters) as reference data, because the functions

mean probability of particle positions along particle–particle distances, which can be

linked to potential energy (21, 22). These resultant potentials are called effective

potentials which are summations of effects of various microscopic components, though

each component does not explicitly appear.

In this study, we developed a method for statistically inferring effective

potentials of cell–cell interactions using nuclear tracking data from live imaging as

reference data (Fig. 1C-i and -ii): force values of cell–cell interactions are fitted to the

nuclear tracking data (Fig. 1C-iii). Our method was validated by using various synthetic

data generated by simulations. Through these analyses, we described what kind of

microscopic mechanical properties such as cell surface tension can be reflected into

effective potentials (Fig. 1C-iv). To evaluate the applicability and limitation of our

method, we investigated influences of non-cellular external factors such as extracellular

matrix. Finally, we applied our method to real multicellular systems including the *C.*

elegans and mouse embryos, and successfully detected effective potentials of cell–cell

interactions. Furthermore, quantitative differences in the profiles of the effective

potentials can describe morphologies of the embryos (Fig. 1C-iv).

Theory and principle for inferring effective potential

In this section, we explain the inference method shown in Fig. 1C.

Particle-based cell models

In our model, particles interact with each other and attractive or repulsive forces

(F_i) are assumed (Fig. 1C-i), where i is an identifier for particle–particle interactions. In

three-dimensional cellular systems with no attachment to substrates, we did not assume

persistent random walks which are originated from cellular traction forces on substrates

(23, 24).

The equation of particle motions is defined below. In cellular-level phenomena,

viscous drag force or frictional force provided by the surrounding medium or tissue is

dominant, as expected from the low Reynolds number; consequently, the inertial force is

negligible in general (3, 6, 25–27). The forces in such a system can be assumed to be

correlated with the velocities of the objects (3, 12, 25, 28, 29). Thus, the velocity ($V_{C|p}$)

of a particle is calculated by the net force ($F_{C|p}$) exerted on the particle as follows (Fig.

1C-i):

$V_{C|p} = F_{C|p} / \gamma$ (Eq. 1),

where p is an identifier for particles and γ is the coefficient of viscous drag and frictional

forces. $F_{C|p}$ is the summation of cell–cell interaction forces exerted on the pth particle. We

assumed the simplest situation, i.e., γ is constant (=1.0). Thus, by giving the values of F_i

from, for instance, a distance–potential curve, a simulation can run.

Data acquisition of time series of cell positions

To define cell positions, we focused on nuclei, because they are most easily

imaged by microscopy (Fig. 1C-ii) in a wide range of organisms from *C. elegans* to

mammals, and these data are accumulating (30–34). We utilized publicly available

nuclear tracking data of a developing embryo of *C. elegans* (30); nuclear tracking data of

developing mouse embryos and Madin-Darby canine kidney (MDCK) cultured cells

derived from dog kidney epithelium were obtained in this study.

Development of method for inferring effective potentials/forces of cell-cell interaction

In the case of ions, molecules, etc., radial distribution functions are often used to

infer the effective potentials of their interactions (21, 22). This method is simple, but is

only applicable to thermodynamically equilibrium systems because this function reflects

the effective potentials under equilibrium states. Therefore, this method is not suitable for

non-equilibrium systems, including morphogenetic events. To infer the effective

potentials in non-equilibrium systems, we fitted the particle-based cell model to the time

series of nuclear positions, where the fitting parameters are forces between all pairs of

cell–cell interactions for each time frame. We systematically searched for the values of

the effective forces between all pairs of cell–cell interactions that minimized the

differences (i.e. corresponding to least squares) between the particle positions in the

simulations and the *in vivo* nuclear positions. The differences (G_{xyz}) to be minimized are

defined as follows.

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$$G_{xyz} = \sum_{t=1}^{T} \sum_{p=1}^{P(t)} \frac{\left\{x_p(t) - x_p^{\text{ref}}(t)\right\}^2 + \left\{y_p(t) - y_p^{\text{ref}}(t)\right\}^2 + \left\{z_p(t) - z_p^{\text{ref}}(t)\right\}^2}{\Delta t}$$

202   (Eq. 2)

Here, p is an identifier for particles, t is an identifier for time frames, and Δt is

the time interval between the time frames. T is the total time frame, and $P(t)$ is the number

of particles at each time frame. The x, y, and z coordinates of the pth particle obtained

from microscopic images are x_p^{ref}, y_p^{ref}, and z_p^{ref}; ref means reference. The coordinates of

the simulations are x_p, y_p, and z_p. Note that, because γ was assumed to be constant in

Equation 1, we can only infer relative but not absolute values of effective forces.

To determine whether our method can correctly infer effective forces, we applied

it to synthetic data generated by simulations under given potentials of particle–particle

interactions, and examined whether the inferred effective forces were consistent with the

given potentials. Unfortunately, Equation 2 did not work well, and therefore, we tried to

incorporate various additional constraints into Equation 2. We found that the following

cost function worked well: the function was set so that force values approach zero at long

distant regions of cell–cell interactions as defined below:

$$G = G_{xyz} + G_{F_0} \qquad (G_{F_0} = \omega_{F_0} \sum_{t=1}^{T} \sum_{i=1}^{I(t)} \psi(D_i) F_i^2 \Delta t)$$ (Eq. 3),

where $I(t)$ is the total number of the cell–cell interactions for each time frame, D_i is the

cell–cell distance of the ith interaction, and ω_{F_0} is a coefficient for determining the

relative contribution of the second term to G. $\Psi(D_i)$ is a distance-dependent weight that

exponentially increases and eventually becomes extremely large (Fig. S1A-iii). We show

validations of this cost function in the next sections. Detailed principles, rationale, and

procedures are described in SI (Section 4).

Results

Systematic validation of inference method using simulation data

226   We systematically validated our inference method using simulation data. We

used the Lenard–Jones (LJ) potential as a test case of the given potentials (Fig. 2A-i), and

generated simulation data under LJ potential, to which we applied our inference method.

Importantly, we assumed cell-intrinsic mechanical activities that were introduced as

fluctuations of the forces relative to the LJ potential (Fig. 2A-i, "fluctuation (% of LJ)"),

because the cells rapidly stop movements without such activities.

In Fig. 2A-i, the particles were initially scattered to some extent, and then

assembled. The inferred effective forces for each pair of particles for each time frame

were plotted against particle–particle distances (Fig. 2A-ii), and by calculating binned

averages, we obtained distance–force (DF) curves (Fig 2A-ii, yellow). In the absence of

the fluctuations, the data points were located around the DF curve (SD = 0%), and the DF

curve showed a similar profile to that from the LJ potential (Fig. 2A-iii, LJ vs. 0%). In

the presence of the fluctuations (SD = 100 or 1,000%), although the data points were

widely distributed (Fig. 2A-ii), the resultant DF curves were equivalent to that of the LJ

potential and of that under SD = 0% (Fig. 2A-iii). These results suggest that our method

is correctly applicable for assembling process even under large fluctuations of the forces.

In Fig. 2B-i, effective DF curves were inferred in systems under steady states

where particles continuously moved due to the force fluctuations (SD = 1,000%). The

inferred DF curves showed an almost similar profile to that of the LJ potential (Fig. 2B-

ii, sampling interval = 1min), but increased sampling intervals caused inconsistency with

the LJ potential (sampling interval = 5 min).

In Fig. 2C-i, effective DF curves were inferred in systems with cell proliferation

where cell numbers were increased from 38 to 47. The inferred DF curves showed a

similar profile to that of the LJ potential (Fig. 2C-ii), and the influence of the sampling

interval was similar to Fig. 2B.

These results suggest that our method can correctly infer the forces of cell–cell

interactions even under large cell-intrinsic fluctuations. Note that long sampling intervals

cause incorrectness of the inference in practice.

Applicability of inference method to epithelial cells

Next, we investigated the applicability of our inference method to epithelial cells.

In epithelial cells, both cell–cell adhesive forces and cell surface tensions are exerted on

the cell–cell junctions in a similar manner to the isolated two cell systems in Fig. 1A-i.

Therefore, we expected that attractive and repulsive forces could describe epithelial cell–

cell interactions. On the other hand, due to the tight packing of cells, potentials other than

pairwise potentials are defined in the relationship among more than 2 cells, called many-

body effects: in a standard mathematical model for epithelia (i.e. vertex model), many-

body effects are assumed (35). If such many-body effects were dominant in epithelial

cells, the relationships such as between cell–cell adhesive forces and attractive forces

would disappear. To test whether attractive forces are detected in epithelial cells, we

applied our inference method to synthetic cell tracking data generated by a vertex model.

We adopted a simplest vertex model where cell–cell adhesive forces and cell

surface tensions are assumed to be exerted on cell–cell junctions (Fig. 3A) (36). The

adhesive forces and surface tensions function to expand and shrink the lengths of cell–

cell junctions, respectively. Similar to the particle model in Fig, 2, fluctuations of forces

were introduced to cell–cell junction tensions (Fig. 3A); without the fluctuations, cells

rapidly stop their movements. The area elasticity reflects excluded volume effect of cells.

This elasticity also contains many-body effect, because the forces are determined by all

contacting cells (>2 cells) for each cell. We performed simulations with several tens of

cells (Fig. 3A, "Simulation") and obtained cell tracking data.

Fig. 3B-i shows the plots of inferred forces against cell–cell distances. In the

absence of the fluctuations of tensions (0%), the distribution of the data points was not so

diverged, and a DF curve was detected (Fig. 3B-i, binned average, and 3B-ii) which

exhibited a typical profile with a peak of the attractive force. In the presence of the

fluctuations, the distributions became wider, but the DF curves were detected whose

profiles were equivalent to that without the fluctuations (Fig. 3B-ii).

Next, we examined whether microscopic features of epithelial cells were

reflected into the effective DF curves. We performed simulations under various values of

the cell–cell adhesive forces (Fig. 3C-i). The inferred DF curves are shown in Fig. 3C-ii,

whose profiles are quantitatively evaluated in Fig. 3C-iii. The absolute values of the

maximum attractive forces were positively correlated with the cell–cell adhesive forces

(Fig. 3C-iii, left panel), and the distances at the maximum attractive forces were

negatively correlated (Fig. 3C-iii, right panel). These results are consistent with the case

in the isolated two cell systems. We also evaluated the effect of the cell surface tensions,

and found that the effect on the maximum attractive forces was opposite to the cell–cell

adhesive forces (Fig. 3D-i and 3D-ii). These results indicate that the effects of the

microscopic features of the cells are conserved among epithelial cells and isolated two

cell systems.

294   Finally, we evaluated the effect of the area elasticity. Under large area elasticity,

one expectation is that the slope of the repulsive region in the DF curve becomes steeper

due to its elasticity, and another expectation is that the typical profiles of DF curves

disappear due to its many-body effect. The inferred effective DF curves and their

quantitative evaluations are shown in Fig. 3E-i and 3E-ii. The typical profiles of DF

curves such as the peak of the attractive forces were clearly detected even under larger

area elasticities. The profiles of the repulsive regions were not obtained in most of the

conditions, though the slope under the area elasticity = 10.0 was steepest.

In summary, effective DF curves are detectable in epithelial cells, and the cell–

cell adhesive forces and cell surface tensions are correctly reflected into the DF curves.

These results suggest that particle models with pairwise potentials can be approximated

models for epithelial cells.

Cell growth is effectively repulsive

Cell growth (i.e. cell volume increase) is an important parameter for cell

behaviors and homeostasis in multicellular systems: cell growth increases pressure in

multicellular systems, leading to contact inhibition of growth, delamination in epithelial

sheets, and apoptosis (37–39). Under increased pressure, cells push/repel each other. In

other words, the intrinsic attractive forces between cells can be effectively cancelled due

to cell growth. To test this hypothesis, we used a mathematical model considering cell

growth. A well-known cell growth model is shown in Fig. 4-i where one cell is modeled

as two particles and the growth is described by the repulsive force between the two

particles (10, 29, 37). When the distance between the two particles reaches a critical value,

cell division occurs. Note that particle–particle interactions between different cells were

implemented by the LJ potential (Fig. 4-i, "LJ").

We performed simulations and inferred effective DF curves between cells (Fig.

4-i, "DF curve" between the orange cells). When the cell growth coefficient B was set to

be larger, cell number was increased (Fig. 4-ii). Fig. 4-iii shows the inferred effective DF

curves and Fig. 4-iv is their quantitative comparisons. The maximum attractive forces

were negatively correlated with the growth forces, and eventually, the attractive

components were absolutely diminished (Fig. 4-iv, left panel). In addition, the distances

at the maximum attractive forces were not changed by the growth forces (Fig. 4-iv, right

panel). These results indicate that cell growth effectively decreases attractive forces of

cell–cell interactions.

Three possibilities of influences of external factors

In real tissues, there are various types of non-cellular external factors which

affect cell behaviors; extracellular matrix, egg shells, liquid cavity, etc. We investigated

the applicability of our inference method to such systems. We think that there are three

possibilities of inference results as follows. 1) External factors do not affect inference

results, where correct DF curves are obtained. 2) External factors spoil inference results,

where obtained DF curves are meaningless. 3) External factors modulate DF curves, but

the effects are correctly reflected into the curves. The third possibility is analogous to

atomic, molecular, and colloidal sciences. For instance, external pressures increase the

density of objects, which is reflected into the radial distribution function linked to

distance–potential curves (18). Another example is solvents, where hydration of particles

by the solvents yields energy barriers in effective distance–potential curves (22). In

multicellular systems, however, it has not been clarified what kind of non-cellular external

factors result into the above three cases. We examined effects of several external factors

as follows.

Influences of external factors; cell–extracellular matrix adhesion is effectively repulsive

We investigated the effect of cell–extracellular matrix (ECM) adhesion (Fig. 5A-

i). Spreading of cells is regulated by competition between cell–ECM and cell–cell

adhesions; increased forces of cell–ECM adhesions lead to the increase in apical cell area

in epithelial cells (Fig. 5A-i) (19, 40, 41). Because the increase in each cell area pushes

surrounding cells away, the cell–ECM adhesive forces would function to repulsive forces

of cell–cell interactions (Fig. 5A-i, "Repulsive force"). Simultaneously, increased cell

areas lead to increases in distances between cells, which should be reflected as a shift of

effective DF curves to rightward along the cell–cell distances (Fig. 5A-i, "Shift of DF

curve").

We modeled cell–ECM adhesion in the vertex model used in Fig. 3. The potential

energy was defined as $E_{\text{ECM}}a_n$ for each cell, where E_{ECM} is the coefficient of the

energy. Under increased cell–ECM adhesive forces, cell areas were increased (Fig. 5A-ii,

E_{ECM} = 1.0). Fig. 5A-iii shows inferred effective DF curves, and Fig. 5A-iv is the

quantitative evaluation of the curves. As expected, the maximum attractive forces were

negatively correlated with the cell–ECM adhesive forces (Fig. 5A-iv, left panel), and the

distances at the maximum attractive forces were increased by the cell–ECM adhesive

forces (Fig. 5A-iv, right panel). These results suggest that the cell–ECM adhesive forces

can be correctly reflected into the effective DF curves.

Influences of external factors; traction force between cell–extracellular matrix

In the presence of ECM, cells possess self-migratory activities through traction

forces between the cells and ECM (23, 42). We examined whether traction forces

influence effective DF curves. We implemented traction forces in the particle model used

in Fig. 2. The directions of the traction forces were set to be random (Fig. 5B-i), and

persist during a given time period (Fig. 5B-ii, "with persistency = 50.0min"). Cell–cell

interaction forces were provided by the LJ potential (Fig. 5B-i, "LJ"). The value of the

traction forces is shown as a relative value to the maximum attractive force of the LJ

potential (Fig. 5B-ii, "1,000% of LJ"). Simulations were performed two-dimensionally.

Fig. 5B-iii shows inferred effective DF curves. In the absence of the traction

forces (0%), the inferred curve showed a similar profile to the given LJ potential, though

an inconsistency was observed at the distant region (distance = ~7μm). In the case that

the value of traction forces was equivalent to the attractive force of the LJ potential

(100%), the curve was consistent with that without the traction forces, whereas, under a

larger traction force (1,000%), the curve became highly repulsive. Fig. 5-iv shows effects

of persistency of the traction forces. Even under the large traction forces (1,000%), a DF

curve was consistent with that from the LJ potential if the persistency was short (left panel,

1.0min). In conclusion, traction forces can significantly modify effective DF curves if

both the force value and the persistency are large. Otherwise, correct DF curves can be

obtained. We speculate that this modification spoils the inference. Similar repulsive

profiles of DF curves were obtained in MDCK cells on substrates, which have high self-

migratory activities (Fig. S3A).

Influences of external factors; egg shell has no influence on effective forces

Next, we introduced spatial constraints corresponding to egg shells. The particles

with the LJ potential were put into cylindrical constraints (Fig. 6A-i). In longer lengths

of cylinders, inferred DF curves were well consistent with the DF curves from the LJ

potential (Fig. 6A-ii; length of cylinder $\geq 25\mu m$). By contrast, under shorter cylinders, the

profiles of inferred DF curves were shifted leftward along the distance (Fig. 6B-ii; length

of cylinder $\leq 20\mu m$). This shift is reasonable as follows. A snapshot of the simulation

under the length = $16\mu m$ is shown in Fig. 6A-ii, where the particle diameters were set to

be equivalent to the mean diameter of cells defined in Fig. 1A-iii. The particles were very

closely contacted each other so that the distances between the adjacent particles seemed

to be less than the diameter of the particles. Therefore, the particles were compressed.

Radial distribution functions under compressed conditions should also shift leftward

along the distance (Fig. 6A-iii, "non-compressive" vs. "compressive"), which are linked

to effective DF curves. Therefore, our inference method can correctively reflect the effect

of compression into effective DF curves. However, in cell biology, we think that the

compressive conditions are not physiologically relevant, because cells are essentially

composed of non-compressive liquid and their volumes are not changed by external

pressure. In conclusion, DF curves are correctly inferred under spatial constraints.

Influences of external factors; liquid cavity is approximated as effective forces

Next, we introduced cavities. Cells can generate cavities by secreting liquid, and

then the pressure of the cavities push the cells away (43–45). Here we implemented

expanding cavities as spatial constraints in simulations (Fig. 6B-i, the radius of the cavity

is increased from 9.6 to 12.6μm), and the particles with the LJ potential move on the

surfaces of the cavities. Fig. 6B-ii shows that inferred effective DF curves were not

consistent with the DF curves from the LJ potential, where repulsive components were

strongly detected especially at distant regions, which we call distant energy barrier (DEB).

415   We then examined whether this modification is meaningless or is a result of a

correct reflection of the expanding cavities. By performing simulations with the

expanding cavities but without the LJ potential (Fig. 6C-i), we solely extracted the

influence of the expanding cavities. Fig. 6C-ii shows that the inferred DF curves were

absolutely composed of repulsive components. Then, we checked the raw data where all

data points were plotted on the distance–force graph. In Fig. 6D-i, "From C", a heat map

of the data points is shown with binned averages (yellow) corresponding to the DF curve

in Fig. 6C-ii. Interestingly, all the data points were closely located around the DF curve

("From C"), implying that the DF curve is a good approximation of the expanding cavities.

424   Finally, by using the above information, we examined whether the correct DF

curve (i.e. LJ potential) can be reconstructed. We subtracted the DF curves of Fig. 6C

from those of Fig. 6B (Fig. 6D-i, "From B – From C"). The resultant DF curves in Fig.

6D-ii were well consistent with the LJ potential under any expansion rates of the cavities.

These results suggest that the effects of the expanding cavities can be approximated as

effective DF curves.

We interpret the above results as described in Fig. 6E. A cell receives forces from

cell–cell interactions ("LJ") and from the pressure from the cavity, where the vector of

the pressure is perpendicular to the surface of the cavity (Fig. 6E, top panel). The repulsive

forces detected as cell–cell interactions in Fig. 6C are described in Fig. 6E, middle panel,

and the vector of the net force is perpendicular to the surface of the cavity, if the cells are

almost uniformly distributed. Therefore, the pressure from the cavity can be equivalent

to the net force from the DEBs (Fig. 6E, bottom panel), leading to the successful

reconstruction of the LJ potential.

We conclude that the expanding cavities can be approximated as effective

potentials. Effective potentials are the summation of different components as explained

in Fig. 1A-iii. External factors are also one of the components in molecular and colloidal

sciences: e.g. by considering hydration of particles by solvents, effective potentials are

modified so as to contain energy barriers around distant regions (21, 22), and such

effective potentials have been used to simulate behaviors of the systems.

Inference of effective forces in C. elegans early embryo

We next investigated whether effective potential could be detected as a function

of cell–cell distance in three-dimensional *in vivo* systems. The nematode *C. elegans* has

well-defined embryogenesis: cell movements in early embryos are almost identical

among different individuals, and the time series of nuclear positions have been reported

previously (30). During early *C. elegans* embryogenesis, a fertilized egg (i.e. one cell)

repeatedly undergoes cell division and cell differentiation in a stiff/undeformable egg

shell, ultimately forming an ovoid embryo containing ~350 cells (Fig. S6A and Movie

S1A). The cells become smaller through cell division (46), and the total volume of the

embryo remains constant. Thus, the volume of each cell is reduced by a factor of 350

relative to the original egg, meaning that mean cell diameter is reduced by a factor of 7.

Because particle diameter is approximately reflected on a DF curve (Fig. 1A-iii), we

expected that inferred DF curves should be gradually shifted to the left side of the

distance–force graph throughout embryogenesis.

Figure 7A is a snapshot that shows nuclear positions with the cell lineage and

inferred effective forces where the color of the lines corresponds to the values of the

forces (Movie S1B). The temporal changes in the mean diameters of the cells were

estimated in Fig. 7B; e.g., the diameter at t (time frame) = 195 is ~28% of that at t = 16.

In our inference in this system, we confirmed that this inference problem has essentially

464 a unique solution (Fig. 7C).

465   We divided the whole embryogenesis into segments containing different time

466 frames, and obtained DF curves. Fig. 7D is an example of the DF curve (binned average)

467 at t = 76-115 with all data points shown as a heat map. Although the data points were

468 widely distributed similar to the previous figures (e.g., Fig. 2A and 3B), a clear DF curve

469 was detected. Fig. 7E shows the DF and DP (distance–potential) curves for each period (t

470 = 16–55, 36–75, 76–115, 116–155, and 156–195). These curves were gradually shifted

471 toward the left side (Fig. 7E), as we had theoretically expected, indicating that the inferred

472 effective potentials were quantitatively consistent with the reduction in cell volume

473 during embryogenesis. To evaluate differences in mechanical properties among the

474 periods, we normalized both the distances and potentials by the distances at the potential

475 minima (Fig. 7F). The curves were almost unchanged during the periods, suggesting that

476 the mechanical properties of cell–cell interactions are not drastically modulated during

477 the development except for the cell sizes.

480 *Inference of effective force in mouse pre-implantation embryos*

481   To further investigate whether effective forces could be obtained in three-

dimensional systems, we focused on mouse pre-implantation embryos, including morulae

at the 8-cell, compaction, and blastocyst stages (Fig. 8A, illustration). In 8-cell stage

embryos before compaction, cell–cell adhesion is weak, and individual cells can be easily

discerned (Fig. 8A, bright field). In the compaction-stage embryos composed of ~16-32

cells, cell–cell adhesion becomes stronger due to elevated expression of cadherin proteins

on cell membrane, and the cells are strongly assembled (47). The surface of the embryo

becomes smooth, and the embryonic shape becomes more spherical (Fig. 8A, bright field).

In blastocyst-stage embryos composed of >64 cells, an inner cavity is formed through

liquid secretion from the cells, and the embryos expand while maintaining their spherical

shape (43–45) (Fig. 8A, bright field and cross-section). Trophectoderm (TE) cells form a

single–cell-layered structure at the outermost surface of the embryo, whereas the cells of

the inner cell mass (ICM) were tightly assembled, forming a cluster (Fig. 8A, illustration).

We performed cell tracking (Fig. 8A, tracking) and inferred effective forces.

Fig. 8B and 8C shows the inferred effective DF and DP curves for all three stages.

The DF curves derived from the 8-cell and compaction stages had typical profiles, with

repulsive and attractive forces detected. On the other hand, the DF curves derived from

the blastocyst stage contained highly repulsive regions (Fig. 8B, DEB), similar to the case

of simulation data considering an expanding cavity (Fig. 6B). Moreover, when we

inhibited the cavitation by an inhibitor for Na^+/H^+ exchanger (S3226) (48), DEB was

diminished in the inferred potentials (Fig. S9), indicating that the cavity yielded the DEBs.

These results indicate that the effective DF curves experience changes in their profiles

during the development.

Inference of effective distance–force curves in MDCK cyst

To further test the applicability of our method to structures harboring cavities,

we focused on MDCK cells which can form cysts containing a cavity when cultured in

suspension (Fig. 9A, illustration) or in gels composed of ECM (49). To exclude adhesion

between the cysts and the ECM, we chose suspension conditions in which a cyst can be

assumed to be a mechanically isolated system. Fig. 9B and 9C show the DF and DP curves.

A DEB was detected in the DF curves.

Effective potentials are capable of describing morphologies

Effective DF/DP curves are the summation of the multiple components including

the excluded volume effect, adhesive forces, and external factors, and are useful to study

behaviors of systems in molecular and colloidal sciences. We evaluated whether inferred

effective DF curves from the *C. elegans*, mouse embryos, and MDCK cysts can reproduce

their morphologies. In simulations of multicellular systems, the morphologies are

determined by both DF curves and initial configurations, because energetic local

minimum states (i.e. metastable state) as well as global minimum states are meaningful.

To find stable states under the DF curves, we performed simulations starting from various

initial configurations of the particles, and the systems were relaxed.

From the DF curves of the *C. elegans* embryos, we observed a tendency that the

particles form an aggregate with an ovoid or distorted shape (Fig. 10A). These results

may be consistent with experimental observations: the embryonic cells can keep a cell

aggregate even when the eggshell is removed, and subsequent culture leads to a cell

aggregate with an ovoid or distorted shape, except for very early stage of development (<

~20 cells) (50, 51).

From the DF curves of the mouse embryos, a spherical aggregate was generated

in the compaction stage, whereas a cavity-bearing structure was in the blastocyst stage

(Fig. 10B); these morphologies are consistent with the *in vivo* situations. To examine

whether the DEB contribute to the formation of a cavity, we artificially eliminated the

DEB from the DF curves, and performed a simulation. We found that no cavity was

generated but an aggregate was formed (Fig. 10B, "DF curve w/o DEB").

From the DF curve of the MDCK cysts, a cavity-bearing structure was generated

(Fig. 10C), and artificial elimination of the DEB led to generation of a no-cavity structure

but an aggregate.

These results suggest that all of the DF curves from the various species and

various embryonic stages are capable of recapitulating their basic morphologies.

Robustness of simulation outcomes

As shown above, the ovoid/distorted shape or spherical shape were generated in a manner

dependent on DF curves. We examined whether our inference robustly results into the

same simulation outcomes. During the minimization of the cost function G, we sampled

DF curves before reaching the minimum of G. Fig. 10D shows the DF curves for the *C.*

elegans embryo t36-75 (left panel), and their values of G are plotted against the maximum

attractive force in the DF curves (right panel); the colors in the two panels correspond

each other. Before reaching the minimum (a red line in left panel and a red circle in the

right), the DF curves exhibited some differences in their profiles. Then, simulations were

performed from an initial configuration which shows a cuboid shape (bottom panel,

"start"). For all the DF curves tested, the particles were not spherically assembled but the

initial cuboid shape was almost sustained. By contrast, in the case of the mouse

compaction stage shown in Fig. 10E, the particles were spherically assembled for all the

DF curves except for an intermediate sample (light blue) which shows two isolated

aggregates. These results suggest that simulation outcomes resulting from our inference

are robust, and the DF curves are sufficient to explain morphologies among different

tissues.

Perturbation experiments for mouse compaction stage embryo

To evaluate the predictive capability of the DF curves inferred by our method,

we performed perturbation experiments. In the mouse compaction stage, the cells are

tightly assembled to form a spherical and symmetric embryonic shape. In other words,

we think that there are two morphological features, 1) increase in symmetry of the

embryos, and 2) smoothing of the embryonic surfaces. The embryos are surrounded by

external structures called zona pellucida which have negligible effects on morphogenesis

(52). Because both E-cadherin and actomyosin are essential for the compaction process

(47, 53, 54), we inhibited these proteins by chemicals: EDTA (ethylenediaminetetraacetic

acid) for E-cadherin, cytochalasin D for F-actin, and blebbistatin for non-muscle myosin

II (Fig. 11A).

The effective DP curves were inferred under these drugs (Fig. 11B). Then, we

quantitatively evaluated the differences among the DP curves and found that the distances

at the potential minima were increased under the three inhibitors (Fig. 11C, left panel).

Because the distances at the potential minima are related to the mean diameters of cells

(Fig. 1A-iv), this result predicted that the distances between adjacent cells were increased.

This prediction was supported through histological observations: each cell exhibited a

nearly spherical shape and seemed that the cells were not so densely assembled especially

under the condition of EDTA compared with the no-drugs condition (Fig. 11D). The

embryonic and cellular shapes are schematically depicted in Figure 11E. In addition, we

found another quantitative difference among the DP curves, related to decay of attractive

forces. We measured distances at 10% energy of potential minima as relative values to

the distances at the potential minima, and found that the relative distances were decreased

under EDTA and blebbistatin (Fig. 11C, right panel). This result means that attractive

forces of long-range interactions were reduced under these drugs.

Predictive capability of effective potential for mouse compaction stage embryo

586   Simulations under the DP curves from the drugs-treated embryos were

performed. The cell particles were spherically or almost spherically assembled under the

potentials of the normal embryos or the cytochalasin D-treated embryos, respectively (Fig.

12A). By contrast, the cell particles were not spherically assembled under the potentials

of the EDTA or blebbistatin-treated embryos. All simulation data are provided in Figure

S18A from which representative results are shown in Fig. 12A.

To relate the profiles of the DP curves to morphological changes in the

compaction process, we first introduced two indices for the morphologies as follows.

Sphericity $(=(36\pi V^2)^{1/3}/S)$ is essentially defined as the ratio of volume (V) to surface area

(S) so that the value becomes 1.0 for spheres. Shapes other than spheres show values less

than 1.0. Thus, both the increases in symmetry and in smoothness of surfaces contribute

to this index. Aspect ratio is defined as the ratio of the length of the longest axis to that of

the shortest axis in an ellipsoid which is fitted to an object of interest. The increase in

symmetry leads to that the aspect ratio becomes 1.0, and otherwise the aspect ratio shows

more than 1.0. The sphericities of all simulation results in Figure 12A and S18A were

measured, and we found that the sphericities were decreased under EDTA and blebbistatin

(Fig. 12B, left panel). Similarly, the aspect ratios were increased under EDTA and

blebbistatin (Fig. 12C, left panel).

We searched for parameters which can describe the sphericities or aspect ratios.

Among several parameters tested, the distances at potential minima measured in Figure

11C showed a tight relationship to the sphericities (Fig. 12B, right panel). The sphericities

showed an abrupt change along the x-axis. These results indicate that the sphericity is the

order parameter for the morphological transition of the compaction process and that the

distance at the potential minimum is the control parameter. On the other hand, the relative

distances at 10% potential minima showed a clear relationship to the aspect ratios (Fig.

12C, right panel). Thus, the morphological transitions of the compaction process are

induced by the quantitative changes in the DP curves.

Modeling of distance–force curves

To comprehensively understand the effect of the differences of the DF curves

on morphogenesis, we modeled the DF curves as a simple mathematical equation. To

analyze the contribution of DEBs, we selected the following equation (Fig. 13A):

618             $$F(D) = \varepsilon(D - D_0)^{-N} \cos\left\{ \frac{2\pi(D - D_0)}{\delta} \right\}, \text{ for } D > D_0 \qquad \text{(Eq. 4)}$$

Here, F is the force, D is the distance, and δ affects the wavelength of the cosine function

by which DEB is also introduced (Fig. 13A, left panel, red). D_0 can transform the DF

curves along D, and thus, the relative positions of DEBs to the mean diameters are

changed (Fig. 13A, D_3 in red vs. blue). N is the exponent of D, affecting the decay of the

DF curves along D (X-axis), and thus, the strengths of DEBs are changed (Fig. 13A, right

panel). All parameters and variables related to lengths/distances were normalized by $(\delta/4)$,

leading to generation of dimensionless parameters and variables such as $D_0^* = D_0/(\delta/4)$.

This enabled us to present simulation outcomes in two-dimensional space (D_0^* and N) in

a manner similar to a phase diagram (Fig. 13B) as explained in the next section.

Appropriate position and strength of DEB are essential for cavity-bearing structures

First, we examined what kind of DF curves can maintain a cavity-bearing

structures. A cavity-bearing structure was set as the initial configuration (Fig. 13B, "Initial

configuration"), and simulations were performed until the systems reached steady states

including metastable states. Fig. 13B shows a phase diagram with representative images

of the simulations, on which the regions of cavity-bearing structures were identified

("cavity" and "cavity with extra particles"). The "cavity" category absolutely depended

on the DEBs, because DF curves whose DEBs were eliminated did not form the "cavity"

as shown in Fig. 13C. In Fig. 13B, the "cavity" category was located around smaller N

values, otherwise aggregates were formed, suggesting that the strengths of the DEBs were

effective. Furthermore, larger D_0 values were required for the "cavity" category,

otherwise multiple clusters were formed, suggesting that the relative positions of DEBs

should be close to the mean diameters. Under a different number of particles, a similar

trend was observed (Fig. S21). In addition, we found cups and tubes adjacent to the

"cavity" in Fig. 13B but not in Fig. 13C, indicating that the DEBs also contribute to the

formation of these structures. The maintenance of tubes was confirmed to be dependent

on DEBs (Fig. S22). Therefore, in real tissues with tubes or cups, inferred effective

potentials may harbor DEBs.

Profiles of distance–force curves for describing 2D sheet, spherical/non-spherical

aggregates

To further investigate the capability of DF curve, we next applied a two-

dimensional (2D) sheet as the initial configuration which corresponds to a monolayered

cell sheet (Fig. 14A, "Initial configuration"). Fig. 14A shows a phase diagram with

representative simulation images. The 2D sheets were maintained ("sheet"), which was

largely dependent on the presence of DEBs (Fig. 14A, w/ DEBs vs. 14B, w/o DEBs). We

confirmed that the 2D sheets were not broken by slight positional fluctuations (Movie S4),

indicating that the structures were stable. The region of the 2D sheets was located around

larger values of D_0, which was a similar trend to the case of the cavity in Fig. 13.

In Fig. 14, both spherical and non-spherical aggregates were generated w/ and

w/o DEBs, and smaller values of N and/or D_0 led to the spherical ones. Under smaller

values of D_0, because the width (W_1) of the attractive force regions in DF curves became

relatively longer to the mean diameter (D_1), the resultant increased attractive forces may

cause the spherical aggregates. Under smaller values of N, the potential energies (P_1)

derived from the attractive forces are increased, possibly leading to the spherical

aggregates. Unexpectedly, the cavity-bearing structures were newly generated even in the

absence of the DEBs (Fig. 14B) in contrast to Fig. 13.

Discussion

In this study, we developed a top-down method for statistically inferring

effective potentials of cell–cell interactions using cell tracking data. We then

demonstrated that effective potentials are detectable as a function of cell–cell distances

with close relations to microscopic features such as cell surface tensions in epithelial cells

and blastomeres. Our findings provide for the first time the experimental quantification

of effective potentials, which have been recognized conceptually (6, 7). Simultaneously,

our findings provide a rationale that particle models with effective potentials can be a

good approximated model for various cells, which will enable us to expand the

applicability of particle models to larger organs. Furthermore, effective potentials with

qualitative and quantitative differences in their profiles were capable of describing

various morphogenesis such as the compaction process in the mouse embryos, cavitations,

formation of spherical/non-spherical aggregates, etc., suggesting that effective potentials

are powerful to explain the emergent properties of multicellular systems.

Effective potentials as measures of mechanical property

We showed that cell–cell adhesive force, cell surface tensions, and cell growth

are reflected into effective potentials (summarized in Table 1). Moreover, inhibitions of

gene function modified effective potentials (Fig. 11, S3, and S9). These facts suggest that

effective potentials can be a measure for evaluating mechanical properties of systems

including mutants in a non-invasive manner.

Influence of external factors on effective potentials

External factors exhibited influences on effective potential in different ways as

summarized in Table 1. Moreover, expanding cavities were approximately reflected into

effective potentials as DEBs, whereas higher self-migratory activities spoiled inference

results. Possibly, if we could subtract the movements derived from the self-migratory

activities by using the traction force microscopy (42, 55), we would correctly infer

effective potentials. Simulations considering DEBs unexpectedly formed cups, tubes, and

2D sheets as well as cavities. These structures are often observed during embryogenesis,

morphogenesis, and organoids prior to the formation of complex tissue structures: cavity-

bearing structures in early embryos of various species, organoids, and cystic diseases (49,

56–59), cell sheets in epithelia and germ layers (41, 60–62), tubes in tubular organs (63,

64), cups in retina (i.e. optic cup) and murine epiblast (65, 66). Our goal is to develop a

framework for explaining diverse morphogenesis in a minimal model. Approximations of

some external factors as effective potentials of cell–cell interaction serve to reduce

degrees of freedom.

Comparison of other inference methods with other models

To understand morphogenetic events, mechanical states and simulations based

on those states are essential. Models such as vertex, Cellular Potts, and phase field models

are often utilized, especially for epithelial cells (3, 56, 67–69). These models successfully

recapitulated various morphogenetic events, including the formation of the mouse

blastocyst (67) and very early embryogenesis in *C.elegans* (70). However, it is still

challenging to measure cellular and non-cellular parameters in three-dimensional systems

with high spatiotemporal resolution, although high-resolution inferences of parameters

such as cell–cell junction tensions and stresses have been performed in two-dimensional

situations by fitting a vertex model to experimental observations (71, 72). In addition,

because the assumptions of the vertex model are based on epithelial cells, its application

to other cells is limited including blastomeres and mesenchymal cells. On the other hand,

particle models are mainly used for cell aggregates and self-propelled cells (10, 12), while

some papers applied particle models to epithelial cells (11, 14, 61, 73), meaning that the

applicability of particle models is expanding. Due to its simplicity of particle models (i.e.

low degrees of freedom), our method can provide a framework for quantitatively

connecting model parameters to *in vivo* parameters under three-dimensional situations.

Materials and methods

Details of experimental procedures, mathematical modeling, and statistical methods are

described in Supplementary information.

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927   Figures

Figure 1: Overview of strategy for inferring the effective potential of cell–cell interactions

A. Relationship between microscopic forces and attractive/repulsive forces in isolated

two cell systems. i) Microscopic forces contributing to cell–cell interactions are

exemplified. ii) The microscopic forces are approximated as attractive/repulsive forces

where cells are described as particles with the mean size. iii) Both the repulsive and

attractive forces are provided as cell–cell distance-dependent functions, and the

summation (black broken line) is the distance–force curve of the two particles. The

relationship between the curve and the mean diameters of the cells is shown. iv) A

distance–potential curve is shown where the mean diameters of cells correspond to the

distance at the potential minimum.

B. Approximation of cell–cell interaction forces in multicellular systems. i) Mechanical

parameters are exemplified. ii) The question in this study. iii) Approximation of particle–

particle interactions in molecular sciences.

C. Strategy for inferring effective forces of cell–cell interactions. i) Particle model. A blue

sphere corresponds to a cell. Attractive or repulsive force between the particles (blue

spheres #1–4), was considered; vectors of cell–cell interaction forces (F_i) are illustrated

by black arrows in the case of particle #3. The net force ($F_{\mathrm{C}|p}$) of particle #3 is shown by

a red vector. The summation of F_i results in $F_{\mathrm{C}|p}$ which determines the velocity ($V_{\mathrm{C}|p}$) of

pth particle. ii) Nuclear tracking data were obtained and used as a reference data during

the inference. iii) Effective forces of cell–cell interactions were inferred by fitting. Red

line, attractive; blue line, repulsive. iv) From the inferred effective forces, we examined

whether distance–force curves are detected.

Related figure: Figure S1 (inference method).

Figure 2: Validation of inference method using simulation data

Simulations were performed on the basis of a distance–force (DF) curve obtained from

the Lenard-Jones potential (LJ). The DF curve is shown in A-i. The simulation conditions

contain "Assembling process" (A), "Steady state" (B), and "Cell proliferation" (C). For

A-C, snapshots of the simulations are shown where the particles are of the mean size of

cells (i). In A-ii, the procedure of data analyses is exemplified where effective forces of

interactions for each pair of cells for each time frame were plotted against the distance of

the cell–cell interactions, and shown as a colored heat map representing the frequencies

of the data points (Frequency index (FI)). Averaged values of the forces are shown in

yellow (binned average). In A-iii, B-ii, and C-ii, the resultant effective DF curves are

shown with the DF curves from the LJ potential.

Related figures: Figure S2 (in the case of other given potential and random walk).

A Vertex model: a standard epithelial model

Model

$$\lambda_{Tot} = 2\lambda_S - \lambda_{AD} + \sigma$$
Cell-cell adhesion

$$\lambda_{Tot} = \lambda_S + \sigma$$
Cell surface tension

K_a
Area elasticity

σ: fluctuation of tension

Simulation

$\lambda_S = 0.5$
$\lambda_{AD} = 0.8$
$K_a = 1.0$

Fluctuation of tension,
$\sigma = 0$ % of λ_{Tot}

t = 150 min   t = 450

B Fluctuation of tension

i. Plot & binned average of inferred effective force

ii. Inferred effective distance-force curve

Fluctuation of tension, σ (% of λ_{Tot})
— 0
— 20
— 50
— 100

C

Cell-cell adhesion force

i. Simulation

cell-cell adhesion force, λ_{AD} [A.U.]
0.9   0.0

Thick lines:
elevated tension due to fluctuation

ii. Inferred effective distance-force curve

cell-cell adhesion force, λ_{AD} [A.U.]
— 0.9
— 0.8
— 0.5
— 0.2
— 0.0

iii. Quantitative comparisons

Mean ± SD, N = 4 simulations

D Cell surface tension

i. Inferred effective distance-force curve

cell surface tension, λ_S [A.U.]
— 0.45
— 0.5
— 0.6
— 0.8
— 1.0

ii. Quantitative comparisons

Mean ± SD, N = 4 simulations

E Area elasticity

i. Inferred effective distance-force curve

area elasticity, K_a [A.U.]
— 0.5
— 1.0
— 2.0
— 5.0
— 10.0

ii. Quantitative comparisons

Mean ± SD, N = 4 simulations

Figure 3: Inference of effective forces of cell–cell interaction in epithelial cell model

A. Vertex model. λ_{Tot} is the line tension exerted on cell–cell junctions or on cell edges of

outer boundary. The potential energy on a junction or edge is $\lambda_{\text{Tot}} L^{<k,l>}$, where L is the

length of the junction or edge composed of kth and lth vertices. The potential energy for

a cell provided by the area elasticity is $(1/2)K_{\text{a}}\left(a_n/a_{\text{o}}-1\right)^2 a_{\text{o}}$, where a_n is the area of

nth cell and a_{o} is the natural area. An example of simulations is shown with the parameter

values in the right panel.

B. Inferred effective distance–force (DF) curves under various values of the fluctuations

of tension, σ. i) The inferred forces are plotted against cell–cell distances, and binned

averages are show. ii) Inferred DF curves.

C. Inferred DF curves under various values of cell–cell adhesive forces, λ_{AD}. i) Simulation

outcomes are shown where the cell cluster tends to form a circular colony under increased

values of the adhesive forces ($\lambda_{\text{AD}} = 0.9$). ii) Inferred DF curves. iii) Quantitative

comparisons of the DF curves.

D. Inferred DF curves under various values of cell surface tensions, λ_{S}. i) Inferred DF

curves. ii) Quantitative comparisons of the DF curves.

E. Inferred DF curves under various values of area elasticities, K_{a}. i) Inferred DF curves.

ii) Quantitative comparisons of the DF curves.

Figure 4: Inference of effective forces of cell–cell interaction in growing cells

i) Model of cell growth. Orange, a cell; green, particle. The growth force between the two

particles is provided as a repulsive force as follows: $B/(D+C)^2$, $C = 5.6$. $D_{CR} = 5.0$. ii)

Examples of simulations under different values of B, where the particles but not the cells

are visualized. iii) Inferred DF curves. iv) Quantitative comparisons of the DF curves.

External factors: extracellular-matrix (ECM)

A Cell-ECM adhesion energy

B traction force of random direction between cell-ECM

Figure 5: Influence of extracellular-matrix to effective forces of cell–cell interaction

A. Cell–ECM adhesion energy is assumed in the vertex model used in Fig. 3. i) The

energy for a cell is defined as $-E_{ECM}a_n$, where E_{ECM} is the coefficient of the energy. ii)

Simulation outcomes are exemplified where the cell areas are increased under larger value

of E_{ECM}. The left and right panels are shown with the same scale. iii) Inferred DF curves.

iv) Quantitative comparisons of the DF curves.

B. Traction forces between cells and ECM are assumed in the particle model used in Fig.

2 except that the simulations were two-dimensionally performed. i) Cell–cell interaction

forces are provided by the LJ potential. The directions of the traction forces are random.

ii) An example of simulations is shown. iii and iv) Inferred DF curves under various

values of the traction forces and under various values of the persistency, respectively.

Related Figures: Figure S3 (inference in MDCK cells on substrates) and S4 (inference in

migratory cells with a uniform direction) show a similar effect of migratory activities on

DF curves to that in B.

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External factors under 3-dimensional situations

A Egg shell-like spatial constraints: cylinder
i. Simulation
t = 210 min
t = 510
length of cylinder = 25 μm
radius of cylinder = fixed (7.5 μm)

ii. Inferred effective distance-force curve
- - - LJ (given)
length of cylinder (μm)
(compressive)

iii. Illustration of radial distribution function
non-compressive
compressive
maximum of probability ≒ minimum of potential

B Expanding cavity w/ cell-cell interactions
i. Simulation
radius of cavity = 9.6 -> 12.6 μm
t = 210 min
t = 510

ii. Inferred effective distance-force curve
DEB
- - - LJ (given)
8.6->10.1
9.6->12.6
9.7->14.2
radius of cavity (μm)

C Expanding cavity w/o cell-cell interactions (i.e. LJ is not given)
i. Simulation
t = 210 min
t = 510

ii. Inferred effective distance-force curve
- - - LJ (not given)
8.6->10.1
9.6->12.6
9.7->14.2
radius of cavity (μm)

D Expanding cavity; cell-cell interaction forces are solely extracted
i. Plot & binned average
From B   From C
narrow distribution of data points

ii. Inferred effective distance-force curve
- - - LJ (given)
8.6->10.1
9.6->12.6
9.7->14.2
radius of cavity (μm)

E Relationship among B,C,D
Pressure from cavity
LJ
cavity
cell
cell
B (LJ + pressure)

C (net force from DEB)
net force from DEBs
DEB
if ~uniform distribution of cells

B - C = D
if pressure from cavity ≒ net force from DEBs, → D = LJ
LJ

Figure 6: Influence of external constraints to effective forces of cell–cell interaction

A. Cylindrical constraints corresponding to egg shells are assumed in the particle model used in Fig. 2. i) An example of simulations with labeling three cells (red, yellow, and green). ii) Inferred DF curves. For the condition of the cylindrical length = 16μm, a snapshot of the simulation is shown ("compressive"). iii) Effect of compression on the

radial distribution function is described. The functions under the compressive and non-

compressive conditions are illustrated (purple and green lines). The maxima of the

functions are expected to the minima of the effective potentials of cell–cell interactions.

The numbers of the particles are the same among the different cylindrical constraints.

B. Expanding cavities are assumed in the particle model. i) An example of simulations

with the change in the radius of the cavity. ii) Inferred DF curves with the DEBs. The

numbers of the particles are the same among the different cavities.

C. Expanding cavities are assumed whereas cell–cell interaction forces are not introduced.

i) An example of simulations. ii) Inferred DF curves.

D. Reconstruction of cell–cell interaction forces under expanding cavities. i) All the data

points in B and C under the radius of the cavity = 9.7 -> 14.2μm are plotted on distance–

force graph with the binned averages. ii) DF curves obtained by subtracting the DF curves

in C from those in B: i.e. B – C as exemplified in D-i.

E. The subtraction performed in D is schematically explained in the relationship among

B, C, and D.

Related Figures: Figure S5 (inference under spherical constraints) and S6 (inference in

cylindrical constraints) show a similar effect of spatial constraints on DF curves to that in

A. Figure S7 (inference under non-expanding cavities) shows almost no modification of

DF curves.

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Figure 7: Inference of effective force of cell–cell interaction in *C.elegans* embryos

A. Snapshot of the nuclear positions in the *C.elegans* embryo with cell lineages at time

frame = 76 in the left panel. Snapshots with inferred effective forces with the force values

described coloed lines in right three panels at *t* = 16, 76, and 195. Forces are depicted in

arbitrary units (A.U.); 1 A.U. of the force can move a particle at 1μm/min. The nuclear

tracking data were obtained from a previous report (30).

B. Mean diameters of cells at each time frame estimated from cell numbers. Given that

the volume of the embryos is constant (= *Vol*) during embryogenesis, the mean diameters

were estimated from the cell numbers (N_c) at each time frame as follows: mean diameter

$= \{Vol / (4/3 \ \pi \ N_c)\}^{1/3}$. The diameters relative to that at time frame = 16 are shown with

cell numbers. The sizes of the circles reflect the diameters, whose colors roughly

correspond to the colors in the graph in E.

C. Uniqueness of solution of effective force inference was examined. The minimizations

of the cost function G were performed from different initial force values as described in

the x- and y- axes, and the inferred values of each cell-cell interaction were plotted by

crosses.

D. The inferred effective forces of cell–cell interactions were plotted against the distance

of cell–cell interactions with binned averages at $t = 76$-115.

E. Inferred DF and DP curves at various time frames.

F. DP curves normalized by the distances at the potential minima at various time frames.

Related figure: Figure S8 (uniqueness of solution was examined).

Related movies: Movie S1A (tracking data) and S1B (force map).

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Figure 8: Inference of the effective force of cell–cell interaction in mouse pre-implantation embryos

A. Eight-cell, compaction, and blastocyst stages of mouse embryo are illustrated, and their confocal microscopic images are shown: bright field, maximum intensity projection (MIP) and cross-section of fluorescence of H2B-EGFP. Snapshots of nuclear tracking are also shown; blue spheres indicate the detected nuclei. In the nuclear tracking image of the blastocyst, ICM cells are located around the bottom region of the image, as indicated by *. Scale bars = 15μm.

B and C. Inferred DF and DP curves with the DEBs.

Related figures: Figure S9 (inference in cavitation-inhibited embryos), S10 (data from other embryos), and S11 (DF and DP curves in ICM and TE cells, and the outer and inner cells in the compaction stage).

1086 Related movies: Movie S2A-C (tracking data) and Movie S2D-F (force maps)

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Illustration | Bright field | Histone-EGFP(nuclei)
cavity | | MIP | Cross-section

dish

B effective distance-force (DF) curve

C effective distance-potential (DP) curve

Figure 9: Inference of effective force of cell–cell interaction in cysts formed by MDCK cells

A. MDCK cysts formed under suspension conditions are illustrated, and confocal microscopic images are shown: bright field, maximum intensity projection (MIP) and cross-section of fluorescence of H2B-EGFP. Scale bars = 10µm.

1099 B and C. Inferred DF and DP curves. In C, an enlarged view is also provided. A DEB is

1100 indicated.

1101 Related figures: Figure S12 (all DP curves in other cysts show DEBs.).

1102 Related movies: Movie S3A (tracking data) and Movie S3B (force maps)

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Figure 10: Outcomes of simulations based on inferred distance–force curves

A-C. Simulations results under the DF curves derived from *C. elegans* and mouse

embryos, and the MDCK cyst are exemplified. In B and C, cross-sections are also shown.

In the case of the mouse blastocyst, two parallel cross-sections (shown in blue and green)

are merged.

D and E. DF curves sampled before reaching the minima of *G*, and simulation outcomes.

DF curves, left panels; the values of *G* and the maximum attractive forces in the DF curves,

right panels; simulation outcomes for each DF curve with the initial configuration

("start"), bottom panels. The values of *G* are relative to that in the case of all forces = 0.

The colors in each three panels in D and E correspond each other. In the right panels, the

numbers of the data points are 14 and 12 in D and E, respectively, and the representative

ones (colored circles) are selected for presenting the DF curves and the simulation

outcomes.

Related figure: Figure S13 (other simulation results with initial configurations showed

equivalent results in Fig. 10A-C).

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Figure 11: Inference of effective potentials of cell–cell interaction in compaction-

inhibited mouse embryos

A. Microscopic images of embryos under chemicals. CytoD, cytochalasin D; Bleb,

blebbistatin.

B. Inferred DP curves in the drug-treated embryos. N=6~10 for each condition.

C. Quantitative differences in the DP curves. Distances at the potential minima in the DP

curves, left panel; Distances providing 10% energy of the potential minima as the relative

value to the distances at the potential minima, right panel. Mann–Whitney–Wilcoxon tests

were performed and the resultant p-values for "No Drugs" vs. "EDTA", vs. "CytoD", and

vs. "Bleb" are 0.011, 0.23, and 0.00040, respectively, in the left panel. In the right panel,

distances providing other % energies instead of 10% are shown in Fig. S16B.

D. Confocal microscopic images of cell shapes. Cell shapes were visualized by staining

F-actin or E-cadherin. E. The embryonic and cellular shapes illustrated based on D.

Related figures: Figure S14 (experimental design), S15 (enlarged view of DP curves),

S16 (details of quantification of DP curves), and S17 (histological images of other

embryos).

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Figure 12: Simulations under inferred distance–potential curves in drug-treated embryos, and identification of parameters explaining morphological transition

A. Simulation results for the drug-treated embryos. All simulation data are provided in Figure S18, and the representative results which nearly showed the mean values of the sphericities for each condition are chosen here.

B. Sphericities in the simulations of the drug-treated embryos (left panel), and the sphericities plotted against the distances at the potential minima calculated in Figure 11C. Mann–Whitney–Wilcoxon tests were performed: *p*-values for "No Drugs" vs. "EDTA", vs. "CytoD", and vs. "Bleb" are 0.011, 1.0, and 0.00080, respectively.

C. Aspect ratios in simulations of the drug-treated embryos (left panel), and the aspect ratios plotted against the relative distances providing 10% energy of the potential minima calculated in Figure 11C. Mann–Whitney–Wilcoxon tests were performed: *p*-values for "No Drugs" vs. "EDTA", vs. "CytoD", and vs. "Bleb" are 0.21, 0.97, and 0.33,

1160   respectively.

1161   Related figures: Figure S18 (all simulation outcomes), S19 (sphericities and aspect ratios

1162   from a different initial configuration), and S20 (Relationships of sphericities or aspect

1163   ratios to other tested parameters).

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Figure 13: Modeling of distance–force curves and diagrams of simulation outcomes;

cavity-bearing structures

A. Modeling of DF curves using four parameters: N, D_0, δ, and ε. A DF curve without the

cosine term is always >0 (repulsive) ($F = \varepsilon D^{-N}$, green broken line). Upon introduction of

the cosine (purple broken line), the curves acquire regions with <0 (attractive) and a DEB

(red line). Upon introduction of D_0, the curves are translated along the distance (blue line).

As shown in the blue line, the DEB ranges from $3\delta/4+D_0$ to $5\delta/4+D_0$ (D_2). N affects the

gradient of the curves and the height of DEBs (right panel). DF curves from $D = 0$ to D

at the end of DEBs (w/ DEB) or the curves from $D = 0$ to D before starting DEB (w/o

DEB) were used in the following simulations.

B. Outcomes of simulations under various values of N and D^*. Some conditions on the

diagram were designated by symbols (circle, square, and triangle), and their simulation

results are visualized (blue spheres) with the profiles of the DF curves. Cross-sections are

visualized for some simulation results. The diameters of the blue spheres are equivalent

to the mean diameter. For "cup" [orange rings, mouth of the cup; white dots, particles

located on the ring; crosses, the particles located neither on the ring nor at the center of

the ring]. For "tube" [orange crosses, open ends of the tube]. For "cavity with extra

particles" [arrows, extra particles where multiple- but not single-layered]. D_1, mean

diameter; D_2, distance of DEBs. The definition of each phase is explained in SI (section

7-2). Gray crosses, data points for depicting the lines separating each phase.

C. Simulation outcomes without DEBs.

Related figure: Figure S21 (phase diagrams under a different number of particles), S22

(maintenance of tubes was examined under DF curves with DEBs).

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Figure 14: Diagrams of simulation outcomes; 2D sheets, spherical/non-spherical

aggregates

A. Outcomes of simulations starting from a two-dimensional (2D) sheet with slight

positional fluctuations. The results are shown in a similar manner to Fig. 13B, except that

the diameters of the blue spheres are equivalent to $0.4\times$ the mean diameter. D_1, mean

diameter; W_1, width of attractive force regions; P_1, potential energy derived from

attractive forces.

B. Simulation outcomes without DEBs.

Related movie: Movie S4 (2D sheets were stably maintained under fluctuations).

Table: effect of cellular and external factors on effective force of cell-cell interaction

	Effect on force (attractive or repulsive)	Effect on distance at maximum attractive force	Others	Figures
Cellular factors				
cell-cell adhesion	attractive	N.C.		3C
cell surface tension	repulsive	N.C.		3D
area elasticity	neutral	N.C.	core stiffness increased?	3E
cell growth	repulsive	N.C.		4
External factors				
cell-ECM adhesion	repulsive	increased		5A
cell-ECM traction force				
i. random direction	neutral/repulsive	N.C.		5B
ii. uniform	neutral	N.C.		S4A
iii. leader cells	repulsive	N.C.		S4B
egg-shell	neutral	N.C.	shift of DF curve under compresssive condition (non-physiological)	6A,S5,S6
cavity				
i. expanding	repulsive	N.C.	DEB generated	6B
ii. non-expanding	neutral	N.C.		S7

N.C; not changed

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