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Dopaminergic Neurons Linking Threat Processing to

Cardiac Modulation and Locomotor Responses

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ABSTRACT

Heartbeat and behavior are tightly coordinated during defensive states, yet the neuronal

mechanisms linking threat processing to cardiac modulation—and the potential

contribution of cardiac dynamics to behavioral output—remain poorly understood. Here

we show in *Drosophila* that mechanical threat triggers locomotion together with cardiac

deceleration. We identify two dopaminergic neurons, termed DA-WED neurons, that

mediate this cardiac response: silencing these neurons markedly attenuates threat-

induced cardiac deceleration, whereas optogenetic activation induces cardiac

deceleration in the absence of threat. Calcium imaging further shows that DA-WED

neurons are activated by mechanical threat. Linking cardiac dynamics to behavior,

direct optogenetic manipulation of cardiomyocytes that quantitatively reproduces threat-

evoked cardiac deceleration is accompanied by increased locomotion. Together, these

results identify a dopaminergic descending pathway that links threat processing to

cardiac modulation and suggest that cardiac dynamics may contribute to shaping

defensive behavior.

INTRODUCTION

Heartbeat dynamics are tightly coordinated with behavioral state. Defensive states, for example, are accompanied by coordinated modulation of cardiac activity, including transient cardiac deceleration during threat detection and cardiac acceleration during active coping in mammals[1]. Such tight coordination between behavioral state and cardiac dynamics is likely advantageous for survival: cardiac deceleration may minimize the brain-wide representations of the heartbeat[2–5] to sharpen sensory processing[16], whereas cardiac acceleration boosts the delivery of metabolic resources to muscles[7]. Although much of the existing work on heart–behavior coupling has focused on mammals, comparable threat-associated cardiac modulation has also been reported in invertebrates. In decapod crustaceans, for instance, sensory stimuli elicit time-locked heart rate changes that parallel defensive behaviors, suggesting that coordinated heart–behavior responses are evolutionarily widespread[8,9]. Despite this well-documented coupling, the circuit mechanisms linking threat processing in the brain to cardiac modulation—and whether cardiac dynamics contribute to behavioral output—remain incompletely understood.

In mammals, heartbeat is governed by sympathetic and parasympathetic branches of the autonomic nervous system (ANS) that innervate the heart[7,10–17]. Sympathetic output that accelerates the heartbeat arises from brainstem and hypothalamic circuits and projects through spinal intermediates to the heart[7]. On the other hand, the parasympathetic nervous system, which decelerates the heartbeat[7,18], originates from the dorsal motor nucleus of the vagus nerve and nucleus ambiguus, and projects directly to the heart[18,19]. These autonomic pathways are engaged in threatened animals by the so-

called fear circuitry in the brain[20–22] to shape cardiac responses, typically producing

cardiac deceleration followed by acceleration[1,23–28]. Circuit-wise, the periaqueductal

gray (PAG) is considered the output hub of the fear circuitry and modulates the

heartbeat through the hypothalamus, midbrain, pons, and medulla oblongata[29]. In

addition, hypothalamic nuclei such as the dorsomedial hypothalamus (DMH)[30] and the

arcuate nucleus (ARC), as well as the anterior cingulate cortex (ACC)[31], also modulate

the heartbeat upon threats[32–38].

In parallel, ascending feedback from the heart to the brain has attracted increasing

attention. Such interoceptive signaling[39] is conveyed by sensory neurons innervating the

heart and aortic arch[39], which project to NTS and onward to hypothalamic and cortical

regions including paraventricular nucleus of the hypothalamus (PVN) [40], ACC, insular,

and prefrontal cortex[40]. These pathways have been implicated in learned fear[41], anxiety-

like behavior[42] or sleep[43]. Together, these findings suggest that bidirectional

communication between brain and heart may shape physiological and behavioral

responses during defensive states. However, how central circuits orchestrate threat-

associated cardiac modulation, and whether cardiac dynamics influence defensive

behavior, remain unresolved.

The fruit fly *Drosophila melanogaster* provides a genetically tractable system to

dissect brain–body interactions. The *Drosophila* heart, an evolutionarily conserved

organ[44–47], consists of two rows of cardiomyocytes forming a tubular structure that runs

through the midline of the abdomen[48,49]. Like mammalian heart, *Drosophila* heart

receives rich neuronal projections throughout[50,51]. Recent work has shown that visual

threat induces cardiac deceleration in *Drosophila*[52], suggesting the existence of the

neuronal mechanism in the brain that modulates the heart. However, the neuronal

substrate of such a mechanism, and the behavioral consequences of cardiac modulation

during threat, remain largely unknown.

We have recently reported that a train of air puffs elicit hyperactivity, avoidance of

puffs, and aversion from an otherwise neutral visual object, suggesting that air puffs

serve as mechanical threat[53]. Building on this work, we established an experimental

paradigm to assess how mechanical threat modulates heartbeat and behavior. Using this

system, we identify two pairs of dopaminergic neurons in the brain, termed DA-WED

neurons, that are responsible for threat-induced cardiac deceleration. We further

examine how cardiac deceleration relates to threat-induced locomotion. Together, our

findings identify a pair of dopaminergic neurons that link threat processing in the brain

to cardiac modulation and suggest that cardiac dynamics may contribute to shaping

defensive behavior.

RESULTS

I. Air puffs induce cardiac deceleration and locomotion

We have previously reported that a train of air puffs serve as mechanical threats, eliciting a host of fear-like behaviors such as hyperactivity, avoidance of puffs, and aversion from an otherwise neutral visual object[53]. This motivated us to test how the air puff might influence heartbeat, and its relation to behavior. For this purpose, we developed a paradigm to monitor heartbeat and behavior simultaneously (Fig. 1a). Our paradigm images the heart chamber closest to the thorax, called conical chamber, which is visualized through the dorsal cuticle by cuticle-penetrating infare-red light (Fig. 1a, "CAM1"). Simultaneously, the fly's behavior is recorded from the side of the fly (Fig. 1a, "CAM2"). We further developed a set of software to automatically detect heartbeat and behavior (Supplementary Movie 1). Our heartbeat detection software takes two consecutive frames and calculates for each pixel the optical flow, which are used to quantify the overall relaxation (diastole) or shrinkage (systole) of the heart (Supplementary Fig. 1a-c). Based on such quantification, our software detects the timings at which the heart was shrunk most (systole peak), which were counted to obtain the heart rate (HR). Our analysis pipeline for behavior detection first tracks the coordinate of body parts (joints of each leg, eye, neck, haltere, rostral tip of the abdomen, all on the right side of the fly), utilizing SLEAP software[54]. The tracked coordinates are then fed into our custom support vector machine-based program to detect locomotion. Our analysis pipeline allowed us to visualize the HR and locomotion over time in a synchronized fashion.

Using our paradigm, we tested how the air puff might influence the HR and

locomotion. Specifically, we applied for each fly a 0.5 s air puff (either 20 mL/min, 50

mL/min, 200 mL/min). We repeated 10 trials for each fly with an inter-puff interval of

90s (Fig. 1b). The results of 10 trials were averaged, as we did not observe noticeable

trial effects (Supplementary Fig. 2a, c). We found that the air puff transiently decreased

the HR (Fig. 1c-e; Supplementary Fig. 2a, b; Supplementary Movie 1). Similar

tendency was observed but was statistically insignificant for the strongest puff (200

mL/min), which is likely due to the following cardiac acceleration (Fig. 1d, e). Surgical

removal of body parts and silencing experiments of external sensilla or chordotonal

organ[55,56] suggest that hair plate neurons and chordotonal organs are at least partially

indispensable for puff-induced cardiac deceleration (Supplementary Fig. 3). We also

found that the air puff persistently increased the fraction of time walking, in line with

previous reports (Fig. 1f, g; Supplementary Fig. 2c, d)[53,57]. Thus, our data revealed that

the air puff induces cardiac deceleration and locomotion. Notably, in our paradigm the

air puff robustly induces locomotion and does not elicit sustained freezing, indicating

that the observed cardiac deceleration cannot be attributed to freezing-associated

bradycardia described in visually induced threat paradigms in flies[52] or in other contexts

in rodents[1]. This prompted us to next identify neurons responsible for cardiac

deceleration.

II. Dopaminergic system is responsible for puff-induced cardiac deceleration

To aid in identifying neurons responsible for cardiac deceleration, we developed yet

another paradigm to quantify the HR with higher throughput. In this paradigm, we

drove the expression of GFP in the cardiomyocytes using the enhancer of the Hand

gene[45], to aid in heartbeat imaging (Fig. 2a, b). GFP signals in pericardiocytes (also

known as nephrocytes) are likely due to their function to incorporate any molecules in

the hemolymph[58]. The fly's ventral side of the thorax and abdomen were glued to a

slide glass, and the GFP signals in the conical chamber were acquired through the intact

dorsal cuticle by confocal microscopy (Fig. 2a, b). The air puffs of 20 mL/min were

applied frontally to the fly's head through a glass pipette (Fig. 2a). Heartbeat was

detected using our custom software (Supplementary Fig. 4a-c). A single trial consisted

of 60 s of interval, 10 s of air puffs, and 60 s of recording, which was repeated twice for

each fly with 90s interval (Fig. 2c). This experiment revealed that air puffs induce

cardiac deceleration by roughly 10% (Fig. 2d-f; Supplementary Movie 2), consistent

with our earlier finding (Fig. 1). Similar results were obtained when the air puff was

applied for 1s (Supplementary Fig. 4d, e), 20s (Supplementary Fig. 4f, g), and in both

sexes (Supplementary Fig. 4h, i).

Monoaminergic systems have repeatedly been implicated in HR regulation across

species, including Drosophila[59–68]. We thus wondered whether monoaminergic systems

might be involved in puff-induced cardiac deceleration. When we silenced with TNT

the neurons expressing either serotonin, octopamine (insect equivalent of

norepinephrine), and dopamine, we found that silencing of octopaminergic or

dopaminergic neurons significantly suppressed puff-induced cardiac deceleration (Fig.

2g, h; Supplementary Fig. 5a, b). Note, however, that when we expressed in

serotonergic neurons the inward-rectifying potassium channel Kir2.1, it did decrease the

puff-induced cardiac deceleration (Supplementary Fig. 5c, d), suggesting that

serotonergic neurons may also be indispensable for puff-induced cardiac deceleration.

In line with this, a *loss-of-function* mutation of a serotonin synthetic enzyme *TrH* also

showed decrease in the puff-induced cardiac deceleration (Supplementary Fig. 5e-g).

To further probe the roles of monoaminergic neurons, we next tested whether

thermogenetic activation of these neurons can induce cardiac deceleration without air

puffs. To this end, we expressed a heat-gated cation channel dTrpA1 in monoaminergic

neurons, and shifted the temperature from 21℃ to 28℃ while monitoring the HR (Fig.

2i). This revealed that, while the HR of cold-blooded Drosophila increased as a function

the temperature even in the driver-less control (Fig. 2j, black), such cardiac acceleration

was suppressed by activation of dopaminergic neurons (Fig. 2j, blue) but not by

octopaminergic neurons (Fig. 2j, gray). On the other hand, activation of serotonergic

neurons exaggerated the heat-induced cardiac acceleration (Fig. 2j, red). The average

HR during 28℃ period indeed revealed that the activation of dopaminergic neurons

significantly decreased the HR compared to the driver-less control, while the activation

of serotonergic neurons significantly increased the HR (Fig. 2k). Dopaminergic neurons

were the only monoaminergic population whose silencing and activation consistently

implicated them in driving cardiac deceleration (Fig. 2g-k). The role of dopaminergic

neurons is further reinforced by loss-of-function experiments of dopamine receptors,

which revealed that mutations of *Dop1R2* or *Dop2R* significantly decrease the puff-

induced cardiac deceleration (Fig. 2l, m; Supplementary Fig. 5h, i). A mutation of

DopEcR also showed a tendency to decrease the puff-induced cardiac deceleration

albeit not quite reaching the statistical significance (Fig. 2l, m; Supplementary Fig. 5h,

i). Together, our data demonstrates that dopamine system is responsible for puff-

induced cardiac deceleration.

III. Two pairs of dopaminergic neurons in the brain, DA-WED neurons, are

indispensable for cardiac deceleration

There are approximately 130 dopaminergic neurons scattered throughout the Drosophila

brain[69,70]. To identify the subpopulation of dopaminergic neurons responsible for puff-

induced cardiac deceleration, we turned to a host of dopamine-related GAL4 driver

lines[69] (Fig. 3a). Each of these drivers carries different bits of enhancers of dopamine-

related genes, and presumably for this reason these drivers are known to label partially

overlapping but distinct subpopulations of dopaminergic neurons[69]. When we drove the

expression of TNT by these drivers, we found that neuronal silencing by 4 out of 10

drivers decreased puff-induced cardiac deceleration (R76F01-, R76F02-, R76F05-,

R60F07-GAL4; Fig. 3b, blue plots) without significantly influencing the baseline HR

(Supplementary Fig. 6a), suggesting that these drivers label the subset of dopaminergic

neurons indispensable for puff-induced cardiac deceleration. Identification of these "hit"

drivers allowed us to next employ a split-GAL4 approach to further narrow down the

indispensable neurons (Fig. 3c). In the split-GAL4 method, the whole GAL4 protein is

split into the DNA-binding domain ("DBD") and the activation domain ("AD"), each

fused with a leucine-zipper domain[71]. When these "hemi-drivers" collide, they bind to

each other through their respective leucine zipper, re-constituting the functional GAL4.

Thus, by placing each of these hemi-drivers under different enhancers, one can achieve

the expression of functional GAL4 only in cells in which both enhancers are active (Fig.

3c). When we tested all split combinations of the 4 "hit" enhancers, we found that only

one combination, namely R76F05-DBD and R60F07-AD, significantly decreased the

puff-induced cardiac deceleration (Fig. 3d), without significantly influencing the

baseline HR (Supplementary Fig. 6b). Our immunohistochemical analysis revealed that,

as reported by a previous report[69], the split combination of R76F05-DBD and R60F07-

AD labeled two different subpopulations of dopaminergic neurons: one subpopulation

from the PPL1 cluster named PPL1-SMPγ, and another subpopulation from the PPM2

cluster named DA-WED (Fig. 3e), with additional one or two neurons occasionally

labeled in some brains. We further sought to identify which of these two subpopulations

is indispensable for puff-induced cardiac deceleration. Taking advantage of the

recently-developed analysis pipeline that identify a list of candidate GAL4 drivers that

may label any neuron of interest[72,73], we obtained a list of candidate PPL1-SMPγ and

DA-WED drivers. By testing several split combinations of enhancers used in these

drivers, we could identify the split combinations that label one but not the other (Fig.

3f). We note that each of these combinations labels additional neurons, in either

subesophageal zone (Fig. 3f, left) or optic lobes (Fig. 3f, right). Using these split

drivers, we silenced either PPL1-SMPγ or DA-WED with TNT, and found that

silencing of DA-WED significantly decreased puff-induced cardiac deceleration (Fig.

3g; Supplementary Fig. 6c). Together, our data suggests that DA-WED neurons are

indispensable for puff-induced cardiac deceleration.

IV. DA-WED neurons are responsible for puff-induced cardiac deceleration

While our data so far suggests the role of DA-WED neurons in cardiac deceleration, the

split driver we used to label DA-WED also labeled neurons in the optic lobes (Fig. 3f;

right). We thus further improved the labeling specificity through intersection strategy.

In this strategy, the effector gene is expressed under the control of UAS sequence, but a

"stop" sequence is inserted in between UAS and GFP, blocking the function of GAL4.

Now, the expression of "molecular scissors" called flippase (FLP) is driven by a

Tyrosine hydroxylase (TH) promoter ("TH-FLP"), which excises out the stop sequence.

Hence, GAL4 can function only in cells in which TH promoter is active. This strategy,

combined with our split GAL4 combination, indeed achieved near-perfect specificity

for DA-WED neurons, apparently labeling no other cells throughout the body (Fig. 4a;

Supplementary Fig. 6d). When we silenced DA-WED neurons with Kir2.1, it decreased

puff-induced cardiac deceleration (Fig. 4b, c), without noticeably influencing the

baseline HR (Supplementary Fig. 6e).

We next tested if DA-WED neurons function through dopamine. Our dopamine

receptor mutant analysis (Fig. 2l, m) suggests that dopamine signaling through Dop1R2

and Dop2R is indispensable for cardiac deceleration. Consistent with this, we found that

RNAi of a dopamine synthesis enzyme ple in DA-WED neurons reduced puff-induced

cardiac deceleration (Supplementary Fig. 6f-h). It is thus plausible that DA released

from DA-WED neurons binds to Dop1R2 and/or Dop2R to drive cardiac deceleration.

DA-WED neurons have previously been reported to drive protein preference

behavior in protein-deprived flies[74,75]. Indeed, suppression of DA-WED neurons

decreased protein preference (Supplementary Fig. 7a-d)[74,75] in addition to cardiac

deceleration (Supplementary Fig. 7e, Fig.4b, c). This prompted us to ask whether these

neurons drive cardiac deceleration and protein preference through shared, or instead

distinct, mechanisms. Interestingly, *Dop2R* mutant flies failed to show cardiac

deceleration (Fig. 2l, m), but showed normal preference compared to the wildtype

(Supplementary Fig. 7f, g). Similarly, suppression of FB-LAL neurons, through which

DA-WED neurons drive protein preference[74,75], failed to influence cardiac deceleration

(Supplementary Fig. 7h, i). These results suggest that DA-WED neurons drive protein

preference through FB-LAL neurons, while driving cardiac deceleration through Dop2R

independent of FB-LAL. This hypothesis is further reinforced by our observations that

protein deprivation, which drives protein preference (Supplementary Fig. 7j), fails to

influence puff-induced cardiac deceleration (Supplementary Fig. 7k) nor the baseline

HR (Supplementary Fig. 7l). Together, our data suggests that DA-WED neurons drive

cardiac deceleration and protein preference through distinct mechanisms

(Supplementary Fig. 7m).

We next wondered how DA-WED neurons might respond to air puffs. To this end,

we expressed jGCaMP7s in DA-WED neurons, and imaged their calcium activities

while applying a train of air puffs (Fig. 4d). We found that the calcium level of DA-

WED neurons steadily increased as air puffs are applied (Fig. 4e, f; Supplementary Fig.

8a; Supplementary Movie 3). The increased jGCaMP7s signals returned to the baseline

in less than 5 s when puffs ceased (Fig. 4f). Given the slow kinetics of jGCaMP7s[76], the

increased activity of DA-WED neurons likely returns to the baseline immediately when

the puffs cease. While there are two pairs of DA-WED neurons in the brain, one pair

being more medial than the other, we found no noticeable difference in medial vs lateral

DA-WED neurons' activities in response to puffs (Supplementary Fig. 8b-d). Our data

suggests that all four DA-WED neurons transiently get activated by air puffs.

To test if increased activities of DA-WED neurons can replace the air puff to

induce cardiac deceleration, we photoactivated DA-WED neurons without puff

application (Fig. 4h). For this, we expressed a light-gated cation channel CsChrimson in

DA-WED neurons, and shined light on the fly's head to activate these neurons. We

found that the photoactivation of DA-WED neurons could induce cardiac deceleration

by ~10% in the retinal-fed test flies, but not in the retinal-unfed control flies (Fig. 4i, j;

Supplementary Movie 3).

Together, our data establishes that DA-WED neurons are responsible for puff-

induced cardiac deceleration (Fig. 4k).

V. Cardiac interoception possibly contributes to threat-induced locomotion

Cardiac interoception has recently been implicated in modulating behavioral responses

[41–43]. We therefore asked whether cardiac deceleration is associated with changes in

locomotion in *Drosophila*. To test this, we silenced DA-WED neurons using Kir2.1 to

block puff-induced cardiac deceleration, and assessed locomotor output. We found that

silencing DA-WED neurons markedly suppressed puff-induced locomotion compared

to controls (Fig. 5a, b). Conversely, photoactivation of DA-WED neurons using

CsChrimson promoted locomotion in the absence of puff (Fig. 5c, d). These findings

suggest that DA-WED neurons coordinate cardiac deceleration with locomotor

responses during threat.

An alternative interpretation is that DA-WED neurons function as general threat

detectors that broadly regulate puff-evoked behaviors. If this were the case,

manipulating these neurons should affect all of behavioral outputs induced by puff. In

addition to promoting locomotion, air puff suppressed grooming (Supplementary Fig.

9a, b). However, silencing DA-WED neurons failed to disrupt puff-induced grooming

suppression (Supplementary Fig. 9c, d), despite markedly reducing cardiac deceleration

(Fig. 4b, c) and locomotion (Fig. 5a, b). Likewise, photoactivation of DA-WED neurons

failed to suppress grooming (Supplementary Fig. 9e, f), while robustly inducing cardiac

deceleration (Fig. 4b, c) and locomotion (Fig. 5c, d). Thus, manipulation of DA-WED

neurons does not reproduce the full behavioral repertoire triggered by puff. These

findings argue against the idea that DA-WED neurons function as general threat

detectors and instead support a more specific role in coordinating cardiac and locomotor

responses.

To directly test whether cardiac deceleration can influence locomotion, we

optogenetically mimicked puff-induced cardiac deceleration by expressing the light-

gated anion channel GtACR1 in cardiomyocytes using Hand-GAL4 (Fig. 5e). We

selected an anion channel to prolong diastole, unlike a previous report using a cation

channel[77], as puff-induced cardiac deceleration is characterized by elongated diastolic

intervals (Fig. 1c). Brief green light pulses (28 ms; Fig. 5f) transiently arrested the heart

in diastole (Fig. 5g; Supplementary Movie 5), reducing heart rate by ~10% (Fig. 5h, i),

comparable to puff- and DA-WED-induced deceleration (Fig. 1d, e; Fig. 4i, j). Notably,

optogenetic induction of cardiac deceleration in cardiomyocytes—independent of

central dopaminergic activation—was accompanied by increased locomotion (Fig. 5j,

k). In contrast, this manipulation failed to alter grooming behavior (Supplementary Fig.

9g-i). These observations are consistent with the possibility that cardiac deceleration

may influence locomotor responses during threat.

Together, these findings identify DA-WED neurons that drive cardiac deceleration

during threat and suggest that the resulting cardiac state may influence locomotor

responses (Fig. 5l).

Altogether, these results identify a group of dopaminergic neurons that mediate threat-

induced cardiac deceleration and point to a potential role of cardiac dynamics in shaping

locomotor responses during threat.

DISCUSSION

Here we demonstrate that mechanical threat engages dopaminergic neurons that induce

rapid cardiac deceleration and is associated with increased locomotion. Air puff

stimulation elicited both cardiac deceleration and locomotor activation (Fig. 1), and we

identified two pairs of dopaminergic neurons, termed DA-WED neurons, as key

mediators of the cardiac response (Fig. 4). Silencing these neurons attenuated threat-

induced cardiac deceleration and locomotion, whereas optogenetic activation of DA-

WED neurons elicited both responses in the absence of threat (Fig. 4, Fig. 5). Moreover,

direct optogenetic cardiac deceleration was accompanied by increased locomotion (Fig.

5), suggesting that cardiac deceleration may influence behavioral responses. Together,

these findings support a model in which descending dopaminergic control of cardiac

activity contributes to the coordination of physiological and behavioral responses to

threat, potentially via interoceptive feedback from the heart.

Cardiac deceleration accompanies active defensive locomotion

Our data show that air puff stimulation induces cardiac deceleration together with increased locomotion (Fig. 1). Stronger puff results in more pronounced locomotion but diminished cardiac deceleration (Fig. 1d-g), suggesting that cardiac deceleration is likely not simply a byproduct of locomotion.

Although cardiac deceleration is often associated with freezing in mammals[1], cardiac deceleration has also been observed during early threat detection and orienting responses[78], suggesting that it reflects engagement of a defensive processing rather than motor inhibition *per se*. Consistent with this view, dissociation between threat-evoked cardiac modulation and freezing has been reported across taxa. In mammals, for example, disruption of autonomic output can abolish cardiac deceleration without eliminating freezing[79], suggesting that cardiac deceleration is not merely a secondary consequence of freezing. Similarly, in decapod crustaceans and *Drosophila*, visual stimuli elicit reproducible and time-locked changes in heart rate that accompany both freezing and fleeing[8,9,80]. Our findings extend these observations by showing that cardiac deceleration can accompany active fleeing behavior in response to mechanical threat. Thus, cardiac deceleration is not restricted to passive defensive strategies but can occur during active locomotor responses, supporting the idea that cardiac dynamics are flexibly coupled to different components of the defensive repertoire.

Dopaminergic neurons in the brain are responsible for puff-induced cardiac deceleration

The present study identifies two pairs of dopaminergic neurons in the brain, termed DA-WED neurons, as key mediators of puff-induced cardiac deceleration. Silencing/ photoactivating DA-WED neurons disrupts/ mimics puff-induced cardiac deceleration, respectively (Fig. 4b, c, h-j). Furthermore, DA-WED neurons exhibit calcium elevation upon air puffs (Fig. 4d-g). Moreover, knockdown of the dopamine synthetic enzyme *ple* in DA-WED neurons suppresses puff-induced cardiac deceleration (Supplementary Fig. 6f–h), suggesting that dopamine release from these neurons is required for cardiac deceleration.

Circulatory dopamine has long been associated with cardiac acceleration across species[81]. In *Drosophila*, pharmacological application of DA to the exposed heart accelerates the heartbeat[60–63], seemingly at odds with our findings. However, the responsible source of circulatory DA or DA receptor, as well as whether DA directly acts on cardiomyocytes or instead through some yet unidentified cells, remain elusive. In mammals, cardiomyocytes *per se* synthesize DA and express DA receptors, hinting at autocrine mechanism[81]. Circulatory DA also increases the levels of epinephrine and norepinephrine, complicating the interpretation of "DA-induced" cardiac acceleration[82]. From our ple RNAi experiment (Supplementary Fig. 6f-h), DA released from DA-WED neurons appears indispensable for puff-induced cardiac deceleration. Notably, neurites of DA-WED neurons never exit the brain, suggesting that DA-WED neurons engage circulation or yet unidentified neuronal circuitry to indirectly modulate the heartbeat. Circulation is unlikely to mediate DA-WED neurons' function, however, given that the

air puff and DA-WED activation both induce cardiac deceleration within a second (Fig.

1, Fig. 4). Interestingly, DA acting as a local neuromodulator to drive cardiac

deceleration has been documented in mammals by a few literatures, either in the ventral

tegmental area (VTA) or lateral habenula (LHb)[83,84]. Together, our findings and

previous literature suggest that dopamine may act not only as a circulating hormone that

accelerates heart rate, but as a centrally deployed neuromodulator capable of driving

cardiac deceleration during defensive states.

DA-WED neurons coordinate cardiac and behavioral threat responses

Across species, threatening stimulation elicits cardiac and behavioral responses in an

orchestrated fashion. Cardiac interoception is postulated to serve as key feedback to link

cardiac and behavioral responses[39]. Cardiac interoception is mediated by sensory

neurons innervating the heart and aortic arch[39], which convey information to ACC,

insular, and prefrontal cortex[40] through brain stem NTS and hypothalamic PVN[40]. These

ascending pathways have been proposed to modulate learned fear[41], anxiety-like

behavior[42] or sleep[43]. Although models propose that descending control of the heart and

ascending interoceptive feedback jointly shape defensive behavior, experimental

validation of this bidirectional framework within a single system has been limited.

Our results provide partial support for such a model. We show that (1) mechanical

threat induces cardiac deceleration and locomotion (Fig. 1), (2) DA-WED neurons in

the brain are responsible for threat-induced cardiac deceleration (Fig. 4), (3) optogenetic

cardiac deceleration is accompanied by increased locomotion (Fig. 5d-j). Our data

points to a scenario in which DA-WED neurons induce cardiac deceleration upon threat,

which may in turn influence threat-induced locomotion (Fig. 5k).

Notably, the behavioral consequences of cardiac deceleration appear to be selective

rather than global. Although air puff stimulation suppressed grooming, neither silencing

nor activation of DA-WED neurons significantly affected grooming responses

(Supplementary Fig. 9), despite robust effects on cardiac deceleration and locomotion

(Fig. 4, Fig. 5). Similarly, direct optogenetic induction of cardiac deceleration failed to

influence grooming behavior. These dissociations indicate that cardiac feedback does

not uniformly modulate defensive behaviors but preferentially facilitates locomotor

output. Such selectivity is consistent with the possibility that interoceptive signals from

the heart may bias specific behavioral strategies rather than simply increasing overall

arousal.

Our data suggest that descending dopaminergic control of cardiac function and

ascending cardiac feedback may form a functional loop that shapes adaptive defensive

behavior. Although the specific cardiac sensory pathways mediating feedback to the

brain remain to be identified in *Drosophila*, future work may determine whether flies

possess interoceptive circuits functionally analogous to vertebrate NTS–PVN pathways.

Establishing such circuitry would provide a powerful platform to dissect how central

commands and peripheral physiological states interact to coordinate survival behaviors.

Limitations of this study

While our data are consistent with a model in which DA-WED neurons couple

cardiac deceleration to locomotor responses during threat, several questions remain.

Although cardiac deceleration can promote locomotion, we have not directly tested

whether it is required for DA-WED–evoked locomotion, leaving open the possibility of

parallel downstream pathways. In addition, the sensory mechanisms that relay cardiac

state to locomotor circuits in *Drosophila* remain unidentified. Finally, despite the rapid

timescale and behavioral specificity of our manipulations, we cannot fully exclude

indirect physiological contributions secondary to altered cardiac dynamics. Future

dissection of descending and ascending circuits will clarify these mechanisms.

Overall, we identify a discrete population of dopaminergic neurons that drive rapid

cardiac deceleration in response to mechanical threat. We further show that these

neurons coordinate cardiac responses and are associated with behavioral components of

the defensive response, potentially by engaging interoceptive feedback from the heart.

Our findings establish *Drosophila* as a tractable model for dissecting how exteroceptive

and interoceptive signals are integrated to couple organ physiology with adaptive

behavior, opening new avenues for understanding the neural logic by which internal and

external states are coordinated to promote survival.

ONLINE METHODS

Fly stocks

The following strains were obtained from Bloomington Stock Center (Indiana University): TrH-GAL4 (#38388), Tdc2-GAL4 (#9313), TH-GAL4 (#8848), UAS-TNT (#28838), UAS-Kir2.1::EGFP (#6596), UAS-CsChrimson::mVenus (#55135), UAS-dTrpA1 (#26263), UAS-mCD8::GFP (#32186), UAS-RedStinger (#8547), UAS-IVS-jGCaMP7s (#79032), UAS-GFP RNAi (#41560), UAS-Ple RNAi (#65875), VT046828-AD (#73115), R12D12-DBD (#69213), R48A08-AD (#70707), VT008692-DBD (#86909), empty-AD; empty-DBD (#79603), R70G12-GAL4 (#39552), R38B08-AD (#71032), R81E10-DBD (#68529),VT043775-DBD (#73728), R74C07-GAL4 (#39847), Aes1N-GAL4 (#39847), iav-GAL4 (#52273), R48A07-GAL4 (#50340), UAS-mCherry (#52267), Hand-GAL4 (#48396).

The following strains were obtained from Kyoto Drosophila Stock Center (Kyoto Institute of Technology): Tes1N-GAL4 (#103660).

Hand-GFP was a gift from Dr. Zhe Han (The University of Maryland).

UAS-FRT-stop-FRT-Kir2.1, and UAS-FRT-stop-FRT-CsChrimson::mVenus were gifts from Dr. Barry Dickson (The University of Queensland).

TH-C-GAL4, TH-D-GAL4, TH-F1-GAL4, Vmat-R76F01-GAL4, Vmat-R76F05-GAL4, Ddc-R61H03-GAL4, Ddc-R60F07-GAL4, DAT-R55C10-GAL4, Vmat-R76F01-AD, Vmat-R76F05-AD, Ddc-R60F07-AD, Vmat-R76F01-DBD, Vmat-R76F05-DBD, Ddc-R60F07-DBD, TH-FLP, UAS-FsF-mCD8GFP were gifts from Dr. Mark Wu (Johns Hopkins University).

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470 UAS-GtACR1::tdTomato (III) was gift from Dr. Tabata (The University of Tokyo).

471 Genotypes and sample sizes used in this study are summarized in Supplementary

472 Data 1.

Fly husbandry

Flies were maintained on conventional cornmeal-agar-molasses medium under a

9AM:9PM light/ dark cycle at 25 ˚C and 60 +/- 5 % humidity. Flies were collected 0–1

day post eclosion and housed in a group of 9-10 for 2-5 days before testing unless

otherwise stated. Male flies were used throughout except for Supplementary Fig. 4h, i,

in which both male and female were used. All experiments were carried out between 10

am and 8 pm at 25 +/- 0.8 C and 60 +/- 5 % humidity.

Heartbeat and behavior recording

Flies were tethered above an air-supported foam ball (8 mm diameter; Yuzawaya,

Japan) mounted in a custom sphere holder. Airflow was continuously monitored using a

digital flowmeter (MF-FP10N-H06-010, Horiba Estec Inc.) and maintained at 500 ± 10

mL/min. Behavioral imaging was performed from the right side under 850 nm infrared

illumination using a CMOS camera (GE60, Himawari; 640×480 pixels).

Simultaneously, cardiac activity was imaged from the dorsal side through the intact

cuticle under 850 nm illumination using a second CMOS camera (CS135MU, Thorlabs;

800 × 500 pixels). Behavioral and cardiac imaging streams were externally triggered

and synchronized at 70 Hz using an Arduino Uno board.

Immediately prior to the experiment, flies were briefly (< 1 min) cold-anesthetized,

and the dorsal thorax and abdomen were glued to a coverslip using UV-curable

adhesive (Bondic BD-SKCJ) polymerized with 405 nm UV light (OSV5XME1C1E,

Akizuki Electronics Inc.). The coverslip was positioned above the air-supported ball,

allowing the fly to freely walk on the ball. Each recording session, except for DA-WED

optogenetic activation experiment, consisted of a 20 min acclimation period followed

by puff-response testing (950 s). During puff-response testing, a 500 ms air puff was

delivered once every 90 s for a total of 10 puffs. Recording continued for 30 s after the

final puff. DA-WED optogenetic activation experiment consisted of a 20 min

acclimation period followed by photoactivation-response testing (950 s), in which a 1 s

617nm light was delivered once every 90 s for a total of two (See "Optogenetic

activation of DA-WED neurons" below), to avoid potential desensitization of

CsChrimson.

Heartbeat (without behavior) recording

Cardiomyocytes expressing GFP were imaged dorsally through the intact cuticle.

Images (104 × 50 pixels) were acquired at 24 Hz using a Leica SP8 confocal

microscope equipped with a 10× objective lens (NA 0.4).

Immediately before recording, flies were briefly (< 1 min) cold-anesthetized, and

the ventral thorax and abdomen were glued to a glass slide using UV-curable adhesive

(Bondic BD-SKCJ) polymerized with 405 nm UV light (OSV5XME1C1E, Akizuki

Electronics Inc.). The slide was positioned beneath the objective lens for imaging. Each

recording session consisted of a 10 min acclimation period followed by puff-response

testing (350 s total). A single puff-response test consisted of 1 min baseline recording,

followed by a train of 10 air puffs delivered at 1 Hz (10 s total), and a subsequent 1 min

post-stimulation recording. For each fly, the puff-response test was repeated twice with

a 90 s inter-trial interval.

Automatic heartbeat detection

To automatically detect individual heartbeats, we developed custom software tools. For

infrared (IR)–based heart imaging obtained during simultaneous recordings of cardiac

activity and behavior, the detection pipeline (Supplementary Fig. 1a) computed optical

flow for each pixel between consecutive video frames. These optical flow

measurements were used to quantify global cardiac relaxation (diastole) and contraction

(systole). Time points corresponding to maximal contraction were identified as systolic

peaks, and peak counts were used to compute heart rate (HR). The precision of the

automated detection was evaluated by comparing both absolute HR values and percent

changes in HR during air-puff stimulation relative to baseline with manual annotations.

These analyses demonstrated that the automated method detected both absolute HR and

stimulus-evoked HR changes with accuracy indistinguishable from manual scoring

(Supplementary Fig. 1b, c).

To detect heartbeats in confocal microscopy images of GFP-expressing

cardiomyocytes (recorded in the absence of behavioral measurements; Supplementary

Fig. 4a), each frame was subtracted from the subsequent frame to compute pixel-wise

differences between consecutive image pairs. This procedure generated positive and

negative pixel values in regions surrounding the cardiomyocytes during cardiac

contraction (systole) and relaxation (diastole). During systole, pixels within the heart

tube exhibited positive values corresponding to the current positions of cardiomyocytes,

whereas pixels outside the heart tube exhibited negative values corresponding to their

previous positions; the opposite pattern was observed during diastole. Systolic and

diastolic phases were distinguished by: (i) calculating the standard deviation of the

positions of positive-value pixels along the axis perpendicular to the heart tube (the y-

axis in Supplementary Fig. 4a), denoted $SD(t)$; (ii) calculating the standard deviation of

the positions of negative-value pixels along the same axis, denoted $SD(t–1)$; and (iii)

computing the difference $SD(t) − SD(t–1)$. Negative values of $SD(t) − SD(t–1)$

indicated systole, whereas positive values indicated diastole (Supplementary Fig. 4a).

Time points corresponding to maximal contraction were identified as systolic peaks,

and peak counts were used to compute HR. The precision of this algorithm was

evaluated as described above. Although absolute HR values were slightly overestimated

(Supplementary Fig. 4b), stimulus-evoked changes in HR were captured with accuracy

indistinguishable from manual annotation (Supplementary Fig. 4c).

To obtain a continuous HR time course, peak counts were binned into 0.2 s

intervals, and the number of beats per bin was calculated for each fly and trial. For

visualization of HR dynamics relative to stimulus onset, HR traces were aligned to puff

onset (time 0) and averaged across repeated trials within each fly. In experiments with a

single air puff, puff-induced HR modulation was quantified by comparing the mean HR

during the 1 s following puff onset with the mean HR during the 10 s baseline period

preceding puff onset. Percent change was calculated as [(HR_post − HR_baseline) /

HR_baseline] × 100. In experiments involving 10 puffs delivered over a 10 s window,

HR modulation was quantified as the mean HR during the entire 10 s stimulation period

relative to the 10 s pre-stimulus baseline.

Automatic behavioral identification

To automatically identify behavior on a frame-by-frame basis, videos were analyzed

offline using a custom Python-based pipeline. Body-part coordinates—including the

joints of each leg, the eye, neck, haltere, and the rostral tip of the abdomen on the right

side of the fly—were tracked using SLEAP software[54]. The tracked coordinates were

subsequently transformed to normalize body length and orientation across individuals.

Using these standardized coordinates, the speed of each body part was calculated for

each pair of consecutive frames. Both the standardized coordinates and corresponding

speed measurements were then provided as inputs to a custom support vector machine

(SVM)–based classifier, which labeled each frame as "groom," "walk," or "halt." The

SVM was trained using the standardized body-part coordinates and speed features as

predictors, with manually annotated behavioral labels serving as the dependent

variables. For each fly and each time point relative to puff onset, we calculated the

fraction of frames classified as walking or grooming across 10 repeated trials. For

visualization of behavioral dynamics, these fraction time courses were aligned to puff

onset (time 0) and averaged across trials within each fly. Puff-induced changes in

walking and grooming were quantified by comparing the mean fraction during the 10 s

and 3 s, respectively, following puff onset with the mean fraction during the 10 s

baseline period preceding puff onset. Percent change was calculated as [(fraction_post −

fraction_baseline) / fraction_baseline] × 100.

Mechanical stimulation

Mechanical stimulation was delivered through a glass pipette (tip diameter of ~2 mm),

placed ~2mm in front of the fly, connected with air hose to a compressor (EARTH

MAN, Takagi, Japan) via a solenoid valve (EXA-C6-02C-4, CKD). The solenoid valve

was controlled by an Arduino Uno board, which in turn received connection from a

desktop computer running the python program which orchestrated the video recordings

and puff application. The mechanical stimulation was generated by alternating the

solenoid valve between 500 ms-open and 500 ms-closed states (1 Hz). The mechanical

stimulation lasted for either 1s, 10s, or 20s, as specified in each figure. The air flow was

monitored with a digital flowmeter (MF-FP10N-H06-010, Horiba estec. Inc) and was

adjusted to either 20 mL, 50 mL, or 200 mL/min, as specified in each figure.

Optogenetic activation of DA-WED neurons

Flies expressing CsChrimson, a red-shifted channelrhodopsin variant, in DA-WED

neurons were raised on food containing 500 µM all-trans retinal for 2 - 3 days, in the

dark, prior to testing. Photoactivation was performed by delivering a 1s LED light pulse

(617nm, Thorlabs) to the fly's head. The output for LED was measured with a power

meter (S120C and PM120D, Thorlabs) at a position corresponding to the fly's head, and

was adjusted to 1 µW/mm^2. Light stimuli were triggered by python through an Arduino

board connected to the LED driver.

Optogenetic cardiac deceleration

Flies expressing GtACR1, a light-gated anion channel, in cardiomyocytes were raised

on food containing 500 µM all-trans retinal for 2 - 3 days, in the dark, prior to testing.

Photoactivation was performed by delivering a 28ms-long LED light pulse (530nm,

Thorlabs) to the fly's heart through the objective lens. The light intensity was adjusted,

for each fly prior to the recording, to the minimum intensity required for a light pulse of

roughly 2s to briefly stop the heartbeat. After the recording, the output for LED was

measured with a power meter (S120C and PM120D, Thorlabs) at a position

corresponding to the fly's heart, and ranged from $9.88 – 21.8 \mu W/mm^2$. Light stimuli

were triggered by python through an Arduino board connected to the LED driver.

Immunohistochemistry

The following antibodies were used: mouse nc82 (1:10 Developmental Studies

Hybridoma Bank), goat anti-mouse Alexa 633 (1:100, Molecular Probe #A21050).

Whole brain immunohistochemistry was performed as described previously[85,86]. Briefly,

brains were dissected out in 0.3 % PBST, and were fixed in 2 % paraformaldehyde/

PBS for 90 min at room temperature. Brains were then washed in 0.3 % PBST, for > 3

h, and were blocked in 10 % normal goat serum/ 0.3 % PBST for 30 min. Brains were

incubated in the primary antibodies in 10% normal goat serum/ 0.3% PBST at 4 ˚C for 2

days. Brains were then washed in 0.3 % PBST for > 5 h, and were blocked in 10 %

normal goat serum/ 0.3 % PBST for 30 min. Brains were then incubated in the

secondary antibodies in 10 % normal goat serum/ 0.3 % PBST at 4°C for 2 days.

Afterward, brains were washed in 0.3 % PBST for > 5 h, and incubated in 50 %

glycerol/ 0.3 % PBST for 2 h at 4 ˚C. Lastly, brains were mounted on slide glass in

Vectashield (Vector Laboratories). Images were taken with Leica TCS SP8 confocal

microscope, and processed in ImageJ (NIH) software.

Calcium imaging

Two-photon calcium imaging was conducted as described previously[53] with a few

modifications. Two-photon microscopy (Bergamo II, Thorlabs) with a 16x objective

lens (16x CFI LWP Plan Flour Objective, Nikon) and with near-infrared excitation (930

nm, Mai Tai 2, SpectraPhysics. Inc., Mountain View, CA) was used. Cuticle of the top

of the flies' head and the fat and trachea beneath it were surgically removed. The

exposed brain was submerged in saline solution. The extracellular saline had the

following composition (in mM): 103 NaCl, 3 KCl, 5 HEPES, 10 trehalose, 10 glucose,

7 sucrose, 26 $NaHCO_3$, 1 NaH_2PO_4, 1.5 $CaCl_2$, 4 $MgCl_2$. We identified DA-WED

neurons using the baseline fluorescence of GCaMP. Images were acquired from 1 plane

at 152 frames per s (160 x 96 pixels, pixel size = 0.388 μm, dwell time = 0.246 μs).

During calcium imaging, a large fraction of the fly's body was glued to the holding

plate, and part of the fly's eye compounds was covered with the holder, and the fly was

hung in the air. Each fly underwent the sequence of stimuli per fly once or twice, to

scan DA-WED neurons on both hemispheres whenever possible. The time courses of

$\Delta F/F_0$ were calculated by, for each bin, taking the percent difference from F 10s prior to

the onset of the initial puff application (t = -10 through 0s in Fig. 4f).

Surgery

In search of sensory organs indispensable for air puffs to induce cardiac deceleration, halteres, wings, legs, and a3 segments of the antennae were surgically removed using a pair of forceps on ice just prior to testing. Flies that underwent cold anesthesia just prior to testing served as controls.

Feeding preference test

Two days post eclosion male flies were protein deprived by maintaining on 200 mM sucrose (vials with a kimwipe soaked with 2mL of sucrose solution) for 8 days (kimwipe is exchanged every other day). Prep 7.5% yeast and 200mM sucrose in 0.9% of agar, color-labeled with either blue (brilliant blue FCF) or red (sulforhodamine B) tasteless food dyes. The two types of food mix, 1mL each, were then aliquoted into 35mm petri dish separated by a 5x5x35mm acrylic bar into two chambers. A group of 70 flies starved for 3 hours in an empty vial with a kimwipe soaked with 2 mL of water were cold-anesthetized and transferred into petri dish at ZT2 and allowed to feed for 2 hours in the dark. The flies were then killed by transferring the dish to -30C, upside-down, and scored by examining the color of their abdomen. Preference Index (PI) for yeast was calculated as (# flies consuming yeast - # flies consuming sucrose) / (total # flies that fed). Flies with insufficiently colored abdomen were discarded as poorly fed flies.

Data analyses

Data analyses were performed using our custom-written R and python programs.

Statistics

We did not predetermine the sample sizes. The distribution of normality of each group

was assessed using Shapiro-Wilk normality test. Parametric tests (unequal variances t-

test known as Welch's t-test or Dunnett's test) were used only when distributions were

deemed normal; otherwise, non-parametric tests were used (Wilcoxon signed rank test,

Wilcoxon rank sum test, or Dunn's test). All statistical tests were two-sided. We

employed Bonferroni correction to correct for two tests, and correction implemented in

Dunnett's or Dunn's test for more than two tests. $p < 0.05$ after corrections for multiple

comparison was deemed statistically significant. Neither randomization nor blinding

was performed for the group allocation during experiments or data analysis. All box

plots are generated so that center line indicates median, box limits indicate upper and

lower quartiles, and whiskers indicate 1.5x interquartile range. All the statistical results

are summarized in Supplementary Data 2.

DATA AVAILABILITY

Source data for all main text and Supplementary Figures are available via request to the

corresponding author.

CODE AVAILABILITY

Source codes used in the current study are available at

https://github.com/mtsuji172/heart_behavior.

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AUTHOR CONTRIBUTIONS

M.T. designed the experiments. M.T., J. D., Y. U., and A.O. performed the experiments.

M.T. analyzed the data. M.T. and K.E. interpreted the results and wrote the paper.

COMPETING FINANCIAL INTERESTS

The authors declare no competing financial interests.

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TABLES

Supplementary Data 1 List of genotypes and sample sizes used in this study

Supplementary Data 2 Statistics of data presented in this study

MOVIES

Supplementary Movie 1 An air puff induces cardiac deceleration and promotes locomotion. A 50 mL/min puff is applied in the middle of the movie, as indicated by the red text that appears on the top left panel of the movie. The bottom left panel shows a behavioral recording, with automated body parts tracking (blue dots and lines) superimposed on the raw data. The top right panel shows the raw heartbeat recording, and the bottom right panel shows the pixel-wise, color-coded optical flow (color-to-direction mapping is shown on the top right of the panel). The playback speed is reduced to 0.25 of the original file.

Supplementary Movie 2 A train of 10 air puffs induce cardiac deceleration in a Hand>GFP fly. The playback speed is reduced to 0.25 of the original file.

Supplementary Movie 3 Air puffs activate DA-WED neurons. The left panel shows a

schematic of the DA-WED neurons and the actual calcium imaging data (averaged

over the total recording), capturing both DA-WED neurons in the right hemisphere.

An arrow indicates the neuron shown on the right panel. The right panel shows

GCaMP signals at time 0 on the top, and the time-lapse imaging from there during

which air puffs were applied.

Supplementary Movie 4 Optogenetic activation of DA-WED neurons induces cardiac

deceleration and promotes locomotion. The playback speed is reduced to 0.25 of the

original file.

Supplementary Movie 5 Optogenetic cardiac deceleration promotes locomotion. The

playback speed is reduced to 0.25 of the original file.

Fig. 1 Mechanical threat induces cardiac deceleration and locomotion

a. Schematics of the paradigm. The fly is fixed on an air-supported ball. Left: the heart rate (HR) was videotaped by an IR-sensitive camera from the dorsal side through the cuticle ("CAM1"). Of the four cardiac chambers, our system videotaped the chamber closest to the thorax called conical chamber. We could easily distinguish diastole and systole in the captured video (blue dashed lines indicate the heart wall). Right: simultaneously, locomotion was videotaped from the right side of the fly ("CAM2"). Blue dots and lines indicate automatically tracked body parts. **b.** The time course of the experiment. An air puffs of 0.5 s was applied once. The trial was repeated 10 times for each fly, the results of which were averaged. **c.** An example M-mode of the heartbeat. An air puff was applied during the red-shaded time window. **d.** Time course of the HR (% change from baseline defined as the average during the 10 s preceding puff onset). N = 14, 17, 22 for 20mL/min (gray), 50mL/min (sky blue), and 200mL/min (dark blue), respectively. The inlet shows the magnified view of the cardiac deceleration indicated by the box. **e.** Change in HR, calculated for each fly as the % difference between the mean fraction during the 1 s following stimulation onset and the mean fraction during the 10 s baseline period preceding stimulation. N = 14, 17, 22 for 20mL/min (gray), 50mL/min (sky blue), and 200mL/min (dark blue), respectively. **p < 0.01, *p < 0.05, n.s.: p > 0.05, Wilcoxon's signed rank test followed by Bonfferoni correction. **f.** Time course of the walking fraction (% change from baseline defined as the mean fraction during the 10 s preceding puff onset). N = 14, 17, 22 for 20mL/min (gray), 50mL/min (sky blue), and 200mL/min (dark blue), respectively. ***p < 0.001, n.s.: p > 0.05, Wilcoxon's signed rank test followed by Bonfferoni correction. **g.** Change in walking fraction, calculated for each fly as the % difference between the mean fraction during the 10 s following stimulation onset and the mean fraction during the 10 s baseline period preceding stimulation. N = 14, 17, 22 for 20mL/min (gray), 50mL/min (sky blue), and 200mL/min (dark blue), respectively. ***p < 0.001, n.s.: p > 0.05, Wilcoxon's signed rank test followed by Bonfferoni correction.

Fig. 2 Dopamine system is responsible for puff-induced cardiac deceleration

a. Experimental setup. Hand enhancer drives the GFP expression in the cardiomyocytes (and in pericardiocytes). The fly was glued onto a slide glass, and the GFP signals were acquired through the intact cuticle. The air puffs were applied frontally to the fly's head. **b.** Example heartbeat. (Upper) Cartoon of the acquired image. Two rows of small cardiomyocytes and one pair of large pericardiocytes are visible. (Lower) Diastole and systole can be distinguished by the changing distance between two rows of cardiomyocytes (arrows). **c.** The time course of the experiment. Air puffs of 0.5 s were applied at 1 Hz for 10 times (totalling 10 s). The trial was repeated twice for each fly, the results of which were averaged. **d.** Time course of the HR. Air puffs are applied during red-shaded window. Lines and shaded areas represent means and SEM, respectively. N = 28. **e.** The HR averaged during puff application window ("puff +") vs 10 s before puff application ("puff -"). Each line corresponds to each fly. N = 28, ***p < 0.001, two-tailed *t*-test. **f.** Difference between puff+ HR and puff- HR, calculated for each fly. N = 28, ***p < 0.001, two-tailed *t*-test. **g.** Time course of the HR (% change from baseline defined as the average during the 10 s preceding puff onset). Air puffs were applied during the red-shaded time window. Lines and shaded areas represent means and SEM, respectively. TNT expression is driven by indicated drivers. "+" indicates driver-less control. Dashed line shows the lowest mean of "+" control during puffs. N = 55, 30, 29, 34, for +, TrH, Tdc2, TH, respectively. **h.** Change in HR, calculated for each fly as the % difference between the mean HR during the 10 s stimulation period and the mean HR during the 10 s baseline period preceding stimulation. N = 55, 30, 29, 34, for +, TrH, Tdc2, TH, respectively. *p < 0.05, n.s.: p > 0.05, Dunn's test. **i.** Time course of the experiment. The heat plate beneath the slide glass warmed up the fly. The temperature of the slide glass is held at 21℃ for 10 min and ramped up to 28℃ for 5min. Note it took approximately 17 s for the temperature to ramp from 21℃ to 28℃. **j.** Time course of the HR, shown as % change from average HR at 21℃. Temperature was rampted from 21℃ to 28℃ during red-shaded window. **k.** % Changes in the HR (28℃ vs 21℃) from the baseline (average over initial 60 s) averaged over 75s - 180s window (shown as black bar in j.). N = 33, 20, 14, 31, for +, TrH, Tdc2, TH, respectively. *p < 0.05, n.s.: p > 0.05, Dunn's test. The upper dashed line shows the median of "+" control. **l.** Time course of the HR (% change from baseline defined as the average during the 10 s preceding puff onset). Air puffs were applied during the red-shaded time window. Lines and shaded areas represent means and SEM, respectively. N = 31, 29, 28, 35, 23, for +, WT, *Dop1R1*, *Dop1R2*, *Dop2R*, *DopEcR*, respectively. **m.** Change in HR, calculated for each fly as the % difference between the mean HR during the 10 s stimulation period and the HR HR during the 10 s baseline period preceding stimulation. N = 31, 29, 28, 35, 23, for +, WT, *Dop1R1*, *Dop1R2*, *Dop2R*, *DopEcR*, respectively. **p < 0.01, n.s.: p > 0.05, Dunn's test.

Fig. 3 Two pairs of dopaminergic neurons in the brain are paritally indispensable for cardiac deceleration

a. AsSchematic of different DA-related GAL4 drivers. **b.** Change in HR, calculated for each fly as the % difference between the mean HR during the 10 s stimulation period and the HR HR during the 10 s baseline period preceding stimulation. N = 74, 22, 26, 21, 36, 20, 12, 25, 23, for +, TH-C, TH-D, TH-F1, Vmat-R76F01, Vmat-R76F05, Ddc-R61H03, Ddc-R60F07, DAT-R55C10, respectively. **p < 0.01, *p < 0.05, n.s. (data shown in gray): p > 0.05, Dunnett's test. **c.** A schematic of split-GAL4 strategy. **d.** Change in HR, calculated for each fly as the % difference between the mean HR during the 10 s stimulation period and the HR HR during the 10 s baseline period preceding stimulation. N = 106, 27, 27, 26, 41, 32, 24, for driver-less control, R76F01 ∩ R76F02, R76F02 ∩ R76F05, R76F01 ∩ R76F02, R76F02 ∩ R76F07, R76F05 ∩ R60F07, R76F01 ∩ R60F07, R76F01 ∩ R76F05, respectively. *p < 0.05, n.s.: p > 0.05, Dunn's test. **e.** Brain of R60F07-AD ∩ R76F01-DBD>mCherry (red). An arrow indicates the soma of PPL1-SMPγ, while arrowheads indicate the soma of DA-WED. Scale bar: 25 um. Similar results were obtained across 3 independent samples. **f.** Brains of VT046828-AD ∩ R12D12-DBD>mCherry and R48A08-AD ∩ VT008692-DBD>mCherry (red) immunostained with anti-neuropil marker nc82 (blue). Scale bars: 25 um (inlet: 5 um). Similar results were obtained across 5 independent samples for each genotype. **g.** Change in HR, calculated for each fly as the % difference between the mean HR during the 10 s stimulation period and the HR HR during the 10 s baseline period preceding stimulation. N = 51, 41, 36 for empty>TNT, PPL1-SMPγ>TNT, DA-WED>TNT, respectively. *p < 0.05, n.s.: p > 0.05, Dunnett's test.

Fig. 4 DA-WED neurons are responsible for puff-induced cardiac deceleration
a. The brain of R48A08-AD ∩ VT008692-DBD ∩ TH-FLP>mCD8::GFP (green) immunostained with anti-neuropil marker nc82 (blue). Scale bar: 30 um. Similar results were obtained across 5 independent samples. **b.** Time course of the HR (% change from baseline defined as the average during the 10 s preceding puff onset). Air puff was applied during the red-shaded time window. Lines and shaded areas represent means and SEM, respectively. N = 28, 27, for empty>Kir2.1, DA-WED>Kir2.1, respectively. **c.** Change in HR, calculated for each fly as the % difference between the mean HR during the 1 s following stimulation onset and the mean HR during the 10 s baseline period preceding stimulation. N = 28, 27, for empty>Kir2.1, DA-WED>Kir2.1, respectively. *p < 0.05, Two-tailed *t*-test. **d.** Experimental setup. **e.** Representative images of DA-WED neurons expressing GCaMP7s before and during puff application. Scale bar: 5μm. **f.** Time course of $\Delta F/F_0$. Puffs were applied at 1Hz for 10 times (over 10 s), as indicated by red-shaded boxes. N = 6 flies. **g.** $\Delta F/F_0$ averaged over 10s of puff application. When multiple neurons were recorded from the same fly (max 4 neurons per fly), results were averaged so that each dot represents one fly. N = 6 flies. two-tailed *t*-test. **p < 0.01. **h.** Time course of the experiment. After 20 min of acclimation, the heartbeat of the fly expressing light-gated cation channel CsChrimson in DA-WED neurons, with ("Ret +") or without ("Ret -") being fed with the co-factor all-trans retinal (ATR) for 2 days prior to experiment, was recorded for 10s, followed by 1s of light application, and 20s of recording. **i.** Time course of the HR (% change from baseline defined as the average during the 10 s preceding puff onset). Red light was shined during the red-shaded time window. Lines and shaded areas represent means and SEM, respectively. N = 19, 22, for Ret-, Ret+, respectively. **j.** Change in HR, calculated for each fly as the % difference between the mean HR during the 1 s following stimulation onset and the mean HR during the 10 s baseline period preceding stimulation. N = 13, 12, for Ret-, Ret+, respectively. *p < 0.05, two-tailed *t*-test. **k.** Model.

Fig. 5 Cardiac interoception possibly contributes to threat-induced locomotion

a. Time course of the walking fraction (% change from baseline defined as the mean fraction during the 10 s preceding puff onset). An air puff was applied during the red-shaded time window. Lines and shaded areas represent means and SEM, respectively. N = 28, 27, for empty>Kir2.1, DA-WED>Kir2.1, respectively. **b.** Change in walking fraction, calculated for each fly as the % difference between the mean fraction during the 10 s following stimulation onset and the mean fraction during the 10 s baseline period preceding stimulation. N = 28, 27, for empty>Kir2.1, DA-WED>Kir2.1, respectively. **p < 0.01, Two-tailed *t*-test. **c.** Time course of the walking fraction (% change from baseline defined as the mean fraction during the 10 s preceding puff onset). Red light was applied during the red-shaded time window. Lines and shaded areas represent means and SEM, respectively. N = 13, 12, for ret -, +, respectively. **d.** Change in walking fraction, calculated for each fly as the % difference between the mean fraction during the 10 s following stimulation onset and the mean fraction during the 10 s baseline period preceding stimulation. N = 13, 12, for ret -, +, respectively. **p < 0.01, Two-tailed *t*-test. **e.** A schematic of the strategy. Cardiomyocytes beat by oscillating between shrunk (systole) and relaxed (diastole) states. Diastole is driven by efflux of cation and resultant hyperpolarization. We expressed a light-gated anion channel GtACR1 in cardiomyocytes using Hand-GAL4, thus artificially driving hyperpolarization by shining light. **f.** Time course of the experiment. After 20 min of acclimation, the heartbeat of the fly expressing GtACR1 in cardiomyocytes, with or without being fed with the co-factor all-trans retinal (ATR) for 2 days prior to experiment, was recorded for 90s, followed by a 28ms light pulse, and 45s of recording. The experiment was repeated twice for each fly. **g.** An example M-mode during optogenetic cardiac deceleration. Green bar indicates when the light was shined. **h.** Time course of the HR (% change from baseline defined as the average during the 10 s preceding puff onset). Green light was shined during the breen-shaded time window. Lines and shaded areas represent means and SEM, respectively. N = 10, 11, for ret -, ret +, respectively. **i.** Change in HR, calculated for each fly as the % difference between the mean HR during the 1 s following stimulation onset and the mean HR during the 10 s baseline period preceding stimulation. N = 10, 11, for ret -, ret +, respectively. *p < 0.05, Two-tailed *t*-test. **j.** Time course of the walking fraction (% change from baseline defined as the mean fraction during the 10 s preceding puff onset). Light was shined during the green-shaded time window. Lines and shaded areas represent means and SEM, respectively. N = 10, 11, for ret -, ret +, respectively. **k.** Change in walking fraction, calculated for each fly as the % difference between the mean fraction during the 10 s following stimulation onset and the mean fraction during the 10 s baseline period preceding stimulation. N = 10, 11, for ret -, ret +, respectively. *p < 0.05, two-tailed *t*-test. **l.** Model.