De novo designed bifunctional proteins for targeted protein degradation

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Author contributions: BM, BK, DH, AJW, LSI and DNW conceived the project and designed the experiments. BM designed the scaffold and binders, and purified and characterised them using solution-phase biophysics. AMAJ and AM purified the target proteins and measured the binding affinities of the binders against them. BM and AMAJ determined the protein X-ray crystal structures with help from TAE. BK performed all cell assays. BM and DNW wrote the paper. All authors have read and contributed to the preparation of the manuscript. TAE, LSI, DNW, and AJW raised the funding.

ABSTRACT

Targeted protein degradation (TPD) is a therapeutic strategy to remove disease-causing

proteins by routing them to the ubiquitin-proteasome, autophagy, or lysosme machineries. For

instance, proteolysis-targeting chimeras (PROTACs) are synthetic hetero-bifunctional small

molecules that simultaneously bind the target and an E3 ubiquitin ligase to drive ubiquitination

and degradation by the proteasome. Despite considerable success, designing such molecules

is challenging and the number of currently addressable ubiquitin E3 ligases is limited. Here

we demonstrate hetero-bifunctional *de novo* designed proteins as alternatives for TPD to

access more targets and ligases. First, we develop a stable and highly adaptable helix-turn-

helix scaffold for presenting different binding sites. Next, we use computational protein design

to incorporate and embellish hot-spot- binding sites to target BCL-x_L, plus short linear motifs

(SLiMs) for KLHL20 ligase recruitment. The resulting mono- and bi-functionalised proteins bind

the targets *in vitro*, and the latter degrade BCL-x_L in cells leading to apoptosis.

MAIN

Over the past two decades, targeted protein degradation (TPD) has developed into a promising therapeutic strategy[1,2]. While multiple degradation machineries are under investigation[3,4], the proteasome remains the most extensively studied[1,2,5]. For instance, molecular glue degraders[6] and proteolysis-targeting chimeras (PROTACs)[7] simultaneously bind a protein of interest (POI) and an E3 ubiquitin ligase (E3), inducing ubiquitination of the POI and its subsequent proteasomal degradation. Unlike classical inhibitors, PROTACs can work by engaging any region of the POI and are not limited to recognition of functional sites. Through this encounter-driven mechanism, the process can be catalytic, with multiple copies of a POI being eliminated by each PROTAC molecule[1,2,8]. As a result, lower doses of cytotoxic compounds can be used[9].

Despite encouraging progress in clinical trials[5], bottlenecks remain for small-molecule PROTACs. The degradation efficiency is driven by ternary complex formation, which depends on multiple factors, including individual binding constants of the two recognition elements, linker lengths between them, the locations of binding sites on the targets and proximity of suitable lysine residues to which ubiquitin can be conjugated[8]. Secondly, despite the vast potential E3 repertoire, most PROTACs harness just two E3s – Cereblon (CRBN) or von Hippel-Lindau (VHL)[5,10,11]. Whilst this is changing with new E3 ligands being described[12-14],exploring new modes of targeting and binding the POI and ligases will help advance and generalise the technology[1]. For instance, peptide-based PROTACs[15] have the potential to overcome these limitations by using natural short linear motifs (SLiMs) as a common protein-protein interaction (PPI) modality to access more targets and E3s[7,16-18]. However, SLiMs often have weak binding affinities, making it difficult to direct precise and stable complex formation.

Recent advances in protein-structure prediction and protein design might help overcome these limitations. Deep learning-based methods have accelerated the fields dramatically[19-22], with AlphaFold2[23] and related methods[24] for rapid and accurate modelling, and tools such as RFdiffusion[25] and ProteinMPNN[26] for *de novo* protein backbone and sequence design, respectively. Computational design pipelines, either alone or in combination with experimental screening of many variants, are achieving protein binders approaching pM binding affinities[27-29]. In addition, tools like BindCraft[29] are democratizing binder design, and allow targeting of specific regions on the POI's surface. These successes have encouraged the field to move beyond binding a single protein. For example, proteins have been designed to inhibit multiple different POIs,[30] or to display multiple viral epitopes[31]. Designed proteins have been fused together via a flexible linker to drive internalisation of membrane proteins[32] or to cause degradation or stabilisation of intracellular targets[33]. Nonetheless, these strategies do not leverage the full potential of protein design, which, in principle, allows for the precise positioning of multiple binding sites to drive specific ternary complex formation.

Here, we describe a *de novo* designed protein-based PROTAC. For the POI, we target
BCL-x_L, a member of the therapeutically important B-cell lymphoma 2 (BCL-2) family. BCL-x_L
is an anti-apoptotic protein that can be inhibited by binding helical peptide effectors leading to
apoptosis[34,35]. As this interaction is well characterised with high-resolution X-ray crystal
structures[36], together with homologues such as MCL-1 it has served as a testing ground for
developing methods leading to the design of many peptide-, protein- and small-molecule-
based binders[37-40]. Moreover, due to interest in BCL-x_L as an anti-apoptotic cancer target,
small-molecule inhibitors and PROTACs have been developed for it[41]; *e.g.*, a PROTAC
synthetic molecule, DT2216, is currently undergoing clinical trials[42]. Like many PROTACs, this
uses a VHL-binding ligand to induce ubiquitination. Recently, we have identified other E3s
compatible with TPD of BCL-x_L, including Kelch-like protein 20 (KLHL20) with an in-cell, GFP-
based degradation assay (accompanying manuscript). X-ray crystal structures[43] indicate that
the KLHL20 binding-competent SLiM adopts a compact loop conformation. Indeed, binding
affinity can be improved by constraining the SLiM as a cyclic peptide, and these have been
used in the design of small-molecule/peptide hybrid PROTACs[17].

To generate and validate a *de novo* protein-based PROTAC against BCL-x_L, we
develop the following design pipeline (Fig. 1a). First, using rationally seeded computational
protein design[44], we make a straightforward helix-loop-helix scaffold. Next, we add a binding
site for BCL-x_L using hot-spot-grafting combined with ProteinMPNN optimisation and
AlphaFold2 modelling and evaluation. To test the versatility of the scaffold and approach, we
design and compare binders for BCL-x_L and MCL-1, exploring specificity with *in vitro* binding
assays and structural studies. Subsequently, we graft on a SLiM (degron) for KLHL20 and
optimise its binding affinity. These bindings sites were tested individually in the in-cell, GFP-
based degradation assay for their capacity to act as targeting sequences or degrons. Finally,
the best performing binding sequences were combined and assessed for their ability to
degrade BCL-x_L and induce apoptosis in a lung-cancer cell line. Specifically, we compare
single and bifunctional constructs with binding sites against BCL-x_L and/or KLHL20, and the
small molecule in clinical trials, DT2216. Only the constructs with both modalities—*i.e.*, for
target and E3 ligase binding—function as BCL-x_L degraders in cells.
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Figure 1: *De novo* **design of a scaffold for display of multiple binding motifs. a,** Schematic overview of this work. From left to right: helix-loop-helix scaffold (sc-apCC-2) designed based on the heterodimeric, antiparallel, coiled-coil peptides, apCC-Di-AB peptide[45]; grafting of the BCL-x_L binding site; addition of a second interaction site for the E3 ligase adapter, KLHL20, into the loop; and testing for BCL-x_L degradation and apoptosis in human cell lines. **b,** Circular dichroism (CD) spectra for apCC-Di-AB (grey) and sc-apCC-2 (magenta). CD spectra were recorded at 20 °C and 50 μM total peptide/protein concentrations. **c,** Thermal response of CD signals at 222 nm for apCC-Di-AB (grey) and sc-apCC-2 (magenta), at 50 μM and 10 μM, respectively. **d,** Sedimentation-equilibrium analytical ultracentrifugation measurements at 52,000 RPM (blue), 56,000 RPM (red) and 60,000 RPM (yellow). The ratio between experimentally fitted and theoretical mass was 0.9 over the three speeds. **e,** X-ray crystal structure of the sc-apCC-2 scaffold, electron density around the loop shown at sigma level 1 (PDB id: 9TLL; 1.5 Å). Parts of this figure were made with BioRender.

RESULTS

Rational design yields a highly stable display scaffold

To create a small, highly thermostable and, highly designable scaffold for displaying helical target-binding sites and additional sites for E3 recruitment, we applied our rationally seeded peptide-to-protein approach[44]. Specifically, we generated a helix-loop-helix scaffold from a previously characterised antiparallel, heterodimeric *de novo* coiled coil, apCC-Di-AB[45]. Starting with the X-ray crystal structure of apCC-Di-AB, motif searching with MASTER[46] was used to find loops from the PDB to connect the two helices. Next, the sequence of one loop and flanking residues was optimized for the scaffold using Rosetta remodel[47] (Supplementary Fig. 1). Initially, this designed hairpin was made by Fmoc-based solid-phase peptide synthesis. Unlike the dimeric parent peptide, this was highly thermostable by CD spectroscopy. An X-ray crystal structure at 1.5 Å resolution (PDB id: 9TLL) had an overall backbone RMSD of 0.36 Å

between the design model and experimental structure, and it confirmed to the loop design. We

called this new 67-residue miniprotein scaffold, sc-apCC-2, using our systematic naming

system[44].

ProteinMPNN-embellished motif grafting gives robust binders to the POI

Previously, we have shown that dimeric coiled-coil peptides can bind to BCL-2 family proteins

by grafting hot-spot residues onto the outer helical surfaces[48,49]. To improve on this, we added

modern AI tools such as ProteinMPNN[26] and AlphaFold2[23] to the following computational

design pipeline, which is depicted in Fig. 2a. To seed binder designs, first, we examined

experimental structures of natural binders and targets in the BH3-only BCL-2 family and

identified six hot-spot positions. To generate starting sequences for these sites, we used a

small amino-acid pallet reflecting the sequences of BCL-2 effector proteins. For example, to

target BCL-X_L binding, we started with 18 different sequence motifs (Supplementary Table 10)

and grafted these onto 3 plausible locations on the solvent-exposed surface of the *de novo*

scaffold. Models for each of the resulting 54 seed sequences were aligned onto 5 models for

BCL-x_L:effector complexes where the pose of effector peptide was rotated incrementally by

10º (Supplementary Fig. 2), leading to 270 models. Next, to explore the potential to extend

the complementary binding surfaces, we applied ProteinMPNN-RosettaRelax protocols[26] and

varied the number of residues in the scaffold to be mutated. This yielded 609 different

sequences. For each of these, AlphaFold2 was used to predict complexes with BCL-x_L. These

models were filtered and assessed based on pLDDT, different AlphaFold2 metrics, shape

complementarity (Sc),[50] and Rosetta energy (ΔG)[51] to select candidates for experimental

testing. We repeated this protocol for MCL-1 as a secondary target. While also a member of

the BCL-2 family, it has a distinct selectivity profile and frequently shows increased levels as

a response to BCL-x_L inhibition[52].

We chose 14 designs against the primary target BCL-x_L and 4 against MCL-1 for

expression from synthetic genes in *E. coli*. All but one of these could be purified as soluble

protein, and the remaining 13 were highly thermostable helical proteins (Supplementary Fig.

3). X-ray crystal structures revealed that the surface mutations were accommodated by the

scaffold (PDB ids: 9TLM, 9TLN, 9TLO, 9TLP, 9TLQ, 9TLR, Supplementary Fig. 4-5). Initial

binding to both targets was probed using a competitive fluorescent anisotropy (FA) assay with

the natural effector peptide, BID, as the labelled competitor peptide that was displaced (K_D =

71 nM against BCL-x_L and K_D = 21.5 nM against MCL-1, Supplementary Fig. 6 and

Supplementary Table 11)[48,49]. 12 of the expressed designs had sub-µM IC_{50} values against

their intended targets, near the edge of the dynamic range for this assay (Supplementary Table

12). The MCL-1-targeting sequences were highly selective, while nearly all BCL-x_L targeting

designs bound both targets equally.

Isothermal titration calorimetry (ITC) was used to validate BCL-x_L binding for a selected

binder, Sc-apCC-2-BCL-x_L-3. This binder had an IC$_{50}$ of 196 ± 14 nM by FA, and a K_D of 3 nM

at 37 °C by ITC (Fig. 2d and Supplementary Table 14). A 3 Å resolution X-ray crystal structure

for this complex revealed that side chains in the binding interface matched the predicted

conformation (Fig. 2e; PDB id 9TLU, 3.0 Å). Crystal structures of two MCL-1 binders in complex

with the target were also obtained (Fig. 2f and Supplementary Fig. 7; PDB ids 9TLV, 9TLW),

likewise confirming the accuracy of the designs and AlphaFold2 predictions.

Figure 2: *De novo* designed binders for BCL-2-family proteins. a, Design schematic. From
left to right: hot-spot residues selected from natural BCL-x_L and MCL-1 effectors were grafted

onto the scaffold at all feasible surface-exposed locations of the scaffold and then aligned to
the binding cleft; ProteinMPNN was used to add residues at the interface to improve binding.
All final designed sequences were predicted as complexes with the target using AlphaFold2.
Numbers in brackets refer to the motifs/designs at each step in the pipeline. **b**, Fluorescence
anisotropy (FA) data for a BCL-x_L binder against BCL-x_L (dark blue, IC$_{50}$: 196 ± 14 nM) and
MCL-1 (red, IC$_{50}$: 660 ± 50 nM). **c**, Similar FA data for a MCL-1 binder against MCL-1 (red, IC$_{50}$:
64 ± 2 nM) and BCL-x_L (dark blue IC$_{50}$: 40 ± 20 µM). **d**, ITC data and analysis for the BCL-x_L
binder against BCL-x_L (K$_D$: 3 nM. **e**, Co-crystal X-ray structure of the BCL-x_L binder with BCL-
x_L (PDB id 9TLU). The experimental structure of the sc-apCC-2 component (shown in rainbow
colours) is aligned with its predicted model (grey), and the experimental structure of BCL-x_L is
rendered as a surface (blue). The zoom shows details of the interacting side chains, the non-
interacting helix and side chains are not shown for clarity. **f,** Similar images to **e**, but for the co-
crystal X-ray structure of the MCL-1 binder and MCL-1 (PDB id 9TLV). The scaffold
components in **e** and **f** are aligned vertically to highlight the shift in the designed binding sites.
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Computational negative selection improves selectivity for the POI

Presumably due to the similarity between the peptide-binding interfaces on MCL-1 and BCL-

x_L, the designed BCL-x_L binders showed little specificity. To improve this, we added the

following computational negative-selection step as follows to identify selective designs for

BCL-x_L. AlphaFold2 was used to model the complexes of all previously designs with both

target proteins (Fig. 3a). These models were then scored and ranked based on the pLDDT of

the motif residues, overall pAE score, and Sc. Sequences with large differences in rank for

each metric and a combined metric were selected (Fig. 3b, and Supplementary Fig. 8). In total

four further designs targeting BCL-x_L and two for MCL-1 were expressed in *E. coli*. Five of

these could be purified as soluble proteins. Their biophysical characteristics were similar to

the foregoing designs (Supplementary Fig. 9). From the FA assay showed that, the BCL-x_L

binder selected by Sc, Sc-apCC-2-BCL-x_L-17, retained a high affinity for BCL-x_L and,

moreover, it bound MCL-1 >1000-fold more weakly (Fig. 3c). The other designs selected using

the other metrics—pLDDT and pAE, and a combination of these plus Sc—either showed little

specificity or had decreased affinity for both targets (Supplementary Fig. 7 and 8). Thus,

ProteinMPNN-enhanced motif grafting with some filtering—in this case based on shape

complementarity scores—can generate tight and selective binders. That said, while the

number of designs tested here is limited, these data suggest that current confidence-based

metrics do not reliably distinguish between candidates for experimental testing. Further work

is needed to assess computational designs more effectively, and to make pipelines like those

outlined here more predictive.

Figure 3: Designing selective binders for BCL-x$_L$ through computational negative
selection. a, Schematic of the selectivity procedure. After the ProteinMPNN design step
against the desired target, AlphaFold2 was used to predict the complex with both targets, MCL-
1 (red) and BCL-xL (blue). **b,** Designs were ranked for binding to both targets based on metrics
such as shape complementarity (Sc, shown in this scatterplot; for others supplementary Fig.
6). Designs predicted to be selective for BCL-x$_L$ are located in the bottom right corner. The
designs selected based on Sc is shown as a dark blue diamond, and all previously tested anti-
BCL-x$_L$ designs as cyan circles. **c,** FA data for the BCL-x$_L$ selective sequence based on Sc,
binding data against BCL-x$_L$ (dark blue, IC$_{50}$: 52 ± 3 nM) and MCL-1 (red, IC$_{50}$: 68 ± 80 μM).
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E3 targeting by grafting a SLiM for KLHL20 into the designed loop

With potent BCL-x$_L$ binders in hand, we turned to E3 targeting. The SLiM for KLHL20 adopts

a turn-like conformation upon binding[43]. Therefore, we hypothesised that grafting the SLiM into

the loop between the two helices of sc-apCC-2 might promote an active conformation and

improve binding affinity. We replaced the loop with either the natural SLiM in two different

lengths (short, 5 residues; or long, 11 residues) based on previous studies of KLHL20

binding[43], and we predicted models for the complexes with KLHL20 using AlphaFold2.

Encouragingly, the positions of the SLiM hot-spot residues matched those in a known

KLHL20/DAPK1 peptide complex[43]. However, the confidence of these initial predictions was

low with pLDDT of the grafted motif <60. Therefore, we applied the ProteinMPNN-

RosettaRelax protocol keeping the four central hot-spot residues of the SLiM fixed. This

increased the pLDDT to >90 (Fig. 4a). Both the natural and optimised sequences were tested

experimentally with two designs for each length. Biophysical characterisation and crystal X-

ray structures confirmed that the SLiM-based loops were tolerated (PDBs id 9TLS, 9TLT, Fig.

4b and Supplementary Fig. 10 and 11). In a competitive FA-binding assay for KLHL20 binding,

all designs had low micromolar IC$_{50}$ values, (direct titration of the tracer indicated a K$_D$ of 12

μM, see Supplementary Fig. 5, similar to previous reports[43]). Thus, the SLiM binding sequence

can be grafted into the loop of sc-apCC-2 to yield KLHL20 binders without compromising other

scaffold properties. Although the designs with the longer, 11-residue loops had higher affinities

as did the ProteinMPNN-optimised designs relative to the natural sequences, the differences

were small with all IC$_{50}$ values in the low µM range (Supplementary Fig.10; Supplementary
Table 13).

Figure 4: Incorporation of a SLiM for E3 ligase recruitment into the *de novo* scaffold.
a, A natural SLiM sequence (brown) was grafted into the loop of the scaffold, and AlphaFold2
used to predict the complex with the recognition domain of KLHL20. ProteinMPNN was used
to alter residues close the target. **b,** X-ray crystal structure of the sc-apCC2-KLHL20-3
(ProteinMPNN short-loop design; PDB id 9TLS), electron density shown around the loop at
sigma level 1. **c,** FA data for KLHL20 binding with the natural short-loop design (grey) (IC$_{50}$:
3.9 ± 0.2 µM) and the ProteinMPNN short-loop design (brown) (IC$_{50}$: 3.16 ± 0.18 µM).

BCL-x$_L$ and KLHL20 binders recruit their targets in a GFP-based degradation assay

To test the capacity of the monofunctional BCL-xL and KLHL20 binders to recruit their targets,
we used a previously established GFP-based degradation assay HEK293 cells (accompanying
paper). The assay follows degradation of transiently expressed protein and allows a medium-
throughput assessment of individual binders to inform those that could be combined in single
construct. In brief, to test the BCL-x$_L$ binders, HEK293 cells engineered to express a BCL-
x$_L$:GFP fusion protein stably were transfected with BCL-x$_L$ binders fused to the full-length
SPOP E3 ligase. 4 out of 8 binders showed significantly decreased GFP fluorescence
compared to the negative control. To test the KLHL20 binders, the same HEK293 cells were
transfected with the KLHL20 binders fused to an anti-GFP nanobody. All 4 binders lowered
GFP fluorescence (see Supplementary. Fig. 12).

Bifunctional designs are potent degraders of BCL-x$_L$ and induce apoptosis

After validating their degradation capacity individually, we combined the BCL-xL and KLHL20
binding sites into a single scaffold, and we tested for endogenous BCL-x$_L$ degradation in a
lung-cancer cell line (A549). For this, we chose the most potent and best performing BCL-x$_L$
binder from the GFP-based degradation assay, sc-apCC2-BCL-x$_L$-5, and combined it with the
KLHL20-binding module, sc-apCC2-KLHL20-3. These were configured in two ways (Fig. 5a):
one with two binding motifs combined within a single coiled-coil module; and a second with the
two monofunctional modules linked in tandem (Supplementary Fig. 13). For negative controls

we used both *de novo* binding proteins individually. As a positive control we used PROTAC

DT2216, which comprises small-molecule ligands for BCL-x$_L$ and VHL (Supplementary

Fig.14). A fluorescently labelled anti-BCL-x$_L$ antibody was used to measure endogenous BCL-

x$_L$ levels. Neither of the separate monofunctional controls significantly decreased BCL-x$_L$ levels

(Fig. 5b&d. However, both bifunctional designs showed significant decreases in BCL-x$_L$, just

as DT2216 (Fig. 5b&d). Addition of the proteasome inhibitor carfilzomib decreased the level of

degradation significantly, indicating a proteasome-depended mechanism (see Supplementary

Fig. 15). Combinations of other BCL-x$_L$ and KLHL20 binding sequences yield similar results,

highlighting the versatility of the scaffold and the binding site design (Fig. 5d and

Supplementary Fig. 16).

Figure 5: **Bifunctional binders cause endogenous BCL-x$_L$ degradation and apoptosis. a,**
Schematic of the molecules tested. All the designs use the same BCL-x$_L$- and KLHL20-binding
motifs. Negative controls are monofunctional (*i.e.*, contain only the BCL-x$_L$-binding motif (blue)
or the KLHL20-binding motif (brown). Small-molecule PROTAC DT2216 was used as a

positive control (the chemical structure is only a cartoon representation). **b,** Flow cytometry
results for the endogenous degradation, representative results for the negative control and
combined binders are shown. Histograms for design (blue) and mCherry control (black). **c,**
Flow cytometry results for the apoptosis assay Annexin V level on the x-axis, and DAPI signal
indicating membrane disruption on the y-axis. Representative results are shown for negative
control and combined binder. **d,** Degradation assay for native BCL-x_L in the A549 cell line.
BCL-x_L levels were calculated by the Overton positive method, average of at least three
biological repeats. Significance levels calculated with Welch t-test against the BCL-x_L binder.
e, Apoptosis assay, bars show combined early and late apoptosis averaged over at least three
biological repeats. Significance levels calculated with a Welch t-test against the BCL-x_L binder.
Significance levels are represented as N.S.: P > 0.05, ∗: P ≤ 0.05, ∗∗∗∗: P ≤ 0.0001. Parts of
this figure were made with BioRender.
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Depleting BCL-x_L should increase apoptosis. To test this, we used another 2D FACS
assay to measure (i) externalised phosphatidylserine indicative of early-stage apoptosis using
FITC-labelled Annexin V (x-axis), and (ii) cell viability using DAPI to monitor loss of membrane
integrity associated with late-stage apoptosis (y-axis)[53] (Fig. 5c). Overall apoptosis (combined
early and late) mirrored the protein-degradation assay (compare Fig. 5c&e): the individual
binders did not increase apoptosis above baseline, whilst the bifunctional helix-loop-helix
constructs showed significant increases, comparable to the addition of DT2216. These results
were mirrored in a ApoTox-Glo™ Triplex Assay, which assesses cell viability, cytotoxicity and
apoptosis events simultaneously (Supplementary Fig. 17). Combined, these experiments
show that transfection of bifunctionalised scaffolds into live cells causes robust degradation
and subsequent induction of apoptosis on a par with the small-molecule PROTAC.
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DISCUSSION
In summary, to develop *de novo*-protein-based PROTACs, we report the computational design
of a small, highly stable protein scaffold to present multiple epitopes that engage different
subcellular proteins. Using this, we introduce a binding site for the anti-apoptotic, cancer target
BCL-x_L and another for an E3 ubiquitin ligase, KLHL20. Effectively, this produces a *de novo*
protein based PROTAC that brings these proteins together in cells. Indeed, the bifunctional
proteins do cause degradation of BCL-x_L and increase apoptosis in a cancer cell line. The
designed proteins are characterised fully *in vitro* allowing them and the design methods to be
evaluated.
Recently, the incorporation of multiple, independent binding sites into a single *de novo*
scaffold has been reported[31]. Moreover, others have combined engineered or designed
proteins to render the EndoTag and GPlad systems for clearing proteins by internalisation into
cells, or via modification followed by proteolysis within cells, respectively[32,33,54]. In The
PROTAC field polypeptides have long been used as modules[7]. Recently, protein design tools
such as RFDiffusion[25] and ProteinMPNN[26] have been used to generate bifunctional
unstructured peptides that bind the androgen receptor and the E3, VHL, leading to degradation

of the former[55]. The design of a structured helical dimer comprising a SOS mimetic and p53

mimetic within a crosslinked dimer has been shown to engage MDM2 E3 ligase, and reduce

levels of RAS[56]

Our designs are distinct from the peptide-based systems, as they are stable, folded

proteins that simultaneously bind a target and an E3 ligase. Nonetheless, they still allow the

flexible introduction of different binding sites by grafting onto structured helical surfaces or

within the constrained loop. This promises opportunities in future to screen target—E3 pairings,

and to direct the orientation of the bound proteins for tailored ubiquitination. This *de novo*

design approach also offers possibilities for generating proteins that intervene in and direct

other post-translational modifications such as phosphorylation[57].

Our approach also facilitates full biophysical and structural characterisation of the

designs, as demonstrated by several co-crystal structures that we report here. In turn, this

helps critically assess the designs and design methods. For instance, we use motif grafting

embellished with computational sequence design using ProteinMPNN followed by AlphaFold2

structure predictions. In almost all cases, the addition of residues in direct contact with the

targets improves the AlphaFold2 and physical-scoring metrics. Interestingly, and as reported

by others[26,27] extending ProteinMPNN to residues outside of the binding site improves the

AlphaFold2 confidence metrics but does not alter the physical scoring metrics untouched

(Supplementary Fig. 19). Moreover, improvements suggested by *in silico* modelling and

assessment are not necessarily reflected in experimental measurements of binding constants.

For instance, for the BCL-2-family binders, extending the binding site beyond the natural, hot-

spot motif proved essential to achieve better binding; however, when targeting the KLHL20-

binding site there was no improvement beyond using the natural (SLiM) sequence. This raises

the potential problem of false positives in design pipelines. Moreover, and aligned with recent

large-scale *de novo* binder studies[58] and other benchmarks[59], we find that none of the AI

confidence predictors or physical scoring metrics correlate well with the measured

experimental binding affinities (Supplementary Fig. 20-24). Thus, in our view and corroborated

by others[58-60], the development of better *in silico* predictors of binding affinity, or simply better

ranking schemes for the best binders to test experimentally are key and important challenges

for the *de novo* design field.

MATERIALS AND METHODS

Computational loop design

The last and first six residues from the A and B chain of the previously published crystal

structure of apCC-Di-AB (PDB:7Q1T) respectively were used as a search query for

MASTER[46]. The original database made available with the publication was used. Results up

to 0.6 Å RMSD were separated by the number of residues in between the helices. Loops of 4

residues were the most common and the lowest RMSD hit (PDB id 2XPI residues 470-473)

was chosen as the starting structure for remodelling. Starting from the aligned and inserted

loop, 100 Rosetta remodel[47] trajectories were run, a total of 6 residues (the 4 loop residues

and 2 flanking residues) were mutated to any amino acid but cysteine. The remaining

sequence was fixed. The lowest energy model was selected for experimental testing.

Computational binding site design

For the BCL-x_L binder design, a selection of 6 residue motifs based on the natural binders

(BAD and BIM) were created. All motifs have the following structure Φ_1...L..Φ_2XD.F with

Φ_1 either Y,F or I, Φ_2 either F,I,M and X either G,S. The full list of motifs is shown in

supplementary table 10. These motifs were grafted onto a modified model of sc-apCC-2, so

that none of the core coiled-coil heptad positions (**a** and **d**) were altered. To accommodate the

binding sites better, 4 residues were added to each helical termini, the R@**a**, D@**e** pairs were

split and charges were more evenly distributed at **e** and **g** heptad positions as is the case in

apCC-Di[45]. This scaffold could accommodate the motifs at 3 locations resulting in a total of 54.

These models were aligned on 5 slightly modified AlphaFold2 predictions of natural

effector:protein complexes. A Rosetta script introduced a small angular shift in the effector

binding angle, the resulting 5 models are shown in supplementary figure 2. Subsequently, 4

different strategies were used to modify the sequence with a ProteinMPNN-RosettaRelax

pipeline: Strategy 1, no additional mutations were made; Strategy 2 non-motif, non-core and

non-loop residues within 6 Å from BCL-x_L are allowed to mutate; Strategy 3 all non-motif, non-

core and non-loop residues are allowed to mutate; Strategy 4 all non-core residues are allowed

to mutate (thus including the natural motifs and designed loop). The ProteinMPNN-

RosettaRelax pipeline consisted of 3 cycles of ProteinMPNN at a temperature of 0.2, grafting

of the top sequence onto the helix-loop-helix and a short relax following the

InterfaceRelax2019 script. After the final relax run, Rosetta scores including shape

complementarity and interface ΔG were calculated. In addition, an AlphaFold2 prediction was

made of each final sequence with and without a pre-generated MSA of BCL-x_L. Designs were

filtered based on pLDDT (>85 as a monomer and >90 as a complex) and a final selection was

made based pLDDT, pAE, ΔG or shape complementarity. All selected sequences with their

respective strategy and selection method are shown in supplementary table 4.

For MCL-1, the same method was employed but only the MPNN implementation in strategy 2

was used. Instead of strategy 1, the entire previously described binding site[48] was grafted onto

the modified sc-apCC-2 model. Selected sequences are shown in supplementary table 3.

For KLHL20, the previously designed loop was replaced with the natural SLiM sequences -

AGLPDLVGA- (short) or -AGLGLPDLVAKYNGA- (long). AlphaFold2 models were predicted

with a pre-genrated MSA for KLHL20. Subsequently the same three cycle ProteinMPNN-

RosettaRelax pipeline was used keeping the middle -PDLV- of the SLiM fixed.

All code and inputs are available from the labs Github page.

Computational selectivity screening

For the BCL-x_L and MCL-1 selectivity screening, AlphaFold2 predictions were made of the final

sequences of strategy 2 with the opposite target's MSA. In addition, the final sequences were

grafted on sc-apCC-2 and target complexes and subsequently relaxed and scored by Rosetta.

For pLDDT, pAE and Shape Complementarity the rank of each sequence against each target

was determined, sequences with the largest difference in rank favouring the desired target

were selected. All code and input are available from the labs Github page.

Solid-phase peptide synthesis and purification

All peptides used in this study (see Supplementary Table 1) were synthesised following

standard Fmoc automated microwave solid-phase peptide synthesis procedures with a Liberty

Blue (CEM) as described before[44,49]. N,N'-diisopropylcarbodiimide (DIC) and Oxyma Pure in

N,N-dimethylformamide (DMF) were used as activators and a 20% (v/v) solution of morpholine

or piperidine in DMF was used in the deprotection step. Peptides with acetyl (Ac) caps were

treated with pyridine or diisopropylethylamine and acetic anhydride. 5-carboxyfluorescein

(FAM) coupled peptides were prepared by coupling of 6-(amino)-hexanoic acid and FAM with

the standard DIC and Oxyma Pure in DMF mixture. Peptides were cleaved from the resin with

a trifluoracetic acid (TFA):water:triisopropysilane mixture in 95:2.5:2.5 (v/v) ratio at room

temperature. Subsequently, cleaved peptides were precipitated with ice-cold diethyl ether.

The freeze-dried peptides were dissolved in a water/acetonitrile mixture and purified with

reverse-phase HPLC using Water and acetonitrile with 0.1% (v/v) TFA as solvents. Peptide

purity was assessed by analytical HPLC (see Supplementary Fig. 25, 31, 33, 35, 37), and

matrix-assisted laser desorption/ionization-time of flight (MALDI-TOF) mass spectrometry (see

Supplementary Fig. 25, 30, 32, 34, 36).

Protein expression and purification

The genes encoding the designed binders and target proteins (BCL-x_L, MCL-1 and KLHL20)

were cloned into a pet28a vector with Kanamycin resistance. *E. coli* BL21 DE3 cells were

transformed with the plasmids (see Supplementary Tables 2-7 for protein sequences). Cells

were grown in Luria Broth at 37° C until an optical cell density of 0.6 was reached. Protein

production was induced by addition of isopropyl-β-D-thiogalactoside and cultures were kept at

20 ºC overnight. Afterwards, the cells were harvested by centrifugation and frozen until further

use.

For purification of the binders, the cells were resuspended in binding buffer (25 mM Tris, 300

mM NaCl, 10 mM imidazole pH 8.0) and lysed by sonication. The lysate was clarified by

centrifugation. The supernatant was applied on a His-trap column equilibrated with binding

buffer and washed with (30 mM imidazole. The protein was eluted with 300 mM imidazole.

Subsequently, the imidazole was removed by a PD-10 desalting column and incubated

overnight with TEV protease at room temperature. After His-tag cleavage, the protein solution

was reapplied on the His-trap column and flow-through was collected. This flow-through was

applied on a HiLoad 16/600 superdex75 column equilibrated in biophysics buffer (25 mM Tris,

150 mM NaCl, pH 7.4). The peak containing the monomeric proteins was collected and

concentrated for later use.

For BCL-x_L and MCL-1 protocols were followed as previously described[49]. The cells were

resuspended in lysis buffer (25 mM Tris, 500 mM NaCl, pH 8.0 cOmplete, Mini, EDTA free

protease inhibitor cocktail, Roche and 5 mg lysozyme and 3 mg DNAse, Roche). Afterwards,

they were sonicated and clarified via centrifugation. The soluble fraction was applied on a His-

trap HP column (Merck) pre-equilibrated with wash buffer (10 mM imidazole, 25 mM Tris, 500

mM NaCl, pH 8.0). The column was then washed four times with increasing concentration of

imidazole up to 100 mM, before a final elution with 400 mM imidazole. The protein solution

was dialysed overnight together with His-Ulp1 to remove the SUMO-tag. The next day the

solution was applied on the His-trap HP column and the flow-through was collected. This flow

through was collected and passed-through size exclusion chromatography with a HiLoad

26/60 Superdex 75 column. This column was previously equilibrated with 20 mM Tris 250 mM

NaCl, 0.5 mM DTT, 2.5% glycerol, pH 8.0. The fractions containing the monomeric protein

were pooled and concentrated before storage for later use. Protein purity and quality was

assessed by mass spectrometry (see Supplementary Fig. 26-27) and CD (see Supplementary

Fig. 29).

The cells that overexpressed KLHL20 overnight were resuspended in lysis buffer (50 mM

HPEES pH 7.5, 500 mM NaCl 5% glycerol, 0.5 mM TCEP, 5 mg lysozyme, 3 mg DNAse and

1 cOmplete, Mini, EDTA free protease inhibitor cocktail tablet). Afterwards, the cells were

sonicated and clarified by centrifugation. The supernatant was applied to 5 mL HisPur Ni-NTA

resin (Thermo Fisher), preequilibrated with binding buffer (50 mM HEPES pH 7.5, 500 mM

NaCl, 5% glycerol, 0.5 mM TCEP) and left rotating at 4 ºC overnight. The flow through was

collected using a peristaltic pump and the bead were washed four times with increasing

imidazole concentration (10 mM -100 mM). Subsequently, the protein was eluted with 300 mM

imidazole in the same buffer. The eluted protein was dialysed overnight with TEV protease,
before being applied again on the Ni-NTA beads. The supernatant was collected and
concentrated before storage for later use. Protein purity and quality was assessed by mass
spectrometry (see Supplementary Fig. 28) and CD (see Supplementary Fig. 29).

Circular dichroism spectroscopy

Circular dichroism (CD) spectroscopy data were collected on a JASCO spectropolarimeter
instrument fitted with a Peltier temperature controller. The binders were prepared to 20 µM
concentration in 20 mM Tris 150 mM NaCl, pH 7.4 buffer unless otherwise stated in figure
legends. Data were collected in a 1-mm quartz cuvette with a 200 nm to 260 nm wavelength.
The following instrument settings were used: band width, 1 nm; data pitch, 1 nm; scanning
speed, 100 nm/min; response time 1 s. Each spectrum is the background subtracted average
of 8 scans. For the thermal denaturation scans, the circular dichroism signal was followed at
222 nm wavelength while increasing the temperature from 5 ºC to 95 ºC at a ramp rate of 1
ºC/min. BCL-x_L, MCL-1 and KLHL20 were measured in 10 mM K_2HPO_4 adjusted with NaOH
to pH 7.4 at 50 µM protein concentration. The spectra were normalized to mean residue
ellipticities (deg cm^2 dmol^{-1}res^{-1}) by normalizing for concentration of peptide bonds and the cell
path length using equation $MRE = \frac{\theta \times 10^6}{c \times l \times n}$ with θ the measured difference in absorbed circularly
polarized light in mdeg, c the concentration in µM, l the path length in mm and n the number
of amide bonds in the proteins.

Analytical size exclusion chromatography

526 Analytical size exclusion chromatography was performed on a JASCO HPLC system with a
527 superdex 75 increase 10/300 column. 20 µL of protein solution at a concentration of 100 µM
528 in 20 mM Tris, 150 mM NaCl, pH 7.4 was injected at 0.5 mL/min. The UV absorbance at 230
529 nm was recorded, the background was subtracted and the normalized signal was plotted in
530 function of elution volume.

Analytical ultracentrifugation

Sedimentation equilibrium experiments were performed on a Beckman Optima X-LI analytical
ultracentrifuge with an An-60-Ti rotor (Beckman-Coulter) and data was fitted using SEDPHAT
software[61] to single-species model. Monte Carlo analysis was performed to yield 95%
confidence limits. A peptide concentration of 100 µM in PBS (8.2 mM sodium phosphate
dibasic, 1.8 mM potassium phosphate monobasic, 137 mM NaCl, 2.4 mM KCl, pH 7.4) was
used. The sample was spun at 52000, 56000 and 60000 RPM after 8-hour equilibration at
each speed, the measurement at each speed was duplicated.

Competitive fluorescence anisotropy assay

Competitive fluorescence anisotropy assay

The competitive fluorescence anisotropy experiment were performed following previously

described procedures[49]. Each experiment was run in triplicate and the fluorescence anisotropy

measured using a CLARIOstar plus plate reader (BMG Labtech), with excitation at 482nm

(bandwidth = 16nM), emission at 530nm (bandwidth = 40nm) and polarised dichroic mirror at

504nm. For the direct titration assay, stock concentrations of 1mg/ml peptide were made in

DMSO and then further diluted to a working stock of 100nM in FA buffer (20mM tris, 150mM

NaCl pH7.4 1mM DTT 0.01% triton x100) for use in the assay. For MCL-1 and BCL-x_L

experiments, the target protein concentration was fixed at 150 nM and tracer concentration

fixed at 25 nM. For KLHL20 experiments, KLHL20 concentration was fixed at 8 µM and 83.3

nM tracer concentration. The competitor protein was titrated in.

Perpendicular (P) and parallel (S) intensities of the control wells were averaged and deducted

from each corresponding samples to give the corrected values, P_{corr} ($P_{corr} = P_{sample} - P_{av. control}$)

and S_{corr} ($S_{corr} = S_{sample} - S_{av. control}$). The total sample intensities (I) and anisotropies (r) were

calculated with the follow equations: $I = (2 \times P_{corr}) + S_{corr}$, $r = (S_{corr} - P_{corr}) / I$

The points for each competition curve were normalised between 0 and 1. The obtained values

were plotted against competitor concentrations and fit to a logistic function of the form $Y = A2$

$+ (A1 - A2) / (1 + (x/IC_{50})^p)$ to determine the half-maximal inhibitory concentration (IC_{50}) of the

peptide competitor (where A2 is the upper asymptote and A1 the lower asymptote).

Isothermal Titration Calorimetry

Isothermal titration calorimetry (ITC) experiments were carried out using a MicroCal PEAQ-

ITC system (Malvern Panalytical) at 37 °C. A stock solution of BCL-xL was dialyzed into ITC

buffer overnight (20 mM Tris, 150 mM NaCl pH 7.4), and the same buffer was employed to

dissolve a solid portion of the tested binder. For each experiment, initially, the cell was filled

with 275 µl of binder (20 µM) and the syringe was loaded with the BCL-xL at 200 µM

concentration. An initial injection of 0.4 µL was then followed by 18 injections of 2 µL, every

150s, with a constant syringe rotation speed of 750 rpm throughout. The signal for the enthalpy

of dilution of the protein into buffer was independently measured in a control titration

experiment and then subtracted from the experimental binding traces. NITPIC[62] was used to

integrate the injections. The data was then fitted with SEDPHAT software[61] to extract K_D, $\Delta G°$,

$\Delta H°$ and $-T\Delta S°$ using an adjusted single-site binding model.

Crystallisation trials

Protein crystals were grown using a sitting-drop, vapor diffusion method with commercial

sparse matrix screens. 0.3 µL of a concentrated protein solution or 1:1 mixture of proteins in

case of the binders was mixed with 0.3 µL of the screening solution in MRC 96 well plates.

The plates were incubated at 20 ºC until protein crystals were observed. The crystallisation
condition for each structure can be found in Supplementary table 15. The crystals were
mounted and transferred to a cryoprotecting solution made of the screen supplemented to 25%
glycerol before flash freezing in liquid nitrogen.

The proteins were diffracted at Diamond light source or the European Synchrotron Radiation
Facility. Data processing was done on the beamline with either XDS[63] or Dials[64]. Aimless[65] was
used for scaling. Molecular replacement was done with PHASER[66] using AlphaFold2 models.
Phenix Refine[67] was used for refinement of the structures using translation/liberation/screw
(TLS) parameters for each chain. Data and refinement quality statistics can be found in
supplementary table 16.

Cell culture
All cell culture procedures were carried out according to standard procedures. In brief, all cell
lines were maintained at 37 °C in an atmosphere of 5% CO_2 and ≥95% humidity. HEK293T
cells were cultured in Dulbecco's Modified Eagle Medium (DMEM; Gibco™) supplemented
with 10% foetal bovine serum (FBS), while A549 cells were grown in Nutrient Mixture F-12
Ham medium (Merck) supplemented with 10% FBS. DNA transfections were performed using
the cationic lipid reagent TransIT-2020 (Mirus Bio).

Stable GFP–Bcl-x_L cell lines (see Supplementary Table 8) were generated in a previous study
(accompanying paper) through antibiotic selection followed by sorting of live GFP-positive cells
for subsequent propagation.

Flow cytometry assay of degradation of GFP-BCL-x_L
BCL-x_L binders were synthetized in pcDNA3.1Hygro(+) plasmid (GenScript) in such a way that
they are preceded by a single FLAG tag and followed by the SPOP E3 ligase and mCherry
with a T2A self-cleaving peptide sequence. The KLHL20 binder constructs were in the same
plasmid preceded by a FLAG tag and anti-GFP nanobody and followed by the same mCherry
T2A combination. Full protein sequences are found in Supporting Table 8.

The flow cytometry assay was performed as previously described (accompanying paper).
Briefly, on day 1, cells were seeded at a density of 300,000 per well supplemented DMEM
without antibiotics. On day 2, cells were transfected following the manufacturer's instructions,
with a ratio of 0.5 µg DNA to 1.5 µL transfection TransIT-2020. On day 4 (48 hours after
transfection), cells were washed with PBS, trypsinized, resuspended in FACS buffer and
stained with DAPI (1 µg/mL) prior to flow cytometry on a Attune NxT instrument (ThermoFisher
Scientific). The data was analysed with FlowJo v10. Events were gated based on fluorescence
of cells stably expressing GFP-BCL-x_L and transfected with an mCherry-only control (quadrant

Q2). Degradation of BCL-x$_L$ was indicated by reduced GFP fluorescence intensity and a shift

to Q1. Results represent at least three independent experiments and are expressed as the

percentage of remaining GFP-BCL-x$_L$ (100 x Q2/(Q1 + Q2) ± standard deviation). Statistics

were calculated using a two-sided Welsch's T-test. Significance levels are represented as

N.S.: P > 0.05, ∗: P ≤ 0.05, ∗∗: P ≤ 0.01, ∗∗∗: P ≤ 0.001, ∗∗∗∗: P ≤ 0.0001.

Flow cytometry assay of endogenous BCL-x$_L$ degradation

The protein constructs for the endogenous degradation assays were in the same

pcDNA3.1Hygro(+) plasmid (GenScript). Constructs had N-terminal FLAG tag and were

followed by mCherry preceded by a T2A self-cleaving peptide.

The flow cytometry assay was performed as previously described (accompanying paper).

A549 cells were cultured as above and fixed in 4% formaldehyde 48 hours after transfection

or 48 hours after treatment with 1 μM concentration of DT2216 (#37311, Cayman Chemical).

Then, following a PBS wash the cells were permeabilized with cold methanol for 15 minutes

on ice and incubated overnight at 4 ºC with BCL-x$_L$ (54H6) Rabbit mAb (Alexa Fluor 488

Conjugate) antibody and a Rabbit IgG Isotype control, Alexa Fluor 488 Conjugated (Cell

Signaling, BS-0295P-A488-BSS-100uL Startech Scientific Ltd, respectively). The cells were

washed and resuspended in PBS for flow cytometry measurements. For the proteasome

inhibitor experiments cells were treated with 20 μM carfilzomib for 24 hours prior to

measurements (Carfilzomib (PR-171), #A1933, APExBIO). The data was analysed with

FlowJo v10. Results were plotted as events of BCL-x$_L$ Alexa 488 channel. The percentage of

cells that lost fluorescence was calculated by subtracting out the mCherry control using the

Overton positive method. Data are from at least 3 independent experiments Statistics were

calculated using a two-sided Welsch's T-test. Significance levels are represented as N.S.: P >

0.05, ∗: P ≤ 0.05, ∗∗: P ≤ 0.01, ∗∗∗: P ≤ 0.001, ∗∗∗∗: P ≤ 0.0001.

Flow cytometry apoptosis assay

The same DNA constructs as in the endogenous degradation assay were used. The flow

cytometry apoptosis assay was performed as described above (accompanying paper). Briefly,

48 hours before flow-cytometry measurements A549 cells were transfected with degraders or

treated with DT2216 at 1 μM (#37311, Cayman Chemical). Then, cells were detached, washed

with PBS and incubated for 30 minutes to allow recovery. Afterwards, the cells were stained

with FITC-conjugated Annexin V (BioLegend) in accordance with the manufacture's protocol

except for a longer 45-minute incubation time. Next, the cells were washed in 1x binding buffer

and resuspend in 300 μL of binding buffer containing DAPI (BD Pharmingen). Cells,

undergoing early apoptosis have externalized phosphatidylserine binding to Annexin in a

calcium-dependent manner. Cells in late-stage apoptosis lose membrane integrity and get

stained by DAPI. Apoptosis was calculated as the sum of cells in early and late stages and expressed as percentage of total cell count.

ApoTox-Glo™ Triplex Assay

Viability, cytotoxicity and apoptosis assays were performed using the Promega kit according to the provided protocols, with the exception of additional filters to eliminate the mCherry fluorescence background; fluorescence filter wavelengths were 485 ± 10 nm for excitation and 520±20 nm for emission for the cytotoxicity measurements, and 400 ± 20 nm for excitation and 505±20 nm for emission for the viability measurements. Luminescence readings at 545±40 nm were used for the apoptosis measurements.

ACKNOWLEDGMENTS

This work was primarily supported by grants from the BBSRC (BB/V006231/1, BB/V006703/1 BB/V008412/1, and BB/V008412/2), with additional support from BB/V003577/1, BB/V003577/2 and BB/Y007816/1. X-ray diffraction experiments were supported by Diamond beam time awarded under proposal number MX34438, MX31440 and MX37593 and ESRF beamtime awarded under proposal number MX2373. DTH was supported by Cancer Research UK core funding (A29252). We thank Simon Coulton and Andrew Lovering for assistance with crystallographic data acquisition. We thank Diana Gimenez for preparation of the KLHL20 tracer used in FA KLHL20 competition assays. Some Figure elements were created with BioRender (https:// BioRender.com/8n9fh89, https://BioRender.com/eg0oktl, https://BioRender.com/l2psuaa).

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