

Toxicity Management in CAR T cell therapy for B-ALL: Mathematical modelling as a new avenue for improvement.

Shalla Hanson,^{1,2} David Robert Grimes,³ Jake P. Taylor-King,^{4,5} Benedikt Bauer,⁶ Pranav I. Warman,⁵ Ziv Frankenstein,⁵ Artem Kaznatcheev,⁵ Michael J. Bonassar,⁵ Vincent L. Cannataro,⁷ Zeinab Y. Motawe,⁸ Ernesto A. B. F. Lima,⁹ Sungjune Kim,¹⁰ Marco L. Davila,¹¹ and Arturo Araujo⁵

¹*Department of Mathematics, Duke University, Durham, NC, USA*

²*Laboratoire Jacques-Louis Lions, Université Pierre et Marie Curie & INRIA, Paris, France*

³*Cancer Research UK / MRC Institute for Radiation Oncology,
Gray Labs, University of Oxford, Oxford, OX3 7DQ, UK*

⁴*Mathematical Institute, University of Oxford, Oxford, OX2 6GG, UK*

⁵*Department of Integrated Mathematical Oncology,*

H. Lee Moffitt Cancer Center and Research Institute, Tampa, FL, USA

⁶*Department of Evolutionary Theory, Max Planck Institute for Evolutionary Biology, D-24306 Plön, Germany*

⁷*Department of Biology, University of Florida, Gainesville, FL, USA*

⁸*Department of Molecular Medicine, University of South Florida, College of Medicine, Tampa, FL, USA*

⁹*Institute for Computational Engineering and Sciences (ICES),*

The University of Texas at Austin, Austin, TX, USA

¹⁰*Department of Radiation Oncology, H. Lee Moffitt Cancer Center and Research Institute, Tampa, FL, USA*

¹¹*Department of Blood and Marrow Transplantation,*

H. Lee Moffitt Cancer Center and Research Institute, Tampa, FL, USA

(Dated: April 22, 2016)

Abstract. Advances in genetic engineering have made it possible to reprogram individual immune cells to express receptors that recognise markers on tumour cell surfaces. The process of re-engineering T cell lymphocytes to express *Chimeric Antigen Receptors* (CARs), and then re-infusing the CAR-modified T cells into patients to treat various cancers is referred to as CAR T cell therapy. This therapy is being explored in clinical trials - most prominently for B Cell Acute Lymphoblastic Leukaemia (B-ALL), a common B cell malignancy, for which CAR T cell therapy has led to remission in up to 90% of patients. Despite this extraordinary response rate, however, potentially fatal inflammatory side effects occur in up to 10% of patients who have positive responses. Further, approximately 50% of patients who initially respond to the therapy relapse. Significant improvement is thus necessary before the therapy can be made widely available for use in the clinic.

To inform future development, we develop a mathematical model to explore interactions between CAR T cells, inflammatory toxicity, and individual patients' tumour burdens *in silico*. This paper outlines the underlying system of coupled ordinary differential equations designed based on well-known immunological principles and widely accepted views on the mechanism of toxicity development in CAR T cell therapy for B-ALL - and reports *in silico* outcomes in relationship to standard and recently conjectured predictors of toxicity in a heterogeneous, randomly generated patient population. Our initial results and analyses are consistent with and connect immunological mechanisms to the clinically observed, counterintuitive hypothesis that initial tumour burden is a stronger predictor of toxicity than is the dose of CAR T cells administered to patients.

We outline how the mechanism of action in CAR T cell therapy can give rise to such non-standard trends in toxicity development, and demonstrate the utility of mathematical modelling in understanding the relationship between predictors of toxicity, mechanism of action, and patient outcomes.

I. INTRODUCTION

Traditionally three major modalities have dominated in cancer therapy: surgery, radiation, and chemotherapy. While these interventions have lengthened survival times for cancer patients, they continue to undergo significant evolution in hopes of eventually finding a cure. Recently, efforts to find effective treatments without the severe side effects of traditional chemo- and radiation therapies have given rise to a new class of *targeted* drugs, which can distinguish potentially harmful cells from those that are likely healthy [1]. However, even with these continual advancements, cancer is still a challenge to treat. This is due in part to the fact that

cancers often become resistant to therapies, and in part to the fact that even the best therapies often cause severe side effects that prevent high-dose or prolonged administration. These difficulties prompted interest in harnessing the power of the human immune system, which remarkably has both the ability to identify and attack specifically pathogenic cells and the ability to adapt to changing populations of cancer cells, to enhance treatments currently available for cancer patients. Today, *immunotherapy* presents an exciting new frontier in cancer therapy, replete with the possibility of reprogramming the human immune system itself to recognise and fight against cancer [2–4].

Toxicity in cancer therapy. Chemo- and radiation therapies work by exploiting the fact that certain behaviours, in particular cell division, are more common in cancerous tissue than in healthy tissue. These therapies damage cells much more severely when they begin certain cellular processes, so if cancer cells undergo these processes more frequently than healthy cells do, more cancer cells are damaged by the therapy than healthy cells. Unfortunately, most healthy cells, to some extent, still undergo the same cellular processes exploited by traditional therapies and are thus indiscriminately damaged when they do.

Targeted agents, on the other hand, typically have a type of biochemical ‘switch’ which is turned ‘on’ when they encounter potentially malignant cells but remains ‘off’ otherwise. Ideally, the targeted agent is then toxic only to cells identified as harmful. The efficacy as well as the amount of toxicity caused by direct injury of healthy tissue thus depends on the specificity of the targeted agent. That is, the more malignant cells the agent is able to correctly identify as harmful and kill, the more effective the therapy. Conversely, the more healthy cells the agent is able to correctly identify as innocuous and leave alone, the lower the toxicity. Advances in targeted therapies have focused for some time on increasing the specificity of targeted agents, and include, for example, the addition of multiple biochemical switches to help identify malignant cells more accurately [5].

As promising as these therapies may be, this has unfortunately unveiled a second mechanism of toxicity development due, not to direct killing of healthy cells by the drug, but instead due to cancer cells being killed *too rapidly*. While killing cancer cells is precisely the intended outcome of these therapies, an extremely high rate of cell death within the body, regardless of cell type, can have severe consequences causing, for example seizures, renal failure, arrhythmias, and death [6]. This phenomenon is referred to as Tumour Lysis Syndrome (TLS) and has been increasing in incidence as cancer therapies become more and more targeted [7].

Another cell-death-associated side effect often seen in targeted immunotherapies is Cytokine Release Syndrome (CRS), which occurs when immune cells secrete massive quantities of inflammatory cytokines upon identifying pathogenic cells. Toxicities caused by CRS vary in severity but are often life-threatening, and include dangerously high fevers, precipitous drops in blood pressure, hypoxia, and neurological disorders [8].

Recent studies on toxicity associated with CD19-targeted CAR T cell therapy for B-ALL have reported very little correlation between toxicity and the dose of CAR T cells received by patients [9]. On the other hand, inflammatory toxicity *has* been reported to be much more highly correlated with individual patients’ tumour burdens than with the dose of CAR T cells administered [10, 11]. Nevertheless, despite the enigmatic toxicity profiles seen in these patients, a number of patients receiving the therapy have also shown sustained complete re-

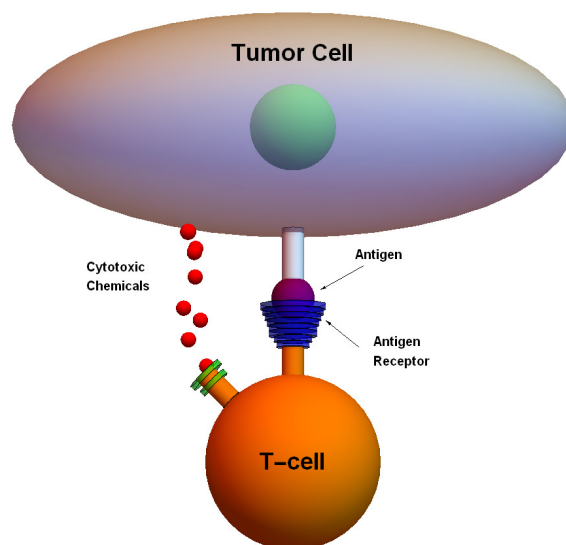


Figure 1: Chimeric Antigen Receptor (CAR)-modified T cell interacting with its cognate antigen on the surface of a tumour cell.
A CAR-modified Cytotoxic T cell re-engineered to express a receptor specific to a tumour cell antigen identifies a tumour cell and secretes cytotoxic molecules which cause lysis of the tumour cell.

sponses with minimal toxicity development [12]. It is clear that in order for these types of outcomes to be possible for a broader patient population, we must first develop more a sophisticated understanding of toxicity development in targeted immunotherapies.

Nonetheless, due to the life-threatening results experienced by others, it is clear that major improvements must be made in toxicity management before such therapies can be safely administered. The following section reviews current research on mechanisms of action and toxicity development in CAR T cell therapy in B-ALL.

CAR T cell therapy for B-ALL. The advent of stem-line engineering practices, which can endow cytotoxic (killer) T cells with the ability to identify and subsequently attack malignant cells [13], has propelled rapid progress in cancer treatment. This concept is the basis of CAR T cell therapy. Under this paradigm, T cells are collected from a patient or donor and genetically re-engineered to express Chimeric Antigen Receptors (CARs), which recognise tumour-specific markers called antigen. These cells are then stimulated to divide *in vitro* until a sufficiently large population (often on the order of 10^9 cells) is produced, and are then intravenously infused back into the patient [9].

CAR T cell approaches for B cell tumours have been tentatively explored most often involve CARs specific for the B cell CD19 antigen [14–16]. CD19 is expressed on normal B cells, and is rarely lost due to mutations in B cell malignancies such as low-grade chronic lymphocytic

We will define the inflammatory response as $I(t)$ and the B-ALL tumour burden as $B(t)$. Initially and for simplicity, we make the assumption that tumour growth is logistic. We note, however, that for some patients, Gompertzian or other growth laws may give more accurate representations of tumour growth, and this will be considered in future work. For the present study, we write

$$\frac{dB}{dt} = r_1 B \left(1 - \frac{B}{k_1}\right) - d_1 B C_e \quad (2)$$

where r_1 and k_1 are constants of logistic growth, and d_1 a constant associated with the killing potential of C_e cells.

The immune response is modelled to account for the fact that CAR-modified T cells secrete inflammatory molecules when they interact with CD19-positive B cells. While these inflammatory molecules decay naturally, if this decay is not fast enough, clinical interventions are sometimes necessary to mitigate inflammatory toxicity. Here we denote the immunosuppressant drug dose by $D(t)$. We may now write the immune response to treatment and modulation as

$$\frac{dI}{dt} = p_1 B C_e - d_2 I - D(t) \quad (3)$$

where p_1 , and d_2 are production and decay constants respectively. Finally, we represent the respective populations of Cytotoxic and Helper T cells with the following system of ODEs:

$$\frac{dC_e}{dt} = 2^n a_1 B C_m I (1 + a_2 H_e) - d_3 C_e \quad (4)$$

$$\frac{dC_m}{dt} = r_2 C_m (1 - \mathcal{L}/\ell)^+ - a_1 B C_m (1 + a_2 H_e) \frac{I^2}{I^2 + b^2} \quad (5)$$

$$\frac{dH_e}{dt} = 2^n a_3 B H_m \frac{I^2}{I^2 + b^2} - d_4 H_e \quad (6)$$

$$\frac{dH_m}{dt} = r_3 H_m (1 - \mathcal{L}/\ell)^+ - a_3 B H_m \frac{I^2}{I^2 + b^2} \quad (7)$$

$$\frac{dL}{dt} = p_2 + r_4 L (1 - \mathcal{L}/\ell)^+ - d_5 L \quad (8)$$

where n is the average number of divisions a differentiating T cell undergoes before becoming exhausted, b is the concentration of inflammatory cytokines which induces half-maximal differentiation rates in memory T cells, ℓ represents the normal concentration of lymphocytes, and a_i , p_i , r_i , and d_i are rate constants associated respectively with activation, production, replication, and decay of the lymphocyte populations. The 2^n factor in the activation of memory T cells is used to account for the fact that T cells undergo successive divisions while differentiating from the memory to effector phenotype. The symbol $+$ indicates the positive component, so $x^+ = \max\{x, 0\}$. The term $(1 - \mathcal{L}/\ell)^+$ thus quantifies the degree (or absence) of lymphopenia. The Hill function, $\frac{I^2}{I^2 + b^2}$, was chosen, firstly, to maintain a realistic bound on the activation rate of T cells, and secondly to include the presence of a homeostatic buffer which allows small changes

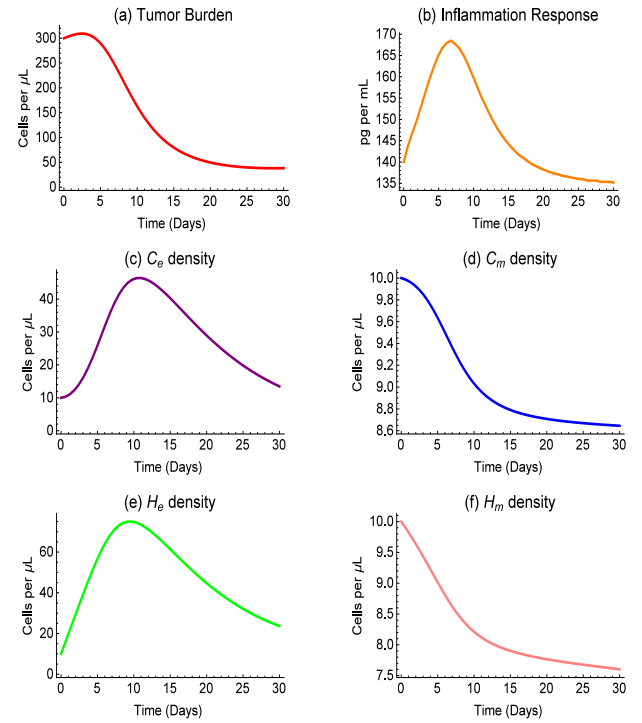


Figure 3: Simulated patient response: A simulated standard patient is administered CAR T cells on day 0 and monitored over 30 days. The tumour burden is depicted in (a), the inflammatory response in (b), and respective T cell populations are depicted in (c)-(e) inclusive. Simulation details are outlined in the text.

of cytokine levels within the normal range without creating massive bursts in T cell activation.

Using these forms, we can simulate the effects of infusing different relative populations of CAR-modified T cells, immuno-suppression, and the interplay of different phenotypes in CAR T cell therapy-related toxicity. A simple outline of the model is shown in Figure 2.

Simulation outline. The system of equations outlined in (1)–(8) was solved using an explicit 4th order Runge–Kutta scheme. For the simulation in Figure 3, the initial conditions were chosen as listed in Table I, and parameters chosen as listed in Table II.

Table I: Initial Conditions

Variable	Symbol	
Effector	$E(t)$	
Target	$T(t)$	140 $\frac{pg}{mL}$
CAR Memory CTLs	$C_m(t)$	10 $\frac{cells}{\mu L}$
CAR Effector CTLs	$C_e(t)$	10 $\frac{cells}{\mu L}$
CAR Memory Helper T cells	$H_m(t)$	10 $\frac{cells}{\mu L}$
CAR Effector Helper T cells	$H_e(t)$	10 $\frac{cells}{\mu L}$
Other lymphocytes	$L(t)$	1600 $\frac{cells}{\mu L}$

Table II: Parameter Values

Parameter	Value	Unit
n	6	<i>none</i>
r_1	3×10^{-3}	$\frac{1}{h}$
r_2	0.1	$\frac{1}{h}$
r_3	0.1	$\frac{1}{h}$
r_4	0.1	$\frac{1}{h}$
d_1	2×10^{-4}	$\frac{\mu L}{cell \cdot s \cdot h}$
d_2	1.5	$\frac{1}{h}$
d_3	4×10^{-3}	$\frac{1}{h}$
d_4	4×10^{-3}	$\frac{1}{h}$
d_5	2×10^{-4}	$\frac{1}{h}$
p_1	.002	$\frac{pg \cdot \mu L^2}{mL \cdot cells^2 \cdot h}$
p_2	0.4	$\frac{cells}{\mu L}$
a_1	4×10^{-7}	$\frac{\mu L}{cell \cdot s \cdot h}$
a_2	2	$\frac{\mu L}{cells}$
a_3	8×10^{-5}	$\frac{\mu L}{cell \cdot s \cdot h}$
b	800	$\frac{pg^4}{mL^4}$
ℓ	1600	<i>cells</i>
k	4800	<i>cells</i>

For clinical data simulations, a heterogeneous patient population ($N = 200$) was generated by randomly selecting parameter values and initial background endogenous lymphocyte concentrations either uniformly distributed between 75% and 125% of the mean values given above, or normally distributed about the means above, with standard deviations equal to 25% of the mean. Any non-physical (negative) parameter values generated were corrected to be within physical ranges. Initial tumour burden per patient was randomly selected from a uniform distribution between 1 and 1000 cells/ μL , and initial doses of each of the four CAR-modified T cell populations were similarly randomly selected from uniform distributions between 1 and 30 cells/ μL (such that the total CAR T cell dose administered per patient varies in the range of 1 to 120 cells/ μL).

III. IN SILICO EXPERIMENTAL RESULTS

Detailed results for a single simulated patient are shown in Figure 3. For this patient, we see that CAR T cells undergo significant expansion and effector differentiation after infusion into patients with CD19⁺ B-ALL, and inflammatory responses peak between 5-10 days post-infusion concurrent with a rapid decrease in tumour burden. Subsequently, as the tumour burden declines, effector T cell populations decay and inflammation subsides. Further, we see that while the tumour burden may remain low for some time, the CAR T cell population continues to decline, predisposing the patient to relapse. These *in silico* results are consistent with clinical outcomes reported in [8, 10, 12].

Patient outcomes were also observed *in silico* in a ran-

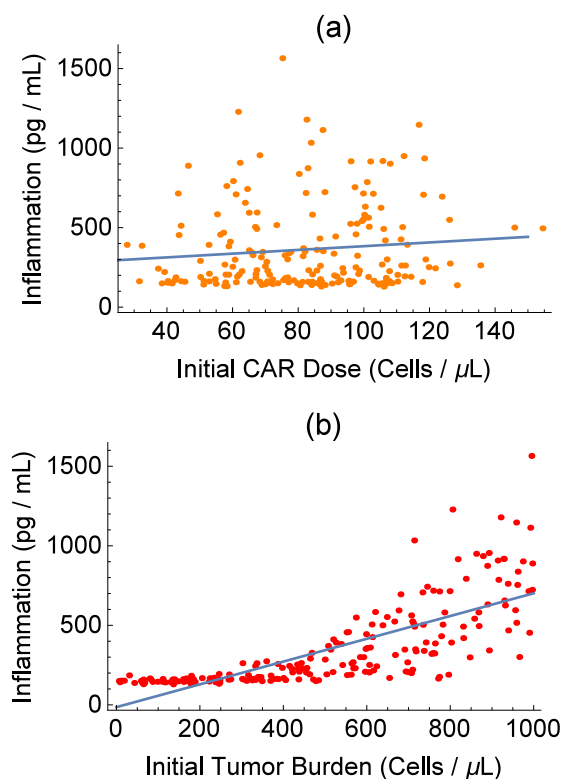


Figure 4: **Simulated Clinical Data:** Inflammatory molecules are secreted by CAR T cells when they interact with tumour cells, potentially resulting in life-threatening toxicities. (a) Maximum degree of inflammation experienced by patients ($N=200$) with initial CAR T cell dose in a simulated patient population. Linear best-fit is shown in blue, with a p-value 0.1412 suggesting no correlation between CAR load and toxicity. (b) Maximum degree of inflammation experienced by patients ($N=200$) with initial tumour burden in a simulated patient population. Linear best-fit is shown in blue, with a p-value 5.3×10^{-38} , indicating extremely high correlation between tumour burden and toxicity. Data shown above was simulated from a patient population with individual characteristics (parameter values) chosen to be uniformly distributed about the mean. Simulations from a normally distributed patient population were also carried out and yield similar results.

domly generated generated population ($N=200$) as outlined in the methodology. Consistent with the clinical results reported in [8–10, 12], we find that while inflammatory toxicity is only minimally correlated with the CAR T cell dose administered, it is in fact highly correlated with patients' initial tumour burden (See Figure 4).

IV. DISCUSSION AND CONCLUSION

The observation that efficacy and toxicity are more highly correlated with tumour burden than with the ini-

tial dose of CAR T cells administered to patients [8–10, 12] is contrary to what is observed with most pharmaceuticals [27]. Specifically, in non-targeted therapies, including chemo- and radiotherapy, toxicity results primarily from direct injury of healthy cells (or their daughter cells) by the therapeutic agent alone. As a result, the toxicity experienced by patients is independent of the size or density of the tumour. On the other hand, in CAR T cell therapy for B-ALL, toxicity results primarily from indirect injury of healthy tissue due to excessive cytokine secretion by CAR T cells when they encounter tumour cells (as depicted in Figure 1).

Our results demonstrate that this well-known mechanism of inflammatory cytokine secretion [28] is sufficient to give rise to tumour-burden-correlated toxicity as suggested in [8]. Our results also support the hypotheses of [9] that CAR T cell dose alone correlates poorly with the degree of toxicity experienced by patients, and along with the work of [8–10, 12], suggests that to best take advantage of this exciting new technology, we must also take steps to advance our practices for managing toxicity in targeted immunotherapies.

Mathematical analysis is a valuable tool for deepening our understanding of how the mechanisms of action of particular therapies connects to patient outcomes in the clinic [29]. It can potentially offer insight into how protocols may be modified based on individual patient characteristics to decrease toxicity, increase persistence

of CAR T cell populations, and potentially decrease relapse rates in B-ALL. While the simple model presented here is at a very early stage of development, it illustrates the utility of mathematical modelling. Future work will focus on refining this approach, increasing precision in model predictions through experimental validation, and expansion to solid and other more heterogeneous tumours for which a single targetable antigen is not preserved in the tumour cell population.

V. ACKNOWLEDGEMENTS

The group would like to kindly thank H. Lee Moffitt Cancer Center and Research Institute and in particular Alexander R. A. Anderson for the organisation and funding of the 5th IMO workshop: Immune Cancer; and also Jean Clairambault and David Basanta for generously offering their guidance and expertise. SH received funding in part from the NSF under grant reference number DMS-0943760; and in part from NESCent, TriCEM, the Embassy of France in the United States, and INRIA-Paris. JPT-K received funding from the EPSRC under grant reference number EP/G037280/1. DRG is funded by CR:UK grants C5255/A15935 and C53469/A19834. B.B is funded by the Max Planck Society. EABFL is funded by the NSF under Grant DMS-1115865. AA is funded by DoD grant 14091003.

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