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1 **The within-subject application of diffusion tensor MRI and**
2 **CLARITY reveals brain structural changes in *Nrxn2* deletion**
3 **mice**

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30 **Abstract**

31 **Background**

32 Of the many genetic mutations known to increase the risk of autism spectrum
33 disorder, a large proportion cluster upon synaptic proteins. One such family of
34 presynaptic proteins are the neurexins (NRXN), and recent genetic and
35 mouse evidence has suggested a causative role for *NRXN2* in generating
36 altered social behaviours. Autism has been conceptualised as a disorder of
37 atypical connectivity, yet how single-gene mutations affect such connectivity
38 remains under-explored. To attempt to address this, we have developed a
39 quantitative analysis of microstructure and structural connectivity leveraging
40 diffusion tensor MRI (DTI) with high-resolution 3D imaging in optically cleared
41 (CLARITY) brain tissue in the same mouse, applied here to the *Nrxn2α*
42 knockout (KO) model.

43 **Methods**

44 Fixed brains of *Nrxn2α* KO mice underwent DTI using 9.4T MRI, and diffusion
45 properties of socially-relevant brain regions were quantified. The same tissue
46 was then subjected to CLARITY to immunolabel axons and cell bodies, which
47 were also quantified.

48 **Results** DTI revealed decreases in fractional anisotropy and increases in
49 apparent diffusion coefficient in the amygdala (including the basolateral
50 nuclei), the anterior cingulate cortex, the orbitofrontal cortex and the
51 hippocampus. Radial diffusivity of the anterior cingulate cortex and
52 orbitofrontal cortex was significantly increased in *Nrxn2α* KO mice, as were
53 tracts between the amygdala and the orbitofrontal cortex. Using CLARITY, we

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54 find significantly altered axonal orientation in the amygdala, orbitofrontal
55 cortex and the anterior cingulate cortex, which was unrelated to cell density.

56 **Conclusions**

57 Our findings demonstrate that deleting a single neurexin gene (*Nrxn2a*)
58 induces atypical structural connectivity within socially-relevant brain regions.
59 More generally, our combined within-subject DTI and CLARITY approach
60 presents a new, more sensitive method of revealing hitherto undetectable
61 differences in the autistic brain.

62

63 **Key Words**

64 MRI, CLARITY, social, autism, axons, diffusion, structure, imaging

65

66 **Background**

67 Autism is a common neurodevelopmental disorder, which is highly heritable
68 (1). While heritability is high, it is also clear that autism is highly polygenic.
69 Around ~400-1000 genes are involved in autism susceptibility (2-5). Many of
70 these genes cluster upon proteins relating to synaptic signaling (6). A family of
71 presynaptic proteins garnering recent interest have been the neurexins
72 (*NRXNs*). *NRXNs* are encoded by three genes (*NRXN1*, *NRXN2*, *NRXN3*;
73 note that *CNTNAP1* and *CNTNAP2* are sometimes referred to as *NRXN4*), of
74 which two major isoforms exist: the longer α proteins with six
75 laminin/neurexin/sex hormone (LNS) binding domains, and the shorter β
76 proteins with one LNS binding domain (7, 8).

77

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78 Mutations within all three *NRXN* genes have been linked to autism (6).
79 Heterozygous deletions within *NRXN2* have been identified in a number of
80 individuals with autistic phenotypes. These include an autistic boy and his
81 father (who had severe language delay but not autism) who both had a
82 frameshift mutation within exon 12 of *NRXN2* (9); a 570-kb de novo deletion
83 of 24 genes at chromosome 11q13.1, including *NRXN2*, in a 21-year old man
84 displaying a clinical phenotype including autistic traits (10); a 1.6Mb deletion
85 at chromosome region 11q12.3-11q13.1, including *NRXN2*, in a 23-year old
86 man with intellectual disability and behavioral problems (11); a de novo
87 frameshift mutation identified in a Chinese man with autism spectrum disorder
88 (ASD) (12), a 921 kb microdeletion at 11q13 in a 2 year old boy who had
89 language and developmental delay (although did not meet the autism
90 diagnosis criteria) (13) and a paternally inherited microRNA miR-873-5p
91 variant in an ASD individual which altered binding affinity for several risk-
92 genes including *NRXN2* and *CNTNAP2* (*NRXN4*) (14). Furthermore, recently,
93 two large-scale reports have identified *NRXN2* with ASD risk. A study of 529
94 ASD patients and 1,923 controls in a Chinese population identified two
95 *NRXN2* variants which significantly increase ASD risk (15). The second study
96 employed machine learning approaches across 5000 ASD families to rank the
97 importance of ASD candidate genes, and ranks *NRXN2* in the top ~0.5% of
98 genes, i.e. 113th (16). For comparison, *NRXN1*, for which the evidence base
99 for its links to ASD is broader and stronger, ranks 45, and *CNTNAP2* ranks
100 211th (16). Consistent with these association studies, we and others have
101 previously found that homozygous or heterozygous deletion of *Nrxn2α*
102 induces impairment in social approach and social recognition (17-19). In

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103 summary, although mutations within *NRXN2* are rare, understanding how they
104 may drive social, ASD-relevant behavioural changes is important. One
105 important goal is to help elucidate how apparently convergent
106 pathophysiology in ASD emerges despite marked genetic heterogeneity
107 (Insert ref Geschwind & State, 2015 cited above); mapping brain alterations
108 driven by different single genes is thus a crucial task.

109

110 Currently it is unknown whether deletion of *Nrxn2 α* changes the brain's
111 microstructure and connectivity. One previous study found coarse alterations
112 to cell layer thickness within the hippocampus of *Nrxn2 α* homozygous KOs
113 (20). However, cell density measurements are unlikely to reveal the true
114 extent of changes within the autistic brain. Within the current study, we have
115 addressed this by developing a dual imaging approach (DTI and CLARITY)
116 that quantifies the alignment and density of white matter, applied here to brain
117 regions known to support social behavior in a mouse model of autism.

118

119 Diffusion tensor MRI (or DTI) is based upon the movement of water
120 molecules, a measure that is termed fractional anisotropy (FA). Apparent
121 diffusion coefficient (ADC) is similar to FA, but quantifies diffusion restriction
122 as opposed to the spatial symmetry of diffusion. This approach has been used
123 to explore neuropathological markers in autistic patients; alterations in
124 myelination, axonal abundance, size and orientation all modify FA and ADC
125 values (21-23). Using the preferred direction of the diffusion of tensors
126 between brain regions can be used to explore their potential connection.
127 Quantification of those computed streamlines by FA and axial and/or radial

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128 diffusion can indicate impairments in regional structural connectivity. Since
129 aberrant brain connectivity is likely a core feature of autism (24), we reasoned
130 that the candidate method for probing the autistic brain should combine
131 tractographic techniques. Accordingly, here, we combined high resolution
132 imaging of labelled neuronal tracts in brains rendered transparent by
133 CLARITY with DTI.

134

135 CLARITY is a recent development that renders tissue optically transparent
136 and macromolecule permeable (25). This permits antibody staining and
137 imaging of much larger tissue volumes than possible under traditional
138 immunofluorescence techniques. By examining fiber orientation without
139 sectioning-related artefacts and biases, axonal staining in cleared tissue
140 affords a deeper understanding of the microstructure and structural
141 connectivity of a brain region.

142

143 Given the social impairments found within *Nrxn2 α* mice, we sought to
144 examine those brain regions most closely linked with social behavior (See
145 Supplemental Materials). Briefly, we identified four regions of interest (ROIs):
146 the amygdala, and three brain regions strongly and directly connected to the
147 amygdala; the hippocampus, orbitofrontal cortex (OFC), and anterior cingulate
148 cortex (ACC). As predicted, structural connectivity was abnormal in *Nrxn2 α*
149 mice.

150

151 **Methods**

152 **Ethics**

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153 All procedures were approved by the University of Leeds and Durham
154 University Animal Ethical and Welfare Review Boards and were performed
155 under UK Home Office Project and Personal Licenses in accordance with the
156 Animals (Scientific Procedures) Act 1986.

157

158 **Animals**

159 Full details of the animals, their background, genotyping and housing can be
160 found elsewhere (17). In brief, male B6;129-
161 *Nrxn3tm1Sud/Nrxn1tm1Sud/Nrxn2tm1Sud/J* mice (JAX #006377) were
162 purchased from the Jackson Laboratory and outbred once to the
163 C57BL/6NCrl strain (Charles River, Margate, United Kingdom) to obtain mice
164 that were individually *Nrxn2α* KO heterozygotes. Subsequently, HET knockout
165 males were bred with HET females (cousin mating).

166

167 **Experimental animals**

168 6 adult wild-type males (Charles River, Margate, UK) and 6 age matched
169 littermate *Nrxn2α* KO homozygotes (71 days \pm 6 days old (SEM)) were
170 perfused-fixed with 4% paraformaldehyde (PFA) in 0.1 M phosphate buffer
171 saline (PBS) and the brains extracted. The brains were immersed in 4%
172 PFA/0.1 M PBS for a minimum of 48 hours prior to imaging. During imaging,
173 the samples were placed in custom-built MR-compatible tubes containing
174 Fomblin Y (Sigma, Poole, Dorset, UK).

175

176 Due to the relatively low variance, and owing to the complexity and
177 methodological nature in our experimental approach, we achieved

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178 significance by groups of 6 (power provided in Results). No data was
179 excluded from the study. Sample randomisation was performed by JD, with
180 experimenters (EP and ALT) blinded to genotype.

181

182 **Data Acquisition**

183 Image acquisition has been described elsewhere (26). Each brain was 3D
184 imaged using the protocol TE: 35 ms, TR: 700 ms and 10 signal averages.
185 The field of view was set at 128 x 128 x 128, with a cubic resolution of 100
186 $\mu\text{m}/\text{pixel}$ and a b value of 1200 s/mm^2 . Further details can be found in
187 Supplemental Materials.

188

189

190 **Image Processing**

191 Parsing of the raw data was semi-automated using DSI Studio, in order to
192 obtain b-values for every normalized gradient vector on the x, y and z
193 orientations. Unwanted background, setting a threshold, smoothing of the
194 data and definition of tissue boundaries was performed prior to the
195 reconstruction of the final 3D image. DTI analysis parameters were calculated
196 as previously described (28).

197

198 The *ex vivo* mouse brain 3D diffusion-weighted images were reconstructed
199 from the Bruker binary file using DSI Studio (<http://dsi-studio.labsolver.org>)
200 (29). Direction Encoded Colour Map (DEC) images were generated by
201 combining the information from the primary eigenvectors, diffusion images
202 and the FA. Images of the primary vectors and their orientation were

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203 reconstructed and superimposed on corresponding FA images to guide the
204 segmentation of discrete anatomical locations according to the brain atlas
205 (Figure 1B-D). Region of interest definition was performed by author EP and
206 corroborated independently by JD, with region area compared between the
207 experimenters (data not shown). We identified a canonical coronal slice (100
208 μm) for a given ROI from the standard mouse brain atlas (Figure 1A-D; Supp.
209 Figure 1) (27). We analysed three coronal slices centred on the canonical
210 slice, totalling 300 μm in anterior/posterior extent. For whole brain region
211 analysis, we used a similar approach, except regions were segmented for
212 every other slice in the anterior to posterior extent. The DSI Studio DTI
213 reconstruction characterizes the major diffusion direction of the fibre within the
214 brain (30, 31). Extraction of FA (calculated (26)) and ADC was performed
215 within selected segmented brain areas for every 3D reconstructed mouse
216 brain.

217

218 **Regions of Interest (ROIs)**

219 Our DTI approach was to undertake an *a posteriori* analysis of neural
220 organization in regions of interest (ROIs) identified by previous literature as
221 socially-relevant. Given the social impairments found within *Nrxn2 α* mice, for
222 the current study, we identified the brain regions of interest (ROIs) most
223 closely linked with social behavior, using previously published reports of brain
224 region involvement in social behaviour. Quantification of c-Fos
225 immunoreactivity has highlighted the importance of several amygdala nuclei
226 (including the basolateral) following social exposure (32), but also the anterior
227 cingulate cortex (ACC), prefrontal cortex and the hippocampus (33). Lesions

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228 to the primate amygdala alter social interactions (34, 35), and amygdala
229 neurons in primates including humans increase firing rates during social
230 scenarios (36-38). Consistent with these animal studies, amygdala damage in
231 humans (39) and amygdala dysfunction in ASD patients (40) impair social
232 responses. Other socially-important brain regions have also been proposed.
233 Notably, several studies have implicated the rodent hippocampus in social
234 behavior, including social memory and sociability (41-43). For instance,
235 intrahippocampal administration of neurolide-2, which interacts with α -
236 neurexin, specifically impairs sociability, but not anxiety and spatial learning in
237 rats (44). These findings are consistent with reports of social deficits in
238 humans with hippocampal damage (45) and hippocampal abnormalities in
239 ASD (46, 47). Finally, several studies link the frontal cortex, particularly the
240 orbitofrontal cortex, which is strongly anatomically connected with the
241 amygdala(48), to social processing (49, 50), consistent with findings of
242 abnormalities in orbitofrontal cortex in ASD (48, 51). Control regions of the
243 primary motor cortex (M1), primary sensory cortex (S1) and the barrel field
244 were chosen for CLARITY (Supp. Figure 12N-O).

245

246 **CLARITY**

247 Following MR imaging, the brains were washed in PBS to remove all Fomblin
248 Y and then incubated for 7 days in hydrogel solution at 4°C prior to
249 polymerisation at 37°C for 3.5 hours. The tissue was cut into 1.5 mm coronal
250 sections using a custom 3D-printed brain-slicing matrix based on MRI scans
251 of an adult C57BL/6 mouse brain (52) and incubated in clearing buffer for 24
252 days at 37°C with shaking. The cleared tissue was then washed in PBSTN₃

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253 (0.1% TritonX-100 and 1.5 mM sodium azide in PBS) for 24 hours at room
254 temperature and incubated in primary antibody solution (neurofilament (Aves
255 NF-H) 1:100 in PBSTN₃) at 37°C with shaking for 13 days. Samples were
256 washed, and then incubated in secondary antibody (AlexaFluor 488 goat anti-
257 chicken IgY) as per the primary. Sections were washed again, and incubated
258 in 3.6 µM DAPI (4',6-diamidino-2-phenylindole) followed by 85% glycerol in
259 PBS for refractive index matching.

260

261 Cleared samples were imaged using a Zeiss 7MP multiphoton microscope at
262 770 nm using a 20x objective lens (W Plan-Apochromat, NA 1.0, WD 1.7
263 mm). Images (512 x 512 x 512 voxels or 265 x 265 x 265 µm with an isotropic
264 resolution of 520 nm) were acquired in ACC, basolateral (BLA) and
265 basomedial amygdala and OFC) in both hemispheres. DAPI and
266 neurofilament signal was segmented into cell nuclei and axons, and the
267 resulting binary images were used to generate values for cell density, axonal
268 density and axonal alignment.

269

270 Full CLARITY methodological details are available within Supplemental
271 Materials.

272

273 **Data Availability**

274 Codes to analyse CLARITY datasets are made available by author LCA by
275 email request to either JD or LCA, subject to reference to the current paper.
276 The datasets used and/or analysed during the current study are available
277 from the corresponding author on reasonable request.

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278

279 **Data Analysis**

280 All data are expressed as mean \pm standard error of the mean (SEM). To
281 assess the variance between genotypes within a single brain structure across
282 hemispheres (given the importance of hemispheric differences in ASD (53)),
283 data was analyzed by within subject repeated measures two-way ANOVAs,
284 with Sidak multiple corrections employed on post hoc testing, or unpaired T-
285 tests. To correct for multiple comparisons, we employed the Benjamini-
286 Hochberg Procedure (corrected P values stated). Non-significant statistical
287 results, particularly hemisphere comparisons, can be found in Supplemental
288 Materials. Statistical testing and graphs were made using GraphPad Prism
289 version 6 and SPSS v22.

290

291 **Results**

292 ***Nrxn2* α deletion disrupts DTI measures of microstructure in social brain** 293 **regions**

294 To assess whether *Nrxn2* α deletion alters gross morphology, we quantified
295 whole brain volume using DTI. We found total brain volume for wild-types and
296 *Nrxn2* α KOs was similar (456.0 ± 14.76 vs. 466.2 ± 11.0 mm³ (respectively);
297 $t_{(10)} = 0.55$, $p = 0.59$). Thus, *Nrxn2* α deletion does not change total brain size.

298

299 To quantitatively measure DTI, we examined FA and ADC. FA analyses
300 changes in the linear orientation (i.e. along an axonal tract), whereas ADC
301 (mean diffusivity) averages diffusion in all directions (i.e. the X, Y and Z axis),
302 which is sensitive to changes such as altered alignment. The amygdala is

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303 critically important for social behaviours. To assess whether amygdalar
304 alterations might account for social impairments in *Nrxn2α* KO mice, we
305 segmented the whole amygdala structure and the basolateral nuclei along the
306 anterior-posterior axis.

307

308 The posterior amygdala showed a significant reduction in FA in *Nrxn2α* KO
309 mice (Figure 2A-B) (anterior: genotype ($F_{(1, 10)} = 5.81$, $p = 0.056$); posterior:
310 genotype ($F_{(1, 10)} = 11.2$, $p = 0.025$, power = 85.4%)). This FA reduction was
311 also observed specifically in the BLA, a region strongly associated with social
312 behaviours (Figure 2C; genotype ($F_{(1, 10)} = 6.31$, $p = 0.049$, power = 62.1%)).
313 ADC was not significantly altered in the anterior amygdala, posterior
314 amygdala or BLA (Figure 2D-F; all genotype: $F_{(1, 10)} < 1$).

315

316 We conducted the same analysis for the two prefrontal regions implicated in
317 social behaviour and autism: the OFC and ACC. The pattern of results was
318 similar for both regions: FA was not altered, while ADC was increased in the
319 OFC (Figure 3A-B) and the ACC (Figure 3C-D). FA for the OFC was not
320 significantly altered (genotype: ($F_{(1, 10)} = 3.04$, $p = 0.079$)) but ADC was
321 significantly increased (genotype: ($F_{(1, 10)} = 8.20$, $p = 0.043$, power = 73.3%)).
322 The ACC was unaltered in FA ($t_{(10)} = 1.70$, $p = 0.08$) but had significantly
323 increased ADC ($t_{(10)} = 7.52$, $p = 0.002$, power = 99.9%).

324

325 We sought to examine whether changes in the amygdala (Supp. Figure 4),
326 OFC or ACC FA and ADC were driven by diffusion in the primary axis (λ_1) or
327 the radial orientations (λ_2 and λ_3) by characterisation of AD (primary) and RD

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328 (radial). Within the OFC (Figure 3E-F), AD was significantly increased
329 (genotype: ($F_{(1, 10)} = 10.74$, $p = 0.029$, power = 83.9%)), as was RD (genotype:
330 ($F_{(1, 10)} = 18.26$, $p = 0.009$, power = 97.0%)), suggesting that both along-tract
331 diffusion and tract branching were affected. However, in the ACC (Figure 3G-
332 H), only RD was significantly increased ($t_{(10)} = 5.65$, $p = 0.007$, power =
333 99.9%), with no alteration in AD ($t_{(10)} = 1.69$, $p = 0.09$). Increased RD is
334 thought to reflect demyelination or changes in axonal density or orientation
335 (54).

336

337 **DTI reveals altered hippocampal microstructure in *Nrxn2α* KO mice**

338 The hippocampus has recently been associated with social motivation and
339 social recognition. Since the specific contributions of the dorsal and ventral
340 hippocampal poles remain unclear, we segmented the whole hippocampus
341 into anterior (Bregma -1.94 mm), middle (Bregma -2.46 mm) (both dorsal) and
342 posterior (Bregma -3.28 mm) (incorporating ventral regions) levels.

343

344 FA values in the anterior, mid and posterior hippocampus were not
345 significantly altered (see Supp. Table 1 for statistics and Supp. Figure 5A-C).
346 Similarly, ADC was unaltered for the anterior and mid hippocampus (Supp.
347 Table 1 for statistics and Supp. Figure 5D-E), but was significantly increased
348 in *Nrxn2α* KO mice in the posterior hippocampus (genotype: ($F_{(1, 10)} = 8.80$, p
349 = 0.036, power = 76.6%); Supp. Figure 5F). There were no significant
350 genotype differences in AD in any of the hippocampal regions (Supp. Figure
351 6A-C). However, RD was significantly increased in the posterior hippocampus
352 in *Nrxn2α* KO mice (genotype: ($F_{(1, 10)} = 10.83$, $p = 0.027$, power = 84.2%;

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353 Supp. Figure 6F) but not in anterior and mid regions (see Supp. Table 1;
354 Supp. Figure 6D-E). The theoretical approach undertaken hitherto was to
355 segment ROIs using a single coronal plane (as outlined in the Methods),
356 which subsequently allowed for the same anterior/posterior region to be
357 analysed by CLARITY. However, this restricted analysis could theoretically
358 miss diffusion differences across a whole brain region (as in, for example, the
359 entire anterior to posterior ACC). As a further quantification, we segmented
360 whole regions for the amygdala (Supp. Figure 7), the anterior and posterior
361 hippocampus (Supp. Figure 8) and the OFC and ACC (Supp. Figure 9). We
362 found that although there were more statistical differences between the
363 genotypes for the ‘whole’ anterior hippocampus region compared to the
364 ‘single plane’ analysis, overall the two analysis methods suggested broadly
365 similar structural alterations.

366

367 Lastly, given DTI is most commonly associated with analysis of white matter
368 tracts, we also quantified the corpus callosum. Changes within the corpus
369 callosum have repeatedly been highlighted in autism (55, 56), including
370 mouse models of autism (57, 58). Here, we found significantly increased FA
371 and reduced ADC in *Nrxn2α* KO mice, which were driven by a significant
372 reduction in RD (Supp. Figure 10).

373

374 In summary, the microstructural measures most altered by *Nrxn2α* deletion
375 were increases in ADC and RD, including in the hippocampus, in line with
376 recent work suggesting a role for ventral hippocampus in social memory (43).

377

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378 **DTI tractography reveals *Nrxn2α* deletion affects structural connectivity**
379 **between the amygdala and orbitofrontal cortex**

380 The amygdala is strongly and bidirectionally connected to both the
381 hippocampus (59) and the OFC (60). As all three regions are themselves
382 important for social behaviour, and autism is thought to be, at least in part,
383 related to abnormal structural connectivity (24), we performed tractography
384 analysis between the amygdala (and specifically the BLA) and the
385 hippocampus, and between the amygdala and the OFC.

386

387 From the anterior amygdala, we examined the diffusivity (AD and RD) of
388 connections to the anterior and posterior hippocampus (Supp. Figure 11). We
389 did not observe differences in RD in the tracts connecting the amygdala with
390 the hippocampus (see Supp. Table 2 for non-significant statistics). Although
391 AD between the anterior amygdala and anterior hippocampus did not differ by
392 genotype, there was a significant interaction between genotype and
393 hemisphere (genotype x hemisphere ($F_{(1, 10)} = 12.12$, $p = 0.023$, power =
394 88.0%; Figure 4A); post hoc analysis shows this was driven by larger right-vs-
395 left hemisphere AD values within the *Nrxn2α* KOs only ($p = 0.012$). This
396 difference could be driven by the BLA; there was increased AD in both the
397 BLA/anterior hippocampus tracts (genotype x hemisphere ($F_{(1, 10)} = 10.53$, $p =$
398 0.032, power = 83.2%) and the BLA/posterior hippocampus tracts (genotype x
399 hemisphere ($F_{(1, 10)} = 12.97$, $p = 0.020$, power = 90%), which again was
400 related to larger right-vs-left hemisphere values in the *Nrxn2α* KOs
401 (BLA/anterior hippocampus: $p = 0.004$ and BLA/posterior hippocampus: $p =$
402 0.001, (Figure 4C-D)) but not the wild-type (anterior: $p = 0.87$; posterior: $p =$

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403 1.00). These results indicate that there are differences for the structural
404 connectivity of the amygdala with the hippocampus within the left and right
405 hemisphere in *Nrxn2α* KO mice, with increased axial diffusivity in the right
406 hemisphere. This finding is particularly interesting, as hemispheric differences
407 in functional connectivity, particularly affecting connections from the right
408 amygdala, have been found children with ASD (61, 62).

409

410 Finally, we tested connections between the amygdala and the OFC. For AD,
411 wild-type and *Nrxn2α* KO mice did not differ by genotype (Figure 4E:
412 genotype: ($F_{(1, 10)} = 2.85$, $p = 0.09$), hemisphere: ($F_{(1, 10)} = 6.38$, $p = 0.052$). RD
413 was strikingly higher in *Nrxn2α* KO mice (Figure 4F: genotype: ($F_{(1, 10)} = 26.06$,
414 $p = 0.023$, power = 99.5%)), indicative of a change in demyelination, axonal
415 density or orientation (54).

416

417 **CLARITY reveals fibre disruption in *Nrxn2α* KO mice in the amygdala,**
418 **orbitofrontal cortex, and anterior cingulate cortex**

419 To further explore the differences as revealed by DTI, we performed CLARITY
420 on the same brain tissue used in DTI, and stained with neurofilament and
421 DAPI to label axons and cell bodies, respectively. We were then able to derive
422 both the axonal alignment (as in, the geometric alignment of axons (from
423 linear alignment to random) within 3D space (see Supp. Figure 2)) and
424 density of the stained fibers, in addition to the cell density.

425

426 The pattern of results was broadly similar for both the prefrontal cortical ROIs.

427 That is, first, axonal alignment was increased in *Nrxn2α* KO mice in the ACC

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428 (Figure 5D: genotype: ($F_{(1, 10)} = 16.06$, $p = 0.011$, power = 94.9%) but not the
429 OFC (Figure 5G: genotype: ($F_{(1, 10)} = 5.56$, $p = 0.059$). Second, this could not
430 be explained by a difference in cell density, since that was similar between the
431 KO and wild-type mice in both the ACC (Figure 5F: genotype: ($F_{(1, 10)} < 1$),
432 hemisphere: ($F_{(1, 10)} = 1.73$, $p = 0.11$) and the OFC (Figure 5H: genotype: ($F_{(1,$
433 $10) = 3.09$, $p = 0.08$). An increase in axonal density in *Nrxn2α* KO mice was
434 reliable in the ACC (Figure 5E: genotype: ($F_{(1, 10)} = 14.64$, $p = 0.014$, power =
435 93.0%), but not in the OFC (Figure 5H: genotype: ($F_{(1, 10)} = 3.09$, $p = 0.083$).

436

437 We further examined two regions of the anterior amygdala, the BLA and
438 basomedial (BMA) nuclei, where altered social cellular responses have been
439 reported in human autism (38). We did not observe any significant differences
440 for axonal alignment or fibre density in the BLA (see Supp. Figure 12A-C), but
441 whereas axonal alignment (Figure 5J, genotype: $F_{(1, 10)} = 7.70$, $p = 0.045$,
442 power = 70.6%) but not axonal density (Figure 5K: genotype: ($F_{(1, 10)} = 6.10$, p
443 = 0.054) was increased in *Nrxn2α* KO mice in the basomedial nuclei, while
444 cell density was unaffected (Figure 5L: genotype: ($F_{(1, 10)} < 1$). Alterations in
445 axonal alignment and density as directly revealed by CLARITY could explain
446 the increases in diffusivity and RD in the prefrontal regions, as measured by
447 DTI.

448

449 To test the specificity of these alterations, we examined three further brain
450 regions; the primary motor cortex (M1; Supp. Figure 12D-F), the primary
451 somatosensory cortex (S1; Supp. Figure 12H-J) and the barrel field (BF;
452 Supp. Figure 12K-M). Interestingly, although there were differences between

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453 the hemispheres, there were no statistical differences between the genotypes
454 or genotype x hemisphere interactions for any measure (Supp. Table 3),
455 suggesting some specificity of the alterations in social-relevant brain regions
456 in *Nrxn2α* KO mice.

457

458 In summary, in both the prefrontal ROIs, namely the OFC, and the ACC, DTI
459 showed that ADC and RD were increased in *Nrxn2α* KO mice, likely related to
460 complementary analysis from CLARITY showing that axonal alignment was
461 altered in *Nrxn2α* KO mice in both prefrontal ROIs.

462

463 **Discussion**

464 Interestingly, the single-gene deletion of *Nrxn2α* captures several key aspects
465 of human ASD. In terms of behaviour, three studies have now found social
466 deficits associated with *Nrxn2α* KO (17-19); in terms of brain structure, as
467 reported here (summarised below), the *Nrxn2α* KO mouse model shows
468 altered microstructure and structural connectivity patterns in socially-relevant
469 brain regions reminiscent of changes in ASD.

470

471 A DTI approach has been used for some time to explore neuropathological
472 markers in autistic patients; alterations in myelination, axonal abundance, size
473 and orientation all modify FA and ADC values (21, 63), specifically by
474 reducing amygdala FA (23, 63), and have been used as a quantitative
475 measure of changes to brain white matter integrity (23, 24). Increased cortical
476 ADC typically indexes reduced functionality: e.g. increased hippocampal ADC
477 is associated with mild cognitive impairment (64, 65) and predicts verbal and

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478 visuospatial memory in old healthy controls (66). Furthermore, both increased
479 RD of various white matter tracts (67, 68) and increased whole-brain AD (68)
480 have been observed in ASD. The *Nrxn2α* KO mouse reproduces many of
481 these specific changes, including reduced FA and increases in ADC, AD and
482 RD. Whole brain increases in ADC, AD and RD (but not FA) have been
483 reported in ASD children, as have increases in ADC and RD in frontal cortex
484 tracts (68). This is in agreement with other studies noting increased ADC in
485 frontal cortex in ASD (63), as we observed here in both the prefrontal regions
486 examined, the OFC and ACC. Likewise, FA was reduced in the amygdala in
487 ASD children and adolescents (69), and right-sided lateralisation of abnormal
488 amygdala/hippocampus-related connections, as seen in our *Nrxn2α* KO
489 mouse, has been noted in high-functioning adolescents/adults with autism
490 (70).

491

492 Whilst the current study specifically explores structural connectivity, it is
493 difficult to extrapolate as to what these structural changes mean for functional
494 connectivity in the *Nrxn2α* KO mouse. Hyper and hypo connectivity theories of
495 autism have remained contentious, and vary in humans by cohort studied
496 (e.g. by age of participant) (71). Further, in studies that have combined resting
497 state functional MRI (rsfMRI) and DTI, functional and structural connectivity
498 do not always overlap (72-74). Our current data suggests that DTI differences
499 can be explained by altered axonal patterning (i.e. CLARITY). Others have
500 explored the biological mechanisms linking structural connectivity to altered
501 functional connectivity. Zhan et al. (2014) found that deletion of the
502 chemokine receptor *Cx3cr1* resulted in impaired synaptic pruning of long-

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503 range connections during development, which manifested as impaired social
504 behavior caused by decreased frontal functional connectivity, reduced
505 synaptic multiplicity and weakened coherence of local field potentials (75).
506 Thus, it is possible that impairments in neuronal structural maturation can
507 generate functional connectivity deficits that encapsulate core autism
508 phenotypes.

509

510 Our findings corroborate these quantifications of clinical autism, but highlights
511 the question of what do the different measures of ADC, FA, AD and RD
512 represent? Importantly, we observed these microstructural changes in various
513 socially-relevant brain regions against a background of unchanged cell
514 density in all our study's ROIs. Unexpectedly, this highlights the power of our
515 new approach. Dudanova et al. (2007) concluded from measures of cell
516 counting and cortical cell layer thickness that *NRXN2* played little role in
517 normal brain development (20). Indeed, in earlier studies, it was suggested
518 that deletion of all *Nrxns* was unlikely to affect synaptic development but
519 instead disrupts synaptic function (76). We propose that measures such as
520 two-dimensional cell counting may be underestimating the impact of genetic
521 mutations upon normal development. By staining cleared brain tissue with a
522 nuclear marker and performing automated three-dimensional cell counting, we
523 found no effect of *Nrxn2a* deletion on cell density in any region of interest
524 examined. But this belies the clear effects upon microstructure integrity across
525 multiple regions as measured by both DTI and CLARITY, and its specificity;
526 only the socially-relevant brain regions we tested were disrupted, and not
527 primary sensory or motor regions. Future studies will benefit from employing

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528 more sensitive measures of brain structural connectivity to determine the
529 relevance of genetic mutations in development.

530

531 FA and ADC can be influenced by changes in axonal density and alignment
532 (e.g. by myelination, demyelination, axonal damage, loss of white matter
533 coherence (77)). It is likely that the axonal alignment metric used to quantify
534 CLARITY more closely reflects the ADC measure of DTI, given that ADC (or
535 mean diffusivity) equally weights diffusion across all eigenvectors and does
536 not bias the primary eigenvector as FA does. Thus, it is likely that alterations
537 in the properties of axons in *Nrxn2a* KO mice are driving these changes in FA
538 and ADC. Given we mostly see differences in RD, thought to reflect tract
539 branching and myelination (as it measures λ_2 and λ_3), it is possible that the
540 orientation in the perpendicular not parallel orientation of fibres is mostly
541 affected. Given the differences in the amygdala, OFC and ACC, it is possible
542 that even though neuronal densities are similar in the *Nrxn2a* KO brain, it is
543 the connections between neurones and brain regions that are perturbed. This
544 would be consistent with the idea that structural connectivity disruption may
545 represent a core feature of autism (78). A broader question is how does the
546 loss of *Nrxn2a* account for changes in axonal organisation? Ultimately, this
547 question requires further studies. Others have shown that in *Nrxn2a* KO mice,
548 excitatory transmitter release is reduced, as is short-term plasticity (18).
549 Reduced glutamatergic release, even at a relatively long range to the
550 synapse, can change the complexity of dendritic arbors (79). As this is a gene
551 deletion model, it is conceivable that altered glutamatergic signalling during
552 early development impairs appropriate synapse maturation, leading to the

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553 structural changes we see herein. Further, how or whether these structural
554 changes fully explain the social impairments of *Nrxn2* α KO mice would require
555 new studies. Conceivably, inducible knock-down of *Nrxn2* (by inducible
556 knockout, siRNA, optogenetics etc.) within a specific brain region would
557 provide evidence that social abnormalities are being driven by *Nrxn2* loss.
558 However, developmentally-dependent altered structural connectivity would be
559 harder to definitively manipulate to explain changes in social behaviours.

560

561 Here we have developed a new application of CLARITY to quantitatively
562 investigate disease models by combining DTI with high resolution 3D imaging
563 and automated analysis of axonal fibres in a within subject study. Inevitably,
564 there are some technical limitations that will require future refinement as this
565 technology matures.

566

567 First, while we used CLARITY and immunolabeling to identify axons, we
568 cannot know whether axon-related changes alone reflect all the changes we
569 observed for our DTI measures. Second, whilst we can segment entire brain
570 regions for DTI analysis, it was not practical to image larger brain areas at the
571 necessary resolution for CLARITY. While it is theoretically possible that we
572 may bias sampling of each brain region by picking ROIs for multiphoton
573 imaging, this was done using atlas-defined coordinates and by an
574 experimenter blind to the DTI results, so minimising any bias. However, within
575 the current study, we were only able to apply the CLARITY approach to the
576 amygdala, OFC and ACC. It was not practical to apply this methodology to the
577 hippocampus, due to its extremely heterogeneous structure. The small cubic

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578 ROIs could not be reproducibly positioned, and larger ROIs to average across
579 larger areas of the hippocampus were not possible. Although imaging of fibre
580 tracts in large volumes of cleared tissue is possible (80), fluorescent labelling
581 limitations make it impractical for a study of this nature. Despite this, as the
582 adoption of the CLARITY technique increases, we hope that the use of DTI
583 and CLARITY to study structural connectivity across spatial scales will
584 become commonplace.

585

586 As yet, no one DTI protocol has emerged as the standard for *in vivo* or *ex vivo*
587 imaging. Indeed, there has been debate regarding the best number of
588 diffusion gradients to use, among other parameters (81). Whilst some claim a
589 minimum of 30 directions are required to estimate anisotropy (81), others
590 claim that the benefits of using more than six are limited (82-85). A limitation
591 of these studies is that these competing claims have not been complemented
592 with standard neuroanatomical techniques. Where we found DTI differences,
593 these were corroborated by the quantification of CLARITY (OFC, ACC, with
594 BLA differences not reaching statistical significance after multiple-comparison
595 correction). A further potential limitation of the current study is that groups of
596 six animals may be underpowered. We argue for our approach here as
597 follows. First, low variance in the datasets permits smaller group sizes.
598 Second, for 18 of our 22 significant results, the observed power was more
599 than 80%. Third, given the technical complexity of this approach, particularly
600 in its early adoption and refinement stages, large sample throughput of
601 multiple brain regions is challenging.

602

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603 In summary, our combined use of DTI and CLARITY has revealed changes in
604 microstructure and structural connectivity of socially-relevant brain regions in
605 *Nrxn2a* KO mice that may underlie their deficits in social behaviour. It is hard
606 to conceive how these changes could have been observed using classical
607 experimental approaches. We envisage this approach will deliver a new level
608 of detail in structural connectivity approaches to understanding autism.

609

610 **Abbreviations**

611 ACC: anterior cingulate cortex

612 AD: axial diffusivity

613 ADC: apparent diffusion coefficient

614 ASD: autism spectrum disorder

615 BLA: basolateral amygdala

616 CLARITY: optically cleared brain tissue

617 DTI: diffusion tensor imaging

618 FA: fractional anisotropy

619 OFC: orbitofrontal cortex

620 *Nrxn2*: neurexin II

621 RD: radial diffusivity

622 ROI: region of interest

623

624 **Declarations**

625 **Ethics approval and consent to participate**

626 All experiments were performed under UK Home Office Project and Personal
627 Licenses in accordance with the Animals (Scientific Procedures) Act 1986,

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628 and with the approval of the University of Leeds and Durham University
629 Animal Ethical and Welfare Review Boards.

630

631 **Consent for publication**

632 Not applicable

633

634 **Availability of data and material**

635 The codes used to quantify the CLARITY datasets are made available by
636 author LCA by email request to authors LCA or JD, subject to reference to the
637 current paper. The datasets used and/or analysed during the current study
638 are available from the corresponding author on reasonable request.

639

640 **Competing interests**

641 The authors declare no competing interests.

642

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660

661 **Authors' contribution**

662 EP, ALT, LCA and JD conceived the study. EP and ALT performed the
663 experiments. EP, ALT, LCA and JD analysed the data. SJC, RJR, LCA and
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665 have read and approved the final manuscript.

666

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669

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931 **Figure Legends**

932 **Figure 1**

933 Quantification of CLARITY imaging. **A** Sections of DTI-scanned brain were
934 segmented at different Bregma levels for (i) the orbitofrontal cortex, (ii) the
935 anterior hippocampus and amygdala, (iii) the mid hippocampus and posterior
936 amygdala and (iv) the posterior hippocampus. **B-D** DTI-scanned brains were
937 computed for tracts. Tissue from wild-type and *Nrxn2α* KO mice were cleared
938 and stained for neurofilament and DAPI (**E**). **F** Automated MATLAB scripts
939 were used to segment the DAPI (blue) and neurofilament (purple) channels
940 such that cell density and axonal density and orientation could be calculated.
941 **G** is representative of a CLARITY-derived 3D stacked image of a DAPI and
942 neurofilament of a region of interest, with **H** being the corresponding
943 segmented image. Scale bar: 100 μm.

944

945 **Figure 2**

946 Deletion of *Nrxn2α* reduces amygdala fractional anisotropy (FA) but not
947 apparent diffusion coefficient (ADC). DTI images of the amygdala was
948 segmented at two regions; anterior (Bregma -1.94 mm) and posterior (Bregma
949 -2.46 mm). FA of the whole amygdala structure was significantly reduced in
950 the posterior (**B**) but not (**A**) region. FA was also significantly reduced in the
951 anterior basolateral amygdala (BLA) (**C**). However, ADC was similar between
952 the genotypes in the anterior (**D**), posterior (**E**) and BLA (**F**). **= $P < 0.01$,
953 *= $P < 0.05$. Error bars represent s.e.m. Wild-type n=6, *Nrxn2α* KO n=6.

954

955 **Figure 3**

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956 *Nrxn2α* KO mice have increased apparent diffusion coefficient (ADC) and
957 axial (AD) and radial diffusivity (RD) in the orbitofrontal cortex (OFC) and the
958 anterior cingulate cortex (ACC). Although reduced, there was no significant
959 difference between wild-types and *Nrxn2α* KO mice for FA in the OFC (**A**) and
960 ACC (**C**), but ADC was significantly increased in *Nrxn2α* KO mice in both
961 prefrontal regions (**B** and **D**). The OFC has significantly increased AD and RD
962 (**E-F**), whereas only RD was increased in the ACC (**G-H**). ***=P=0.0005,
963 ***=P<0.001, **=P<0.01, *=P<0.05. Error bars represent s.e.m. Wild-type n=6,
964 *Nrxn2α* KO n=6.

965

966 **Figure 4**

967 Tractographic analysis of amygdala-hippocampus and amygdala-orbitofrontal
968 cortex (OFC) connectivity. Amygdala-hippocampal connections are
969 characterised by greater right hemisphere axial diffusivity (AD) *Nrxn2α* KO
970 mice (**A**) but not radial diffusivity (RD) (**B**). Specific to the BLA, connections to
971 the anterior hippocampus (**C**) and posterior hippocampus (**D**) have greater
972 right hemisphere AD. Although the amygdala-OFC connection was similar
973 between the genotypes for AD (**E**), *Nrxn2α* KO mice had significantly
974 increased RD (**F**). *=P<0.05, ***=P<0.001. Error bars represent s.e.m. Wild-
975 type n=6, *Nrxn2α* KO n=6.

976

977 **Figure 5**

978 CLARITY reveals differences in axonal alignment and fibre density in *Nrxn2α*
979 KO mice. (**A-C**) Representative images of the CLARITY-treated brain, with
980 ROI defined for the anterior cingulate cortex (ACC), orbitofrontal cortex

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981 (OFC), basomedial amygdala (BMA) and basolateral amygdala (BLA). For the
982 ACC, the axonal alignment (**D**) and axon density (**E**) were significantly altered
983 in KO mice, but cell density was unaltered (**F**). Within the medial OFC, only
984 axonal alignment was significantly altered in KOs (**G**), with axon density (**H**)
985 and cell density (**I**) being similar. For the BMA, both the axonal alignment (**J**)
986 and axon density (**K**) were significantly increased, whilst cell density was
987 unaltered (**L**). *=P<0.05, **=P<0.01. Error bars represent s.e.m. Wild-type
988 n=6, *Nrxn2α* KO n=6.
989

**The within-subject application of diffusion tensor MRI and CLARITY
reveals brain structural changes in *Nrxn2* deletion mice**

Supplemental Material

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Supplemental Materials and Methods

Diffusion Tensor MRI

Data Acquisition

Brain MR imaging was performed on a vertical 9.4 Tesla spectrometer (Bruker AVANCE II NMR, Ettlingen, Germany) with an 89 mm wide bore, 3 radio frequency channels with digital broadband frequency synthesis (6-620 MHz) and an imaging coil with diameter of 25 mm for hydrogen (^1H). 3D images for each brain were obtained using a DT-MRI protocol (TE: 35 ms, TR: 700 ms, 10 signal averages). The field of view was set at 128 x 128 x 128, with a cubic resolution of 100 $\mu\text{m}/\text{pixel}$ and a b value of 1200 s/mm^2 . For each brain, diffusion weighted images were obtained in 6 directions, based upon recent published protocols (1-5). The subject of the number of diffusions gradients has been debated (6), with studies suggesting limited benefits of using more than 6 directions in biological tissue (7-9). The imaging time for each brain was 60 hours.

CLARITY

Solutions:

Hydrogel solution: 2% PFA 2% acrylamide 0.05% bis-acrylamide and 0.25% VA-044 thermal initiator (2,2'-Azobis[2-(2-imidazolyl) propane] dihydrochloride) in PBS, pH 7.4.

Clearing buffer: 8% Sodium dodecyl sulfate in 200mM boric acid, pH 8.5.

Multiphoton imaging – methodological outline

Cleared samples were mounted in custom 3D printed chambers for two-photon imaging. Images were acquired using ZEN Black (Zeiss, Germany). DAPI signal was detected using a 485 nm short pass filter, and neurofilament using a 500-550 nm band pass filter. The power of the excitation laser was varied to maximise the dynamic range for each image, but all other parameters were kept constant. The images were analysed using custom MATLAB (version 9.1, The Mathworks Inc.) scripts. Two-dimensional images were visualised using ImageJ (10) and three-dimensional images using Vaa3D (11).

Multiphoton imaging and analysis – image analysis method

Pre-processing

Image files were loaded into MATLAB (The Mathworks Ltd.) using the BioFormats toolbox (12), and the raw image data were obtained along with the precise voxel dimensions from the metadata. Each two-dimensional (2D) image from the three-dimensional (3D) stack was initially corrected for uneven background illumination by element-wise division by a 2D reference image. This reference image was calculated as the mean 2D image through the 3D stack, which was smoothed using a 2D Gaussian kernel with a full-width at half maximum (FWHM) of 20 % of the geometric mean of the dimensions of the 2D image (mean dimension). The image was denoised by filtering the image with a Gaussian kernel with a standard deviation of one pixel. Background subtraction was carried out by subtracting a smoothed, filtered image (FWHM 10 % of the mean dimension). Each pixel was then smoothed using a 3D Gaussian kernel with FWHM of 1.5 μm (the largest axonal diameter expected according to Perge et al. (13)).

Segmentation

The numerical gradient of the image in each dimension ($\Delta X, \Delta Y, \Delta Z$) was calculated, and these were combined to calculate the magnitude of the gradient ($\sqrt{\Delta X^2 + \Delta Y^2 + \Delta Z^2}$). The resulting image was thresholded, using a combination of the Otsu (1979) and Rosin (2001) methods (Rosin threshold + 2/5 Otsu threshold) (14, 15). The gradient image highlights the edge of each axon; to combine these into a single object, the image was dilated and then eroded with a cubic structuring element (each side being 1.5 μm , to 'close' the largest axons as per Perge et al. (13)). Very small objects (less than 50 μm^3) were removed from the image as they reflected noise, very small neuronal processes and gradients around cells.

Owing to variations in staining intensity of different axons, the thresholding produced segmented axons of various thicknesses that did not necessarily reflect the true structure. To remove this bias, the thresholded image was skeletonised using a homotopic thinning algorithm (16) implemented in MATLAB(17). The resulting image was dilated and then eroded using a cubic structuring element (10 pixels on each side for dilation, 9 for erosion) to produce connected processes with a uniform two-pixel diameter. This dilation ensured that the voxels in the binary image were connected via their faces (6-connected) rather than just their corners (26-connected), which better reflects the true structure of biological processes. This method detects

most large axons at the expense of smaller processes, and the loss of any information about axon diameter. These steps are outlined in Supp. Figure 2.

Analysis

The density of axons was calculated as the fraction of the image volume taken up by the segmented axons. A measure of axonal alignment was calculated by determining the mean axonal alignment along each dimension. This alignment was calculated by moving along the 3D image in a single dimension, keeping the coordinates in the other dimensions constant, and counting the number of times the pixel intensity did not change (i.e. how many times an axon was not entered or left). This number was averaged across each face of the image volume and scaled to the length of each dimension to produce a metric of how constant the image intensity is in that dimension. The perfect case of no intensity change (i.e. all axons are aligned perfectly with a particular dimension) gives a value of 1. The greater the difference between this measure in each three dimensions, the more aligned the axons must be (i.e. their directions are anisotropic). The standard deviation of this measure across the three dimensions was calculated as the axonal alignment.

The alignment calculation is illustrated in Supp. Figure 3 for a simple, two-dimensional case. Supp. Figure 3a shows the case of low axonal alignment, and Supp. Figure 3b shows the case of high axonal alignment. In each case, for illustration, each pixel represented by a small square on the grid is classed as either containing an axon or not. In the real images, the pixels are smaller, and are actually binary. In each axis, the number of pixel transitions in which the presence of an axon does not change is divided by the number of transitions, and the average is calculated. The standard deviation of this average for all axes is the measure of axonal alignment. When the alignment is low, the two averages are similar, and the standard deviation is low. When the alignment is high the two averages are very different, and the standard deviation is high. To analyse the real data, this same calculation is carried out in 3D, but in a much larger grid of voxels. Cell density was calculated as the number of cells per mm³.

Supp. Table 1

Brain Region	DTI Measure	ANOVA Comparison	F Value	P Value
Anterior Hippocampus	FA	Genotype	$F_{(1,10)} = 3.91$	$P = 0.063$
		Hemisphere	$F_{(1,10)} = 3.89$	$P = 0.065$
Mid Hippocampus	FA	Genotype	$F_{(1,10)} = 3.12$	$P = 0.07$
		Hemisphere	$F_{(1,10)} < 1$	$P = 0.146$
Posterior Hippocampus	FA	Genotype	$F_{(1,10)} = 1.99$	$P = 0.104$
		Hemisphere	$F_{(1,10)} = 1.95$	$P = 0.101$
Anterior Hippocampus	ADC	Genotype	$F_{(1,10)} = 3.17$	$P = 0.073$
		Hemisphere	$F_{(1,10)} = 2.20$	$P = 0.095$
Mid Hippocampus	ADC	Genotype	$F_{(1,10)} < 1$	$P = 0.160$
		Hemisphere	$F_{(1,10)} = 1.62$	$P = 0.115$
Posterior Hippocampus	ADC	Genotype	$F_{(1,10)} = 8.88$	$P = 0.036$
		Hemisphere	$F_{(1,10)} < 1$	$P = 0.180$
Anterior Hippocampus	AD	Genotype	$F_{(1,10)} < 1$	$P = 0.187$
		Hemisphere	$F_{(1,10)} = 1.07$	$P = 0.121$
Mid Hippocampus	AD	Genotype	$F_{(1,10)} < 1$	$P = 0.153$
		Hemisphere	$F_{(1,10)} = 1.04$	$P = 0.124$
Posterior Hippocampus	AD	Genotype	$F_{(1,10)} = 3.45$	$P = 0.07$
		Hemisphere	$F_{(1,10)} = 6.19$	$P = 0.052$
Anterior Hippocampus	RD	Genotype	$F_{(1,10)} = 3.03$	$P = 0.086$
		Hemisphere	$F_{(1,10)} < 1$	$P = 0.137$
Mid Hippocampus	RD	Genotype	$F_{(1,10)} < 1$	$P = 0.140$
		Hemisphere	$F_{(1,10)} = 1.33$	$P = 0.119$
Posterior Hippocampus	RD	Genotype	$F_{(1,10)} = 10.83$	$P = 0.027$
		Hemisphere	$F_{(1,10)} = 3.48$	$P = 0.07$

Statistical analysis of the anterior (Bregma -1.94 mm), mid (Bregma -2.46 mm) and posterior (Bregma -3.28 mm) hippocampus for fractional anisotropy (FA), apparent diffusion coefficient (ADC), axial diffusion (AD) and radial diffusion (RD). Analysis was performed using repeated measure two-way ANOVAs for genotype and hemisphere (Benjamini-Hochberg corrected (corrected P values stated)).

Supp. Table 2

Brain Region	DTI Measure	ANOVA Comparison	F Value	P Value
Amygdala-Anterior Hippocampus	AD	Genotype	$F_{(1,10)} < 1$	P = 0.164
		Hemisphere	$F_{(1,10)} = 2.10$	P = 0.097
		Genotype x Hemisphere	$F_{(1,10)} = 12.12$	P = 0.023
Amygdala-Anterior Hippocampus	RD	Genotype	$F_{(1,10)} < 1$	P = 0.149
		Hemisphere	$F_{(1,10)} = 1.32$	P = 0.106
		Genotype x Hemisphere	$F_{(1,10)} < 1$	P = 0.155
Amygdala-Posterior Hippocampus	AD	Genotype	$F_{(1,10)} < 1$	P = 0.142
		Hemisphere	$F_{(1,10)} < 1$	P = 0.189
		Genotype x Hemisphere	$F_{(1,10)} = 4.54$	P = 0.061
Amygdala-Posterior Hippocampus	RD	Genotype	$F_{(1,10)} < 1$	P = 0.151
		Hemisphere	$F_{(1,10)} < 1$	P = 0.135
		Genotype x Hemisphere	$F_{(1,10)} < 1$	P = 0.128
BLA-Anterior Hippocampus	AD	Genotype	$F_{(1,10)} < 1$	P = 0.167
		Hemisphere	$F_{(1,10)} = 6.59$	P = 0.047
		Genotype x Hemisphere	$F_{(1,10)} = 10.53$	P = 0.032
BLA-Anterior Hippocampus	RD	Genotype	$F_{(1,10)} < 1$	P = 0.158
		Hemisphere	$F_{(1,10)} = 2.59$	P = 0.092
		Genotype x Hemisphere	$F_{(1,10)} < 1$	P = 0.173
BLA-Posterior Hippocampus	AD	Genotype	$F_{(1,10)} < 1$	P = 0.169
		Hemisphere	$F_{(1,10)} = 12.79$	P = 0.018
		Genotype x Hemisphere	$F_{(1,10)} = 12.97$	P = 0.02
BLA-Posterior Hippocampus	RD	Genotype	$F_{(1,10)} < 1$	P = 0.162
		Hemisphere	$F_{(1,10)} = 3.11$	P = 0.077
		Genotype x Hemisphere	$F_{(1,10)} < 1$	P = 0.178

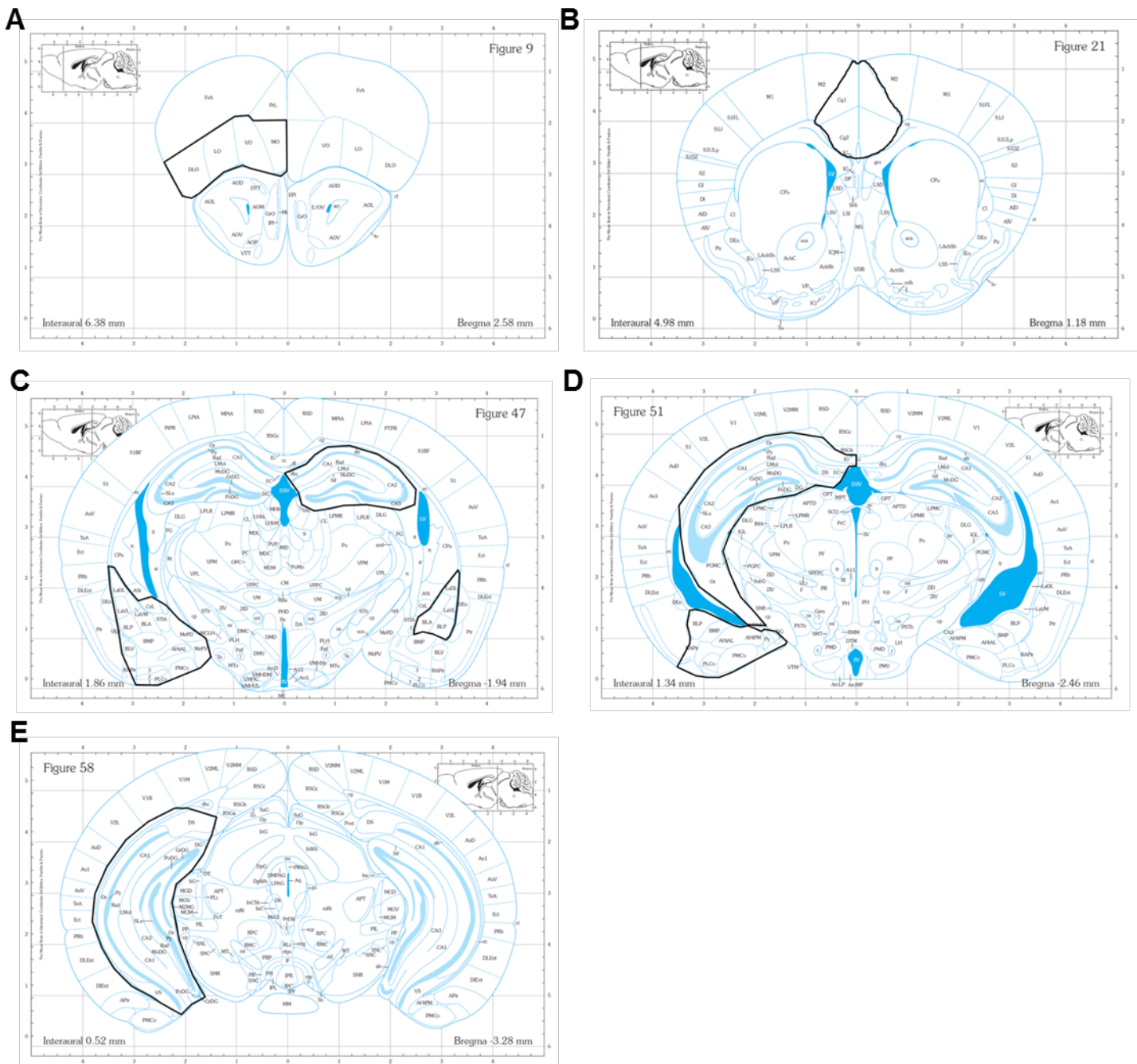
Statistical analysis of the anterior (Bregma -1.94 mm), and posterior (Bregma -3.28 mm) amygdala-hippocampal connections, analysed for axial diffusion (AD) and radial diffusion (RD). Analysis was performed using repeated measure two-way ANOVAs for genotype and hemisphere (Benjamini-Hochberg corrected (corrected P values stated)).

Supp. Table 3

Brain Region	CLARITY Measure	ANOVA Comparison	F Value	P Value
M1	OI	Genotype	$F_{(1,10)} < 1$	P = 0.182
		Hemisphere	$F_{(1,10)} = 1.74$	P = 0.108
M1	Cell Density	Genotype	$F_{(1,10)} = 2.04$	P = 0.099
		Hemisphere	$F_{(1,10)} = 1.41$	P = 0.117
M1	Fibre Density	Genotype	$F_{(1,10)} < 1$	P = 0.171
		Hemisphere	$F_{(1,10)} < 1$	P = 0.176
S1	OI	Genotype	$F_{(1,10)} < 1$	P = 0.185
		Hemisphere	$F_{(1,10)} = 36.86$	P = 0.005
S1	Cell Density	Genotype	$F_{(1,10)} < 1$	P = 0.131
		Hemisphere	$F_{(1,10)} = 13.73$	P = 0.016
S1	Fibre Density	Genotype	$F_{(1,10)} = 1.73$	P = 0.110
		Hemisphere	$F_{(1,10)} = 8.51$	P = 0.038
BF	OI	Genotype	$F_{(1,10)} < 1$	P = 0.191
		Hemisphere	$F_{(1,10)} = 10.59$	P = 0.034
BF	Cell Density	Genotype	$F_{(1,10)} < 1$	P = 0.133
		Hemisphere	$F_{(1,10)} = 8.70$	P = 0.041
BF	Fibre Density	Genotype	$F_{(1,10)} < 1$	P = 0.144
		Hemisphere	$F_{(1,10)} < 1$	P = 0.126

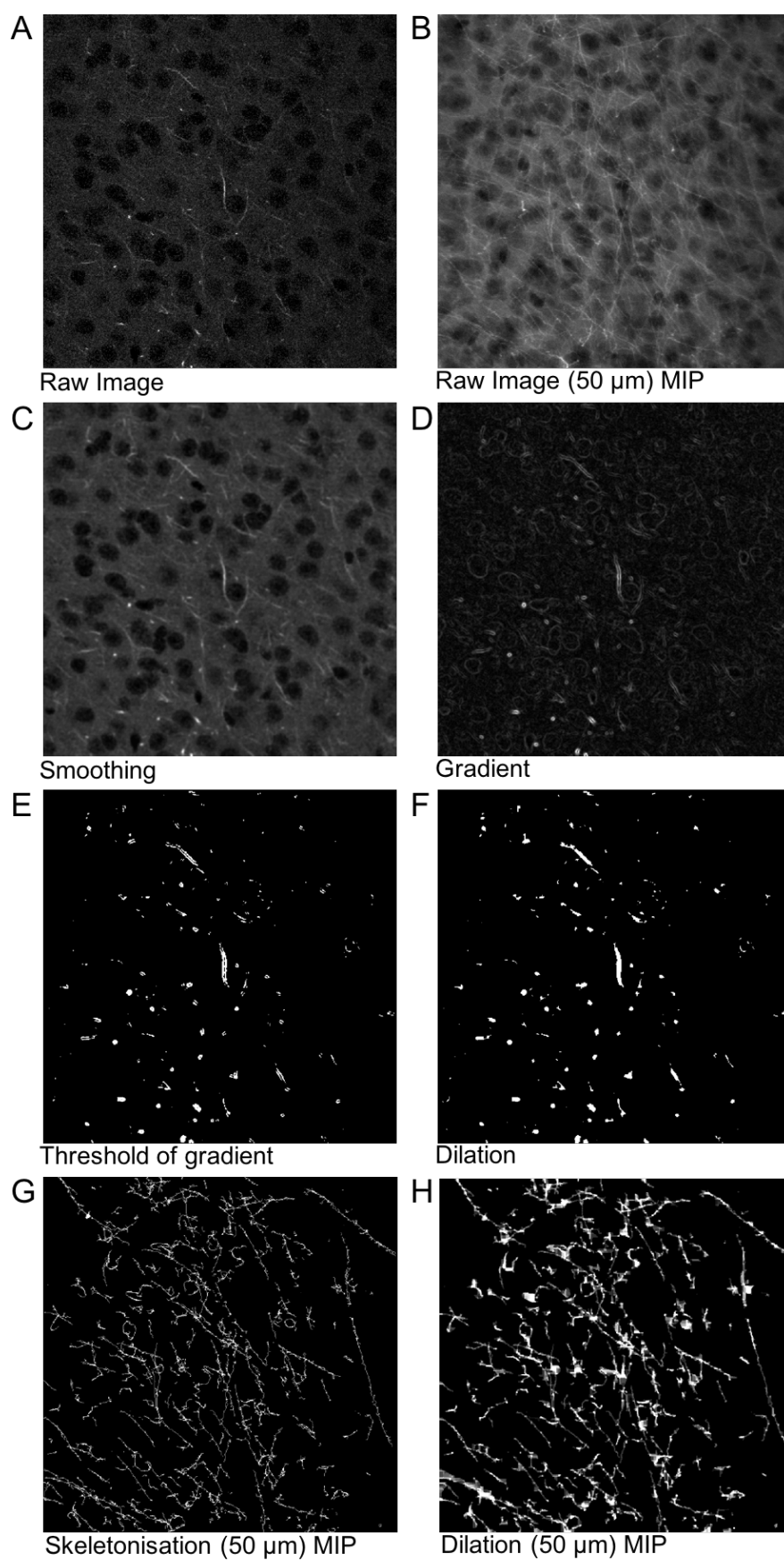
Statistical analysis of the primary motor cortex (M1), primary somatosensory cortex (S1) and the barrel field (BF). CLARITY imaged regions were then analysed for orientation index (OI), cell density and fibre density. Analysis was performed using repeated measure two-way ANOVAs for genotype and hemisphere (Benjamini-Hochberg corrected (corrected P values stated)).

Supp. Figure 1



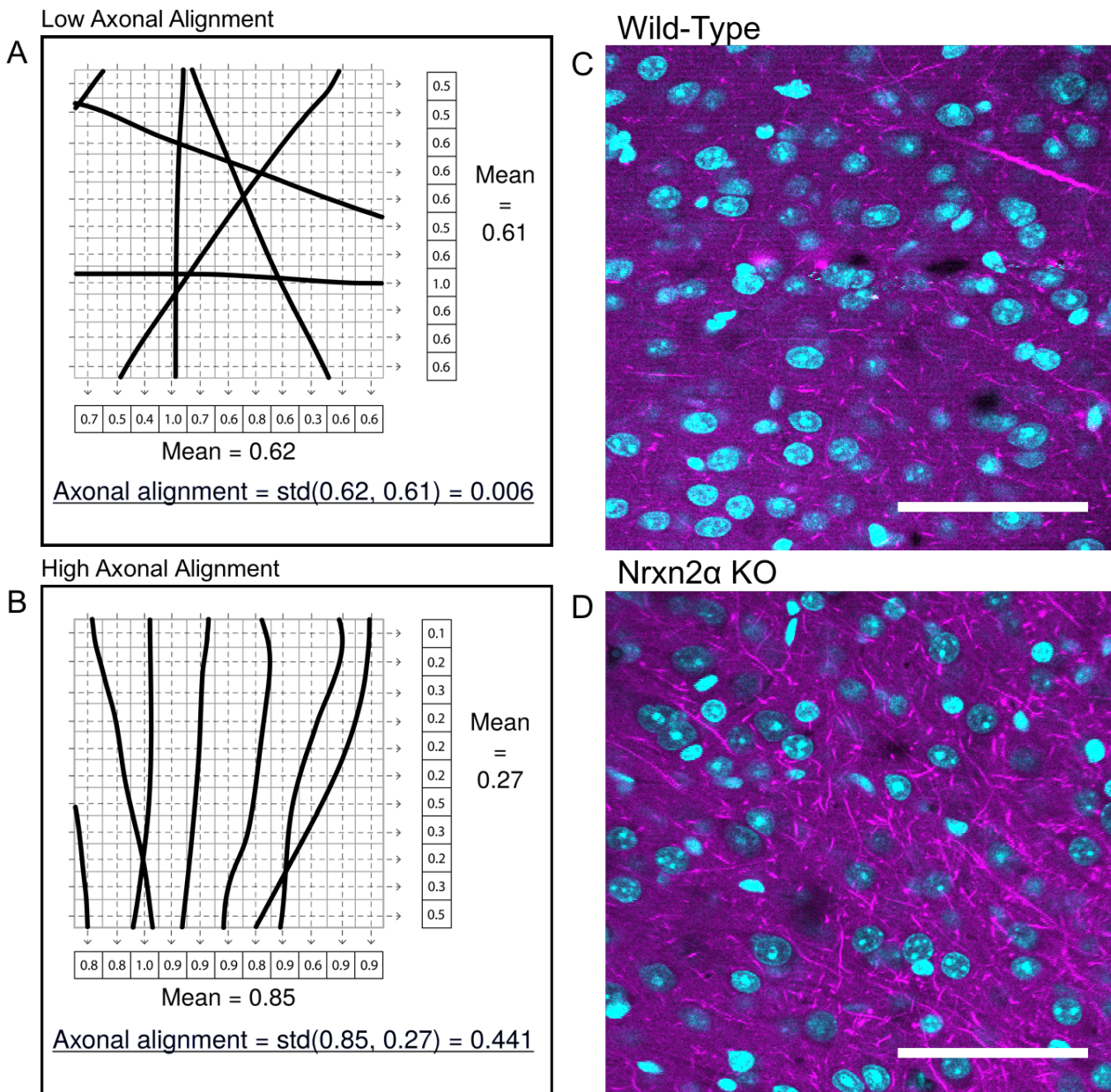
Atlas maps representing manual segmentation of regions of interest (ROI). (A) The orbitofrontal cortex ROI. (B) The ACC ROI. (C) The anterior hippocampus, anterior amygdala and basolateral amygdala ROI. (D) The mid hippocampus and posterior amygdala ROI. (E) The posterior hippocampus ROI. The atlas maps were used with the permission of the Authors (18).

Supp. Figure 2



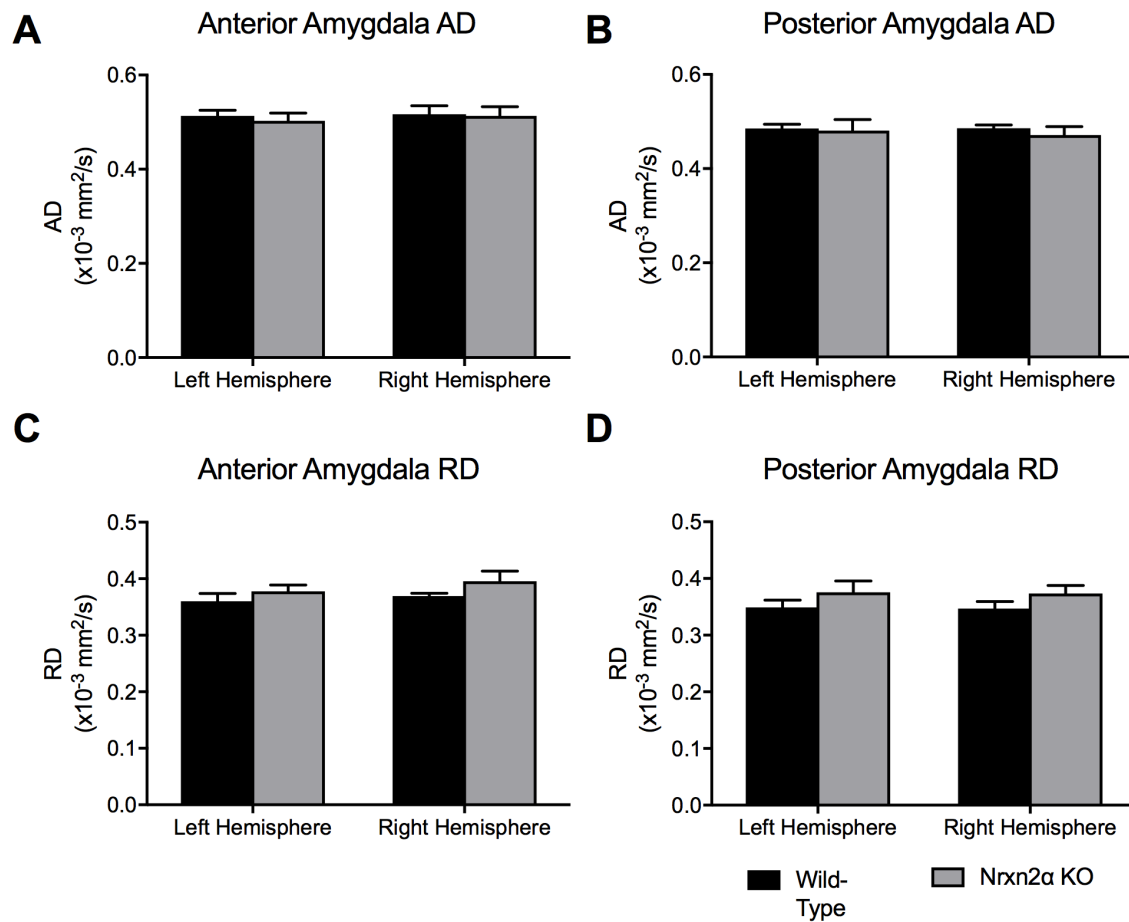
Analysis methodology of axonal segmentation from multiphoton images.

Supp. Figure 3



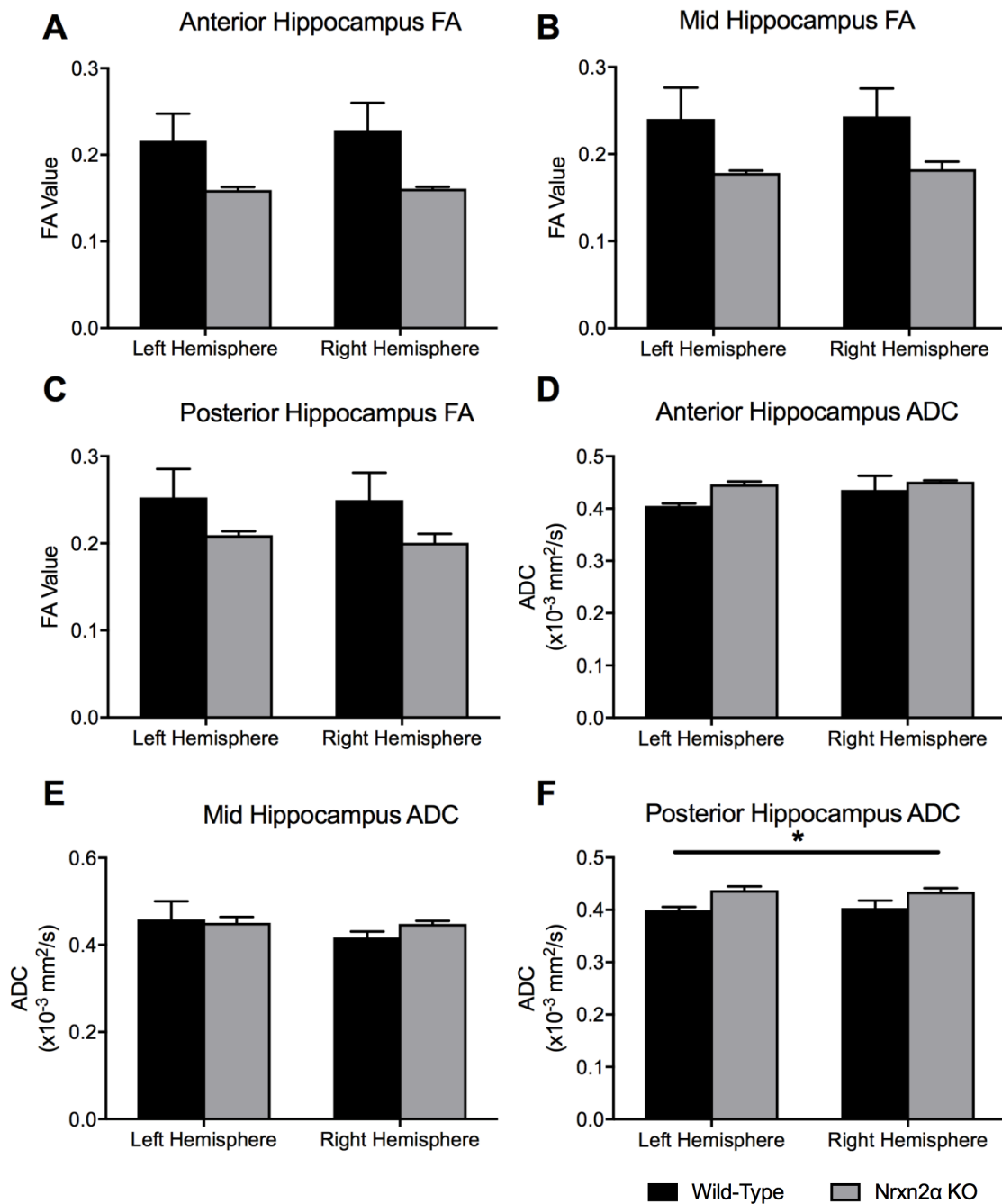
A and B. Illustration of the axonal alignment calculation in a simple two-dimensional case. The grey grid represents the image pixels, the black lines axons and the dashed lines represent the calculation process. Standard deviation denoted as *std.* **C and D.** Cingulate cortex images taken from wild-type and Nrnx2 α KO mice, visually representing the greater axonal alignment and density in KO mice.

Supp. Figure 4



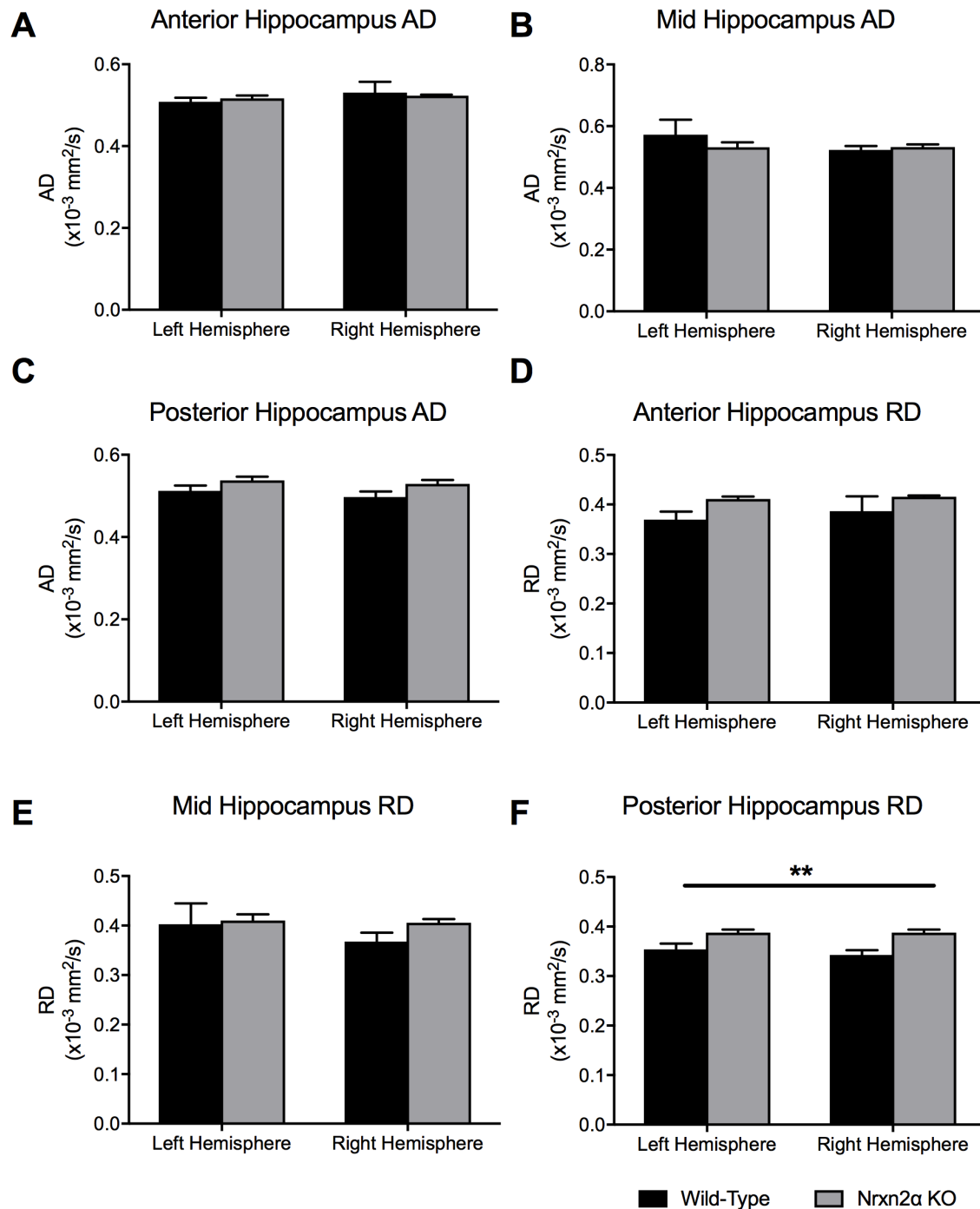
Axial diffusivity (AD) and radial diffusivity (RD) in the amygdala. The entire amygdala was segmented from DTI images at two regions; anterior (**A** and **C**: Bregma -1.94 mm) and posterior (**B** and **D**: Bregma -2.46 mm). No significant differences were observed between the genotypes for anterior or posterior regions. Error bars represent s.e.m. Wild-type n=6, Nrnx2 α KO n=6.

Supp. Figure 5



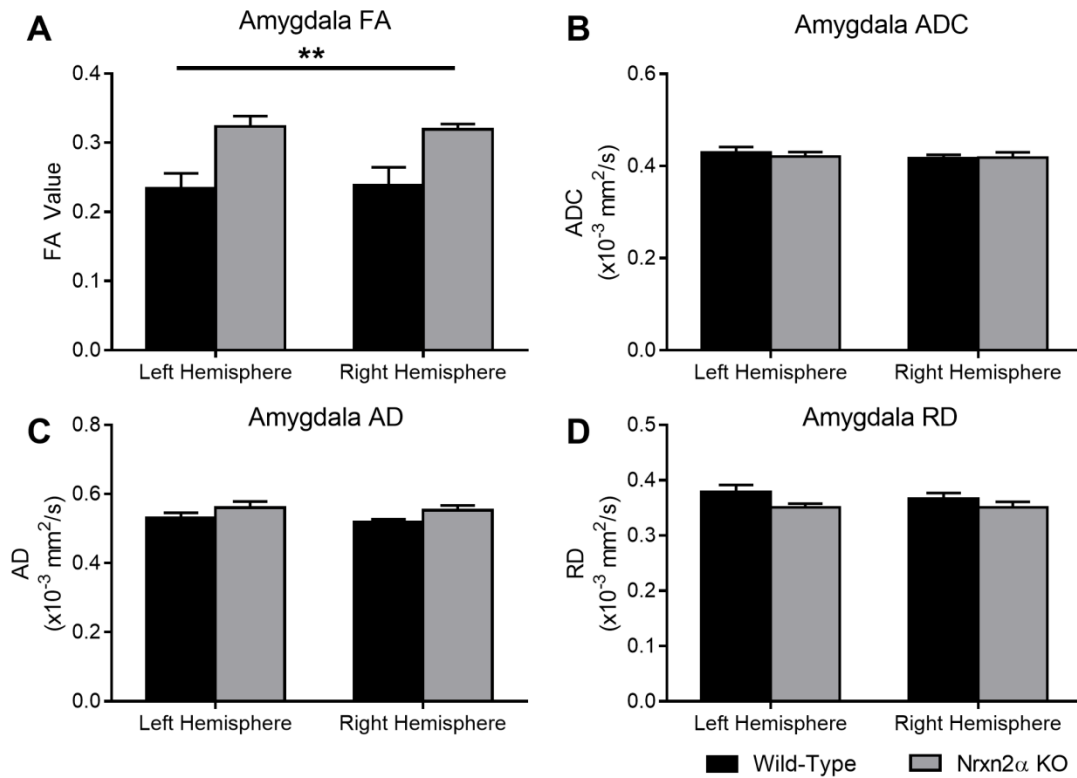
Fractional anisotropy (FA) and apparent diffusion coefficient (ADC) of the anterior to posterior hippocampus. Although Nrnx2 α KO had trends towards lower FA in the anterior (A), mid (B) and posterior (C) hippocampus, there were no significant differences. Similarly, anterior (D) and mid (E) hippocampal regions did not vary between the genotypes, the posterior hippocampus (F) had significantly increased ADC (f). * = P<0.05. Error bars represent s.e.m. Wild-type n=6, Nrnx2 α KO n=6.

Supp. Figure 6



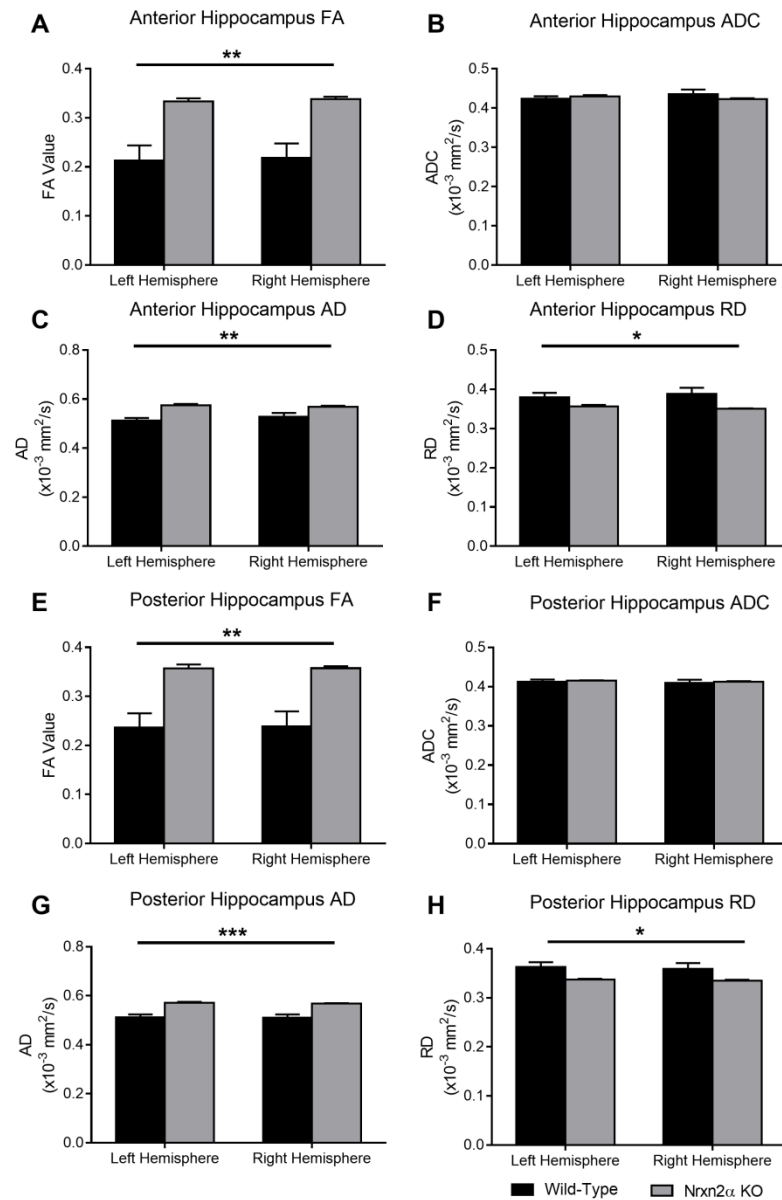
Axial diffusivity (AD) and radial diffusivity (RD) of the anterior to posterior hippocampus. AD did not differ in either the anterior (A), mid (B) and posterior (C) hippocampus. Although the anterior (D) and mid (E) hippocampal regions did not vary between the genotypes, the posterior hippocampus (F) had significantly increased RD (f). ** = P < 0.01. Error bars represent s.e.m. Wild-type n=6, Nrnx2 α KO n=6.

Supp. Figure 7



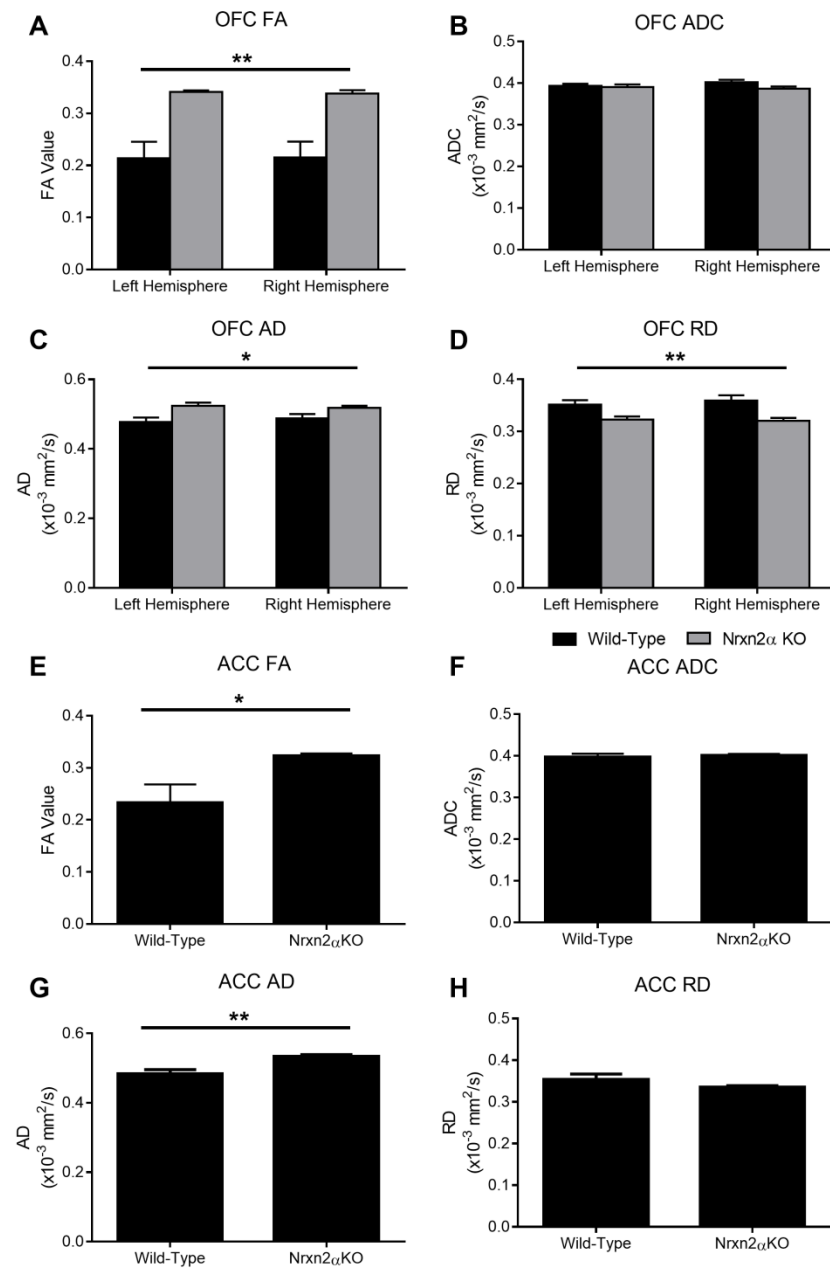
DTI quantified for the whole amygdala volume. **(A)** Fractional anisotropy (FA) was significantly increased in Nrnx2 α KO mice (genotype: $F_{(1,10)} = 11.15$, $p = 0.008$). However, **(B)** apparent diffusion coefficient (ADC) was not significantly altered (genotype: $F_{(1,10)} < 1$, $p = 0.782$), nor was **(C)** axial diffusivity (AD) (genotype: $F_{(1,10)} = 3.06$, $p = 0.111$) or **(D)** radial diffusivity (RD) (genotype: $F_{(1,10)} = 2.47$, $p = 0.147$). Error bars represent s.e.m. ** = $P < 0.01$. Wild-type $n=6$, Nrnx2 α KO $n=6$.

Supp. Figure 8



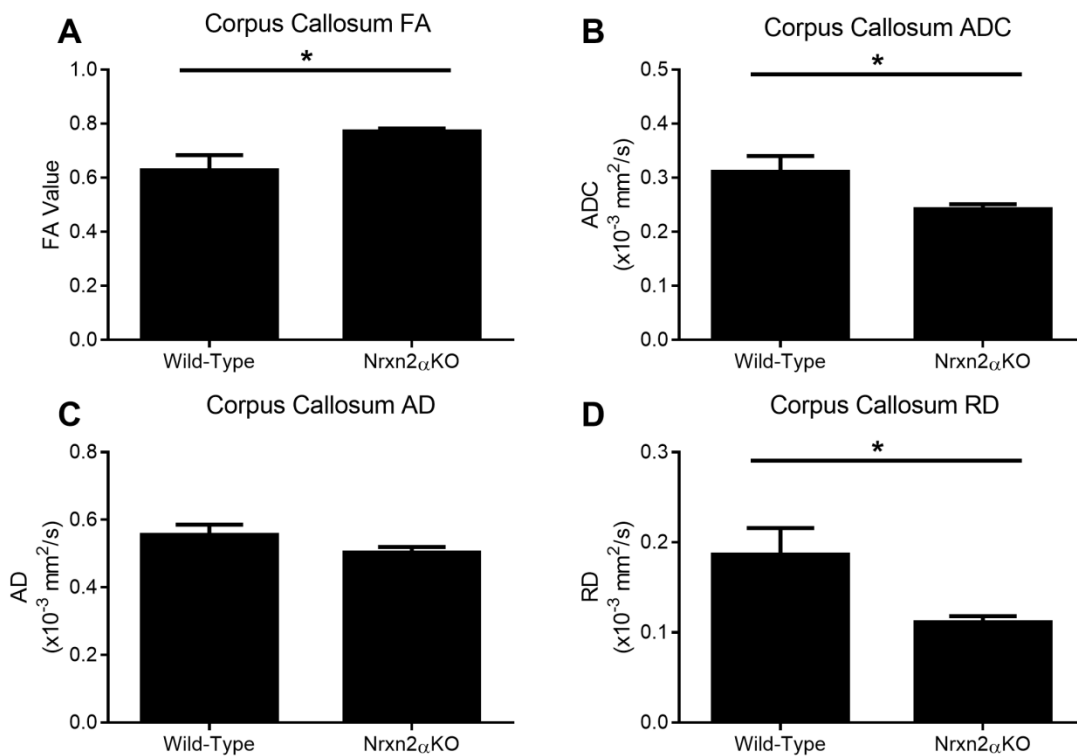
DTI quantified for the whole anterior hippocampus (Bregma -1.06 mm – -2.46 mm) and posterior hippocampus (Bregma -2.54 mm – -3.16 mm). (A) Fractional anisotropy (FA) in the anterior hippocampus was significantly increased in Nrnx2 α KO mice (genotype: $F_{(1,10)} = 15.63$, $p = 0.0027$) but (B) apparent diffusion coefficient (ADC) was not altered (genotype: $F_{(1,10)} < 1$, $p = 0.738$). (C) Axial diffusivity (AD) (genotype: $F_{(1,10)} = 16.17$, $p = 0.0024$) and (D) radial diffusivity (RD) (genotype: $F_{(1,10)} = 5.05$, $p = 0.048$) were both significantly altered in Nrnx2 α KO mice. In the posterior hippocampus, in Nrnx2 α KO mice, (E) FA was significant increased (genotype: $F_{(1,10)} = 15.62$, $p = 0.0027$), (F) ADC was similar to wild-types (genotype: $F_{(1,10)} < 1$, $p = 0.679$), (G) AD was increased (genotype: $F_{(1,10)} = 22.31$, $p = 0.0008$) and (H) RD was significantly reduced (genotype: $F_{(1,10)} = 5.34$, $p = 0.043$). Error bars represent s.e.m. * = $P < 0.05$, ** = $P < 0.01$, *** = $P < 0.001$. Wild-type n=6, Nrnx2 α KO n=6.

Supp. Figure 9



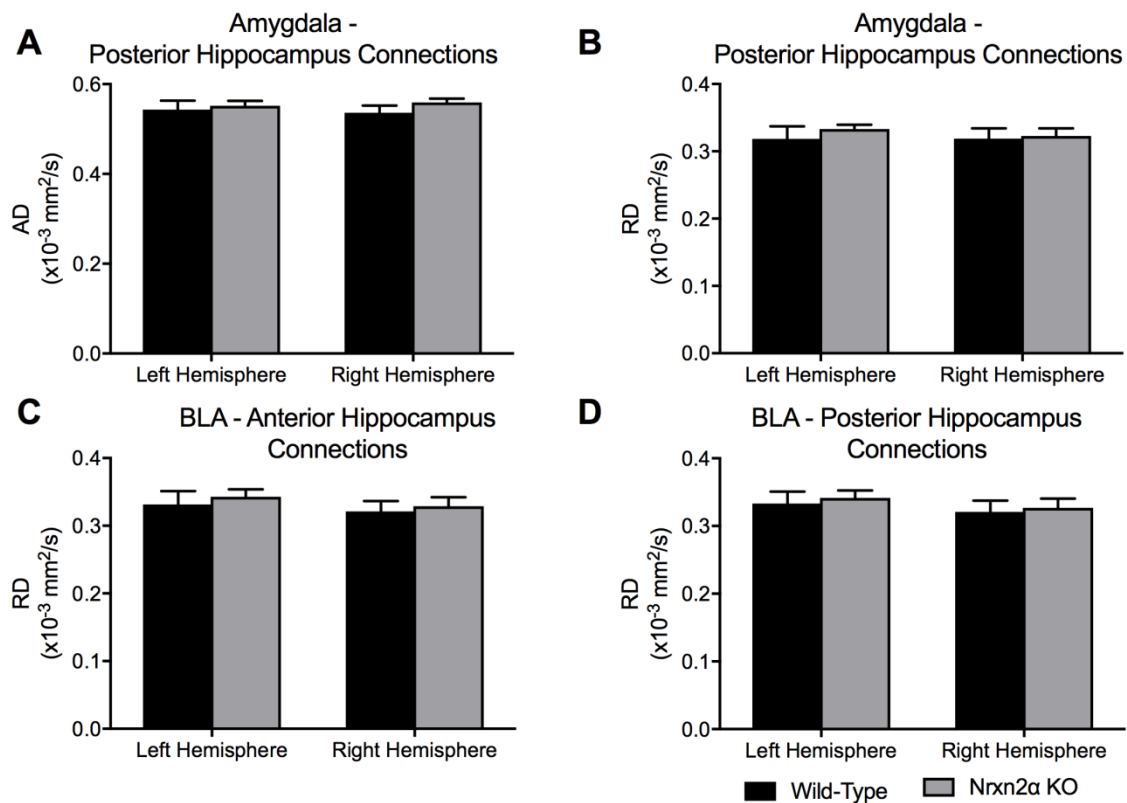
DTI quantified for the whole orbitofrontal cortex (OFC) and anterior cingulate cortex (ACC) and posterior hippocampus (Bregma -1.34 mm – -0.46 mm). **(A)** Fractional anisotropy (FA) in the OFC was significantly increased in Nrnx2 α KO mice (genotype: $F_{(1,10)} = 16.14$, $p = 0.0024$) but **(B)** apparent diffusion coefficient (ADC) was not altered (genotype: $F_{(1,10)} = 1.43$, $p = 0.260$). **(C)** Axial diffusivity (AD) (genotype: $F_{(1,10)} = 6.71$, $p = 0.027$) and **(D)** radial diffusivity (RD) (genotype: $F_{(1,10)} = 10.07$, $p = 0.0099$) were both significantly altered in Nrnx2 α KO mice. In the ACC of Nrnx2 α KO mice, **(E)** FA was significant increased (genotype: $t_{(10)} = 2.55$, $p = 0.029$), **(F)** ADC was similar to wild-types (genotype: $t_{(10)} = 2.55$, $p = 0.618$), **(G)** AD was increased (genotype: $t_{(10)} = 3.89$, $p = 0.003$) and **(H)** RD was not significantly different (genotype: $t_{(10)} = 1.35$, $p = 0.208$). Error bars represent s.e.m. * = $P < 0.05$, ** = $P < 0.01$. Wild-type $n=6$, Nrnx2 α KO $n=6$.

Supp. Figure 10



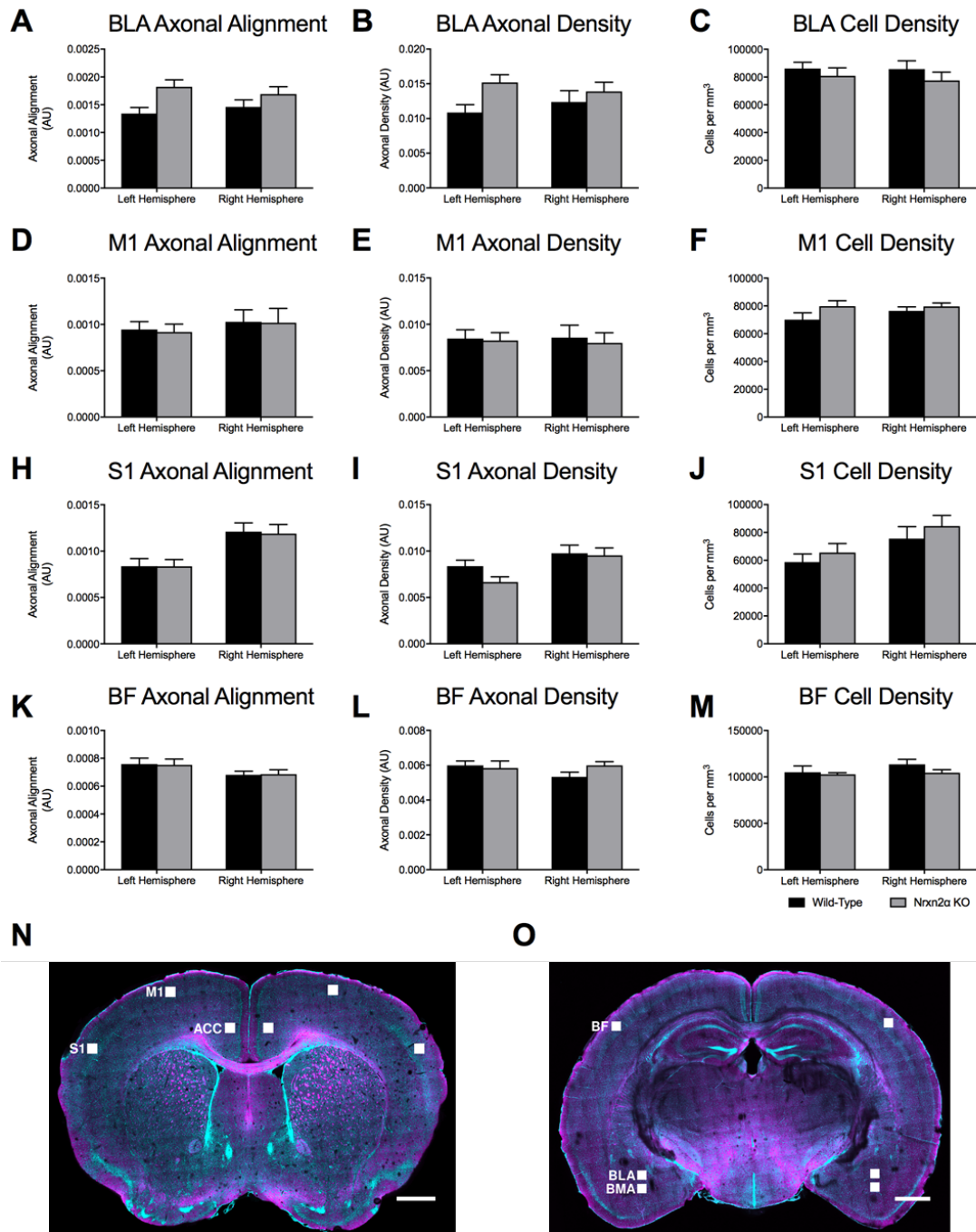
DTI quantification of the corpus callosum (Bregma 0.98 mm). To examine the integrity of white matter tracts within Nrnx2 α KO mice, we examined diffusivity in the corpus callosum. **(A)** Fractional anisotropy (FA) was significantly increased in Nrnx2 α KO mice (genotype: $t_{(10)} = 2.50$, $p = 0.032$) and apparent diffusion coefficient (ADC) **(B)** significantly decreased (genotype: $t_{(10)} = 2.28$, $p = 0.046$). This difference appeared to be driven predominantly by radial diffusivity (RD), as axial diffusion (AD) **(C)** was not significantly different (genotype: $t_{(10)} = 1.49$, $p = 0.168$) whilst RD **(D)** was significantly reduced in Nrnx2 α KO mice (genotype: $t_{(10)} = 2.45$, $p = 0.034$). Error bars represent s.e.m. * = $P < 0.05$. Wild-type $n=6$, Nrnx2 α KO $n=6$.

Supp. Figure 11



Axial diffusivity (AD) and radial diffusivity (RD) of computed tracts of connections from the amygdala to hippocampus. Tracts from the anterior amygdala to the posterior hippocampus (Bregma -2.46 mm) were analysed for AD (**A**) and RD (**B**). No significant differences between the tracts of Nrnx2 α KO mice were observed. No significant differences were found for RD of tracts specifically from the basolateral nuclei of the amygdala (BLA) to the anterior (**C**) or posterior (**D**) hippocampus. Error bars represent s.e.m. Wild-type n=6, Nrnx2 α KO n=6.

Supp. Figure 12



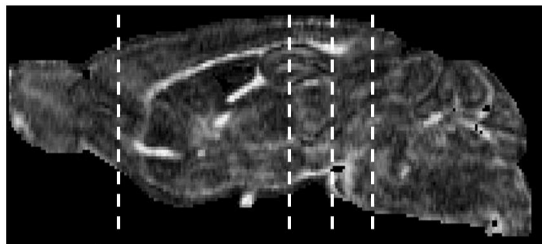
CLARITY-derived quantification of fibres and cell density within the basolateral amygdala (BLA) and control regions (**A**) Although there were trends towards increased axonal alignment and fibre density (**B**) in Nrnx2α KO mice, no significant differences were found. (**C**) Cell density in the BLA was similar between the genotypes. Statistical analysis (Supp. Table 4) was performed for the primary motor cortex (M1; **D-F**), primary somatosensory cortex (S1; **H-J**) and the barrel field (BF; **K-M**). No genotypic differences were found for any measure within these cortical regions. (**N-O**) CLARITY images of the scanned regions of interest. Error bars represent s.e.m. Wild-type n=6, Nrnx2α KO n=6.

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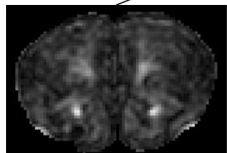
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Figure 1

A

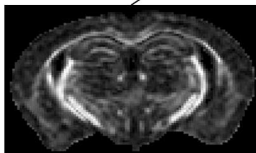


i



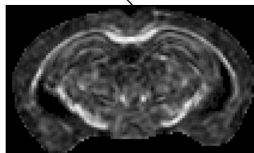
Bregma +2.58 mm

ii



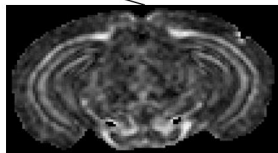
Bregma -1.94 mm

iii



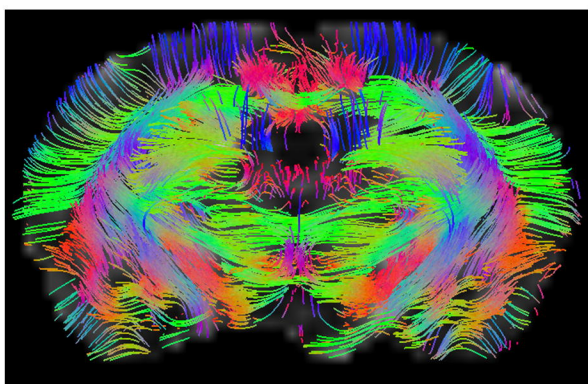
Bregma -2.46 mm

iv

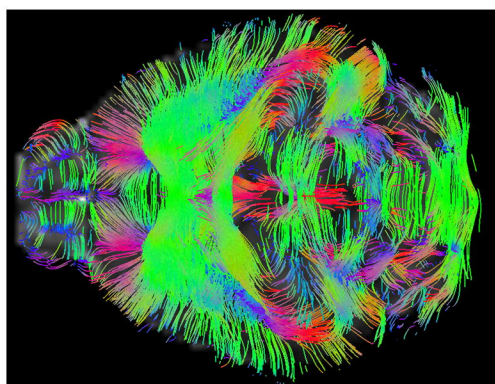


Bregma -3.28 mm

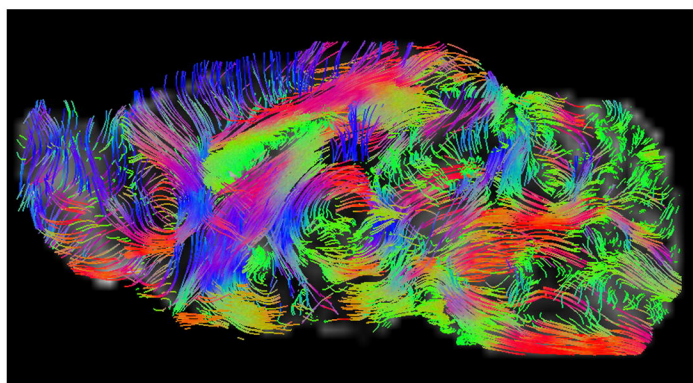
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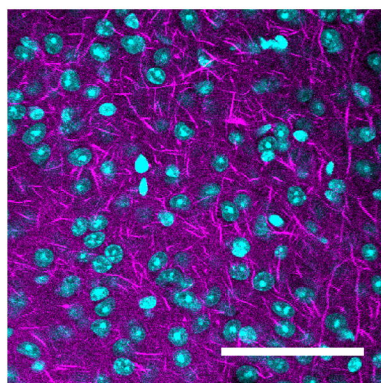
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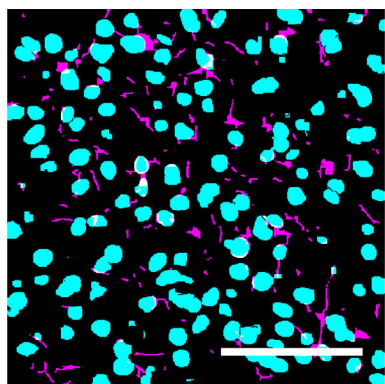
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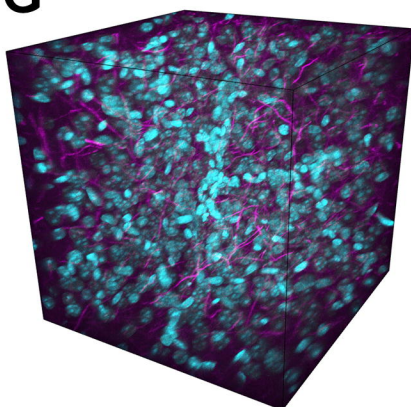
E



F



G



H

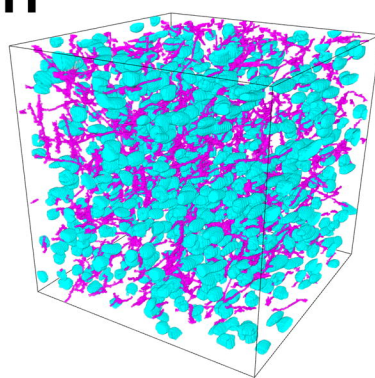


Figure 2

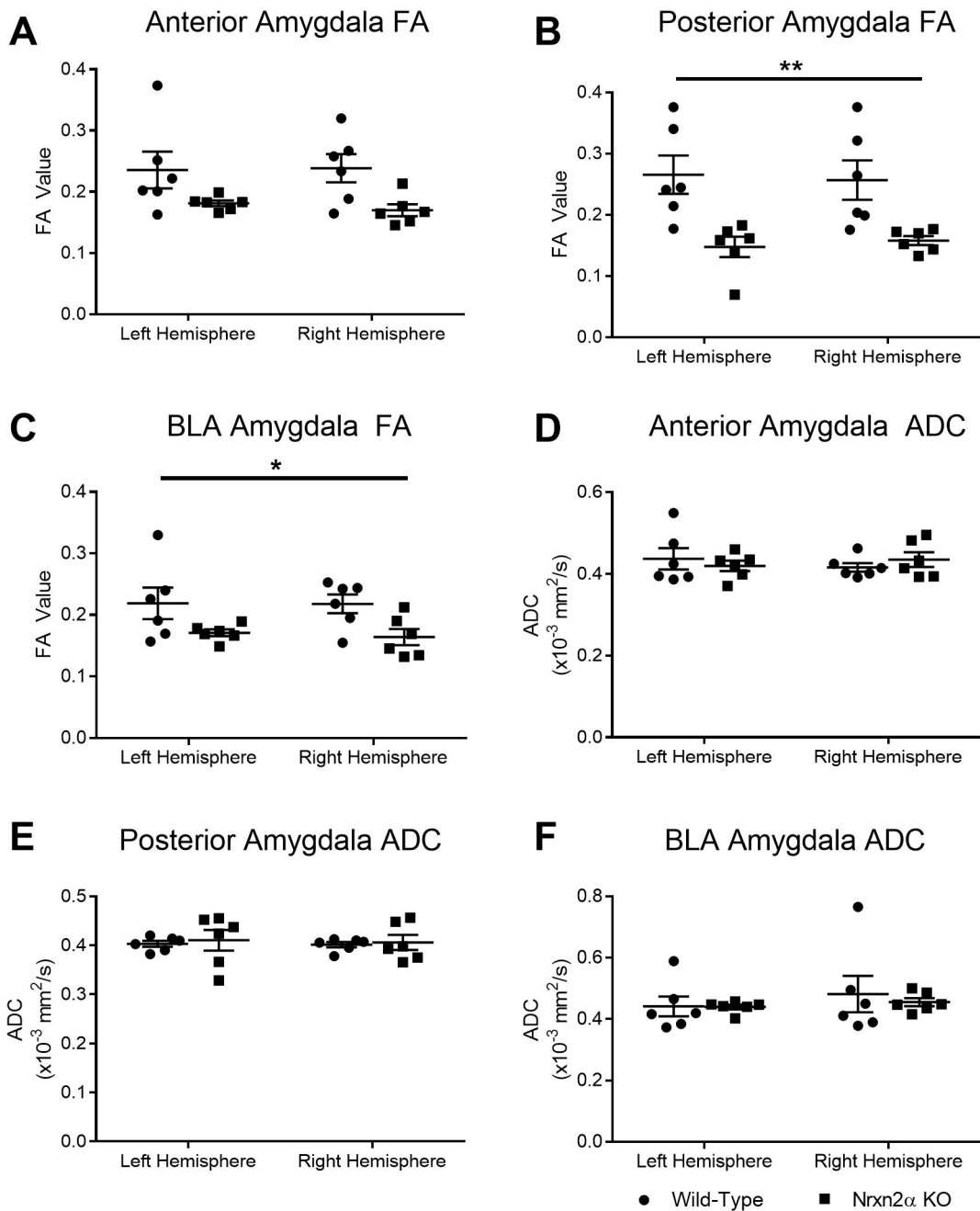


Figure 3

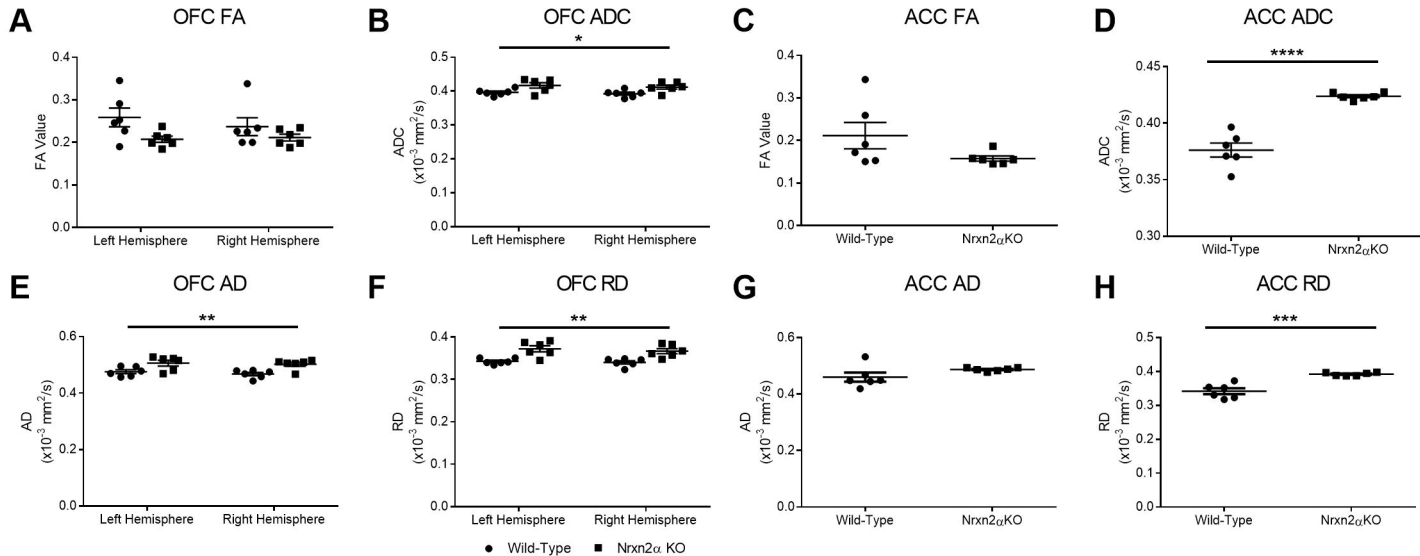


Figure 4

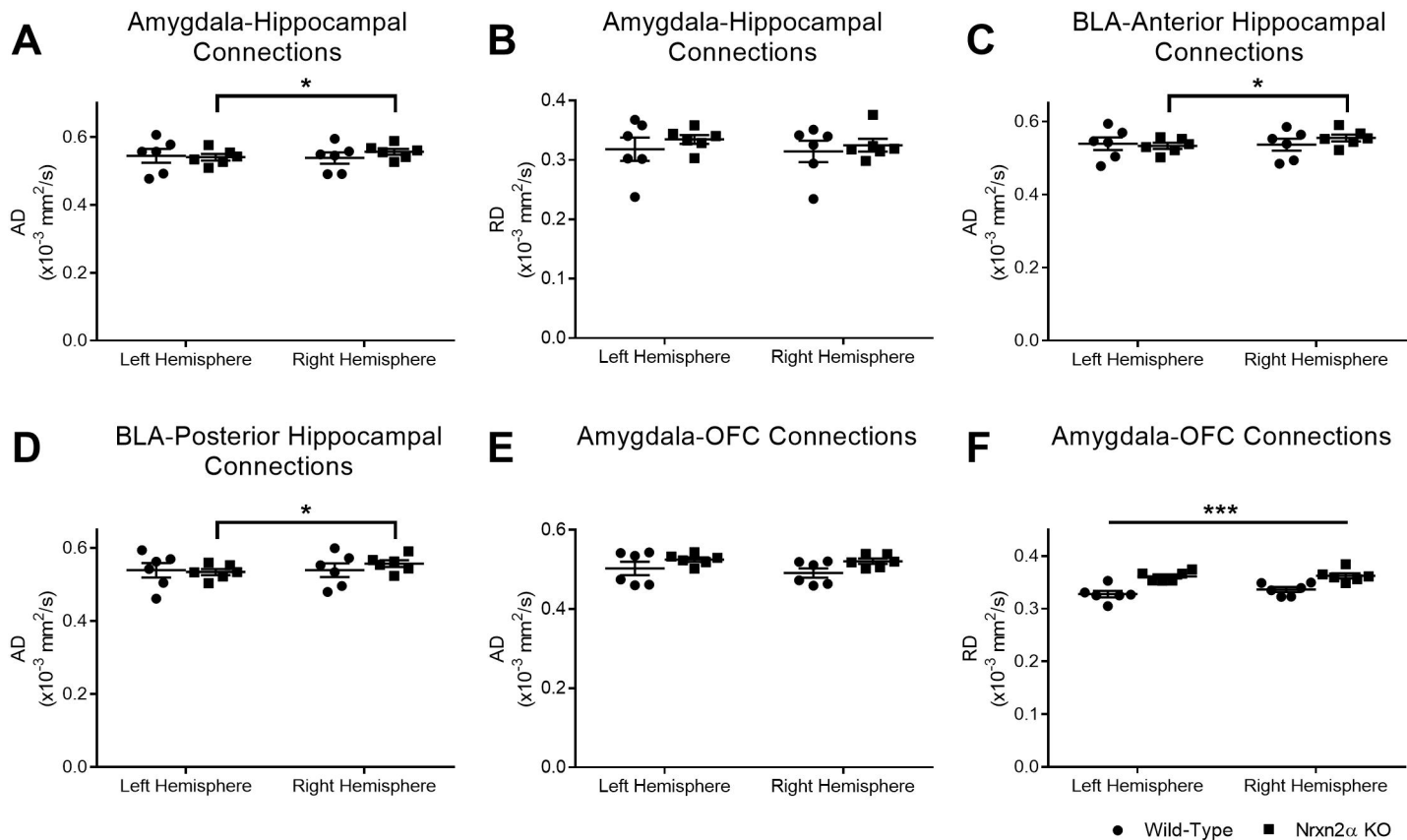
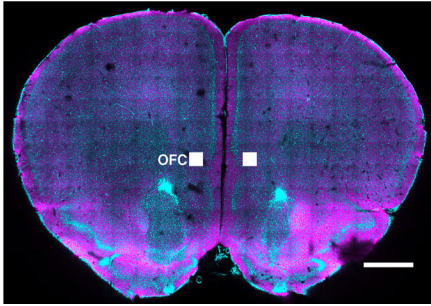
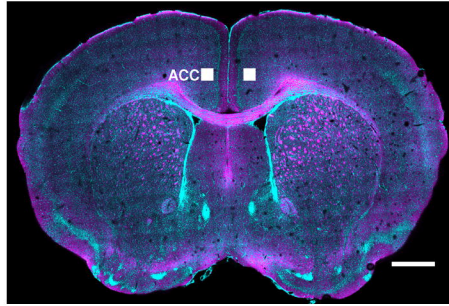


Figure 5

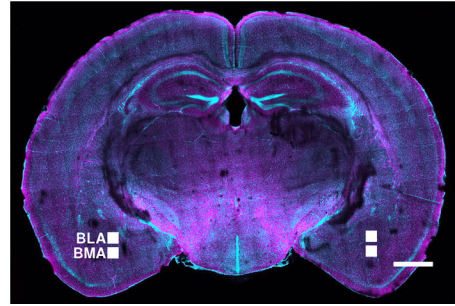
A



B

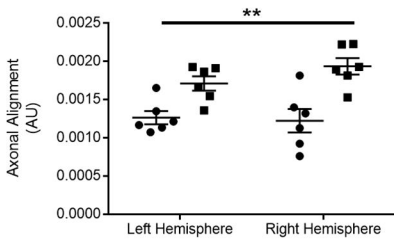


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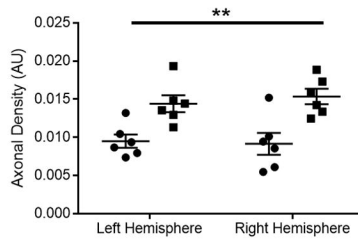
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ACC Axonal Alignment



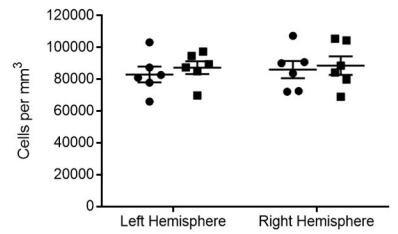
E

ACC Axonal Density



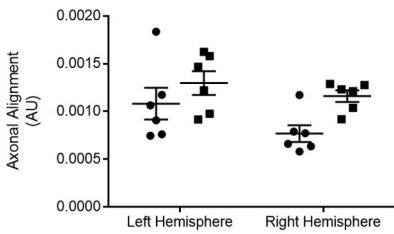
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ACC Cell Density



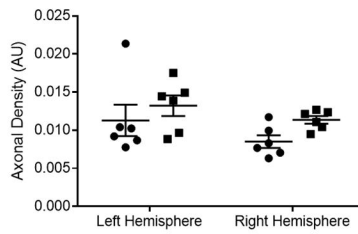
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Medial OFC Axonal Alignment



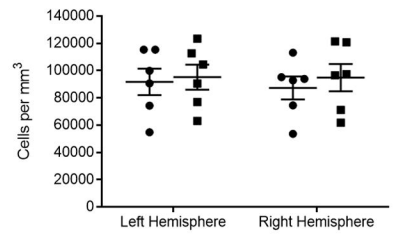
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Medial OFC Axonal Density



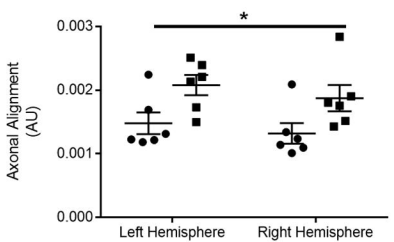
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Medial OFC Cell Density



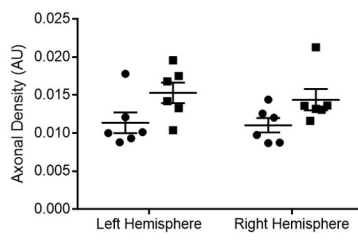
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BMA Axonal Alignment



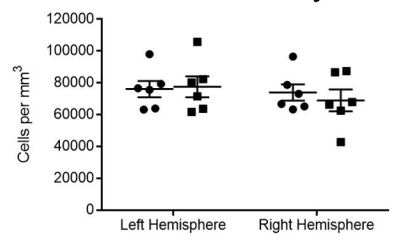
K

BMA Axonal Density



L

BMA Cell Density



● Wild-Type ■ Nrnx2α KO