

1 Individual heterogeneity in the functional network

2 topography of medial prefrontal cortex

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7 **Abstract**

8 Human medial prefrontal cortex (mPFC) and posterior cingulate cortex (PCC) are implicated in multiple
9 cognitive functions, including subjective valuation processes and processes linked to the default network (DN).
10 Our ability to interpret these seemingly co-localized effects is constrained by a limited understanding of the
11 individual-level heterogeneity in mPFC/PCC functional organization. Here we used cortical surface-based
12 meta-analysis to identify a parcel in human PCC that was preferentially implicated in DN effects relative
13 to valuation. We then used resting-state fMRI data and a data-driven network analysis algorithm, spectral
14 partitioning, to partition mPFC and PCC into “DN” and “non-DN” subdivisions in individual participants
15 (n = 100 from the Human Connectome Project). The spectral partitioning algorithm efficiently identified
16 individual-level cortical subdivisions that were reliable across test/retest sessions and varied markedly across
17 individuals, especially in mPFC. Our results point toward a new generation of strategies for assessing whether
18 distinct cognitive functions engage common or distinct mPFC subregions.

19 **Keywords:** brain networks; DN; individual differences

20 Introduction

21 Human medial prefrontal cortex (mPFC) and posterior cingulate cortex (PCC) are jointly associated with a
22 large and diverse set of cognitive functions (Hiser & Koenigs, 2018; Kragel et al., 2018). One such function is
23 subjective valuation during economic decision making. Both mPFC and PCC (together with ventral striatum)
24 consistently show greater BOLD activity in response to more highly valued choice prospects and outcomes,
25 relative to prospects and outcomes that are less highly valued (Bartra, McGuire, & Kable, 2013; Clithero
26 & Rangel, 2014; Hiser & Koenigs, 2018; Kable & Glimcher, 2007; Levy, Lazzaro, Rutledge, & Glimcher,
27 2011). Both mPFC and PCC are also among the regions implicated in a set of functions associated with the
28 default network (DN). DN effects include a decrease in BOLD activity during cognitively demanding tasks
29 compared with less-demanding task conditions or periods of rest (Laird et al., 2009; McKiernan, Kaufman,
30 Kucera-Thompson, & Binder, 2003), as well as a distinctive pattern of inter-region correlations in resting-state
31 fMRI data (Fox et al., 2005; Greicius, Krasnow, Reiss, & Menon, 2003; Yeo et al., 2011).

32 Coordinate-based meta-analyses of the fMRI literature show that valuation and DN effects occur in overlapping
33 and largely indistinguishable regions of ventral mPFC (Acikalin, Gorgolewski, & Poldrack, 2017). The two
34 sets of effects diverge in other brain areas; a region of the striatum is preferentially associated with valuation,
35 whereas bilateral temporoparietal junction is linked with the DN. Within PCC and adjacent precuneus,
36 a more posterior subregion appears DN-specific, whereas a more anterior subregion is implicated in both
37 effects. One possible interpretation of these findings is that mPFC and anterior PCC operate as common
38 nodes within partially overlapping distributed brain systems that subservise valuation and DN effects. This
39 colocalization has prompted theories that valuation and DN-related processes share common elements at the
40 psychological level. For example, the two sets of processes might share elements of self-referential cognition,
41 episodic memory, mental simulation, or monitoring and regulation of internal states (Acikalin et al., 2017;
42 Clithero & Rangel, 2014; Northoff & Hayes, 2011; Reddan, Wager, & Schiller, 2018).

43 However, strong conclusions about functional colocalization require consideration of individual-level hetero-
44 geneity in topographic patterns of brain activity. A recognized limitation of group averaging and meta-analysis
45 is that the functional topography of individual brains can be misaligned and blurred (Fedorenko, Duncan, &
46 Kanwisher, 2012; Guntupalli, Feilong, & Haxby, 2018; Michalka, Kong, Rosen, Shinn-Cunningham, & Somers,
47 2015; Tobyne et al., 2018; Wang et al., 2015; Woo et al., 2014), exaggerating the apparent overlap across
48 domains. This concern is especially pronounced in mPFC, which is subject to considerable idiosyncratic
49 cortical folding (Lopez-Persem, Verhagen, Amiez, Petrides, & Sallet, 2019; Mackey & Petrides, 2014; Zilles,
50 Palomero-Gallagher, & Amunts, 2013) and inter-subject functional variability (Mueller et al., 2013). An

51 alternative approach is to focus on analyses at the individual-participant level. Individual-level analyses of
52 fMRI data have identified idiosyncratic, reliable, and valid patterns of functional organization that would be
53 blurred in aggregative estimates (Gordon et al., 2017; Gratton et al., 2018; Laumann et al., 2015; Tobyne et al.,
54 2018), and subject-specific network arrangements have been found to predict behavioral characteristics (Kong
55 et al., 2018). Recent work has uncovered fine-grained subdivisions within the DN using both data-driven
56 clustering and individually customized seed-based connectivity analysis (Braga & Buckner, 2017; Braga, Van
57 Dijk, Polimeni, Eldaief, & Buckner, 2019). It is therefore possible that the previously reported overlap of DN
58 and valuation effects can be attributed to low effective spatial resolution, and that the organization of mPFC
59 and PCC would be better understood at the individual level. An important first step, and the goal of the
60 present paper, is to quantify the degree of topographic heterogeneity of DN effects within mPFC and PCC in
61 a large sample of individuals.

62 A useful way to characterize individual-specific brain organization is to examine patterns of resting-state
63 functional connectivity. Connectome-based analyses of resting-state functional connectivity have been fruitful
64 in identifying individualized functional subregions that correspond well to task-induced activity patterns
65 (Gordon et al., 2017; Laumann et al., 2015; Smith et al., 2009; Tobyne et al., 2018). A functional connectome
66 can be represented in the form of a network, and graph theoretic methods can be applied to analyze the
67 network's structure (Bassett & Sporns, 2017; Rubinov & Sporns, 2010). In the context of network analysis,
68 community detection algorithms subdivide brain networks into sets of nodes that share more connections
69 with each other than with the rest of the network (Fortunato & Hric, 2016; Garcia, Ashourvan, Muldoon,
70 Vettel, & Bassett, 2018). Here we use the technique of spectral partitioning (SP), an efficient community
71 detection algorithm that deterministically subdivides a network into two communities (Belkin & Niyogi, 2003;
72 Chung, 1997; Fiedler, 1975). SP has previously been used to characterize the posterior-anterior functional
73 gradient of the insula using resting-state fMRI data (Tian & Zalesky, 2018), and was shown to robustly
74 and reliably separate both simulated and actual primate ECoG networks (Toker & Sommer, 2019). We use
75 SP here to identify subsets of nodes within mPFC and PCC that share spontaneously covarying temporal
76 activation patterns.

77 In this study, we aimed to subdivide mPFC and PCC into individual-specific DN and non-DN communities,
78 and to quantify the degree of topographic heterogeneity in the resulting community structure over time and
79 across individuals. We did this by capitalizing on the respective strengths of meta-analysis and subject-specific
80 analyses of brain networks. First, we established a search space by selecting parcels from an established
81 brain atlas (Glasser et al., 2016) that corresponded to previously defined DN and limbic networks on the
82 medial cortical wall (Yeo et al., 2011). A cortical surface-based meta-analysis of the DN and valuation

83 literatures identified a parcel in PCC that was DN-specific at the aggregate level. We then derived a functional
84 connectivity network of all the surface vertices within the search space for each of 100 individual resting-state
85 fMRI data sets from the Human Connectome Project (HCP; Van Essen et al., 2012), and used the SP
86 algorithm to subdivide each individual’s network into DN and non-DN communities (labeled according to
87 which community included the meta-analytically identified DN-specific parcel in PCC). Focusing on individual
88 vertices in the search space rather than the parcels (as is typical in brain network analyses) allowed us to
89 finely delineate the topographic extent of each community. The resulting communities varied topographically
90 across individuals, while also appearing to follow common organizational principles. Sliding window and
91 test-retest analyses showed that these partitionings were highly similar across scanning days within (but not
92 between) individuals, and that individual-level idiosyncrasy was greater in mPFC. Partitionings obtained
93 from the SP algorithm had higher test-retest reliability than did analogous results from seed-based functional
94 connectivity. Lastly, we describe how the structure of the resulting automatically defined DN and non-DN
95 communities both aligns with and differs from recently proposed scheme for identifying subdivisions within
96 the DN (Braga & Buckner, 2017; Braga et al., 2019). Our work highlights the usefulness of estimating brain
97 effects at the individual level in mPFC and PCC, and provides a new framework and tool set for future
98 investigations of overlap across cognitive domains.

99 **Methods**

100 All code used in this study is openly available at https://github.com/ctoroserey/mPFC_partitioning

101 *Search space*

102 For all analyses, we defined our search space based on the 17-network parcellation proposed by Yeo et
103 al. (2011). First, we selected vertices on the medial cortical surface that were contained by the DN and
104 limbic networks in HCP’s 32,000 vertex surface space (fs_LR_32k). Next, we overlaid those networks on
105 a parcellated atlas of the human cortical surface (360 regions; Glasser et al., 2016), and retained a set of
106 parcels that covered approximately the same brain regions. This resulted in a search space that consisted of
107 40 parcels across hemispheres (Supplementary Table 1). The search space in each hemisphere was naturally
108 divided into two spatially non-contiguous clusters in PCC and mPFC, facilitating the examination of each
109 region separately.

110 *Meta-analysis*

111 We used a novel approach to cortical surface parcel-based meta-analysis to assess whether individual parcels
112 within the search space were preferentially associated with valuation or DN effects. For subjective valuation,
113 we gathered peak activation coordinates from 200 studies that were associated with positive effects in
114 contrasts of higher-value minus lower-value outcomes or prospects (Bartra et al., 2013). For DN, we acquired
115 coordinates from 80 studies that were related to task-deactivation (Laird et al., 2009). The coordinates
116 represent areas that exceeded the statistical significance threshold in each original study. For each study, we
117 created an indicator map in standard volumetric space (MNI152, 1 mm resolution) which contained values
118 of 1 in a 10 mm radius sphere around each reported activation peak, and values of 0 elsewhere (Wager,
119 Lindquist, Nichols, Kober, & Van Snellenberg, 2009). The indicator map for each study was then projected
120 to a standard cortical mesh (fsaverage, 160,000 vertices, projfrac-max from 0 to 1 by 0.25, registered using
121 mni152.register.dat) using FreeSurfer's mri_vol2surf (Dale, Fischl, & Sereno, 1999; Fischl, Sereno, & Dale,
122 1999) (<http://surfer.nmr.mgh.harvard.edu/>). We then resampled the Glasser et al. (2016) parcellation to
123 fsaverage, and tallied how many studies had positive indicator values intersecting with each cortical parcel (the
124 details of the resampling procedure are described in <https://wiki.humanconnectome.org/display/PublicData/HCP+Users+FAQ#HCPUsersFAQ-9.HowdoImapdatabetweenFreeSurferandHCP>, and were implemented
125 using a custom script available at <https://github.com/stobyne/Spherical-Surface-Swapper>). Two studies from
126 the subjective valuation corpus were removed because they did not contain activation peaks that overlapped
127 with cortex, leaving a final number of 198 studies.

129 To test for parcels that were significantly more strongly associated with one domain than the other, we
130 performed per-parcel chi-squared tests comparing the proportion of studies with activation in that parcel
131 between the two domains. We permuted the study domain labels (DN or valuation) 5000 times while
132 preserving the total number of studies in each domain, and on each iteration stored the maximum resulting
133 chi-squared statistic across all parcels. This gave us a null distribution of 5000 maximum chi-squared
134 values. The 95th percentile of this distribution served as an FWE-corrected significance threshold to evaluate
135 unpermuted chi-squared values.

136 *Resting-state fMRI Data*

137 Our fMRI analyses used resting-state fMRI data from the Human Connectome Project (Van Essen et al.,
138 2012) Q6 release (N = 100, randomly sampled from the total pool of 469 available subjects). Each subject's
139 data was acquired over two days at Washington University in St. Louis on a Siemens CONNECTOM Skyra

140 MRI scanner (Siemens, Erlangen, Germany). Four resting state runs (repetition time = 0.720 s, echo time
141 = 33.1 ms, flip angle = 52° , multiband factor = 8, 72 slices, 2 mm isotropic voxels) each comprised 1200
142 time points (14 min 24 s) for a total of 4800 time points. Two runs were acquired on each day, with the
143 phase encoding direction set to left-right for one run and right-left for the other. Only subjects with both
144 left-right and right-left phase encoding for each day were included (i.e. subjects with four resting-state fMRI
145 sessions). In addition, only datasets with low motion levels (under 1.5 mm) and less than 5% of points over
146 0.5 mm framewise displacement (FD) were used. See (Van Essen et al., 2012) for more details about the data
147 acquisition protocol.

148 Data initially underwent the HCP minimal preprocessing pipeline (Glasser et al., 2013), which included
149 gradient nonlinearity correction, motion correction, EPI distortion correction, high-pass filtering (0.0005
150 Hz threshold), MNI152-based normalization, surface reconstruction, and mapping of functional data to a
151 standardized cortical surface model (details can be found in Glasser et al., 2013). In addition, data underwent
152 temporal denoising based on independent components (FMRIB’s ICA-based X-noiseifier, FIX; Griffanti et al.,
153 2014; Salimi-Khorshidi et al., 2014). Data were further preprocessed using an in-house pipeline described
154 previously (Tobyne, Osher, Michalka, & Somers, 2017). Steps (in order) included linear interpolation across
155 high motion timepoints with over 0.5 mm of framewise displacement, band-pass filtering (allowed frequencies
156 ranged from 0.009 and 0.08 Hz), and temporal denoising via mean grayordinate signal regression (Burgess et
157 al., 2016). After filtering and denoising, the interpolated high-motion time points were censored by deletion
158 and each run was temporally de-meaned. The processed time series had a median of 4799 time points
159 (minimum = 4661) across participants. Each subject’s brain was comprised of 32k standard grayordinates
160 per hemisphere (combined in a CIFTI file). We retained only the cortical surfaces, which resulted in 59,412
161 total surface vertices per subject.

162 *Network Definition*

163 All network analyses were performed using the igraph package (v. 1.1.2; <https://igraph.org/r/>; Csardi &
164 Nepusz, 2006) in R (v. 3.4.1; <https://www.r-project.org/>; R Core Computing Team, 2017). To establish each
165 subject’s network, we selected all the vertices contained within the mPFC/PCC search space ($n = 4,801$ per
166 subject; mPFC = 2854, PCC = 1947) and computed the Pearson correlation of the time series for every pair
167 of vertices. This produced a weighted network for each subject, in which the nodes were surface vertices and
168 the edges were the correlations among them. Next, we applied Fisher’s r to z transformation, and performed
169 a two-sided significance test to identify significant connections. The resulting p-values were corrected for
170 multiple comparisons ($FDR < 0.05$), and edges with non-significant correlations were set to 0 (all other edges

171 retained their respective z-values). The proportion of remaining edges (i.e. network density) was high for all
172 individuals (mean = 0.78, SD = 0.024), and the retained edges mostly consisted of positive correlations (mean
173 proportion positive = 0.69, sd = 0.04). Next, we took the exponential of these values so that all weights were
174 positive while maintaining the ordinal ranks of the original correlation distribution within the set of retained
175 edges. Non-retained edges were reset to 0 to exclude them from the network analyses. We generated and
176 analyzed network weight matrices at four levels: (1) for each subject’s full concatenated dataset (up to 4800
177 TRs); (2) on each step of a sliding window analysis (see Partition Evaluation for more details); (3) for the
178 concatenated time series for the two runs on each day (up to 2400 TRs); and (4) for each run separately (up
179 to 1200 TRs).

180 *Community Detection*

181 Communities (i.e. clusters) were identified using the SP algorithm (Belkin & Niyogi, 2003; Chung, 1997;
182 Fiedler, 1975; Higham, Kalna, & Kibble, 2007). First, each network was represented as an $n \times n$ network
183 weight matrix W as described above (where n equals the number of vertices in the search space, 4,801). The
184 matrix was then transformed into its symmetric normalized Laplacian form

$$L = I - D^{-\frac{1}{2}}WD^{-\frac{1}{2}}$$

185 Where I is an identity matrix of size n , and D is a diagonal matrix containing the strength of each vertex
186 (i.e. the sum of its edge weights with all other vertices). This resulted in a matrix wherein each entry was the
187 negative normalized value of the connection (from 0 to 1) between any two vertices relative to their combined
188 connectivity strength, and with ones along the diagonal. The transformation ensures that every row sums to
189 zero. We then computed the eigenvalues and eigenvectors of the symmetric normalized Laplacian matrix, and
190 used the eigenvector associated with the second-to-lowest eigenvalue (traditionally called the ‘Fiedler vector’)
191 to divide the network into two. The Fiedler vector consists of a set of positive and negative values and is
192 binarized by sign to partition the network into two similarly-sized communities (Fiedler, 1975). In this way,
193 SP avoids producing communities that are too small to be physiologically meaningful (for example, small sets
194 of vertices that are spuriously correlated due to measurement noise). Given that this data-driven method does
195 not label the two communities or establish correspondence across participants, we defined each individual’s
196 “DN” community as that which contained the DN-specific PCC parcel identified in our meta-analysis. The
197 high density of the graphs ensured that SP did not face the issues associated with its use in sparse networks
198 (Fortunato & Hric, 2016).

199 In order to evaluate the validity of the resulting partitionings across community-detection methods, we also
200 estimated network communities using the more traditional approach of modularity maximization (Garcia et
201 al., 2018), based on the algorithm from Clauset et al. (2004). The method heuristically iterates through
202 many possible combinations of vertices, and selects the partitioning that maximizes the within-community
203 edge weights, relative to a random network containing the same number of edges and communities. Unlike SP,
204 modularity can fractionate a network into more than two communities. Agreement between the partitions
205 provided by the bounded and unbounded community detection methods would suggest the results are not
206 distorted by the restriction of SP to binary partitionings.

207 *Partition Evaluation*

208 We used the Adjusted Rand index (ARI) to evaluate the stability and topographical heterogeneity of the
209 communities within and across individuals (Hubert & Arabie, 1985), which was calculated using the “mcclust”
210 package in R (Fritsch, 2012). The ARI is a metric that quantifies the similarity between two alternative
211 clusterings of the same data. The base of the ARI is computed by the formula

$$\frac{a + b}{a + b + c + d}$$

212 where a is the number of pairs of nodes that were grouped together in both partitionings, b is the number
213 that were grouped separately, and c and d denote the number of nodes grouped together (separately) in one
214 partitioning, but separately (together) in the other. Therefore, the ARI estimates the fraction of all possible
215 node pairs that had the same status (connected or not) in both partitionings (with the denominator equal to
216 $n(n - 1)/2$). The resulting ratio is adjusted against a baseline given by the expectation assuming independent
217 partitionings to yield an index that ranges from 0 to 1, where 0 denotes the value expected by chance. This
218 means that even though differences are heavily penalized, positive ARI values compare favorably against
219 chance clustering (and the index can take negative values if the ratio given by the formula above falls below
220 the chance level). In short, the ARI quantifies the chance-corrected agreement between any two partitions
221 while being agnostic to the labeling scheme.

222 We performed a number of comparisons among partitions. First, we computed the degree of agreement between
223 SP and modularity per subject. SP and Modularity have been previously found to show underfitting and
224 overfitting tendencies, respectively, in their community detection performance in a diverse set of network types
225 (Ghasemian, Hosseinmardi, & Clauset, 2019), so alignment between the two algorithms would increase our
226 confidence in the validity of the resulting partitionings. Next, we compared the subject-level SP partitionings

227 across individuals, and calculated the mean pairwise ARI for the group. We then performed the same
228 evaluation for PCC and mPFC separately, and examined whether there were mean differences in overall
229 agreement within these regions by performing a paired permutation analysis (5000 iterations) on all pairwise
230 ARI comparisons across subjects.

231 To estimate the degree of variability of partitionings per individual we performed a sliding window analysis
232 (20 min windows, 1 min increments, median number of windows per subject = 37, range = 35 - 37), comparing
233 each window's resulting partitioning against the partitioning derived from the subject's whole data set.
234 A 20-min window has previously been found adequate for identifying stable community features in brain
235 networks (Gordon et al., 2017). We assessed whether the magnitude of the Fiedler vector value for a given
236 vertex (for the full subject-level data set) was associated with the stability of that vertex's sub-network
237 assignment across time windows. To do this, we fit a mixed effects logistic regression model, in which the
238 dependent variable was the proportion of times each vertex participated in the DN community across windows,
239 and the explanatory variables included a random effect of subject and a fixed effect of the Fiedler vector
240 value for that vertex (derived from their full time series). Based on this relationship, we identified a threshold
241 Fiedler vector value for each subject, such that above-threshold vertices were persistently associated with
242 either DN or non-DN more than 99% of the time.

243 We then estimated the level of agreement between network partitions estimated using data across individual
244 scan days (with 2 days per participant). If the functional organization estimated by SP is indeed individual-
245 specific, we should see higher agreement within individual (test/re-test across days) than across individuals.
246 We tested this idea by computing the ratio of the mean ARI within and between individuals. Ratios close to
247 one would denote similar within-participant and across-participant alignment, whereas ratios considerably
248 higher than one would suggest that partitions were more similar within-participant than across participants.
249 We then extended this idea by computing the agreement across individual runs (4 per subject). Similar to
250 the day-based analysis, we assessed whether run-level data showed higher agreement within-subject than
251 between subjects.

252 *Seed-based Resting-state Functional Connectivity versus Community Detection*

253 We evaluated the performance of the SP algorithm in comparison to a simpler partitioning approach based
254 on seed-based functional connectivity. Independently for each day (2 per individual), we estimated each
255 subject's DN partition in mPFC based on its vertex-wise functional correlations (Pearson) with the spatially
256 averaged activity across all vertices in PCC. We compared these seed-based maps with the unthresholded

257 Fiedler vectors produced by SP, with the sign of the Fiedler vector oriented so the DN community was
258 marked by positive values in every subject. We calculated three sets of across-day similarity values for each
259 individual: 1) between the two seed-based maps; 2) between the two SP-based maps; and 3) between seed-
260 and SP-based maps. Because the values in the maps were continuous-valued (and not categorical labels, which
261 would be amenable to ARI), we quantified the similarity between maps in terms of the spatial Spearman
262 correlation across vertices. These spatial correlations were meant to determine the test/re-test reliability
263 of each approach, as well as the overall level of agreement between them. For 7 subjects, the communities
264 produced with one of the days' data sets had split coverage of area 7m, and so our community labeling scheme
265 for the Fiedler vector produced a sign mismatch across days. ARI is robust to such labeling issues, but the
266 inconsistency produced strong negative correlations of the Fiedler vector across days for these individuals.
267 Visual inspection showed that the community layout was well aligned across days, and so we matched the
268 labeling of their partitionings based on the day that sufficiently covered area 7m.

269 The two methods were expected to produce somewhat similar results, but the one displaying greater within-
270 subject agreement across days should be preferred (for a discussion on the stability of functional networks
271 see (Gratton et al., 2018; Kong et al., 2018)). We therefore compared the within-subject spatial correlation
272 coefficients produced by each method through a paired permutation analysis. For each of the 100 individuals,
273 we computed the difference in inter-day correlations between methods, randomized the sign of these values
274 5000 times, and computed the mean of these differences on each iteration. The empirical difference in means
275 was then evaluated against this permuted distribution.

276 **Results**

277 *Meta-analysis*

278 We performed a coordinate-based meta-analysis to identify cortical surface parcels within mPFC and PCC
279 that were preferentially associated with the DN or valuation literature. Volumetric coordinates from 80
280 studies with task deactivation contrasts and 198 studies with valuation contrasts were projected onto a
281 cortical surface, and mapped to discrete parcels from a multimodal cortical parcellation (Glasser et al.,
282 2016) to produce a list of brain areas reported per study. The 40 parcels considered were limited to the
283 medial portion of the default and limbic networks defined by the Yeo et al. (2011) 17-network parcellation.
284 Domain-specificity was tested by first permuting the domain labels across studies (DN or valuation) to create
285 a null distribution for the maximum chi-squared statistic in the search space (see Methods for details). The

286 null distribution was used to identify regions that were reported significantly more often in one literature or
287 the other.

288 Figure 1 shows the proportion of times each parcel was reported for each domain, as well as the significant
289 differences between domains. The 95th percentile of the permuted chi-squared distribution was 8.87. Based
290 on this threshold, area 7m in PCC/precuneus was the only parcel to show a preferential association with
291 the DN bilaterally (Left: observed $\chi^2 = 10.07$, $p = 0.029$; Right: observed $\chi^2 = 18.89$, $p < 0.001$). The
292 adjacent area v23 exhibited a similar effect, albeit only unilaterally (Right: observed $\chi^2 = 11.51$, $p = 0.011$;
293 Left: observed $\chi^2 = 8.25$, $p = 0.067$). There appeared to be a bilateral preference toward valuation effects
294 in mPFC area 25 (Left: observed $\chi^2 = 12.91$, $p = 0.005$; Right: observed $\chi^2 = 12.83$, $p = 0.005$); however,
295 closer inspection suggested this effect was driven by subcortical foci centered in adjacent ventral striatum. No
296 other parcels were preferentially implicated in valuation relative to DN. We therefore selected area 7m as an
297 interpretable, bilateral reference point for labeling DN and non-DN communities in the analyses that follow.
298 We note that the area labeled 7m in the parcellation used here (Glasser et al., 2016) is different from (and
299 located inferiorly on the medial surface to) the non-DN area 7m discussed in previous work (Andrews-Hanna,
300 Reidler, Huang, & Buckner, 2010).

301 *Individual-level DN and non-DN communities*

302 Within the mPFC/PCC search space, we estimated the topography of the DN for each individual. Using
303 each individual's full time series (approximately 4800 total TRs from four 14-min scanning runs acquired
304 over two days), we calculated the full vertex-to-vertex correlation matrix for the 4801 surface vertices in the
305 search space. We represented each individual's correlation matrix in the form of a network, with cortical
306 surface vertices as nodes and thresholded/transformed correlation values as edge weights. We then applied
307 the SP community detection algorithm to partition the network into two cohesive functional communities.

308 Figure 2 shows a representative partitioning of the search space for a single participant (100307; additional
309 examples are presented in Supplemental Figure 1). The SP algorithm subdivides a network according to the
310 positive versus negative values in the Fiedler vector (the eigenvector related to the second-to-lowest eigenvalue
311 of the network's Laplacian matrix, see Methods). Since this is a data-driven approach, there is no a priori
312 labeling for the two communities. We assigned the DN label to the community that contained the DN-specific
313 PCC parcel from the meta-analysis (7m). We oriented each individual's Fiedler vector so positive values
314 corresponded to the DN community, and were assigned a value of 1 in the binarized partitionings (with 0
315 denoting non-DN). In qualitative terms, the resulting patterns contained substantial DN coverage in posterior

316 PCC (as dictated by our labeling strategy), with non-DN vertices in anterior PCC. The mPFC region tended
317 to include DN vertices in its ventral-anterior and dorsal-anterior areas, with a persistent non-DN pocket
318 between them. This non-DN section extended posteriorly into pregenual cingulate cortex (area a24).

319 Before evaluating the degree of generalizability of this topographic pattern across individuals, we examined
320 the validity of the partitionings by comparing them to results from an alternative community detection
321 algorithm, modularity maximization (Clauset et al., 2004). Modularity seeks to find the set of communities
322 that maximizes within-community connection weights relative to a null model. Since modularity is not
323 constrained to a predetermined number of communities, it was capable of finding more than two in our data
324 set. We quantified the cross-method agreement in terms of the Adjusted Rand Index (ARI; see Methods),
325 which measures the proportion of node pairs in a network that were either clustered together or separately in
326 both partitionings, while being agnostic to labeling schemes and controlling for chance clustering. The ARI
327 normally takes values ranging from 0 to 1, with 0 indicating chance agreement (but can take negative values
328 if the similarity falls below chance).

329 The two clustering methods had high agreement (mean ARI = 0.87, SD = 0.11). Modularity showed a
330 tendency to produce additional communities (median = 3, range = 2, 4). However, the additional communities
331 encompassed a small number of vertices (median = 14.5, IQR = 4 - 31.75) compared to the principal two
332 (median = 4786.5, IQR = 4769.25 - 4797), suggesting that a binary partitioning provided a reasonable
333 approximation of the network's true community structure.

334 Next, we examined the similarity of SP-based partitionings across individuals by computing the ARI between
335 every pair of subjects, and found modestly above-chance agreement overall (mean = 0.12, SD = 0.05).
336 Qualitative inspection of the community organization showed good alignment for PCC, whereas the pattern
337 in mPFC was consistent but shifted topographically across subjects. To quantify this heterogeneity in mPFC,
338 we calculated the between-subject ARI for each region separately (Figure 3). The functional topography
339 of PCC was better aligned across individuals (mean = 0.18, SD = 0.09) than mPFC (mean = 0.09, SD =
340 0.04; paired permutation, $p < 0.001$; Cohen's D = 1.34), although the mean ARI in mPFC still exceeded the
341 chance value of zero (Wilcoxon signed rank test, $p < 0.001$; Cohen's D = NA).

342 *Pattern variability over time*

343 We next sought to identify a set of temporally stable core nodes in each community. In order to estimate the
344 stability of partitions over time, we performed a sliding window analysis on each subject's full time series
345 (20 min windows shifting by 1 min). We compared the partitioning derived from each window with the

346 partitioning computed using the entire time series (Figure 4).

347 The mean ARI along each subject's time series was high for both PCC (mean = 0.59; SD = 0.14) and mPFC
348 (mean = 0.49; SD = 0.12), with significantly higher ARI for PCC (paired permutation, $p < 0.001$; Cohen's
349 $D = 0.71$). A subset of nodes showed exceptionally high stability, in that they were assigned to the same
350 community in every time window. The percentage of stable nodes ranged from 0 to 73% across individuals
351 (median = 50%, IQR = 32% - 60%).

352 We next tested whether the continuous-valued Fiedler vector (before binarization into discrete communities)
353 carried information about the stability of individual nodes. There is precedent in the literature for the idea
354 that the magnitude (and not just the sign) of the Fiedler vector values conveys important information about
355 the role of each node in the network (Gkantsidis, Mihail, & Zegura, 2003; Tian & Zalesky, 2018). Therefore,
356 we tested whether the magnitude of the eigenvector values was associated with the stability of nodes over
357 time. Specifically, we estimated the proportion of DN affiliations per node as a function of Fiedler vector
358 values, using a logistic mixed effects model (Figure 4). The model identified a positive significant relationship
359 between these features ($\beta = 211.54$, SE = 0.51, $p < 0.001$), signifying that vertices with higher absolute
360 Fiedler vector values were more persistent in their relationship with their corresponding community over
361 time.

362 These analyses suggest that there is potential value in thresholding the Fiedler vector as a means to identify
363 reliable DN and non-DN vertices on an individual subject basis. We therefore thresholded each subject's
364 Fiedler vector to produce these refined maps. For each individual, we estimated the threshold by selecting the
365 smallest absolute Fiedler vector value that yielded an average stability across suprathreshold nodes of 99%,
366 for positive (mean = 0.0132, SD = 0.0051) and negative (mean = -0.0144, SD = 0.0056) values separately.
367 Individuals without such stable nodes ($n = 17$) were not thresholded, and were included in the subsequent
368 analyses in unthresholded form. The median proportion of retained vertices per individual was 0.48 (IQR =
369 0.29 - 0.63). Sub-threshold vertices were set to zero in Fiedler vector maps and 0.5 in the binarized maps
370 (so that they would not bias the calculation of averages). Figure 5A shows the thresholded partitioning for
371 the same individual shown in Figure 2. The maps used in all subsequent analyses were thresholded by this
372 individualized criterion.

373 With these thresholded partitions, we recomputed the overall similarity across participants. Compared to
374 before, there was lower topographic agreement across individuals (mean ARI = 0.07, SD = 0.04). The same
375 was true for both PCC (mean = 0.11, SD = 0.07) and mPFC (mean = 0.04, SD = 0.03) separately, although
376 the significance of the differences between areas was preserved (paired permutation, $p < 0.001$; Cohen's

377 $D = 1.2$). Figure 5B shows the average of the thresholded partitions across all participants, denoting the
378 proportion of times a vertex was affiliated with the DN community. This summary illustrates the common
379 organizational layout of both communities, but also highlights the considerable variability across individuals.
380 To test the possibility that the higher inter-subject variability in mPFC was driven merely by lower signal
381 quality in the retained vertices, we quantified the temporal signal to noise ratio (tSNR) for each region, both
382 before and after thresholding. We calculated tSNR using time series that were not demeaned, but were
383 otherwise equivalent to the data originally used. In terms of tSNR variability across vertices within each region,
384 mPFC had overall greater spatial standard deviation both before and after thresholding (mPFC: pre-threshold
385 mean spatial SD = 33.96, post-threshold mean spatial SD = 30.15; PCC: pre-threshold mean spatial SD =
386 15.28, post-threshold mean spatial SD = 14.59). However, tSNR after thresholding was significantly higher
387 for mPFC than PCC (mPFC: mean = 77.72, SD = 14.54; PCC: mean = 64.78, SD = 10.32; permutation
388 p-value < 0.001, Cohen's $D = 1.03$). This reflected a significant increase in mean tSNR in mPFC as a result
389 of the thresholding step (pre-threshold mean = 66.5, SD = 7.87; paired permutation p-value < 0.001, Cohen's
390 $D = 0.96$), whereas the mean signal quality in PCC was unchanged (pre-threshold mean = 64.56, SD =
391 10.02; paired permutation p-value = 0.2388, Cohen's $D = 0.02$). In short, mPFC had higher overall tSNR,
392 albeit with greater variability across nodes. Applying the thresholding step allowed us to focus the analysis
393 on vertices with high signal quality.

394 *Test/re-test reliability across days*

395 The relatively high inter-individual variability seen in the aggregate map could reflect at least three factors:
396 (1) measurement noise, (2) dynamic variation in mPFC network organization, and (3) stable patterns of
397 functional organization that differ across individuals. To arbitrate among these possibilities, we examined
398 the test/re-test reliability of mPFC/PCC community structure across separate days of testing. Insofar
399 as the observed variability reflects individual-specific brain organization, across-day ARI values should be
400 consistently higher within-individual than between individuals (an example comparison for two individuals is
401 provided in Supplemental Figure 2). Figure 6 shows pairwise comparisons among ten example subjects for
402 PCC and mPFC separately (left).

403 Once again we found low alignment across individuals for PCC (mean = 0.08, SD = 0.06) and mPFC
404 (mean = 0.04, SD = 0.03), but both areas showed comparatively high levels of within-individual agreement
405 (PCC: mean = 0.36, SD = 0.14; mPFC: mean = 0.26, SD = 0.1). We calculated an index of relative
406 specificity by computing the ratio of each individual's across-day (within-participant) ARI to the mean of all

407 between-participant ARI values involving that individual. The index is expected to take on a value near
408 1 if partitionings are well aligned across individuals and/or are subject to a common level of measurement
409 noise. It is expected to exceed 1 insofar as functional network organization is reliable and individual-specific.
410 This index is intended to factor out the potential contributions of measurement noise or dynamic instability,
411 which would introduce variability both across individuals and across days.

412 Figure 6 shows ARI ratios for PCC and mPFC. A signed-rank test showed evidence for specificity (i.e. ratios
413 > 1) in both mPFC (median = 7.38, IQR = 5.93 - 8.77, $V = 5029$, $p < 0.001$) and PCC (median = 4.3, IQR
414 = 3.41 - 5.13, $V = 5034$, $p < 0.001$). Moreover, the ratios for mPFC were significantly greater than those for
415 PCC when compared with a paired permutation test ($p < 0.001$; Cohen's $D = 0.33$). These test/retest results
416 suggest that the topographic variability seen in mPFC arises at least in part from stable and subject-specific
417 organizational patterns.

418 *Test/re-test reliability across runs*

419 We extended the analysis of per-day data by examining whether the organization of the DN could be extracted
420 using per-run data only. The duration of each run (approximately 14 min) falls below a previously suggested
421 stability threshold for fMRI-based modularity estimations (Gordon et al., 2017). Nonetheless, high ARI ratios
422 would indicate that the SP algorithm can reliably estimate individual-specific patterns of DN organization
423 from a single run of data.

424 Run-specific SP results still captured unique organizational patterns to some degree, even though the overall
425 levels of agreement decreased (PCC between subjects: mean = 0.04, SD = 0.05; mPFC between subjects:
426 mean = 0.02, SD = 0.02; PCC within subjects: mean = 0.17, SD = 0.14; mPFC within subjects: mean
427 = 0.1, SD = 0.08). We again computed each subject's ARI ratio in order to quantify the specificity of the
428 partitions, this time using the mean of 6 across-run (within-participant) ARI values in the numerator of the
429 ratio (Figure 6, right).

430 As before, a signed rank test showed that both regions had ARI ratios significantly greater than 1 (mPFC:
431 median = 5.85, IQR = 4.29 - 7.84, $V = 5025$, $p < 0.001$; PCC: median = 3.51, IQR = 2.36 - 4.4, $V = 4961$,
432 $p < 0.001$), and ratios for mPFC were higher than those of PCC (permutation $p = < 0.001$; Cohen's $D =$
433 1.1). This result further confirms that the intrinsic functional organization of mPFC is uniquely arranged
434 per individual, and provides evidence that information about such patterns can be extracted from relatively
435 small amounts of data.

436 *Correlation vs community detection in mPFC*

437 We next explored the possible advantage of community detection relative to a more conventional seed-based
438 functional connectivity analysis for estimating the individual-specific functional topography of mPFC. We
439 examined whether maps generated with SP were more similar per participant across days than those computed
440 from seed-based correlations. We generated a seed time-series by averaging all vertices in the PCC region
441 of our search space, and calculated its correlation with the activity of each vertex in mPFC. We compared
442 the map of correlation values in mPFC to the map of unthresholded Fiedler vector values using Spearman
443 correlations across vertices. Pairwise spatial correlations were calculated among maps computed for each
444 day and method from all individuals. Figure 7A shows that these pairwise comparisons resemble those from
445 the across-day comparisons above, and suggests good alignment between methods, but particularly high
446 agreement within subject and method.

447 Figure 7B shows the test/re-test reliability across days for patterns derived using community detection, seed-
448 based correlation, and across methods (e.g. Day 1 community detection versus Day 2 seed-based correlation).
449 While both approaches were reliable, community detection displayed a significantly higher mean correlation
450 coefficient across days than seed-based correlation (Community: mean = 0.7, SD = 0.26; Seed-based: mean
451 = 0.63, SD = 0.12; paired permutation $p = 0.007$; Cohen's D = 0.32). Agreement across methods was fair
452 (mean = 0.45, SD = 0.24), signifying that the two approaches identified similar topographic features but
453 also had systematic differences. These findings suggest that graph-theoretic community detection algorithms
454 are advantageous for detecting stable functional topologies, in addition to their other advantages of being
455 data-driven, unbiased and observer agnostic.

456 *Alignment of mPFC community structure with a proposed DN sub-network organization*

457 The thresholded partitions we identified had conceptual and topographic similarities to DN sub-networks A
458 and B proposed by Braga and Buckner (2017). We explored the relationship between the two sets of sub-
459 regions by reproducing their seed-based connectivity approach in two of our subjects. In their original work,
460 Braga and Buckner (2017) manually selected individual vertices in areas including the dorsolateral prefrontal
461 cortex (DLPFC), temporo-parietal junction (TPJ), and parahippocampal cortex (PHC) that produced two
462 spatially anticorrelated networks (Braga & Buckner, 2017; Braga et al., 2019). We hypothesized that if the
463 SP communities corresponded to one or both of the previously proposed sub-networks, our partitionings
464 should match networks A and B generated by seed-based functional connectivity in these diagnostic areas.
465 For whole-brain functional connectomes from two individuals (100307 and 101006), we selected seeds for

466 networks A and B in TPJ, and confirmed their placement based on functional connectivity patterns observed
467 in TPJ, PCC, DLPFC, and PHC (correlation coefficients thresholded at 0.2), as stipulated by Braga et al.
468 (2019). The whole-brain seed-based functional connectivity maps for two individuals are juxtaposed with
469 the corresponding community detection results in Figure 8. Visual inspection of these networks shows high
470 similarity between our DN community and the previously reported sub-network A. However, the non-DN
471 community filled areas not covered by either DN-A or DN-B. This result supports the idea that the two
472 approaches serve complementary purposes. Whereas Braga and colleagues (2017; 2019) identified subdivisions
473 within the DN, the present community detection approach might be better understood as partitioning DN
474 from non-DN cortex.

475 Discussion

476 A considerable amount of meta-analytic work has been dedicated to characterizing the brain activity patterns
477 associated with psychological processes in medial prefrontal cortex (mPFC), revealing both dissociable and
478 overlapping activation across domains (De La Vega, Chang, Banich, Wager, & Yarkoni, 2016; Hiser & Koenigs,
479 2018; Kragel et al., 2018). In particular, activation patterns associated with subjective valuation and with
480 the default network (DN) have been suggested to be inseparable in this area, with overlap also partially
481 extending to posterior cingulate cortex (PCC) (Acikalin et al., 2017; Bartra et al., 2013; Clithero & Rangel,
482 2014; Laird et al., 2009). This apparent neural overlap has important implications, as it has motivated
483 theoretical proposals about ways in which these superficially dissimilar domains might involve a shared set of
484 core cognitive processes (Acikalin et al., 2017; Clithero & Rangel, 2014; Northoff & Hayes, 2011).

485 However, the interpretation of overlap in group-level data depends on the degree to which functional
486 organization is heterogeneous across individuals. Recent studies have shown that heteromodal brain regions
487 have considerable variability in functional connectivity across individuals (Mueller et al., 2013), individual-
488 specific functional topography can be occluded in aggregative estimations (Braga & Buckner, 2017; Gordon
489 et al., 2017; Michalka et al., 2015; Tobyne et al., 2018), and overlap in functional activation can vanish
490 with increases in spatial precision (Woo et al., 2014). These findings suggest that group-level and meta-
491 analysis-level overlap does not necessarily imply overlap in individual brains. However, our understanding of
492 the individual-level heterogeneity in the functional topography of mPFC has been mostly descriptive so far
493 (Braga & Buckner, 2017; Braga et al., 2019; Gordon et al., 2017). To affirm that DN and valuation share
494 neural substrates in this area requires a method to reliably and precisely capture the functional topography
495 of mPFC in isolated individuals, as well as a quantitative estimate of the degree of topographic heterogeneity

496 across a large group of individuals.

497 Here we address these challenges by using spectral partitioning (SP), a graph-theoretic community detection
498 algorithm that efficiently separates a network into two (Fiedler, 1975; Higham et al., 2007; Toker & Sommer,
499 2019). For 100 individuals, we subdivided brain regions that typically show overlap between DN and valuation
500 effects into DN and non-DN communities. Restricting our analyses to a general mPFC/PCC search space
501 made it appropriate to use a technique that identified a vertex-wise, binary partitioning that was sensitive
502 to the complex topography of the brain. This contrasts with whole-brain network analyses, which need
503 to allow for multiple sub-networks and which often use parcels that are several orders of magnitude larger
504 than vertices as the units of analysis. Partitioning an individual's brain network through SP has a number
505 of advantages, including identifying communities deterministically, constraining communities to contain a
506 similar number of vertices (i.e. preventing the allocation of most vertices to a single community), providing
507 continuous values that relate to the strength of a node's community affiliation, and the ability to diagnose
508 the connectedness of a network through examination of its resulting eigenvalues (Chung, 1997; Higham et al.,
509 2007). Comparisons with partitionings formed by modularity maximization, which heuristically determines
510 the ideal number of communities (Garcia et al., 2018), suggested the binary partitioning was appropriate.

511 We found a generalizable pattern across individual partitionings, in which the DN community covered
512 ventral/dorsal mPFC and posterior PCC, with the non-DN community concentrated in pregenual ACC and
513 anterior PCC. The precise spatial positioning of this general community structure was highly heterogeneous
514 across individuals, yet stable across test/re-test evaluations within-individual. The idiosyncrasy in functional
515 topography was particularly pronounced in mPFC, and was identified in both run-based and day-based
516 analyses. Individual-specificity could theoretically arise from a variety of sources. For example, the functional
517 topography of mPFC could be governed by its underlying sulcal and gyral organization, which has been
518 shown to vary systematically across individuals (Lopez-Persem et al., 2019; Mackey & Petrides, 2014).
519 Individual variability could also be due to shifts in functional organization that are independent of structural
520 features (Conroy, Singer, Guntupalli, Ramadge, & Haxby, 2013), or be characterized by the pattern of
521 functional connections with the rest of the brain (Mars, Passingham, & Jbabdi, 2018; Passingham, Stephan,
522 & Kötter, 2002; Tobyne et al., 2018). An important goal for future work will be to assess whether the network
523 layout in this region can be predicted on the basis of aspects of brain structure, such as sulcal morphology,
524 myeloarchitecture (Glasser et al., 2016), or structural connectivity (Osher et al., 2016; Saygin et al., 2011,
525 2016).

526 Network-partitioning methods such as SP are data-driven, and therefore provide no labeling information
527 about the resulting communities. We circumvented this issue by independently identifying the DN community

528 based on its coverage of area 7m, a region in PCC that was preferentially associated with the DN relative
529 to subjective valuation in our meta-analysis. We were able to apply labels derived from this group-level
530 approach on the basis of the topography in PCC, where functional organization was more consistent across
531 individuals. Because each community spanned both mPFC and PCC, the labels extended to mPFC where
532 topography was more heterogeneous.

533 Our results extend previous work that described individual-specific brain organization. Several recent
534 investigations have identified topographic heterogeneity using a different data aspect ratio than we used here
535 (a small number of individuals and a large number of scanning sessions per individual; Braga & Buckner, 2017;
536 Braga et al., 2019; Gordon et al., 2017). Previous work has also shown that functional correlations among
537 pre-defined cortical parcels are highly stable within an individual (Gratton et al., 2018; Kong et al., 2018).
538 Here we were able to quantify the variability and stability of functional topography in a large sample at a
539 fine, vertex-level spatial granularity, using moderately low amounts of data (down to a single 14 minute scan).
540 The motivation to sub-divide DN also stems from recent work by Kernbach et al. (2018), which identified
541 specialized communication of parcels within DN with the rest of the brain in a large pool of individuals.

542 In addition to the technical advantages noted above, the SP algorithm offers analytical advantages specific to
543 neuroscience. We found that SP outperformed a traditional seed-based correlation approach in capturing
544 idiosyncratic functional topography. Community detection methods such as SP are stabilized by relying
545 on all pairwise correlations among cortical vertices (rather than correlations with an individual seed). In
546 addition, we found we could increase the temporal stability of SP results by thresholding the underlying
547 Fiedler vector. The magnitude of Fiedler vector values has been recently used to characterize the continuous
548 connectivity profile of the insula with the rest of the brain, challenging the notion of discrete parcellations
549 in that region (Tian & Zalesky, 2018). The combination of discrete classification and graded information
550 yielded by SP provides additional flexibility and richness relative to some other clustering algorithms.

551 The community organization of PCC and mPFC was congruent with DN sub-networks A and B proposed
552 by Braga & Buckner (2017; Braga et al., 2019). The topography of our thresholded DN community closely
553 matched network A, whereas our non-DN community included cortical territory that was not part of either
554 DN network. Subthreshold vertices from the DN community overlapped with DN-B vertices, suggesting that
555 this sub-network could act as a dynamic intermediary between DN-A and other networks. Our findings
556 therefore complement the initial identification of DN sub-networks by quantifying the systematic variability
557 of their underlying topography in a larger group of people. Understanding the interaction of networks A
558 (DN), B, and non-DN is an important goal for future research. These two sets of results collectively suggest
559 that canonical DN regions can be topographically partitioned into DN and non-DN communities, and that

560 the DN community can in turn be further divided into sub-networks A and B.

561 Our findings show that the functional topography of mPFC is variable across a large pool of individuals,
562 and that the SP algorithm is a useful tool for identifying individualized topography in a data-driven way.
563 The ability to capture an individual's functional topography without the need of group priors is clinically
564 relevant, as it could help characterize heterogenous changes in mPFC activity in disorders such as depression
565 and schizophrenia (Hiser & Koenigs, 2018). It will be beneficial for future task-based fMRI experiments
566 to be able to characterize where task-evoked activity is situated relative to an individual's overall mPFC
567 organization. Our work was originally motivated by the apparent spatial overlap between subjective valuation
568 and the default network (Acikalin et al., 2017), but additional distinctions of interest include valuation versus
569 episodic memory functions (Euston, Gruber, & McNaughton, 2012), self-referential thought and theory of
570 mind (Mitchell, Banaji, & Macrae, 2005), and potential topographic distinctions among multiple forms of
571 valuation (Clithero & Rangel, 2014; Shenhav & Karmarkar, 2019; Smith et al., 2010). An individualized
572 frame of reference will enhance the ability of future studies to gauge similarities and differences among brain
573 activity patterns associated with diverse psychological domains.

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582 **Figures**

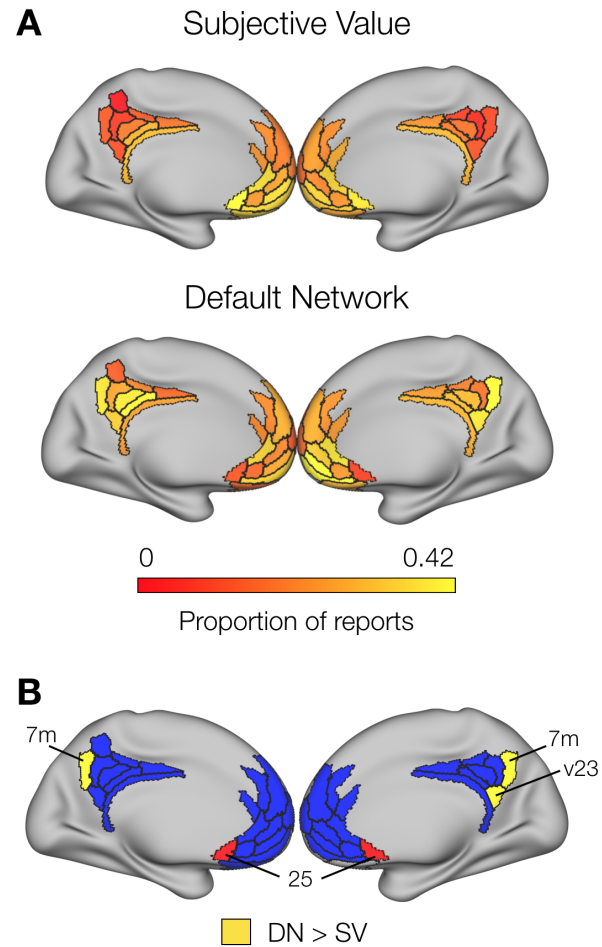


Figure 1: Meta-analysis results. A: Proportion of times each ROI was reported in the valuation and DN literatures. B: Regions identified in permutation-based chi-squared tests contrasting the two literatures (see text for details). Areas in blue represent the remainder of the search space.

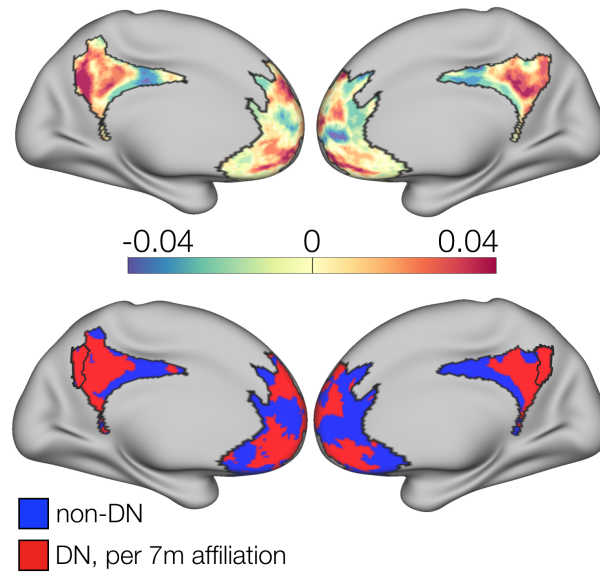


Figure 2: Brain partition for an example subject (100307). Fiedler vector values (top) are mapped onto the brain surface, dividing it into positive and negative communities. The bottom brain shows the binarized Fiedler vector, with red areas denoting the DN community (as indicated by coverage of area 7m, bordered).

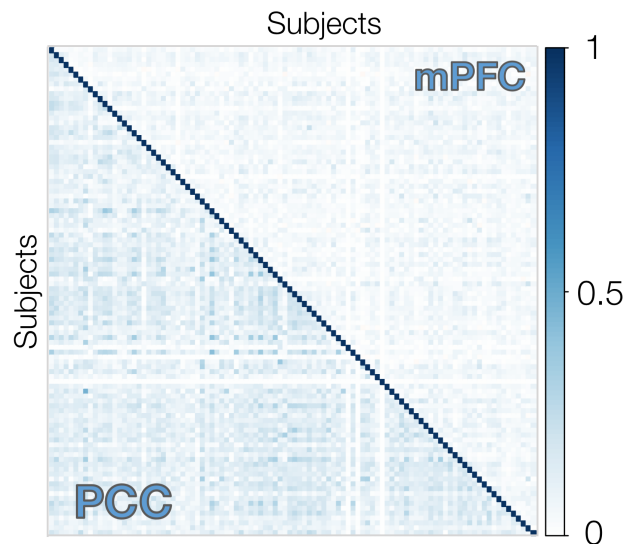


Figure 3: Similarity matrix showing ARI values among all subjects for PCC (lower triangle) and mPFC (upper triangle) separately. Functional topographic patterns were better aligned across individuals in PCC than mPFC.

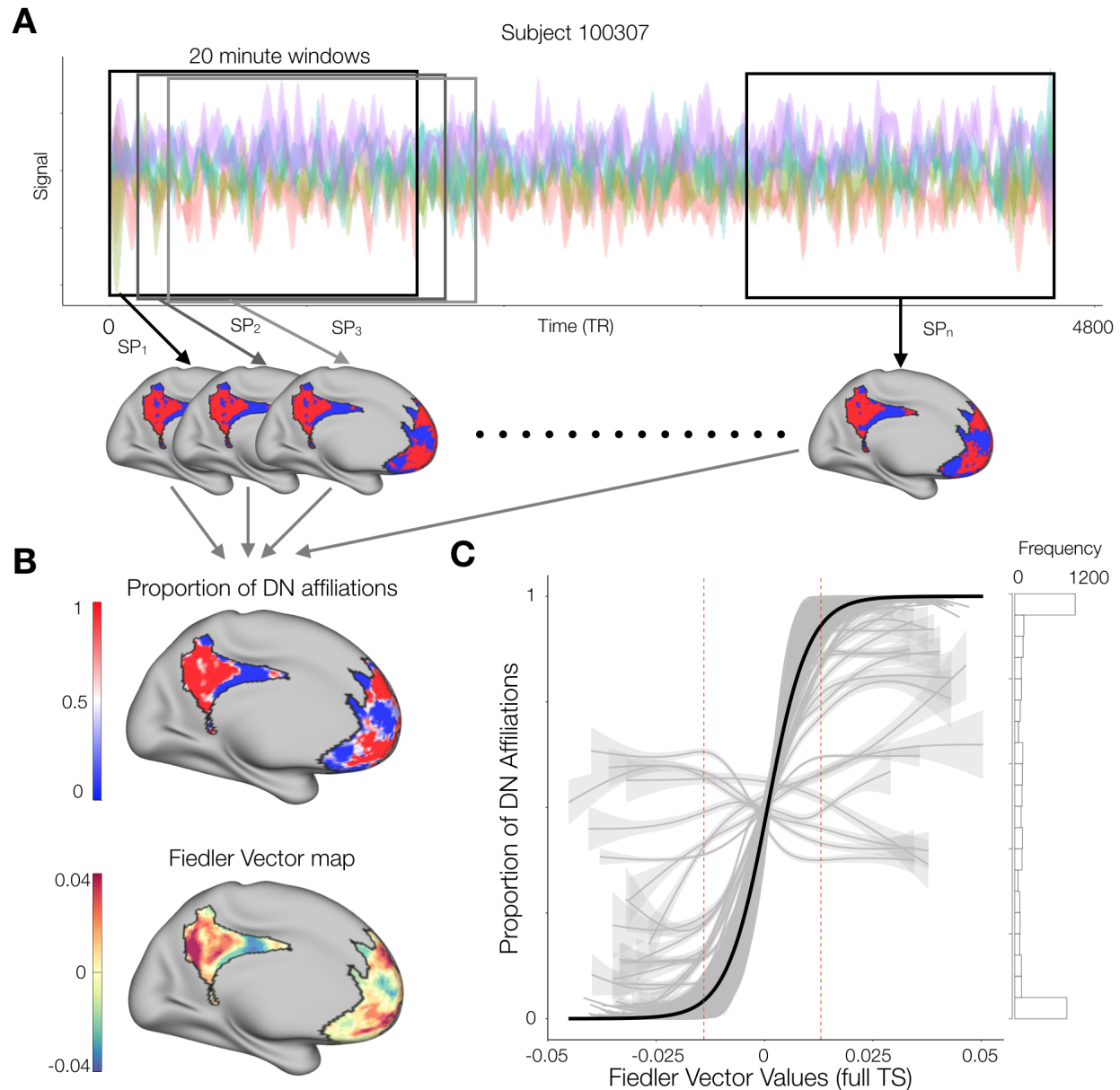


Figure 4: A: For each individual, we produced partitions for each 20 minute sliding window (84 TRs). B: Proportion of times each vertex was affiliated with the DN community across windows (upper), and the continuous Fiedler vector map for the current subject using their full time series (lower). The maps share considerable qualitative similarities in their gradients along the cortical surface. C: Relationship between the magnitude of Fiedler vector values and the proportion of DN affiliations. Grey lines display data for each subject, and the black line shows the fit from a mixed-effects logistic regression. Dashed red lines indicate the mean FV value at which maps were thresholded. The histogram displays the mean frequency distribution of y-axis values.

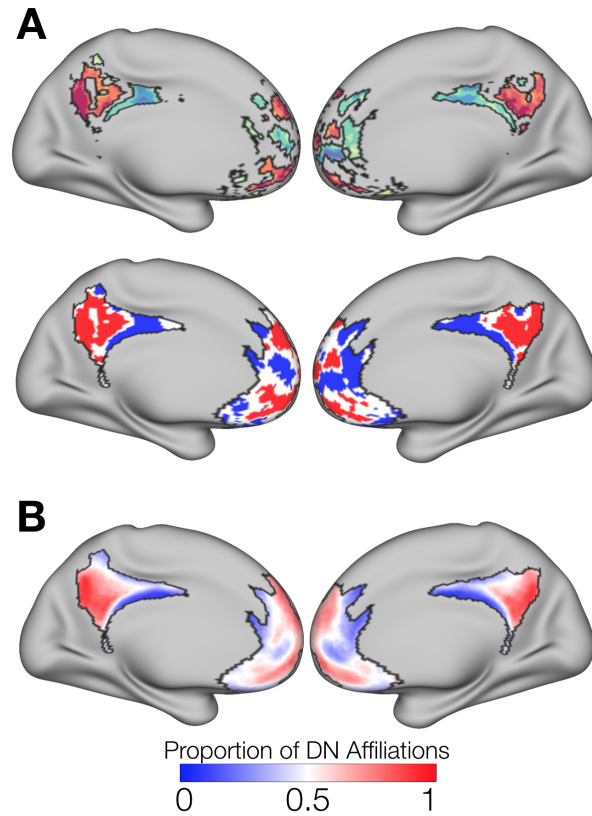


Figure 5: A: Thresholded Fiedler vector maps for subject 100307 (top), and its binarized form (bottom). Subthreshold values effectively formed a third community of high-variability vertices. B: Mean of the binarized maps across all participants, indicating the proportion of DN affiliations per vertex in our sample. This aggregate map shows the common organizational principle of the DN and non-DN communities, while also showing the high level of variability in mPFC.

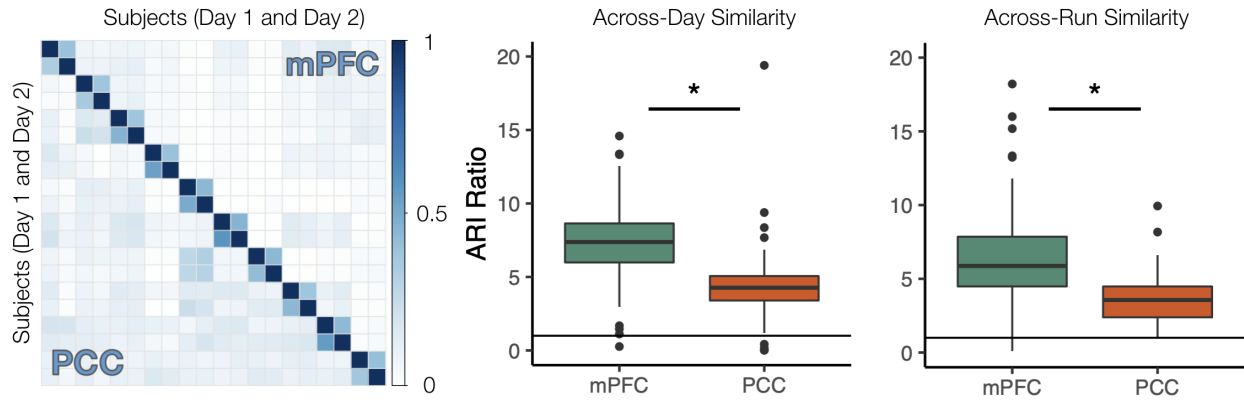


Figure 6: Left: Similarity matrix for 10 example participants (2 scanning days each), showing pattern agreement across days and subjects for PCC and mPFC separately. The block-diagonal structure is indicative of test-retest reliability across days within an individual. Middle: ratio of within-subject ARI to between-subject mean ARI for all individuals across days suggests idiosyncratic community arrangement for both PCC and mPFC (ratios > 1 , solid line), with greater subject-specificity in mPFC. Right: within-to-between subject mean ARI ratios for run-specific partitionings again show greater subject-specific organization for mPFC.

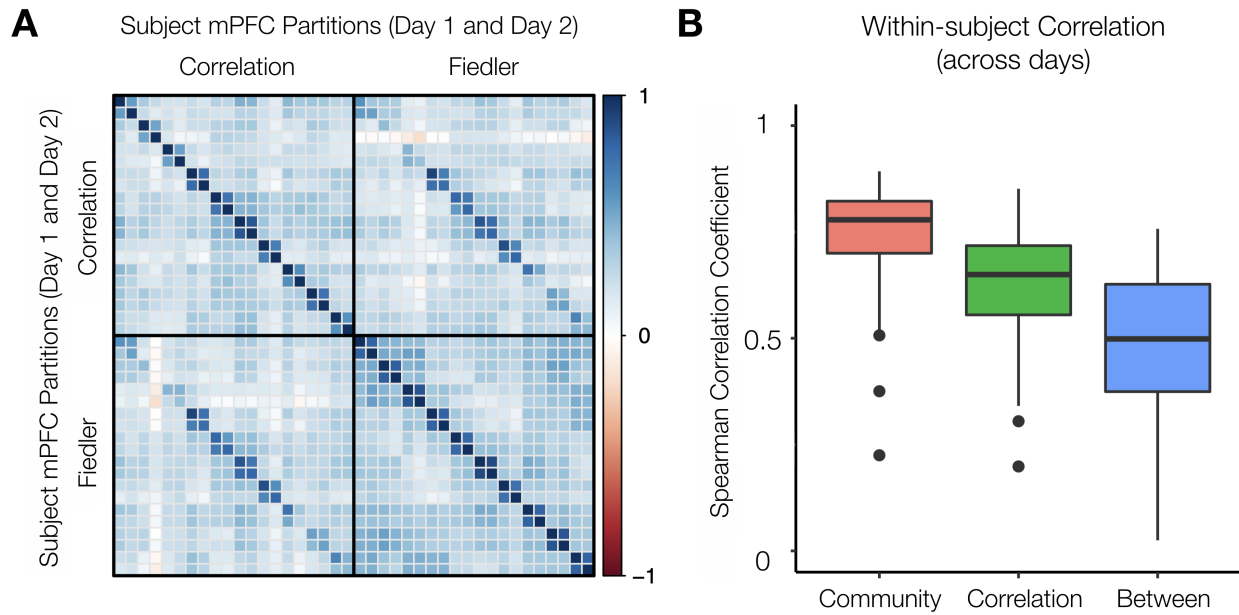


Figure 7: A: Correlation matrix comparing the across-day spatial stability of mPFC maps derived from seed-based functional connectivity (using a PCC seed) and the Fiedler vector for 10 example subjects. The top-left quadrant represents seed-based FC maps, and the bottom-right the Fiedler vector, with two single-day-based maps per individual. The upper-right and lower-left quadrants show across-method agreement. B: Day 1 vs Day 2 within-subject correlation coefficients for each method, as well as between methods. Community detection through spectral partitioning provided more stable estimates, even though both methods showed good levels of agreement.

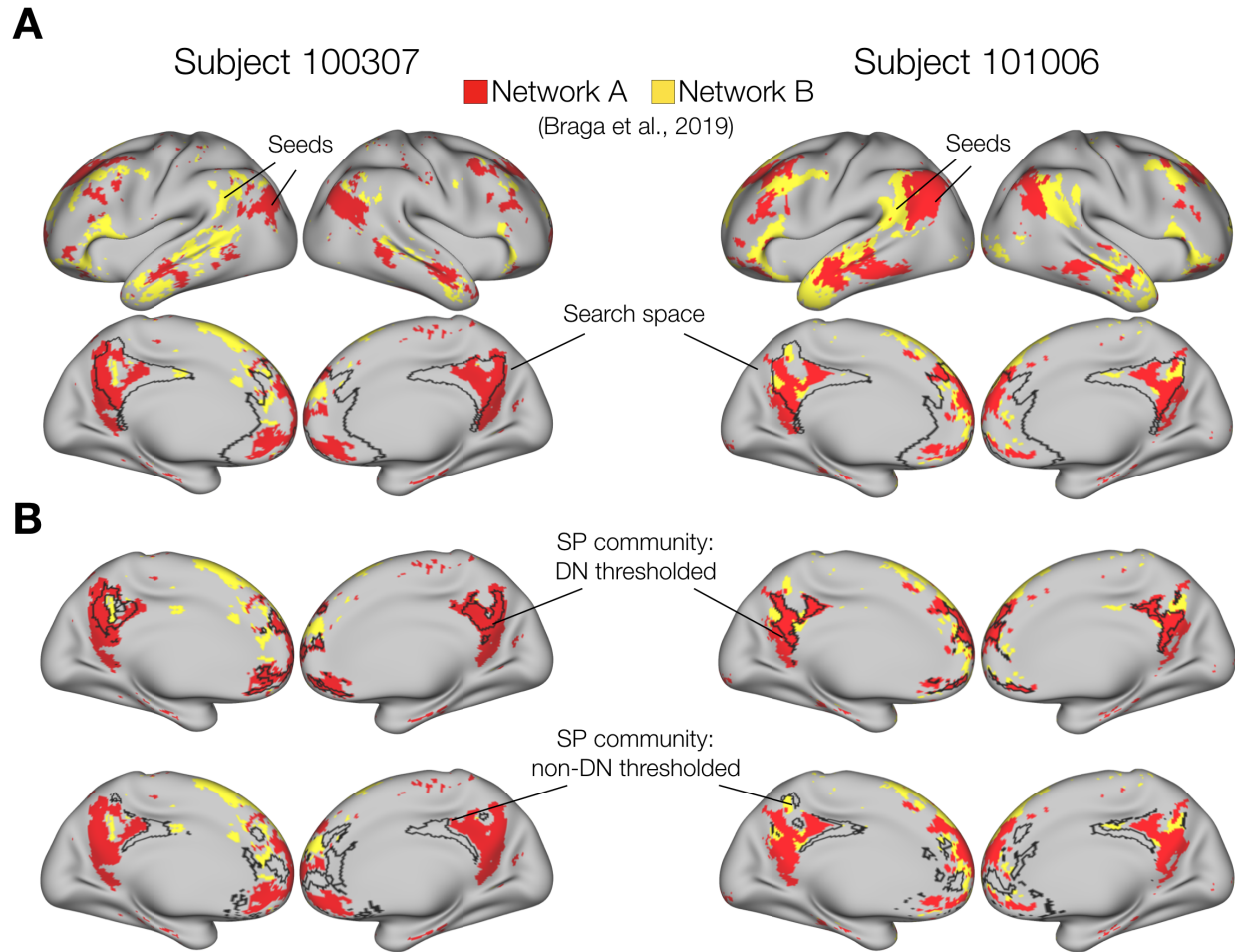


Figure 8: Qualitative comparison between DN sub-networks A and B from Braga et al. (2019) and SP communities for two individuals. Panel A: Whole-brain networks A and B produced by selecting seeds in TPJ, with our community detection search space delineated by black borders. Correlation values are thresholded at 0.2. Panel B: thresholded communities (indicated by borders) show strong resemblance between the DN community and network A. The non-DN community covers sections of cortex not associated with either DN sub-network.

583 **Supplemental Materials**

584 *Table 1. Parcels from Glasser et al. (2016) contained in the search space.*

Hemisphere	mPFC	PCC
Left	10d, 10r, 10v, 25, 9m, a24, d32, OFC, p24, p32, s32	23d, 31a, 31pd, 31pv, 7m, d23ab, PCV, RSC, v23ab
Right	10d, 10r, 10v, 25, 9a, 9m, a24, d32, OFC, p24, p32, s32	23d, 31a, 31pd, 31pv, 7m, d23ab, RSC, v23ab

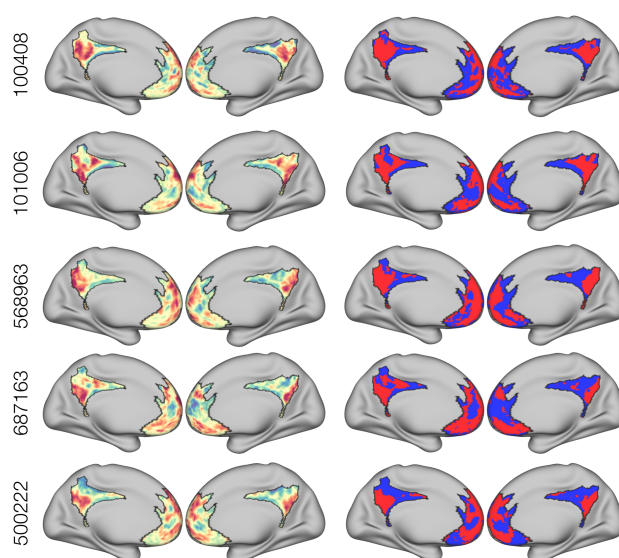


Figure S1: Additional examples of individualized partitionings, showing both Fiedler vector values (left) and binarized communities (right). A common organizational principle is visible, even though it shifts topographically across individuals.

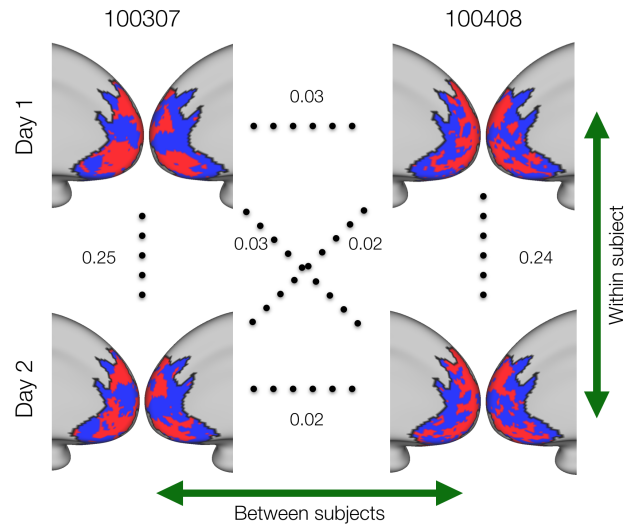


Figure S2: Example of an across-day comparison using ARI for two subjects (100307 and 100408). This reflects how qualitatively similar, within-subject partitionings can have relatively small ARI values (here 0.24-0.25), and how partitionings across individuals are much closer to the chance level of zero.

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