

Benchmarking Risk Predictions and Uncertainties in the NSCR Model of GCR Cancer Risks with Revised Low LET Risk Coefficients

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Abstract

We report on the contributions of model factors that appear in fatal cancer risk projection models to the overall uncertainty in cancer risks predictions for exposures to galactic cosmic ray (GCR) in deep space. Annual GCR exposures to astronauts at solar minimum are considered. Uncertainties in low LET risk coefficients, dose and dose-rate modifiers, quality factors (QFs), space radiation organ doses, non-targeted effects (NTE) and increased tumor lethality at high LET compared to low LET radiation are considered. For the low LET reference radiation parameters we use a revised assessment of excess relative risk (ERR) and excess additive risk (EAR) for radiation induced cancers in the Life-Span Studies (LSS) of the Atomic bomb survivors that was recently reported, and also consider ERR estimates for males from the International Study of Nuclear Workers (INWORKS). For 45-y old females at mission age the risk of exposure induced death (REID) per year and 95% confidence intervals is predicted as 1.6% [0.71, 1.63] without QF uncertainties and 1.64% [0.69, 4.06] with QF uncertainties. However, fatal risk predictions increase to 5.83% [2.56, 9.7] with non-targeted effects. For males a comparison application to GCR using LSS or INWORKS lead to predictions of 1.24% [0.58, 3.14] and 2.45% [1.23, 5.9] without NTEs. The major conclusion of our report is that high LET risk prediction uncertainties due to QFs parameters, NTEs, and possible increase lethality at high LET are dominant contributions to GCR uncertainties and should be the focus of space radiation research.

Key words: Galactic cosmic rays (GCR), HZE particles, high LET radiation, space radiation, cancer risk, relative biological effectiveness (RBE), quality factors (QF).

1 **1. Introduction**

2 In this paper we benchmark the current uncertainties in estimating cancer risks
3 from GCR exposures in the NASA Space Cancer Risk Model (NSCR). Because of the
4 large uncertainties in high charge and energy (HZE) particle radiobiology and the small
5 population of space workers, distinct methods are used at NASA to implement a
6 radiation protection program compared to ground-based radiation workers. The basic
7 approach is derived from recommendations by the National Council on Radiation
8 Protection and Measurements (NCRP) [1-3], however we have developed an approach
9 to make a rigorous uncertainty analysis [4-9], which has undergone external review by
10 the National Research Council (NRC) [10] and NCRP [11].

11 The most recent analysis of GCR risks by the NSCR model [7-9] enjoys a
12 significant reduction in overall uncertainty compared to our previous ones due to an
13 improved treatment of the QF and DDREF and their possible correlations. Estimates of
14 maximum relative biological effectiveness (RBE_{max}) defined by the ratio of initial
15 linear slopes determined at low dose and dose-rate for particles to γ -rays have been used
16 in radiation protection to assign values of QFs. Values of RBE_{max} are highly dependent
17 on the reference radiation used and their responses at low doses and dose-rates. The
18 large values of RBE_{max} found in many experiments can be attributed in-part to the
19 ineffectiveness of low doses or low dose-rates of γ -rays [8,9]. In addition, not all
20 experiments have used either low dose-rates (<0.1 Gy/hr) or lower doses (<0.25 Gy) of
21 γ -rays thus precluding RBE_{max} estimates. We have shown that assigning QF based on
22 RBE 's for acute γ -ray exposures leads to a reduction in risk estimates and uncertainty.

23 The dominant uncertainties found in previous reports were the uncertainties in
24 the parameters in the quality factor model and several uncertainties related to
25 breakdown of the conventional risk assessment approach. Here the conventional
26 approach using QFs only describe quantitative differences between heavy ions and
27 other high LET radiation compared to a low LET reference radiation, while qualitative
28 differences may occur. Furthermore because of the absence of epidemiology data for
29 humans exposed to space radiation, the interpretation of data from experimental models
30 are limited unless accurate extrapolation methods are developed. Previously we
31 discussed two areas of possible qualitative differences, which are the higher lethality
32 of high LET induced tumors compared to γ -rays or background occurring tumors, and
33 the deviation from a linear response model due to non-targeted effects (NTE) [12,13].
34 We include estimates of their impact on GCR risk prediction in the updated analysis of
35 this report.

36 The use of epidemiology data for populations exposed to γ -rays or other high
37 energy photons has been the anchor to models that use RBE based QF's to estimate
38 space radiation risks. Here we note two recent studies provide updated analysis in the
39 life-span study (LSS) of the survivors of the atomic-bomb explosions in Hiroshima and
40 Nagasaki Japan in 1945 [14], and over 200,000 radiation workers from France, the
41 United Kingdom and the United States [15-17]. The LSS analysis of Grant et al. [14]
42 used revised dosimetry assessment and methods to correct for lifestyle factors
43 compared to prior assessments [18-20]. An important finding by Grant et al. [14] is that
44 for total solid cancer risk a linear-quadratic function provided an acceptable fit for

45 males but not females. We consider these new data in our updated model denoted as
 46 NSCR-2020. For males, excess relative risk (ERR) based on linear coefficients are
 47 similar in these studies, however larger differences occur for tissue specific rates
 48 between the LSS and INWORKS studies. Therefore, we restrict our analysis to the
 49 grouped categories of all solid cancers and leukemia's. We note that INWORKS uses
 50 mortality data, while we are using the LSS incidence data analysis converted to
 51 mortality predictions with current data for the US population. In addition, the
 52 INWORKS study does not provide data on the age or latency dependence of ERR or
 53 provide data on excess additive risk (EAR). We consider predictions for the US
 54 Average population, while updates for tissue specific predictions for never smokers
 55 will be reported in the future.

56

57 2. Model Development

58

59 We briefly summarize recent methods developed to predict the risk of exposure
 60 induced death (REID) for space missions and associated uncertainty distributions [7-
 61 9]. The instantaneous cancer incidence or mortality rates, λ_I and λ_M , respectively, are
 62 modeled as functions of the tissue averaged absorbed dose D_T , or dose-rate D_{Tr} , gender,
 63 age at exposure a_E , and attained age a or latency L , which is the time after exposure
 64 $L=a-a_E$. The λ_I (or λ_M) is a sum over rates for each tissue that contributes to cancer risk,
 65 λ_{IT} (or λ_{MT}). These dependencies vary for each cancer type that could be increased by
 66 radiation exposure. However here we will group cancers into just two groups
 67 representing all total solid cancer risks and leukemia risk excluding chronic
 68 lymphocytic leukemias (CLL). The total risk of exposure induced cancer (REIC) is
 69 calculated by folding the instantaneous radiation cancer incidence-rate with the
 70 probability of surviving to time t , which is given by the survival function $S_0(t)$ for the
 71 background population times the probability for radiation cancer death at previous time,
 72 summing over one or more space mission exposures, and then integrating over the
 73 remainder of a lifetime [9]:

$$74 \quad REIC(a_E, D_T) = \sum_{j=1}^{N_m} \int_{a_{Ej}} dt \lambda_{Ij}(a_{Ej}, t, D_{Tj}) S_0(t) e^{-\sum_{k=1}^{N_m} \int_{a_E}^t dz \lambda_{Mk}(a_{Ek}, z, D_{Tk})} \quad (1)$$

75 where z is the dummy integration variable. In equation (1), N_m is the number of
 76 missions (exposures), and for each exposure, j , there is a minimum latency of 5-years
 77 for solid cancers, and 2-years for leukemia assumed. Tissue specific REIC estimates
 78 are similar to equation (1) using the single term from λ_I of interest. The equation for
 79 REID estimates is similar to equation (1) with the incidence rate replaced by the
 80 mortality rate (defined below).

81 The tissue-specific cancer incidence rate for an organ absorbed dose, D_T , is
 82 written as a weighted average of the multiplicative and additive transfer models,
 83 denoted as a mixture model after adjustment for low dose and dose-rates through
 84 introduction of the dose and dose-rate effectiveness factor (DDREF) and radiation
 85 quality through the R_{QF} factor related to the QF as described below:

86
$$\lambda_{IT}(a_E, a, D_T, Z, E) = [v_T ERR_T(a_E, a)\lambda_{0IT}(a) + (1 - v_T)EAR_T(a_E, a)]R_{QF}(Z, E)D_T \quad (2)$$

87 where v_T is the tissue-specific transfer model weight, λ_{0IT} is the tissue-specific cancer
88 incidence rate in the reference population, and where ERR_T and EAR_T are the tissue
89 specific excess relative risk and excess additive risk per Sievert, respectively. The
90 tissue specific rates for cancer mortality λ_{MT} are modeled following the BEIR VII
91 report [20] whereby the incidence rate of Eq. (2) is scaled by the age, sex, and tissue
92 specific ratio of rates for mortality to incidence in the population under study:

93
$$\lambda_{MT}(a_E, a, H_T) = \frac{\lambda_{0MT}(a)}{\lambda_{0IT}(a)} \lambda_{IT}(a_E, a, H_T) \quad (3)$$

94 However, we also consider the possibility that high LET radiation increases incidence
95 to mortality probabilities as described below. The U.S. lifetables from CDC [22] and
96 cancer rates from SEER [23] with data collected from 2013-2017 are used to provide
97 age and sex specific rates for survival of all causes of death and all solid cancer or
98 leukemia excluding CLL. For cancer incidence we used the SEER delay-adjusted rates
99 that accounts for delays that lead under-reporting of incidence data in the most recent
100 year [23].

101

102 *2.1 ERR and EAR Functions*

103 Epidemiology studies for persons exposed to largely γ -radiation fit various statistical
104 models to estimate ERR and EAR functions. The ERR and EAR functions used
105 herein are for all solid cancers and leukemia risk excluding CLL. These functions
106 depend on age at exposure, a_E , and attained aged, a , using the parametric form:

107
$$EAR \text{ or } ERR(a, a_E) = \beta (a/70)^\eta \exp(\gamma (a_E - 30)) \quad (4)$$

108 Values for the parameters in Eq. (4) from several reports [19,20] using similar functions
109 are shown in **Table 1**, with calculations reported here using the recent Grant et al.
110 results for solid cancer [14]. For leukemia risk we use the ERR and EAR functions from
111 the BEIR VII report [21]. The BEIR VII used 60 instead of 70 in Eq. (4) which leads
112 to a small difference in comparisons. The transfer model coefficient v_T have a large
113 impact for individual cancers when background rates vary between the US and Japan,
114 however predictions are less sensitive for total solid cancer risks. We use the mean
115 value of $v_T=0.7$ suggested by the BEIR VII report. For Monte-Carlo sampling we use
116 a uniform distribution on (0,1) with ERR chosen if a random number if <0.7 and EAR
117 chosen if not.

118 The INWORKS study only provide a constant ERR estimate for males for
119 cancer mortality caused by radiation [15-17]. We use their estimate for all solid cancers
120 that assume a 5-year lag as in the LSS study with $ERR = 0.37$ per Gy with 90%
121 confidence intervals [0.1, 0.67]. For all leukemia's excluding CLL, $ERR= 2.96$ [1.17,
122 5.21].

123 **Table 1.** Parameters of ERR and EAR functions described in the report from various sources [14,20,21].

	β_M , Gy ⁻¹	Attained Age power	Age at exposure	β_M , Gy ⁻¹	Attained Age power	Age at exposure, y ⁻¹
	ERR Model, Males			ERR Model, Females		
RERF, 2007*	0.35 [0.28, 0.43]	-1.65 [-2.1, -1.2]	-0.0186 [-0.0073, 0.0288]	0.58 [0.4, 0.54]	-1.65 [-2.1, -1.2]	-0.0186 [-0.0029, 0.0073]
BEIR VII	0.33 [0.24, 0.47]	-1.4 [-2.2, -0.7]	0	0.57 [0.44, 0.74]	-1.4 [-2.2, -0.7]	0
RERF, 2017	-	-	-	0.64 [0.52, 0.77]	-1.36 [-1.86, -0.84]	-0.0249 [-0.0139, -0.0357]
RERF, 2017 LQ model	0.094 [<0.02, 0.23]	-2.7 [-3.58, -1.81]	-0.0249 [-0.0139, -0.0357]	-	-	-
RERF, 2017**	<i>0.33 [0.25, 0.42]</i>	<i>-1.66 [-2.11, -1.2]</i>	<i>-0.0236 [-0.0128, -0.0343]</i>	0.64 [0.52, 0.76]	-1.36 [-1.86, -0.84]	-0.0249 [-0.0139, -0.0357]
	EAR Models, Males per 10,000 PY per Gy			EAR Models, Females per 10,000 PY per Gy		
RERF, 2007*	43 [33,55]	2.38 [1.9, 2.8]	-0.0274 [-0.0174, -0.0386]	60 [51, 69]	2.38 [1.9, 2.8]	-0.0274 [-0.0174, -0.0386]
BEIR VII	22 [15,30]	2.8 [2.15, 3.41]	0	28 [22, 36]	2.8 [2.15, 3.41]	0
RERF, 2017	-	-	-	54.7 [44.7, 65.3]	2.07 [1.64, 2.53]	-0.0357 [-0.0249, -0.0462]
RERF, 2017 LQ model	21.7 [<-1.7, 47.7]	2.89 [2.14, 3.68]	-0.0357 [-0.0249, -0.0462]	-	-	-

124 *90% Confidence intervals

125 2.2. Space Radiation Quality Factor

126 Our radiation quality approach uses concepts for particle track structure to
127 devise a functional form that is fit to available radiobiology data to formulate a radiation
128 quality factor. In this approach QF depends on particle charge number and kinetic
129 energy or equivalent velocity. This is different from the International Commission on
130 Radiological Protection (ICRP) approach where QFs are based on LET alone or similar
131 the use of a radiation weighting factors that is dependent on particle type but not LET.

132 The hazard function in Eq. (1) is scaled to other radiation types and low dose-
133 rates using a scaling factor denoted, R_{QF} , which is made-up of a QF and DDREF. The
134 R_{QF} is estimated from relative biological effectiveness factors (RBE's) determined from
135 low dose and dose-rate particle data relative to acute γ -ray exposures, which we denote
136 as $RBE_{\gamma Acute}$ to distinguish from estimates from RBE_{max} based on less accurate initial
137 slope estimates. The scaling factor is written [9]:

138

$$139 \quad R_{QF} = Q_L(Z, E) / DDREF + Q_H(Z, E) \quad (5)$$

140 where

$$141 \quad Q_L(Z, E) = [1 - P(Z, E)] \quad (5a)$$

142

$$143 \quad Q_H(Z, E) = 6.24 \Sigma_0 P(Z, E) / (\alpha_\gamma L) \quad (5b)$$

144 with the parametric function,

$$145 \quad P(Z, E) = [1 - \exp(-Z^{*2} / \kappa \beta^2)]^m [1 - \exp(-E / 0.2)] \quad (6)$$

146 where E is the particles kinetic energy per nucleon, L is the LET, Z is the particles
147 charge number, Z^* the effective charge number, and β the particles speed relative the
148 speed of light. The three model parameters (Σ_0 / α_γ , κ and m) in Eq.'s (5-6) are fit to
149 radiobiology data for tumors in mice or surrogate cancer endpoints as described
150 previously [8,9,23,24]. Values and the cumulative distribution function (CDF) for
151 Monte-Carlo sampling for the DDREF are described below. Distinct parameters are
152 used for estimating solid cancer and leukemia risks based on estimates of smaller RBEs
153 for acute myeloid leukemia and thymic lymphoma in mice compared to those found for
154 solid cancers [9].

155 An ancillary condition is used to correlate the values of the parameter κ as a
156 function of m as

$$157 \quad \kappa(m) = \frac{4\kappa_0}{(m+1)} \quad (7)$$

158 where κ_0 is value for the most likely value $m=3$. In Monte-Carlo sampling by the model,
159 conditional sampling is used where m is selected from a CDF followed by selection of
160 $\kappa(m)$, which then distributed with a normal distribution with SD shown in **Table 2**.

161 A key assumption of the model is that the low ionization density part of a
 162 particle track is influenced by dose-rate effects as represented by the first term on the
 163 right-hand side of Eq. (5). However, the high ionization density part or so-called core
 164 of a particles track has no dependence on dose-rate as described by the second term on
 165 the right-hand side of Eq. (5). The low ionization density part of the track is high-energy
 166 δ -rays and they are expected to produce biological damage in a manner similar to low
 167 doses of γ -rays [23]. A dose-rate modifier is needed for the low ionization density track
 168 regions because model parameters are largely derived from radiobiological data at
 169 higher doses and dose-rates than those occurring in space, while a DDREF is used for
 170 this estimate.

171 The space radiation QF model corresponds to a pseudo-action cross section of
 172 the form which is of interest for fluence based risk prediction approaches,

$$173 \quad \Sigma_{TE}(Z, E) = \Sigma_0 P(Z, E) + \alpha_\gamma L[1 - P(Z, E)] / 6.24 \quad (8)$$

174 The Σ is denoted as a pseudo-biological action cross section for tumor induction in units
 175 of μm^2 with the designation as “pseudo” given because time-dependent factors have
 176 been suppressed, which impact values for the cross-sectional area predicted by fits to
 177 the experiments.

178 The value of Σ_0/α_γ estimated from mouse tumor studies [9] are shown in **Table**
 179 **3**. We prefer to exclude mouse liver and Harderian gland values. The values for liver
 180 tumors are observed to be much larger in male compared to female mice, which needs
 181 to be further investigated. Harderian gland data are excluded here because this tissue
 182 does not appear in humans, and because related data are used as input for the other QF
 183 parameters so as not to put too much weight on a single model system. The CDF then
 184 follows a Gompertz equation with the parameters listed in **Table 3**.

185

186 **Table 2. Parameters for central estimate of NASA quality factor (QF)**
 187 **parameters for solid cancer and leukemia risks [9].***

Parameter	Solid Cancer	Leukemia
m	3±0.5	3±0.5
κ	624±69 (1000±250)	624 ± 69 (1000±250)
$\Sigma_0/\alpha_\gamma, \mu\text{m}^2 \text{ Gy}$	(2897±357)/6.24	(1750±250)/6.24
Non-Targeted Effects Parameters		
$\eta_0/\alpha_\gamma, \text{Gy}^{-1}$	6 x10 ⁻⁵	-
η_1	833± 200 (1000±150)	-
A_{bys}	2000 μm^2	

188 *Values in parenthesis are distinct values for light ions ($Z \leq 4$).

189 **Table 3.** Cumulative distribution function (CDF) for model parameter (Σ_0/α_γ) determined by fits to data for heavy ions and fission
 190 neutrons*. Means and fits of CDF corresponding to values of **Table 3** using logistic or Gompertz equations are shown with best fit
 191 shown in bold font.

192

<i>Data sets</i>	<i>Mean, $\mu\text{m}^2 \text{Gy}$</i>	<i>A</i>	<i>B, $\mu\text{m}^2 \text{Gy}$</i>	<i>C</i>	<i>Adj R²</i>
<i>All solid cancer data</i>	(4728 \pm 1378)/6.24				
<i>Logistic Equation Fit</i>		1.0\pm0.027	(2699\pm87)/6.24	-2.42\pm0.16	0.997
<i>Gompertz Equation Fit</i>		1.0 \pm 0.02	(2195 \pm 55.2)/6.24	(1551 \pm 84.8)/6.24	0.987
<i>Solid cancer excluding liver, and Harderian gland tumors</i>	(2897 \pm 357)/6.24				
<i>Logistic Equation Fit</i>		1.0 \pm 0.053	(2483 \pm 110)/6.24	-3.26 \pm 0.39	0.974
<i>Gompertz Equation Fit</i>		1.0\pm0.039	(2104\pm68.7)/6.24	(1109\pm110)/6.24	0.979

193

194 *Parameters that result from fits of the logistic equation, $\text{CDF} = A/[1+(\Sigma_0/\alpha_\gamma)/B]^C$ or Gompertz equation $\text{CDF} = A \exp[-\exp(-\Sigma_0/\alpha_\gamma - B)/C]$ to data
 195 for (Σ_0/α_γ) from mouse experiments for heavy ions and fission neutrons.

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2.3. Dose and Dose-Rate Reduction Effectiveness Factor

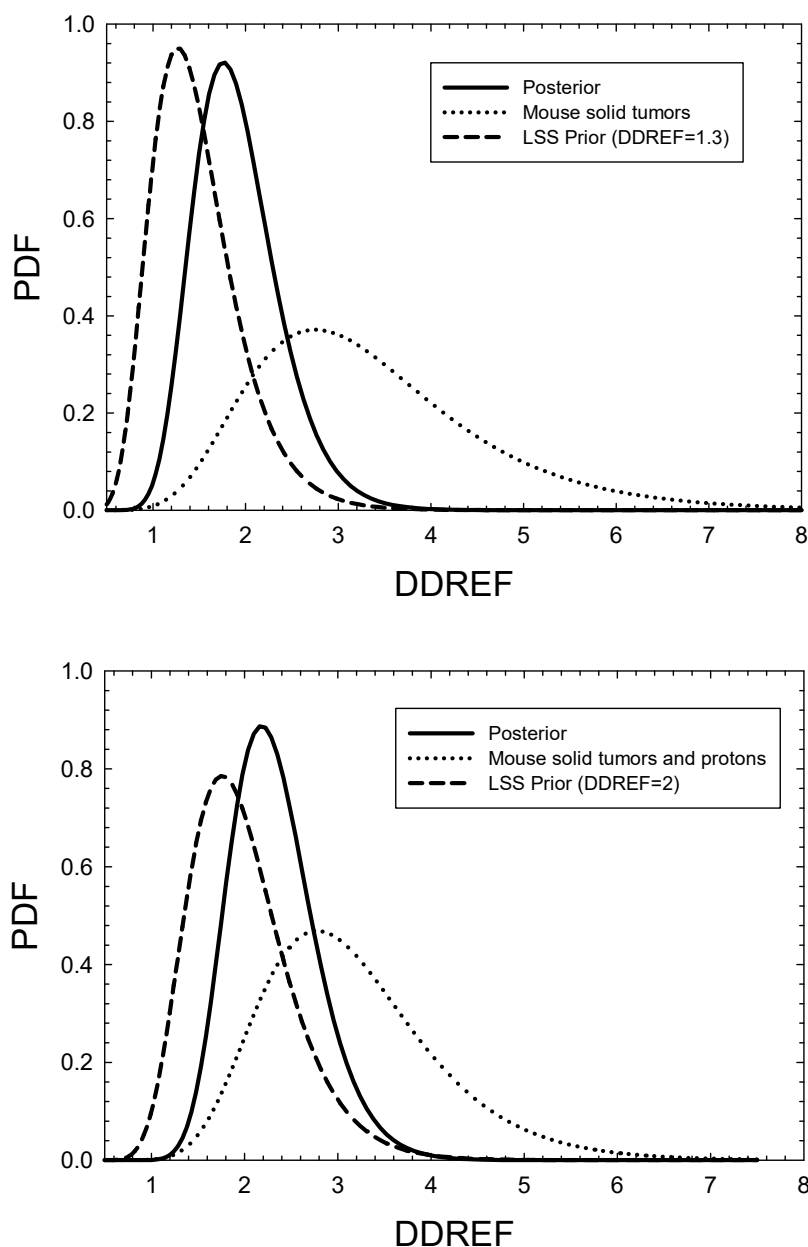
Dose-rate is known to alter radiobiological effects at moderate to high doses. This is due to the effect of DNA repair, and modulation of tissue responses. For experimental studies with low particle fluences corresponding to less than one particle traversal per cell nucleus no dose-rate effect is expected at the molecular or cellular level, however tissue responses cannot be ruled out. For spaceflight of duration of a few years or less dose protraction effects, which are distinct from dose-rate effects, are not considered. Estimating the DDREF for space exposures has the additional consideration compared to photon exposures on Earth because of the possible correlations between a dose-rate modifier and RBEs used to formulate a QF. Large RBE's are often associated with large DDREFs.

In Cucinotta et al. [9], Bayesian analysis was used to model the PDF of uncertainty in the DDREF parameter for solid cancer risk estimates in a manner similar to that used in the BEIR VII report [20] where a prior distribution was estimated from the curvature in the Japanese Life-Space Study (LSS) and the likelihood function from radiobiology data. We denoted as Model A the prior distribution from the BEIR VII Report estimate for the LSS study using a log-normal distribution with a DDREF=1.3 and 95% confidence intervals (CI) of [0.8, 1.9]. However, Hoel [25] has argued that due to subjective assumptions made in the BEIR VII report a mean DDREF of 1.3 is found, while an analysis that considers a distinct dose range from the LSS data or one that includes downward curvature at higher doses due to cell sterilization effects finds a DDREF of 2 or more. Following Hoel's analysis we used in Model B a mean DDREF of 2; however, uncertainties in this value were not modeled by Hoel. Here we assume a log-normal distribution with 90% confidence intervals of [1.2, 3] as a prior distribution for Model B based on the bounds described by Hoel [25]. Interestingly study of the curvature in dose response in the most recent LSS data by Grant et al [14] suggest a DDREF between 2 and 3 for males, while a DDREF~1 for females. The effects of the large heterogeneous population in the study is a challenge for interpretation. In contrast experimental systems offer a more precise method to estimate DDREF, however in less significant model systems and in some cases endpoints.

In our previous report we considered DDREFs from mouse solid tumor studies data where both γ -ray and high LET radiation were available. These data were used as the likelihood function for the Bayesian analysis as shown in **Figure 1** (upper panel). We did not consider ovarian and leukemia mouse data that was used by BEIR VII as appropriate for this analysis [8,9]. More recent experiments on heavy ion induction of colorectal and intestinal tumors (Suman et al., 2016) in mice did not provide other data to modify this aspect of the PDF of uncertainty for the DDREF because the γ -ray components of these experiments were limited, while dose responses for γ -rays in the recent Harderian gland experiments [26] were consistent with earlier data for Harderian gland tumors [27-29].

Values of DDREF's estimated from high-energy proton experiments are of interest because the energy spectra of δ -rays more closely represent that of GCR compared to ^{60}Co γ -rays [9]. We also surveyed published proton radiobiology data for tumors in animals and surrogate endpoints in cell culture models. Here we considered data comparing acute to low dose-rates, and analysis of curvature in acute dose response data to estimate a DDREF. In cell experiments several studies comparing high dose-rate to low dose-rates have been reported, which were summarized earlier [9]. DDREF estimates from proton experiments varied from 2.14 to 4.46 and strongly overlapped

Figure 1. Bayesian analysis of probability distribution function (PDF) for the dose and dose-rate reduction effectiveness factor (DDREF). Upper panel uses prior distribution from the Japanese atomic-bomb lifespan study (LSS) estimated in BEIR VII [20] with mean DDREF of 1.3 and likelihood function from mouse solid tumor studies with γ -rays. Lower panel uses mean DDREF of 2 as described in text for LSS study for the prior distribution, and likelihood function with mouse solid tumor studies with γ -rays and dose-rate studies for protons in surrogate cancer risk endpoints.



1 with estimates from solid cancers in mice exposed to acute and chronic doses of γ -rays.
 2 **Figure 1** (lower panel) shows the resulting PDF of the DDREF uncertainty in Model
 3 B which can be compared to our earlier publication for Model A [9].

4

5 *2.4. Non-Targeted Effect Estimates*

6 Non-targeted effects (NTE) have been shown to impact initiation, promotion
 7 and progression stages of tumorigenesis at low doses of high LET radiation [30-40].
 8 Initiation processes impacted by NTEs include chromosomal exchanges, sister
 9 chromatid exchanges, gene mutation, and neoplastic transformation, which show a
 10 characteristic non-linear dose response at low particle fluences where less than one
 11 particle traverses a cell nucleus. A similar functional response provided an optimal
 12 global fit to the Harderian gland tumor study with several heavy ions [24]. Studies with
 13 La and Nb beams, which have action inactivation cross sections approaching or
 14 exceeding the cell nuclear area, suggest no cells directly traversed by these ions survive
 15 providing important evidence for NTE in this system. The use of chimera models where
 16 irradiated tissues absent of epithelial cells produce tumors after cell implant suggests
 17 changes to the micro-environment promote mammary tumors in mice [31]. Tissue are
 18 complex non-linear signaling systems contain multiple steady-states which can prevent
 19 excitability properties upon relaxation [41] leading to altered signaling and changes in
 20 proliferation and organization contributing to cancer development.

21 In our model we assume the TE contribution is also valid with a linear response
 22 to the lowest dose or fluence considered, while an additional NTE contribution occurs
 23 such a pseudo-action cross section is given by [24],

$$24 \quad \Sigma_{NTE}(Z, E) = \Sigma_{TE}(Z, E) + \eta(Z, E, F) / F \quad (9)$$

25 where F is the particle fluence (in units of μm^2) and the η function represents the NTE
 26 contribution, which is parameterized as a function of $X_{Tr}=Z^2/\beta^2$ as:

$$27 \quad \eta = \eta_0 X_{Tr} e^{-\eta_1 X_{Tr}} [1 - e^{-FA_{bys}}] \quad (10)$$

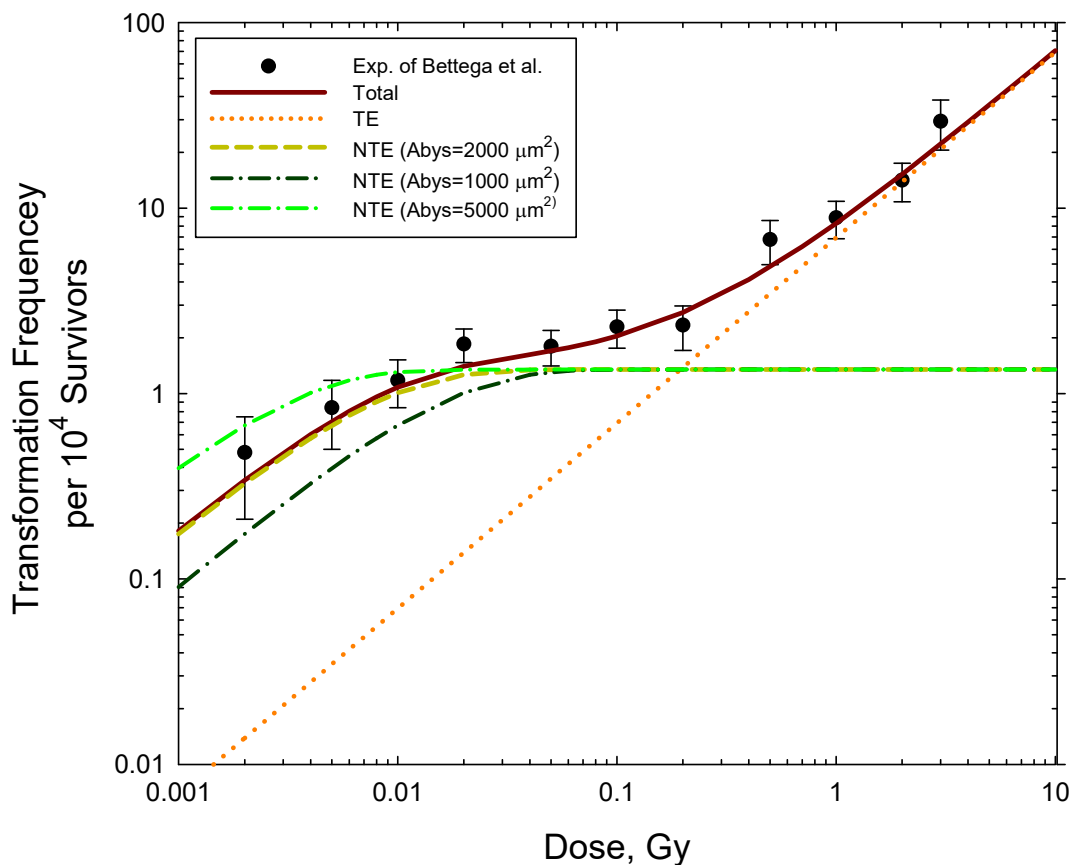
28 In Eq. (10) the area, A_{bys} , reflects the number of bystander cells surrounding a cell
 29 traversed directly by a particle that receives an oncogenic signal. The RBE is related to
 30 the cross section by $RBE = 6.24 \Sigma / (LET \alpha_\gamma)$ where α_γ is the γ -ray linear slope coefficient.
 31 Therefore, only the ratio of parameters η_0/α_γ is needed for risk estimates.

32 The parameters η_0/α_γ and η_1 are estimated from low dose radiobiology
 33 experiments [24]. The second factor on the right- hand side of Eq. (9) describes the
 34 “turning on” of NTE at very low doses. The Harderian gland tumor model and
 35 chromosomal aberration experiments do not provide data of sufficiently low doses
 36 (<0.01 Gy) to determine at which dose or fluence level this occurs, and if it depends on
 37 radiation quality or the temporal patterns of irradiation. Therefore, the parameter A_{bys}
 38 is difficult to estimate. We note that its value is correlated with estimates of η_0 at very
 39 low fluence since Eq. (10) here reduces to $\eta \sim (\eta_0 A_{bys}) X_{Tr} \exp(-\eta_1 X_{Tr}) F$.

40 Several cell culture experiments were performed with α -particle irradiation
41 which allow estimates of A_{bys} . **Figure 2** shows an example for neoplastic
42 transformation by 90 keV/ μm α -particles with symbols with errors from experiments
43 by Bettega et al. [40] and lines our model dose response function illustrating very low
44 dose responses as A_{bys} varies. A possible turn-down of NTE at higher doses (>0.1 Gy)
45 is ignored here because at these doses TE are expected to dominate. We find for a
46 typical mammalian cell nucleus area of $100 \mu\text{m}^2$ that values of A_{bys} of 1000 to 2000 μm^2
47 correspond to an NTE signal of about 1-cell layer and A_{bys} of 5000 μm^2 , a signal that
48 propagates to about 2 cell layers from a directly hit cell. These areas suggest interaction
49 distances of up to 50 microns from a directly traversed cell, and a reduction in NTE for
50 doses below about 0.01 Gy (1 rad) where the NTE contribution decrease from a dose
51 independent to linear response, while at higher doses (>0.1 Gy) TE dominate.

52

53 **Figure 2.** Dose response for neoplastic transformation of C3H10T1/2 cells by 90 keV/ μm
54 alpha particles. Experiments are from Bettega et al. [40]. Model shows characteristic mixed
55 TE and NTE effects with NTE dominating at GCR type heavy ion doses (<0.1 Gy). Area of
56 NTE estimated as $A_{bys} \sim 2000 \mu\text{m}^2$.



57

58

59

60 2.5 Implementation for GCR Exposures

61 GCR exposures include primary and secondary H, He and HZE particles, and
62 secondary neutrons, mesons, electrons, and γ -rays over a wide energy range. We used
63 the HZE particle transport computer code (HZETRN) with quantum fragmentation
64 model nuclear interaction cross sections and Badhwar–O'Neill GCR environmental
65 model to estimate particle energy spectra for particle type j , $\varphi_j(Z,E)$ as described
66 previously [6, 42-46]. These methods agree with spaceflight data in low Earth orbit [4],
67 in transit to Mars [44] and on the Mars surface [45] to within 15% for dose and dose
68 equivalent. However larger differences between measurements and models occur for
69 specific energy regions of particle spectra and therefore we have assigned a 25%
70 variance for $Z>2$ and 35% for $Z=1,2$ ions.

71 For the TE model, a mixed-field pseudo-action cross section is formed by weighting
72 the particle flux spectra, $\varphi_j(E)$ for particle species, j , contributing to GCR exposure
73 evaluated with the HZETRN code with the pseudo-biological action cross section for
74 mono-energetic particles and summing over all particles and kinetic energies:

$$75 \quad (\Sigma F)_{TE} = \sum_j \int \varphi_j(Z, E) \Sigma(Z_j, E) dE \quad (11)$$

76 For estimates of NTEs to GCR exposures we assume: 1.) The probability that a
77 bystander cell receives an oncogenic signal only occurs if the fluence is sufficiently
78 high such that a nearby cell is traversed. 2.) The time dependence of the bystander
79 signals is a few days or less such that interactions of bystander signals from different
80 HZE particles can be ignored because of the low fluence in space. 3.) The probability
81 that a bystander cell is transformed by a direct hit at a different time is small and can
82 be ignored. Equations for the mixed-field pseudo-action cross section in the NTE model
83 as folded with particle specific energy spectra as:

84

$$85 \quad (\Sigma F)_{NTE} = \sum_j \int \{ \varphi_j(Z, E) \Sigma(Z_j, E) + \eta_0 X_{Tr_j} \exp(-\eta_1 X_{Tr_j}) [1 - \exp(-A_{bys} \varphi_j(E))] \} dE$$

86 (12)

87

88 2.6 Sensitivity Study of Increased Tumor Lethality at High LET

89

90 We use the BEIR VII method to convert the LSS data from incidence to
91 mortality predictions. This approach accounts to some extent to differences in
92 conversion rate over time due to time-dependent differences in cure rates. However,
93 these are still major questions on whether the quality of tumors produced depends on
94 radiation quality. RBEs' for both incidence and lethality in mice have not been reported,
95 while differences in rates of metastasis and malignancies of tumors produce suggest
96 difference do occur [47-54]. We estimated the effects of higher tumor lethality for HZE
97 particles and neutrons in the following manner. An upper limit on the possibility of
98 higher tumor lethality would be to use REIC estimates for REID estimates on space
99 missions. However, this estimate would be too large due to the presence of low LET

100 particles such as protons that make up a significant fraction of space radiation organ
 101 doses or the low ionization density part of HZE particle tracks which are a low LET
 102 radiation. To make a more realistic estimate of the effects of an increased lethality the
 103 cancer mortality rate is modified as [7]

104

$$105 \quad \lambda_{MT} \approx \frac{\lambda_{0MT}(a)}{\lambda_{0IT}(a)} \lambda_{IT} \left\{ \sum_j \int dE \phi_{jT}(E) L_j(E) (1 - P(X_{ir})) + (\Sigma_0 / \alpha_\gamma) F_{lethal} \int dX_{ir} \phi_T(X_{ir}) P(X_{ir}) \right\}$$

106 (13)

107

108 The first term in Eq. (13) dominates for low LET radiation and is not altered under the
 109 considerations of increased tumor lethality for highly ionizing radiation. The second
 110 term in Eq. (13) is increased by a tumor lethality fraction, F_{lethal} which estimates the
 111 increased lethality or rates of metastasis observed in mouse tumor induction studies
 112 with heavy ions. The second term in equation (13) has been reduced to be independent
 113 of the particle type, j , using the variable $X_{ir} = Z^2/\beta^2$ as described previously [6-9]. For
 114 the sensitivity study of F_{lethal} , we considered a PDF to represent the uncertainty in the
 115 increased lethality for HZE particles and secondary charged particles from neutrons.
 116 The PDF is modeled as a normal distribution with several values considered assuming
 117 a 25% variance. We note that the RBE values for solid tumors considered previously
 118 were for tumor incidence and the sensitivity study of Eq.(13) is not used for leukemia
 119 risk estimates because there is no evidence for increased high LET mortality compared
 120 to low LET from mouse studies.

121

122 For the application of the NSCR model to space mission predictions, the energy
 123 spectra for each particle type, j of LET, $L_j(E)$ for each tissue, T contributing to cancer
 124 risk denoted as $\phi_T(E)$ is estimated from radiation transport codes. The particle energy
 125 spectra are folded with R_{QF} to estimate tissue specific REIC or total REID values. For
 126 calculations for a fluence $\phi_T(Z,E)$ and absorbed dose, $D_T(Z,E)$ of a particle type
 127 described by Z and E , the Hazard rate is

128

$$129 \quad \lambda_{ZI}(F_T, a_E, a) = \lambda_{\gamma I}(a_E, a) \left\{ D_T(Z, E) \frac{(1 - P(Z, E))}{DDREF} + (\Sigma_0 / \alpha_\gamma) P(Z, E) \phi_T(Z, E) \right\}$$

130 (14)

131 where $\lambda_{\gamma I}$ is the inner bracketed terms that contains the ERR and EAR functions for
 132 individual tissues. As described previously [9] calculations are made using models of
 133 the GCR environments and radiation transport in spacecraft materials and tissue, which
 134 estimate the particle energy spectra, $\phi_j(E)$ for 190 isotopes of the elements from $Z=1$ to
 135 28, neutrons, and dose contributions from pions, electrons and γ -rays.

136

137 The calculation is simplified by introducing the fluence spectra, $F(X_{ir})$ where
 138 $X_{ir} = Z^2/\beta^2$, which can be found by transforming the energy spectra, $\phi_j(E)$ for each
 particle, j of mass number and charge number, A_j and Z_j respectively as:

139
$$F(X_{tr}) = \sum_j \left(\frac{\partial X_{tr}}{\partial E} \right)^{-1} \phi_j(E) \quad (15)$$

140 where we evaluate the Jacobian in equation (12) using the Barkas form for the
141 effective charge number given by

142
$$Z^* = Z(1 - e^{-125\beta/Z^{2/3}}) \quad (16)$$

143 This transformation allows the REID calculation to occur with the tissue specific Z^*/β^2
144 spectra for light and heavy ions rather than the individual Z and E spectra.

145

146 *2.7. Summary of Parameter Uncertainty PDFs*

147 For the various parameters that enter into the model PDFs that are estimated
148 from experimental data and model comparisons to represent plausible ranges of values.
149 The uncertainty in the ERR and EAR parameters are taken directly from the
150 publications noted above. Values showed modest skewing and therefore we used a
151 normal distribution for each parameter with standard deviations (SD) estimated from
152 the publications. Our recent report [9] used solid tumor data in mice directly to model
153 the value and PDF for the parameter Σ_0/α_γ , where the PDF is represented by the
154 Gompertz equation (**Table 3**). Bayesian analysis is used to model the uncertainty in the
155 DDREF parameter. The BEIR VII Report estimate [17] for the Japanese Life-Span
156 Study (LSS) study of DDREF=1.3 with 95% confidence intervals (CI) of [0.8, 1.9] was
157 used as the prior distribution, which is updated using Bayes' theorem with the
158 likelihood function represented by a log-normal distribution. The resulting posterior
159 distribution has a mean value of 1.88 with 95% CI of [1.18, 3.0]. For the central values
160 of REID estimates for space missions discussed below we continue to use the value
161 DDREF=2, however the posterior distribution is used to represent the PDF for the
162 DDREF uncertainty in the analysis described here, which is also fit to a log-normal
163 distribution (**Table 4**). Other parameters are similar to early versions of NSCR.

164

165 **Table 4.** Summary of Probability Distribution Function (PDF) used for various terms
 166 and their parameters.

Model Term	CDF for Monte-Carlo Sampling	Parameters
ERR, EAR functions	Normal	SD for parameters from source with additional 10% variance added.
DDREF	Log-Normal	GM=0.83; GSD=1.22
QF parameter, Σ_0	Gompertz Equation	See Table 3.
QF parameter, m	Normal	SD=0.333
QF parameter, κ	Conditional sampling on m , followed by Normal	SD=0.25
NTE parameter, $\eta_0 \times A_{\text{bys}}$	Normal (See Table 2).	SD=0.333
NTE parameter, η_1	Normal (See Table 2)	SD=0.333
Fluence $Z=1,2$	Normal	$M=1$; SD = 0.35
Fluence $Z>2$	Normal	$M=1$; SD = 0.25

167

168 3. Results and Discussion

169

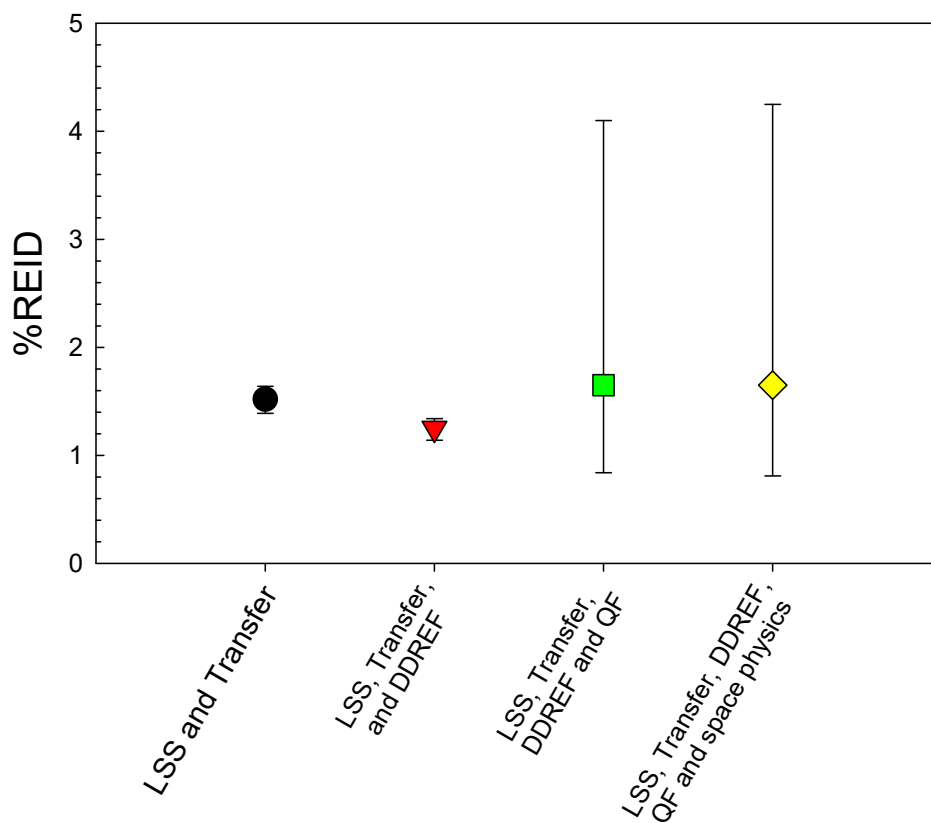
170 For all calculations we considered 45-y US Average male or female astronauts, and
 171 assumed an average spacecraft shielding amount of 20 g/cm² of aluminum for annual
 172 GCR exposures near solar minimum. Predictions of REID for other shielding materials
 173 and amounts, and for other ages at exposure were considered previously for the NSCR-
 174 2012 model [6]. In **Table 4** and **Figure 3** we show %REID predictions and 95%
 175 confidence intervals (CI) for various uncertainty inclusions. We use the value for Σ_0/α_γ
 176 that excludes liver and Harderian gland data. Use of these values would increase
 177 estimates by ~30%. For males we use the linear fits which is consistent with the main
 178 result for females in the LSS report. However, Grant et al. [14] found an improved fit
 179 for males using a linear-quadratic dose response model, which is discussed below. The
 180 inclusion of the DDREF uncertainty tends to lower REID predictions, however it is not
 181 a large effect since the QF has been defined such that the track core term is independent
 182 of dose-rate.

183 The uncertainties in the quality factor parameters dominate the uncertainty and
 184 shift average %REID predictions to higher values. The ratio of the upper 95% CI to the
 185 average value is <2.8. In **Table 5** we show a breakdown of the QF uncertainty for
 186 female astronaut %REID predictions. Result show that the Σ_0/α_γ uncertainty makes the
 187 largest contribution followed by the uncertainty in the κ parameter. **The value of m**
 188 **which is highly constrained based on previous analysis [9,13] plays only a minor**
 189 **role, which suggests the QF has been reduced in effect to a two-parameter model.**

190 For males we made a comparison of the LSS models to the INWORKS models
191 (Table 6). Here the INWORKS analysis considers only ERR and does not consider any
192 age or time after exposure parameterizations for the adult worker populations in the
193 study. The life-table representing age dependent background cancers and deaths due to
194 competing risks thus represent the only time dependent factors in this INWORKS
195 application, while the LSS studies provide time dependencies as described by Eq. (4).
196 It would be difficult to assess the higher prediction of the INWORKS rates to a single
197 factor. Other differences include chronic versus acute exposure, contributions to organ
198 doses from neutrons, and the effects of the various background populations in the
199 different studies. In addition, we are using the incidence data from LSS converted to
200 mortality using Eq. (3), while mortality data is used directly in the INWORKS study.
201 Incidence to mortality conversion varies with time period, host country, and individual
202 subjects health care all of which can impact the result.

203

204 **Figure 3.** %REID predictions for 45-year old Females with different model uncertainties
205 considered.



206
207
208
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211 **Table 4.** % REID and uncertainties for 45 y old female and male astronauts for
 212 annual GCR exposure near solar minimum with 20 g/cm² aluminum shielding.
 213

Uncertainties included	%REID	95% Confidence Intervals
Females		
LSS and Transfer	1.53	[1.38, 1.63]
LSS, Transfer and DDREF	1.19	[0.98, 1.43]
LSS, Transfer, DDREF, and QF	1.6	[0.71, 4.06]
LSS, Transfer, DDREF, QF and space organ dose	1.64	[0.69, 4.35]
Males		
LSS and Transfer	1.14	[1.05, 1.21]
LSS, Transfer and DDREF	0.92	[0.77, 1.09]
LSS, Transfer, DDREF, and QF	1.21	[0.59, 2.91]
LSS, Transfer, DDREF, QF, and space organ dose	1.24	[0.58, 3.14]

214
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Table 5. Comparison of 45-y old males %REID predictions using LSS and INWORKS coefficients in multiplicative risk model or mixture model (LSS linear-quadratic).

Low LET Model	% REID	95% CI
LSS Linear (DDREF=2)	1.24	[0.58, 3.14]
LSS linear-quadratic fit using linear term only (DDREF=1)	0.6	[0.4, 1.18]
INWORKS (DDREF=1)	2.45	[1.23, 5.9]

220
 221
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 224
 225

Table 6. Sensitivity of %REID predictions on uncertainties in parameters of the cancer risk cross section for 45-y old females for annual GCR exposure near solar minimum. All non-QF uncertainties for a conventional model included.

Uncertainty after Model Parameter Eliminated	%REID	95% CI
m	1.6	[0.7, 4.2]
κ	1.42	[0.77, 3.2]
Σ₀/α_γ, μm² Gy	1.46	[0.73, 2.84]
All uncertainties	1.64	[0.69, 4.35]

226
 227

228 3.1. Uncertainties due to Qualitative Differences

229

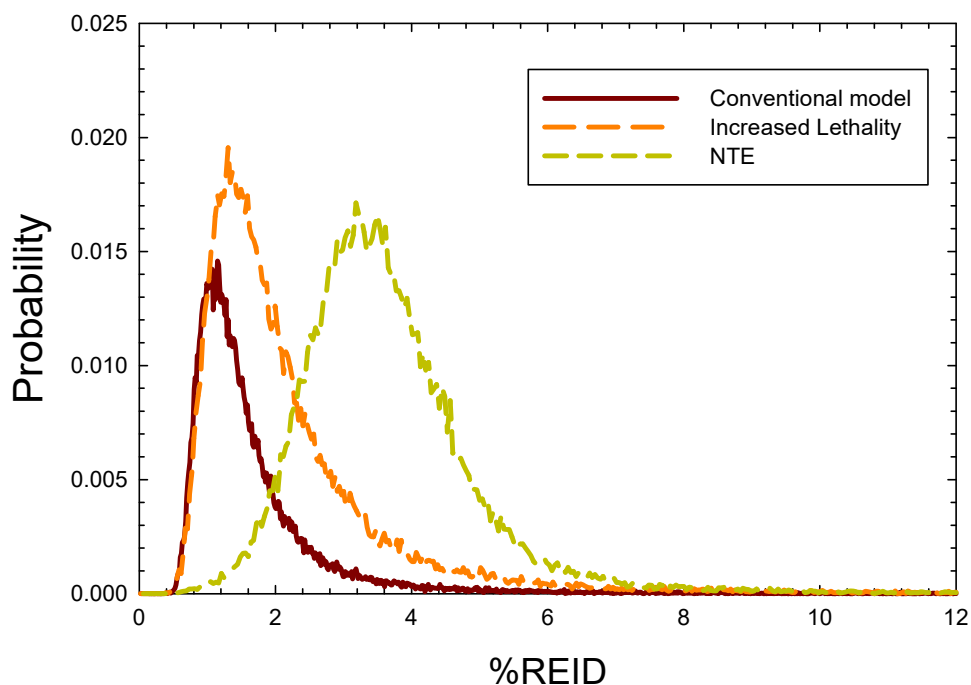
230 The application of radiation quality factors accounts for quantitative differences
231 between radiation types, however does not represent possible qualitative differences in
232 cancer risk for different types of radiation. Possible qualitative differences suggested
233 by past studies include non-targeted effects, and differences in tumor lethality not
234 estimated with RBEs based on tumor incidence or surrogate markers. Differences in
235 latency and genetic background on radiation quality are also possible however there is
236 insufficient data to make numerical estimates in this area.

237 Several reports [47-53] have suggested that HZE particles and neutrons could
238 produce more lethal tumors compared to tumors produced by low LET radiation or
239 background tumors. For low LET radiation there is an implicit assumption made by
240 epidemiology models that the tumors induced by radiation are similar to background
241 tumors in a population. This assumption is consistent with the multiplicative risk
242 model, and also based on lack of information to make an alternative assumption. Using
243 the sensitivity analysis method described earlier [7-9] suggests that increases in tumor
244 lethality for HZE particle and neutrons compared to background or low LET tumors as
245 suggested by animal studies could substantially increase REID and uncertainty
246 estimates.

247

248

249 **Figure 4.** Probability distribution functions for 45-y old females in the conventional model
250 and two predictions of the impact of increased lethality and NTEs.



251

252 **Table 7** shows predictions for increased lethality of tumors at high LET using
 253 the formalism described above. In **Table 8** we show predictions with NTE. Both
 254 important high LET effects shift REID predictions dramatically to higher values. In
 255 **Figure 4** we compare probability distributions for the different models. NTE suggest a
 256 much higher level of concern than increased lethality. Also there is a much larger body
 257 of evidence that NTE's will contribute to the mutation and instability at low doses of
 258 high LET, while few studies have directly investigated tumor quality effects.

259
 260 **Table 7.** Effect of increased tumor lethality for high LET radiation on %REID
 261 predictions for 45-y old females for annual GCR near solar minimum.
 262

Increased High LET Lethality coefficient	% REID	95% CI
0	1.64	[0.69, 4.35]
20%	1.86	[0.71, 5.11]
40%	2.06	[0.74, 5.89]
60%	2.24	[0.77, 6.62]

263
 264 **Table 8.** Predictions of 45-y old females %REID predictions for average GCR
 265 conditions with addition of non-targeted effects.
 266

$A_{\text{bys.}} \mu\text{m}^2$	% REID	95% CI
0	1.64	[0.69, 4.35]
1000	3.67	[1.68, 6.82]
2000	5.83	[2.56, 9.7]
5000	12.2	[5.1, 19.0]

267
 268
 269 **4. Conclusions**

270
 271 Past NAS [54] and NCRP [1-3] reports were highly influential in stressing the
 272 importance of understanding the radiobiology of heavy ion and other high LET
 273 radiation, while not blindly assuming GCR risks are easily projected from low LET
 274 observations of risk. In-fact NCRP Reports No 98 and No 132 were intended only for
 275 low Earth orbit. NCRP Report 132 relied on the uncertainty assessment in NCRP
 276 Report 126 [2,3]. This report used largely subjective methods to estimate uncertainties
 277 in low LET radiation epidemiology including uncertainties in data collection, bias,
 278 errors in organ dose assessments of the atomic bomb exposures, future projections of
 279 immature data sets and statistical uncertainties. Larger uncertainties were estimated for
 280 estimating dose-rate effects for low dose and dose-rate exposures and transfer models
 281 that chose between EAR versus ERR. Since that time low LET radiation epidemiology
 282 data has matured to a great extent, while only modest uncertainties are estimated for
 283 total solid cancer and leukemia risks.

284 The concordance in excess relative risks per Gy found between the LSS study
 285 and INWORKS suggest an agreement of about a factor of 2, however there are many

286 differences in the makeup and maturity of the studies. The lack of an age and latency
287 parameterization in INWORKS is a limitation in comparisons that use applications of
288 these results. For tissue specific cancer risks larger differences occur. For example,
289 Preston et al. [20] find many specific tissues have significant increases attributed to
290 radiation exposure, while Richardson et al. [17] find non-significant results for many
291 of the same tissues including colon, brain, liver, and bladder which makeup important
292 contribution in the LSS study. The reason unknown but could be due to the lower doses
293 in the INWORKS cohorts or differences in genetic or host environmental factors. In
294 this report we considered only total solid cancer and leukemias excluding CLL. The
295 treatment of tissue specific risks and update on background rates for never-smokers
296 will be considered in a future report.

297 High LET related uncertainties in QF parameters, NTEs and tumor lethality
298 were shown to dominate uncertainties. Track segment irradiation studies with heavy
299 ions are need to reduce uncertainties in QF parameters. The dichotomy in the κ for light
300 and heavy ions is likely due to the higher effectiveness of lower energy δ -rays (<5 keV),
301 which has a larger impact of light ions. This effect will be addressed in future version
302 of NSCR. Several recent reviews have noted the importance of NTE's for high LET
303 radiation and the supra-linear dose responses produced by NTE's at low dose can
304 substantially increase RBE estimates and skew PDFs for cancer risk estimates. Similar
305 reports [32-42] have suggested that HZE particles and neutrons could produce more
306 lethal tumors compared to tumors produced by low LET radiation or background
307 tumors, which is a qualitative difference not accounted for in current risk estimates. For
308 low LET radiation there is an implicit assumption made by epidemiology models that
309 the tumors induced by radiation are similar to background tumors in a population. This
310 assumption is consistent with the multiplicative risk model, and also based on lack of
311 information to make an alternative assumption. The potential role for NTEs is the
312 largest uncertainty found in this study. NTEs are supported by many mechanistic
313 studies, however are sparse for dose response modeling. Studies are needed over the
314 low dose range (0.001 to 0.05 Gy) in mouse or other small animals. Also, the use of
315 high Z ions such as Nb, La, Au or Pb with ranges of a few cm or more in tissue are
316 recommended because here directly traversed target cells have a high probability of cell
317 kill. Therefore, tumors observed would likely directly NTEs.

318

319

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