bioRxiv preprint doi: https://doi.org/10.1101/2020.07.29.226647; this version posted July 30, 2020. The copyright holder for this preprint (which was not certified by peer review) is the author/funder. All rights reserved. No reuse allowed without permission.

Dynamic Configuration of Coactive Micropatterns in the Default
 Mode Network during Wakefulness and Sleep

- Yan Cui<sup>1</sup>, Min Li<sup>1</sup>, Bharat Biswal<sup>1, 2, \*</sup>, Wei Jing<sup>1, 3</sup>, Changsong Zhou<sup>4</sup>, Huixiao Liu<sup>1</sup>, Daqing
  Guo<sup>1, 6, \*</sup>, Yang Xia<sup>1</sup>, Dezhong Yao<sup>1, 5, 6, \*</sup>
- <sup>5</sup> <sup>1</sup>The Clinical Hospital of Chengdu Brain Science Institute, MOE Key Lab for NeuroInformation, University of
- 6 Electronic Science and Technology of China, Chengdu 611731, China
- 7 <sup>2</sup>Department of Biomedical Engineering, New Jersey Institute of Technology, Newark, NJ 07102, USA
- 8 <sup>3</sup>Department of Physiology, School of Basic Medicine and Tongji Medical College, Huazhong University of
- 9 Science and Technology, Wuhan, China
- 10 <sup>4</sup>Department of Physics, Centre for Nonlinear Studies and Beijing-Hong Kong-Singapore Joint Centre for
- 11 Nonlinear and Complex Systems (Hong Kong), Institute of Computational and Theoretical Studies, Hong Kong
- 12 Baptist University, Kowloon Tong, Hong Kong
- 13 <sup>5</sup>School of Electrical Engineering, Zhengzhou University, Zhengzhou 450001, China
- 14 <sup>6</sup>Sichuan Institute for Brain Science and Brain-Inspired Intelligence, Chengdu 611731, China
- 15 \*Corresponding authors: <u>dqguo@uestc.edu.cn</u>, <u>dyao@uestc.edu.cn</u> and <u>bbiswal@gmail.com</u>

16

# 17 Abstract

The activity in the default mode network (DMN) rapidly fluctuates in different conscious 18 stages during wakefulness and sleep, indicating high complexity for the role of DMN in 19 consciousness. Tracking the dynamics of these fluctuations is critical for deeply understanding 20 the physiological mechanism of consciousness. Here, we propose a coactive micropattern 21 22 (CAMP) method to extract the dynamic configuration of local field potentials (LFPs) in the 23 rat DMN. Three spatially stable CAMPs were detected from DMN gamma activity (40-80 Hz) across wakefulness and sleep, consisting of a common low-activity level micropattern, an 24 anterior high-activity level micropattern and a posterior high-activity level micropattern. 25 Temporal structures of these CAMPs were specific to different conscious stages. A dynamic 26 balance across CAMPs emerged during wakefulness and was disrupted in sleep stages, 27 demonstrating that the balanced dynamic configuration of CAMPs played a vital role in 28 supporting higher cognitive functions and primary consciousness. Furthermore, all these 29 CAMPs displayed strong phasic relationships to the up-down states of the slow DMN activity 30 during deep sleep. Our study reveals that the consciousness levels of different conscious stages 31 are determined by the dynamic configurations of DMN activity, and provides a potential three-32 state model for the consciousness during wakefulness and sleep. 33

Keywords: default mode network; coactive micropattern; wakefulness and sleep; up-down
 states; dynamic configuration

2

## 36 1. Introduction

37 Multimodal imaging studies of the human brain have discovered that several intrinsic connectivity networks (ICNs) co-exist during the resting state(Beckmann et al., 2005; Liu et 38 al., 2017). Dynamic switching within these ICNs displays a hierarchical structure over time 39 for the brain activity at rest and is significantly associated with the cognitive traits(Fox et al., 40 2016; Vidaurre et al., 2017), suggesting that brain activity is appropriately understood in terms 41 of the dynamic configuration among ICNs. These studies mainly consider each ICN as a whole 42 during brain dynamics but ignore the intrinsic dynamics of individual ICN. Indeed, individual 43 ICN also shows strong fluctuations in brain activity and different ICNs are believed to 44 dominate distinct cognitive functions(Rosazza and Minati, 2011). For a specific brain function, 45 further tracking the dynamic configuration of fluctuations in brain activity at single-ICN level 46 might be critical to reveal the physiological mechanism underlying it. 47 As a task-negative ICN, the default mode network (DMN) has been highlighted and 48 progressively refined as the key neural correlate of consciousness(Fox et al., 2018; Gusnard 49 et al., 2001; Raichle, 2015; Raichle et al., 2001). DMN connectivity between the frontal and 50 posterior areas is reduced during the slow wave sleep (SWS) stage(Sämann et al., 2011), which 51

displayed low level of consciousness. However, at sleep onset and throughout the rapid eye movement sleep (REM) stage with primary consciousness(Hobson, 2009), the DMN regions persisted in their couplings(Horovitz et al., 2008; Larson-Prior et al., 2009). These findings illustrate that DMN activity is functionally reorganized during sleep and might further reflect levels of consciousness. Additionally, fast and ever-changing dynamics of DMN activity have also been observed in various consciousness levels, and the temporal aspects of spontaneous DMN activity might be associated with conscious processes(Kapogiannis et al., 2014; Panda et al., 2016). Therefore, the close association between DMN activity and consciousness represents an important topic to study for an understanding of the physiological mechanism of consciousness by revealing the dynamic configuration of fast DMN activity, which has not been completely elucidated.

On the other hand, recent neurophysiological studies identified the up-down state as a 63 biomarker of low-level consciousness, particularly in the deep sleep stage and anesthesia. The 64 up-down state refers to the alternate epochs in which neurons in various brain regions increase 65 and decrease their firing rates in a highly synchronized and stepwise manner at a rate of 66 approximately 0.5-2 Hz(Amzica and Steriade, 1995; Petersen et al., 2003). Moreover, this up-67 down state emerges in both neuron membrane potentials and local field potentials 68 (LFPs)(Holcman and Tsodyks, 2006), and characterizes the dynamics of slow oscillations 69 during deep sleep(Ji and Wilson, 2007; Lőrincz et al., 2015). However, researchers are still 70 debating the existence of a physiological relationship between the up-down state and the DMN 71 dynamics, another issue that deserves further exploration. 72

In the present study, we developed and applied a new dynamic activity pattern method to 73 address these challenges. The proposed method extracted the dynamic configuration of fast 74 neural activity in different conscious stages based on the coactive phenomena in envelope 75 activity from multi-channels physiological signals. The new method-the coactive micropattern 76 analysis (CAMP)-decomposed the dynamics of neural activity into several instinct CAMPs 77 and defined the configurations across time through the constitutions and transitions among 78 79 these CAMPs. We then applied the CAMP analysis to the recorded LFPs from rat DMN during wakefulness and sleep. Our results demonstrated the reorganized dynamic configurations of 80 CAMPs for the fast DMN activity in different conscious stages, implying that the dynamic 81

configurations of DMN micropatterns might provide underlying neural correlates for the
 consciousness levels observed during wakefulness and sleep.

## 84 2. Material and Methods

2.1. Dataset. Twenty-nine male Sprague-Dawley rats were used in our experiment. Firstly, 85 fifteen electrodes, including seven epidural cortical electrodes and eight depth electrodes, were 86 implanted into the brain of each rat under deep anesthesia (sodium pentobarbital, 60 mg/kg 87 body weight, i.p.) at the coordinates proposed by Lu(Lu et al., 2012) (Fig. 1, Table 1). The 88 reference electrode was placed in the cerebellum, and two electromyographic (EMG) 89 electrodes were implanted bilaterally in the dorsal neck muscles. Here the cerebellum was 90 chosen for the placement of the reference electrode, for that there was lower neural activity in 91 the cerebellum and the cerebellum was not involved in many cognitive functions. Notably, 0.6 92 ml of atropine sulfate (0.5 mg/ml, s.c.) was injected during electrode implantation to prevent 93 excess secretions from the respiratory tract. Meanwhile, the body temperature of the rats was 94 maintained at 37 degrees centigrade with a heating pad. Then, all electrodes were welded to 95 connectors and fixed on the skull of the rat with dental acrylic. After the surgical procedure, 96

	A-P	M-L	D-V
PrL	4.2	$\pm 0.8$	3
OFC	3.7	$\pm 1.8$	4.7
CG	1.7	$\pm 0.7$	2.6
RSC	-3.3	0	0
HIP	-4.3	$\pm 1.4$	3
PPC	-4.5	$\pm 4$	0
V2	-5.2	$\pm 2.4$	0
ТЕ	-5.2	$\pm 8$	5

Table 1. Coordinates of the 15 electrodes (mm). A-P, M-L, and D-V indicate anterior-posterior, mediallateral, and dorsal-ventral directions, respectively. PrL, prelimbic cortex; OFC, orbital cortex; CG,
cingulate cortex; RSC, retrosplenial cortex; HIP, hippocampus; PPC, posterior parietal cortex; V2,
secondary visual cortex; TE, temporal association cortex.

bioRxiv preprint doi: https://doi.org/10.1101/2020.07.29.226647; this version posted July 30, 2020. The copyright holder for this preprint (which was not certified by peer review) is the author/funder. All rights reserved. No reuse allowed without permission.



■ epidural electrode ● depth electrode

101

102 **Fig. 1.** The placement of 15 intracranial electrodes.

penicillin G was administered to prevent infection, and all rats were allowed at least 2 weeks
for recovery before the recording session started. All experimental animal procedures were
approved by the Institutional Animal Care and Use Committee of the University of Electronic
Science and Technology of China.

Prior to the recording sessions, the rats were habituated to the experimental environment and the recording cable for 2 days. During the recording session, all rats were placed in a glass box on a 12-h light/dark cycle (lights on at 8:00 am). Each recording electrode was connected to an acquisition system (Chengyi, RM62160, China). Electrophysiological signals (LFPs) and videos were synchronously and continuously acquired for 72 h. The amplified and filtered (0.16–100 Hz for LFPs, 8.3–500 Hz for electromyogram (EMG), and 50-Hz notch filter) signals were stored on a hard disk (Lenovo Company, USA), and the sample frequency was set to 1,000 Hz. All experiments were performed in a noise-attenuated room, where the background noise was set to  $32.2 \pm 3.0$  dB and the temperature was maintained at  $25 \pm 0.5$ degrees centigrade. The experimenter entered the noise-attenuated room to replace food and water and clean cages at 12:00 am daily.

The dataset used in the current study was selected from the last 24 h of the total recording and was separated into three stages, including the resting (AWAKE), slow wave sleep (SWS) and rapid eye movement (REM) sleep stages. The rules for selecting each stage were based on LFP, EMG and videos, which have been summarized in our previous publications(Jing et al., 2017). Briefly, the scoring of the awake and sleep stages were performed by several experts. We included 29 rats in the current study. For each rat, 30 segments in different stages were recorded, and each segment lasted 10 s (a total of 300 s of LFPs).

125 2.2. The coactive micropattern (CAMP) algorithm. Using functional magnetic resonance imaging (fMRI) data, Liu and colleagues(Liu et al., 2013; Liu and Duyn, 2013) used the 126 coactive pattern method, a point process approach, to identify a set of CAPs with relevant 127 network features to resting state networks, including the default mode network (DMN). In the 128 present study, we developed a coactive micropattern (CAMP) measurement and specifically 129 employed it to analyze neurophysiological data. An overview and procedure of the CAMP 130 method is shown in Fig. 2. This method was used to extract CAMPs based on the extreme 131 values of envelope signals at a high temporal resolution and reveal the fast dynamics of 132 multichannel LFPs. 133

134 Several steps were involved in the CAMP method. First, the original data were bandpass 135 filtered into specific frequency bands. In our study, we filtered the original LFPs into the 136 gamma (40-80 Hz) frequency band for the neural correlation between DMN gamma oscillation bioRxiv preprint doi: https://doi.org/10.1101/2020.07.29.226647; this version posted July 30, 2020. The copyright holder for this preprint (which was not certified by peer review) is the author/funder. All rights reserved. No reuse allowed without permission.



137

Fig. 2. Schematic of the CAMP procedure and three CAMPs of gamma activity in the DMN during 138 wakefulness and sleep. (a) The original LFPs. (b) The envelope signals (blue lines) were extracted by 139 applying the Hilbert transform to the bandpass-filtered signals (gray lines). (c) All the envelope signals 140 were downsampled (blue lines), and the extreme values were detected as the active points for each 141 142 channel (red dots). The dotted lines suggest the coactive points in which more than N (N=7 in the present study) active points were observed across DMN regions. (d) The coactive patterns were the 143 maps of activity of all DMN regions at coactive points. (e) The k-means clustering algorithm was 144 applied to all coactive patterns to detect the CAMPs. (f) A criterion was employed to remove several 145 coactive points and increase the aggregation of the CAMPs. The final CAMPs and CAMP index 146 detected in this step were subjected to further analyses. (g) Spatial structure of the common low-activity 147 level micropattern (cDMN). (h) Spatial structure of the anterior high-activity level micropattern 148 149 (aDMN). (i) Spatial structure of the posterior high-activity level micropattern (pDMN).

150

151 with the cognitive functions. Second, the Hilbert transform was applied to the filtered data to

obtain the envelope signals (Fig. 2b). These envelope signals were normalized and 152 153 downsampled (from 1,000 Hz to 100 Hz) to improve the signal-to-noise ratio (SNR) (Fig. 2c). The envelope signals were normalized by restricting the maximum value of the normalized 154 envelope signal to 0.9 and the minimum value to 0.1. Third, the active points for each channel 155 of envelope signals were then defined as the extreme points of the envelope signals, including 156 local maximum and minimum values. Afterwards, the coactive patterns (CAPs) of the brain 157 were introduced from normalized and down-sampled envelope signals for all states. The CAPs 158 159 were the brain maps in which more than one brain region displayed active points at the same time point (Fig. 2d), and totally there were 1724646 CAPs that were extracted. Thus, we 160 considered the number of brain regions with active points at the same time (parameter N) as 161 one important parameter for extracting these coactive patterns. 162

After extracting the CAPs from envelope signals, we employed the k-means clustering 163 algorithm to all the CAPs based on their spatial similarity to decompose the CAMPs (Fig. 2e). 164 By clustering the CAPs into several distinct groups, we temporally divided the brain activity 165 into multiple CAMPs. We repeated the k-means clustering with k = 2, ..., 10 and applied the 166 contour coefficient estimation (i.e., the sum of the squared errors, SSE) to determine the 167 optimal number of distinct groups and select the optimal number of CAMPs. The optimal 168 number of CAMPs was 3 in our study, according to the elbow of the curve between the k169 values and SSE values (Supplementary Fig. 1b). 170

171 Next, the CAMPs were fit back to the coactive patterns (CAPs), assigning each CAP to 172 the CAMP class with the lowest squared Euclidean distance to the three CAMPs. The CAMP 173 index was then obtained from the assignment, which showed the temporal sequence of CAMPs 174 in the gamma activity of the DMN. Then, we carefully updated the CAMPs and CAMP index

according to the CAPs that belong to the same CAMP class using the following criterion: 175  $|d_i - \overline{d}| < \mu \delta(d)$ , where  $d_i$  is the squared Euclidean distance between the *i* th coactive 176 pattern with its assigned CAMP,  $\overline{d}$  is the mean of all distance,  $\delta(d)$  is the standard 177 deviation of these distance, and  $\mu$  is the penalty parameter we determined. If the distance 178 did not conform to this criterion, then we removed the assignment of the corresponding CAPs 179 from any CAMP class (Fig. 2f). Afterwards, we applied the k-means clustering algorithm to 180 all remaining original CAPs using the same k value detected previously and redefined the 181 clusters. This step was iterated until all distances obeyed this criterion. Using this criterion, 182 we precisely determined the final spatial structures of CAMPs and the CAMP index. Notably, 183 if the CAP was not assigned to any CAMP, we removed it from the CAMP index. 261344 184 CAPs were removed based on this criterion and there were 1463303 CAPs used in subsequent 185 analysis. The final CAMP index only contained the assignments of all CAPs to their 186 corresponding CAMPs. 187

In the present study, we calculated the number of CAPs for different N values ranging 188 from 2 to 15 (Supplementary Fig. 1a) and decomposed the CAMPs from these CAPs. Under 189 different N values, the derived CAMPs exhibited similar spatial structures (Supplementary 190 Fig. 2). Therefore, considering the complexity of the calculation and requirement for 191 additional information about DMN dynamics, we finally set N to 7 in the current study. 192 Additionally, we also altered the penalty parameter  $\mu$  from 1.5 to 3 (step size of 0.1) and 193 described how the proportion of removed CAPs varied with different  $\mu$  values 194 (Supplementary Fig 1c). By extracting the CAMPs with different  $\mu$  values, we observed 195 similar spatial structures of these CAMPs, implying that the penalty parameter might not affect 196 the CAMPs (Supplementary Fig. 3). Therefore, we finally set the value of this parameter to 2 197

in the subsequent analysis.

199	All our analyses of the CAMP algorithm were performed using our own custom MATLAB
200	(release 2019a) scripts and the scripts for CAMP algorithm are available in the Mendeley
201	website (https://data.mendeley.com/datasets/p522rj449p/draft?a=0ef3b254-520e-456e-b257-
202	c398ef632148). If a special description was not included, we extracted the CAMPs of all the
203	CAPs from whole segments acquired from rats in all three conscious stages. For every segment,
204	the CAMPs were obtained by averaging the CAPs belonging to their corresponding clusters
205	in that segment. Meanwhile, the CAMP index of each segment was also acquired from the
206	total CAMP index.
207	2.3. Estimation of the CAMP features. In the present study, we employed five measurements
208	to characterize the features of CAMPs and the CAMP index of each segment.
209	The total occurrence represented the number of CAPs assigned to each CAMP, and the
210	occurrence probability was the proportion of the total occurrence of the number of all CAPs.
211	The total duration characterized the entire time required for each CAMP and the duration
212	probability represented the proportion of that.
213	The duration of one CAP was defined as follows: the start time was the mid-point between
214	the time point of this CAP and the preceding CAP, and the end time was the mid-point between
215	the time point of this CAP and the next CAP.
216	We first defined the event for each CAMP to determine the mean duration of each CAMP.
217	An event for each CAMP was that the coactive pattern before or after it should be different
218	from itself. Thus, in the CAMP index, if the neighboring CAPs belonged to the same CAMP,
219	then they should be included in one event for that CAMP. Using this approach, we obtained a
220	new CAMP index in which the neighboring coactive patterns did not belong to the same

CAMP. We separately estimated the numbers of events for all CAMPs, and the mean duration
for each CAMP was calculated by dividing the total duration by the number of events for that
CAMP.

All values of these CAMP features were calculated for each segment (10 s). The values of these features were averaged based on the rat and conscious stage to which they belonged to calculate the values of CAMP features for each rat in different conscious stages.

227

2.4. Transition probabilities (TPs) for pairs of CAMPs. The transition probabilities for pairs

of CAMPs were the one-step and direct transitions among them. These TPs were separately estimated from the new CAMP index for each segment. Six types of direct transitions were identified in the new CAMP index. The TP for one direct transition was calculated by dividing the number of this transition by the total number of all direct transitions.

# 232 **2.5.** Reliability test for the three CAMPs across the 29 rats and different conscious stages.

We initially applied the CAMP analysis to the segments obtained from each rat in the AWAKE, SWS and REM sleep stages to assess the reliability of these CAMPs. Three different CAMPs were identified for each for each rat in each conscious stage (29\*3\*3 total CAMPs).

The reliability of CAMPs across rats was determined by estimating the correlation coefficients of the CAMPs among pairs of rats in the same conscious stage using the Pearson correlation method. These correlation coefficients were then averaged to obtain the reliability of each CAMP in each conscious stage (3\*3). For different conscious stages, we next averaged the correlations across CAMPs and obtained the reliabilities of all CAMPs for each stage.

For the analysis of the reliability of CAMPs across different conscious stages, we first estimated the correlation coefficients of CAMPs among pairs of conscious stages for each rat (29\*3\*3). Then, the whole correlation coefficient was averaged and the reliability of CAMPs 244 across stages was obtained (3\*3).

245 2.6. Randomization test for the CAMP index. The randomization tests were applied to the
246 new CAMP indices in the AWAKE, SWS and REM sleep stages(Lehmann et al., 2005). The
247 null hypothesis was that if the transition from a preceding CAMP to the next CAMP occurred
248 randomly, then the observed TPs would depend on the occurrence probability of CAMPs.
249 During the test, we considered the expected TP from CAMP *X* to CAMP *Y* to be

250 
$$P_{X \to Y}^* = P_X P_Y / (1 - P_X), \qquad (1)$$

where  $P_X(P_Y)$  is the occurrence probability for CAMP X(Y). The difference between the expected TP and the observed TP was then assessed by calculating the chi-square distance

253 
$$\sum_{X,Y} \left( P_{X \to Y} - P_{X \to Y}^* \right)^2 / P_{X \to Y}^*,$$
 (2)

where the sum was calculated for all 6 pairs of CAMPs for which  $X \neq Y$ . The randomization test (permutation test) was then performed to statistically analyze the significance of this distance between the observed TP and expected TP. The permutation test was performed by shuffling the order of coactive patterns. The number of randomizations in the permutation test was set to 10,000 in our study, and the probability was determined by the rank of the observed difference among the randomly obtained differences.

## 260 2.7. Phasic relationships between CAMPs and up-down states in the slow oscillations of

the DMN during deep sleep. We first averaged the DMN activity to obtain the activity of anterior DMN and posterior DMN in the SWS stage and to assess the phasic relationship between CAMPs and up-down states. The average activity was then bandpass-filtered at 0.5-2Hz and downsampled from 1,000 Hz to 100 Hz, which coincided with the CAMP algorithm. Using this approach, we finally obtained the downsampled slow oscillations in the anterior DMN and posterior DMN regions. Then, the Hilbert transform was applied to these slow oscillations to obtain the instantaneous phase for both slow activity in the anterior DMN and
posterior DMN activity. By combining the acquired instantaneous phase and timing of each
CAMP, we obtained the instantaneous phases of all CAMPs in the slow activity of the anterior
DMN and posterior DMN, and the distributions of phases for the cDMN, aDMN and pDMN
in the SWS stage. Finally, we employed the Rayleigh test to analyze the non-uniformity of
these distributions of phases for the three CAMPs.

273 2.8. Statistical analysis. The statistical comparisons of the CAMP features and the TPs among
274 CAMPs across the three stages were performed using the methods described below. First, an
275 ANOVA was performed among all three stages, and then Student's t test was performed as the
276 post hoc test to determine the significance of differences between pairs of stages. In addition,
277 the p values derived from Student's t tests were corrected with the false discovery rate (FDR)
278 correction.

279 **3. Results** 

3.1. Three CAMPs of gamma activity in the DMN during wakefulness and sleep. The 280 CAMP analysis procedure developed in the present study is schematically illustrated in Fig. 2 281 and section 2.2. The concatenated gamma activity in the DMN of all rats and all stages during 282 wakefulness and sleep was decomposed into three distinct CAMPs, including a common low-283 activity level micropattern (cDMN), an anterior high-activity level micropattern (aDMN) and 284 a posterior high-activity level micropattern (pDMN). In the cDMN, all DMN regions showed 285 similar and low levels of activity (mean normalized activity:  $0.2577 \pm 0.0041$ , Fig. 2g), 286 287 indicating a potential cooperation of these regions in this type of CAMP. However, two different levels of activity were observed in both the aDMN and pDMN. The aDMN exhibited 288 relatively higher levels of activity in the anterior DMN regions (i.e., the prelimbic cortex (PrL), 289

bioRxiv preprint doi: https://doi.org/10.1101/2020.07.29.226647; this version posted July 30, 2020. The copyright holder for this preprint (which was not certified by peer review) is the author/funder. All rights reserved. No reuse allowed without permission.

	cDMN	aDMN	pDMN	Mean Reliability
AWAK	E 0.5806	0.8043	0.8504	0.7451
SWS	0.7588	0.6472	0.8544	0.7535
REM	0.4257	0.6951	0.8843	0.6684
ble 2. The	reliabilities (correlation	n coefficients) of CAMPs	s in the three stages	across rats.
ble 2. The	reliabilities (correlation AWAKE vs. SWS	n coefficients) of CAMPs AWAKE vs. REM	s in the three stages s SWS vs. REM	across rats. Mean Reliability
ble 2. The	reliabilities (correlation AWAKE vs. SWS 0.7214	n coefficients) of CAMPs AWAKE vs. REM 0.6352	s in the three stages a SWS vs. REM 0.5122	across rats. Mean Reliability 0.6229
ble 2. The cDMN aDMN	reliabilities (correlation AWAKE vs. SWS 0.7214 0.7910	n coefficients) of CAMPs AWAKE vs. REM 0.6352 0.8650	s in the three stages a SWS vs. REM 0.5122 0.7087	across rats. Mean Reliability 0.6229 0.7882

291

290

**Table 3.** The reliabilities (correlation coefficients) of CAMPs across the three conscious stages.

292

the orbitofrontal cortex (OFC) and the cingulate gyrus (CG), mean normalized activity: 0.3868 293  $\pm$  0.0018) and lower activity in the posterior DMN structures (i.e., the hippocampus (HIP), the 294 posterior parietal cortex (PPC), the visual cortex area (V2) and the retrosplenial cortex (RSC), 295 mean normalized activity:  $0.3050 \pm 0.0060$ , Fig. 2h). In the pDMN, the posterior DMN 296 structures displayed higher levels of activity (mean normalized activity:  $0.3793 \pm 0.0145$ ), 297 while the anterior DMN regions showed relatively lower levels of activity (mean normalized 298 299 activity:  $0.3073 \pm 0.0021$ , Fig. 2i). Accordingly, both the aDMN and pDMN were considered the high-activity micropatterns in DMN dynamics. 300

We separately decomposed the CAMPs for each rat in every conscious stage and tested 301 their reliability across all 29 rats and different conscious stages by calculating the Pearson 302 correlation coefficient to assess the spatial stability of these detected CAMPs. All three 303 CAMPs exhibited high stability with large correlation coefficients among different rats during 304 wakefulness and sleep (mean correlation coefficients: r = 0.7451, r = 0.7535, r = 0.6684 for 305 the AWAKE stage, SWS stage and REM sleep stage, respectively; Table 2). Besides, the spatial 306 structures of these CAMPs were also similar in distinct conscious stages (mean correlation 307 coefficients: r = 0.6229, r = 0.7882, r = 0.8600 for AWAKE stage, SWS stage and REM sleep 308



309

310 Fig. 3. Comparisons of the temporal features and activity levels of each CAMP during wakefulness 311 and sleep. (a) Comparisons of the total occurrence of each CAMP in different conscious stages. The 312 dots represent the values obtained from 29 rats, and the black stars indicate significant differences with 313 a corrected p < 0.001. (b) Comparisons of the total duration. (c) Comparisons of the mean duration. (d) Comparisons of the mean DMN activity during wakefulness and sleep for different CAMPs. (e-j) 314 Comparisons of activity in DMN nodes for different CAMPs across different conscious stages: (e and 315 h) cDMN, (f and i) aDMN, and (g and j) pDMN. Gray dots indicate decreased normalized activity and 316 317 black dots indicate increased normalized activity. The size of the dot reflects the value of the difference, 318 and the red stars indicate significance differences with a corrected p<0.001.

319

stage, respectively; Table 3). These findings demonstrated high reliability and robustness ofthese CAMPs.

# 322 **3.2.** The temporal features and activity levels of each CAMP during wakefulness and

323 sleep. We computed several temporal measurements to characterize the features and dynamics

of these CAMPS during wakefulness and sleep, including the total occurrence (occurrence 324 325 probability), the total duration (duration probability) and the mean duration. All these features represented the temporal properties of these CAMPs in different conscious stages. Based on 326 the comparisons, all features of the low-activity micropattern cDMN displayed the largest 327 values in the SWS stage and the smallest values in the REM sleep stage, and the two high-328 activity micropatterns (i.e., the aDMN and pDMN) exhibited the largest values for all features 329 in the REM sleep stage and the smallest values in the SWS stage (Fig. 3a-3c). These opposite 330 alterations in features between low-activity micropatterns and high-activity micropatterns 331 above-mentioned comparisons were also highly significant, implying that the alterations in the 332 suggested that these two types of CAMPs observed in DMN dynamics might represent 333 different physiological characteristics of consciousness during wakefulness and sleep. The 334 CAMP features in different conscious stages were remarkable and would help improve our 335 knowledge of the changes in consciousness during wakefulness and sleep. 336

However, all of these CAMPs displayed different activities in DMN regions during 337 wakefulness and sleep. In particular, all DMN regions exhibited reduced activity during SWS 338 stages in all CAMPs (Fig. 3e-3g). Moreover, the regions with significantly reduced activity in 339 the aDMN were the posterior DMN structures, and the regions with significantly reduced 340 activity in the pDMN were the anterior DMN regions, which all showed relatively lower 341 activity in the AWAKE stage. The significant decrease in the activity of regions with a lower 342 level activity indicated a preservation of the major activity in high-activity micropatterns in 343 344 deep sleep (Fig. 3f-3g, red stars). However, all CAMPs displayed increased activity in most DMN regions during the REM sleep stage. The activity in the HIP, OFC and RSC regions was 345 significantly increased during the REM sleep stage in all CAMPs, implying the importance of 346



347

**Fig. 4.** Characteristics of CAMPs and the transitions among them in different stages of consciousness during wakefulness and sleep. (a) Comparisons of the occurrence probability for all CAMPs in the three stages. The black dots indicate the values of the occurrence probability obtained from 29 rats in different CAMPs and stages. The black stars indicate significant differences with a corrected p<0.001. (b) Comparisons of the duration probability. (c) Comparisons of the mean duration. (d-f) The transition structures among CAMPs for the AWAKE (d), SWS (e) and REM sleep stages (f). All the numbers indicate the mean TPs calculated for the 29 rats and the standard deviation. The numbers in blue

indicate a significantly lower transition probability than observed in the AWAKE stage, and the numbers in red indicate a significantly higher transition probability. The significance level is a corrected p<0.001.

358

these DMN regions for REM sleep (Fig. 3h-3j, red stars). In addition, the mean activity level of each CAMP exhibited a similar variation trend across different conscious stages. The lowest mean activity of CAMPs was observed in the SWS stage, while the highest mean activity was observed in the REM sleep stage (Fig. 3d).

3.3. The constitutions and transitions of CAMPs during wakefulness and sleep. The 363 configurations of these CAMPs involved in DMN dynamics in different conscious stages were 364 also distinct (Fig. 4a-4c). All CAMPs presented similar features in the AWAKE stage 365 (occurrence probability: 32.12%, 34.12% and 33.75%; duration probability: 31.68%, 34.15% 366 and 34.17%; and mean duration: 29.79 ms, 24.41 ms and 24.37 ms for the cDMN, aDMN and 367 pDMN, respectively. No significant differences in all features were observed.), indicating that 368 their roles were equivalent and a dynamic balance in DMN activity might exist among CAMPs 369 at wakeful rest. However, the cDMN became the dominant activity pattern of DMN dynamics 370 in the SWS stage, as indicated by its largest occurrence probability (62.66%, 17.56% and 19.78% 371 for the cDMN, aDMN and pDMN, respectively), duration probability (61.47%, 18.02% and 372 20.51% for the cDMN, aDMN and pDMN, respectively) and mean duration (55.58 ms, 21.89) 373 ms and 22.78 ms for the cDMN, aDMN and pDMN, respectively) among all CAMPs. The 374 predominant constituent of the low-activity micropattern suggested that all the DMN regions 375 376 might be in a state of low activity and that the DMN activity preferred a silent pattern in deep sleep. Unlike the SWS stage, the two high-activity micropatterns were the main CAMPs 377 observed in the REM sleep stage, as indicated by the remarkably larger values for all features 378

19

of the aDMN and pDMN than the cDMN (occurrence probability: 19.42%, 42.05% and 38.53%; duration probability: 19.33%, 41.84% and 38.83%; and mean duration: 21.88 ms, 26.92 ms and 26.01 ms for the cDMN, aDMN and pDMN, respectively). The greater percentage of high-activity micropatterns during REM sleep suggested a reactivation of DMN activity in this consciousness stage. In addition, in the comparison between the two highactivity micropatterns, the aDMN displayed significantly larger values for the three features, implying a more important role of the aDMN in REM sleep.

Meanwhile, the temporal concatenations of these CAMPs (i.e., the CAMP indices) in 386 different consciousness stages also showed specific changes. We first performed a 387 randomization test to examine the transition structures of these CAMP indices in different 388 stages. The transitions among CAMPs occurred randomly in the AWAKE stage (p = 0.8157), 389 indicating that the transition probabilities (TPs) of pairs of CAMPs in the resting state were 390 proportional to their occurrences. However, these transitions did not occur randomly in the 391 SWS (p<0.0001) or REM sleep stages (p<0.0001), which suggested the stabilization of the 392 structures of the CAMP indices during the sleep cycle. These stabilizations further implied the 393 existence of several preferred transitions among CAMPs in the SWS and REM sleep stages. 394

Next, we compared the transition probabilities (TPs) for pairs of CAMPs between the two sleep stages and the AWAKE stage. The TPs of different pairs of CAMPs in the AWAKE stages were similar (no significant differences among all TPs, Fig. 4d), suggesting the presence of balanced state transitions among all CAMPs at rest. However, the TPs within the two highactivity micropatterns showed significant reductions in the SWS stage, while the TPs between high-activity micropatterns and the low-activity micropattern increased significantly (Fig. 4e). These changes in TPs emphasized the functional role of inhibitory activity in DMN regions in



402

Fig. 5. Phase locking relationship between each CAMP with slow oscillations in the SWS stage. (a-c)
The phase locking relationships between the cDMN (a), aDMN (b) and pDMN (c) with the slow
oscillations in anterior DMN regions. (d-f) The phase locking relationships between the cDMN (d),
aDMN (e) and pDMN (f) with the slow oscillations in posterior DMN regions. The red lines showed
the significant directionality with Rayleigh test p<0.001.</li>

408

deep sleep. On the other hand, the TPs in the REM sleep stage displayed different alterations 409 than in the SWS stage, including significantly increased TPs within high-activity 410 micropatterns and a remarkable decrease in TPs between high-activity micropatterns and the 411 low-activity micropattern (Fig. 4f). The increased transitions within the two high-activity 412 micropatterns revealed increased activation of DMN regions during REM sleep. Based on 413 these findings, the CAMP indices and the functional roles of these CAMPs were specific for 414 415 different conscious stages. The alterations in DMN activity during wakefulness and sleep might be attributed to the specific temporal combinations of the CAMPs constituting the 416 activity in different conscious stages rather than the spatial structures of CAMPs themselves, 417

418 which were rather stable across different stages.

## 419 **3.4.** Strong phasic relationships between CAMPs with the up-down states in the SWS

stage. Up-down states are considered the predominant pattern of slow oscillations (0.5-2 Hz) 420 during the SWS stage. By estimating the phase distribution of each CAMP in the anterior and 421 posterior DMN slow activity with the Hilbert transform, we observed that these CAMPs 422 displayed strong phasic relationships with the up-down states in the SWS stage. The cDMN 423 preferred the down state of anterior DMN activity (Fig. 5a, significant directionality:  $1.97\pi$ , 424 red line) and the up state of posterior DMN activity (Fig. 5d, significant directionality:  $1.16\pi$ , 425 red line). Additionally, both the aDMN and pDMN were phase locked to the up state of anterior 426 DMN activity (Fig. 5b, significant directionality:  $1.21\pi$  for aDMN. Fig. 5c, significant 427 directionality:  $1.18\pi$  for pDMN) and the down state of posterior DMN activity (Fig. 5e, 428 significant directionality:  $0.23\pi$  for aDMN. Fig. 5f, significant directionality:  $0.18\pi$  for 429 pDMN), implying that these two high-activity micropatterns might belong to the same activity 430 pattern of slow oscillations of the DMN in deep sleep. Furthermore, the difference of 431 significant directionality of all CAMPs suggested that the slow oscillations in anterior and 432 posterior DMN regions tended to have a phasic shift about  $\pi$  during deep sleep. Accordingly, 433 our proposed CAMPs could also reflect the up-down states of DMN slow activity in the SWS 434 stage and there existed a close physiological association between the up-down states with 435 DMN dynamics. 436

# 437 4. Discussion

In the present study, we developed a CAMP algorithm and applied it to reveal the dynamics of gamma activity in rat DMN during wakefulness and sleep. Our results indicated that the fast dynamics of gamma activity in the DMN were decomposed into three different

CAMPs (i.e., micropatterns) in different conscious stages, including the cDMN, aDMN and 441 442 pDMN. These CAMPs showed stable spatial structures across wakefulness and sleep, while their dynamic configurations were specific to different conscious stages. In addition, all these 443 CAMPs were strongly phase locked to the up-down states in the SWS stage, suggesting the 444 temporal sequence of the neural relationship between up-down states and DMN dynamics. 445 Our findings described the distinct dynamic configurations of gamma activity in the DMN 446 during wakefulness and sleep, and proposed a three-state model to reveal the fundamental 447 neural mechanism by which DMN dynamics mediate consciousness. 448

4.1. Physiological significance of three CAMPs. Previous studies have reported a strong 449 correlation between electrophysiological gamma activity and blood oxygen level-dependent 450 (BOLD) signals(Logothetis, 2002; Logothetis et al., 2001; Magri et al., 2012; Scheering et al., 451 2016). Besides, DMN regions also show deactivation in the gamma frequency during the 452 performance of external tasks in several EEG studies(Karim Jerbi\*† et al., 2010; Ossandon et 453 al., 2011), indicating the importance of gamma oscillation in DMN activity. Hence, we 454 specifically focused on the fast dynamics of gamma activity in the DMN in the current study. 455 The gamma activity in the rat DMN was decomposed into three stable CAMPs during 456 wakefulness and sleep that exhibited distinct spatial structures. The differences in these 457 CAMPs provided direct electrophysiological evidence that the DMN regions might not be 458 activated simultaneously. Moreover, all these CAMPs lasted for approximately forty 459 milliseconds, and different CAMPs had distinct periods. These phenomena exhibited 460 differences in the activation times of anterior and posterior DMN structures in the fast 461 dynamics and further illustrated the diversity in the latencies for both the excitation and 462 inhibition of DMN regions(Brett L. Foster, Mohammad Dastjerdi, 2012; Foster et al., 2015). 463

Indeed, functional and neuroanatomical studies have separated the structure of the DMN 464 465 into a parietal subnetwork and a prefrontal subnetwork in both human and animal brains(Cui et al., 2018; Hagmann et al., 2008; Lu et al., 2012; Wu et al., 2017). In the present study, we 466 not only reinforced this finding from the aspect of fast DMN dynamics but also provided a 467 possible dynamic substrate for this separation of the DMN structure. As a key component of 468 the DMN, the prefrontal cortex has historically been posited to integrate interoceptive and 469 exteroceptive information from multisensory stimuli for processing information about the 470 internal and external milieu of the body(Ongur and Price, 2000). Accordingly, we speculated 471 that the high-activity micropattern aDMN might be a type of DMN pattern that makes 472 inferences and guides actions in a timely and environmentally relevant manner. 473

Meanwhile, the retrosplenial cortex (RSC) located in the parietal DMN, another key area 474 in the DMN, has extensive connections and is topographically organized with the hippocampal 475 formation. The projections between the RSC and hippocampal formation provide an important 476 pathway regulating learning, memory and emotional behavior(Wyss and Vangroen, 1992). 477 Furthermore, the hippocampal formation is a limbic structure that forms direct or indirect 478 connections to the other DMN regions. Therefore, the high-activity micropattern pDMN 479 detected in the present study might be a type of DMN activity pattern associated with memory 480 and emotional behavior. Additionally, both the aDMN and pDMN were strongly phase locked 481 to the up state of anterior DMN activity and the down state of posterior DMN activity during 482 the SWS stage, indicating that they may reflect similar performance for the up-down states of 483 slow oscillations during DMN dynamics. Moreover, these two high-activity micropatterns 484 together accounted for more than 70% of the time in the resting state, which helps to explain 485 why the brain requires a high basal cerebral blood flow and metabolism for spontaneous 486

487 activity(Raichle and Mintun, 2006).

In addition, we observed a low-activity micropattern (i.e., cDMN) in DMN dynamics that 488 was widely distributed in all conscious stages during wakefulness and sleep. In the cDMN, all 489 DMN regions displayed relatively lower levels of activity, implicating that cDMN could be 490 viewed as the silent state for DMN activity in which all the DMN regions preferred relaxations 491 and prepared for the next excitation. However, the cDMN was the only one micropattern 492 during DMN dynamics in which all DMN regions operated in the same manner. Thus, the 493 494 appearance of the cDMN suggested that there might be a working mode for DMN with low energy, which desired future work to study. 495

4.2. The balance of dynamic DMN configurations supports consciousness during 496 wakefulness. Based on accumulating evidence, DMN activity is tightly correlated with 497 consciousness levels in health and disease(Buckner et al., 2008; Kapogiannis et al., 2014; 498 Panda et al., 2016; Vanhaudenhuyse et al., 2010). In the AWAKE stage, all the CAMPs showed 499 similar features and the dynamic transitions among them were not statistically different. These 500 similarities illustrated a balanced dynamic configuration among these CAMPs during fast 501 gamma activity in the DMN at rest. The DMN is a key network involved in integrating high-502 order information from multiple sensory modalities based on numerous projections from 503 variable somatic cortex and core limbic structures (HIP and amygdala) to the DMN 504 regions(Heidbreder and Groenewegen, 2003; Reep et al., 1994). These projections provide the 505 anatomical substrate for the correlation of DMN activity to consciousness levels. Accordingly, 506 507 the identified balance of DMN dynamics might be a competitive product between the integration and differentiation of CAMPs in maintaining consciousness during wakefulness 508 (Cavanna et al., 2018; Tononi, 2004; Tononi et al., 2016). Furthermore, this balance of 509

510 dynamic configurations also indicated that the DMN might function in multistable regimes 511 and revealed the potential neural mechanism by which DMN activity supports cognitive 512 functions in the resting state(Andrews-Hanna, 2012; Buckner et al., 2008).

4.3. Functional reorganization of the dynamic configurations of the DMN during sleep. 513 Compared to the resting state, the SWS stage was always accompanied by reduced brain 514 activity, while the commensurate brain activity has been reported in the REM sleep 515 stage(Hobson, 2009; Horovitz et al., 2008). Consistent alterations in the average brain activity 516 associated with CAMPs during DMN dynamics were also observed in our study, suggesting 517 that the activity of CAMPs might also reveal the changes in consciousness during wakefulness 518 and sleep. However, the reduced activity of all CAMPs might not be the main explanation for 519 the decrease in DMN activity observed during deep sleep, due to the stable spatial structures 520 of these CAMPs during wakefulness and sleep. This decrease in activity might result from the 521 increased occurrence probability of the cDMN and the decreased probabilities of the other two 522 high-activity micropatterns. These inversely changed occurrence probabilities in different 523 CAMPs revealed the neural mechanism of reduced activity, that the DMN regions preferred 524 the silent state in deep sleep(Bazhenov et al., 2002; Diekelmann and Born, 2010). 525

The balance of dynamic configurations of the DMN was also disrupted during sleep, indicating the functional reorganization of DMN dynamics. The functional reorganization subsequently led to a loss of consciousness in different sleep stages(Tononi, 2004; Tononi et al., 2016). In the REM sleep stage, the dynamic transitions between aDMN and pDMN increased, indicating more communication between anterior and posterior DMN regions. These communications between anterior and posterior DMN regions might be crucial to primary consciousness, which has been postulated to be preserved in the REM sleep stage(Hobson, 2009). Moreover, these communications displayed a combination of both the top-down and bottom-up mechanisms in the DMN. These two mechanisms are important for information processing in the brain(Buschman and Miller, 2007; Theeuwes, 2010), and an enhancement of these mechanisms might help us elucidate the underlying neurophysiological basis for the preservation of primary consciousness during REM sleep.

In the SWS stage, the dynamic transitions among CAMPs displayed different changes. 538 The dynamic transitions between the low-activity micropattern and two high-activity 539 micropatterns increased significantly. Additionally, a strong phasic relationship was observed 540 between CAMPs and the up-down states during slow oscillations of the anterior and posterior 541 DMN, and these two types of CAMPs corresponded to different up-down states. Accordingly, 542 the dynamic transitions between the low-activity micropattern and two high-activity 543 544 micropatterns were deemed to be the transitions within up-down states in the DMN. The dominant transitions of up-down states in deep sleep further provided the physiological 545 importance for these increased dynamic transitions. However, the dynamic transitions within 546 the two high-activity micropatterns decreased in the SWS stage. These reductions supported 547 our hypothesis that communications between anterior and posterior DMN regions are 548 important for primary consciousness, since both higher cognitive functions and primary 549 consciousness are lost during deep sleep (Hobson and Pace-Schott, 2002). The loss of higher 550 cognitive functions might not be caused by the change in a single type of dynamic transitions 551 within pairs of CAMPs. We speculated that the balance of dynamic configurations of the DMN 552 553 is the underlying neural mechanism supporting higher cognitive functions, which emerged in wakefulness and were deactivated during sleep. The coordination and cooperation of all 554 CAMPs played a core role in the ability of the DMN to perform higher cognitive functions. 555

bioRxiv preprint doi: https://doi.org/10.1101/2020.07.29.226647; this version posted July 30, 2020. The copyright holder for this preprint (which was not certified by peer review) is the author/funder. All rights reserved. No reuse allowed without permission.



### 556

**Fig. 6.** The three-state model of the consciousness levels during wakefulness and sleep. The AWAKE stage requires the cooperation of all three CAMPs, while the SWS stage requires communications between the low-activity micropattern (cDMN) and the high-activity micropatterns (aDMN or pDMN). The REM sleep stage requires interactions within the two high-activity micropatterns.

561

Based on these findings, here, we propose a three-state model to describe the relationship 562 between DMN micropatterns and the underlying consciousness levels observed during 563 wakefulness and sleep. As shown in Fig. 6, the three CAMPs involved in DMN dynamics are 564 the basis of this model and their interactions refer to the underlying mechanism regulating the 565 consciousness level observed in distinct stages. Equal communications among the three 566 CAMPs support conscious awareness in the AWAKE stage. The communications between the 567 low-activity micropattern (i.e., cDMN) and each of the high-activity micropatterns (i.e., 568 aDMN or pDMN) are important for the SWS stage characterized by a low level of 569 consciousness. However, during the REM sleep with primary consciousness, communications 570 within high-activity micropatterns are the predominant. 571

572 According to the proposed three-state model, we conjecture that preservation of conscious 573 awareness not only requires the information processing between anterior and posterior DMN

regions, but also need all DMN regions silent and relaxed during this process. Information 574 processing within anterior and posterior DMN regions is mediated by up-down and bottom-575 up mechanisms and is vital for supporting conscious awareness and primary consciousness. A 576 lack of this process could lead to the loss of consciousness in the SWS stage, and this process 577 alone would result in the consciousness level of REM sleep stage that exists as primary 578 consciousness. This phenomenon highlights the importance of the silent pattern for all DMN 579 regions during the resting state with conscious awareness. However, the roles of the silent 580 pattern in DMN regions and the communications within anterior and posterior DMN regions 581 are unable to be validated by performing some other neurostimulation experiments using the 582 currently available neuroimaging methods. Future studies could validate our model and apply 583 it to the human brain through the application of other neuroimaging measures. 584

4.4. Methodological Perspectives. Consistent with the promising microstate analysis of 585 EEG/LFP signals(Michel and Koenig, 2018), the CAMP analysis reported in the present study 586 also assumes that brain activity consists of several distinct instantaneous patterns. The 587 difference is that the CAMP method focuses on the nature of brain activity in different regions 588 and extracts micropatterns from envelope signals. Envelope signals imply temporal alterations 589 in brain power, and their decomposition directly reveals brain rhythm dynamics. In addition, 590 the coactive patterns analyzed in the CAMP method were chosen based on the distribution of 591 extreme values in the envelope signals of brain regions, which differs from the method used 592 in a microstate analysis. Local extreme values in envelope signals represent the instantaneous 593 594 higher/lower activity of brain regions followed by contrasting changes in activity. Therefore, the derived coactive patterns were considered as the activity patterns leading to an inversion 595 of activity among regions in specific brain networks. Therefore, we postulate that this 596

proposed CAMP method will help researchers extract coactive micropatterns in specific brain
networks and reveal additional underlying information about fast brain dynamics.

## 599 **5. Conclusion**

In the current work, we developed a CAMP algorithm to reveal the dynamics of gamma 600 activity in rat DMN during wakefulness and sleep. The fast dynamics of gamma activity in the 601 DMN could be decomposed into three different CAMPs, which showed stable spatial 602 structures across three conscious stages. However, the dynamic configurations of them are 603 specific to different conscious stages. Besides, we also indicated temporal sequence of the 604 neural relationship between up-down states and these CAMPs during deep sleep. Taken 605 together, our results provided functional descriptions for the dynamics of gamma activity in 606 rat DMN during different conscious stage, and proposed a three-state model to reveal the 607 fundamental neural associations between DMN activity with consciousness levels. 608

609

# **CRediT authorship contribution statement**

Yan Cui: Methodology, Formal analysis, Visualization, Writing-Original draft preparation,
Min Li: Methodology. Bharat Biswal: Investigation, Validation, Writing-Reviewing & Editing.
Wei Jing: Data curation, Visualization. Changsong Zhou: Validation, Writing- Reviewing &
Editing. Huixiao Liu: Formal analysis. Yang Xia: Conceptualization, Resources. Daqing Guo:
Conceptualization, Visualization, Funding acquisition, Writing-Reviewing & Editing.
Dezhong Yao: Conceptualization, Project administration, Supervision, Funding acquisition,
Writing-Reviewing & Editing.

617 Declaration of competing interest: None

## 618 Acknowledgements

619 We thank Prof. Pedro A. Valdes-Sosa for valuable discussions and suggestions on this

620	work. This study was supported by the National Natural Science Foundation of China
621	(81861128001, 61527815, 31771149, 61761166001, 61871420, 11975194 and 81901366), the
622	Sichuan Science and Technology Program (Grant No. 2018HH0003), and the 111 project
623	(Grant No. B12027).

#### 624 **References**

- Amzica, F., Steriade, M., 1995. Short- and long-range neuronal synchronization of the slow
  (<1 Hz) cortical oscillation. J. Neurophysiol. 73, 20–38.</li>
  https://doi.org/10.1152/jn.1995.73.1.20
- 628Andrews-Hanna, J.R., 2012. The Brain's Default Network and its Adaptive Role in Internal629Mentation.Neuroscientist18,251–270.630https://doi.org/10.1016/j.neuroimage.2013.08.045
- Bazhenov, M., Timofeev, I., Steriade, M., Sejnowski, T.J., 2002. Model of thalamocortical
  slow-wave sleep oscillations and transitions to activated states. J. Neurosci. 22, 1.
- Beckmann, C.F., DeLuca, M., Devlin, J.T., Smith, S.M., 2005. Investigations into resting-state
  connectivity using independent component analysis. Philos. Trans. R. Soc. B Biol. Sci.
  360, 1001–1013. https://doi.org/10.1098/rstb.2005.1634
- Brett L. Foster, Mohammad Dastjerdi, and J.P., 2012. Neural populations in human
  posteromedial cortex display opposing responses during memory and numerical
  processing. Proc. Natl. Acad. Sci. 109, 15514–15519.
  https://doi.org/10.1073/pnas.1206580109/-
- 640 /DCSupplemental.www.pnas.org/cgi/doi/10.1073/pnas.1206580109

641 Buckner, R.L., Andrews-Hanna, J.R., Schacter, D.L., 2008. The brain's default network:

- Anatomy, function, and relevance to disease. Ann. N. Y. Acad. Sci. 1124, 1–38.
  https://doi.org/10.1196/annals.1440.011
- Buschman, T.J., Miller, E.K., 2007. Top-Down Versus Bottom-Up Control of Attention in the
- 645 Prefrontal and. Science (80-.). 315, 1860–1863. https://doi.org/10.1126/science.1138071
- 646 Cavanna, F., Vilas, M.G., Palmucci, M., Tagliazucchi, E., 2018. Dynamic functional
- 647 connectivity and brain metastability during altered states of consciousness. Neuroimage

648 180, 383–395. https://doi.org/10.1016/j.neuroimage.2017.09.065

- 649 Cui, Y., Yu, S., Zhang, T., Zhang, Y., Xia, Y., Yao, D., Guo, D., 2018. Altered activity and
- 650 information flow in the default mode network of pilocarpine-induced epilepsy rats. Brain
  651 Res. 1696, 71–80. https://doi.org/10.1016/j.brainres.2018.05.012
- Diekelmann, S., Born, J., 2010. The memory function of sleep. Nat. Rev. Neurosci. 11, 114–
  26. https://doi.org/10.1038/nrn2762
- Foster, B.L., Rangarajan, V., Shirer, W.R., Parvizi, J., 2015. Intrinsic and task-dependent
  coupling of neuronal population activity in human parietal cortex. Neuron 86, 578–590.
  https://doi.org/10.1016/j.neuron.2015.03.018
- Fox, K.C.R., Foster, B.L., Kucyi, A., Daitch, A.L., Parvizi, J., 2018. Intracranial
  Electrophysiology of the Human Default Network. Trends Cogn. Sci.
  https://doi.org/10.1016/j.tics.2018.02.002
- Fox, M.D., Snyder, A.Z., Vincent, J.L., Corbetta, M., Essen, C. Van, Raichle, M.E., Fox, M.D.,
  Snyder, A.Z., Vincent, J.L., Corbetta, M., Essen, D.C. Van, Raichle, M.E., 2016.
  Networks Linked references are available on JSTOR for this article : The human brain is
  intrinsically organized into dynamic , anticorrelated functional networks. Proc. Natl.
  Acad. Sci. U. S. A.
- Gusnard, D.A., Akbudak, E., Shulman, G.L., Raichle, M.E., 2001. Medial prefrontal cortex
  and self-referential mental activity: Relation to a default mode of brain function. Proc.
  Natl. Acad. Sci. U. S. A. 98, 4259–4264. https://doi.org/10.1073/pnas.071043098
- Hagmann, P., Cammoun, L., Gigandet, X., Meuli, R., Honey, C.J., Van Wedeen, J., Sporns, O.,
  2008. Mapping the structural core of human cerebral cortex. PLoS Biol. 6, 1479–1493.
- 670 https://doi.org/10.1371/journal.pbio.0060159
- Heidbreder, C.A., Groenewegen, H.J., 2003. The medial prefrontal cortex in the rat: Evidence
   for a dorso-ventral distinction based upon functional and anatomical characteristics.
- 673 Neurosci. Biobehav. Rev. 27, 555–579. https://doi.org/10.1016/j.neubiorev.2003.09.003
- 674 Hobson, J.A., 2009. REM sleep and dreaming: Towards a theory of protoconsciousness. Nat.
- 675 Rev. Neurosci. 10, 803–814. https://doi.org/10.1038/nrn2716
- Hobson, J.A., Pace-Schott, E.F., 2002. The cognitive neuroscience of sleep: Neuronal systems,
- 677 consciousness and learning. Nat. Rev. Neurosci. 3, 679–693.

# 678 https://doi.org/10.1038/nrn915

- Holcman, D., Tsodyks, M., 2006. The emergence of up and down states in cortical networks.
- 680 PLoS Comput. Biol. 2, 174–181. https://doi.org/10.1371/journal.pcbi.0020023
- 681 Horovitz, S.G., Fukunaga, M., De Zwart, J.A., Van Gelderen, P., Fulton, S.C., Balkin, T.J.,
- 682 Duyn, J.H., 2008. Low frequency BOLD fluctuations during resting wakefulness and
- light sleep: A simultaneous EEG-fMRI study. Hum. Brain Mapp. 29, 671–682.
  https://doi.org/10.1002/hbm.20428
- Ji, D., Wilson, M.A., 2007. Coordinated memory replay in the visual cortex and hippocampus
   during sleep. Nat. Neurosci. 10, 100–107. https://doi.org/10.1038/nn1825
- Jing, W., Guo, D., Zhang, Y., Guo, F., Valdés-Sosa, P.A., Xia, Y., Yao, D., 2017. Reentrant
- 688 information flow in electrophysiological rat default mode network. Front. Neurosci. 11,

689 1–12. https://doi.org/10.3389/fnins.2017.00093

- Kapogiannis, D., Reiter, D.A., Willette, A.A., Mattson, M.P., 2014. Dynamic functional
  connectivity of the default mode network tracks daydreaming. Neuroimage 100, 112–119.
  https://doi.org/10.1016/j.neuroimage.2012.09.029.Posteromedial
- 693 Karim Jerbi\*†, R., V.J., Tomas, , O., Dalal, S.S., Julien Jung, D.H., Minotti, L., Bertrand1,
- O., Kahane, P., Lachaux, and J.-P., 2010. Exploring the electrophysiological correlates
  of the default-mode network with intracerebral EEG. Front. Syst. Neurosci. 4, 1–9.
  https://doi.org/10.3389/fnsys.2010.00027
- Larson-Prior, L.J., Zempel, J.M., Nolan, T.S., Prior, F.W., Snyder, A., Raichle, M.E., 2009.
   Cortical network functional connectivity in the descent to sleep. Proc. Natl. Acad. Sci. U.
- 699 S. A. 106, 4489–4494. https://doi.org/10.1073/pnas.0900924106
- 700 Lehmann, D., Faber, P.L., Galderisi, S., Herrmann, W.M., Kinoshita, T., Koukkou, M., Mucci,
- A., Pascual-Marqui, R.D., Saito, N., Wackermann, J., Winterer, G., Koenig, T., 2005.
  EEG microstate duration and syntax in acute, medication-naïve, first-episode
  schizophrenia: A multi-center study. Psychiatry Res. Neuroimaging 138, 141–156.
  https://doi.org/10.1016/j.pscychresns.2004.05.007
- Liu, Q., Farahibozorg, S., Porcaro, C., Wenderoth, N., Mantini, D., 2017. Detecting large-scale
  networks in the human brain using high-density electroencephalography. Hum. Brain
  Mapp. 38, 4631–4643. https://doi.org/10.1002/hbm.23688

- Liu, X., Chang, C., Duyn, J.H., 2013. Decomposition of spontaneous brain activity into
  distinct fMRI co-activation patterns. Front. Syst. Neurosci. 7, 1–11.
  https://doi.org/10.3389/fnsys.2013.00101
- Liu, X., Duyn, J.H., 2013. Time-varying functional network information extracted from brief
  instances of spontaneous brain activity. Proc. Natl. Acad. Sci. U. S. A. 110, 4392–7.
- 713 https://doi.org/10.1073/pnas.1216856110
- Logothetis, N.K., 2002. The neural basis of the blood-oxygen-level-dependent functional
  magnetic resonance imaging signal. Philos. Trans. R. Soc. B Biol. Sci. 357, 1003–1037.
  https://doi.org/10.1098/rstb.2002.1114
- Logothetis, N.K., Pauls, J., Augath, M., Trinath, T., Oeltermann, A., 2001. Neurophysiological
  investigation of the basis of the fMRI signal. Nature 412, 150–157.
  https://doi.org/10.1038/35084005
- Lőrincz, M.L., Gunner, D., Bao, Y., Connelly, W.M., Isaac, J.T.R., Hughes, S.W., Crunelli, V.,
  2015. A distinct class of slow (~0.2–2 Hz) intrinsically bursting layer 5 pyramidal neurons
  determines UP/DOWN state dynamics in the neocortex. J. Neurosci. 35, 5442–5458.
  https://doi.org/10.1523/JNEUROSCI.3603-14.2015
- Lu, H., Zou, Q., Gu, H., Raichle, M.E., Stein, E.A., Yang, Y., 2012. Rat brains also have a
  default mode network. Proc. Natl. Acad. Sci. U. S. A. 109, 3979–84.
  https://doi.org/10.1073/pnas.1200506109
- Magri, C., Schridde, U., Murayama, Y., Panzeri, S., Logothetis, N.K., 2012. The Amplitude
  and Timing of the BOLD Signal Reflects the Relationship between Local Field Potential
  Power at Different Frequencies. J. Neurosci. 32, 1395–1407.
  https://doi.org/10.1523/JNEUROSCI.3985-11.2012
- Michel, C.M., Koenig, T., 2018. EEG microstates as a tool for studying the temporal dynamics
  of whole-brain neuronal networks: A review. Neuroimage 180, 577–593.
  https://doi.org/10.1016/j.neuroimage.2017.11.062
- Ongur, D., Price, J., 2000. The Organization of Networks within the Orbital and Medial
  Prefrontal Cortex of Rats, Monkeys and Humans. Cereb. Cortex 10, 206–219.
  https://doi.org/10.1093/cercor/10.3.206
- 737 Ossandon, T., Jerbi, K., Vidal, J.R., Bayle, D.J., Henaff, M.-A., Jung, J., Minotti, L., Bertrand,

738

O., Kahane, P., Lachaux, J.-P., 2011. Transient Suppression of Broadband Gamma Power

739	in the Default-Mode Network Is Correlated with Task Complexity and Subject
740	Performance. J. Neurosci. 31, 14521–14530. https://doi.org/10.1523/JNEUROSCI.2483-
741	11.2011
742	Panda, R., Bharath, R.D., Upadhyay, N., Mangalore, S., Chennu, S., Rao, S.L., 2016. Temporal
743	Dynamics of the Default Mode Network Characterize Meditation-Induced Alterations in
744	Consciousness. Front. Hum. Neurosci. 10, 1–12.
745	https://doi.org/10.3389/fnhum.2016.00372
746	Petersen, C.C.H., Hahn, T.T.G., Mehta, M., Grinvald, A., Sakmann, B., 2003. Interaction of
747	sensory responses with spontaneous depolarization in layer 2/3 barrel cortex. Proc. Natl.
748	Acad. Sci. U. S. A. 100, 13638–13643. https://doi.org/10.1073/pnas.2235811100
749	Raichle, M.E., 2015. The Brain 's Default Mode Network. Annu. Rev. Neurosci. 413-427.
750	https://doi.org/10.1146/annurev-neuro-071013-014030
751	Raichle, M.E., MacLeod, A.M., Snyder, A.Z., Powers, W.J., Gusnard, D.A., Shulman, G.L.,
752	2001. A default mode of brain function. Proc. Natl. Acad. Sci. U. S. A. 98, 676-82.
753	https://doi.org/10.1073/pnas.98.2.676
754	Raichle, M.E., Mintun, M.A., 2006. Brain work and brain imaging. Annu. Rev. Neurosci. 29,
755	449-76. https://doi.org/10.1146/annurev.neuro.29.051605.112819
756	Reep, R.L., Chandler, H.C., King, V., Corwin, J. V., 1994. Rat posterior parietal cortex:
757	topography of corticocortical and thalamic connections. Exp. Brain Res. 100, 67-84.
758	https://doi.org/10.1007/BF00227280
759	Rosazza, C., Minati, L., 2011. Resting-state brain networks: Literature review and clinical
760	applications. Neurol. Sci. 32, 773-785. https://doi.org/10.1007/s10072-011-0636-y
761	Sämann, P.G., Wehrle, R., Hoehn, D., Spoormaker, V.I., Peters, H., Tully, C., Holsboer, F.,
762	Czisch, M., 2011. Development of the brain's default mode network from wakefulness
763	to slow wave sleep. Cereb. Cortex 21, 2082–2093. https://doi.org/10.1093/cercor/bhq295
764	Scheering, R., Koopmans, P.J., Van Mourik, T., Jensen, O., Norris, D.G., 2016. The
765	relationship between oscillatory EEG activity and the laminar-specific BOLD signal.
766	Proc. Natl. Acad. Sci. U. S. A. 113, 6761–6766. https://doi.org/10.1073/pnas.1522577113
767	Theeuwes, J., 2010. Top-down and bottom-up control of visual selection. Acta Psychol.

768 (Amst). 135, 77–99. https://doi.org/10.1016/j.actpsy.2010.02.006

769 Tononi, G., 2004. An information integration theory of consciousness., BMC neuroscience.

770 BioMed Central. https://doi.org/10.1186/1471-2202-5-42

- 771
   Tononi, G., Boly, M., Massimini, M., Koch, C., 2016. Integrated information theory: From

   772
   consciousness
   to
   its
   physical
   substrate.
   Nat.
   Rev.
   Neurosci.
- 773 https://doi.org/10.1038/nrn.2016.44
- Vanhaudenhuyse, A., Noirhomme, Q., Tshibanda, L.J.F., Bruno, M.A., Boveroux, P.,
  Schnakers, C., Soddu, A., Perlbarg, V., Ledoux, D., Brichant, J.F., Moonen, G., Maquet,
- The semianers, e., sedaa, m, renearg, m, Beacan, B, Brienand, en, moonen, e., maqued,
- P., Greicius, M.D., Laureys, S., Boly, M., 2010. Default network connectivity reflects the
- level of consciousness in non-communicative brain-damaged patients. Brain 133, 161–
- 778 171. https://doi.org/10.1093/brain/awp313
- Vidaurre, D., Smith, S.M., Woolrich, M.W., 2017. Brain network dynamics are hierarchically
  organized in time. Proc. Natl. Acad. Sci. 201705120.
  https://doi.org/10.1073/pnas.1705120114
- Wu, X. jie, Zeng, L.L., Shen, H., Yuan, L., Qin, J., Zhang, P., Hu, D., 2017. Functional network
  connectivity alterations in schizophrenia and depression. Psychiatry Res. Neuroimaging
  263, 113–120. https://doi.org/10.1016/j.pscychresns.2017.03.012
- Wyss, J.M., Vangroen, T., 1992. Connections between the retrosplenial cortex and the
  hippocampal-formation in the rat a review. Hippocampus 2, 1–12.
  https://doi.org/10.1002/hipo.450020102

788