

1 **Supplementary Methods and Materials**

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3 **Stimuli**

4

5 *Evoked cuff pain*

6 Deep-tissue pain was applied using the Hokanson Rapid Cuff Inflator (D. E. Hokanson, Inc.,
7 Bellevue, WA, USA). Compared to cutaneous quantitative sensory testing (QST) techniques (e.g.,
8 contact heat), deep sustained pain better mimics clinical pain (1, 2), thus providing a more
9 clinically-relevant measure. Unlike more superficial methods of evaluating mechanical sensitivity,
10 cuff pain responses are only marginally affected by sensitization or desensitization of the skin,
11 indicating that this procedure primarily assesses sensitivity in muscle and other deep tissues (3–6).
12 Such cuff pressure algometry is a recently characterized method that is now included in many QST
13 evaluations (3, 4, 7). We have considerable experience applying these techniques in chronic pain
14 patients, with and without neuroimaging, and have found that even subjects with severe
15 fibromyalgia are generally able to tolerate these procedures without any lasting discomfort (8, 9).
16 The cuff was attached to the patient’s left lower leg prior to scanning and was inflated for 15 s
17 duration trials during the experiment.

18

19 *Electroacupuncture*

20 Our decision to use electroacupuncture applied by acupuncturists for evoked cuff pain as an
21 experimental model for dyadic interaction with pain therapy was motivated by our aim to
22 investigate both a consultation/intake and actual treatment with measurable pain outcomes. As

23 opposed to many other pain therapies, this electroacupuncture/cuff pain model enabled us to
24 incorporate acute pain therapy in the MRI environment, with acupuncturists remotely applying
25 treatment relevant to their clinical practice, thus increasing ecological validity while maintaining
26 experimental control.

27 Prior to experimental testing, patients had acupuncture needles (0.20 mm diameter, 25 cm
28 length, Asiamed gauge) inserted with approximately 2-3cm depth at acupoints ST-34 and SP-10 on
29 the anterior/distal aspect of the lower thigh, proximal to the cuff, with electrodes attached to each
30 needle. While we were interested in the influence of therapeutic alliance, and not specific
31 acupuncture effects, on pain outcomes, we wanted to avoid the need for authorized deception in
32 clinicians' IRB consent form. We therefore included trials with both verum and sham electro-
33 acupuncture in a double-blind manner. We used a minimal sub-sensory threshold level (0.1 mA)
34 for verum trials in order to avoid unblinding patients due to any sensory feedback from the electrical
35 stimulation. Thus, verum/sham electro-acupuncture was administered in a double-blind manner, in
36 a pseudorandomized order across trials. Clinicians were instructed to press-and-hold one button for
37 applying treatment, and another ("inactive") button for No-treatment.

38 We did not hypothesize differences in pain for verum vs sham electro-acupuncture
39 treatment, and indeed, a paired t-test comparing patient-rated pain intensity between verum and
40 sham trials did not suggest a difference in pain intensity ($t=0.83$, $P=0.42$). Consequently, we pooled
41 verum/sham trials as 'Treatment' in further statistical analyses, and interpreted intra-individual
42 differences between 'Treatment' and 'No-Treatment' trials as psychosocially induced pain relief
43 ('analgesia').

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45 **MRI acquisition and preprocessing**

46

47 *MRI acquisition*

48 Blood oxygen level-dependent (BOLD) fMRI data were collected from each scanner (Patient
49 scanner: Siemens 3T Skyra; Clinician scanner: Siemens 3T Prisma) using a whole brain,
50 simultaneous multi-slice, T2*-weighted gradient echo BOLD echo-planar imaging pulse sequence
51 (repetition time = 1250 ms, echo time = 33 ms, flip angle = 65°, voxel size = 2 cm isotropic, number
52 of slices = 75, Simultaneous Multi-Slice factor = 5). A high-resolution structural volume (multi-
53 echo MPRAGE) was collected to facilitate anatomical localization and spatial registration of
54 individual fMRI-BOLD volumes to MNI152 standard space (repetition time = 2530 ms, echo time
55 = 1.69 ms, flip angle = 7°, voxel size = 1 mm isotropic). Importantly, to enable a full-face view of
56 each participant for better facial expression tracking by research subjects and the facial expression
57 digitization software (see below), we combined the occipital/bottom portion of a 64 Channel head
58 coil with a flex coil (4 channel) attached to the forehead.

59

60 *fMRI preprocessing*

61 Preprocessing of individual fMRI datasets was carried out using tools from FMRIB's Software
62 Library (FSL, v6.0.0; www.fmrib.ox.ac.uk/fsl), and included the following steps: slice-timing
63 correction, motion correction (MCFLIRT) (10), correction of spatial inhomogeneity (TOPUP) (11,
64 12), nonbrain tissue removal (BET) (13), spatial smoothing (full width at half maximum = 4mm),
65 temporal high-pass filtering ($f=0.011$ Hz as computed by FSL's `cutoffcalc`), and grand-mean
66 intensity normalization by a single multiplicative factor. For each subject, both runs were realigned
67 (6 degrees of freedom) to a common space (7th volume of the first run) before the first-level general
68 linear model (GLM) analyses. The transformation matrix for registration between functional and

69 high-resolution anatomical volumes was calculated using Boundary Based Registration (bbsregister,
70 Freesurfer, v6.0.0 (14)). Two participants had one of their two fMRI runs excluded from analysis
71 due to excessive head motion, based on the following exclusion criteria: 1) $>2^\circ$ head rotation in any
72 direction, and 2) >2 mm frame-by-frame displacement. After excluding these data, mean head
73 rotation was 0.05 ± 0.02 (mean \pm SD) and mean frame-by-frame displacement was 0.13 ± 0.05 . An
74 unpaired t-test indicated higher frame-by-frame displacement for patients (0.15 ± 0.05) relative to
75 clinicians (0.11 ± 0.04 , $t=4.32$, $P<0.001$), but there was no significant group difference for rotation
76 ($t=1.74$, $P=0.09$). For registration from structural to standard space (Montreal Neurological
77 Institute, MNI, 152), we used FSL's Linear registration tool (FLIRT, 12 degrees of freedom) (10,
78 15), followed by FSL's non-linear registration tool (FNIRT) (16). All single-subject analyses were
79 performed in functional space, and then registered to MNI152 standard space before dyadic and
80 group analyses.

81

82 **References**

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Supplementary Figures

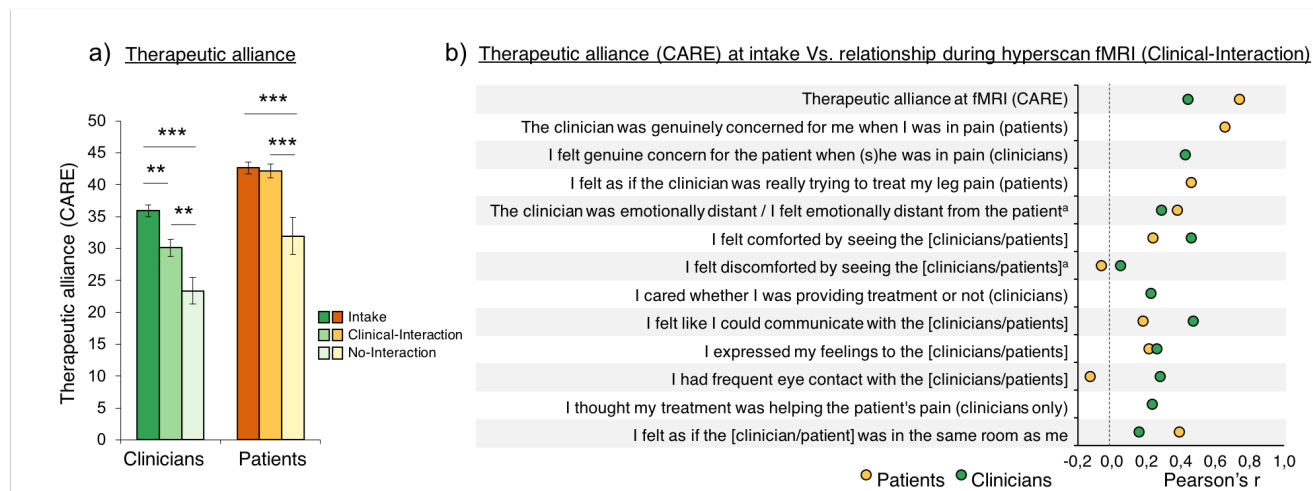
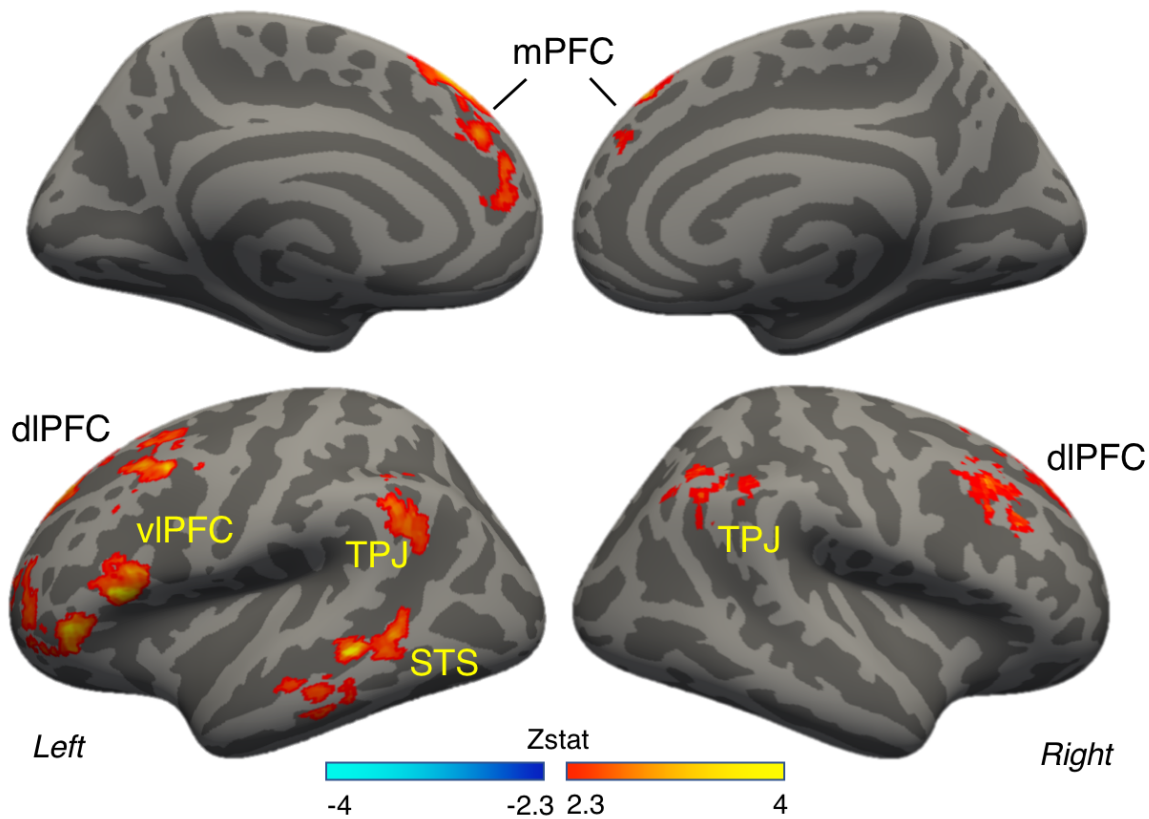


Fig. S1 | Self-reported patient-clinician therapeutic alliance (CARE) across sessions. a) Similarly to patients (see main Article), clinicians reported different levels of therapeutic alliance (CARE scores) depending of the context of the dyadic clinical interaction ($F(1.82,25.42)=12.83$, $P<0.001$, $\eta^2=0.48$). Specifically, the No-interaction MRI context (mean±SD=23.56±7.94) was rated lower than both Intake (35.69±4.08, $t=5.95$, $P<0.001$, Cohen's $d=1.49$, 95% Confidence Interval [CI]=6.63,17.62) and Clinical-Interaction MRI (30.25±5.89, $t=2.84$, $P=0.01$, $d=0.71$, CI=0.34,13.03) contexts. Furthermore, therapeutic alliance at Intake was rated higher than at Clinical-Interaction MRI ($t=3.11$, $P=0.01$, $d=0.78$, CI=0.72,10.16). There was no significant effect of order for neither patient-rated CARE ($F(1.34,18,76)=1.07$, $P=0.34$, $\eta^2=0.07$) nor clinician-rated CARE ($F(1.82,25.42)$, $P=0.63$, $\eta^2=0.03$). b) An ANCOVA indicated that higher therapeutic alliance (CARE scores) at intake positively predicted evaluations of the relationship ('HRS score') at the subsequent Clinical-Interaction MRI, across a range of items related to the relationship and social interaction. This association was evident for both for the patient-rated ($F(1,144)=9.33$, $P=0.003$, $\eta^2=0.06$) and the clinician-rated ($F(1,160)=12.24$, $P<0.001$, $\eta^2=0.07$) scales, indicating the relationship and rapport established at the intake was successfully carried over to the Clinical-Interaction MRI, which was completed on a separate day. There were no main effects or statistical interactions involving 'HRS Item' for neither patients nor clinicians (P 's>0.39), suggesting the association between therapeutic alliance at

56 intake Vs relationship at MRI, as well as HRS scores overall, was not different depending on HRS items.
57 Error bars represent Standard error of the mean; ^aReversed score; CARE=Consultation And Relational
58 Empathy scale.

59

Pressure pain, Patients_{Treat-NoTreat}

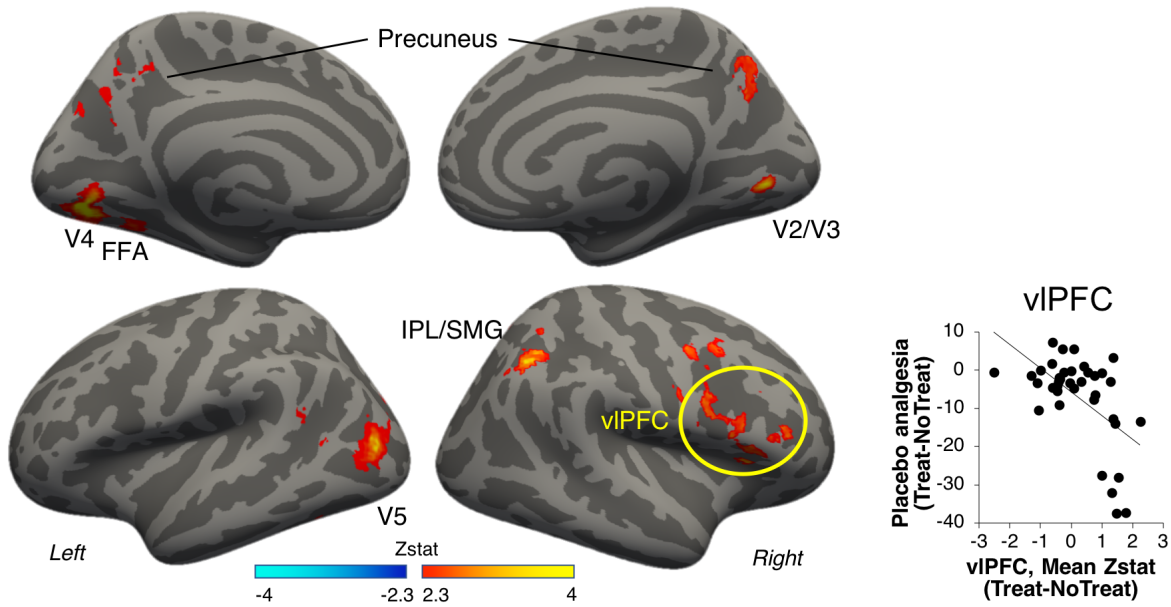


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61 **Fig. S2 | Group map displaying areas where patients showed significant treatment-related (Treat –**
62 **NoTreat) increase in brain response to pressure pain, thresholded at $Z=2.3$, $P=0.05$, cluster-corrected**
63 **for multiple comparisons.** A whole-brain GLM demonstrated increased fMRI activation of bilateral vlPFC,
64 TPJ, dlPFC, and mPFC, in addition to left STS for treated, relative to nontreated, pain. There were no
65 significant effects in the opposite direction (NoTreat – Treat). This is consistent with a recent meta-analysis
66 of experimental fMRI studies investigating placebo analgesia (17), showing that while placebo analgesia
67 was seen in all studies, there was only a marginal BOLD reduction of pain-processing circuitry (18).
68 mPFC=medial Prefrontal Cortex; dlPFC=dorsolateral Prefrontal Cortex; vlPFC=ventrolateral Prefrontal
69 Cortex; TPJ=Temporoparietal Junction; STS=Superior Parietal Junction.

70

Correlation, Patients' Pain_{Treat-NoTreat} Vs placebo analgesia

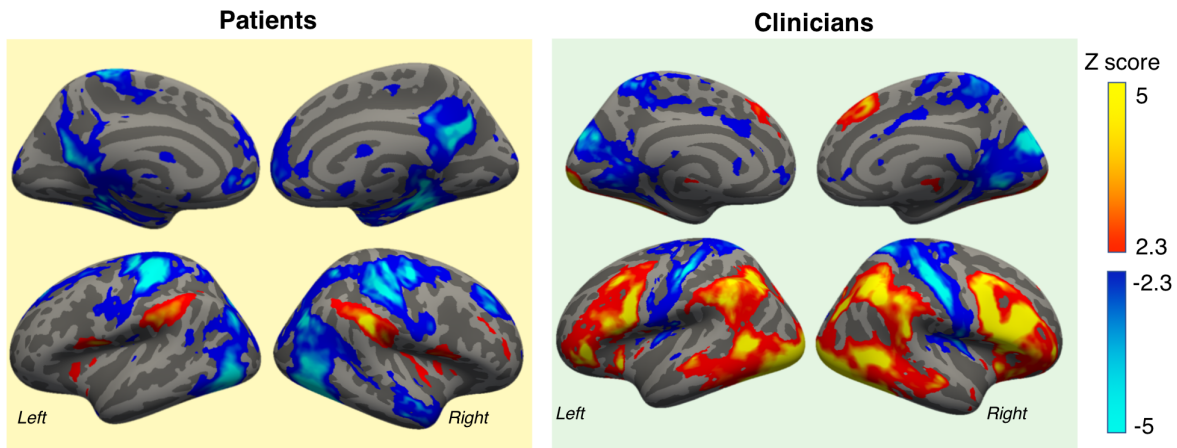


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72 **Fig. S3 | Group map showing areas where stronger treatment-related increases (Treat-NoTreat) in**
 73 **patients' brain response to pressure pain was significantly associated with stronger analgesia**
 74 **(NoTreat-Treat, pain ratings), as indicated by a whole-brain regression analysis.** The displayed group
 75 map was thresholded at $Z=2.3$, $P=0.05$, cluster-corrected for multiple comparisons. V2-5=Visual areas 1-5;
 76 FFA=Fusiform Face Area; IPL=Inferior Parietal Lobule; SMG=Supramarginal Gyrus; vIPFC=ventrolateral
 77 Prefrontal Cortex.

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Overall brain response to Pain / Vicarious pain (Treat, NoTreat)

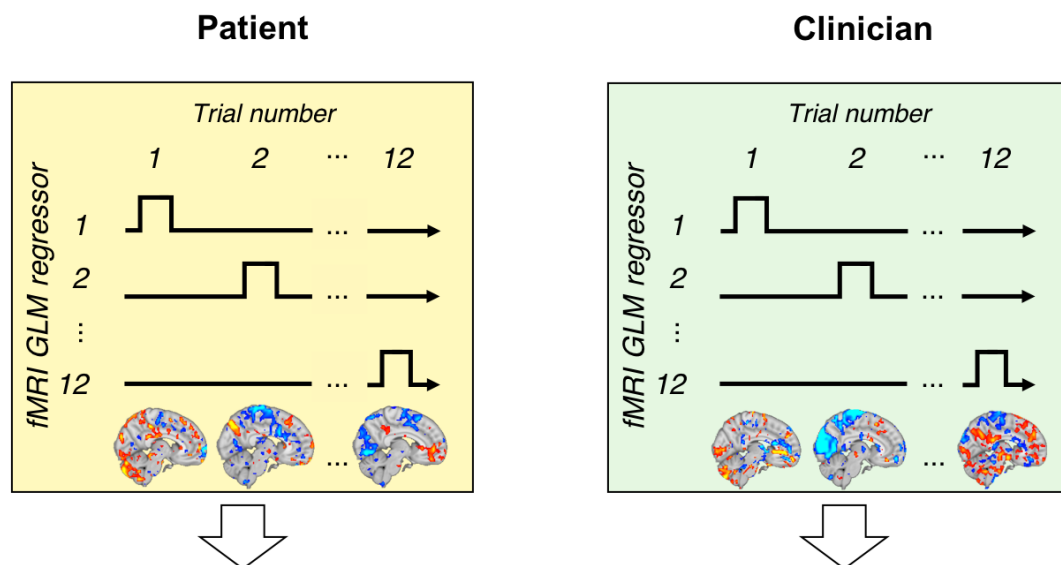


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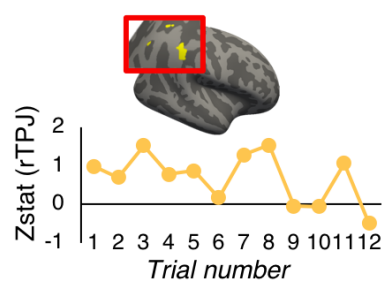
80 **Fig. S4 | Group maps showing overall response to pain (patients, left) and vicarious pain (clinicians,**
81 **right), collapsed over Treat/NoTreat conditions.** The displayed group maps were thresholded at $Z=2.3$,
82 $P=0.05$, cluster-corrected for multiple comparisons.

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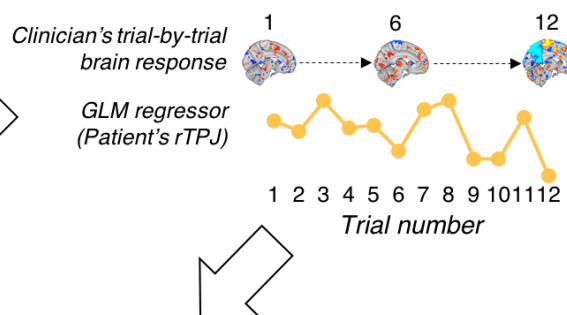
1. First-level GLM (Whole-brain), modeling each trial separately



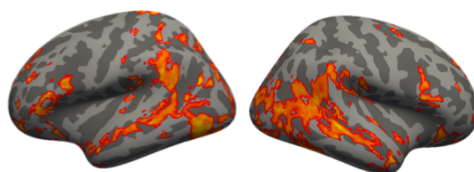
2. Patient ROI extraction (trial-by-trial)



3. Second-level regression for each dyad (fixed-effects GLM)



4. Dynamic concordance group map (for all dyads w/patients' rTPJ)



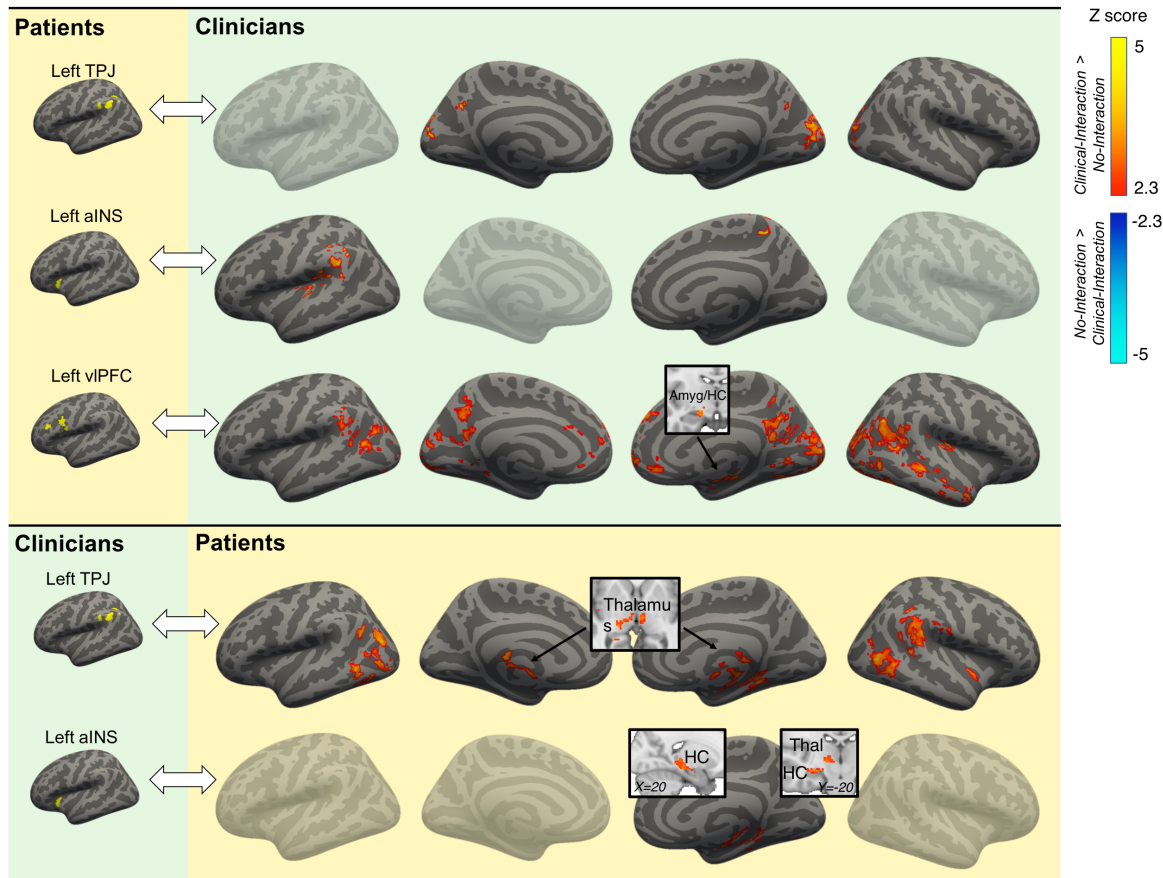
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85 **Fig. S5 | Dynamic concordance analysis pipeline.** 1. To investigate dynamic (time-varying) concordance
86 between patients and clinicians, we first performed a first-level GLM for each subject, where each trial
87 (anticipation phase) was modeled as a separate regressor. This resulted in 12 voxel-wise whole-brain maps
88 (one per trial). 2. For each trial, mean Zstat values were extracted from the patient's social mirroring ROIs
89 (e.g. rTPJ), as identified by a patient-clinician conjunction analysis (see Fig. a). 3. These ROI scores were
90 then used as a regressor in a second-level fixed-effects GLM for the clinician's trial-by-trial brain response

91 during anticipation, which produced a whole-brain map of regions where the clinician's brain response
92 showed dynamic (time-varying) concordance with the patient's social mirroring circuitry (e.g. rTPJ). 4.
93 These steps were taken for each individual dyad, and dynamic concordance maps across dyads were then
94 combined for group analyses. ROI=Region of Interest; rTPJ= right Temporoparietal Junction.

95

**Dynamic concordance with alternative nodes of the social mirroring circuitry
(Clinical-Interaction – No-Interaction group contrast)**



97

98 **Fig. S6 | Dynamic concordance with alternative nodes of the social mirroring circuitry.** Each row shows
 99 a group contrast (Clinical-Interaction – No-Interaction) of dynamic concordance with different social
 00 mirroring ROIs from the partner, as identified by the patient-clinician conjunction group analysis. The top 3
 01 rows show clinician whole-brain concordance with patients' social mirroring ROIs. Patients' left TPJ
 02 showed increased concordance with clinicians' precuneus and medial visual cortex for Clinical-Interaction
 03 relative to No-Interaction. For the same contrast, patients' left aINS showed increased concordance with
 04 clinicians' left TPJ, left posterior insula, and right S1. Left vIPFC showed increased concordance with
 05 clinicians' left TPJ, right amygdala/hippocampus, bilateral STS, right mid/posterior insula,
 06 vmPFC/pregenual ACC (pgACC), dmPFC, lateral/medial visual cortex, and precuneus. The bottom 2 rows
 07 show patient whole-brain concordance with clinicians' social mirroring ROIs. Clinicians' left TPJ showed
 08 increased concordance with patients' right TPJ, right aINS, right STS, lateral visual cortex, and bilateral

09 thalamus for Clinical-Interaction relative to No-Interaction. Left aINS showed increased concordance with
10 the right HC and the right thalamus. None of these contrasts showed significant differences in the opposite
11 direction (No-Interaction – Clinical-Interaction). No other nodes of the social mirroring circuitry showed
12 differences in concordance between Clinical-Interaction and No-Interaction. The displayed group maps were
13 thresholded at $Z=2.3$, $P=0.05$, cluster-corrected for multiple comparisons. There were no significant effects
14 in the opposite direction (No-Interaction – Clinical-Interaction). TPJ=Temporoparietal Junction;
15 aINS=anterior Insula; vlPFC=ventrolateral Prefrontal Cortex; Amyg=Amygdala; HC=Hippocampus.

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