

1 **The virucidal effects of 405 nm visible light on SARS-CoV-2 and influenza A virus**

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15

16 **Abstract**

17 Germicidal potential of specific wavelengths within the electromagnetic spectrum is an
18 area of growing interest. While ultra-violet (UV) based technologies have shown
19 satisfactory virucidal potential, the photo-toxicity in humans coupled with UV associated
20 polymer degradation limit its use in occupied spaces. Alternatively, longer wavelengths
21 with less irradiation energy such as visible light (405 nm) have largely been explored in
22 the context of bactericidal and fungicidal applications. Such studies indicated that 405
23 nm mediated inactivation is caused by the absorbance of porphyrins within the
24 organism creating reactive oxygen species which result in free radical damage to its
25 DNA and disruption of cellular functions. The virucidal potential of visible-light based
26 technologies has been largely unexplored and speculated to be ineffective given the
27 lack of porphyrins in viruses. The current study demonstrated increased susceptibility of
28 lipid-enveloped respiratory pathogens of importance such as SARS-CoV-2 (causative
29 agent of COVID-19) as well as the influenza A virus to 405nm, visible light in the

30 absence of exogenous photosensitizers indicating a potential porphyrin-independent
31 alternative mechanism of visible light mediated viral inactivation. These results were
32 obtained using less than expected irradiance levels which are generally safe for humans
33 and commercially achievable. Our results support further exploration of the use of
34 visible light technology for the application of continuous decontamination in occupied
35 areas within hospitals and/or infectious disease laboratories, specifically for the
36 inactivation of respiratory pathogens such as SARS-CoV-2 and Influenza A.

37 **Key words – Visible light, 405nm, Virucidal, SARS-CoV-2, Influenza, inactivation**

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53 **Introduction**

54 The severe-acute respiratory syndrome corona virus 2 (SARS-CoV-2), the causative
55 agent of the COVID-19 pandemic, is a member of the beta-coronavirus family and it
56 emerged at the end of 2019 in the Hubei province in Wuhan China¹. By late February
57 2021, more than 112 million cases had been reported while accounting for
58 approximately 2.5 million deaths, underscoring the rapid dissemination of the virus on a
59 global scale². As a complement to standard precautions such as handwashing,
60 masking, surface disinfection, and social distancing, other enhancements to enclosed
61 spaces such as improved ventilation and whole-room disinfection are being considered
62 by segments beyond acute healthcare such as retail, dining, and transportation³.

63 Initial guidance from health authorities such as the CDC and WHO on environmental
64 transmission focused on contaminated surfaces as fomites⁴. Data pertaining to the
65 survival of SARS-CoV-2 and other related coronaviruses to date has indicated that
66 virions are able to persist on fomites composed of plastic⁵, wood⁶, paper⁵, metal⁷ and
67 glass⁸ potentially up to nine days. Recent studies have suggested that SARS-CoV-2
68 may also remain viable approximately at least three days in such surfaces and another
69 two studies showed that at room temperature (20-25°C), a 14-day time-period was
70 required to see a 4.5-5 Log₁₀ of the virus^{9, 10}.

71 Since the start of the pandemic, transmission of the virus by respiratory droplets and
72 aerosols has become an accepted method of transmission although the relative impact
73 of each mode of transmission is the subject of much debate. Nevertheless, enclosed
74 spaces with groups of people exercising or singing have been associated with

75 increased transmission. The half-life survival of SARS-CoV-2 in this type of environment
76 has been estimated between 1-2 hours^{6, 11, 12}.

77 Taking this information into consideration, several methods have been evaluated to
78 effectively inactivate SARS-CoV-2. Chemical methods, which focus on surface
79 disinfection, utilize 70% alcohol and bleach and their benefits are well established.
80 These methods are also episodic (or non-continuous) meaning that in-between
81 applications, the environment is not being treated¹³.

82 In addition to chemicals, one of the most utilized methods for whole-room disinfection is
83 germicidal ultra-violet C (UVC; ~254 nm)¹⁴. This technology is well established¹⁵ and
84 has been shown to inactivate a range of pathogens including bacteria¹⁶, fungi¹⁷ and
85 viruses¹⁸. The mechanism of action of UVC is photodimerization of genetic material
86 such as RNA (relevant for SARS-CoV2 and IAV) and DNA (relevant for DNA viruses
87 and bacterial pathogens, among others)¹⁹. Unfortunately, this effect has been
88 associated with deleterious effects in exposed humans such as photokeratoconjunctivitis
89 in eyes and photodermatitis in skin²⁰. For these reasons, UVC irradiation requires safety
90 precautions and cannot be used to decontaminate fomites and high contact areas in the
91 presence of humans²¹.

92 Germicidal properties of violet-blue visible light (380-500 nm), especially within the
93 range of 405 to 450 nm wavelengths have been appreciated as an alternative to UVC
94 irradiation in whole-room disinfection scenarios where it has shown reduction of
95 bacteria^{22, 23} in occupied rooms and reductions in surgical site infections²⁴. Although 405
96 nm or closely related wavelengths have been shown to be less germicidal than UVC, its
97 inactivation potential has been assessed in pathogenic bacteria such as *Listeria* spp

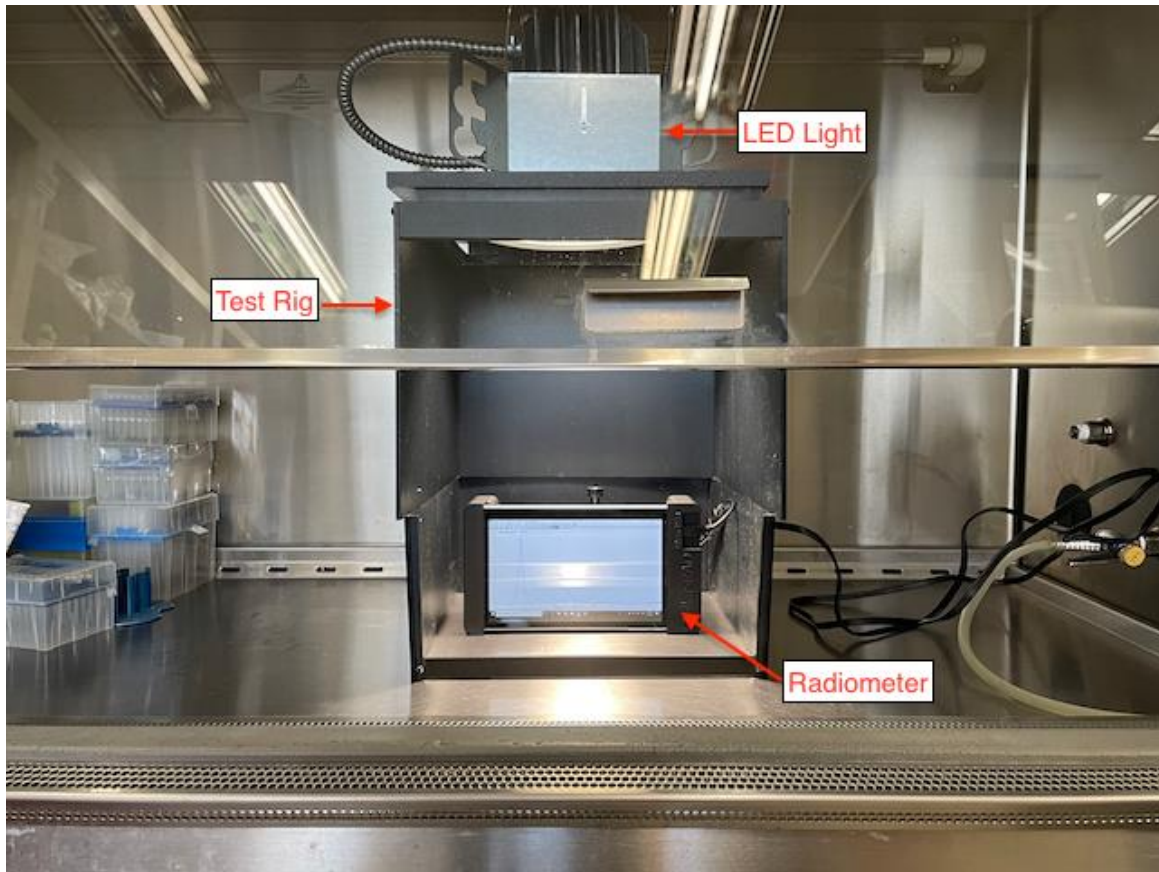
98 and *Clostridium* spp^{24, 25}, and in fungal species such as *Saccharomyces* spp and
99 *Candida* spp²⁶ . It is thought that the underlying mechanism of blue-light mediated
100 inactivation is associated with absorption of light via photosensitizers such as
101 porphyrins which results in the release of reactive oxygen species (ROS) ^{27, 28}. The
102 emergence of ROS is associated with direct damage to biomolecules such as proteins,
103 lipids and nucleic acids which are essential constituents of bacteria, fungi and viruses.
104 Further studies have shown that ROS can also lead to the loss of cell membrane
105 permeability mediated by lipid oxidation²⁹. Given the lack of endogenous
106 photosensitizers such as porphyrins in virions, efficient decontamination of viruses (both
107 enveloped and non-enveloped) may require the addition of exogenous
108 photosensitizers²³. With the use of media suspensions containing both endogenous
109 and/or exogenous photosensitizers, inactivation of viruses such as feline calicivirus
110 (FCV)³⁰, viral hemorrhagic septicemia virus (VHSV)³¹ and murine norovirus-1³² has
111 demonstrated the virucidal potency of 405 nm visible light using porphyrin rich media
112 such as saliva, blood, etc. (to create the ROS required for inactivation) using unsafe,
113 commercially impractical irradiance levels. This highlights the importance of answering
114 the basic scientific questions related to viral inactivation within the context of the applied
115 science required for clinical application. Our study specifically focused on three
116 questions: 1) does the same wavelength of light (405nm) that inactivates bacteria also
117 inactivate enveloped viruses, 2) is a porphyrin rich medium required for this inactivation,
118 and 3) can this inactivation be achieved using safe, commercially practical irradiance
119 levels?

120 In the current study, we show the impact of 405 nm irradiation on inactivation of SARS-
121 CoV-2 and influenza A H1N1 viruses without the use of photosensitizers making it
122 directly relevant to the clinical environment. We show this using a commercially
123 available visible light disinfection system ensuring that the irradiance used is both safe
124 and practically achievable in a clinical setting supporting the possible use of 405 nm
125 irradiation as a tool to confer continuous decontamination of respiratory pathogens such
126 as SARS-CoV-2 and influenza A viruses. We further show the increased susceptibility
127 of lipid-enveloped viruses for irradiation in comparison to non-enveloped viruses, further
128 characterizing the virucidal effects of visible light.

129 **Materials and methods.**

130 **405 nm Exposure System**

131 The visible light disinfection product used in this study was a commercially available 6”
132 LED downlight (Indigo-Clean, Kenall, Kenosha, WI) to allow for use within a BSL-3 level
133 containment hood. Within the hood, the distance between the face of the fixture and the
134 sample was 10”- much less than the normal 1.5 m used in normal, whole-room
135 disinfection applications. The output of the fixture was modified electronically during its
136 manufacture to match this difference and ensure that the measurements would
137 represent the performance of the device in actual use. This test setup is shown in a
138 BSL-2 hood in Figure 1 below. Note the spectroradiometer and the bottom portion of the
139 rig (~6”) used for calibration were removed during the actual study.



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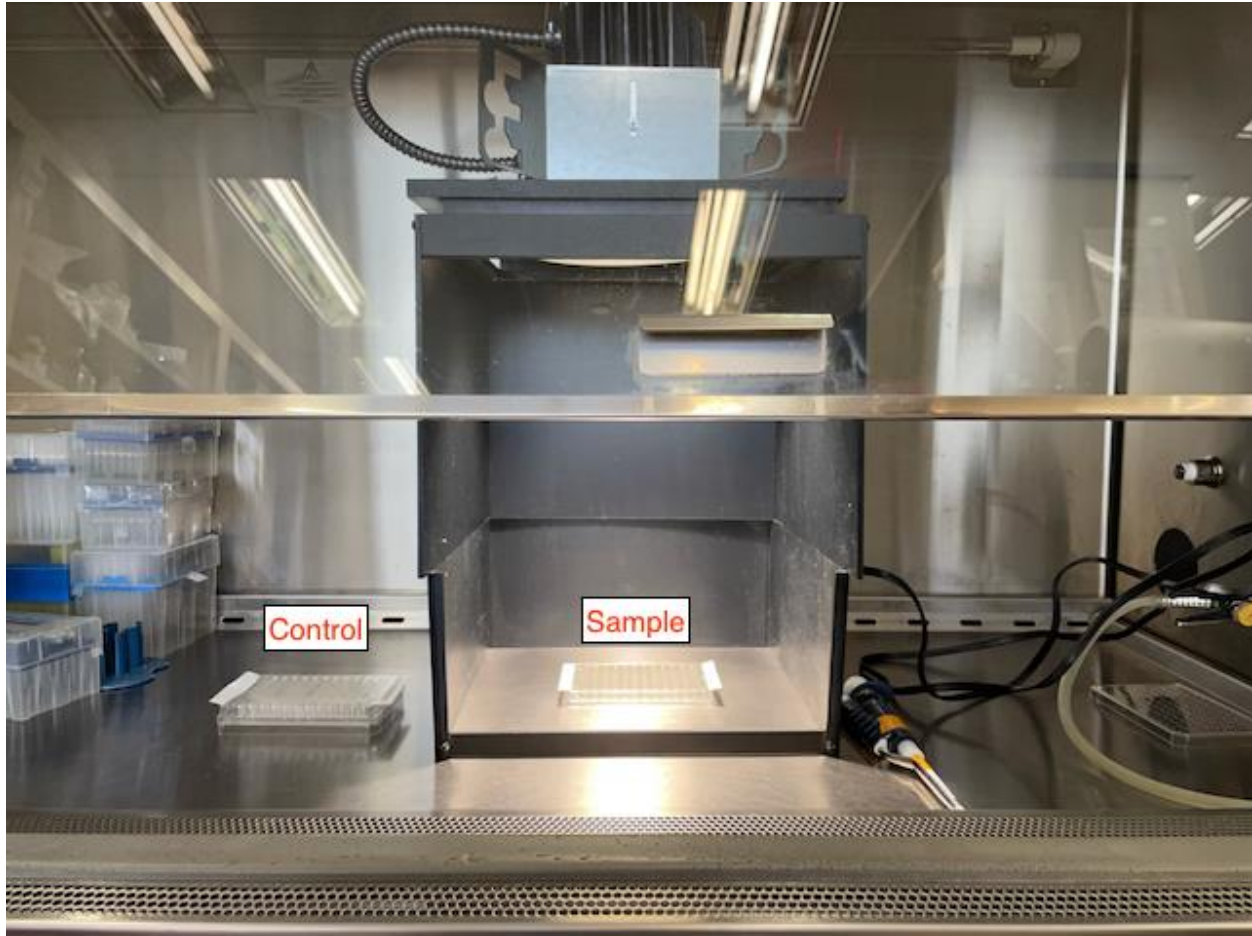
141 **Figure 1. Test setup shown with spectroradiometer and extension used for**
142 **calibration.**

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144 Controls were placed outside the test rig but within the BSL hood as shown in Figure 2.

145 Note that this picture contains the bottom portion of the test rig to highlight the position
146 of the radiometer

147



148

149 **Figure 2. Test setup showing the placement of the control and sample for**
150 **irradiation. Note that the bottom portion of the test rig was removed during the**
151 **actual experiment. This ensures the 10” distance used in the study.**

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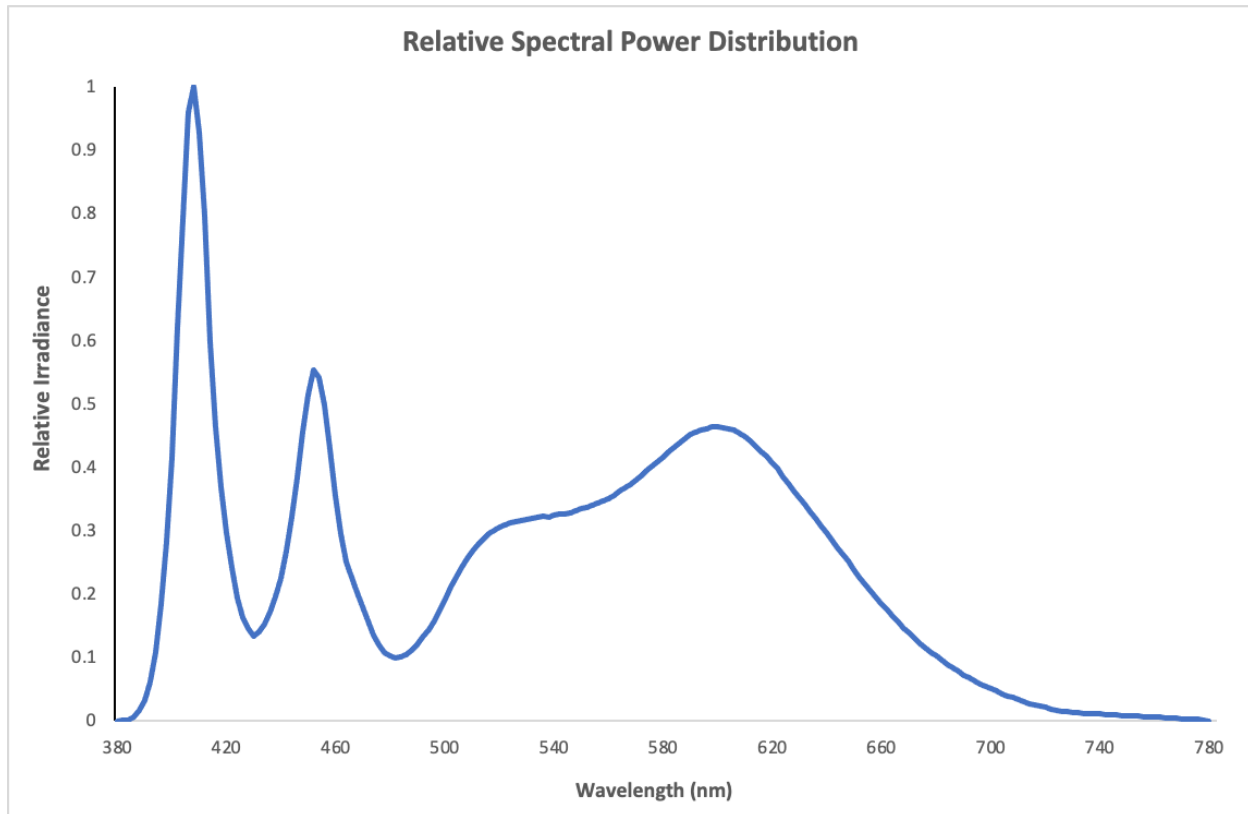
153 For the range of output used in this study, multiple discrete levels were created using
154 pulse width modulation within the LED driver itself. These levels were made to be
155 individually selectable using a simple knob on the attached control module.

156 As expected, the amount of visible light within the 400nm-420nm bandwidth, measured
157 in mWcm^{-2} , is a measurement of the “dose” delivered to the target organism and is used
158 to quantify this relationship similar to that used in UV disinfection applications.

159 To fully examine this effect, a range of irradiance values were used representing actual
160 product deployment conditions in occupied rooms. The lowest value (0.035 mWcm^{-2})
161 represents a single-mode, lower wattage used in general lighting applications while the
162 highest value (0.6 mWcm^{-2}) represents a dual-mode, higher wattage used in critical care
163 applications such as an operating room.

164 The device was placed in a rig to ensure a consistent distance (10") between the fixture
165 and the samples. The output of the fixture in the test rig was measured using a Stellar-
166 RAD Radiometer from StellarNet configured to make wavelength and irradiance
167 measurements from 350nm-1100nm with $< 1\text{nm}$ spectral bandwidth using a NIST
168 traceable calibration. To ensure that the regular white light portion of the illumination
169 (which is non-disinfecting) was not measured, the measurement was electronically
170 limited to a 1nm bandwidth over the 400nm-420nm range. The normalized spectral
171 profile is shown in Fig. 3 below. The absolute value of the measurement was
172 determined using a NIST traceable calibration as previously described.

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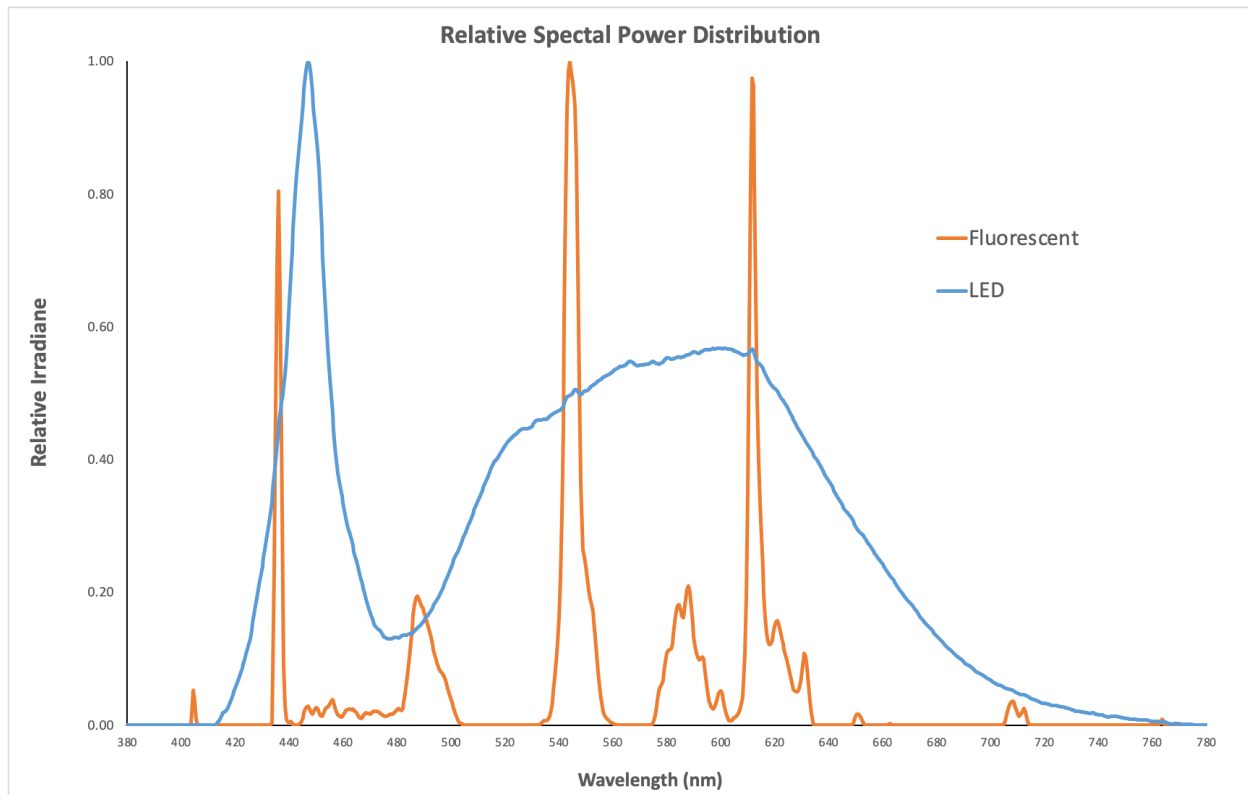
175 **Figure 3. Normalized spectral power distribution showing peak irradiance at**
176 **405nm.**

177 Samples were irradiated with the range of wavelengths depicted in Figure 3. This was
178 deliberately done for two reasons: 1) prior work had shown that visible light disinfection
179 was primarily active at 405nm³³ and 2) to emphasize the applied science associated
180 with actual clinical use where a virus in the environment could be exposed to both
181 405nm and regular white light in an occupied room.

182 To isolate the contribution of 405nm light, the control samples were placed outside the
183 field of irradiation created by the disinfection product but within the biosafety hood.
184 Accordingly, these samples were exposed to the overhead lights within the room which
185 contained virtually no 405nm light (< 0.001 mWcm⁻²).

186 In any assessment of viral inactivation, thermal denaturing of the organism is a concern.
187 Older lighting technologies such as incandescent sources heat a resistive element and
188 were widely used in a variety of applications. This creates heat at both the source and
189 to objects within its field. Fortunately, the disinfecting light (sample) and the overhead
190 lights in the room (control) did not use this technology and therefore contain no infrared
191 emissions ($> 800 \text{ nm}$) a commonly known benefit associated with LED lighting. As a
192 confirmation, the temperature beneath the disinfecting light was measured using a
193 commercially available thermocouple during a 24-hour period. During this time, the
194 temperature at the sample position was constant at $20^{\circ}\text{C} \pm 0.5^{\circ}\text{C}$. even at the highest
195 disinfecting power (0.6 mWcm^{-2}).

196
197 For reference, two spectral profiles, one for traditional fluorescent lighting and the other
198 for standard LED lighting are provided in Figure 4 below. While both types of lighting
199 are commonly used in the overhead lights within buildings, the lights in the BSL-3
200 laboratory were traditional fluorescent. As shown in Figure 2, the controls were
201 exposed only to traditional fluorescent lighting with a negligible amount of disinfecting
202 light ($< 0.001 \text{ mWcm}^{-2}$) between 400nm and 420nm . Due to the inherent differences
203 between fluorescent and LED lighting, the standard LED spectra has a small, but
204 measurable amount of disinfecting light (0.006 mWcm^{-2}) between 400nm and 420nm .
205 As will be later shown, this amount of light can have a measurable disinfecting effect.



206

207 **Figure 4. Normalized spectral power distribution for the fluorescent control light**
208 **(non-disinfecting) and standard LED light (without 405nm) used in the study.**

209 **Each spectrum is normalized relative to its own peak value.**

210

211 **Cells and viruses**

212 Vero-E6 cells (ATCC® CRL-1586™, clone E6) were maintained in Dulbecco's Modified
213 Eagle Medium (DMEM) complemented with 10% heat-inactivated Fetal Bovine Serum
214 (HI-FBS; PEAK serum), penicillin-streptomycin (Gibco; 15140-122), HEPES buffer
215 (Gibco; 15630-080) and MEM non-essential amino-acids (Gibco; 25025CL) at 37°C with
216 5% CO₂. Vero-CCL81 (ATCC® CRL-81™) cells and MDCK cells (ATCC® CCL-34)
217 were cultured in DMEM supplemented with 10% HI-FBS and penicillin/streptomycin at -
218 37°C with 5% CO₂. All experiments involving SARS-CoV2 (USA-WA1/202, BEI

219 resource – NR52281) were conducted within a biosafety-level 3 (BSL3) containment
220 facility at Icahn school of medicine at Mount Sinai by trained workers upon authorization
221 of protocols by a biosafety committee. Amplification of SARS-CoV-2 viral stocks was
222 done in Vero-E6 cell confluent monolayers by using an infection medium composed of
223 DMEM supplemented with 2% HI-FBS, Non-essential amino acids (NEAA), HEPES and
224 penicillin-streptomycin at 37°C with 5% CO₂ for 72 hours. Influenza A virus used here
225 was generated using plasmid based reverse genetics system as previously described³⁴.
226 The backbone used in the study was A/Puerto Rico/8/34/Mount Sinai(H1N1) under the
227 GenBank accession number AF389122. IAV-PR8 virus was grown and titrated in MDCK
228 as previously described³⁴. As a non-enveloped virus, the cell culture adapted murine
229 Encephalomyocarditis virus (EMCV; ATCC® VR-12B) was propagated and titrated in
230 Vero-CCL81 cells with DMEM and 2% HI-FBS and penicillin-streptomycin at 37°C with
231 5% CO₂ for 48 hours³⁵.

232 **405nm inactivation of viruses**

233 The SARS-CoV-2 virus was exclusively handled at the Icahn school of Medicine BSL-3
234 and studies involving IAV and EMCV were handled in BSL-2 conditions. Indicated PFU
235 amounts were mixed with sterile 1X PBS and were irradiated in 96 well format cell
236 culture plates in triplicates. In these studies, A starting dose of 5x10⁵ PFU for SARS-
237 CoV-2 and starting doses of 1x10⁵ PFU for IAV and EMCV were used. The final
238 volumes for inactivation were 250 µl per replicate. The untreated samples were
239 prepared the same way and were left inside the biosafety cabinet isolated from the
240 inactivation device at room temperature. The plates were sealed with qPCR plate
241 transparent seal and an approximate 10% reduction of the intensity was observed due

242 to the sealing film. The distance from the lamp and the samples was measured to be
243 10". All samples were extracted at indicated times and were frozen at -80°C and were
244 thawed together for titration via plaque assays.

245 **Plaque assays**

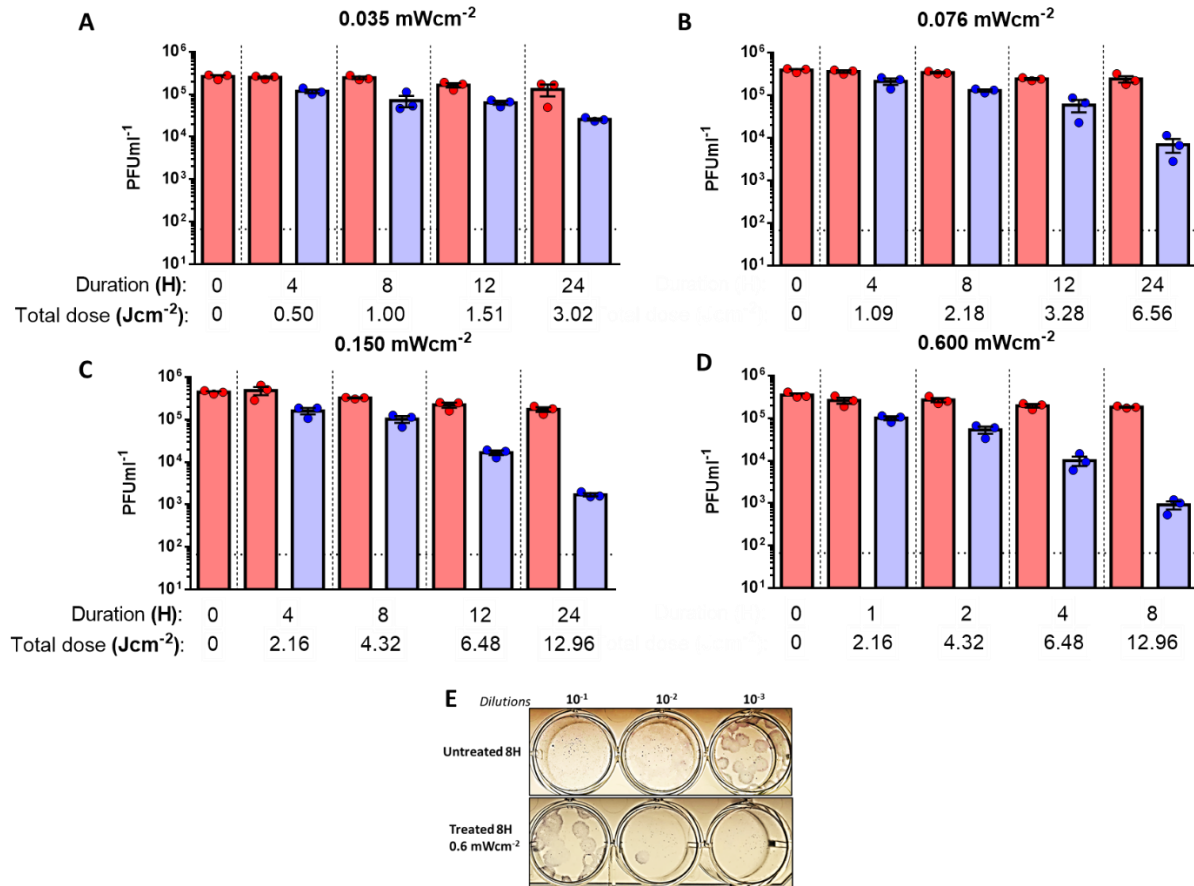
246 For SARS-CoV-2 studies, confluent monolayers of Vero-E6 cells in 12-well plate format
247 were infected (with an inoculum volume 150µl) with 10-fold serially diluted samples in
248 1X phosphate-buffered saline (PBS) supplemented with bovine serum albumin (BSA)
249 and penicillin-streptomycin for an hour while gently shaking the plates every 15 minutes.
250 Afterwards, the inoculum was removed, and the cells were incubated with an overlay
251 composed of MEM with 2% FBS and 0.05% Oxoid agar for 72 hours at 37°C with 5%
252 CO₂. The plates were subsequently fixed using 10% formaldehyde overnight and the
253 formaldehyde was removed along with the overlay. Fixed monolayers were blocked with
254 5% milk in Tris-buffered saline with 0.1% tween-20 (TBS-T) for an hour. Afterwards,
255 plates were immunostained using a monoclonal antibody against SARS-CoV2
256 nucleoprotein (Creative-Biolabs; NP1C7C7) at a dilution of 1:1000 followed by 1:5000
257 anti-mouse IgG monoclonal antibody and was developed using KPL TrueBlue
258 peroxidase substrate for 10 minutes (Seracare; 5510-0030). After washing the plates
259 with distilled water, the number of a plaques were counted. Plaque assays for IAV and
260 EMCV were done in a similar fashion. For IAV, confluent monolayers of MDCK cells
261 supplemented with MEM-based overlay with TPCK-treated trypsin was used and was
262 incubated for 48 hours at 37°C with 5% CO₂. For EMCV, Vero-CCL81 cells were used
263 to do plaque assays in 6 well plate format with an inoculum volume of 200µl and was
264 incubated for 48 hours at 37°C with 5% CO₂. Plaques for IAV and EMCV were

265 visualized using crystal violet. Data shown here is derived from three independent
266 experimental setups.

267 **Results.**

268 **Dose and time dependent inactivation of SARS-CoV-2 in the absence of** 269 **photosensitizers.**

270 The lowest irradiation dose of 0.035 mWcm^{-2} was applied for SARS-CoV-2 and when
271 compared to the T_{4H} untreated control, a reduction of $0.3288 \log_{10}$ was seen as early as
272 4 hours and after 24 hours of irradiation, an inactivation of $1.0325 \log_{10}$ (approximately
273 10 times reduction in infectivity) was observed for SARS-CoV-2 via plaque assays
274 (Figure 5A). A slightly higher dose of 0.076 mWcm^{-2} yielded $0.4123 \log_{10}$, $0.6118 \log_{10}$
275 and $1.5393 \log_{10}$ reduction by 4, 8 and 12 hours post irradiation when compared to the
276 respective untreated controls (Figure 5B). Subsequent increase of the irradiation dose
277 to 0.150 mWcm^{-2} resulted in a reduction of $0.4771 \log_{10}$ after 4 hours which then had a
278 $1.1206 \log_{10}$ after 12 hours. Irradiation for 24 hours at 0.150 mWcm^{-2} suggested a total
279 reduction of $2.0056 \log_{10}$ (256 times) for SARS-CoV-2 and (Figure 5C). As a final
280 experiment, a high irradiation dose of 0.6 mWcm^{-2} was used to assess the inactivation
281 potential within a much shorter time frame. Irradiation for one hour resulted in a
282 reduction of $0.4150 \log_{10}$ which reached $1.2943 \log_{10}$ reduction by four hours and 2.309
283 \log_{10} (385 times) after 8 hours in comparison to untreated controls samples at the
284 corresponding times. (Figure 5 D and E). All experimental conditions demonstrated the
285 stability of untreated SARS-CoV-2 which was left at room temperature in PBS, as
286 shown by the marginal reduction of viral titer over time.



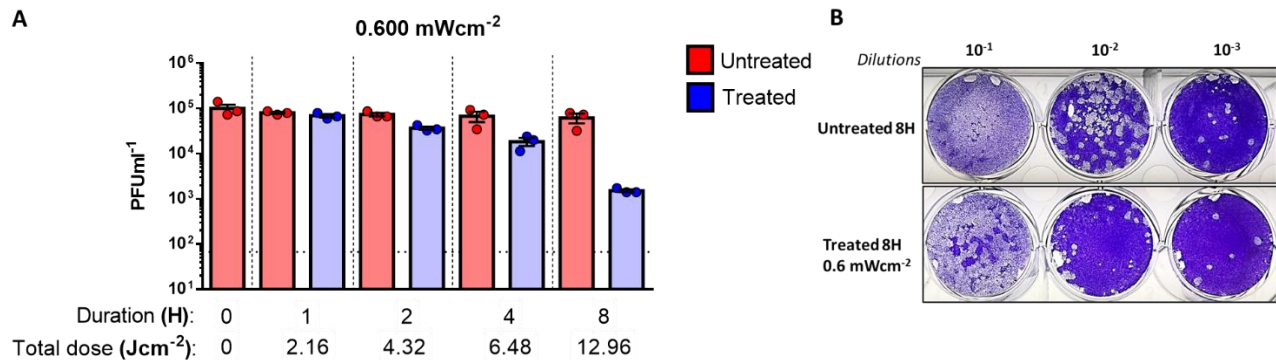
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288 **Figure 5. Dose and time dependent inactivation of SARS-CoV-2 virus in PBS by 405 nm irradiation.** A. A dose of 0.035
 289 mWcm⁻² or B. a dose of 0.076 mWcm⁻² or C. a dose of 0.150 mWcm⁻² or D. a dose of 0.6 mWcm⁻² was applied to irradiate samples
 290 at 405 nm over a course of 24 while sampling at 4, 8, 12 and 24 hours (for A, B and C) or over a course of 8 hours while sampling at
 291 1, 2, 4 and 8 hours (D) was done in independent triplicates. Blue bars indicate treated samples and red bars correspond to the
 292 untreated equivalent that was left at the biosafety cabinet under the same conditions while not subjecting to disinfecting irradiation.
 293 Data shown as PFU ml⁻¹ in triplicate assessed by plaque assay. E. Plaque phenotype comparison from one independent experiment
 294 at an irradiation dose of 0.6 mWcm⁻². Fixed and blocked plaques were immunostained using anti-SARS-CoV-2/NP antibody before
 295 developing using TrueBlue reagent. Data show in here are from three independent replicates (Mean+SEM).

296 **Influenza A virus is susceptible to 405 nm inactivation in the absence of**
 297 **photosensitizers.**

298 Given the observations derived from SARS-CoV-2, a separate inactivation study using a
 299 different lipid-enveloped RNA virus was conducted by using influenza A Puerto Rico
 300 (A/H1N1/PR8-Mount Sinai) virus strain. Irradiation with a high dose of 0.6 mWcm⁻²

301 suggested a time dependent reduction of infectious titers as calculated by the 0.1619
302 \log_{10} , 0.5609 \log_{10} , and 1.6115 \log_{10} (66 times) reductions at 1, 2, 4 and 8 hours
303 respectively (Figure 6A). And the reduction of plaques was apparent (figure 6B).

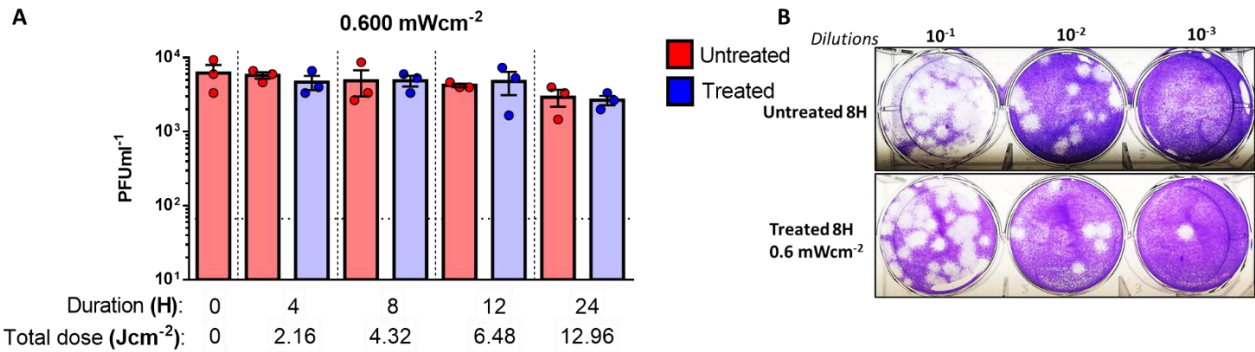


304
305 **Figure 6 Inactivation of Influenza A virus in PBS by 405 nm irradiation.** A. A dose of 0.6 mWcm⁻² was applied to irradiate
306 samples at 405 nm over a course 8 hours while sampling at 1, 2, 4 and 8 hours (done in independent triplicates). Blue bars indicate
307 treated samples and red bars correspond to the untreated equivalent that was left at the biosafety cabinet under the same
308 conditions while not subjected to disinfecting irradiation. Data shown as PFUml⁻¹ in triplicate assessed by plaque assay. B. Plaque
309 phenotype comparison from one independent experiment at an irradiation dose of 0.6 mWcm⁻². Fixed and blocked plaques were
310 stained using crystal violet. Data show in here are from three independent replicates (Mean+SEM).

311 The stability of IAV virus at room temperature for a period of 8 hours was found to be
312 the negligible in untreated IAV spiked PBS samples (Figure 6A).

313 **Encephalomyocarditis virus (EMCV) as a model non-enveloped virus indicates**
314 **reduced susceptibility to 405 nm inactivation in the absence of photosensitizers.**

315 In order to better understand the effect of the lipid-envelope in viral inactivation by 405
316 nm irradiation, we used a non-lipid enveloped RNA virus derived from the
317 *Picornaviridae* family. EMCV virus was irradiated at a high dose of 0.6 mWcm⁻² similar
318 to SARS-CoV-2 and IAV.



319

320 **Figure 7. Encephalomyocarditis virus (EMCV) in PBS shows reduced susceptibility to 405 nm irradiation. A.** A dose of 0.6
321 mWcm⁻² was applied to irradiate samples at 405 nm over a course 8 hours while sampling at 1, 2, 4 and 8 hours (done in
322 independent triplicates). Blue bars indicate treated samples and red bars correspond to the untreated equivalent that was left at the
323 biosafety cabinet under the same conditions while not subjected to disinfecting irradiation. Data shown as PFUml⁻¹ in triplicate
324 assessed by plaque assay. **B.** Plaque phenotype comparison from one independent experiment at an irradiation dose of 0.6 mWcm⁻².
325 Fixed and blocked plaques were stained using crystal violet. Data show in here are from three independent replicates
326 (Mean+SEM).

327 In this case however, a total reduction of 0.0969 (approximately 2 times) in comparison
328 to the untreated after 8 hours of irradiation was observed (Fig 7A and 7B) indicating a
329 lower rate of inactivation (despite identical dosing) in contrast to the lipid-enveloped
330 RNA viruses tested in this study. The plaque reduction at 8 hours did not indicate the
331 same dramatic reduction as observed with the latter studies.

332 As shown in Figure 4, standard LED lighting (without the specific addition of 405nm
333 light) has a small but measurable amount of disinfecting light (0.006 mWcm⁻²) in the
334 400nm to 420nm range. To quantify the disinfecting effect of this light, irradiations were
335 performed for 4h, 8h, 12h, and 24 h. A reduction was observed. {Raveen to add
336 detail}. These results at 24h were largely consistent with other irradiation levels and
337 reinforce the general observation of a 405nm dose-dependent effect. The intermediate
338 irradiation levels (4h, 8h, and 12h) were generally larger than expected even when
339 accounting for experimental uncertainty.

340

341 **Discussion**

342 The ongoing SARS-CoV-2 pandemic has affected the day-to-day functions in the entire
343 world, raising concerns not only with regards to therapeutics but also in the context of
344 virus survivorship and decontamination³⁶. Taking into consideration the rapid spread of
345 SARS-CoV-2 from person to person by droplets, aerosols, and fomites, whole-room
346 disinfection systems can be viewed as a supplement to best practices for interrupting
347 transmission of the virus.

348 Given the ongoing COVID-19 pandemic, we wanted to explore the impact of 405 nm
349 enriched visible light technology on inactivation of respiratory pathogens such as SARS-
350 CoV-2 and influenza A virus.

351 Without the use of exogenous photosensitizers, we were able to show that irradiation
352 with low intensity (0.035 mWcm^{-2}) visible light yielded a reduction of $\log_{10} 0.3288$
353 inactivation after four hours (0.5 Jcm^{-2}) and a total $\log_{10} 1.0325$ inactivation of SARS-
354 CoV-2 after 24 hours (3.02 Jcm^{-2}). A slightly higher dose (0.076 mWcm^{-2}) resulted in
355 $\log_{10} 1.5393$ reduction after 24 hours (6.56 Jcm^{-2}) while an irradiation dose of 0.150
356 mWcm^{-2} showed a reduction $\log_{10} 2.0056$ after 24 hours (12.96 Jcm^{-2}) of irradiation.
357 Finally, increasing the dose to 0.6 mWcm^{-2} yielded $\log_{10} 2.3010$ reduction only after
358 eight hours (12.96 Jcm^{-2}), indicating a both time and dose dependent inactivation of
359 infectious viruses.

360 **The irradiations using standard LED lighting raise some interesting questions for further**
361 **discussion. With nearly 6x the amount of disinfecting light as compared to traditional**
362 **fluorescent lighting but 1/6th the lowest amount of 405nm used in the study; it is**
363 **conceivable that a reduction could be observed. The magnitude of this effect at less**

364 than 24h was larger than expected based on other irradiations performed in this study.
365 A similar effect was observed by Bache, et. al {REF} in whole-room bacterial reduction
366 studies. They saw a disinfecting effect for irradiance values as low as 0.023 mWcm⁻².
367 This effect was shown to be uncorrelated to the level of irradiance used suggesting that
368 the mere abundance of 405nm light can initiate the oxidizing chemical reaction.
369 Nevertheless, our results clearly show a dose-dependent effect. One possible
370 explanation for this observation is that the lower irradiance levels expose different
371 responses by specific organisms within a population based on the individual biology of
372 that organism. Clearly, these results suggest that additional factors may be at work and
373 warrant further investigation.

374 We selected conventional plaque assays as the read out to specifically estimate
375 infectious virus titers upon disinfection. Methods based in the quantification of viral RNA
376 via PCR based techniques might be misleading as they detect viral RNA from both
377 infectious and noninfectious virions.

378 SARS-CoV-2 is a lipid-enveloped virus composed of a ssRNA genome and our data
379 indicates its susceptibility to visible light mediated inactivation. To further confirm these
380 observations, we used influenza A virus. which is another human respiratory virus with a
381 lipid envelop and an segmented-RNA genome. Upon irradiating for 1 hour at 0.6
382 mWcm⁻² (2.16 Jcm⁻²), we observed a total reduction of log₁₀ 0.1619 for the influenza A
383 virus compared to the reduction of log₁₀ 0.4150 for SARS-CoV-2 under the same
384 conditions. While both viruses have lipid envelopes, there is clearly a difference here
385 that will require further study. One possible explanation is the difference in the virion
386 size creating a physically smaller cross-section for absorption. (IAV ~120 nm and

387 SARS-CoV-2 ~200 nm)^{37, 38}. Nevertheless, both viruses were largely inactivated after
388 eight hours achieving more 1.5 log₁₀ reduction. Intriguingly, it was observed that both
389 RNA viruses were able to remain stable at room temperature for at least 24 hours,
390 indicating minimal decay which is consistent with previous studies^{36, 39}. We next
391 irradiated a non-enveloped RNA virus, EMCV. Previous results for visible light against
392 non-enveloped viruses demonstrated the need for external photosensitizers such as
393 artificial saliva, blood, feces, etc^{30, 36}. Without a porphyrin containing medium, we
394 expected little to no inactivation when this virus was irradiated with visible light. For
395 these measurements, we used the highest available irradiance of 0.6 mWcm⁻². As
396 anticipated, we observed only a log₁₀ 0.0969 reduction after eight hours, however, this
397 appears to be with the statistical precision of the measurement based on the results
398 obtained from shorter irradiations (1, 2, and 4 hours). For comparison, a study involving
399 the M13-bacteriophage virus (a non-enveloped virus) showed a 3-Log reduction using
400 an irradiance of 50mWcm⁻² (almost 100 times greater than the highest irradiance used
401 in this study) for 10 hours at 425 nm further supporting the idea that non-enveloped
402 viruses may require higher doses of visible light⁴⁰.

403 Our study was conducted using a neutral liquid media composed of PBS without any
404 photosensitizers and we were able to show that visible light can indeed inactivate lipid-
405 enveloped viruses, differing from the theory that states that photosensitizers are a
406 requirement for inactivation. While these results provide insight into the basic science
407 involved, they were performed within the context of the applied science needed to show
408 the potential impact of this technology upon the current COVID-19 pandemic. By using

409 safe, commercially practical irradiance levels, our results are more directly translatable
410 to occupied rooms in the clinical environment.

411 Other studies which used visible light-based irradiation have shown similar results in the
412 absence of photosensitizers, indicating the possibility of an alternative inactivation
413 mechanism^{23, 25, 30}. Studies have proposed two theories for this observation primarily
414 due to non-405nm wavelengths emitted by the source: 1) some amount of 420-430 nm
415 emitted from the source is contributing to the viral inactivation ⁴¹, and 2) the presence of
416 UV-A (390 nm) within the source. This wavelength is known to create oxidative stress
417 upon viral capsids⁴².

418 Longer wavelengths, such as 420-430nm, have shown inactivation of the murine
419 leukemia virus (MRV-A) ⁴¹. While this is an intriguing study, it used a broad-spectrum
420 lamp with optical filters to selectively identify the spectrum primarily responsible with
421 their results. Unfortunately, they did not quantify the amount of light (using radiometric
422 units) within the spectrum of interest used to irradiate the virus. While transmission
423 profile of the filters used were provided, it does not consider the spectral composition of
424 the source itself making any direct quantitative comparison between our studies
425 impossible. It is interesting to note that they did observe viral inactivation in their
426 controls from wavelengths less than 420nm confirming the qualitative findings of our
427 study without confirming the specific use of 405nm. This suggests that the viral
428 inactivation is a likely a broad response (> 20nm) with relative contributions unique to
429 the chemistry of each organism. They also considered much longer exposures (~7
430 days) and much higher illuminance (> 200 lux) than that used in our study although this
431 is again difficult to compare given the lack of radiometric quantification of their light

432 source. It is important to note that the control samples used in our study were exposed
433 to the same overhead (non-405nm) lights as the irradiated samples and our results are
434 the observed difference between the two demonstrating the contribution from 405nm
435 over and above that potentially from 420-430nm. Future experiments can further
436 quantify the potential effect.

437 The other theory, potential UV-A irradiation, was historically applied to lamp-based
438 sources with broad spectral (> 100nm) outputs. Again, the use of LED technology
439 addresses this question as the peak irradiance at 390nm of the device used in this
440 study was < 1% of its peak irradiance at 405nm without the need for any additional
441 filtration. Future experiments can further quantify the potential effect.

442 Another consideration to be addressed is thermal heating of the virus by the LED
443 source. Tsen and Achilefu used a pulsed laser method at 425nm⁴³ with ~100 mWcm⁻²
444 average power density for < 2h while simultaneously measuring the sample temperature
445 with a thermocouple. They detected less than a 2°C demonstrating minimal temperature
446 impact even under a power density nearly 9 orders of magnitude larger than that used
447 in this study. This was confirmed by our thermocouple measurements as stated earlier.
448 Nazari, *et al* used an 805nm source with an average power density of > 0.3 Wcm⁻² for
449 10s, nearly 1000 times that used in this study⁴⁴. While the total energy delivered was
450 more comparable to that used in our study, they did not make explicit temperature
451 measurements, their analysis ruled out any potential thermal effects.

452 One possible explanation for the observed differences between the enveloped and non-
453 enveloped organisms is absorption of the 405nm light by the lipid envelope itself. This
454 could, in turn, lead to the creation of reactive oxygen species (causing an oxidative

455 effect) or simply destruction of the envelope leading to a denaturing of the organism.

456 This question could serve as the basis for a range of future studies.

457 The results obtained suggest that the performance of visible light against SARS-CoV-2

458 is similar to other organisms commonly found in the environment such as *S. aureus*.

459 Previous studies have shown that the visible light irradiance levels used in this study

460 (0.035 mWcm^{-2} to 0.6 mWcm^{-2}) reduce bacteria levels in occupied rooms and improve

461 outcomes for surgical procedures. It is therefore reasonable to conclude that visible light

462 might be an effective disinfectant against SARS-CoV-2. More importantly, this

463 disinfection can operate continuously as it is safe for humans based upon the exposure

464 guidelines in IEC 62471⁴⁵. This means that once it has been in use for a period of time,

465 the environment will be cleaner and safer the next time it is occupied by humans.

466 One limitation of this study is that the inactivation assays were performed in static liquid

467 media as opposed to aerosolized droplets. While the use of visible light in air

468 disinfection has been briefly studied where it was shown that its effectiveness increased

469 approximately 4-fold⁴⁶, further studies involving dynamic aerosolization are needed to

470 better understand the true potential of visible light mediated viral inactivation.

471 In any case, our study shows the increased susceptibility of enveloped respiratory viral

472 pathogens to 405 nm mediated inactivation in the absence of photosensitizers. The

473 irradiances used in this study are very low and might be easily applied to disinfect

474 occupied areas safely and continuously within hospitals, schools, restaurants, offices

475 and other locations. Of particular interest is the potential for standard LED lighting to

476 play a role in reducing the presence of SARS-CoV-2 in the environment.

477 **Conclusions**

478 We have demonstrated the basic science of inactivation of enveloped viruses such as
479 SARS-CoV-2 and Influenza-A using 405nm visible light within the context of the applied
480 science required for this technology to have an impact upon the current COVID-19
481 pandemic. Without the need for exogenous photosensitizers and by using safe,
482 commercially practical irradiance levels, our results can be easily translated to the
483 clinical environment.

484 **Future Efforts**

485 Future work should focus on explaining the difference between the enveloped and non-
486 enveloped results. This may include transmission electron microscopy (TEM),
487 hemagglutination assay (HA), or other methods focusing on the potential role that a
488 mediated reaction (due to the envelope itself) might play. The size of the virion particle
489 may play a role in photoelectric absorption and could be studied for different viral
490 species. We acknowledge that while unlikely, other wavelengths of visible light, beyond
491 400-420nm may play a role in the inactivation process and future studies should explore
492 this possibility as well. Finally, the inactivation kinetics of low irradiances could add
493 valuable insight into clinical applications of this technology.

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503 **Conflicts of interest**

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507 agreements for the following companies involving cash and/or stock: Vivaldi
508 Biosciences, Pagoda, Contrafect, 7Hills Pharma, Avimex, Vaxalto, Accurius, Pfizer and
509 Esperovax. RR, CY and AGS have filed for a provisional patent based upon these
510 results.

511 **References**

- 512 1. Andersen, K. G., Rambaut, A., Lipkin, W. I., Holmes, E. C. & Garry, R. F. The
513 proximal origin of SARS-CoV-2. *Nat. Med.* **26**, 450-452 (2020).
- 514 2. Worldometer, D. COVID-19 coronavirus pandemic. *World Health Organization*,
515 www.worldometers.info (2020).
- 516 3. Buitrago-Garcia, D. *et al.* Occurrence and transmission potential of asymptomatic and
517 presymptomatic SARS-CoV-2 infections: A living systematic review and meta-analysis.
518 *PLoS medicine* **17**, e1003346 (2020).
- 519 4. [https://www.who.int/news-room/commentaries/detail/modes-of-transmission-of-virus-
520 causing-covid-19-implications-for-ipc-precaution-recommendations](https://www.who.int/news-room/commentaries/detail/modes-of-transmission-of-virus-causing-covid-19-implications-for-ipc-precaution-recommendations).
- 521 5. Dehbandi, R. & Zazouli, M. A. Stability of SARS-CoV-2 in different environmental
522 conditions. *The Lancet Microbe* **1**, e145 (2020).
- 523 6. Van Doremalen, N. *et al.* Aerosol and surface stability of SARS-CoV-2 as compared
524 with SARS-CoV-1. *N. Engl. J. Med.* **382**, 1564-1567 (2020).
- 525 7. Behzadinasab, S., Chin, A., Hosseini, M., Poon, L. & Ducker, W. A. A surface coating
526 that rapidly inactivates SARS-CoV-2. *ACS applied materials & interfaces* **12**, 34723-
527 34727 (2020).

- 528 8. Chan, K. *et al.* Factors affecting stability and infectivity of SARS-CoV-2. *J. Hosp.*
529 *Infect.* **106**, 226-231 (2020).
- 530 9. Biryukov, J. *et al.* Increasing Temperature and Relative Humidity Accelerates
531 Inactivation of SARS-CoV-2 on Surfaces. *mSphere* **5**, 10.1128/mSphere.00441-20
532 (2020).
- 533 10. Aboubakr, H. A., Sharafeldin, T. A. & Goyal, S. M. Stability of SARS-CoV-2 and
534 other coronaviruses in the environment and on common touch surfaces and the
535 influence of climatic conditions: A review. *Transboundary and emerging diseases*
536 (2020).
- 537 11. Smither, S. J., Eastaugh, L. S., Findlay, J. S. & Lever, M. S. Experimental aerosol
538 survival of SARS-CoV-2 in artificial saliva and tissue culture media at medium and high
539 humidity. *Emerging microbes & infections* **9**, 1415-1417 (2020).
- 540 12. Schuit, M. *et al.* Airborne SARS-CoV-2 is rapidly inactivated by simulated sunlight.
541 *J. Infect. Dis.* **222**, 564-571 (2020).
- 542 13. Kampf, G., Todt, D., Pfaender, S. & Steinmann, E. Persistence of coronaviruses on
543 inanimate surfaces and their inactivation with biocidal agents. *J. Hosp. Infect.* **104**, 246-
544 251 (2020).
- 545 14. Rutala, W. A. & Weber, D. J. Disinfection and sterilization in health care facilities:
546 what clinicians need to know. *Clinical infectious diseases* **39**, 702-709 (2004).
- 547 15. Rathnasinghe, R. *et al.* Scalable, effective, and rapid decontamination of SARS-
548 CoV-2 contaminated N95 respirators using germicidal ultra-violet C (UVC) irradiation
549 device. *medRxiv* (2020).
- 550 16. Escombe, A. R. *et al.* Upper-room ultraviolet light and negative air ionization to
551 prevent tuberculosis transmission. *PLoS Med* **6**, e1000043 (2009).
- 552 17. Nakpan, W., Yermakov, M., Indugula, R., Reponen, T. & Grinshpun, S. A.
553 Inactivation of bacterial and fungal spores by UV irradiation and gaseous iodine
554 treatment applied to air handling filters. *Sci. Total Environ.* **671**, 59-65 (2019).
- 555 18. Tseng, C. & Li, C. Inactivation of viruses on surfaces by ultraviolet germicidal
556 irradiation. *Journal of occupational and environmental hygiene* **4**, 400-405 (2007).
- 557 19. Kowalski, W. in *Ultraviolet germicidal irradiation handbook: UVGI for air and surface*
558 *disinfection* (Springer science & business media, 2010).
- 559 20. Zaffina, S. *et al.* Accidental exposure to UV radiation produced by germicidal lamp:
560 case report and risk assessment. *Photochem. Photobiol.* **88**, 1001-1004 (2012).

- 561 21. Leung, K. C. P. & Ko, T. C. S. Improper Use of the Germicidal Range Ultraviolet
562 Lamp for Household Disinfection Leading to Phototoxicity in COVID-19 Suspects.
563 *Cornea* **40**, 121-122 (2021).
- 564 22. Maclean, M. *et al.* Environmental decontamination of a hospital isolation room using
565 high-intensity narrow-spectrum light. *J. Hosp. Infect.* **76**, 247-251 (2010).
- 566 23. Maclean, M., McKenzie, K., Anderson, J. G., Gettinby, G. & MacGregor, S. J. 405
567 nm light technology for the inactivation of pathogens and its potential role for
568 environmental disinfection and infection control. *J. Hosp. Infect.* **88**, 1-11 (2014).
- 569 24. Murrell, L. J., Hamilton, E. K., Johnson, H. B. & Spencer, M. Influence of a visible-
570 light continuous environmental disinfection system on microbial contamination and
571 surgical site infections in an orthopedic operating room. *Am. J. Infect. Control* **47**, 804-
572 810 (2019).
- 573 25. Maclean, M., Murdoch, L. E., MacGregor, S. J. & Anderson, J. G. Sporicidal effects
574 of high-intensity 405 nm visible light on endospore-forming bacteria. *Photochem.*
575 *Photobiol.* **89**, 120-126 (2013).
- 576 26. Murdoch, L., McKenzie, K., Maclean, M., Macgregor, S. & Anderson, J. Lethal
577 effects of high-intensity violet 405-nm light on *Saccharomyces cerevisiae*, *Candida*
578 *albicans*, and on dormant and germinating spores of *Aspergillus niger*. *Fungal Biology*
579 **117**, 519-527 (2013).
- 580 27. Dai, T. *et al.* Blue light for infectious diseases: *Propionibacterium acnes*,
581 *Helicobacter pylori*, and beyond? *Drug Resistance Updates* **15**, 223-236 (2012).
- 582 28. Bumah, V. V. *et al.* Spectrally resolved infrared microscopy and chemometric tools
583 to reveal the interaction between blue light (470 nm) and methicillin-resistant
584 *Staphylococcus aureus*. *Journal of Photochemistry and Photobiology B: Biology* **167**,
585 150-157 (2017).
- 586 29. Hadi, J., Dunowska, M., Wu, S. & Brightwell, G. Control Measures for SARS-CoV-2:
587 A Review on Light-Based Inactivation of Single-Stranded RNA Viruses. *Pathogens* **9**,
588 737 (2020).
- 589 30. Tomb, R. M. *et al.* New proof-of-concept in viral inactivation: virucidal efficacy of 405
590 nm light against feline calicivirus as a model for norovirus decontamination. *Food and*
591 *environmental virology* **9**, 159-167 (2017).
- 592 31. Ho, D. T. *et al.* Effect of blue light emitting diode on viral hemorrhagic septicemia in
593 olive flounder (*Paralichthys olivaceus*). *Aquaculture* **521**, 735019 (2020).

- 594 32. Wu, J. *et al.* Virucidal efficacy of treatment with photodynamically activated
595 curcumin on murine norovirus bio-accumulated in oysters. *Photodiagnosis and*
596 *photodynamic therapy* **12**, 385-392 (2015).
- 597 33. Maclean, M., MacGregor, S. J., Anderson, J. G. & Woolsey, G. High-intensity
598 narrow-spectrum light inactivation and wavelength sensitivity of *Staphylococcus aureus*.
599 *FEMS Microbiol. Lett.* **285**, 227-232 (2008).
- 600 34. Martinez-Sobrido, L. & Garcia-Sastre, A. Generation of recombinant influenza virus
601 from plasmid DNA. *J. Vis. Exp.* **(42)**. pii: **2057**. doi, 10.3791/2057 (2010).
- 602 35. Carocci, M. & Bakkali-Kassimi, L. The encephalomyocarditis virus. *Virulence* **3**, 351-
603 367 (2012).
- 604 36. Derraik, J. G., Anderson, W. A., Connelly, E. A. & Anderson, Y. C. Rapid evidence
605 summary on SARS-CoV-2 survivorship and disinfection, and a reusable PPE protocol
606 using a double-hit process. *MedRxiv* (2020).
- 607 37. Bouvier, N. M. & Palese, P. The biology of influenza viruses. *Vaccine* **26**, D49-D53
608 (2008).
- 609 38. Bar-On, Y. M., Flamholz, A., Phillips, R. & Milo, R. Science Forum: SARS-CoV-2
610 (COVID-19) by the numbers. *Elife* **9**, e57309 (2020).
- 611 39. Wang, X., Zoueva, O., Zhao, J., Ye, Z. & Hewlett, I. Stability and infectivity of novel
612 pandemic influenza A (H1N1) virus in blood-derived matrices under different storage
613 conditions. *BMC infectious diseases* **11**, 1-6 (2011).
- 614 40. Tomb, R. M. *et al.* Inactivation of *Streptomyces* phage ϕ C31 by 405 nm light:
615 Requirement for exogenous photosensitizers? *Bacteriophage* **4**, e32129 (2014).
- 616 41. Richardson, T. B. & Porter, C. D. Inactivation of murine leukaemia virus by exposure
617 to visible light. *Virology* **341**, 321-329 (2005).
- 618 42. Girard, P. *et al.* *UVA-induced damage to DNA and proteins: direct versus indirect*
619 *photochemical processes* (Journal of Physics: Conference Series Ser. 261, IOP
620 Publishing, 2011).
- 621 43. Tsen, S. D. *et al.* Studies of inactivation mechanism of non-enveloped icosahedral
622 virus by a visible ultrashort pulsed laser. *Virology journal* **11**, 1-9 (2014).
- 623 44. Nazari, M. *et al.* Plasmonic enhancement of selective photonic virus inactivation.
624 *Scientific reports* **7**, 1-10 (2017).
- 625 45. IEC 62471: Photobiological safety of lamps and lamp systems. (2006).

626 46. Dougall, L. R., Anderson, J. G., Timoshkin, I. V., MacGregor, S. J. & Maclean, M.
627 *Efficacy of antimicrobial 405 nm blue-light for inactivation of airborne bacteria* (Light-
628 Based Diagnosis and Treatment of Infectious Diseases Ser. 10479, International
629 Society for Optics and Photonics, 2018).

630

631

632 Ref3 = Nazari M, Xi M, Lerch S, Alizadeh MH, Ettinger C, Akiyama H, Gillespie C,
633 Gummuluru S, Erramilli S, Reinhard BM, *Plasmonic Enhancement of Selective Photonic*
634 *Virus Inactivation*. Scientific Reports, **7**, 11951 (2017).

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637