

## ***Exogenous Sex Hormone Effects on Brain Microstructure in Women: A diffusion MRI Study in the UK Biobank***

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### ***Abstract***

Changes in estrogen levels in women have been associated with increased risk for age-related neurodegenerative diseases, including Alzheimer's disease, but the impact of exogenous estrogen exposure on the brain is poorly understood. Oral contraceptives (OC) and hormone therapy (HT) and are both common sources of exogenous estrogen for women in reproductive and postmenopausal years, respectively. Here we examined the association of exogenous sex hormone exposure with the brain's white matter (WM) aging trajectories in postmenopausal women using and not using OC and HT (HT users: n=3,033, non-users n=5,093; OC users: n=6,964; non-users n=1,156), while also investigating multiple dMRI models. Cross-sectional brain dMRI data was analyzed from the UK Biobank using conventional diffusion tensor imaging (DTI), the tensor distribution function (TDF), and neurite orientation dispersion and density imaging (NODDI). Mean skeletonized diffusivity measures were extracted across the whole brain, and fractional polynomial regressions were used to characterize age-related trajectories for WM microstructural measures. Advanced dMRI model NODDI revealed a steeper WM aging trajectory in HT users relative to non-users, and for those using unopposed estrogens relative to combined estrogens treatment. By contrast, no interaction was detected between OC status and age effects on the diffusivity measures we examined. Exogenous sex hormone exposure may negatively impact WM microstructure aging in postmenopausal women. We also present normative reference curves for white matter microarchitectural parameters in women, to help identify individuals with microstructural anomalies.

**Keywords:** Diffusion magnetic resonance imaging (dMRI), aging, sex hormones, hormone therapy, diffusion tensor imaging, fractional polynomials

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## INTRODUCTION

There are known sex differences in the risk for age-related neurodegenerative diseases such as Alzheimer's disease (AD) (see Salminen et al., 2022 for review). On average, women over the age of 40 are at a greater risk of developing AD than age-matched men, and endogenous and exogenous estrogen levels also influence this risk in women (Shumaker et al. 2003; Savolainen-Peltonen et al. 2019; Song et al. 2020). Sex, as well as age, affects many aspects of grey and white matter (WM) microstructure across the lifespan (Cox et al. 2016; Nir et al. 2017; Ritchie et al. 2018; Toschi et al. 2020; Lawrence et al. 2021). Additionally, AD incidence and the menopause transition have frequently been linked, especially when the transition is induced surgically, or occurs at a younger age (Costantino et al. 2022)

Despite this evidence, women's brain health is historically understudied (Covan 2005), and we know little about brain mechanisms underlying the reported sex differences in risk for degenerative diseases and how female-specific factors may influence women's brain health throughout life. Given the growing population of older adults and the high percentage of females taking exogenous sex hormones worldwide, this is a major gap in the literature that requires immediate attention (Boyle et al. 2020).

Population based observational studies, as opposed to clinical trials, offer the large sample size, diversity, and statistical power required to investigate factors that influence aging trajectories across the lifespan. The UK Biobank is currently the largest prospective study of aging, gathering extensive questionnaires, physical and cognitive measures, neuroimaging data and biological samples in a population-based cohort of middle- to older-aged adults living in the United Kingdom (UK). Such large-scale population-based studies can identify subtle effects that could go undetected in smaller samples. Factors that modulate aging processes could inform future clinical trials and clinical decisions and guide recommendations for women at risk for age-related neurodegenerative disorders.

Some prior neuroimaging studies report relationships between levels of endogenous sex hormones - such as estradiol - and developmental processes, lifespan trajectories of aging (Salminen et al. 2022) and brain plasticity (Boyle et al., 2020; Galea et al., 2014; Simerly, 2002). Several brain structural changes have been associated with estrogen fluctuations in pregnant women (Hoekzema et al. 2017) and in pre-menopausal women across the menstrual cycle (Barth et al., 2016). Beneficial effects of endogenous estrogen levels have been reported generally for gray matter, with larger brain volumes for women during the reproductive years (den Heijer et al. 2003; Lisofsky et al. 2015). Even so, negative effects of endogenous estrogen levels on brain regional volumes have been reported in menopausal women (Resnick et al. 2003).

While evidence suggests that estrogen exerts a neuroprotective effect in reproductive and pre-menopausal women and unfavorable effects post-menopause, whether post-menopausal *exogenous* estrogen exposure is beneficial or detrimental for cognition is still an open question and warrants further investigation. Hormone therapy (HT) is a common source of exogenous estrogen in women menopausal years. A large randomized, double-blind, placebo-controlled clinical trial (N=4,894, Women's Health Initiative Memory Study, WHIMS) of post-menopausal

women ( $\geq 65$  years) receiving estrogen plus progestin therapy reported for the first time that postmenopausal HT exposure may be detrimental for cognition (measured through 4 phases of neuropsychological and psychiatric assessments) and may increase their risk for probable dementia (Shumaker et al. 2003). A subsequent study using the WHIMS cohort reported greater brain atrophy in post-menopausal women treated with unopposed and conjugated estrogens (Resnick et al. 2003). Estrogen therapy is also called unopposed estrogen therapy because a second hormone (progestin) is not used along with the estrogen, whereas conjugated estrogen therapy includes a second hormone in addition to estrogen. A longitudinal study (Kantarci et al. 2016) reported increasing ventricular enlargement over 4 years in recently menopausal women (5-36 months past menopause) following conjugated estrogens. More recently, a large-scale UK Biobank population study of 16,854 middle to older-aged women (de Lange et al. 2020) reported that higher cumulative sex hormone exposure was associated with more adverse effects on the brain's gray matter (i.e., more advanced *brain age*, a biomarker for aging); no information on HT treatment type was reported. In APOE $\epsilon$ 4 carriers, conjugated estrogens were found to reduce amyloid- $\beta$  deposition (Kantarci et al. 2016), and higher levels of estradiol following HT were associated with less pronounced brain aging (de Lange et al. 2020); all relative to non-carriers. Other neuroimaging studies report a neuroprotective effect of unopposed estrogen treatment on WM (Ha et al. 2007).

The inconsistency of HT neuroimaging markers highlights the fact that there is still much to learn about the therapeutic potential of exogenous estrogen use. This variability and lack of consensus regarding HT effects on brain structure in women is a major gap in the literature. Large clinical trials suggest that the duration of HT and age of onset may be key factors in estrogen-mediated effects on the brain; the timing of the initiation of HT relative to menopause, age, or both, may relate to the health of the underlying vascular tissue and to other factors such as reduction in or down-regulation of estrogen receptors. Several clinical studies of HT exposure effects on the brain led to the critical period hypothesis, which states that HT may be neuroprotective if initiated near the time of cessation of ovarian function – that is, within around 5 years of menopause (MacLennan et al. 2006; Espeland et al. 2015). Consistent with the critical period hypothesis, in 65 women (63% receiving unopposed estrogen), Erickson and colleagues (2010) suggested that there is a limited window of opportunity for HT at the time of menopause, whereby shorter intervals between menopause and the initiation of treatment were associated with larger hippocampal volumes compared with longer intervals (Erickson et al. 2010). Other studies in favor of this hypothesis, such as KEEPS (a randomized double-blind placebo-controlled study; Gleason et al., 2015) indicated no adverse effects on measures of cognition in recently menopausal women, beneficial mood effects up to 4 years using conjugated estrogens, but not using estrogen only (oral 17 $\beta$ -estradiol). The ELITE study (randomized double-blind placebo-controlled study; Hodis et al., 2016) also indicated that women prescribed HT (oral 17 $\beta$ -estradiol) much later ( $>10$  years after menopause) may be at higher risk of AD, as opposed to commencing therapy within 6 years after menopause. Findings by Gleason et al., (2015) and Hodis et al., (2016) were perhaps mediated by women's cardiovascular risk profiles (Gleason et al. 2015; Hodis et al. 2016). In the UK Biobank genetic factors were also found to contribute to how timing of treatment

initiation influenced women's brain aging trajectories (de Lange et al. 2020); indicating beneficial effects of HT initiation before onset of menopause in APOE $\epsilon$ 4 carriers, relative to non-carriers. However, a study using the WHIMS data (conjugated estrogens; (Espeland et al. 2015) showed that conjugated therapy delivered near the time of menopause provided no detectable cognitive benefit or detriment.

Traditionally, research on steroid actions in the brain has focused mainly on postmenopausal HT and has rarely controlled for the use of hormonal oral contraception (OC). The effects of synthetic steroids contained OC on brain and cognitive abilities is understudied, despite the increasing use of OC globally (World Health Organization 2019). OC have been on the market for over 50 years and used by 100 million women (Christin-Maitre 2013; Pletzer and Kerschbaum 2014; Daniels and Abma 2019; World Health Organization 2019). Contemporary OC literature has focused mainly on comparing cognitive performance in users and non-users across the menstrual cycle of pre-menopausal women (Mordecai et al. 2008; Gogos 2013). Even so, these studies are inconclusive due to the small sample sizes considered. One study in postmenopausal women indicates that OC usage was not associated with more evident brain aging (de Lange et al. 2020).

There is a need for large-scale studies to expand on previous research and further evaluate sex-hormone factors specific to women in the context of aging on the brain. Here, for the first time, we set out to measure and model age-associated effects on WM microstructure to infer possible effects of exogenous sex hormones on the brains of postmenopausal women by using multiple diffusion MRI (dMRI) models.

Diffusion MRI is an *in vivo* imaging technique that allows quantitative investigation of microstructural differences in WM tracts by exploiting the Brownian motion of water molecules, and the dependency of this diffusion process on the cellular environment (Jones 2008). Late-life cognitive decline may be caused, in part, by microstructural deterioration in the brain's neural pathways. Processes such as neuronal and glial cell loss, impaired myelin production, and axonal demyelination, may impair information transfer efficiency in the brain's WM networks. The WM *disconnection theory* is largely supported by emerging data from dMRI studies of the brain, in both healthy and diseased subjects (Bennett and Madden 2014; Pievani et al. 2014; Lawrence et al. 2021). Thus, an accurate characterization of how and where the brain's WM microstructure changes with age is a vital goal in brain aging research.

Here, we aimed to address the gap in variability and lack of consensus regarding exogenous sex hormone effects on brain structure in women by examining the association of HT and OC exposure with the brain's white matter aging trajectories in postmenopausal women. We explored this association using different dMRI models and accounting for several clinical variables and confounding factors. Drawing on the existing literature on sex hormone effects on the brain, we hypothesized that sex hormone therapy would *negatively* impact women's WM aging. We followed up with exploratory analyses to evaluate differences in HT regimen type (unopposed or conjugated estrogens), as these were hypothesized to differentially impact WM aging trajectories in women based on previous literature (Gleason et al. 2015; Savolainen-Peltonen et al. 2019). Further analyses were carried out to evaluate how WM aging relates to the duration of therapy, age at therapy onset and age at menopause, in women. We analyzed single- and multi-shell dMRI

brain data from the UK Biobank (Miller et al. 2016a) and processed them using 3 increasingly complex dMRI models. We hypothesized that more sophisticated dMRI models that relate the signals from diffusion MRI to geometric models of tissue microstructure, as opposed to traditional tensor-based methods, will estimate more sensitively the microstructural complexity of aging WM trajectories in women using sex hormone therapy. Diffusion indices were extracted and averaged across a whole brain WM skeleton. We used fractional polynomial (FP) regression to characterize sex hormone effects on age-related trajectories for WM metrics. We also computed normalized centile curves to visualize WM aging trajectories for the major diffusivity metrics.

## **MATERIALS & METHODS**

### **Sample**

Our sample was drawn from the UK Biobank (Miller et al. 2016b) and included postmenopausal women aged 45-80 years old. We focused on the subsample of the overall UK Biobank that had neuroimaging data available for download at the time of writing. Exogenous sex hormone exposure in women was estimated from the HT and OC variables. Our primary analyses involved HT exposed women (N=3,033; **Table 1**), where age effects on WM measures were compared to those in women who never took HT (N=5,093). Subsequently, we investigated age effects on WM measures in OC users (N=6,964, **Table 2**), relative to those who never took OC (N=1,156). There was an overlap of N=748 women between HT and OC non-users; HT and OC models were run separately.

We note that hormone exposure and hormone treatment are not randomized across individuals, as would be the case in a randomized clinical trial; instead, the study is a naturalistic epidemiological study of a large population (for assumptions and limitations of this approach, see *Discussion*).

### **Analysis of Aging Trends**

We modeled the effect of age on diffusion metrics (described in **Table 3**) in HT and OC users using higher order polynomial (FP) regressions (Royston and Altman 1994; Sauerbrei et al. 2006). Specifically, we used the multivariate fractional polynomial (*mfp*) package implemented in R (R Core Team, 2016). The *mfp* package used a predefined set of power terms (-2, -1, -0.5, 0.5, 1, 2, 3) and the natural logarithm function, and up to two power combinations to identify the best fitting model. FP for age was written as  $\text{age}^{(p_{0.5}, p_1, \dots)}$  where  $p$  in age refers to regular powers, and  $\text{age}^{(o)}$  refers to  $\ln(\text{age})$ . Classic multiple regression models assume a linear relationship between the independent and dependent variables. However, age effects on the brain may be nonlinear; effects are the aggregate of a vast number of cellular processes, each with potentially different profiles of acceleration and decline. As the age effects are likely highly nonlinear, with a functional form that is not known *a priori*, fractional polynomials may offer a more adaptive modeling approach (Royston and Altman 1994). These have been used to chart age trajectories for volumetric and other structural measures by the ENIGMA Lifespan group (Dima et al. 2022; Frangou et al. 2022).

Main nuisance covariates included years of education, waist/hip ratio, population structure, measured using the first four genetic principal components, and the Townsend index. These covariates were also used in recent UK Biobank structural investigations (Lawrence et al. 2021; Salminen et al. 2022). In detail, educational attainment was assessed using a sociodemographic questionnaire in which participants reported their completed qualification level (UK education system). These results were generalized beyond the UK education system and converted to the corresponding number of years using ISCED harmonization guidelines (Goujon et al. 2016) and dichotomized into 'high school' versus 'college' ( $\geq 17$  years) education. Waist-to-hip ratio is a common index of central fat distribution (Gadekar et al. 2020) and used as a proxy of atherosclerotic burden in overweight individuals and postmenopausal women (Lee et al. 2015;

Scicali et al. 2018). Population structure was obtained from the UK Biobank's genetic ancestry analyses (Bycroft et al. 2017). The first four genetic principal components were regressed out to account for differences in ethnicity within the sample. Participants' socioeconomic status (SES) was measured using the Townsend Index (Townsend et al. 2012), a British measure of societal deprivation based on the postal code of each participant – this index has been often used as a proxy measure of SES (Smith et al. 2001). For any of the variables of interest, women who had missing data, responded 'do not know' or 'preferred not to answer' were excluded from each analysis.

Our primary hypotheses include a hormone by age interaction on advanced diffusivity metrics (ISOVF<sup>NODDI</sup>, OD<sup>NODDI</sup>, and ICVF<sup>NODDI</sup>). A previous investigation of age and sex effects on microstructure in the UK Biobank reported the highest effect sizes for advanced NODDI metrics in sex by age interactions on full white matter (Lawrence et al. 2021). False discovery rate (FDR) was used to account for multiple comparisons (corrected at  $p < .05$ ) (Benjamini and Hochberg 1995). Secondary hypotheses include age by treatment type interaction on the advanced diffusivity NODDI metrics and a steeper aging trajectory for women taking unopposed estrogen treatment relative to combination estrogen users; additionally, a significant association between duration of hormone use, age at therapy onset and age at menopause for women taking hormones.

*Post-hoc* exploratory investigations considered the effects of HT compound composition (combined vs unopposed estrogen treatment) on WM aging trajectories; data was available for only a subset of the UK Biobank participants in the sample (unopposed estrogen users,  $n=300$ ; combination users,  $n=98$ ).

Supplemental analyses included Spearman's correlations to investigate a potential association between significant dMRI measures and duration of HT and OC usage, age at which the participant began HT or OC therapy, and age at menopause in HT and OC users. For any significant association, these variables were additionally covaried for in our fractional polynomial analyses.

Furthermore, centile curves (Bethlehem et al. 2018; Nobis et al. 2019; Lv et al. 2020) for each diffusion metric with respect to age were calculated and plotted in R; kernel density plots, indicating the degree of data point overlap (and sampling density across the age range), are included in the plots.

### ***MRI processing***

For detailed descriptions of the UK Biobank data acquisition, neuroimaging protocol, and validation, see work by Miller (Miller et al. 2016b) and Alfaro-Almagro and colleagues (Alfaro-Almagro et al. 2018). In brief, dMR images were acquired at  $b=1000$  and  $2000$  s/mm<sup>2</sup> along with 50 non-coplanar diffusion directions per shell with 5  $b=0$  s/mm<sup>2</sup> (and 3  $b=0$  blip-reversed) using a standard ('monopolar') Stejskal-Tanner pulse sequence (voxel dimensions: (2 mm)<sup>3</sup> isotropic, field of view: 104x104x72 mm; gradient timings: small delta=21.4 ms, big delta=45.5 ms) for a total imaging time of 7 minutes. All images underwent pre-processing, involving noise correction (Veraart et al. 2016), Gibbs-ringing correction (Kellner et al. 2016), estimation of echo-planar imaging distortions, motion and eddy current and susceptibility distortion corrections (Andersson

and Sotiropoulos 2016), spatial smoothing (*fslmaths* in FSL) with Gaussian kernel (1 mm FWHM)<sup>3</sup> and diffusion metric estimation. Diffusion tensor (DTI) and Neurite Orientation Dispersion and Density Imaging (NODDI) diffusion maps (Zhang et al. 2012) were computed by UK Biobank, while the tensor distribution function (TDF) (Leow et al. 2009; Nir, Jahanshad, Villalon-Reina, Isaev, Zavaliangos-Petropulu, Zhan, Leow, Jack Jr, et al. 2017) was computed locally using code available at <https://git.ini.usc.edu/ibagari/TDF>. Diffusivity indices considered by this study are detailed below and summarized in **Table 3**. For more details on these methods, please refer to the *Supplemental Material*.

Diffusion tensor imaging (DTI) fitting was performed on the  $b=1000$  s/mm<sup>2</sup> shell (50 diffusion-encoding directions) using the DTI fitting (*DTIFIT*, FSL) tool to create maps of the following tensor-derived measures: fractional anisotropy ( $FA^{DTI}$ ), representing the degree of anisotropic diffusivity - often considered to be sensitive to the density of white matter fibers and the degree of directional coherence within a fiber bundle (Pierpaoli et al. 1996; Jones and Cercignani 2010). Other DTI indices included mean diffusivity ( $MD^{DTI}$ ), describing the molecular diffusion rate in a fiber bundle, radial diffusivity ( $RD^{DTI}$ ), reflecting diffusivity perpendicular to the axonal fibers (or the principal direction of diffusion), and axial diffusivity ( $AD^{DTI}$ ) describing the magnitude of diffusion parallel to fiber tracts.

Diffusion MRI data ( $b=1000$  s/mm<sup>2</sup>, 50 diffusion-encoding directions) was also used as input data to estimate the tensor distribution function (TDF) at each voxel in the (Leow et al. 2009; Nir, Jahanshad, Villalon-Reina, Isaev, Zavaliangos-Petropulu, Zhan, Leow, Jack Jr, et al. 2017). This approach extends multi-tensor models of diffusion to describe intravoxel fibers mathematically as a probabilistic collection of tensors, or, alternatively, a continuous mixture of Gaussian densities. The fitted TDF function was employed to create diffusion maps of FA, based on the mixture of tensors ( $FA^{TDF}$ ). This approach overcomes some known limitations of the single diffusion tensor model in regions of fiber mixing or crossing and has been shown in other datasets to boost effect sizes for associations with external variables of interest, such as age, Alzheimer's disease, or clinical measures of dementia severity (Nir, Jahanshad, Villalon-Reina, Isaev, Zavaliangos-Petropulu, Zhan, Leow, Jack Jr, et al. 2017; Villalon-Reina et al. 2018; Lawrence et al. 2021).

In addition to TDF and DTI models, the dMRI data (all shells) were input into Neurite Orientation Dispersion and Density Imaging (NODDI) (Zhang et al. 2012) biophysical models, using the AMICO (Accelerated Microstructure Imaging via Convex Optimization) tool (Daducci et al. 2015), to obtain the following voxel-wise microstructural parameters:  $ODI^{NODDI}$  (orientation dispersion index, a measure of within-voxel white matter tract disorganization),  $ICVF^{NODDI}$  (intracellular volume fraction, and index of white matter neurite density) and  $ISOVF^{NODDI}$  (isotropic or free water volume fraction). These metrics have been shown to be sensitive to aging effects in smaller samples than that analyzed here (Thomopoulos et al. 2020), including measures of brain amyloid burden measured with PET (Thomopoulos et al. 2021).

Voxel-wise statistical analysis of the images was performed using Tract-based Spatial Statistics (Smith et al. 2006) (TBSS; **Figure 1**) using the [ENIGMA-DTI processing pipeline](#), with the following steps:  $FA^{DTI}$  images were non linearly registered to a standard-space white matter skeleton, the ENIGMA  $FA^{DTI}$  white matter template, representing the center of all white matter FA



voxels in MNI space using ANTs symmetric image normalization (SyN) method (Avants et al. 2009). The resulting transformation was applied to the maps of each metric (TDF and NODDI). White matter metrics were projected onto the ENIGMA template skeleton based on the  $FA^{DTI}$  metric using FSL's TBSS. Average whole-brain measures of  $FA^{DTI}$ ,  $MD^{DTI}$ ,  $RD^{DTI}$ ,  $AD^{DTI}$ ,  $FA^{TDF}$ ,  $ODI^{NODDI}$ ,  $ISOVF^{NODDI}$ ,  $ICVF^{NODDI}$  were extracted for each participant. As part of the quality control processes, 2D images of the output from each processing step in the dMRI pipeline were visually reviewed. Careful visual checks were performed for individuals whose derived data were flagged as outliers. Prior to any group-level analysis, participants with low-quality data (such as gross visual artifacts) were eliminated. A total of N=114 subjects were excluded from our analyses.

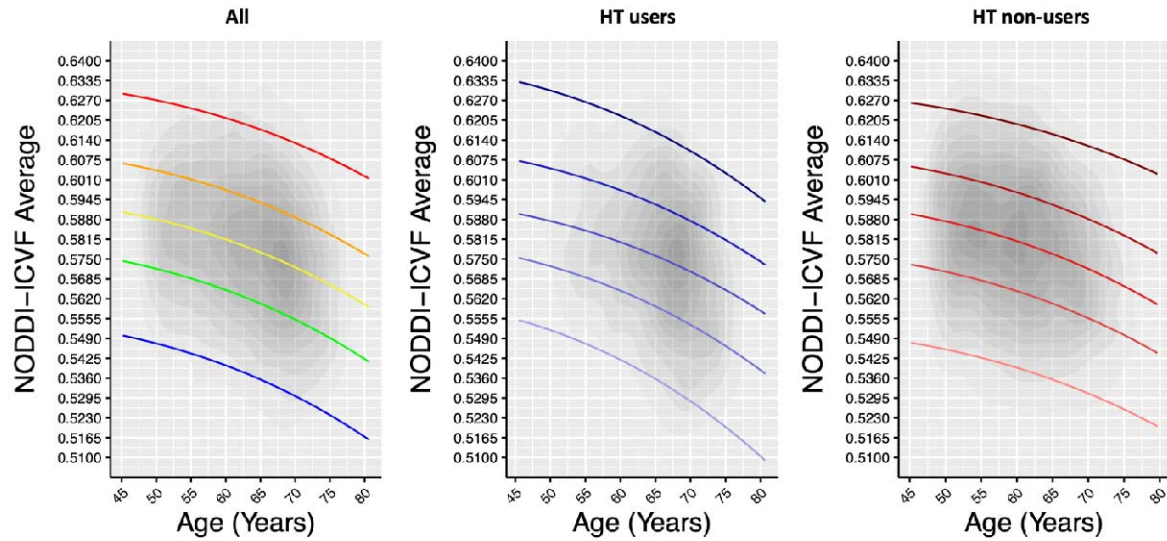
## RESULTS

### Age-related trajectories in HT

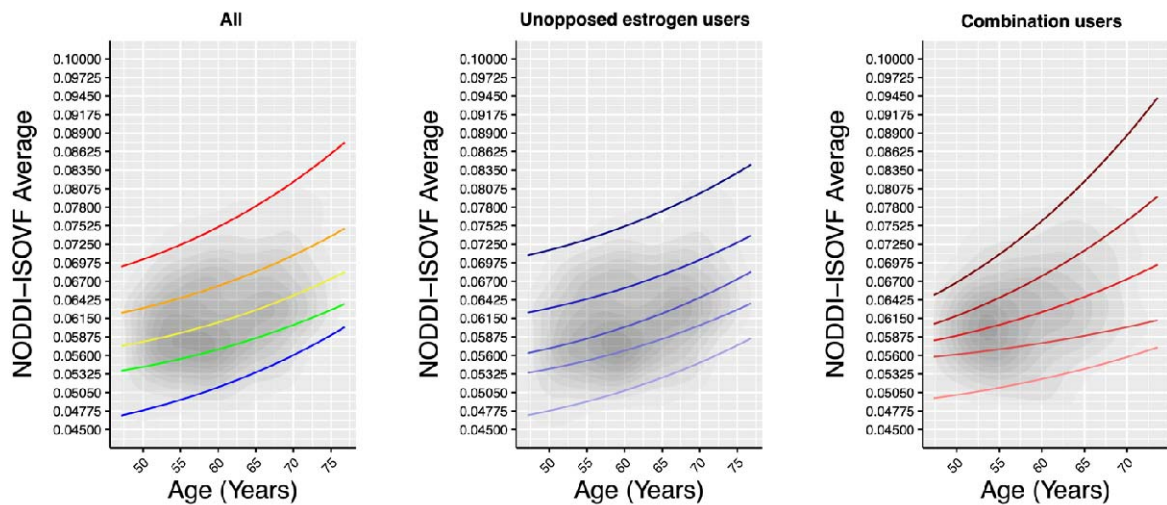
There was a significant interaction between age and HT status on diffusion metrics ICVF<sup>NODDI</sup>; (decreased intra-cellular volume fraction with age;  $p=.0009$ ;  $age^{(p0.5)}$ ) when including the main nuisance covariates (**Figure 1**). We did not detect significant interactions between age and HT status on diffusion metrics DTI or TDF. Age effects on ICVF<sup>NODDI</sup> were confirmed when adjusting for history of OC (decreased with age;  $p=.001$ ;  $age^{(p0.5)}$ ). Supplemental analyses also adjusting for surgical history (hysterectomy and oophorectomy), cancer history, and number of childbirths as nuisance covariates did not confirm the significant age effect seen on diffusivity metric ICVF<sup>NODDI</sup> in HT users and non-users. Within the group of HT users (N=3,033), no association was found between the significant dMRI measures and duration of HT use, age at HT initiation and age at menopause (all  $p>.05$ ).

Follow-up *post-hoc* exploratory analyses in the HT users group – examining unopposed (N=300, age (mean±SD)=61.1±7.4) and combined (N=90; age (mean±SD)=58.4±6.2) estrogen treatments – revealed a significant age interaction on diffusion metric ISOVF<sup>NODDI</sup> (increased free water with age in both groups;  $p=.033$ ;  $age^{(p1)}$ ; **Figure 2**). No significant interaction was found on diffusion metrics DTI or TDF. Adjusting for history of OC confirmed findings on ISOVF<sup>NODDI</sup> (increased with age;  $p=.034$ ;  $age^{(p1)}$ ). Additionally adjusting for duration of HT, age at HT onset and age at menopause, did not alter age effects seen on ISOVF<sup>NODDI</sup> in HT users using unopposed and combination estrogen treatments ( $p=.01$ ;  $age^{(p1)}$ ,  $p=.01$ ;  $age^{(p1)}$ , and  $p=.02$ ;  $age^{(p1)}$ , respectively). Specifically, in combination HT (estrogen + progestin) users, later age at HT onset (*left panel Figure 1 Supp Material*), prolonged duration of HT therapy (*middle panel*), and later age at menopause (*right panel*), were associated with higher ISOVF<sup>NODDI</sup>, relative to estrogen only HT users. In the estrogen only HT group, no significant association was found between clinical variables duration of use, age at initiation and age at menopause and ISOVF<sup>NODDI</sup> ( $r=0$  to  $0.1$ ,  $p=.9$  to  $1.0$ ). In the combination HT group, a weak positive correlation was found between duration of HT and ISOVF<sup>NODDI</sup> ( $r=.2$ ,  $p=.04$ ), while no significant association was found between ISOVF<sup>NODDI</sup> and age at HT initiation ( $r=.15$ ,  $p=.16$ ), or age at menopause ( $r=.18$ ,  $p=.13$ ) in this group (**Figure 1 Supp Material**).

Representative centile curves for each significant diffusion metric are presented in **Figures 1 and 2** with colored lines indicating 5th (black), 25th (blue), 50th (red), 75th (green), and 95th (purple) centiles, and kernel density maps indicating the degree of data point overlap. Curves show age-dependent trajectories for ICVF<sup>NODDI</sup> (**Figure 1**), and ISOVF<sup>NODDI</sup> (**Figure 2**). In summary, all the HT status effects on the diffusion metrics were in the direction of ‘more aging’ – decreased ICVF<sup>NODDI</sup>, and increased ISOVF<sup>NODDI</sup>.



**Figure 1. Normative centile reference curves for  $ICVF^{NODDI}$  in HT users and non-users.** Whole brain white matter averages for  $ICVF^{NODDI}$  are shown for HT (*middle panel*) and non-users (*right panel*), and collectively (*left panel*). Solid colored lines, bottom-up, indicate the following centiles: 5th, 25th, 50th, 75th, 95th. Kernel densities indicating the degree of data point overlap (and sampling density across the age range), are shown in grey.



**Figure 2. Normative centile reference curves for  $ISOVF^{NODDI}$  in unopposed and combination estrogen users.** Whole brain white matter averages for  $ISOVF^{NODDI}$  shown for estrogen users and combination users, collectively (*left panel*) and separately for unopposed estrogen (*middle panel*) and combination (*right panel*) users. Unopposed estrogen users (N=300) displayed a steeper  $ISOVF^{NODDI}$  aging trajectory compared to combination users (N=98). Solid colored lines, bottom-up, indicate the following centiles: 5th, 25th, 50th, 75th, 95th. Kernel densities indicating the degree of data point overlap (and sampling density across the age range), are shown in grey.

### ***Age-related trajectories in OC***

There was no significant interaction between age and OC status on any of the diffusion metrics assessed when including the main nuisance covariates ( $p > .05$ ). Supplemental analyses including surgical history (hysterectomy and oophorectomy), cancer history, and number of childbirths as nuisance covariates confirmed no significant interaction between diffusion metrics and age in OC users and non-users ( $p > .05$ ).

## DISCUSSION

We examined the association between exogenous sex hormone exposure and the brain's WM aging trajectories in post-menopausal middle aged and older women with and without hormone therapy (HT), as well as oral contraceptives (OC). To thoroughly examine microstructure, we used 3 increasingly sophisticated diffusion models, from single-shell tensor-based (DTI and TDF) to multi-shell (NODDI) methods. We also present normative reference curves for various aspects of white matter microarchitecture in women, which may one day allow us to identify individuals with the most severe neural pathology.

As a whole, age and sex hormone exposure usage were both statistically associated with WM metrics, with advanced dMRI model NODDI capturing these differences most sensitively. We found that HT usage was associated with less favorable aging patterns, observed as more pronounced white matter changes on advanced white matter metrics, relative to those who did not use HT (**Figure 1**). The observed less favorable aging trajectories in this sample were independent of previous OC usage; however, history of pregnancies, surgeries, or cancer were found to influence these trajectories. Furthermore, accounting for differences in hormone therapy formulation, we showed that not all HT formulations may exert a detectable neuroprotective effect, at least on the white matter measures we examined here. Hormone replacement therapy containing conjugated estrogens may be associated with marginally more beneficial aging patterns (less pronounced white matter changes) than formulations containing estrogen alone (**Figure 2**). These aging effects on white matter metrics were independent of the duration of hormone therapy, the age at which hormone therapy was initiated and the age at which women entered menopause (**Figure 1 Supp**). Moreover, OC was not found to alter the derived white matter measures considered in this study, nor did clinical factors modulate white matter aging trajectories in OC users and non-users. To the best of our knowledge, the current work is the first study of the associations between exogenous hormone exposure effects on aging in white matter in a population-based cohort.

HT usage was associated with a steeper WM aging trajectory, and this was evidenced by lower neurite density (ICVF<sup>NODDI</sup>) in the HT user group relative to non-users (**Figure 1**). Furthermore, unopposed estrogen usage was associated with a steeper WM aging trajectory, and this was evidenced by increased isotropic volume fraction (ISOVF<sup>NODDI</sup>) relative to combination estrogen usage. NODDI is a multi-shell model of tissue microstructure developed to better describe the underlying WM tissue structure than traditional diffusion-tensor models like DTI or its mathematical extension TDF. While tensor-based models assume that each voxel comprises of a single tissue compartment, NODDI directly models multiple aspects of the cellular environment (Zhang et al., 2012). Notably, the NODDI model can remove the effect of CSF contamination (e.g., following cortical atrophy due to aging processes), increasing the specificity to the cytoarchitecture subjected to investigation. The diffusion metric ISOVF<sup>NODDI</sup> represents the fraction of water molecules that are not restricted or directed and is also described as 'free water'. Higher free water may also be an index of neuroinflammation as neuroinflammatory processes can increase the proportion of water molecules diffusing freely in the extracellular space. Thus, the observed

increase in circulating sex-hormone levels following HT use in postmenopausal women, and specifically in women taking HT formulations containing estrogen alone, may suggest increased susceptibility to mechanisms of neuroinflammation or neuronal loss in this group. These findings are in line with our hypothesis that sex hormone therapy would *negatively* impact women's WM aging. This corroborates prior reports of negative effects of exogenous sex hormones on brain structural measures and expands them to include WM microstructural deficits. Prior aging and AD research has implicated the progression of tau protein to neurofibrillary tangles and the resulting destabilization of axonal microtubules (Spillantini and Goedert 2013), as well as cortical grey matter volumetric reductions and neuronal dispersion (Colgan et al. 2016). It is possible that in postmenopausal women, with age, as the cortical structure atrophies, the space becomes occupied by CSF (or free water), which is reflected by higher isotropic volume fraction values. While further clinical measures and investigations at the microstructural level are necessary, our findings may suggest increased susceptibility to developing tau-dependent pathologies such as AD later in life in middle- and older-aged women with a history of HT use, specifically in estrogen-only HT users. Conversely, our findings are consistent with a neuroprotective effect of sex hormones during normal development but a subsequent deterioration in WM metrics in later life in women using combination HT.

We failed to detect changes in WM aging trajectories in middle- and older-aged women following OC treatment. Prior investigations in the UK Biobank reported reductions in cortical gray matter volume in OC users relative to never-users, worsening by duration of OC treatment (de Lange et al. 2019). To the best of our knowledge, this is the largest investigation of OC effects on white matter aging trajectories in middle-aged to older women. While it is possible that chronic ovarian hormone suppression (induced by OC treatment) may progressively affect WM microstructure (as well as cortical volume) later in life, longitudinal studies are needed to draw further conclusions. We cannot exclude that the lack of detectable effects in OC users on the brain's WM in this sample may depend on the type of OC formulation, which was not possible to assess in the current study with the currently available data in the UK Biobank. Birth control formulations vary from ethinylestradiol-only formulations to those with added concentrations of progestin, and we may expect that differences in formulation may exert a differential effect on diffusion metrics. With this in mind, future studies should disentangle effects of birth control formulation on aging trajectories in women. There are also changes occurring in the societal use and duration and timing of OC use. The number of women availing of OC treatment is increasing, while the age of first contraceptive use is constantly decreasing to sensitive neuroplastic periods during puberty. Given these factors, future research efforts are warranted to investigate OC effects on the brain longitudinally across the lifespan.

The female immune system changes significantly during pregnancy and menopause (Mor et al. 2011; Mishra and Brinton 2018), and evidence suggests that immune regulation during these major transitional phases may influence women's brain aging trajectories later in life (Ding et al. 2013; Mosconi et al. 2017; Fox et al. 2018). Hormonal fluctuations and their interactions with immune processes play a role in maternal brain adaptations, but their long-term effects on brain

aging in women are unknown (Barth and de Lange 2020). Pregnancies are associated with alterations in microglia density, number, and activity which could modulate neuroplastic compensation in response to perimenopausal inflammation processes (Barth and de Lange 2020). The E2 receptor is a key neuroplasticity regulator in the female brain (Barha and Galea 2010), and it has been suggested that neuroplasticity may be important in understanding the boundaries between normal aging and the early stages of Alzheimer's disease (Fjell et al. 2014). In our analyses, the number of childbirths may modulate the age effects on neurite density (a steeper aging WM trajectory) in HT users relative to non-users. Pregnancy-related immune adaptations, in conjunction with endocrinological modulations, may influence maternal brain plasticity during pregnancy and *post-partum*, potentially influencing the course of neurobiological aging later in life. In this study women had on average ~2 children, thus we cannot exclude that a higher number of childbirths, alongside other clinically relevant factors (such as number of abortions and miscarriages), may differentially influence aging trajectories on WM metrics. Prior investigations within the UK Biobank have shown that subjects with two or three offspring had significantly reduced brain age compared to those without offspring (Ning et al., 2020). Although beyond the scope of this analysis, irrespective of HT, we found that parity affected the dispersion of intra-voxel freely diffusing water molecules (ISOVF<sup>NODDI</sup>) overall in the brain, which may corroborate our study findings and findings by Ning et al., (2020) on apparently reduced brain aging and altered cognitive function in subjects with two or three offspring (Ning et al. 2020).

The 'healthy cell bias of estrogen action hypothesis' (Brinton 2008) suggests that neuronal viability and general health - before starting hormone therapy - might be of importance for exogenous estrogens to exert therapeutic effects. This hypothesis may be relevant for women undergoing surgeries that can cause a drop in circulating estrogen levels such as hysterectomy and/or oophorectomy and lead to early menopause. A history of hysterectomy and/or oophorectomy was accounted for in the present study and was found to influence age effects on neurite density seen in HT users relative to non-users. Our results support the 'critical period hypothesis' for estrogens, as an early initiation of (combination) HT was associated with less evident white matter aging (particularly before menopause, as findings did not change when covarying for age at menopause). Of note, HT can be also used to slow or stop the growth of cancers that use hormones to grow, such as some breast cancers. In this study, age effects on neurite density seen in HT users relative to non-users were influenced by cancer history in women (also including breast, womb, and ovarian cancers).

The second theory regarding hormone therapy effects is known as the 'critical period hypothesis' (Maki 2013), whereby HT may be neuroprotective if initiated soon after cessation of ovarian function (<5 years from menopause; (MacLennan et al. 2006; Erickson et al. 2010; Espeland et al. 2015), but carry detrimental effects if initiated much later (>10 years from menopause, (Hodis et al. 2016). Substantial evidence suggests that HT formulation, administration, dosage, compound composition, and mode of administration are clinically relevant to the course of aging in women (Gleason et al. 2015; Savolainen-Peltonen et al. 2019). Within the groups of HT and OC users, we failed to detect any meaningful association between the significant dMRI measures and duration of HT use, age at HT initiation and age at menopause (all  $p>0.05$ ). We

observed a weak positive association between duration of HT and ISOVF<sup>NODDI</sup>, whereby later commencement of therapy was associated with higher volume fraction of extracellular isotropic free water in the combination estrogen group (trends depicted in **Figure 1 Supp**). Even so, controlling for duration of treatment in our analyses did not alter age effects on ISOVF<sup>NODDI</sup> in this treatment group. We cannot exclude that later commencement of HT may be associated with greater reductions in age-dependent metrics of WM microstructure beyond those assessed by the present study, and that other clinical factors (e.g., examining genotype interactions) not considered by the present study may further explain this association. Observing the effects of HT on brain aging in women within such a short interval (within 5 years from menopause) could have implications for understanding hormone-related dementia pathogenesis in women. Future studies should account for such differences to disentangle effects of HT treatment regime on WM microstructural decline in women and identify other vulnerability factors and critical age windows for administering HT in women.

Estrogens interact with multiple neurotransmitter systems in our brain to modulate mood and cognition (Barth et al. 2015); in particular, the interaction with dopamine might be of interest considering its role in pathophysiological processes of neurological, as well as psychiatric disorders, and its modulation of executive functions such as working memory and reward processing which are often impaired in subjects with dementia or AD (Reeves et al. 2009). Estrogen receptors (ERs) - ER $\alpha$  and ER $\beta$  – are widely distributed in the brain and found in subcortical limbic gray matter and basal ganglia areas, as well as prefrontal and temporal cortices (Barth et al. 2015). Studies focusing on the role of estrogen receptors and endogenous estrogen signaling have reported neuroprotective effects on the brain, via their effect promoting synthesis of neurotrophins and protecting the brain from inflammation and stress (Brann et al. 2007). The expression of the ERs can be overlapping or distinct, dependent upon brain region, sex, age, and exposure to hormones. During the time of menopause, there may be changes in receptor expression profiles, post-translational modifications, and protein-to-protein interactions that could lead to a very different environment for estrogen to exert its effects (Mott and Pak 2013). These effects have been considered in clinical trials of those suffering from psychiatric disorders where estrogen-signaling pathways have been shown to be compromised (Hwang et al. 2021). Changes in circulating estrogen levels may modulate the microstructure of WM and contribute to pathophysiological processes of neurological and psychiatric disorders in women with a history of HT.

Moreover, studies in experimental animal models have established a role for sex hormones including estrogen in WM abnormalities and have provided a convincing rationale for HT in prevention and treatment of dementia (Birge 1996; Cerghet et al. 2009). Interventional trials of estrogen and its analogs (often in conjunction with other adjuvants) are ongoing to investigate the long-term safety and efficacy of these compounds to restore structural integrity and related cognitive function of the brain in participants with dementia and early-stage AD. A comprehensive and integrated understanding of estrogens and estrogen signaling across multiple levels of the brain system architecture, from cellular to molecular to systemic, is key to elucidate the mechanisms involved in its effects in diseased brains. Future studies are warranted to examine longitudinal white matter changes in women following sex-hormone therapy – both HT and OC.



There are some methodological considerations in this study. Besides using multiple statistical approaches, a strength of the current work was the inclusion of multiple diffusion metrics, from tensor-based to “beyond-tensor” models to provide a richer understanding of the underlying WM structure than traditional diffusion metrics alone. Besides the tensor-based metric, FA, we considered the estimated number of crossing fibers, fiber complexity, neurite dispersion and estimated numbers of fiber compartments. Diffusion metric FA can lack specificity as it does not directly delineate changes in tissue microstructure – for example a reduction in FA can be associated with different types of microstructural changes, such as demyelination, or a reduction in axonal density. A decline in FA with age could result from many cellular factors, including decreases in the density or an increase in the dispersion orientation of neurites (Pines et al. 2020). Multi-compartment models such as NODDI attempt to overcome this by modeling diffusion data using a set of indices that are more directly related to WM microstructure.

Moreover, TBSS is a widely used method for whole-brain voxel-based analysis but has some limitations. TBSS reduces individual white matter tracts to a skeleton, delineating the center of the tracts and projecting onto it only the highest value of FA along the projection. This may result in loss of microstructural information and potential artifacts (Bach et al. 2014), some due to misregistration. In this study, we carried out careful qualitative and quantitative assessments of registration for each subject’s diffusion metric. Additionally, while we measured diffusivity indices on the FA skeleton, some of these indices may not have a local maximum at the exact same location as FA. Future studies should investigate if findings hold without white matter skeletonization, i.e., without warping images into a predefined template, but by averaging values within regions of interest (ROIs) in native space (Nir et al. 2021). TBSS has limited anatomical specificity (adjacent tracts may not be distinguished) and thus may be susceptible to false positives (Bach et al. 2014). Also, while these limitations may arise for tract-specific diffusion metrics, we chose to focus our analyses on whole-brain diffusion averages.

Unlike a randomized clinical trial, where treatments are randomized to individuals, and the effects are studied longitudinally, the current design is a naturalistic study of people using medications. As such, we report associations that may still be important in understanding brain aging trends in a broad and inclusive population and suggest mechanisms that could be tested in a causally informed design (such as an RCT). To further understand confounders in the population, future studies could seek demographic, educational, or cultural factors that might affect HT/OC use or access, and test if such factors might mediate any detected effects.

We also note that the meaning of the term “trajectories” may differ when inferred from cross-sectional rather than longitudinal data, as individuals at different parts of the age range may differ from each other in their childhood developmental experiences, environments, and health risks throughout life. As the participants range in age by almost 40 years, any interactions with age could also be due to societal changes in the incidence of use, duration of use, and breadth and diversity of access to HTs and OCs. Also, attrition of individuals late in life (due to mortality, or ill health) means that older individuals who participate in the study may show less steep aging trajectories than a typical individual in the population (due to selection bias, or survivor bias).

This study shows the value of testing alternative models for lifespan trajectories beyond popular linear and quadratic models, especially when dealing with large samples. The fractional polynomial approach may offer a more flexible alternative to linear or quadratic models and may be useful for estimating age effects on health outcomes. Large scale datasets such as the UK Biobank offer the opportunity to test alternative models for lifespan trajectories beyond traditional statistical models. Studies with a large number of data points may benefit from evaluating findings across alternative explanatory models to understand the robustness of findings.

The cross-sectional nature of this study does not enable causal inference, so future studies should use longitudinal designs – ideally randomized – which are vital to fully understand how estrogen exposure influences brain aging across the lifespan. The various effects of exogenous sex hormones on brain function deserve greater critical observation to unravel possible pathogenetic mechanisms, as well as to identify individuals at high risk of hormone therapy-related adverse consequences such as dementia or AD. Future studies may benefit from including further clinical and plasma measures and examining genotype interactions (e.g., with apolipoprotein E genotype) to better understand how estrogen exposure influences brain aging and genetic predisposition for neurological disorders in women. Such studies have long-term public health implications and may eventually improve early detection, clinical intervention, and quality of life for individuals at risk for age-related neurodegenerative disorders.

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	HT users	non-users	t-test	p
Sample, N	3,033	5,093		
Age at scan [years] <i>mean±SD</i> <i>range</i>	65.4±6.5 45.5-80.7	60.3±7.1 45.2-79.6	32.1	<0.001
Age at Menopause <i>mean±SD</i>	49.1±5.9	51.0±4.1	14.6	<0.001
Number of live births <i>mean±SD</i> <i>median</i> <i>range</i>	1.81±1.1 2 0-7	1.72±1.2 2 0-9	3.7	<0.001
Waist-to-hip <i>mean±SD</i>	1.6±0.5	0.81±0.5	3.4	<0.001
Education [N] <i>high school / college</i>	1290 / 1743	1713 / 3380	64.6	<0.001
			$\chi^2$ -test	p
Menopause [N, %] <i>yes</i>	2,998 (98.9%)	4,508 (88.5%)	250.5	<0.001
Hysterectomy [N, %] <i>yes</i>	404, 13.3%	210, 4.1%	677.7	<0.001
Oophorectomy [N, %] <i>yes</i>	535, 17.6%	175, 3.4%	491.4	<0.001
Age at HT onset <i>mean±SD</i>	47.8±5.6	-	-	-
Duration of HT therapy [years] <i>mean±SD</i> <i>median</i> <i>range</i>	7.1±6.2 5 0.3-38	-	-	-
Diabetes <i>yes</i>	113, 3.7%	159, 5.2%	101.7	<0.001
Hypertension <i>Heart attack</i> <i>Angina</i> <i>Stroke</i> <i>High blood pressure</i>	15 29 20 447	17 24 19 515	48.9	<0.001
Diagnosis of Major Depression Disorder <i>Probable recurrent major depression (severe)</i> <i>Probable recurrent major depression (moderate)</i> <i>Single probable major depression episode</i>	73 160 92	93 237 116	101.1	<0.001

**Table 1. Sample demographics for HRT users and non-users.** Data shown as Mean  $\pm$  standard deviation (SD), % for each variable in each of the groups, N = sample size; BMI = body mass index; HT = hormone replacement therapy;  $\chi^2$ -test = chi-squared test.



	OC users	non-users	t-test	p
Sample, N	6,964	1,156	-	-
Age at scan [years] <i>mean±SD</i> <i>range</i>	61.8±7.1 45.2-80.7	65.1±7.9 46.1-79.6	14.6	<0.001
Age at Menopause <i>mean±SD</i>	50.3±5.0	50.3±5.1	0.27	0.79
Number of live births <i>mean±SD</i> <i>median</i> <i>range</i>	1.8±1.1 2 0-9	1.7±1.4 2 0-8	2.03	0.04
Waist-to-hip <i>mean±SD</i> <i>median</i>	0.81±0.7 0.80	0.81±0.07 0.81	0.26	0.797
Education [N] <i>high school / college</i>	2,495 / 4,468	507 / 649	27.4	<0.001
			$\chi^2$ -test	p
Menopause [N, %] <i>yes</i>	5,327, 76.5%	926, 80.1%	4.1	0.04
Hysterectomy [N, %] <i>yes</i>	496, 7.1%	118, 10.2%	13.4	<0.001
Oophorectomy [N, %] <i>yes</i>	599, 8.6%	111, 9.6%	1.2	0.23
Age at OC onset <i>mean±SD</i>	20.8±4.3	-	-	-
Duration of OC therapy [years] <i>mean±SD</i> <i>median</i> <i>range</i>	11.7±8.4 10 1-46.6	-	-	-
Diabetes <i>yes</i>	232, 3.3%	40, 3.5%	101.4	<0.001
Hypertension <i>Heart attack</i> <i>Angina</i> <i>Stroke</i> <i>High blood pressure</i>	28 48 32 791	4 5 7 172	48.9	<0.001
Diagnosis of Major Depression Disorder <i>Probable recurrent major depression (severe)</i> <i>Probable recurrent major depression (moderate)</i> <i>Single probable major depression episode</i>	148 350 182	18 47 27	86.0	<0.001

**Table 2. Sample demographics for OC users and non-users.** Data shown as Mean ± standard deviation (SD), % for each variable in each of the groups, N = sample size; BMI = body mass index; OC = oral contraceptive;  $\chi^2$ -test = chi-squared test.

<i>Method</i>	<i>Metric</i>	<i>Description</i>	<i>Advantages</i>	<i>Limitations</i>	<i>Reference</i>
Diffusion-tensor imaging (DTI)	FA <sup>DTI</sup>	Fractional anisotropy. Describes the level of anisotropy in a diffusion process	<ul style="list-style-type: none"> <li>Diffusion-tensor metrics are widely used as surrogate measures of microstructural tissue change during normal brain development and aging, or during the onset and progression of neurological disorders. DTI provides sensitivity to tissue microstructure</li> <li>It is a widely used scalar measure to characterize tissue microstructure</li> <li>Short acquisition protocols</li> </ul>	<ul style="list-style-type: none"> <li>It can only model a single fiber population, with a single dominant orientation, at every voxel. Limited in crossing and curving areas, cannot model dispersing, crossing or kissing fibers</li> <li>Assumes that each voxel comprises a single tissue compartment, which creates a partial volume effect due to the presence of extracellular free water, such as the CSF</li> <li>The biological interpretation of its microstructural parameters can be often equivocal</li> <li>Cannot be used on multi-shell data</li> </ul>	(Pierpaoli et al. 1996; Jones and Cercignani 2010)
	MD <sup>DTI</sup>	Mean diffusivity. Describes the mean rate of diffusion			
	RD <sup>DTI</sup>	Radial diffusivity. Measures diffusivity across the principal tensor direction			
	AD <sup>DTI</sup>	Axial diffusivity. Measures diffusivity along the principal tensor direction			
Tensor distribution Function (TDF)	FA <sup>TDF</sup>	Fractional anisotropy. Describes the level of anisotropy in a diffusion process	<ul style="list-style-type: none"> <li>Reconstruct multiple underlying streamlines by representing the diffusion profile as a probabilistic mixture of Gaussian tensors</li> <li>Increased sensitivity compared to DTI measures. Resolves more complicated white matter configurations, e.g., crossing fiber tracts, relative to corresponding DTI-derived measures</li> </ul>	<ul style="list-style-type: none"> <li>Remains a diffusion-tensor model with limitations in areas where fibers are crossing and curving; can reconstruct only one fiber direction</li> <li>Cannot be used on multi-shell data</li> </ul>	(Leow et al. 2009; Isaev et al. 2017; Nir, Jahanshad, Villalon-Reina, Isaev, Zavaliangos-Petropulu, Zhan, Leow, Jack, et al. 2017)
Neurite Orientation Dispersion and Density Imaging (NODDI)	OD <sup>NODDI</sup>	Orientation dispersion. Describes the angular variation and spatial configuration of neurite	<ul style="list-style-type: none"> <li>Multi-shell model of tissue microstructure developed to better describe the underlying tissue structure than diffusion-tensor models.</li> <li>Greater biophysical specificity, compared to tensor-based models: accounting for different</li> </ul>	<ul style="list-style-type: none"> <li>Absence of any direct diffusivity estimation. Cannot evaluate the complex neurite anisotropic dispersion as it models only the isotropic dispersion of neurite.</li> </ul>	(Zhang et al. 2012)

	ICVF <sup>NODDI</sup>	Isotropic volume fraction. Describes the amount of neurites within a voxel	<p>tissue compartments.</p> <ul style="list-style-type: none"> <li>• Ability to disentangle the contributions of axonal/dendritic density and fiber orientation to microscopic changes.</li> <li>• Ability to provide the characteristics of angular variations of neurites in each voxel.</li> <li>• Can be used on multi-shell data.</li> </ul>	<ul style="list-style-type: none"> <li>• Requires multi-shell data (ODI can be performed on single-shell data).</li> </ul>	
	ISOVF <sup>NODDI</sup>	Isotropic volume fraction. Measures the volume fraction of the isotropic compartment ( <i>free-water</i> , or CSF).			

**Table 3. Diffusivity indices considered by this study.** Diffusivity indices investigated in this study are described, alongside their advantages and limitations.