

1 Supplemental methods

2 1.1 Datasets

3 For all datasets we only extracted data for individuals with more than one time point con-
4 taining non-missing data. For AIBL and ADNI1 age was approximated based on birth year,
5 or both birth year and month respectively.

6 1.1.1 ADNI1

7 Data used in the preparation of this article were obtained from the ADNI database (adni.loni.usc.edu;
8 [3]). The ADNI was launched in 2003 as a public-private partnership, led by Principal Inves-
9 tigator Michael W. Weiner, MD. The primary goal of ADNI has been to test whether serial
10 magnetic resonance imaging (MRI), positron emission tomography (PET), other biological
11 markers, and clinical and neuropsychological assessment can be combined to measure the
12 progression of mild cognitive impairment (MCI) and early Alzheimer’s disease (AD). For
13 up-to-date information, see <http://www.adni-info.org>.

14 1.1.2 AIBL

15 AIBL study methodology has been reported previously [21]. Longitudinal MMSE Data was
16 collected by the AIBL group and was obtained from the AIBL database:

17 <http://www.aibl.csiro.au/adni/index.html>

18 1.1.3 CAMD (C-1013 and C-1014)

19 Data used in the preparation of this article were obtained from the Coalition Against Major
20 Diseases (CAMD) database (<http://c-path.org/programs/camd/>; [4]). The CAMD database
21 provides data only for the placebo arm of AD trials, and provides no further information
22 about the trials or individuals diagnosis at first visit. To ensure sufficient follow-up, we only

23 used data from the two longest running clinic trials in the CAMD database (trials C-1013
24 and C-1014).

25 In 2008, Critical Path Institute, in collaboration with the Engelberg Center for Health
26 Care Reform at the Brookings Institution, formed the CAMD. The Coalition brings together
27 patient groups, biopharmaceutical companies, and scientists from academia, the U.S. Food
28 and Drug Administration (FDA), the European Medicines Agency (EMA), the National In-
29 stitute of Neurological Disorders and Stroke (NINDS), and the National Institute on Aging
30 (NIA). The CAMD includes over 200 scientists from member and non-member organiza-
31 tions. The data available in the CAMD database has been volunteered by CAMD member
32 companies and non-member organizations.

33 1.2 Notation

34 A dataset contains information on individuals $i \in \{1, 2, \dots, n\}$. The set of time points at
35 which individual i has been observed is denoted $\boldsymbol{\tau}^i := (\tau_1^i, \dots, \tau_{\#TP(i)}^i)$. The longitudinal
36 univariate observations (in this example MMSE score) for individual i at time t are given
37 by $x_i(t)$, which is only observed for $t \in \boldsymbol{\tau}^i$ (Figure 1a). $\phi(t; \boldsymbol{\theta})$ is a proposed (parametrised)
38 trajectory (Supplementary Methods), which along with an individual’s offset δ_i is believed
39 to explain the data, i.e. $x_i(t) \approx \phi(t + \delta_i; \boldsymbol{\theta})$. Define an individual’s estimated Disease Time
40 (\hat{DT}) at time t as: $\hat{DT}(i, t) := t + \delta_i$ (Figure 1b).

41 1.3 Estimating disease time

42 Given $\phi(t, \boldsymbol{\theta})$, $\boldsymbol{\tau}^i$ and $x_i(t)$, for each i define a local loss function using sum of squares:

$$local_loss(i, \delta_i, \boldsymbol{\theta}) := \|x_i(\boldsymbol{\tau}^i) - \phi(\boldsymbol{\tau}^i + \delta_i; \boldsymbol{\theta})\|_2^2 \quad (1)$$

43 Using this we estimate the ‘optimal’ offset ($\hat{\delta}_i$), which determines estimated disease time,

44 using ordinary least squares:

$$\hat{\delta}_i(\boldsymbol{\theta}) := \underset{\delta_i}{\operatorname{argmin}} \operatorname{local_loss}(i, \delta_i, \boldsymbol{\theta}) \quad (2)$$

45 This can be minimised (locally) using the *optimise* function.

46 1.3.1 Estimating trajectory parameters

47 For a set of parameters $\boldsymbol{\theta}$ we define a loss function over all individuals:

$$\operatorname{loss}(\boldsymbol{\theta}) := \sum_i \operatorname{local_loss}(i, \hat{\delta}_i(\boldsymbol{\theta}), \boldsymbol{\theta}) \quad (3)$$

48 This involves first estimating $\hat{\delta}_i(\boldsymbol{\theta})$ for all individuals i as above. The $\hat{\boldsymbol{\theta}}$ that minimises *loss*
49 is the one that ‘best’ fits the data. We can estimate a $\hat{\boldsymbol{\theta}}$ leading to a local minimum in loss
50 using the *optim* function.

51 1.3.2 Trajectory models

52 To fit this model we need a parametrised trajectory model $\phi(t, \boldsymbol{\theta})$. In this study we used
53 compared two alternatives:

54

55 (a) a sigmoidal trajectory (also used in [13] and similar to that used in [2]).

$$\phi(t; \boldsymbol{\theta}) = \frac{\theta_1}{1 + \exp(-\theta_2 t)} + \theta_3 \quad (4)$$

56 (b) an exponential decline trajectory (similar to that used in [12])

$$\phi(t; \boldsymbol{\theta}) = \theta_1 - \exp(\theta_2 t) \quad (5)$$

57 1.4 Temporal Clustering algorithm

58 Let K be the number of clusters, and $k \in \{1, \dots, K\}$ represent an individual cluster. Let
59 $c(i) : \{1, \dots, N\} \rightarrow \{1, \dots, K\}$ be the cluster assignment function mapping individuals
60 to clusters. Let θ^k be the parameters of the model representing the k^{th} cluster (Figure
61 1b) and θ_{-1}^k be the all except the first of the trajectory parameters, i.e. excluding θ_1 . To
62 perform clustering we introduce an algorithm based on K-means and our trajectory modelling
63 approach (Algorithm 1).

Algorithm 1 Temporal Clustering

Choose number of clusters K .

1). First fix θ_1 by estimating it across all individuals by minimising Equation 3 with respect to θ .

2). Randomly assign each individual to a cluster,

i.e. sample $c(i)$ for all i randomly with replacement from $\{1, \dots, K\}$.

3). Repeat the following steps up to convergence, defined as no change in $c(i)$.

- For each cluster k , minimise Equation 3 with respect to θ_{-1}^k using only data from individuals for whom $c(i) = k$.
- For each cluster k and individual i , use θ^k and the estimated individual offset $\hat{\delta}_i(\theta^k)$ to calculate the *local_loss* using Equation 1. Reassign each individual i to the cluster k'_i which results in the smallest *local_loss*, i.e. $c(i) \leftarrow k'_i$.

64 For supplementary simulation results only we also used a version of Temporal Clustering
65 without a fixed baseline (θ_1), i.e. a separate baseline version that allowed different clusters
66 to have different baseline (θ_1).

67 Free parameters in Temporal Clustering include the allowed range for δ (default: \pm
68 50,000 days), the initial guess at trajectory parameters (θ ; default: $(28, 4 \times 10^{-4})$), the
69 allowed range for θ_2 if a two parameter trajectory model is being used (default: 0 – 0.005),
70 the number of clusters (K ; here fixed at 2) and the maximum number of iterations (default:
71 30).

72 1.5 Simulation study

73 Two types of simulation study were performed, a disease time estimation simulation (equiva-
 74 lent to $K = 1$) and a Temporal Clustering simulation (i.e. $K = 2$). We performed simulations
 75 based on both the combined dataset, i.e. with the same number of individuals, similar time
 76 points and with longitudinal MMSE data resembling the real data when plotted.

77 First, vectors of true δ were uniformly sampled from an interval chosen to generate
 78 visually plausible data. The interval chosen depended on the value of true θ_2 (Table S4). To
 79 generate time points simulated individuals were randomly assigned the time points of a real
 80 individual in such a way that the last time point would have $\text{MMSE} > 0$ (before error was
 81 added). This simulated missing data due to ‘death’ at $\text{MMSE} > 0$, i.e. no individual had
 82 data with $\text{MMSE} < 0$, simulating death at MMSE equal to zero. To minimise duplicates
 83 of time points used, individuals were sampled without replacement, unless no remaining
 84 individual had a last time point with $\text{MMSE} > 0$ in which case they were sampled from the
 85 full set of individuals. In other words, almost all the simulated individuals will have different
 86 timepoints, but a very small number of simulated individuals will have the same timepoints
 87 but different data.

88 Data was generated based on our model, i.e.

$$x_i(\tau^i) = \phi(\tau^i + \delta_i; \theta) + \epsilon_{i\tau^i} \quad (6)$$

89 Where $\epsilon_{i\tau^i} := \{\epsilon_{i\tau_1^1}, \dots, \epsilon_{i\tau_{\#TP(i)}^1}\}$ and $\epsilon_{it} \sim N(0, 1.5)$ i.i.d.

90 For all the simulations true θ_1 was set to 29. For both the disease time estimation and
 91 Temporal Clustering simulations a range of five θ_2 were used to test the methods sensitivity to
 92 this parameter. For each θ_2 100 simulations were performed. For the disease time estimation
 93 we used $\theta_2 \times 10^4 = 1, 3, 5, 7$ and 9. For the Temporal Clustering simulation we used
 94 $\theta_2^1 \times 10^4 = 5, 3, 5, 6, 8$, and $\theta_2^1 \times 10^4 = 5, 1, 1, 10, 10$.

95 The simulation with $\theta_2^1 = \theta_2^2 = 5 \times 10^4$ was used to test what would happen if there was
96 only one cluster, but the user attempted to find two. This simulation was only used to study
97 trajectory parameter estimation, and was not used in the clustering accuracy calculations as
98 the cluster labels would have been meaningless.

99 To study the impact of various biases we investigated three different data transformations
100 that led to progressively more realistic and biased data in the disease time estimation sim-
101 ulation . The first transformation simulated a floor effect by rounding the few cases where
102 $\text{MMSE} < 0$, due to the addition of noise, up to zero. The second also rounded each $x_i(t)$ to
103 its nearest integer, as MMSE can only take integer values. The third additionally imposed
104 a ceiling of $\text{MMSE} = 30$, the maximum score from the real MMSE test, i.e. all $x_i > 30$ were
105 set to 30. For the Temporal Clustering simulation featured in Figure 3 we only generated
106 simulated data with all three of these transformations applied.

107 2 Supplementary results

108 In a simulation the disease time estimation approach worked best with a δ range of $\pm 50,000$
109 days (Figures S2 - S3), i.e. using this led to trajectory parameter estimates that were closer
110 to their true value, especially when the true rate parameter was low (e.g. $\theta_1 = 1 \times 10^{-4}$;
111 Figures S2a and S3a). This seemingly high number is probably a sign that overfitting of
112 individual offsets (δ_i) are occurring. For more on this see the Discussion.

113 In a two-cluster simulation the fixed baseline was better than the separate baseline version
114 of Temporal Clustering at avoiding unrealistic θ_1 estimates, i.e. $\theta_1 > 30$ (Figure S4). In
115 cases where accurate rate estimation is the priority it could make sense to use the separate
116 baseline version, but the fixed baseline version is preferred here as it leads to both trajectory
117 parameters being interpretable, i.e. within realistic bounds.

118 **Supplementary tables**

Table S1: Table comparing diagnosis at last visit with either (a) diagnosis at first visit, or (b) clusters. For (a) a mixture of actual (ADNI & AIBL) and estimated (C-1013 and C-1014) diagnoses are used. For (b) only actual diagnoses for individuals in ADNI and AIBL are used, with clusters filtered (discrimination score > 2). MMSE = Mini-Mental State Examination, NC = Normal Cognition, MCI = Mild Cognitive Impairment, AD = Alzheimer’s disease.

Diagnosis at last visit	Diagnosis at first visit			Filtered clusters (ADNI & AIBL only)	
	NC	MCI	AD	k = 1	k = 2
NC	361	19	0	32	22
MCI	30	476	75	60	43
AD	8	425	1018	99	236

Table S2: Table of delta ranges used to simulate data. Range used depended on θ_2 .

$\theta_2 \times 10^4$	Minimum $\delta \times 10^3$	Maximum $\delta \times 10^3$
1	10	30
3	0	10
5	0	6
6	0	5
7	0	4
8	0	3.5
9	-1	3.5
10	-1.5	3

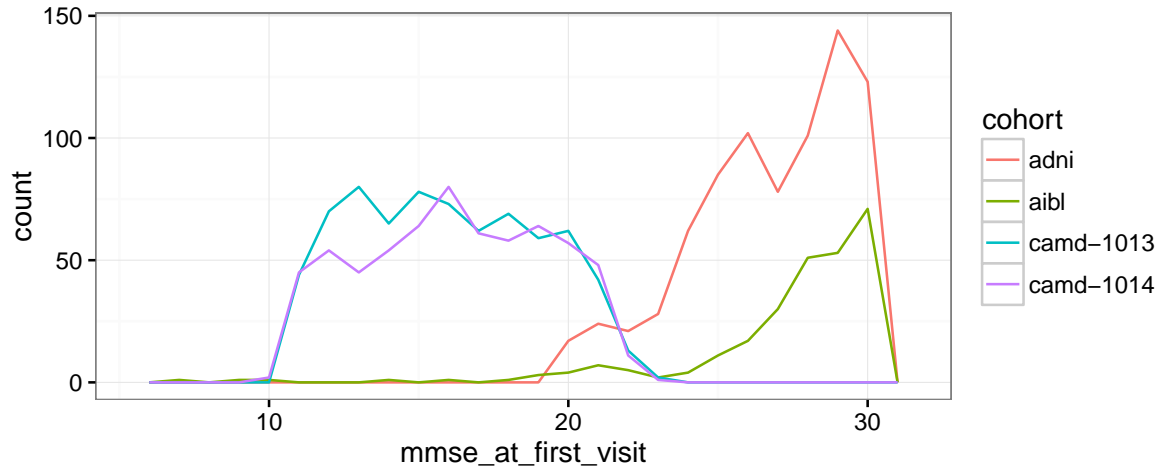


Figure S1: Distribution of MMSE scores at first visit, grouped by cohort.

119 **Supplementary Figures**

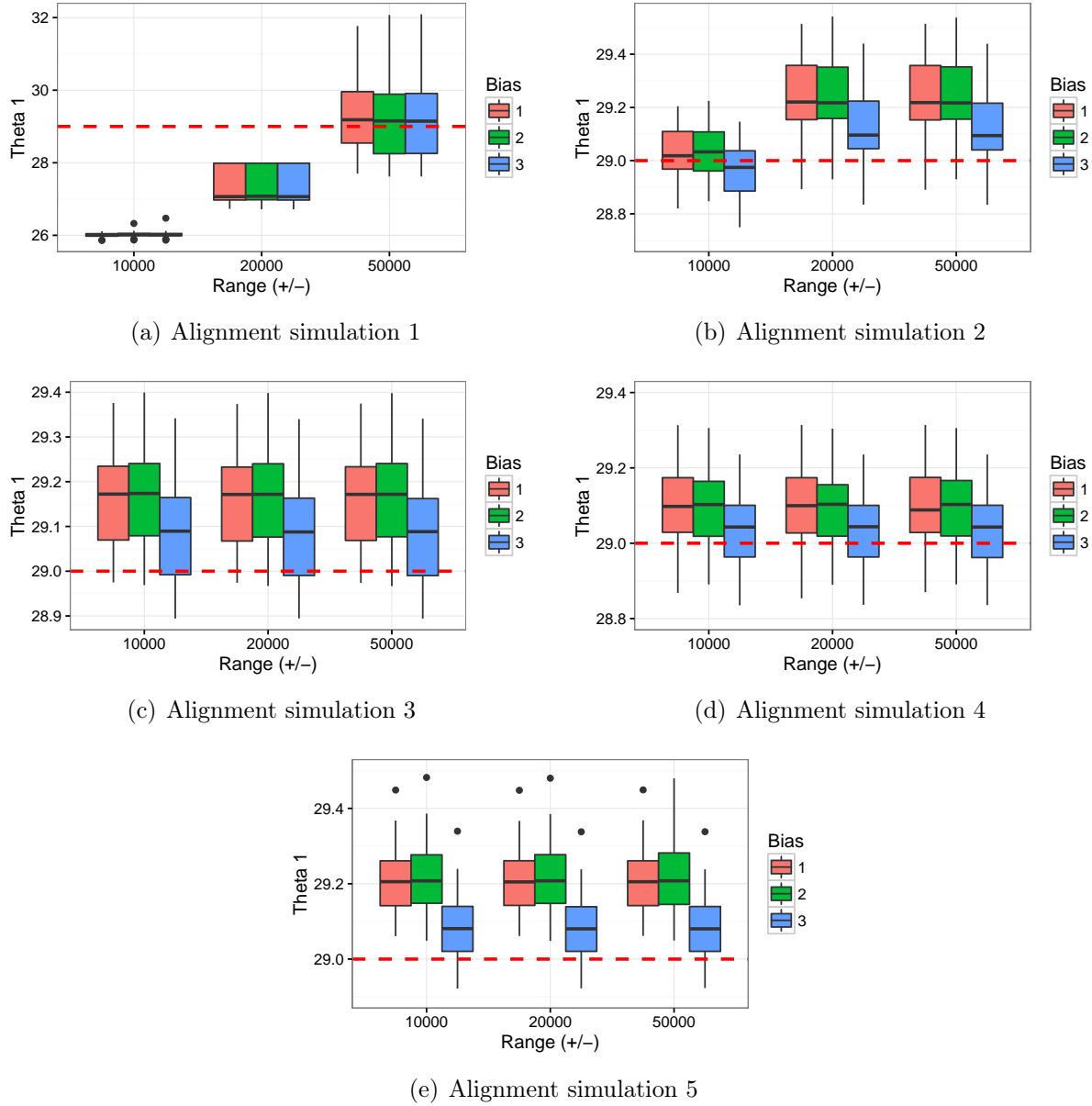
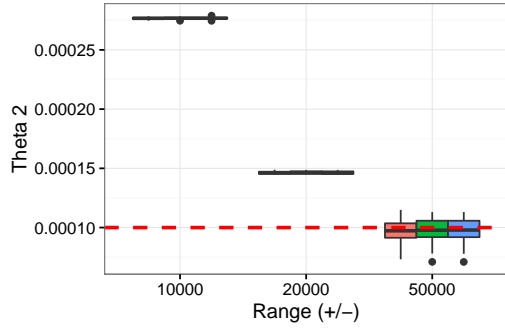
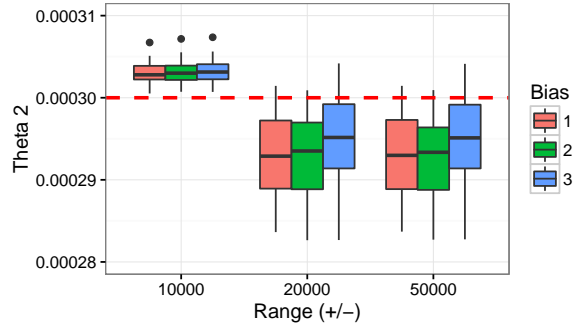


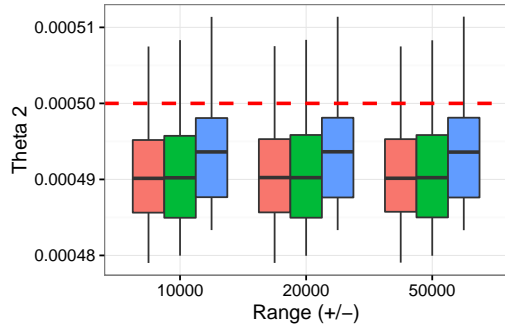
Figure S2: Grouped boxplots showing θ_1 estimates from the disease time estimation simulation. Five simulations each use a fixed true θ , with the true θ_1 indicated by dashed red lines. Each simulation differs only in the true value of θ_2 : (a) 0.0001, (b) 0.0003, (c) 0.0005, (d) 0.0007 and (e) 0.0009. Simulations are based on the combined cohort, i.e. time points, number of samples and visual appearance. For alignment three different δ ranges were used: ± 10000 , 20000 or 50000 . Three versions of each dataset we generated, each with an increasing amount of bias and plausibility. Bias 1 = Real valued data, but with simulated death (i.e. MMSE < 0 removed). Bias 2 = Integer rounded data with simulated death. Bias 3 = Integer rounded data with simulated death and a ceiling effect (MMSE > 30 set to 30). Outliers excluded in plot for clarity: (b) 2 points ~ 28 , (d) 4 points > 30.5 excluded and (e) 1 point > 30.5 excluded.



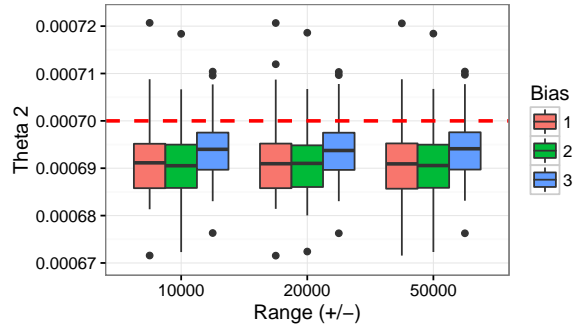
(a) Alignment simulation 1



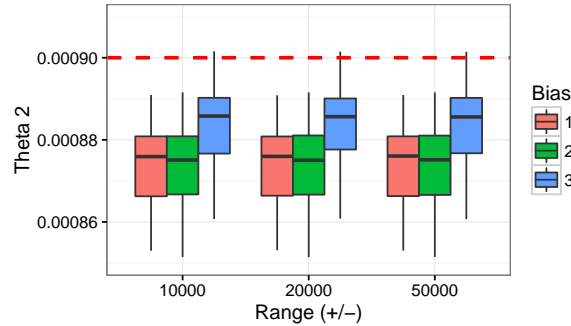
(b) Alignment simulation 2



(c) Alignment simulation 3

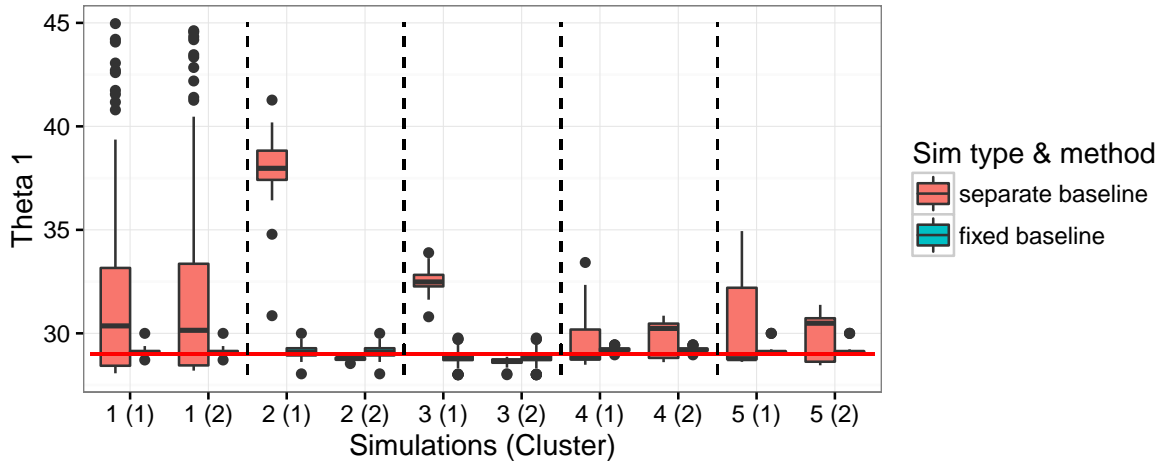


(d) Alignment simulation 4

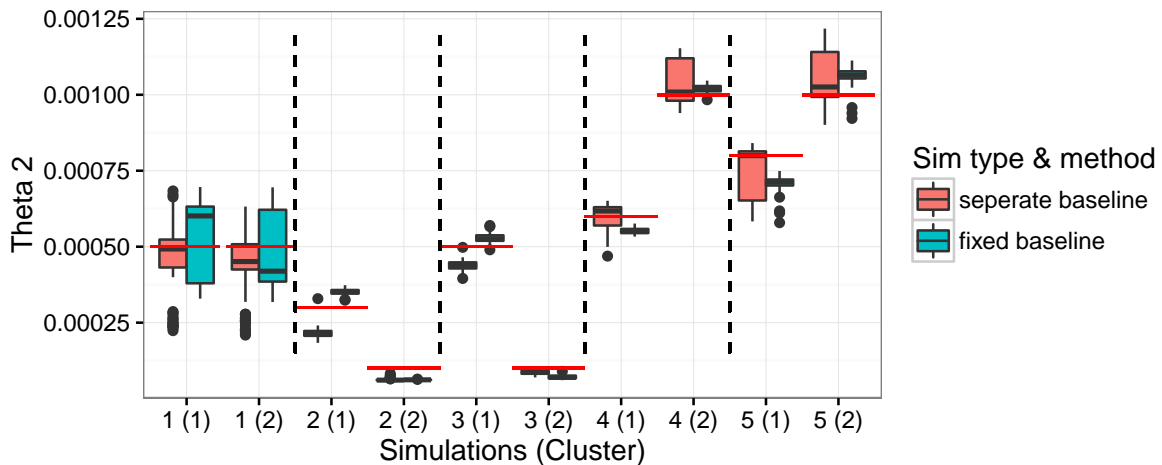


(e) Alignment simulation 5

Figure S3: Grouped boxplots showing θ_2 estimates from the disease time estimation simulation. Five simulations each use a different fixed true θ . Each simulation differs only in the true value of θ_2 , indicated by dashed red lines. Simulations are based on the combined cohort, i.e. time points, number of samples and visual appearance. For alignment three different δ delta ranges were used: ± 10000 , 20000 or 50000 . Three versions of each dataset we generated, each with an increasing amount of bias and plausibility. Bias 1 = Real valued data, but with simulated death (i.e. MMSE < 0 removed). Bias 2 = Integer rounded data with simulated death. Bias 3 = Integer rounded data with simulated death and a ceiling effect (MMSE > 30 set to 30). Outliers excluded in plot for clarity: (b) 2 points > 0.00032 , (d) 4 points ~ 0.0006 excluded and (e) 10 point < 0.00085 excluded.

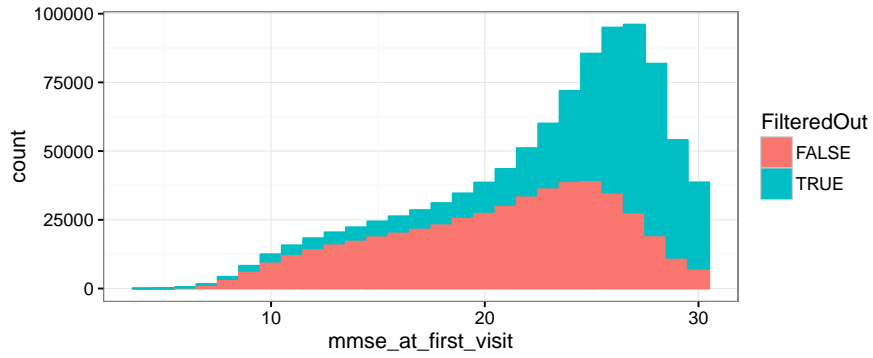


(a) Temporal clustering ($K = 2$) simulation - θ_1 estimates

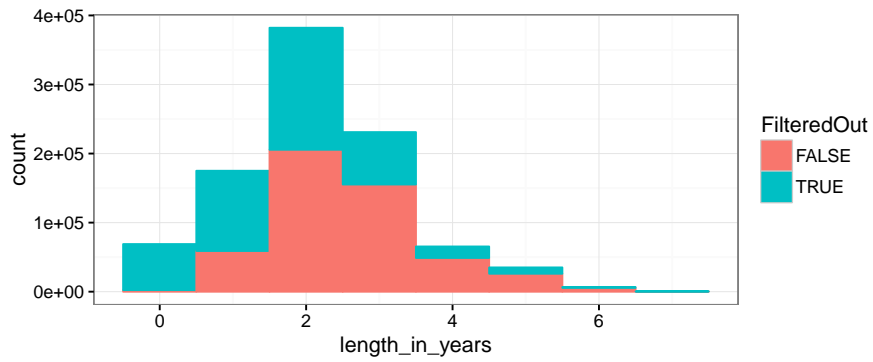


(b) Temporal clustering ($K = 2$) simulation - θ_2 estimates

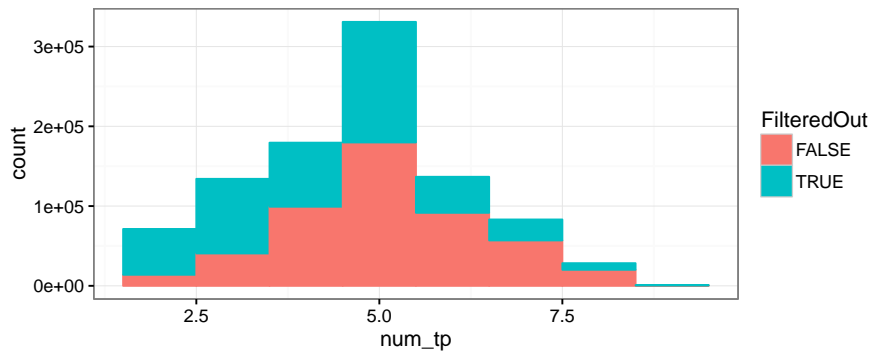
Figure S4: Grouped boxplots showing the result of a simulation study of temporal clustering ($K = 2$). Each simulation differs only in the true value of θ_2^1 and θ_2^2 . The results for each simulation are separated by dashed lines. Simulations are based on the combined cohort, i.e. time points, number of samples and visual appearance. True θ are indicated in red lines. Results are shown for both fixed and separate baseline versions of Temporal Clustering.



(a) MMSE at first visit



(b) Length of follow-up



(c) Number of time points

Figure S5: Characteristics of the simulated individuals removed by a discrimination score filter of two. Stacked histograms are given over 2412 simulated individuals from each 100 iterations of all four simulation types, i.e. different choices of θ_2^1 and θ_2^2 (not including the simulation with $\theta_2^1 = \theta_2^2$). Stacked histograms of the distribution with and without filter of (a) MMSE score at first visit, (b) number of time points and (c) the length of follow-up in days (in year bars).